



## Correspondence

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# Pulsed low-dose rate radiotherapy has an improved therapeutic effect on abdominal and pelvic malignancies

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Until now, there has been a lack of standard and effective treatments for patients with recurrent malignant tumors or abdominal and pelvic malignancies with extensive invasion (Morris, 2000). Generally, these patients face problems such as inability to undergo surgery or chemotherapy resistance (Combs et al., 2016). Re-radiotherapy has achieved a prominent place in the treatment of patients who have received radiotherapy previously and developed in-field recurrences (Straube et al., 2018). However, re-radiotherapy is very complicated, requiring comprehensive consideration of appropriate radiation dose, interval from first radiotherapy, boundary of the radiotherapy target area, and damage to surrounding normal tissues (Straube et al., 2019). In other words, it is necessary to focus on the protection of surrounding normal tissues while maximizing the efficacy of re-radiotherapy in such patients.

Over the years, many studies have been done on the effect of dose rate in radiotherapy (Martin et al., 2013). According to the classical cell survival curve of hypersensitivity (Fig. 1a), hyper-radiosensitivity (HRS) is observed in cancer cells exposed to low-dose rate radiotherapy (<0.30 Gy), with a steeper slope of survival

curve than that of high-dose rate radiotherapy. When the radiotherapy dose reaches 0.30–0.60 Gy, radiosensitivity begins to shift to increased radioresistance (IRR) (Todorovic et al., 2020). The HRS/IRR phenomenon can be defined using the induced repair model:  $SF(d) = \exp\{-\alpha_s[1+(\alpha_h/\alpha_s-1)\exp(-d/d_c)]d-\beta d^2\}$ , where SF is surviving fraction,  $d$  is radiation dose,  $\alpha$  is the slope of survival curve of high-dose rate radiation,  $\alpha_s$  is the slope of survival curve of low-dose rate radiation,  $d_c$  is the threshold of transition from HRS to IRR, and  $\beta$  indicates the indirect lethal effect of radiation on cells (Wang et al., 2017). Therefore, rapidly proliferating cancer cells should be more sensitive to low-dose rate radiotherapy than normal tissue cells with low or no proliferation. Moreover,  $d_c$  is different between cancers ( $d_c=0.30-0.50$  Gy) and normal tissues ( $d_c<0.20$  Gy) (Dai et al., 2009). That is to say, at low-dose rates, HRS occurred in tumors while over-repair effects occurred in normal tissues. On the radiobiological basis of HRS/IRR and sublethal injury repair (Fig. 1b) (Elkind et al., 1965), pulsed low-dose rate (PLDR) radiotherapy emerged as the times require.

The implementation strategy for PLDR involves dividing 2.00 Gy into ten fractions and administering each irradiating dose of 20 cGy at an interval of 3 min before the next low-dose radiation (Li et al., 2019). The pulse dose is within the dose range for tumor radiosensitivity and normal tissue radioresistance, which can contribute to a higher rate of tumor cell apoptosis while better protecting normal tissues from radiation damage. Relevant basic and clinical studies have shown that PLDR improves the local control

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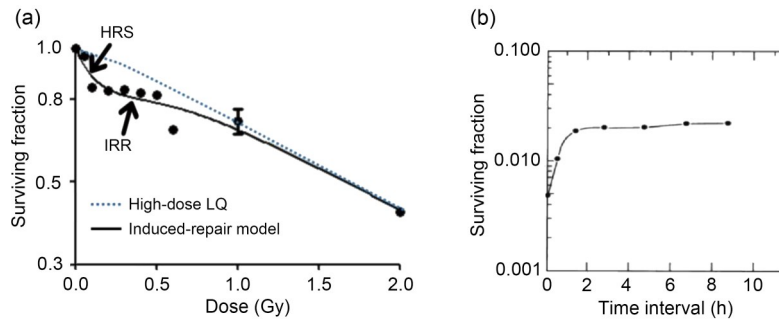
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**Fig. 1** Induced-repair model of PLDR. (a) Typical cell survival curve with evidence of HRS/IRR. Broken line shows low-dose extrapolation from linear quadratic model applied to high-dose survival data. Solid line shows induced repair fit. (b) The description of the sublethal repair half time of normal cells by Elkind et al. (1965). The hamster cells were irradiated with total 1558 cGy, which divided evenly into 763 cGy and 795 cGy with different intervals and cells were placed at room temperature during the interval. PLDR: pulsed low-dose rate; HRS: hyper-radiosensitivity; IRR: increased radioresistance; LQ: linear-quadratic model.

