Relating response inhibition, brain connectivity, and freezing of gait in people with Parkinson's disease

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Abstract

Objective: Freezing of gait (FoG) in Parkinson's disease (PD) has been associated with response inhibition. However, the relationship between response inhibition, neural dysfunction, and PD remains unclear. We assessed response inhibition and microstructural integrity of brain regions involved in response inhibition (right-hemisphere inferior frontal cortex (IFC), and bilateral pre-supplementary motor areas (preSMA) and subthalamic nuclei (STN)) in PD subject with and without FoG and elderly controls.

Method: Twenty-one people with PD and FoG (PD-FoG), 18 without FoG (PD-noFOG) and 19 age-matched controls (HC) completed a stop-signal task and MRI scan. Probabilistic fiber tractography assessed structural integrity (fractional anisotropy, FA) among IFC, preSMA, and STN regions.

Results: Stop-signal performance did not differ between PD and HC, nor between PD-FoG and PD-noFoG. Differences in white-matter integrity were observed across groups ($0.001<p<0.064$), but were restricted to PD versus HC groups; no differences in FA were observed between PD-FoG and PD-noFoG ($p>0.096$). Interestingly, worse FoG was associated with higher (better) mean FA in the r-preSMA, ($\beta=.547$, $p=.015$). Microstructural integrity of the r-IFC, r-preSMA, and r-STN tracts correlated with stop-signal performance in HC ($p=<0.019$), but not people with PD.

Conclusion: These results do not support inefficient response inhibition in PD-FoG. Those with PD exhibited white matter loss in the response inhibition network, but this was not associated with FoG, nor with response inhibition deficits, suggesting FoG-specific neural changes may occur outside the response inhibition network. As shown previously, white matter loss was associated with response inhibition in elderly controls, suggesting PD may disturb this relationship.

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CONFLICTS OF INTEREST

OHSU and Dr. Horak have a significant financial interest in APDM, a company that may have a commercial interest in the results of this research and technology. This potential institutional and individual conflict has been reviewed and managed by OHSU.

INTRODUCTION

Freezing of gait, described as, a "brief, episodic absence or marked reduction of forward progression of the feet despite the intention to walk" (Nutt et al., 2011)(p. 734), is a debilitating feature of Parkinson's disease (PD) that restricts mobility (Walton et al., 2015). Although multifactorial, one hypothesized factor in FoG is altered cognition. The "cognitive control hypothesis" suggests that altered cognitive function may contribute to or precipitate a FoG event (Nieuwboer & Giladi, 2013). Indeed, deficits have been observed in motor inhibition and set switching in those with FoG (Bissett et al., 2015; Naismith, Shine, & Lewis, 2010; Smulders, Esselink, Bloem, & Cools, 2015; Vandenbossche et al., 2011). Although the tasks used in these studies are varied and tap into multiple cognitive processes, they share an overlapping component whereby the participant is confronted with a stimulus that triggers two competing responses. Resolution of this conflict requires inhibition of one response and facilitation of the other, and an impaired ability to appropriately inhibit tasks or switch across tasks could overwhelm the nervous system and result in a neural "traffic jam" that subsequently could express as a freezing episode (Lewis & Barker, 2009).

Inhibition (or cancellation) of a preplanned response can be assessed with stop signal test paradigms. In these paradigms, a stimulus cues a motor response, and then in about 25% of trials, a second stimulus is presented to halt the motor response. Converging evidence suggests that inhibition in stop-signal paradigms is facilitated by a specific network consisting of the right hemisphere's inferior frontal gyrus (r-IFC) and bilateral pre-supplementary motor areas (preSMA) and subthalamic nuclei (STN) (Aron, Robbins, & Poldrack, 2014; Coxon, Van Impe, Wenderoth, & Swinnen, 2012; Rae, Hughes, Anderson, & Rowe, 2015).

People with PD and FoG exhibit altered supra-spinal neuronal connectivity. Although results are somewhat mixed and need confirmation in larger samples, recent studies have indicated that changes in structural (Fling et al., 2013) and functional (Bharti et al., 2019; Fling et al., 2014) connectivity may be more pronounced in the right hemisphere in people with FoG compared to people without FoG, and may overlap the response inhibition network (Fling et al., 2014; Fling et al., 2013; Gilat et al., 2015). Given the preliminary evidence of deficits in stop-signal-related neural circuitry in people with FoG, as well as the hypothesized relationship between inhibition and FoG, it is plausible that stop-signal ability is related to freezing of gait. However, evidence on this topic is mixed. For example, Bissett showed that performance on a stop-signal paradigm was impaired in people with PD who experience FoG compared to people with PD without FoG (Bissett et al., 2015), while Stefanova et al. found no differences across groups (Stefanova et al., 2014). Together, these conflicting results reflect an incomplete understanding of the links (or lack thereof) between inhibitory control and freezing behavior, as well as the neural circuitry that underlie them.

Therefore, the primary objective of the current study was to characterize the relationship between FoG, inhibition (measured via a stop-signal paradigm), and structural connectivity in the response inhibition network in people with PD with and without FoG. Specifically, in people with PD with and with FoG we: 1) compared response inhibition performance with a stop-signal task, 2) compared microstructural integrity within the response-inhibition network (r-IFC, preSMA, STN), and 3) correlated stop-signal performance with microstructural integrity in this response-inhibition network. We hypothesized that people with FoG would show poorer response inhibition performance, measured by longer stop-signal reaction times, and poorer microstructural integrity within the right hemisphere's response inhibition network. We also hypothesized that response inhibition performance would be correlated with white matter integrity of the response-inhibition network.

