

# Tissue clearing technique: Recent progress and biomedical applications

Ting Tian<sup>1</sup> | Zhaoyang Yang<sup>2,3</sup> | Xiaoguang Li<sup>1,2,3</sup> 

<sup>1</sup>Beijing Key Laboratory for Biomaterials and Neural Regeneration, School of Biological Science and Medical Engineering, Beihang University, Beijing, China

<sup>2</sup>Department of Neurobiology, School of Basic Medical Sciences, Capital Medical University, Beijing, China

<sup>3</sup>Beijing International Cooperation Bases for Science and Technology on Biomaterials and Neural Regeneration, Beijing Advanced Innovation Center for Biomedical Engineering, Beihang University, Beijing, China

## Correspondence

Xiaoguang Li, Beijing Key Laboratory for Biomaterials and Neural Regeneration, School of Biological Science and Medical Engineering, Beihang University, No. 37 Xueyuan Road, Haidian District, Beijing, 100083, China.

Email: lxgchina@sina.com

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## Abstract

Organisms are inherently three dimensional, thus comprehensive understanding of the complicated biological system requires analysis of organs or even whole bodies in the context of three dimensions. However, this is a tremendous task since the biological specimens are naturally opaque, a major obstacle in whole-body and whole-organ imaging. Tissue clearing technique provides a prospective solution and has become a powerful tool for three-dimensional imaging and quantification of organisms. Tissue clearing technique aims to make tissue transparent by minimizing light scattering and light absorption, thus allowing deep imaging of large volume samples. When combined with diverse molecular labeling methods and high-throughput optical sectioning microscopes, tissue clearing technique enables whole-body and whole-organ imaging at cellular or subcellular resolution, providing detailed and comprehensive information about the intact biological systems. Here, we give an overview of recent progress and biomedical applications of tissue clearing technique. We introduce the mechanisms and basic principles of tissue clearing, and summarize the current tissue clearing methods. Moreover, the available imaging techniques and software packages for data processing are also presented. Finally, we introduce the recent advances in applications of tissue clearing in biomedical fields. Tissue clearing contributes to the investigation of structure-function relationships in intact mammalian organs, and opens new avenues for cellular and molecular mapping of intact human organs. We hope this review contributes to a better understanding of tissue clearing technique and can help researchers to select the best-suited clearing protocol for their experiments.

## KEYWORDS

data processing, light scattering, optical sectioning microscope, tissue clearing technique, whole-body imaging

## 1 | INTRODUCTION

Systematic investigation of the morphology and structure of the organism at single-cell resolution is essential for elucidating the associated mechanisms in health and disease. However, extracting detailed information with a global perspective from an intact biological specimen has been a fundamental challenge in biomedicine, because

biological tissues are mostly opaque, which hinders light penetration into deep tissue and restricts imaging depth and contrast (Zhu *et al.*, 2013).

Conventional histological sectioning techniques provide two-dimensional information about anatomical structures and cellular constituents within tissue samples (Seo *et al.*, 2016). However, biological tissues are virtually three dimensional. For example,

most individual neurons have an irregular structure with neural processes extending in multiple directions, their native structure definitely cannot be ascertained by a thin section (Furth *et al.*, 2018). Therefore, three-dimensional (3D) imaging is indispensable for whole-body and whole-organ cell profiling (Feuchtinger *et al.*, 2016; Matsumoto *et al.*, 2019). Noninvasive imaging techniques, such as computer tomography (CT) (Goldman, 2007), magnetic resonance imaging (MRI) (Hamaide *et al.*, 2016), and positron emission tomography (PET) (Nader and Banks, 2014), allow detailed 3D visualization of anatomical structures in living organisms, and can be applied repeatedly on the same organism for the study of spatiotemporal changes. However, these techniques have limited resolutions, which are insufficient to extract the properties of individual cells. 3D images are traditionally acquired by serial sectioning and postimage reconstruction. Nevertheless, piecemeal reconstructions are laborious and time consuming, and may result in image distortion from folded, compressed, or stretched sections. Automated sectioning imaging techniques can avoid information loss and image alignment in manual sectioning, and have been successfully applied in both light and electron microscopes (Briggman *et al.*, 2011; Li *et al.*, 2018a). Yet these approaches are destructive: the sample is destroyed in a single imaging sequence. Furthermore, the complicated and expensive setup restricts wide applications of these techniques. Nonsectioning imaging techniques have also been developed. For instance, the advent of multiphoton microscope has increased the imaging depth up to hundreds of microns in opaque samples (Denk *et al.*, 1990), but imaging resolution and contrast decline in deeper regions of the tissue due to light scattering. Therefore, multiphoton microscope is inadequate for 3D imaging of large volume tissues like brain and liver.

The recently emerging tissue clearing technique is a promising solution, which allows rapid 3D visualization of intact organs or even whole bodies. Tissue clearing technique renders tissue optically transparent and allows full penetration of light deep into the cleared tissues, hence accelerating the progress of whole-body imaging (Figure 1). In this review, we introduce the mechanisms

and basic principles of tissue clearing, describe the currently available tissue clearing methods, imaging techniques and data processing, and finally present the biomedical applications of tissue clearing.

## 2 | MECHANISMS AND PRINCIPLES OF TISSUE CLEARING

Biological tissues are composed of heterogeneous substances with different optical properties (e.g., refractive index), such as connective tissue fibers, organelles, lipids particles, and proteins (Johnsen and Widder, 1999; Tuchin, 2005). Heterogeneity of RIs among these intrinsic components causes light scattering (Tuchin, 2005; Kim *et al.*, 2018). The incoming light is scattered multiple times as it travels through the tissue, causing decay of light intensity in the forward direction (Tuchin, 1997). Furthermore, light absorption by endogenous light-absorbing substances, such as heme and melanin, further attenuates the light transmission (Weissleder, 2001; Tuchin, 2015a). Light scattering and light absorption inside tissues are the main reasons of tissue opacity, which is a major obstacle for whole-body and whole-organ imaging (Susaki and Ueda, 2016). Controlling the optical properties of tissues may contribute to tissue transparency by physical or chemical manipulation (Tuchin *et al.*, 1997; Vargas *et al.*, 1999; Tuchin, 2015b). Therefore, tissue clearing aims to clarify tissue by reducing light scattering and light absorption inside tissues (Figure 2), thus facilitating volumetric imaging. The ideal tissue clearing technique should have excellent clearing capacity while preserving fluorescent proteins (FPs), native architecture, and key molecular information (Park *et al.*, 2019).

### 2.1 | Common procedures of tissue clearing

Although a large number of tissue clearing techniques now exist, they are usually conducted by two to four of the following steps:

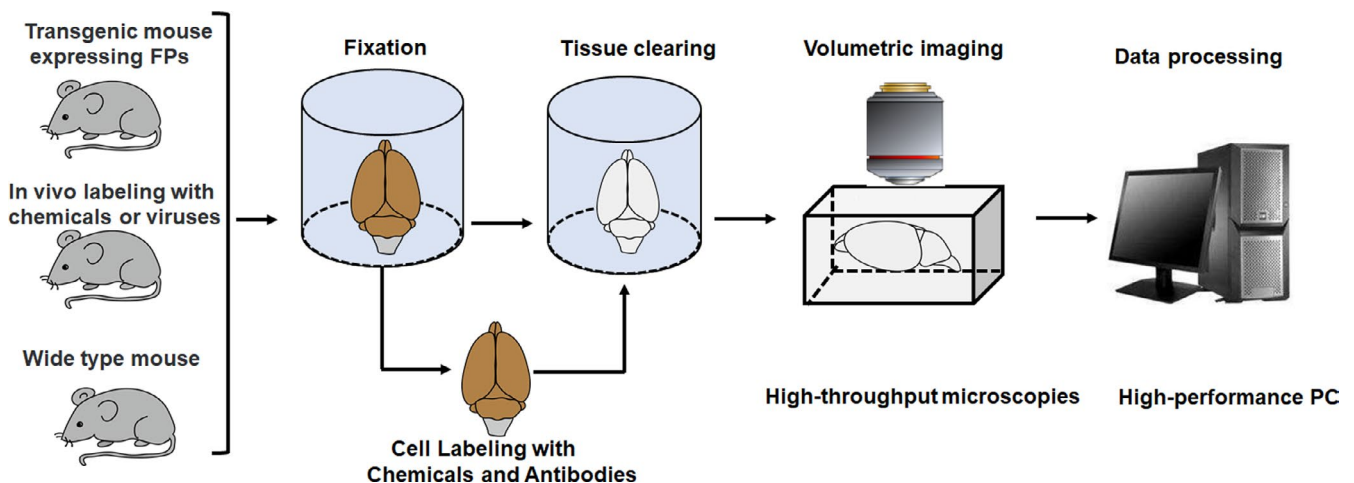
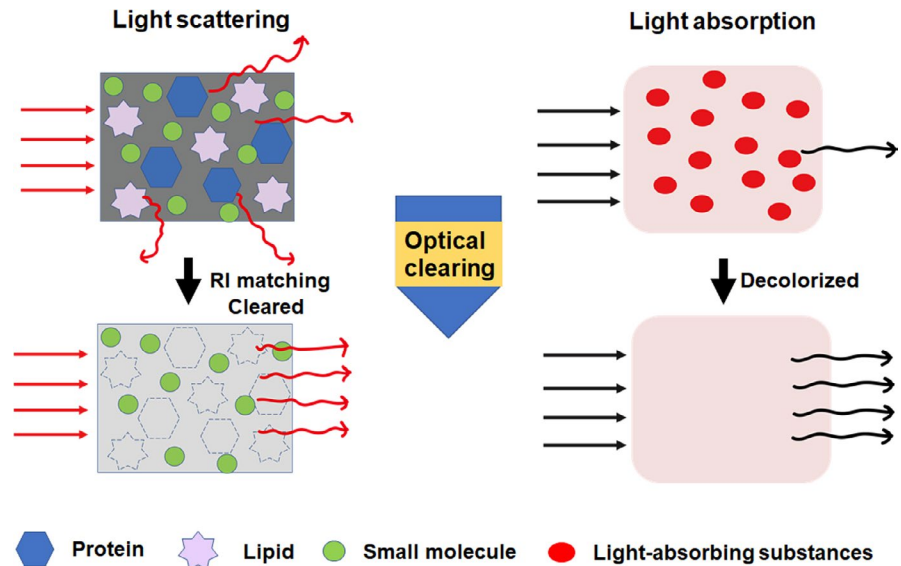


FIGURE 1 Tissue clearing technique and steps for volumetric imaging

**FIGURE 2** Mechanisms and principles of tissue clearing technique. Light scattering and light absorption are the leading causes of tissue opacity, which blocks light propagation. Light scattering is caused by heterogeneous components such as lipids and proteins. Light absorption is resulted from endogenous light absorbers like hemoglobin and melanin. Tissue clearing technique makes tissue optically transparent by minimizing light scattering and light absorption



(a) tissue fixation, (b) permeabilization, (c) decolorization, and (d) RI matching (Figure 3).