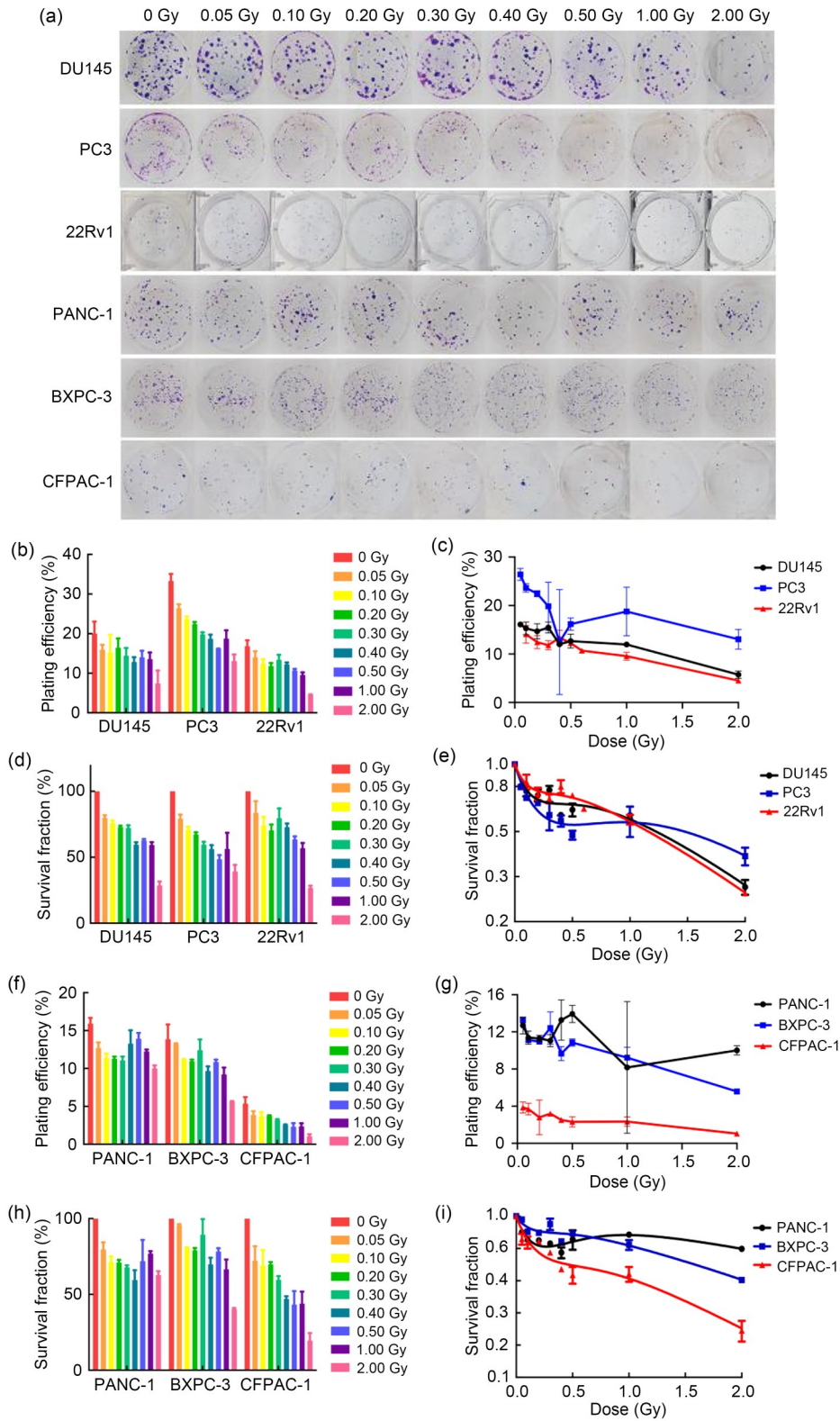
rate and the quality of life of cancer patients (Li et al., 2019).