METHODS

Participants

Sixty people were recruited (41 people with PD and 19 healthy adults). Convenience sampling was used for participant recruitment. Specifically, participants were contacted from existing participant databases. We also relied on fliers placed in the community and clinician referral. Finally, some participants were recruited via the Parkinson's Center of Oregon at the Oregon Health & Science University. Of the 41 PD participants, twenty patients self-reported FoG via the New Freezing of Gait Questionnaire (NFOG-Q1 = 1; PD-FoG) (Nieuwboer et al., 2009), and thus were included in the PD-FOG group, and 21 age- and gender-matched PD patients without report of FoG were included in the PD-noFoG group. One subject without self-reported FoG showed FoG during turning (confirmed by a movement disorders neurologist; J.N.) and was added to the PD-FoG group.

Inclusion criteria were: idiopathic PD according to UK Brain Bank criteria (Hughes, Daniel, Kilford, & Lees, 1992) confirmed by movement disorders neurologists, Hoehn and Yahr (H&Y) (Hoehn & Yahr, 1967) stage II-IV, aged 50–90 years, and ability to walk or stand for two minutes without an assistive device. Exclusion criteria were: implanted electrodes for deep brain stimulation, dementia (Montreal Cognitive Assessment < 18) (Nasreddine et al., 2005), or contra-indications for MRI scans. Finally, participants were excluded if they presented with any peripheral, central nervous system, or musculoskeletal disorders affecting gait or balance other than PD. Severity of Parkinsonian signs was assessed by trained raters using the Movement Disorders Society Unified Parkinson's Disease Rating Scale part III (MDS-UPDRS-III)(Goetz et al., 2008). Two subjects with PD (both PD-nonFOG) had invalid stop-signal task results. Specifically, these participants probability to stop was above 0.7, the cutoff for validity and interpretability of outcomes such as the SSRT (Verbruggen et al., 2019). After removal of these two participants, final numbers were: 21 PD-FoG, 18 PD-noFoG and 19 healthy subjects (Table 1).

Data were collected in compliance with the regulations of OHSU and the Helsinki Declaration, and the study was approved by the OHSU Institutional Review Board. Each subject gave informed written consent before participating.

Protocol and outcomes

All assessments (clinical assessments [MDS-UPDRS-III, MoCA, etc], objective assessment of FOG, Stop Signal Reaction Time (SSRT), and neuroimaging were conducted in the OFF Medication state, after a minimum of 12 hr withdrawal of all PD medications (dopamine replacement and agonists). Assessments occurred in the morning to reduce OFF-medication burden for the PD participants.

Objective assessment of Freezing of Gait

We used objective and continuous measures to assess severity of FoG as described previously (Mancini et al., 2017). Briefly, a FoG ratio was calculated from acceleration of the shins (measured via inertial sensors, Opals by APDM) during a 1-minute turning task in which subjects made alternating 360° turns as fast as safely possible (Fig. 1). Power spectral density from antero-posterior acceleration signals were calculated. Then, a FoG ratio was calculated as the ratio of total power in the "freezing band" (3–8 Hz) and the "locomotion band" (0.5–3 Hz). Higher freezing ratios indicate higher severity of FoG. FOG ratio has been shown to correlate well with FOG severity as measured by video review of turning in place (Mancini et al., 2017).

Stop Signal Reaction Time Task

Response inhibition was assessed using the stop-signal paradigm (Verbruggen, Logan, & Stevens, 2008). The test consists of one practice block (32 trials) and 3 experimental blocks (each 64 trials). Short rest breaks occurred between blocks. Subjects were seated comfortably in front of a 38×30cm monitor, and were instructed to use their left and right hands, respectively to press the "Z" key (bottom left corner of the keyboard) for a square and the '/' key (bottom right side of the keyboard) for a circle as fast as possible without errors. Wrists were resting comfortably on a table for all trials. The stimulus was presented until the subject had responded, with a maximum reaction time of 1250ms. Inter-stimulus intervals were 2000ms. In 25% of the trials, a stop signal was presented as an auditory tone. Subjects had to stop their response in these trials. The interval between the stimulus and the stop signal depended on the success of the previous stop trial using a staircase tracking procedure. Successful stop trials led to 50ms increase in stimulus-stop delay (SSD), whereas unsuccessful stop trials led to 50ms shorter SSD, resulting in an overall probability of successful stopping around 50%. Initial SSD was set at 250ms. Participants were reminded not to wait for a stop signal to occur between each block, and were provided feedback after each block regarding the percentage of stop trials actually stopped. These measures are in-line with recent guidelines regarding SST administration (Verbruggen et al., 2019).

The Stop Signal Reaction Time (SSRT) was calculated using the integration method (Verbruggen, Chambers, & Logan, 2013). First, all reaction times of non-stop trials were rank-ordered. The probability of successfully inhibiting a response whenever a stop signal was present, p(stop|signal), was calculated for every subject. The p(stop|signal) was then used to select the corresponding RT (i.e.; if p(stop|signal)=45%, stop RT is RT at 45th percentile). SSRT was calculated as stop RT - mean SSD. Two PD-FoG subjects were excluded because of p(stop|signal) > 0.7, indicating invalid tests (Verbruggen et al., 2019). Accuracy (correct left-right responses) was also calculated.