Tissue fixation is the primary step to preserve structural and molecular information during the clearing process. Paraformaldehyde (PFA), glutaraldehyde (GA) (Murray *et al.*, 2015), and acrylamide hydrogel embedding (Chung *et al.*, 2013) are usually used for tissue fixation during clearing. Permeabilization is essential for promoting the diffusion of high RI medium and antibodies into a 3D tissue. The commonly used permeabilizing reagents include solvents, hyperhydration reagents, and delipidation reagents (Tainaka *et al.*, 2016; Richardson and Lichtman, 2017). Light absorption from endogenous pigments decays light propagation and interferes with optical observations (Weissleder, 2001). Decolorizing these light absorbers would contribute to light transmission and 3D imaging. Mismatches of RI inside tissues is the primary reason of light scattering and tissue opacity (Johnsen and Widder, 1999). Equilibrating RI of the entire tissue can reduce light scattering, thus contributes to improve clearing efficacy and imaging quality as the light penetrates deeper into the samples (Susaki and Ueda, 2016; Tainaka *et al.*, 2016). Aromatic solvents, hydrophilic reagents, and contrast reagents have been widely used for RI matching (Table 1).

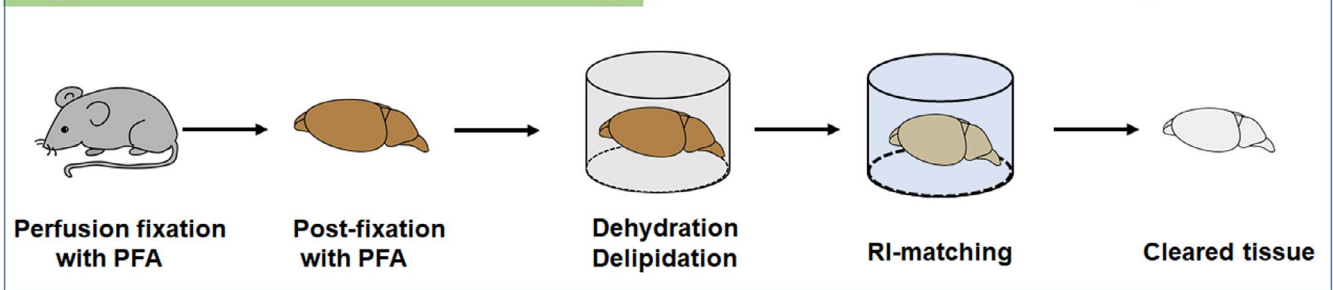
### 3 | AVAILABLE PROTOCOLS FOR TISSUE OPTICAL CLEARING

In recent years, many attempts have been made to develop tissue clearing techniques for optical imaging, and a number of tissue clearing methods are emerging (Figure 4). Generally speaking, the current clearing methods can be classified into three groups: organic solvent-based tissue clearing, aqueous-based tissue clearing, and hydrogel embedding tissue clearing (Richardson and Lichtman, 2015).

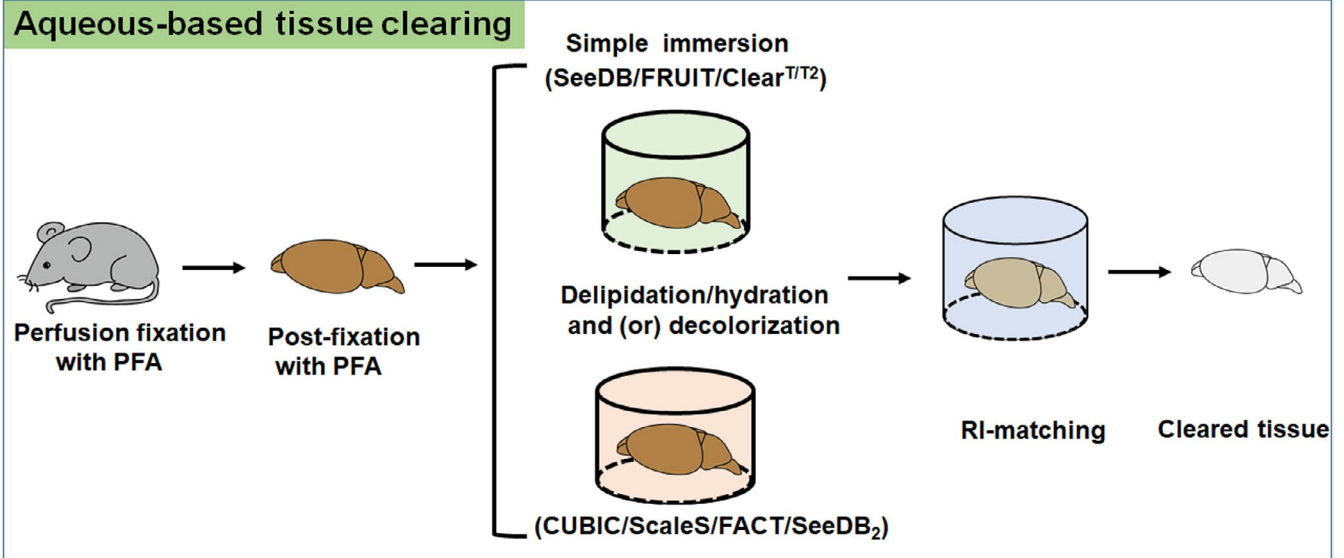
#### 3.1 | Organic solvent-based tissue clearing

Organic solvent-based tissue clearing methods achieve extremely excellent tissue transparency by homogenizing RI of different components with high RI organic solvents (Table 2). BABB clearing could fully clarify embryos and young mouse brain (Dodt *et al.*, 2007), but this protocol degraded GFP signals quickly and failed to clear myelinated tissues. 3DISCO was able to achieve robust transparency of most adult rodent organs by introducing THF and DBE, and preserved FPs for a few days (Erturk *et al.*, 2012). In contrast to 3DISCO, uDISCO enabled whole-body clearing and imaging and maintained endogenous FPs over months (Pan *et al.*, 2016). a-uDISCO is a modified version of uDISCO, which improved fluorescence intensity and stability by adjusting pH condition (Li *et al.*, 2018b). However, both uDISCO and a-uDISCO could not efficiently clear highly colored organs and hard tissues. To address these limitations, Zhao's team developed a polyethylene glycol (PEG)-associated solvent system (PEGASOS), which could clear nearly all types of tissues while preserving endogenous fluorescence (Jing *et al.*, 2018). Zhu's group developed a 3DISCO-based clearing protocol, termed FDISCO, by temperature and pH adjustments. FDISCO effectively conserved FPs and chemical fluorescent tracers, and allowed repeated revisiting of the cleared samples over months (Qi *et al.*, 2019). The recently developed sDISCO further retained the fluorescence signals by stabilizing DBE with antioxidant addition. The fluorescence of FPs could be maintained for more than 1 year (Alnuami *et al.*, 2008; Hahn *et al.*, 2019). The preservation of endogenous FPs is certainly valuable, but these proteins can also be visualized by immunolabeling. iDISCO developed by Renier *et al.* allowed whole-mount immunolabeling and volumetric imaging of mouse embryos and adult organs (Renier *et al.*, 2014). vDISCO was a whole-body immunolabeling technology based on nanobodies. This technology enhanced the signal intensity of FPs more than 100 times, and revealed whole-body neuronal projections in Thy1-GFP-M mice (Cai *et al.*, 2019).

### Organic solvent-based tissue clearing (BABB/3DISCO/FDISCO/uDISCO/PEGAOS)



### Aqueous-based tissue clearing



### Hydrogel embedding tissue clearing

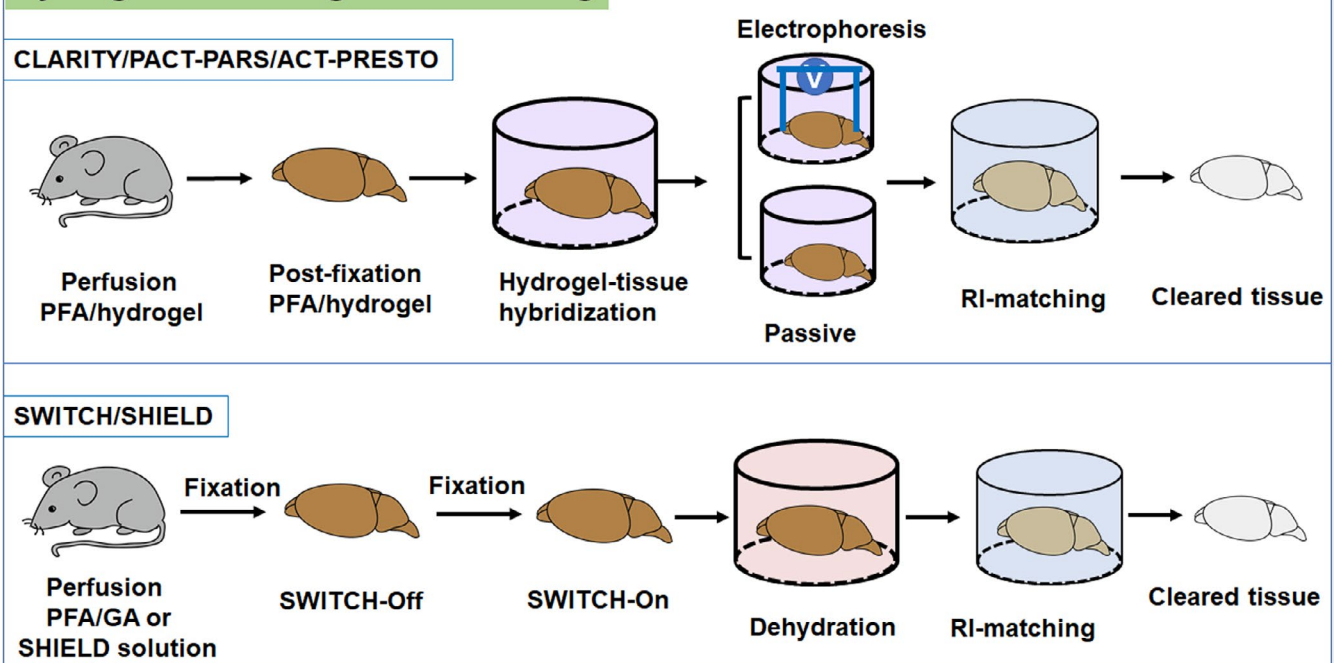


FIGURE 3 Methodology of tissue clearing technique

Although solvent-based tissue clearing methods showed brilliant clearing performance and achieved whole-body imaging with sub-cellular resolution, some drawbacks should not be neglected. Their

versatility is constrained by certain deficiencies, such as substantial shrinkage of samples, toxicity of most organic solvents, and quenching of fluorescent proteins.