Considering that the optimal pulse dose for different cancers is different (Pavlopoulou et al., 2017), it is important to study the optimal PLDR model for different types of tumors, especially abdominal and pelvic malignancies, so as to achieve effective treatment and make the PLDR technique accessible on a larger scale. Hence, we studied the optimal PLDR models for pancreatic cancer and prostate cancer.

We first investigated the HRS phenomenon in prostate cancer and pancreatic cancer by colony formation assay (Fig. 2a). Prostate cancer cells (PC3, 22Rv1, and DU145) and pancreatic cancer cells (PANC-1, BXPC-3, and CFPAC-1) were one-off irradiated with 0, 0.05, 0.10, 0.20, 0.30, 0.40, 0.50, 1.00, and 2.00 Gy, at a dose rate of 100 cGy/min. Our results (Table 1, Figs. 2b–2d, and Figs. 2f–2h) showed that after low-dose (<0.30 Gy) radiotherapy, the plating efficiencies (PEs) and SFs of cancer cells decreased rapidly; however, when the radiation dose was 0.30–1.00 Gy, the PEs and SFs did not decrease significantly, but slightly increased. The survival curves (Figs. 2e and 2i) showed the same trend, suggesting that prostate cancer cells and pancreatic cancer cells changed from HRS to IRR within the dose range of 0.30 to 1.00 Gy. Furthermore, according to the parameter values in the induced repair model shown in Table 1, we found that the  $\alpha_s$  of each cancer cell was markedly higher than the  $\alpha_c$ , indicating that the radiation sensitivity under low-dose conditions was significantly higher than that under conventional-dose conditions. These results indicated that all six cancer cell lines used in this study displayed the HRS/IRR

phenomenon. We also found that both radiosensitive cells (such as BXPC-3, DU145, and CFPAC-1) and radioresistant cells (such as PANC-1) had HRS phenomena, suggesting that HRS/IRR was not unique to radioresistant cancer cells. Compared with other cancer cells, PANC-1 cells had the most evident radiation resistance, but not the most significant HRS phenomenon. Therefore, it is not the case that the more obvious the radiation resistance at the conventional dose, the more significant the HRS phenomenon at a low dose. In order to fully guarantee the radiation sensitivity of cancer cells, the pulse dose  $d$  in PLDR should be less than or equal to the transition dose  $d_c$ ; in other words, the pulse dose  $d$  should be as close as possible to  $d_c$ . Based on the  $d_c$  of each cell shown in Table 1, we determined the pulse dose  $d$  of both pancreatic and prostate cancer cells to be 0.20 Gy.

Next, we studied the time interval in PLDR in terms of the sublethal repair half-time ( $t_{1/2}$ ) of peripheral normal cells. According to previous study (Li et al., 2019), time interval in PLDR is calculated by the following formulae:  $t = t_{1/2}/(m-1)$ ,  $m = D/d$  ( $t$  is the time interval,  $t_{1/2}$  is the sublethal repair half-time,  $D$  is radiation dose,  $d$  is pulse dose, and  $m$  is pulse number). The normal tissues around pancreatic cancer include pancreas, small intestine, and liver; the normal tissues around prostate cancer include prostate, rectum, and bladder. HRS mainly affects early-response tissues, while liver and bladder are late-response tissues with the radiobiologic ratio of lethal to sublethal damage ( $\alpha/\beta$ ) smaller than that of tumors; they are thus more likely to repair damage at low-dose radiation levels (Harney et al., 2004). Therefore, we did not consider



**Fig. 2** HRS/IRR phenomenon in human prostate cancer cells and pancreatic cancer cells. (a) The colony formation of human prostate cancer cells and pancreatic cancer cells irradiated with different doses. (b–i) The plating efficiencies, survival fractions, and survival curves of human prostate cancer cells (b–e) and human pancreatic cancer cells (f–i). Values were presented as mean±SD ( $n=3$ ). HRS: hyper-radiosensitivity; IRR: increased radioresistance; SD: standard deviation.