Image acquisition

Neuroimaging scans occurred in a 3.0T Siemens Magnetom Tim Trio scanner with a 12-channel head coil at Oregon Health and Science University's Advanced Imaging Research Center. We acquired one high-resolution T1-weighted MP-RAGE sequence (orientation = Sagittal, echo time =3.58msec, repetition time=2300msec, 256 X 256 matrix, resolution 1.0×1.0×1.1 mm.; scan time=9min 14sec). High angular resolution diffusion images (HARDI) were also collected using a 72-gradient direction, whole-brain echo-planar imaging sequence (TR=7,100ms, TE=112ms, field of view=230×230 mm^2, b value=3,000 s/mm^2, isotropic voxel dimensions=2.5 mm^3) and ten images in which the b value was equal to zero. A static magnetic field map was also acquired using the same parameters as the diffusion weighted sequence.

Diffusion Tensor Imaging Analysis

Diffusion data were processed using the tools implemented in FSL (Version 5.0; www.fmrib.ox.ac.uk/fsl). Briefly, diffusion data were corrected for eddy current distortions and motion artifacts, averaged to improve signal-to-noise ratio and skull-stripped (Eickhoff et al., 2010). For each individual, the fractional anisotropy images were normalized into Montreal Neurological Institute (MNI) space by using a linear (affine) registration and Fourier interpolation through the FMRIB linear image registration tool. A probabilistic diffusion model that accommodates crossing fibers was applied to calculate fiber tract probability distributions at each voxel to identify tract quality (Behrens, Berg, Jbabdi, Rushworth, & Woolrich, 2007; Behrens et al., 2003). Probabilistic tractography was run from cortical seed masks, constrained by a target and termination mask, to delineate the following tracts: (1) r-IFC to r-preSMA; (2) r-IFC to r-STN; (3) r-preSMA to r-STN; (4) l-preSMA to l-STN; (5) l-IFC to l-preSMA; and (6) l-IFC to l-STN. Seed masks for probabilistic tractography were determined in MNI space using procedures previously outlined (Coxon et al., 2012) and transformed to subject diffusion space using the inverse of the FA registrations.

FA region of interest analysis

Due to the strong body of literature identifying r-IFC, preSMA, and STN as critical nodes in a neural network for response inhibition (Aron et al., 2014; Coxon et al., 2012; Rae et al., 2015), we utilized an *a priori* ROI-based approach. Resultant fiber tracts were thresholded, transformed to MNI space, binarized, and summed across participants (Aron, Behrens, Smith, Frank, & Poldrack, 2007). Voxels that were present in >95% of participants' maps were retained (Fig 2A). For ease of interpretation, the ROIs are labeled according to the common seed/target node (e.g., the r-IFC ROI was determined by the multiplication of the tract between r-IFC and r-preSMA and the tract between r-IFC and r-STN). Thus, the value for each ROI can be thought to reflect the integrity of white matter projections to/from the other neural nodes (e.g., r- IFG contains voxels projecting to/from both r-preSMA and r-STN). The resulting MNI space tract ROIs were subsequently used to extract the mean from each subjects' FA image. FA is a rotationally invariant index that ranges from 0 (*isotropic*) to 1 (*anisotropic*), higher FA values indicating higher white matter integrity.

Statistical Analysis

Demographic, clinical and response inhibition differences among groups were tested with ANOVAs (comparing all groups), independent t-tests (PD-FoG vs PD-noFoG) or chi-square for categorical variables.

FA data and some behavioral (i.e., SSRT) data were non-normally distributed. Therefore, non-parametric tests were used to assess across group differences in FA and behavioral data. Specifically, Kruskall-Wallis tests assess overall group-effects, and Mann-Whitney U tests assessed pre-planned, across group comparisons (HC vs. PD-noFOG, HC vs. PD-FOG, and PD-noFOG vs. PD-FOG). Hodges-Lehmann CI estimates were calculated for these assessments.

Regression models were run in PD-FoG to analyze the association between ROI FA values and FoG ratio, adding age, gender and disease duration as covariates. FoG ratio was positively skewed across all PD subjects with median of 1.22 (range from 0.23 to 34.48). Hence, logarithmic transformation (ln) of the FoG ratio was used to equalize variances for this analysis.

The relationship between FA of each ROI and the stop-signal task behavior was analyzed using regression models with dependent variable SSRT and ROI FA was the independent variable. Age and gender were included as covariates. Planned within group (HC, PD-noFOG, and PD-FOG) models were also run. Despite non-normal distributions of some FA outcomes, residuals of the regression models were *not skewed* (Shapiro-Wilk test outcomes p>0.205 for all models). Nonetheless, to identify potential outlier bias, in all instances where significance between the FA ROI and SSRT was observed, Cooks distance values were calculated. Model outcomes with high-leverage data points excluded are presented.

RESULTS

Results describing SSRT performance across groups, structural integrity across groups, and the relationship between SSRT and structural integrity are presented in turn.

SSRT performance (Table 2)

Means and statistical outcomes of SST performance are shown in table 2. Across all subjects, the average RT of Go trials (692±172ms) and was longer than the average RT of the failed stop trials (627±155ms; $t_{1,57}$ =10.97, p<.001). Accuracy rates were high and not significantly different among groups ($F_{2,55}$=1.49, p=.235). Average SSRT of the whole sample was 268±61.6ms. Mean SSRT also did not differ between groups (main group effect: $F_{2,55}$=0.38, p=.686).