**TABLE 1** Common procedures of tissue clearing

Procedure	Reagent	Method	References
Tissue fixation	PFA	3DISCO	Erturk <i>et al.</i> , 2012
	GA	SWITCH	Murray <i>et al.</i> , 2015
	Acrylamide hydrogel	CLARITY	Chung <i>et al.</i> , 2013
Permeabilization			
Solvents	Ethanol	BABB	Dotd <i>et al.</i> , 2007
	THF, DCM	FDISCO	Qi <i>et al.</i> , 2019
	Tert-butanol	uDISCO	Pan <i>et al.</i> , 2016
Hydration	Urea	Scale	Hama <i>et al.</i> , 2011
Delipidation	Aminoalcohols	CUBIC	Susaki <i>et al.</i> , 2014
	SDS	FACT	Xu <i>et al.</i> , 2017
	Saponin	SeeDB2	Ke <i>et al.</i> , 2016
	Triton X-100	Ce3D	Li <i>et al.</i> , 2017
Decolorization	H <sub>2</sub> O <sub>2</sub>	iDISCO	Renier <i>et al.</i> , 2014
	Quadrol	PEGASOS	Jing <i>et al.</i> , 2018
	Ammonium	CUBIC	Tainaka <i>et al.</i> , 2014
	N-alkylimidazole	CUBIC-L/R+	Tainaka <i>et al.</i> , 2018
	Thioglycerol	FRUIT	Hou <i>et al.</i> , 2015
RI matching	DBE	3DISCO	Erturk <i>et al.</i> , 2012
	DPE	uDISCO	Pan <i>et al.</i> , 2016
	PEG	PEGASOS	Jing <i>et al.</i> , 2018
	Sucrose	SeeDB	Ke <i>et al.</i> , 2013
	Aromatic amide	CUBIC-L/R+	Tainaka <i>et al.</i> , 2018
	FocusClear	CLARITY	Chung <i>et al.</i> , 2013
	RIMS	PACT-PARS	Yang <i>et al.</i> , 2014
	Iohexol	SeeDB <sub>2</sub>	Ke <i>et al.</i> , 2016

Abbreviations: BABB, benzyl alcohol and benzyl benzoate; DBE, dibenzyl ether; DCM, dichloromethane; DPE, diphenyl ether; GA, glutaraldehyde; PEG, polyethylene glycol; PFA, paraformaldehyde; SDS, sodium dodecyl sulfate; THF, tetrahydrofuran.

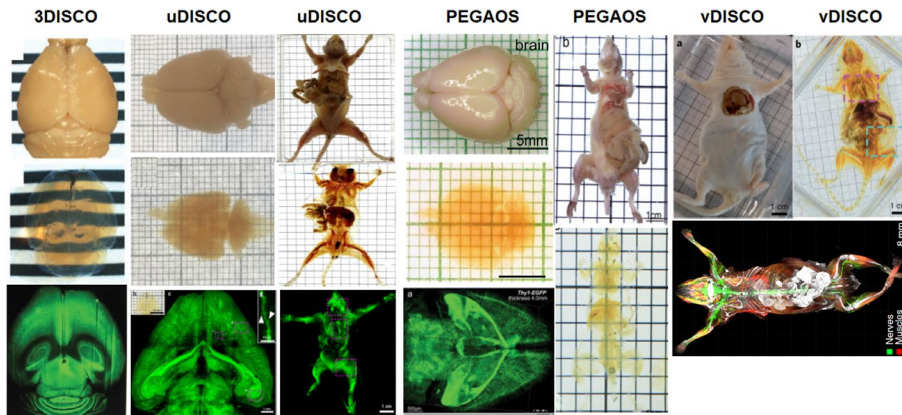
### 3.2 | Aqueous-based tissue clearing

The disadvantages of solvent-based tissue clearing propelled researchers to develop aqueous-based techniques that are relatively simple, safe, and friendly to FPs. The aqueous-based tissue clearing methods can be categorized into two groups: (a) simple immersion and (b) delipidation and (or) hydration (Table 3). In simple immersion, samples are impregnated in high RI aqueous solutions and become transparent gradually. Fructose, 2,20-thiodiethanol (TDE) and formamide are commonly used for this purpose. The fructose-based SeeDB could clear mouse brain samples with minimal tissue deformation, but it was impractical for whole-organ clearing (Ke *et al.*, 2013). The SeeDB-derived FRUIT addressed this limitation by urea addition and achieved whole-brain clearing of adult rabbit (Hou *et al.*, 2015). Formamide-based Clear<sup>T/T2</sup> could rapidly clear mouse embryos, but was insufficient to clear adult brain (Kuwajima *et al.*, 2013). RTF was a Clear<sup>T2</sup> variation, which achieved better clearing performance on adult brain tissues (Yu *et al.*, 2018).

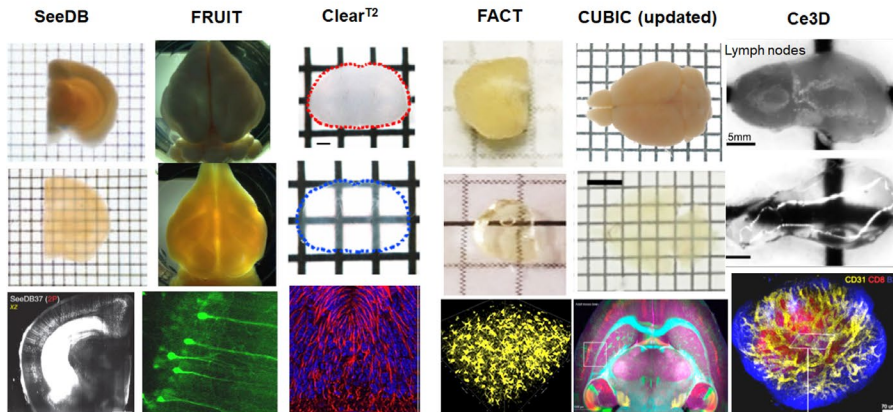
Simple immersion methods cannot provide highly transparent samples because they do not remove lipids, which are the

main source of light scattering. Tissue delipidation could improve clearing efficiency and quality (Tainaka *et al.*, 2016). This can be accomplished with aminoalcohols or detergents like sodium dodecyl sulfate (SDS), saponin, and Triton X-100. Fast Free-of-Acrylamide Clearing Tissue (FACT) was a new SDS-based clearing method for whole-tissue imaging (Xu *et al.*, 2017; Wang *et al.*, 2019a). With SDS delipidation, FACT enabled fast tissue clearing and high quality 3D imaging, and has been successfully applied for murine whole-tissue clearing (Rezazadeh *et al.*, 2018; Khoradmehr *et al.*, 2019). OPTIClear was a novel RI matching solution developed for human brain tissues. With SDS treatment, OPTIClear rendered human brain blocks highly transparent without noticeable structural distortion (Lai *et al.*, 2018). SeeDB<sub>2</sub> is a refined version of SeeDB, which utilized iohexol and saponin to improve clearing efficiency (Ke *et al.*, 2016). FOCM was an ultrafast optical clearing method, which could rapidly clear brain slices within 2 min without noticeable tissue deformation and fluorescent toxicity (Zhu *et al.*, 2019). Similarly, clearing-enhanced 3D (Ce3D) could achieved excellent transparency of most murine organs within 24 h (Li *et al.*, 2017, 2019b). Urea has

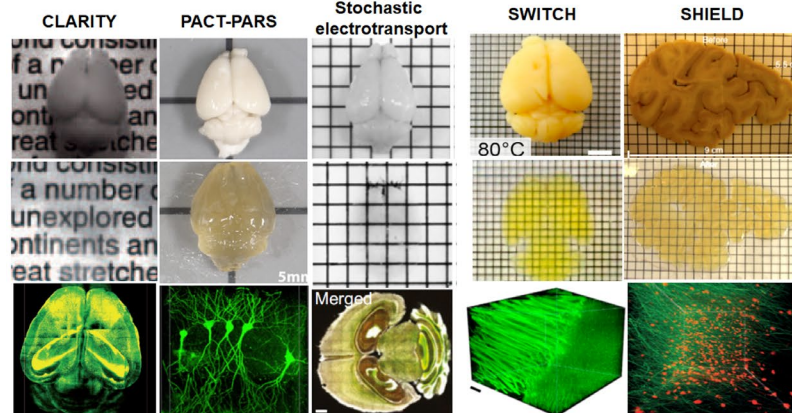
## A Organic solvent-based tissue clearing



## B Aqueous-based tissue clearing



## C Hydrogel embedding tissue clearing



**FIGURE 4** Optical clearing and imaging of diverse tissue clearing techniques. (a) Organic solvent-based tissue clearing and volumetric imaging. Images adapted from Refs (Erturk *et al.*, 2012; Pan *et al.*, 2016; Jing *et al.*, 2018; Cai *et al.*, 2019). (b) Aqueous-based tissue clearing and optical imaging. Images adapted from Refs (Ke *et al.*, 2013; Kuwajima *et al.*, 2013; Hou *et al.*, 2015; Ke *et al.*, 2016; Li *et al.*, 2017; Xu *et al.*, 2017; Tainaka *et al.*, 2018). (c) Hydrogel embedding tissue clearing and 3D imaging. Images adapted from Refs (Chung *et al.*, 2013; Yang *et al.*, 2014; Kim *et al.*, 2015; Murray *et al.*, 2015; Park *et al.*, 2019)

strong hyperhydration abilities, Miyawaki's group designed the Scale clearing reagent based on urea-mediated hydration (Hama *et al.*, 2011). Later, they upgraded Scale to improved clearing performance and developed ScaleS, which rendered mouse brain transparent without damaging FPs and subcellular structures (Hama *et al.*, 2015). The urea-based CUBIC enabled whole-body

clearing and imaging of adult mice by introducing aminoalcohols (Susaki *et al.*, 2014; Tainaka *et al.*, 2014). The CUBIC recipe has been continuously updated to improve clearing performance (e.g., CUBIC-L/R+ and CUBIC-X protocol) (Murakami *et al.*, 2018; Tainaka *et al.*, 2018). Urea-Based Amino-Sugar Mixture (UbasM) was another effective clearing agent, which rapidly cleared