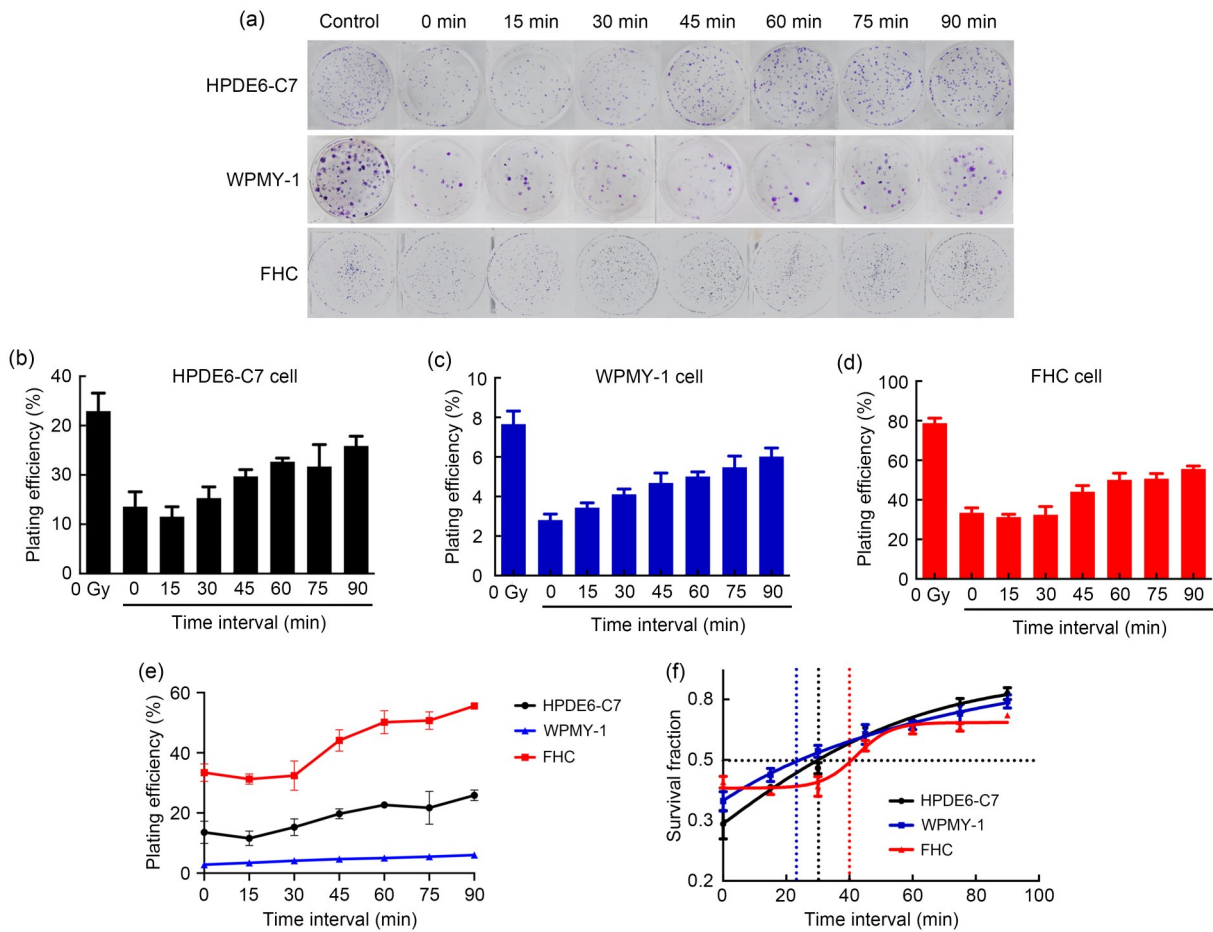
**Table 1 Parameters of HRS/IRR-induced repair model**

Cell line	$\alpha_r$	$\alpha_s$	$d_c$ (Gy)	$\beta$	$\alpha/\beta$
DU145	0.4386	3.8260	0.2177	0.0894	4.9060
PC3	0.2610	3.8910	0.3666	0.0953	2.7387
22Rv1	0.4988	3.2410	0.1701	0.0787	6.3380
PANC-1	0.1761	4.6510	0.2357	0.0275	6.4036
BXPC-3	0.3650	2.4200	0.1830	0.0442	8.2579
CFPAC-1	0.7707	4.4800	0.2810	0.0136	56.6691