Microstructural integrity of the stopping network

Across and within group analyses of all FA values can be found in Table 3. Models showed statistically significant differences across groups for r-IFC (p=0.005), l-IFC (p=0.003), l-preSMA (p=0.001), and l-STN (p=0.004), and trends toward significance in r-preSMA (p=0.057) and r-STN (p=0.064). Within-group analyses showed that: 1) HC exhibited larger (better) FA compared to PD-noFOG across all ROIs (0.001 < p < 0.042), 2) HC - PD-FoG

differences were less robust, and more commonly observed in the left hemisphere ROIs (0.001 < p < 0.033) than the right hemisphere ROIs (0.036 < p < 0.72), and 3) no significant differences were observed between PD-FOG and PD-noFOG in FA in any ROIs (0.096 < p < 0.955).

Microstructural integrity of the response inhibition network and behavioral response inhibition

Regression analysis outputs for models relating SSRT to FA of each ROI in all groups can be found in the Supplemental Table. Analyzing all subjects together, relationships between SSRT and STN, SMA, and IFG were modest in the right (0.081 < p < 0.167) and left (0.035 < p < 0.252) hemispheres. No significant associations between the left or right nodes and SSRT were observed in either PD group.

However, planned, within-group assessments showed that in HC, higher (i.e., better) FA values of the right hemisphere were related to faster SSRT's (r-IFC: B=−1301 (SE 332), p = .001; r-STN: B=−495 (SE 162), p=.008; Fig 2B). None of the left hemispheres nodes associated significantly with SSRT in healthy subjects. For the HC models, one participant was noted to contribute a data-point that exhibited a notably large Cook's distance value (>4/(n-k-1) (Hair, Anderson, Tatham, & Black, 1998)) for r-IFC, r-SMA, and r-STN (0.44, 0.34 and 0.37, respectively). Removal of this data-point reduced the significance of each of the FA-SSRT relationships (r-STN: p=0.044, r-SMA: p=0.079; r-IFC: p=0.064). For the l-SMA total group model, one participant had a large Cook's value (0.12). Removal of this participant slightly increased the significance of the model (p=0.023 after removal; see Supplemental Table for details).

Severity of FoG and integrity of the response inhibition network

The FoG ratio correlated with NFOG-Q total score (r=.641, p=.002) and was significantly larger in PD-FoG than PD-noFoG (p=.028) or neurotypical adults (<.001). FA values of the r-preSMA and r-STN were significantly associated with the FoG ratio (p=.015 and .012, respectively; Table 4), indicating that larger tract integrity associated with *higher* (i.e., worse) FoG ratio (B=17.47 (5.43), p = .015). Neither the r-IFC nor any of the left hemisphere nodes were associated with the FoG ratio.

DISCUSSION

Our results did not support the hypothesis that FoG is associated with response inhibition deficits or that microstructural integrity of the right hemisphere's IFC-preSMA-STN circuitry is disproportionately altered in PD-FOG. First, in contrast to our expectation, PD subjects with FoG did not have poorer stop-signal task performance or poorer structural integrity within the predefined response inhibition network compared to those without FoG. Second, the integrity of white matter tracts within the right IFC-preSMA-STN network was *higher* in subjects with more severe FoG. Third, we observed the expected positive relationship between stopping network structural integrity and stopping behavior, but only in neurotypical older adults.

Behavioral differences between PD with and without FoG

Our results suggest that neither PD (generally) or the presence of FoG within the PD group resulted in poorer efficiency in response inhibition, measured as stop-signal task performance. Previous work has yielded inconsistent results regarding the effect of PD or FoG on stopping performance. For example, some studies have reported longer (worse) SSRT in PD compared to healthy subjects (Di Caprio, Modugno, Mancini, Olivola, & Mirabella, 2020; Gauggel, Rieger, & Feghoff, 2004; Manza et al., 2018; Obeso et al., 2011; Obeso et al., 2014; Wylie et al., 2018), and others reported no differences, consistent with our findings (Bissett et al., 2015; Claassen et al., 2015; Kohl et al., 2015; Vriend et al., 2015). Two previous reports investigated the impact of freezing status on SSRT performance. First, and consistent with the current report, Stefanova et al. measured SSRT performance in people with (n=30) and without FoG (n=36), showing *no differences* across groups (Stefanova et al., 2014). However, Bisset et al. measured SSRT in neurotypical adults (n=21), people with (n=20) and without FoG (n=22). They noted that while people with PD on the whole did not have worse SSRT times compared to neurotypical adults, a pre-planned comparison between people with and without FoG exhibited a subtle, but significant, worsening in SSRT in those with FoG.

The reason for the discrepancy in results when comparing FoG and non-FoG groups is unclear, but could be related to at least three differences between our and Bisset et al.'s paradigms. First, the mode of stop-signal presentation was different across studies, as Bisset and colleagues provided a visual (color change) stop signal, while the protocol in our study and that of Stefanova et al. was auditory. Although speculative, differences in salience of the stimulus, or specific processing impairments of visual, but not auditory, stimuli in subjects with PD with FoG may have contributed to the discrepancy in results (Davidsdottir, Cronin-Golomb, & Lee, 2005; Fearon, Butler, Newman, Lynch, & Reilly, 2015). Second, unlike Bisset et al., participants in our study completed the stop-signal task while in the 'Off' levodopa state. Although the effect of dopamine on SSRT times has been mixed (Claassen et al., 2015; Manza et al., 2018; Obeso et al., 2011; Wylie et al., 2018), it is possible that dopamine replacement therapy impairs SSRT performance. Finally, Bisset and colleagues also measured (and included in their analysis) SSRT times with the feet as an effector (in addition to the hands). While there were no effector by group interactions observed, inclusion of these data may have contributed to the significance observed in that study. In sum, while additional work will be necessary to provide consensus, the existing literature suggests FoG status likely has relatively modest effect on SSRT performance. Further, these studies underscore the diversity in SST methodological paradigms. For subsequent studies, adoption of reliable and standardized methodologies (e.g. (Verbruggen et al., 2019)) should be applied to increase generalizability of findings.