**TABLE 2** Comparison of organic solvent-based tissue clearing

Method	Tissue scale	Clearing time	FP preservation	Dil Compatible	Tissue size	Toxic	References
BABB	Whole young mouse brain	10 days	Half day	No	Shrinkage	Yes	Dotd <i>et al.</i> , 2007
3DISCO	Whole adult mouse brain	3 days	A few days	No	Shrinkage	Yes	Erturk <i>et al.</i> , 2012
FDISCO	Whole adult mouse brain	3-4 days	Over months	No	Shrinkage	Yes	Qi <i>et al.</i> , 2019
sDISCO	Whole adult mouse brain	4 days	More than one year	No	Shrinkage	Yes	Hahn <i>et al.</i> , 2019
uDISCO	Whole mouse body without skin	3-4 days	Over months	No	Shrinkage	Yes	Pan <i>et al.</i> , 2016
PEGASOS	Whole mouse body with skin	2 weeks	Over months	No	Shrinkage	Yes	Jing <i>et al.</i> , 2018
iDISCO	Whole-brain immunolabeling	4 days	Many months	No	Shrinkage	Yes	Renier <i>et al.</i> , 2014
vDISCO	Whole-body immunolabeling	4 days	18 months	No	Shrinkage	Yes	Cai <i>et al.</i> , 2019

**TABLE 3** Comparison of aqueous-based tissue clearing

Method	Clearing capability	Tissue size	Dil Compatible	TEM Compatible	Tissue validation	References
Simple immersion						
SeeDB	Weak	Constant	Yes	yes	Mouse hemi-brain clearing	Ke <i>et al.</i> , 2013
FRUIT	Medium	Constant	Yes	N.T.	Whole adult rabbit Brain clearing	Hou <i>et al.</i> , 2015
Clear <sup>T/T2</sup>	Weak	Constant	Yes	N.T.	Young mouse brain clearing	Kuwajima <i>et al.</i> , 2013
RTF	Medium	Constant	Yes	N.T.	Adult mouse brain blocks clearing	Yu <i>et al.</i> , 2018
Delipidation						
FACT	Strong	Minor shrinkage	No	No	Whole adult mouse brain clearing	Xu <i>et al.</i> , 2017
SeeDB <sub>2</sub>	Medium	Constant	Yes	No	Mouse hemi-brain clearing	Ke <i>et al.</i> , 2016
FOCM	Strong	Constant	yes	N.T.	Mouse hemi-brain clearing	Zhu <i>et al.</i> , 2019
Ce3D	Strong	Minor shrinkage	N.T.	N.T.	Whole lymph node clearing	Li <i>et al.</i> , 2017
Hydration/delipidation						
Scale	weak	expansion	N.T.	yes	Adult mouse brain section clearing	Hama <i>et al.</i> , 2011
ScaleS	Strong	Transient expansion	yes	yes	Mouse hemi-brain clearing	Hama <i>et al.</i> , 2015
CUBIC	Strong	Expansion	no	no	Whole adult mouse Brain clearing	Susaki <i>et al.</i> , 2014
Updated CUBIC	Very strong	Expansion	no	no	Whole adult mouse Body clearing	Tainaka <i>et al.</i> , 2018
UbasM	Strong	Expansion	yes	N.T.	Mouse hemi-brain clearing	Chen <i>et al.</i> , 2017

Abbreviations: N.T., not tested; TEM, transmission electron microscope.

centimeter-scale samples while preserving FPs and membrane integrity (Chen *et al.*, 2017).

### 3.3 | Hydrogel embedding tissue clearing

Detergents can extract lipids efficiently, but high concentrations of detergents and harsh treatments may result in loss of native biomolecules and damage of tissue architecture. Methods of coupling these biomolecules to tissue-gel hybrids, such as CLARITY and SWITCH, can avoid these risks (Table 4).

In CLARITY, the utilization of hydrogel embedding and electrophoretic tissue clearing (ETC) contribute to rapidly achieve uniformly transparent tissues with minimal structural disturbance and biomolecule loss (Chung *et al.*, 2013). Since then many variants of CLARITY have been presented, such as ACT-PRESTO and PRE-CLARITY, which modified the ETC process and device to accelerate clearing process and increase the depth and speed of antibody penetration (Lee *et al.*, 2016; Du *et al.*, 2019). Although ETC system facilitated lipid removal, high electric fields needed for fast clearing might cause structural destruction and tissue degradation. This limitation could be addressed by stochastic electrotransport, which accelerated both clearing and staining process of intact tissues while preserving structural integrity (Kim *et al.*, 2015). ETC-independent approaches like passive CLARITY could also bypass these risks (Tomer *et al.*, 2014). However, the slow clearing rate of passive CLARITY limited its application in whole-body clearing. Another passive clarity technique (PACT) was then presented, which replaced ETC with perfusion-assisted agent release in situ (PARS). PACT-PARS allowed rapid whole-body clearing and immunolabeling in adult rodents (Yang *et al.*, 2014). Later, modified CLARITY protocols for specific experimental objectives

were also proposed, such as bone CLARITY (Greenbaum *et al.*, 2017) for bone tissue clearing, and EDC-CLARITY for RNA preservation and detection in clarified tissues (Sylwestrak *et al.*, 2016). In addition to acrylamide-based hydrogel-tissue hybridization, other gelation mechanisms have also been reported. Chung's group introduced SWITCH technique, which maintained tissue architecture and antigenicity under harsh clearing condition by synchronizing GA-tissue-gel formation (Murray *et al.*, 2015). The SWITCH-mediated SHIELD further preserved key molecular information in intact tissues by using polyfunctional crosslinkers (Park *et al.*, 2019).

## 4 | AVAILABLE MICROSCOPY FOR IMAGING OPTICALLY TRANSPARENT TISSUES

With advances of fluorescent light microscopy, many optical sectioning techniques for 3D imaging have been developed. Of these techniques, two-photon microscopy is less sensitive to light scattering, thus is best suited for deep imaging in noncleared tissues. However, light scattering is minimized in cleared samples, implying that imaging depth is no longer restricted by light penetration but by microscopy (Richardson and Lichtman, 2015). Therefore, researchers need to reselect the most suited microscopy for their cleared specimens (Table 5). Equipped with optimized objectives (working distance >5 mm, NA >0.9), both confocal and two-photon microscopy permit 3D cellular imaging of cleared samples at high resolution and contrast (Conchello and Lichtman, 2005; Helmchen and Denk, 2005; Lidke and Lidke, 2012; Richardson and Lichtman, 2015). The main disadvantage of confocal and two-photon microscopy is the slow scanning speed. Both of them

**TABLE 4** Comparison of hydrogel embedding tissue clearing

Method	Electrophoretic driven	Tissue validation	Clearing rate	Immunostaining	Antigenicity preservation	TEM	References
CLARITY	Yes	Whole mouse brain	Fast	Yes	Good	No	Chung <i>et al.</i> , 2013
ACT-PRESTO	Yes	Mouse and rabbit brain	Fast	Yes	Good	No	Lee <i>et al.</i> , 2016
PRE-CLARITY	Yes	Whole mouse brain	Fast	Yes	Good	No	Du <i>et al.</i> , 2019
Stochastic electrotransport	Yes	Whole mouse brain	Very fast	Yes	Good	No	Kim <i>et al.</i> , 2015
passive CLARITY	No	Whole mouse brain	Slow	Yes	Good	No	Tomer <i>et al.</i> , 2014
PACT-PARS	No	Whole mouse body	Fast	Yes	Good	No	Yang <i>et al.</i> , 2014
bone CLARITY	No	Bones of trunk and limbs	Fast	Yes	Good	No	Greenbaum <i>et al.</i> , 2017
SWITCH	No	Rat brain human sample	Very fast	Yes	Excellent	No	Murray <i>et al.</i> , 2015
SHIELD	No	Mouse brain human block	Very fast	Yes	Excellent	No	Park <i>et al.</i> , 2019



**TABLE 5** Comparison of microscopy techniques for cleared samples

Microscopy	Advantage	Disadvantage	Reference
Confocal microscopy	1. Achieving 3D imaging at high image contrast and resolution; 2. Enabling multispectral imaging without cross-excitation; 3. Obtaining multicolor confocal images quickly.	1. Slow scanning speed; 2. The out-of-focus planes can also be illuminated during imaging, resulting in phototoxicity and sample photobleaching.	Conchello and Lichtman, 2005; Richardson and Lichtman, 2015
Two-photon microscopy	1. Utilizing nonlinear techniques to generate signal contrast, reducing sample photobleaching; 2. Less sensitive to light scattering; 3. Adoption of near-infrared light enhances tissue penetration and generates less phototoxicity and autofluorescence.	Utilization of laser scanning results in limited image acquisition rate.	Helmchen and Denk, 2005; Mertz, 2011; Lidke and Lidke, 2012
Light sheet microscopy	1. Allowing volumetric imaging at much higher speeds and signal-to-noise ratios; 2. Selective lower power illumination leads to less photobleaching and low phototoxicity.	Inability to image samples with sufficient pixel density at low magnification.	Keller and Ahrens, 2015; Hillman <i>et al.</i> , 2019
SRS microscopy	1. Enabling fast super-multiplex optical imaging without histological staining; 2. Utilization of nonlinear Raman effects improves the sensitivity and biocompatibility of spontaneous Raman imaging.	The penetration depth of SRS microscopy is limited in highly scattering tissues.	Wei <i>et al.</i> , 2017; Wei <i>et al.</i> , 2019

utilize point detector to scan specimens point by point, resulting in limited image acquisition rate (Mertz, 2011). Therefore, they are only suited for high-resolution imaging of localized region within cleared tissues (Richardson and Lichtman, 2015). Unlike point-scanning microscopy, light sheet fluorescence microscopy (LSFM) selectively illuminates the entire x-y plane of interest from the side of samples with a thin light sheet, while region in out-of-focal plane is free of excitation, thus significantly reducing photobleaching and background signal (Susaki and Ueda, 2016; Hillman *et al.*, 2019). LSFM enables volumetric imaging at much higher speeds, higher signal-to-noise ratios, and lower phototoxicity compared to point-scanning Methods (Keller and Ahrens, 2015; Hillman *et al.*, 2019). Therefore, LSFM is more practical for whole-body and whole-organ imaging. Currently, several variants of LSFM have been developed to facilitate rapid high-resolution 3D imaging of larger intact tissues, including OCPIM, iSPIM, SCAPE/OPM, and LSTM (Migliori *et al.*, 2018). Stimulated Raman scattering (SRS) microscopy allows fast super-multiplex optical imaging without histological staining (Wei *et al.*, 2017; Wei *et al.*, 2019). Recently, SRS microscopy was also combined with tissue clearing to facilitate deep volumetric imaging (Wei *et al.*, 2019; Li *et al.*, 2019a).