HRS: hyper-radiosensitivity; IRR: increased radioresistance;  $\alpha_s$ : the slope of survival curve of low-dose rate radiation;  $\alpha_r$ : the slope of survival curve of high-dose rate radiation;  $d_c$ : the threshold of transition from HRS to IRR;  $\beta$ : the indirect lethal effect of radiation on cells;  $\alpha/\beta$ : the radiobiologic ratio of lethal to sublethal damage.

the  $t_{1/2}$  of liver and bladder cells.  $t_{1/2}$  values of normal pancreas (HPDE6-C7), normal prostate (WPMY-1), and normal rectum (FHC) were calculated by colony formation assay (Fig. 3a) and all normal cell types

were irradiated with 2.00 Gy, which was divided evenly into two 1.00 Gy with different intervals at a dose rate of 300 cGy/min. As shown in Fig. 3, when the interval was less than 15 min, the PEs (Figs. 3b–3e) and SFs (Fig. 3f) of normal cells clearly decreased, and subsequently, the survival rate showed a gradually increasing trend with the prolongation of the radiation interval. When the interval was longer than 60 min, radiotherapy did little damage to normal cells, as seen from the latter part of the survival curve, which was almost flat. We defined the location of 50% of sublethal repair on the survival curve as  $t_{1/2}$ , and the result indicated that the  $t_{1/2}$  values of HPDE6-C7, WPMY-1, and FHC cells were 31.2, 22.5, and 40.0 min, respectively. According to the formulae  $t = t_{1/2}/(m-1)$ ,  $m = D/d$ , the time interval in PLDR of prostate cancer and pancreatic cancer was 3.5 and 2.5 min, respectively. Based

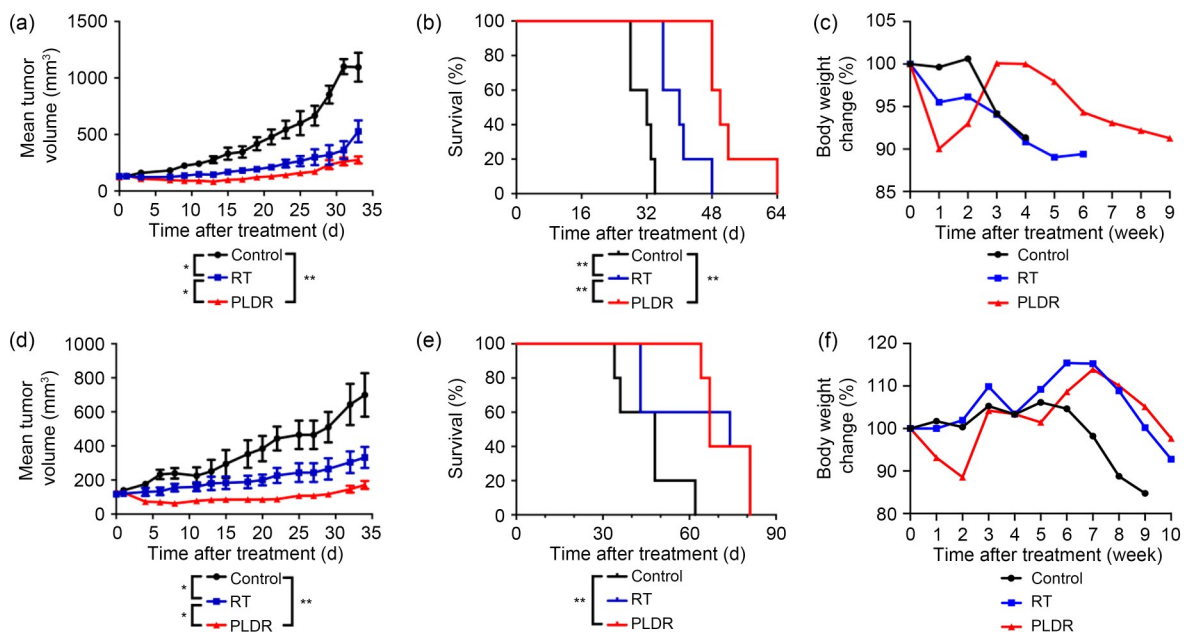


**Fig. 3** Sublethal repair half-time ( $t_{1/2}$ ) of human normal cells. (a) The colony formation of human normal cells irradiated with different time intervals; (b–e) The plating efficiencies of human normal pancreatic cells (HPDE6-C7), human normal prostate cells (WPMY-1), and human normal colorectal cells (FHC); (f) The survival curves of human normal cells. Values are presented as mean±SD ( $n=3$ ). SD: standard deviation.