We selected the stop-signal paradigm as a measure of inhibition because of 1) the strong evidence of the neural circuitry involved, 2) early work indicating potential deficits in these regions in PD-FOG, and 3) potential behavioral deficits in this group. However, we recognize that using upper limb responses rather than stepping responses limits validity for the task for FoG. Interestingly, two recent studies investigated response inhibition tasks during stepping, also showing mixed results. Beaulne-Seguin et al. did not find clear

inhibition deficits in freezers compared to non-freezers when instructed to execute or stop a prepared stepping response to a visual cue (Beaulne-Seguin & Nantel, 2016). Alternatively, Georgaides and colleagues asked PD participants with and without FoG to perform a virtual reality stepping task with an embedded inhibition component (Georgiades et al., 2016). Participants laid supine and tapped their feet while they were shown a first-person view moving through corridors. While tapping their feet, participants were given a visual signal to stop stepping. Authors found that people with PD and FoG took more steps after the stop signal than people without FoG, thus exhibiting more difficulty "stopping" the stepping task. There are important differences between stopping an ongoing task (stepping) versus a released reaction time task (as in the SSRT), which may have also contributed to the partially conflicting findings between findings of Gorgiades et al. and the current report. However, together, these efforts represent an important step in developing effector-specific and FoG- specific paradigms to further understanding of inhibitory processes relevant to freezing of gait.

We also acknowledge "inhibition" is in itself a broad domain, which is not entirely described by the SST. Further, FOG events may be related to one's (in)ability to both inhibit a response and "switch" to another task. Switching ability, often measured by tasks such as Trails B-A, has been shown to be related to freezing in some (Factor et al., 2014; Naismith et al., 2010; Shine et al., 2013), albeit not all (Morris et al., 2020), previous work. Therefore, it is possible that the null findings in the current study were due to a somewhat myopic view of "inhibition", measured specifically by SST, which incompletely assesses other relevant FOG-related domains such as switching. Some research has identified neural regions associated with switching, showing partial overlap to the "stopping" network-- e.g., (Sylvester et al., 2003). However, there is currently limited information relating switching ability (e.g., Trails performance), neural regions specifically associated with switching, and FOG severity across PD-FOG and PD-nonFOG groups. This information could provide additional insights into factors that contribute to FOG.

White matter integrity in PD with and without FoG

We restricted our current analysis to the supposed response inhibition network ROIs, only considering the overlapping tracts among the ROIs, thus providing a measure of the strength of each node within this network (Coxon et al., 2012). Within this apriori selected network, we observed subjects with PD to have poorer microstructural integrity in the IFC-preSMA-STN circuitry than healthy subjects, with particular deficits in the left hemisphere. This result is consistent with previous work showing widespread cortical and subcortical white matter dysfunction in PD (Bohnen & Albin, 2011; Isaacs et al., 2019; Uribe et al., 2018).

In contrast to our expectations, we observed no statistical differences when comparing white matter tract integrity (FA) between the IFC, preSMA and STN in those with PD who do and do not experience FoG. Previous literature suggests that when using whole-brain analyses, people with FoG often exhibit reduced quality and structural integrity of white matter tracts compared to people without FoG, with particular changes to long associative white matter bundles and in white matter emanating from brainstem regions (e.g.; pedunculopontine nucleus) (Fling et al., 2013; Vercruysse et al., 2015). However, to our knowledge, no

previous investigations focused specifically on the response inhibition network, and few, if any, whole brain analyses identified deficits in connectivity in these specific nodes. Therefore, making comparisons to previous research is difficult. In addition, the lack of significant differences in the two PD groups specifically in the response inhibition nodes may be expected given the lack of difference in response inhibition between our cohorts.

White matter integrity, SSRT performance, and FOG severity

As noted above, although people with PD (with or without FoG) exhibited altered microstructural integrity compared to HC, no differences were observed between people with PD who do and do not freeze. Given the demonstrated link between the stopping network and SSRT performance, it is therefore not entirely surprising that freezing status did not impact SSRT performance. However, previous results (Coxon et al., 2012) would suggest that within each group SSRT behavior would be correlated to stopping network integrity. Indeed, consistent with previous results (Coxon et al., 2012) we did observe a correlation between SSRT outcomes structural integrity in healthy older adults in the r-IFC, r-preSMA, and l-preSMA.