## 5 | DATA STORAGE AND PROCESSING

Gigabytes or even terabytes of images are produced during large-scale volumetric imaging. Handling these massive datasets poses a

great challenge for both software and hardware. Therefore, a high-performance workstation is truly necessary for data storage and analysis. The computer used for data processing is advised to maximize the RAM (128 GB or more) and afford multicore CPU as well as professional grade hardware with multiple terabytes. Solid-state drive (SSD) and graphics processing units (GPU) are also essential (Watson and Watkins, 2019). At present, a number of commercially available software have been exploited to assist researchers in dealing with these large volumetric data, including Imaris, Vision4D, Image-Pro Plus, and Amira. Some open-source software packages are also developed, such as Fiji/ImageJ, BigDataViewer, and NeuroTrace (Susaki and Ueda, 2016; Watson and Watkins, 2019).

## 6 | APPLICATIONS OF TISSUE CLEARING IN BIOMEDICAL FIELDS

Tissue clearing technique enables large-scale volumetric imaging of intact tissues and accelerates our understanding of the complex organisms at the system level. In recent years, tissue clearing technique has been widely applied in biomedical fields.

### 6.1 | Applications in neuroscience

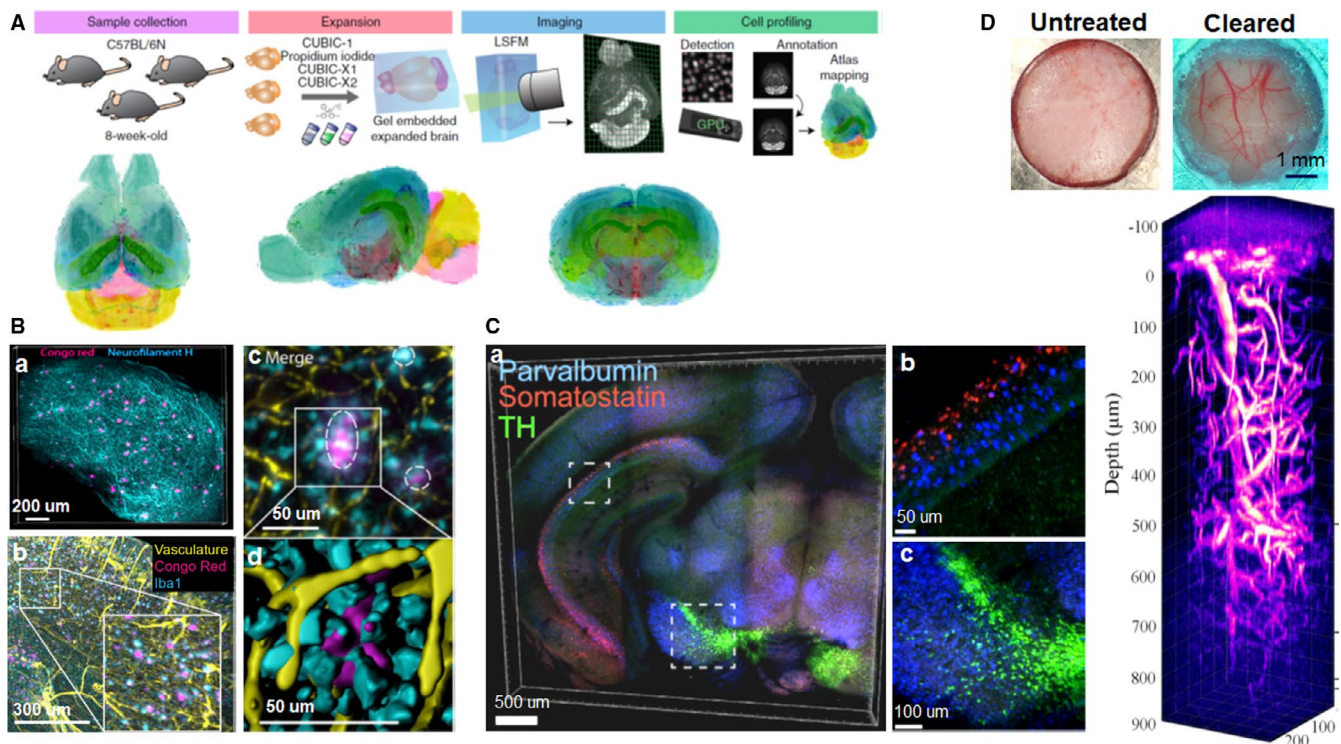
Neuroscience has always been the focus of life science. High-resolution volumetric imaging is indispensable for mapping the

structural and functional connectivity of neurons. Coupled with advanced microscopies, tissue clearing techniques facilitate the elucidation of mechanisms underlying the neuromodulation of proper behavior and contribute to reveal the pathogenesis of neurological diseases.

Ueda's group achieved virtual-multiplex whole-brain imaging with single-cell resolution by combining CUBIC-L/R+ protocol and fluorescently labeled mouse samples (Tainaka *et al.*, 2018). They also constructed a point-based mouse brain atlas with single-cell annotation (CUBIC-Atlas) using CUBIC-X expansion protocol and customized LSFM (Figure 5A). CUBIC-Atlas enabled whole-brain cell profiling and revealed inhomogeneous whole-brain development. Probabilistically mapping of pharmacologically activated cells onto CUBIC-Atlas uncovered a novel functional subarea in the hippocampal dentate gyrus. CUBIC-Atlas provided a new platform for 3D brain mapping and for unbiased system-level cellular analysis (Murakami *et al.*, 2018). They then presented a whole-organ cell profiling pipeline by combining advanced CUBIC protocol, customized LSFM, and cell-nucleus-detection algorithm. With this protocol, they recounted the cell number of the adult whole mouse brain, and quantified the whole-brain infection efficiency of AAV-PHP.eB

(NSE-H2B-mCherry) (Matsumoto *et al.*, 2019). CUBIC was also applied to trace spatial projections of sweet and bitter cortical neurons in mouse brains (Wang *et al.*, 2018). Liebmann *et al.* studied plaque formation in Alzheimer's disease (AD) mouse model using iDISCO. They demonstrated 3D spatial distribution of beta-amyloid plaques together with microglia and vasculature (Figure 5B). The combination of volume imaging and ClearMap analysis allowed them to accurately quantify the amyloid plaques within the intact AD mouse brain. They also evaluated the 3D amyloid patterns (TAPs) in archived human brain tissues, which exhibited large variation and complexity compared to those in mouse models (Liebmann *et al.*, 2016). Hildebrand's group introduced a novel cytoarchitectonic labeling approach for cleared human samples, termed MASH (Multiscale Architectonic Staining of Human cortex). Combining MASH and modified DISCO protocol, they achieved optical clearing and labeling of 5-mm-thick archival adult human brain samples (formalin fixed for 14 to 30 months). Furthermore, they characterized the 3D cortical architecture, and classified cytoarchitectonic layers over the entire cortical depth at cellular resolution (Hildebrand *et al.*, 2019).

To achieve volumetric nucleic acid labeling of large tissue volumes, Sylwestrak *et al.* developed a technique using carbodiimide



**FIGURE 5** Applications of tissue clearing in neuroscience. (A) Overview of construction of mouse brain atlas with single-cell annotation (CUBIC-Atlas), and the volume-rendered images of the CUBIC-Atlas from the horizontal, sagittal, and coronal view. (B) 3D visualization of amyloid plaques in AD using iDISCO clearing. a, Amyloid plaques and neurofilament H imaging in a cleared cortex slice of 10-month-old 2xTg AD mouse (500  $\mu\text{m}$  thick). b, Maximum projection of vasculature, amyloid plaques, and microglia staining from an 11-month-old 2xTg AD mouse brain (1 mm thick). The insert is the magnification of the indicated region (white rectangle). c, The magnified optical section from the AD brain in b, the circles indicate the plaques surrounded by reactive microglia and vessels. d, The magnified surface render in c. (C) Multiplexed detection of mRNAs in EDC-CLARITY. a, Multiplexed in situ hybridization of coronal section (0.5 mm thick) using somatostatin (red), parvalbumin (blue), and tyrosine hydroxylase (green) probe sets. b, c, Magnified view of indicated boxes. (D) 3D imaging of mouse brain vasculature labeled with Texas Red through the transparent skull window. Images adapted from Refs (Liebmann *et al.*, 2016; Sylwestrak *et al.*, 2016; Murakami *et al.*, 2018; Chen *et al.*, 2019)

compound (EDC)-based chemistry for enhanced and stable RNA preservation in CLARITY-cleared tissue. Coupled with DNA-based amplification system, this technique enabled robust detection of diverse coding RNA variants and noncoding RNAs in clarified mouse and human tissues, and also allowed multiplexed RNA labeling in EDC-CLARITY tissue (Figure 5C) (Sylwestrak *et al.*, 2016). Morawski's group presented a tailored histological method for hMRI validation based on adapted CLARITY and optical 3D imaging. They achieved overall transparency of postmortem human brain tissue with the thickness of up to 8 mm, and achieved efficient immunostaining of 5-mm-thick human postmortem brain tissue. With customized image processing tools, they demonstrated cell type classification, fiber orientation, and spatial distribution of pyramidal and nonpyramidal cells within the cortex. Combined with MRI, this tailored histological approach provided a promising tool for validating MRI-based histology in humans (Morawski *et al.*, 2018).