on the above results, we proposed PLDR strategies for human pancreatic and prostate cancers as follows: (1) human prostate cancer: daily radiation dose 2.00 Gy divided into 10 pulses, interval between two pulses of 2.5 min, and dose rate of 100 cGy/min; (2) human pancreatic cancer: daily radiation dose 2.00 Gy divided into 10 pulses, interval between two pulses of 3.5 min, and dose rate of 100 cGy/min. These two PLDR models were different from the PLDR scheme established by Tome and Howard (2007). This indicated that the dose domain of the HRS phenomenon was different in different tumor tissues, as well as the repair capacity and repair rate of sublethal damage of different normal tissues after radiation. Hence, the establishment of personalized cancer PLDR models may have guiding significance for future clinical treatment.

After determining the PLDR scheme for prostate and pancreatic cancer cells, we compared the effects of PLDR and conventional radiotherapy on the growth of subcutaneous transplanted tumors. Considering that the HRS/IRR phenomena of PC3 cells and PANC-1 cells were more prominent than those of the other cell lines in vitro, we selected PC3 and PANC-1 cells for in vivo experiments. Fifteen male BALB/c nude mice (4–6-weeks old) were injected with PC3 or PANC-1 cells subcutaneously in the distal lower right extremity.

When the volume of subcutaneous tumors reached 100–150 mm<sup>3</sup>, the mice were randomly divided into three groups (five per group) for different treatments: a control group (no treatment), a conventional radiotherapy group (RT group; 2.00 Gy/d for 3 d at a dose rate of 300 cGy/min), and a PLDR group (treated with the radiotherapy scheme described above). Tumor volumes were measured and calculated every 3 d. Mice were weighed every week. When tumor volumes reached 3000 mm<sup>3</sup> or the surface of the tumor ulcerated, mice were euthanized by carbon dioxide overdose. We obtained tumor growth curves (Figs. 4a and 4d), overall survival curves (Figs. 4b and 4e), and body weight change curves (Figs. 4c and 4f) of tumor-bearing mice. Compared with the control and RT groups, the PLDR group showed significant inhibition of the growth of PC3 and PANC-1 subcutaneous transplanted tumors (PC3: PLDR vs. RT,  $P=0.045$ ; PANC-1: PLDR vs. RT,  $P=0.049$ ). With regard to survival time, PLDR significantly prolonged the survival time of PC3 tumor-bearing mice (PLDR vs. control,  $P=0.0038$ ; PLDR vs. RT,  $P=0.0045$ ). For PANC-1 mice, although radiotherapy did not extend survival time, surprisingly, PLDR did (PLDR vs. control,  $P=0.0041$ ). However, it is regrettable that there was no significant difference between the PLDR group and the RT group (PLDR



**Fig. 4** Effects of PLDR on PC-3 and PANC-1 subcutaneous transplanted tumors. Tumor growth curves (a, d), survival curves (b, e), and body weight change curves (e, f) of mice bearing PC-3-xenograft tumors (a–c) and PANC-1-xenograft tumors (d–f) were generated. Values are presented as mean±SD ( $n=5$ ). \*  $P<0.05$ , \*\*  $P<0.01$ . RT: radiotherapy; PLDR: pulsed low-dose rate; SD: standard deviation.

vs. RT,  $P=0.7455$ ). The results showed that compared with RT, PLDR could significantly inhibit the growth of PC3- and PANC-1-transplanted tumors and prolong the survival of PC3-bearing mice. However, PLDR treatment was not superior to RT in prolonging the survival time of PANC-1-bearing mice, so we conjectured that perhaps PLDR had no advantage in reducing side effects such as weight loss, and that some stress injury response may occur continuously in PANC-1-bearing mice.