However, this relationship did not persist in either PD cohort. This lack of correlation was not due to reduced variability in SSRT or structural integrity outcomes. Several possible, albeit speculative, reasons are presented. First, low correlations between the right hemisphere's IFC-preSMA-STN circuitry and behavioral response inhibition in people with PD might be explained by the fact that most of the SSRTs variance in the stop-signal task can be explained by the actual stopping phase of the inhibition process, occurring just milliseconds before the SSRT (Boucher, Palmeri, Logan, & Schall, 2007; Wessel & Aron, 2015). Hence, processing in the r-IFC-preSMA-STN might be more related to preparatory processes such as detecting and processing the stop-signal and triggering the stop response, which are essential steps for response inhibition, but have a less direct correlation with SSRT variance. Second, given the pathological state of PD patients, it is possible that other variables, not measured in the current study, such as noradrenaline or dopamine levels (Eagle, Bari, & Robbins, 2008), may be more powerful drivers of the variability in SSRT variance than structural integrity. Finally, parkinsonian pathology causes widespread neural changes and likely results in other pathways contributing to and compensating for behavioral functions, such as response inhibition (Snijders et al., 2016). Therefore, it is possible that people with PD rely less or differently on the stopping network than healthy adults for inhibition tasks. Indeed, we observed that, in people with PD and FoG, freezing severity was *positively* correlated to stopping-network structural integrity. Although this relationship was reduced after correcting for disease severity, these findings suggests that the relationship between stopping network integrity and behavior may be altered in this population. Larger (better) than normal FA has previously been shown to reflect pathological changes related to abnormal behavior in neurological populations (Hoeft et al., 2007), further supporting this speculation. Additional work in larger samples will be necessary to determine whether the stopping network plays a similar role in inhibition tasks (such as SSRT task) in people with PD as it does in neurotypical adults.

Limitations

Our results should be interpreted in the context of the following limitations. First, we focused on mean FA values of a predefined network, and we recognize that our chosen structural integrity measure (FA) does not necessarily reflect poorer physiological connectivity between brain areas. Second, although our sample size was larger than some previous neuroimaging studies in PD with FoG (Fling et al., 2013; Vercruysse et al., 2015) the heterogeneity commonly found in subjects with FoG calls for even larger sample sizes. Third, the stop-signal paradigm that we administered carried a small working memory component ('square is left, circle is right') that might have been disadvantageous for PD subjects. Although accuracy was high in all groups, a paradigm with direct cues (arrows) may be preferable over indirect stimuli that we used. Fourth, as noted in the results section, one outlier contributed to the observed FA-SSRT relationship in HC. Although residuals of these analyses were normally distributed, these findings should be considered with caution. Fifth, given that PD-FOG often exhibit more severe motor symptoms, it is plausible that the SSRT comparison across PD-nonFOG / PD-FOG participants may have been impacted by motor severity. However, we included disease severity (measured as MDS-UPDRS III) into the SSRT analysis. Second, the "go" reaction time outcomes were not different across the FOG and non FOG groups, further indicating that motor symptoms were unlikely to have impacted the interpretation of SSRT data in the current study. Finally, tract quantity (i.e.; the volume of white matter tracts) were unable to be evaluated in this study as it was previously (Fling et al., 2013). Rather, we focused on tract quality reflecting fiber density, axonal diameter, and myelination in white matter (i.e.; FA).

Conclusion

In summary, our results are consistent with the literature that microstructural brain changes exist in the response inhibition network in people with PD compared to neurotypical adults and that integrity of the response inhibition network relates to response inhibition in elderly people without PD. However, freezing status in people with PD did not impact efficiency of response inhibition (measured via the SST), nor white matter changes in the response inhibition brain network (r-IFC, preSMA, STN). Although preliminary, our findings do not support a cognitive inhibition deficit in people with PD and FoG.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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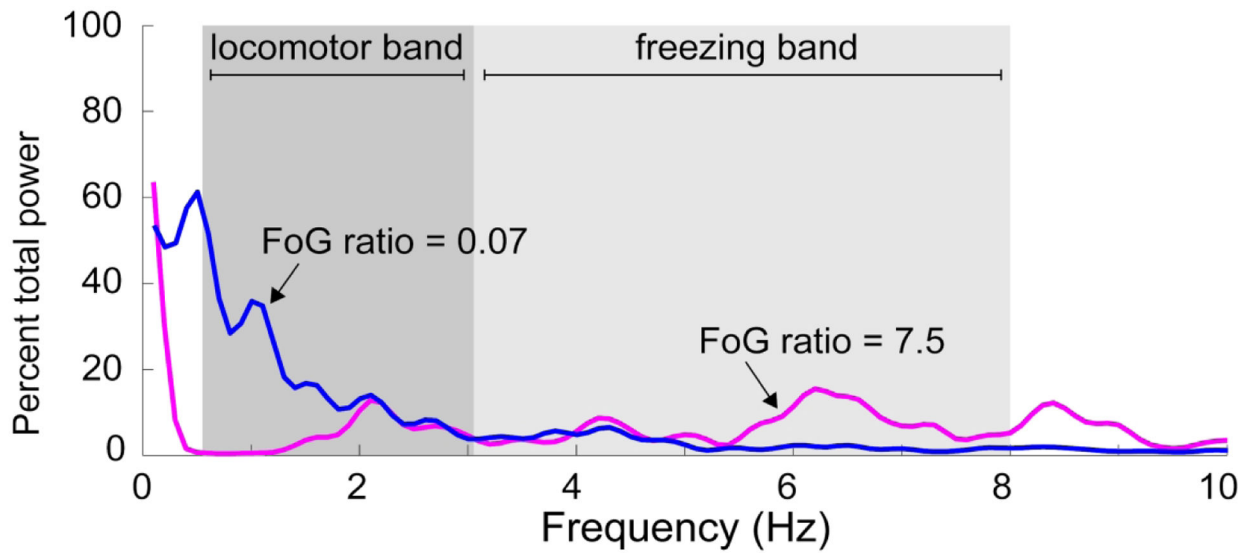
Figure 1: Calculation of FoG ratio.
The FoG ratio is calculated from anterior-posterior accelerations of the shins while turning.
The power spectral density of this signal is plotted here. Gait stepping during turning occurs
at 0.5–3 Hz (locomotor band), whereas high frequency movements reflect 'trembling of the
knees" during freezing episodes (3–8 Hz, freezing band). The FoG ratio is calculated as the
ratio between the area under the power density curve in the freezing band divided by the area
under the curve of the locomotor band. Two example trials are presented in which no FoG
(blue, FoG ratio of 0.07) and multiple FoG episodes occurred (magenta, FoG ratio of 7.5).