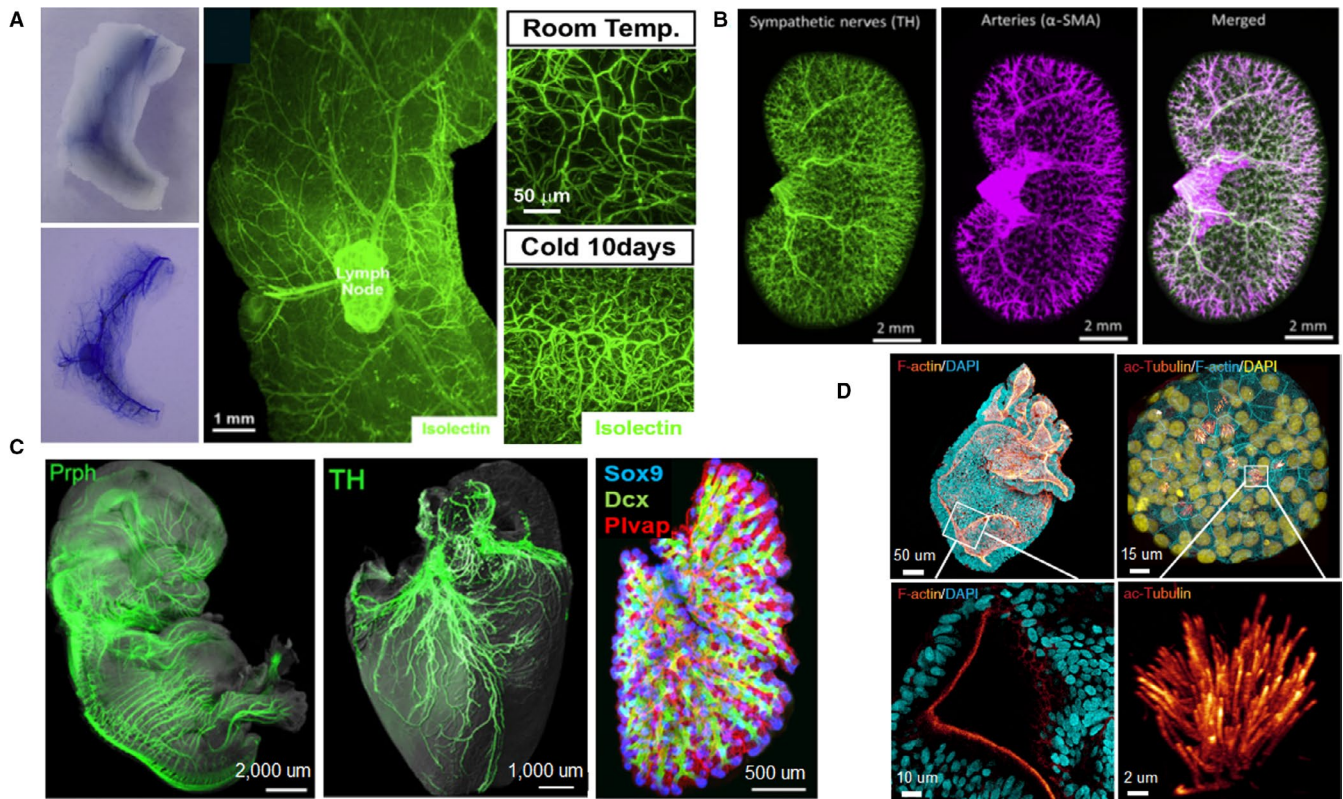
Noninvasive imaging of cerebral vasculature and neurocytes in the living brain is an indispensable method to investigate cerebrocortical structure and function. Using skull optical clearing agents (OCAs), Zhu's group developed a transparent skull window to study cortical vessels without craniotomy. Combined with several optical imaging techniques, the skull optical clearing window (SOCW) not only enhanced imaging contrast and depth but also allowed monitoring the cortical hemodynamic changes after middle cerebral artery occlusion surgery (Zhang *et al.*, 2018). In addition, they utilized the SOCW technique to repeatedly image dendritic spines, microglia processes, and microvasculature in the superficial cortical layers. They also applied this method to monitor the plastic changes of dendrites and microglia after laser ablation (Zhao *et al.*, 2018). With hyperspectral SRS imaging of a mouse skull, Chen *et al.* developed an optimized clearing strategy, which converted the turbid skull into an optically transparent skull window. Coupled with three-photon microscope, the optimal clearing method enabled 3D imaging of mouse vascular structures at a depth of 850  $\mu\text{m}$  beneath the cleared skull window (Figure 5D) (Chen *et al.*, 2019). Overall, skull optical clearing technique provided an alternative way for imaging cortical structures *in vivo* without craniotomy, rendering a better understanding of pathophysiologic processes of neurological disorders.

## 6.2 | Applications in soft tissue organs

Tissue clearing has also been widely applied in soft tissues, such as vasculature, kidney, pancreas, and organoids. To characterize the neuro-insular network of pancreas, Tang's group prepared transparent pancreas of young mice with optical clearing agent (RapiClear). They achieved 3D panoramic visualization of pancreatic microstructure, islet distribution, neurovascular network, and neural network remodeling in disease (Tang *et al.*, 2018). Fowler *et al.* utilized the modified transparent tissue tomography (T3) to generate 3D reconstructions of entire human pancreas. They visualized islet cellular composition and architecture as well as native pancreatic microenvironment, including ducts, capillaries, and the extracellular matrix.

They also exhibited that intraislet capillary density was positively related to the islet size while islet sphericity was negatively related to the islet size (Fowler *et al.*, 2018). Cao *et al.* presented a 3D volume fluorescence-imaging protocol to visualize the entire vascular network in mouse adipose tissues by combining 3DISCO/iDISCO clearing, immunolabeling, and LSFM imaging. They evaluated the pathological remodeling of intra-adipose vasculatures under obese conditions. In addition, they assessed vascular plasticity in white adipose tissues (WATs) in response to a cold challenge (Figure 6A), and found that the cold-induced vascular plasticity was regulated by the sympathetic-derived catecholamine signal and was associated with being process of WAT (Cao *et al.*, 2018). Using CUBIC clearing protocol, Hasegawa *et al.* achieved comprehensive 3D imaging of adult mouse kidney. They visualized the spatial distribution of sympathetic nerves (Figure 6B), and revealed 3D structure of collecting duct, early segments of proximal tubules, and glomeruli of mouse kidney. Moreover, they confirmed sympathetic denervation and nor-epinephrine decrease after ischemia-reperfusion injury (Hasegawa *et al.*, 2019). CUBIC-kidney provided a macroscopic perspective for kidney research. Mzinza *et al.* introduced 3DISCO/iDISCO and LSFM to assess bronchus-associated lymphoid tissue (BALT) in mice. They demonstrated qualitative and quantitative analysis of BALT induced by modified vaccinia virus Ankara (MVA) in whole mouse lung lobes, and characterized the development and organization of heat-inactivated *E. coli*-induced BALT (Mzinza *et al.*, 2018). Vargas's team combined optimized BABB clearing and large-scale 3D microscopy to study murine lung fibrosis. They revealed 3D fibrillar collagen network in whole murine lungs at high resolution, and quantified collagen deposition at the airway level throughout the entire lungs (Ochoa *et al.*, 2018).

An accurate atlas of human embryo is indispensable for better understanding of embryogenesis and developmental biology under healthy and pathological conditions. Belle *et al.* combined 3DISCO/iDISCO+clearing, immunostaining, and LSFM to build a 3D cell atlas of human development during early gestation (Belle *et al.*, 2017). They generated high-resolution 3D images of human embryos by performing whole-mount immunostaining on 36 human embryos and fetuses with over 70 antibodies. Furthermore, they demonstrated the dynamic development of peripheral nervous, vascular, muscular, cardiopulmonary, and urogenital systems during the first trimester of gestation (Figure 6C). Organoid systems reproduce cellular organization and architectural microenvironment of biological tissues, and have proved to be a powerful tool for modeling diseases and developing personalized or regenerative medicine (Rios and Clevers, 2018; Costa *et al.*, 2019). Rios's group presented a simple clearing protocol based on fructose-glycerol for 3D visualization of entire organoids (Figure 6D). They achieved high-resolution volumetric imaging of various intact organoids, including human colon, airway, fetal liver, breast tumor, as well as mouse small intestine, and mammary gland organoids (Dekkers *et al.*, 2019). Cora *et al.* optimized the passive clearing technique (PACT) for 3D imaging of intact retinal organoids. Using cleared retinal organoids, they demonstrated the fine morphology and structural organization of photoreceptor cells and



**FIGURE 6** Applications of tissue clearing in soft tissue organs. (a) Tridimensional imaging of the vasculatures in white adipose tissues (WAT) after optical clearing, and the vascular plasticity in WAT (right) in response to cold challenge. (b) Spatial distribution of sympathetic nerves (TH, green) and arteries ( $\alpha$ -SMA, magenta) in the kidney. (c) 3D Analysis of the developing peripheral nerves, heart, and lung in solvent-cleared human embryos. (d) 3D whole-mount images (top) and magnified view (bottom) of human colonic and airway organoids. Images adapted from Refs (Belle *et al.*, 2017; Cao *et al.*, 2018; Hasegawa *et al.*, 2019; Dekkers *et al.*, 2019)

bipolar cell layers. They also visualized neural processes and synaptic interconnections of photoreceptor cells in three dimensions (Cora *et al.*, 2019).

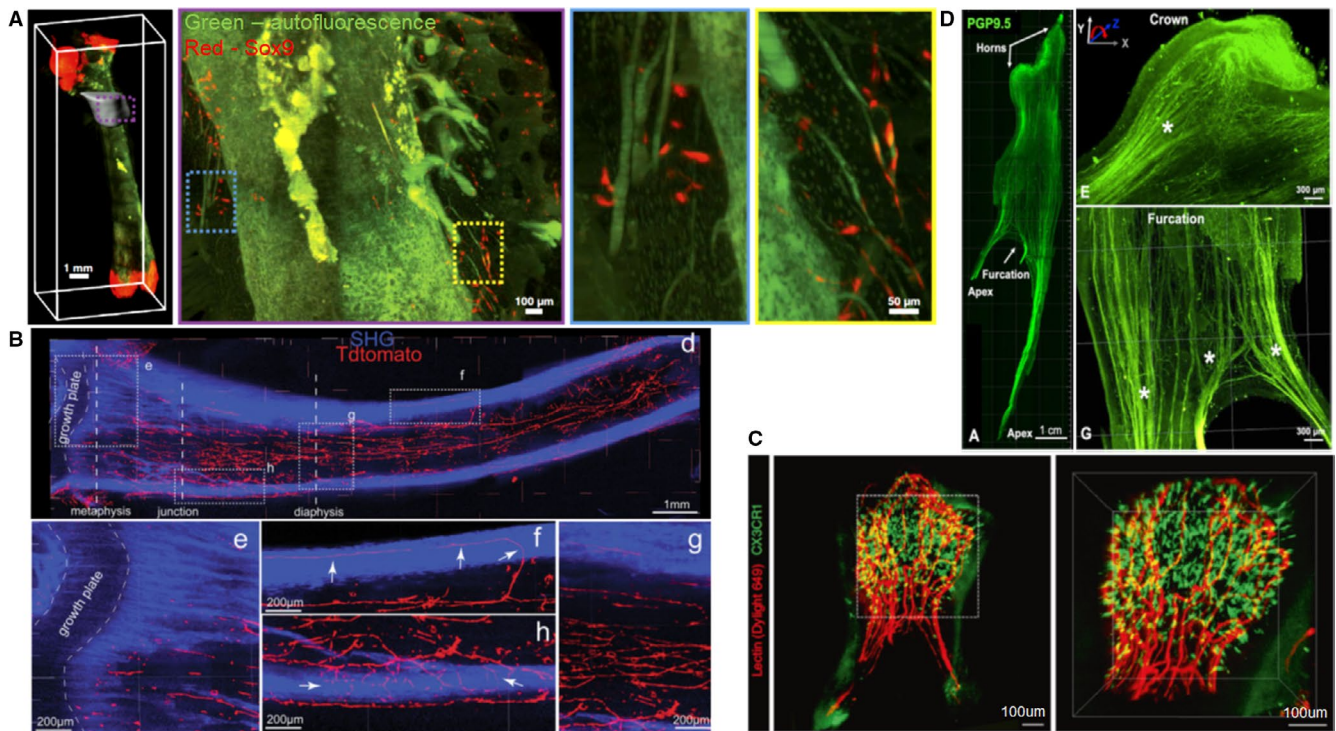
### 6.3 | Applications in hard tissue organs

Hard tissues like bones and teeth contain rich minerals and low lipids. Thus, tissue clearing techniques specially developed for soft tissues are not applicable to hard tissues. Recently, several optimized tissue clearing protocols have been presented to clarify hard tissues.