Finally, we further investigated whether PLDR inhibited DNA double-strand break (DSB) damage repair and then promoted cancer cell death compared with the traditional radiotherapy schedule (Li and Yuan, 2021). The adherent PC3 and PANC-1 cells seeded in six-well plates were irradiated according to the radiotherapy and PLDR schedules (radiotherapy schedule: both PC3 and PANC-1 cells were irradiated with 6.00 Gy singly at a dose rate of 300 cGy/min; PLDR schedule: PC3 cells were irradiated with 6.00 Gy, which was delivered using 0.20 Gy separated by 2.5 min at a dose rate of 100 cGy/min and PANC-1 cells were irradiated with 6.00 Gy, which was delivered using 0.20 Gy separated by 3.5 min at dose of 100 cGy/min). At different time points after irradiation, cells were harvested for western blot, as in a previous study (Yao et al., 2016). As is well known, phosphorylation of H<sub>2</sub>AX at Ser139 ( $\gamma$ -H<sub>2</sub>AX) in cell nuclei, which occurs at DSB damage sites, is used as a marker of DNA DSBs (Olive, 2004). Nonhomologous end joining (NHEJ) is one of the main repair methods for DSBs and is mediated by the DNA-dependent protein kinase (DNA-PK), which cannot identify the damage site and requires the helper protein factor KU80 (Zhang and Gong, 2021). Once radiation-induced DSBs form, DNA-PK catalytic subunit (DNA-PKcs) is first recruited to the damaged site, and a KU heterodimer (KU70/KU80) assists the DNA-PK enzyme to recognize the damaged site and participate in DNA damage repair (Blackford and Jackson, 2017). As shown in Figs. 5a, 5e, 5f, and 5j, we found that whether irradiated on traditional radiotherapy or PLDR schedules, PC3 and PANC-1 cells all expressed a higher level of  $\gamma$ -H<sub>2</sub>AX as early as 2 h after irradiation ( $P<0.01$ ). Moreover, PC3 or PANC-1 cells irradiated on the PLDR schedule expressed significantly higher levels of  $\gamma$ -H<sub>2</sub>AX than cells irradiated on the radiotherapy schedule ( $P<0.01$ ). DNA-PKcs

expression showed a similar trend 2 h after irradiation (Figs. 5b and 5g). However, 4 h (PANC-1) or 6 h (PC3) after irradiation, the DNA-PKcs and  $\gamma$ -H<sub>2</sub>AX expression levels of cells irradiated with PLDR showed no difference from those of non-treated cells, while DNA-PKcs and  $\gamma$ -H<sub>2</sub>AX expression levels of cells irradiated with radiotherapy remained relatively high for a long time. At the same time, KU70/KU80 expression in the PLDR group was the same as that in the control group (Figs. 5c, 5d, 5h, and 5i). This indicated that both PLDR and radiotherapy schedules could induce DSBs, but compared with RT, PLDR did not promote effective DNA damage repair. This may explain why cells showed higher radiation sensitivity when irradiated with PLDR than with traditional radiotherapy.

In summary, HRS is a noteworthy phenomenon that plays an important role in traditional radiobiology, and PLDR is an effective re-radiotherapy method. However, most of the research results on the HRS/IRR phenomenon come from studies on isolated cells and animals. The application of HRS/IRR in clinical treatment has just begun, and therefore a large number of clinical studies on PLDR are still needed to provide a stronger theoretical basis and more realistic ideas for clinical treatment of tumors.