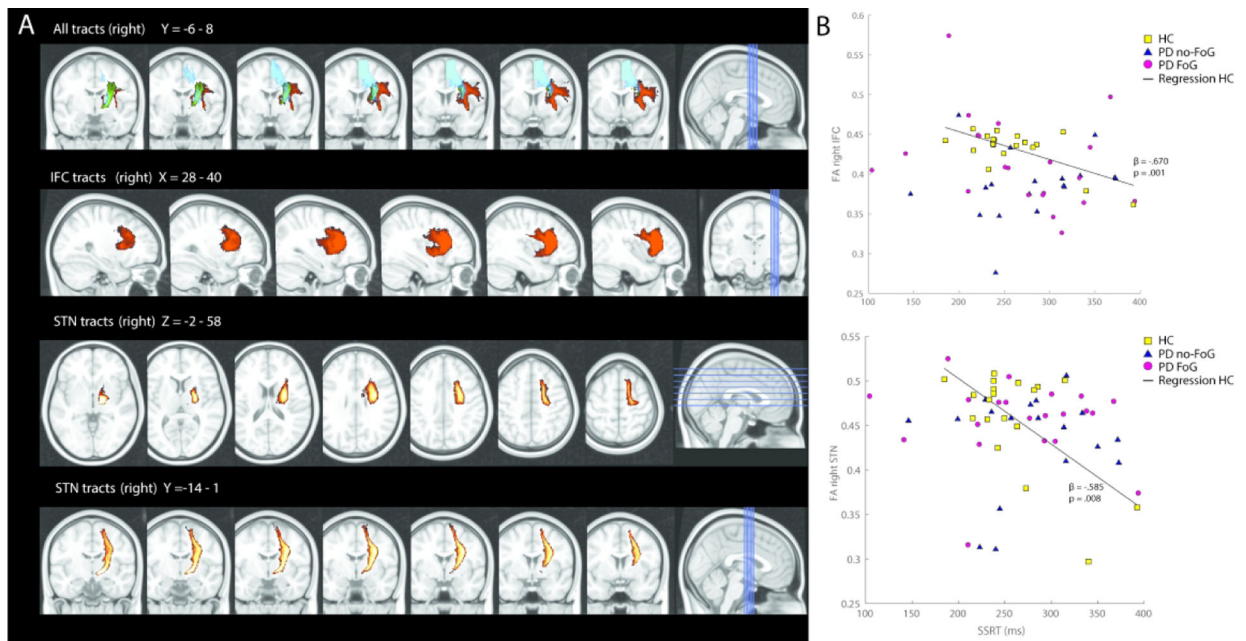**Figure 2:**

A. Identified white matter tracts within the response inhibition network. In the upper panel, all tracts are shown between the right hemisphere's inferior frontal cortex (IFC, in red), pre-supplementary motor area (preSMA, in blue), and subthalamic nucleus (STN, in green). All tracts are thresholded to include fibers where at least 95% of the participants had identifiable tracts. In the lower panels, the IFC and STN tracts are shown separately. **B. Correlations between behavioral response inhibition performance and microstructural integrity in the response inhibition network**. Higher mean fractional anisotropy (FA) of the identified right IFC (top) and STN (bottom) tracts correlated with higher stop signal reaction times (SSRT) in neurotypical, healthy controls (HC; see regression line), but not in subjects with Parkinson's disease (PD) with or without FoG. Presented ß-values for the relationship between FA and SSRT in panel B represents correlations between these variables while controlling for age and gender.

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Table 1:

Demographic and Clinical Characteristics of all Participants.

		PD-FOG	PD-noFOG	HC	P
n		21	18	19	
Age		68 ± 8	67 ± 7	69 ± 8	.978
Gender (%M)		84 %	83 %	86 %	.965[2]
MoCA		26 ± 4	26 ± 4	27 ± 2	.571
MDS UPDRS-III (0–132)[*]		43 ± 15	34 ± 11	NA	.045[1]
Disease duration		10 ± 7	5 ± 4	NA	.011[1]
NewFOGQ (0–24)		14.1 (7.0)	--	--	--
FOG Ratio		4.08 (7.60)	0.98 (0.61)	0.39 (0.24)	<0.001
H&Y	2	15 (71 %)	17 (94 %)	--	
	3	4 (19 %)	1 (6 %)	--	.156[1,2]
	4	2 (10 %)	0 (16 %)	--	

MoCA: Montreal Cognitive Assessment; MDS UPDRS-III: Movement Disorders Society Unified Parkinson's Disease Rating Scale part III (Motor examination); H&Y: Hoehn & Yahr. For MDS-UPDRS-III, NFOGQ, and FOG Ratio, and H&Y, larger values reflect worse symptoms or performance; for MoCA, larger values reflect better cognitive performance.

[1] Comparing PD-noFOG and PD-FOG;

[2] Chi-square test;

[*] MDS UPDRS-III captured while in the "OFF" medication state.