Morrison's team modified Murray's clearing to clear bisected long bones. They obtained deep imaging of bone marrow to a depth of up to 600  $\mu$ m using confocal microscopy, and identified the location of dividing and nondividing haematopoietic stem cells throughout the bone marrow (Acar *et al.*, 2015). Greenbaum *et al.* introduced Bone CLARITY to detect Sox9-tdTomato+osteoprogenitor cells in the bone tissues of adult transgenic mice (Figure 7A). Coupled with a customized LSFM and the data processing pipeline, Bone CLARITY mapped 3D spatial distribution of Sox9-tdTomato+osteoprogenitor cells in their native microenvironment, and detected their responses to sclerostin antibody treatment. Bone CLARITY provided a platform for studying the physiological processes of intact bone tissues

in healthy and disease (Greenbaum *et al.*, 2017). Wang *et al.* developed BoneClear method for robust clearing and immunolabeling of intact mouse bone tissues. With BoneClear, they fully cleared mouse intact femurs and unsectioned vertebral column and hindpaws. They also achieved 3D visualization of neural anatomy and pathology with whole-tissue immunolabeling of mouse femurs and hindpaws (Wang *et al.*, 2019b).

Zhao's group designed a PEGASOS clearing protocol, which could clear almost all types of tissues including brain, liver, bones, and teeth (Figure 7B) (Jing *et al.*, 2018). They applied the PEGASOS method to investigate the dental implant-bone interface and achieved multichannel 3D imaging of implant-tissue interface at high resolution. They revealed that angiogenesis process occurred at both titanium and stainless steel implant-bone interfaces, while osseointegration only progressed surrounding titanium implants. The PEGASOS method provided a useful tool for studying implant-tissue interface (Yi *et al.*, 2019). Later, they combined the PEGASOS-based 3D imaging and various labeling strategies to study mouse postnatal craniofacial bone development. They demonstrated a strong spatial association between craniofacial osteogenesis and angiogenesis during the entire postnatal development. Additionally, Gli1+ mesenchymal stem cells within sutures were also closely coupled with osteogenic activity and vasculature in adult craniofacial bones (Luo *et al.*, 2019).



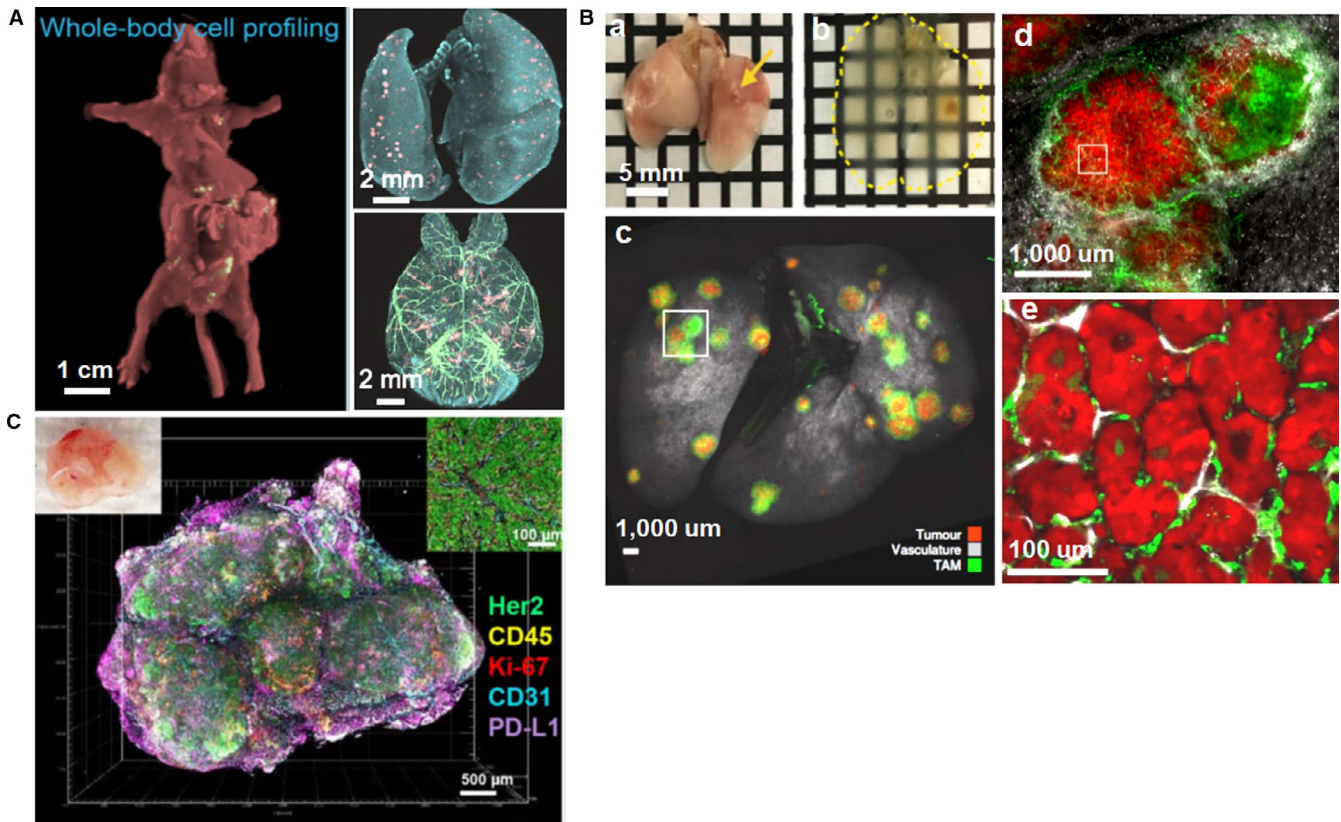
**FIGURE 7** Applications of tissue clearing in hard tissue organs. (a) Maximum intensity projection (MIP) fluorescence image of the femur revealing Sox9+ cells distribution in the vicinity of the third trochanter. Dotted boxed regions in the MIP represent progressive magnification. (b) Spatial distribution of nerves and arteries within the marrow space of the tibia. Dotted areas are magnified in e-g. Arrows in f and h show nerve fibers penetrating the cortical bone. SHG, second harmonic generation signal. (c) Volumetric imaging of immune cell distributions in an upper third molar from a CX3CR1-GFP transgenic mouse, with lectin labeled (red) endothelial cells in blood vessels. Maximal intensity Z-projection image (left) and 3D reconstruction image (right) in the dotted area. (d) Tridimensional innervation of a human premolar (left) and high-magnification images (right) of distinctive nerve splitting patterns in coronal and furcation direction. Images adapted from Refs (Greenbaum *et al.*, 2017; Jing *et al.*, 2018; Franca *et al.*, 2019; Hong *et al.*, 2019)

Dental pulp plays a significant role in maintaining tooth integrity and function. Extensive efforts have been made to investigate the structure and function relationships of the dental pulp tissues. França *et al.* applied CLARITY to study the neurovascular components of human dental pulp. They achieved 3D visualization of entire neuronal and vascular networks in human dental pulp (Figure 7C). Furthermore, they characterized the complex morphological interconnection of the dental innervation and vasculature, which improved the understanding of physiologic and pathologic conditions affecting the teeth (Franca *et al.*, 2019). Hong *et al.* modified the Murray's clearing approach for rapid clearing of the intact mouse teeth. They achieved 3D cellular visualization of the entire microvasculature as well as 3D distribution of immune cells inside the mouse dental pulp (Figure 7D). In addition, they visualized the recruitment of granulocytes and microvasculature changes in a carious tooth at cellular level (Hong *et al.*, 2019). To better understand the auditory perception and transduction, Okabe's group constructed 3D cellular mapping of the organ of Corti by combining modified ScaleS clearing protocol and machine learning-based automatic cell detection. They achieved high-fidelity recording and analysis of hair cells throughout the organ of Corti, including density, position, and morphology. They

also evaluated subcellular components and structural integrity under normal and pathological conditions, uncovering different effects of aging and noise on spatial characteristics of hair cell loss (Urata *et al.*, 2019).

#### 6.4 | Applications in tumor research

Solid tumor metastasis determines the survival of cancer patients. To overcome tumor metastasis, it is imperative to detect the metastatic progression and microenvironments of tumor cells at early stages. Ueda's group applied CUBIC-based cancer (CUBIC-cancer) analysis to investigate cancer metastasis within 13 mouse models using nine cancer cell lines (Figure 8A). CUBIC-cancer analysis enabled comprehensive spatiotemporal profiling of cancer metastasis at single-cell resolution throughout the mouse body, and could distinguish different patterns of metastasis formation. In addition, CUBIC-cancer analysis enabled therapeutic evaluation of antitumor drugs on cancer metastasis and bridged the spatial resolution gap between *in vivo* imaging and 2D histology. CUBIC-cancer analysis provided a novel platform for analyzing cancer metastasis throughout the body (Kubota *et al.*, 2017). Targeted delivery of



**FIGURE 8** Applications of tissue clearing in tumor research. (A) Whole-body and whole-organ (lung and brain) imaging of cancer metastasis at single-cell resolution. (B) Whole lung clearing allows identification of tumors and visualization of tumor burden. a-b, Whole lung clearing and identification of small tumors (small arrows); c, Whole lung imaging of KP tumour-bearing mouse; d, Magnification of a tumor from box in c; e, Magnification imaging from box in d. (C) 3D reconstruction image of multiple tumor immune microenvironment components and biomarkers in an intact mammary tumor from a BALBNeuT mouse. Images adapted from Refs (Cuccarese *et al.*, 2017; Kubota *et al.*, 2017; Lee *et al.*, 2017)

nanoparticles to micrometastases could offer a way to stop tumor growth at early phases. Kingston *et al.* combined tissue clearing, 3D microscopy and machine learning-based automated image analysis to analyze nanoparticle interaction with micrometastases. They assessed the physiological features of micrometastases and track the delivery, penetration, and distribution of nanoparticles within individual micrometastases. Using a machine learning algorithm, they could predict nanoparticle delivery to metastatic tumors based on their physiology. This technique enabled personalized treatment for patients based on the specific physiology of micrometastases (Kingston *et al.*, 2019).

Investigation of heterogeneity is crucial for tumor diagnosis and treatment, because it is associated with carcinogenesis, metastasis, and drug tolerance (Waclaw *et al.*, 2015). Integrating the iDISCO protocol and LSM, Tanaka *et al.* developed a tumor-phenotyping pipeline to study and diagnose human formalin-fixed paraffin-embedded (FFPE) tumors in three dimensions. With this pipeline, they achieved whole-tissue phenotyping of both mouse and human FFPE tumors. They demonstrated the inner landscape and spatial features of the solid tumors, and revealed distinct patterns of cancer heterogeneity (Tanaka *et al.*, 2017). Investigation of tumour immune microenvironment provides much valuable information on tumor

biology. Cuccarese *et al.* used tissue clearing technique and whole lung imaging protocol to study the spatial distribution of tumor-associated macrophages (TAM) and their responses to drug delivery in mouse pulmonary carcinoma. They analyzed lung tumor burden and visualized TAM characteristics at cellular resolution (Figure 8B). Using different pulmonary tumor models, they revealed notable heterogeneity of TAM density and infiltration, and demonstrated therapeutic response to different drug delivery. These findings facilitate the study of tumor and host-cell heterogeneity in the entire organs (Cuccarese *et al.*, 2017).

Lee *et al.* presented transparent tissue tomography (T3) for 3D mapping and analysis of the breast tumor microenvironment within Her2 transgenic mouse models (Figure 8C). Using T3 protocol, they revealed heterogeneous expression of programmed death-ligand 1 (PD-L1) throughout the tumors, and demonstrated the heterogeneity of tumor immune microenvironment by simultaneously evaluating multiple tumor parameters (Lee *et al.*, 2017). Afterwards, they applied T3 to track macromolecular drug delivery in mouse mammary tumors. They determined the unique distributions and spatial pharmacokinetics of anti-PD-L1 antibody in different tumor microenvironments (Lee *et al.*, 2019). To predict drug uptake and therapeutic responses in tumors, Esposito

et al. present a framework by combining mathematical modelling, tissue clearing and *in vivo* imaging techniques. They applied this framework to simulate steady-state fluid dynamics and the delivery of MRI contrast agent Gd-DTPA, and model drug uptake and response to OXi4503 treatment. Their results validated the feasibility and accuracy of this framework and demonstrated the interactions between individual tumor and therapeutic agents (d'Esposito *et al.*, 2018).

## 7 | DISCUSSION

Tissue clearing technique enables high-resolution volumetric imaging and contribute to reveal anatomical and functional connectivity within intact organisms, thus providing a powerful tool for systematic understanding of the complicated biological systems at multiple levels. In recent years, a variety of tissue clearing techniques have sprung up and each has distinct applications.

The major advantage of organic solvent-based clearing is the high clearing efficiency and quality, making it more suited for clearing larger tissue volumes. Both uDISCO and PEGASOS protocols render the whole adult rodent body highly transparent and preserve endogenous fluorescent proteins, thus they are the first choice for whole-body and whole-organ clearing (Pan *et al.*, 2016; Jing *et al.*, 2018). Aqueous reagent-based clearing methods like updated CUBIC protocol also efficiently clear the entire mouse body as well as large primate and human tissues through decalcification and decolorization (Tainaka *et al.*, 2018). Moreover, the hydrogel embedding-based PACT-PARS and ACT-PRESTO can render whole mouse body transparent (Yang *et al.*, 2014; Lee *et al.*, 2016). However, the limited clearing quality and the need for special equipment restrict their applications in whole-body clearing. Lipophilic dyes (e.g., Dil and CM-Dil) are commonly used neural tracers and play an important role in the study of neural circuits. Solvent-based clearing methods are not compatible with lipophilic tracers because the membrane integrity is destroyed during delipidation step. Passive immersion clearing methods, such as SeeDB, FRUIT, and Scale (Hama *et al.*, 2011; Ke *et al.*, 2013; Hou *et al.*, 2015), are simple, economical, and have a good compatibility with lipophilic tracers, yet their clearing efficiency is not as high as solvent-based or other aqueous-based clearing methods. Therefore, they are only applicable to clear lipophilic tracer-labeled tissue slices. By contrast, SWITCH and ScaleS, which clear tissues with high transparency while preserving membrane integrity (Hama *et al.*, 2015; Murray *et al.*, 2015), are more suited for clearing larger samples labeled with lipophilic dyes. It is critical to preserve the structural and molecular integrity of samples during the clearing process. Gel-embedding clearing procedures, such as CLARITY, PACT-PARS, SWITCH, and SHIELD (Chung *et al.*, 2013; Yang *et al.*, 2014; Murray *et al.*, 2015; Park *et al.*, 2019), preserve fluorescent proteins, tissue architectures, antigenicity, and transcripts through covalent cross-linking, thus can be applied to RNA transcripts detection and ultrastructure analysis. However, they are unable to fully clear hard tissues like bones and teeth. Accordingly,

no individual clearing technique is ideally suited for all applications, researchers need to select the best-suited clearing scheme for their research objectives, considering clearing efficiency, key information preservation, as well as type and volume of tissues.

Despite its rapid development, tissue clearing technique is still facing some challenges that limit its large-scale application in large-scale volumetric imaging. First, whole human organ clearing has always been challenging, especially for the adult brain tissue. Tissue clearing techniques dedicatedly developed for rodent samples exhibit its limited capacity in clearing human organs, because of the difference of tissue size and physiochemical properties between rodents and humans. Although with much efforts, tissue transparency was limited to small pieces of human organs (Lai *et al.*, 2018). Fortunately, the newly developed clearing method SHANEL achieved clearing and labeling of whole adult human brain, paving the way for charting the cellular and molecular architecture of intact adult human organs (Zhao *et al.*, 2020). However, the clearing speed of SHANEL is slightly slow, the total processing time for one adult human brain is up to 4 months, and the cost is relatively high. In the future, nontoxic, inexpensive and more effective clearing reagents should be developed to improve clearing efficiency in human fresh biopsy specimens and post mortem tissues. Second, low antibody penetration hinders the wide adoption of volumetric immunolabeling and imaging. The large molecular weight of antibody restricts its rapid penetration throughout the tissues, resulting in extremely long incubation times and nonuniform tissue staining. Although clearing methods such as AbScale, PACT-PARS, ACT-PRESTO, Ce3D (Yang *et al.*, 2014; Hama *et al.*, 2015; Lee *et al.*, 2016; Li *et al.*, 2017) have improved antibody penetration deep inside the tissue, the immunostaining depth is confined to several millimeters. Therefore, it is urgently needed to enhance antibody tissue penetration to achieve whole-body and whole-organ immunolabelling. Use of Fab antibody fragments, nucleic acid aptamers, or nanobodies should facilitate antibody diffusion and staining homogeneity (Richardson and Lichtman, 2015). vDISCO adopted nanobodies for whole-body immunolabeling and achieved panoptic imaging of neuronal projections using transparent Thy1-GFP mice (Cai *et al.*, 2019). However, the current nanobodies are designed mainly for *in vivo* applications but not for fixed samples, and the types of available nanobodies are limited at present. Therefore, it is imperative to produce diverse nanobodies for tissue volume immunolabeling in the future. Furthermore, microwave or electrophoresis technology may also promote 3D immunolabeling of intact organisms (Ferris *et al.*, 2009; Cheng and Xie, 2015). Third, high-resolution deep imaging is challenging. LSFM is an attractive choice for volumetric 3D imaging due to high-speed image acquisition, good signal-to-noise ratios, and low phototoxicity. However, LSFM employs low NA objectives to provide a wide field of view, thus the spatial resolution is poor, especially the axial resolution. Reflective imaging technique has been developed to improve spatio-temporal resolution of LSFM (Wu *et al.*, 2017). Moreover, specialized objective lenses with high NA and longer working distance are also crucial for LSFM to image intact organisms at subcellular resolution. Apart from imaging resolution, the subsequent data processing is

also troublesome. Dedicated workstations for quantitative analysis of extremely large datasets are urgently needed. Currently, a variety of commercial and open-source software packages have been exploited to handle these datasets. However, each of them concentrates on particular challenges. A computational framework possessing comprehensive imaging analysis tools should be developed, for better processing and understanding these massive datasets. Finally, tissue clearing techniques have been widely used for *ex vivo* tissues, but they are still in their infancy about *in vivo* applications. To date, *in vivo* optical transparency is only achieved in the skin and skull bone (Inyushin *et al.*, 2019). The optical clearing agents (OCAs) developed for *ex vivo* tissues are usually toxic, chemical aggressive, and irreversible. The safety and biocompatibility issues limit applications of OCAs in living organisms. At present, the OCAs used for *in vivo* biological tissues are confined to aqueous solutions, such as glycerol, sugars, propylene glycol, or polyethylene glycol (Costantini *et al.*, 2019). *In vivo* tissue optical clearing shows enormous potential for *in vivo* biomedical imaging, clinical diagnosis, and therapy. Much efforts need to be made to eliminate the potential detrimental effects of OCAs and develop safe optical clearing methods for *in vivo* applications on humans.

Undoubtedly, tissue clearing technique will continue to evolve in the near future. With advances in novel clearing reagents, 3D immunolabeling, volumetric imaging, and massive dataset analysis, tissue clearing will have a broader range of applications and pave the way for biomedical scientists to achieve whole-body cell profiling.

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## CONFLICT OF INTEREST

The authors declare no conflict of interest.

## AUTHOR CONTRIBUTIONS

Ting Tian designed the content of this review and drafted the manuscript. Zhaoyang Yang and Xiaoguang Li revised the manuscript. Xiaoguang Li approved the manuscript.

## ORCID

Xiaoguang Li  <https://orcid.org/0000-0002-2566-7907>

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