Table 2:

Stop Signal Task (SST) output means and statistical comparisons across the three groups: PD who freeze (PD-FOG), PD who do not freeze (PD-noFOG), and healthy controls (HC). SST outcomes (and in particular, SSRT) were largely similar across all groups. Non-parametric Kruskall-Wallis, MannWhitney U, and Hodges-Lehmann assessments were used due to the non-normal distribution of data.

SST outcome	PD-FOG (n=21)	PD-noFOG (n=18)	HC (n=19)	All groups[a]		Within-group, Post-hoc assessments								
						HC vs PD-noFOG[β]			HC vs. PD-FOGP[β]			PD-FOG vs PD-noFOG[β]		
	M ± sd			χ^2	p	U	p	CI[c]	U	p	CI[c]	U	p	CI[c]
SSRT	267±73	278±61	260±48	1.31	0.518	134	0.261	−19.21 [−58.21, 14.64]	175	0.507	−12.40 [−55.95, 27.19]	170	0.592	10.06 [−35.65, 56.74]
Accuracy	94±8	94±6	97±5	4.42	0.110	105	0.042	2.14 [0.00, 5.57]	144.5	0.131	1.42 [0.00, 4.90]	170	0.592	−0.70 [−3.55, 2.11]
Go RT	728±155	698±180	647±182	4.68	0.096	169	0.951	−64.19 [−167.0, 45.76]	120	0.031	−78.11 [−222.79, 10.83]	136	0.135	−37.78 [−152.01, 77.23]
SSD	428±172	393±192	372±204	1.50	0.473	157	0.671	−33.02 [−151.6, 84.09]	156	0.233	−68.96 [−191.67, 41.67]	162	0.447	−43.96 [−162.96, 87.22]
Failed Stop RT	657±141	634±174	588±150	3.07	0.216	134	0.261	−46.00 [−134.8, 41.44]	135	0.081	−70.00 [−171.00, 10.29]	173	0.652	−29.04 [−133.72, 70.51]
p(stop|signal)	0.56±0.05	0.53±0.07	0.52±0.04	3.28	0.194	134	0.261	0.00 [−0.03, 0.05]	136	0.085	0.031 [0.00, 0.062]	161	0.430	0.03 [−0.011, 0.064]

SSRT: Stop Signal Reaction Time; Go RT: Reaction time for "go" trials; SSD: Stop Signal Delay; p(stop|signal): probability of stopping a trial with a stop signal.

[a]Kruskall-Wallis Test;

[β]MannWhitney U Test;

[c]Hodges-Lehmann CI estimate

Table 3:

Across-group comparisons of microstructural integrity in a-priori regions of interest.

ROI	PD-FOG (n=21)	PD-noFOG (n=18)	HC (n=19)	All groups[a]		HC vs PD-noFOG[β]			HC vs. PD-FOG[β]			PD-FOG vs PD-noFOG[β]		
	M ± sd			χ^2	p	χ^2	p	CI[c]	χ^2	p	CI[c]	χ^2	p	CI[c]
r-IFC	0.41 ± 0.06	0.39 ± 0.04*	0.43 ± 0.02	10.7	0.005	11.4	0.001	0.052 [0.038, 0.063]	3.2	0.72	.028 [−0.003, 0.054]	1.8	0.185	−0.022 [−0.055, 0.009]
r-preSMA	0.40 ± 0.04	0.39 ± 0.04	0.42 ± 0.05	5.7	0.057	4.1	0.042	0.034 [0.001, 0.058]	4.4	0.036	0.029 [0.004, 0.055]	0.003	0.955	−0.001 [−0.029, 0.022]
r-STN	0.46 ± 0.04	0.43 ± 0.06	0.46 ± 0.06	5.5	0.064	4.5	0.033	0.028 [0.000, 0.048]	1.1	0.297	0.014 [−0.015, 0.029]	2.8	0.096	−0.017 [−0.042, 0.002]
l-IFC	0.39 ± 0.04*	0.38 ± 0.02*	0.44 ± 0.06	11.5	0.003	10.0	0.002	0.071 [0.056, 0.094]	6.4	0.011	0.065 [0.042, 0.084]	0.92	0.338	−0.006 [−0.019, 0.007]
l-preSMA	0.39 ± 0.02*	0.38 ± 0.02*	0.45 ± 0.05	14.9	0.001	11.0	0.001	0.083 [0.055, 0.102]	10.5	0.001	0.077 [0.050, 0.096]	1.03	0.310	−0.004 [−0.014, 0.005]
l-STN	0.42 ± 0.04	0.40 ± 0.02*	0.45 ± 0.06	11.1	0.004	9.6	0.002	0.065 [0.040, 0.091]	4.5	0.033	0.047 [0.007, 0.068]	2.76	0.096	−0.014 [−0.019, 0.007]

[a]Kruskall-Wallis Test;

[β]HMannWhitney U Test;

[c]Hodges-Lehmann CI estimate

Table 4:

Regression models to associate FOG severity (ln FOG ratio) with FA values of the ROIs in PD with FoG

N = 21	B (SE)	95% CI	β	p
r-IFC	0.14 (4.92)	[−.027,.027]	.006	.978
r-preSMA	17.47 (5.43)	[.004,.032]	.547	.015
r-STN	14.04 (4.95)	[.006,.042]	.514	.012
l-IFC	2.92 (8.00)	[−.014,.019]	.089	.720
l-preSMA	12.63 (14.41)	[−.003,.010]	.175	.396
l-STN	3.35 (7.27)	[−.014,.022]	.110	.652