## Materials and methods

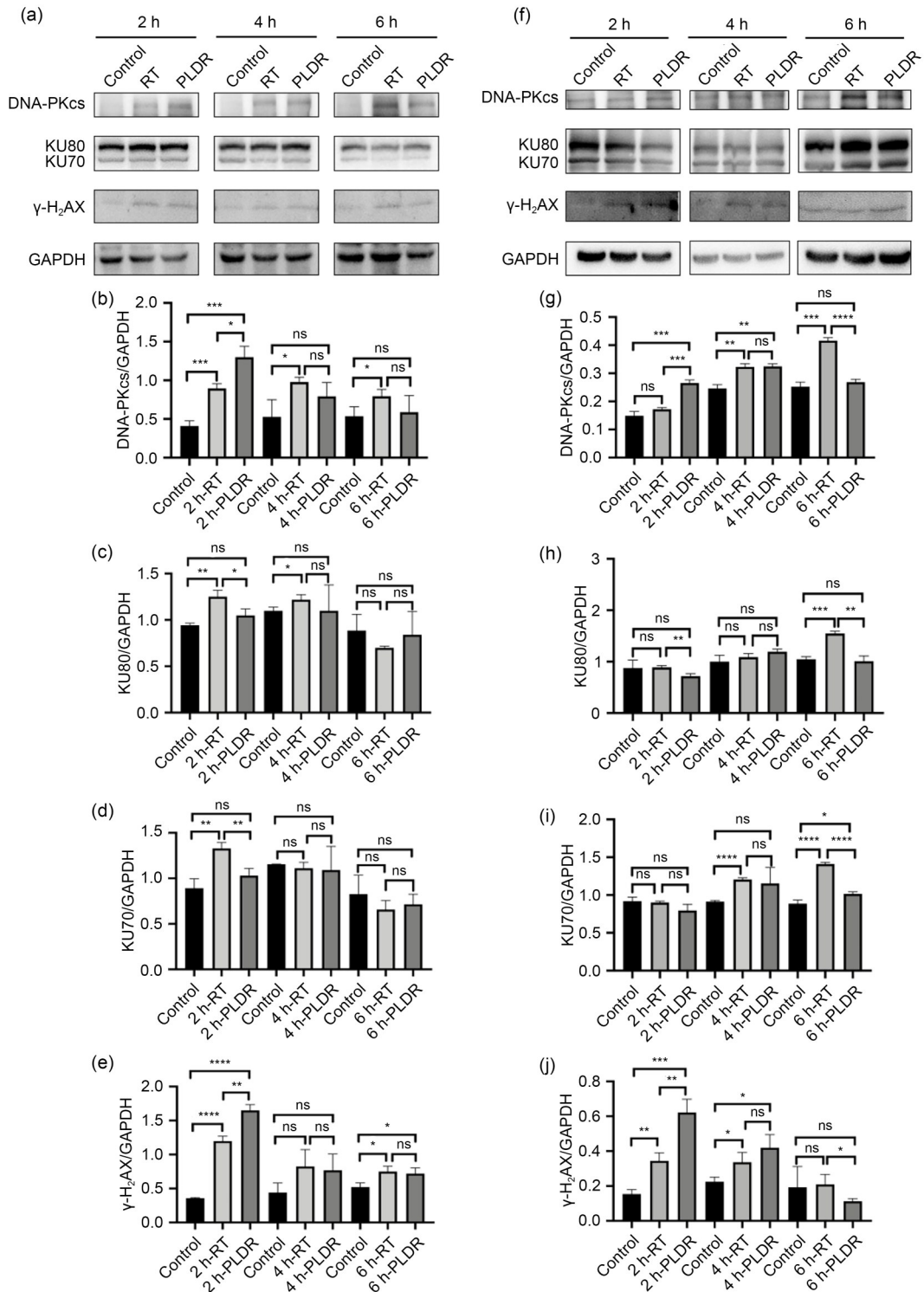
Detailed methods are provided in the electronic supplementary materials of this paper.

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## Author contributions

Xin WEN performed the experimental research and data analysis, wrote and edited the manuscript. Hui QIU and Zhiying SHAO contributed to the writing and editing of the manuscript. Guihong LIU and Nianli LIU contributed to the study design and experiment guidance. Aoxing CHEN and Xingying ZHANG contributed to the establishment of animal models. Xin DING and Longzhen ZHANG performed the study design, paper guidance, and financial support. All authors have read and approved the final manuscript and, therefore, have full access to all the data in the study and take responsibility for the integrity and security of the data.



**Fig. 5** Effects of RT and PLDR schedules on the expression levels of DNA damage proteins in PANC-1 (a–e) and PC3 (f–j) by western blot. PANC-1 (a) and PC3 (f) cell lysates were collected at different time points for western blot. The band intensities of DNA-PKcs (b, g), KU80 (c, h), KU70 (d, i), and  $\gamma$ -H<sub>2</sub>AX (e, j) in PANC-1 (b–e) and PC3 (g–j) cells were quantified after normalized to GAPDH. \*  $P < 0.05$ , \*\*  $P < 0.01$ , \*\*\*  $P < 0.001$ , \*\*\*\*  $P < 0.0001$ . Values are presented as mean  $\pm$  SD ( $n = 3$ ). RT: radiotherapy; PLDR: pulsed low-dose rate; DNA-PKcs: DNA-dependent protein kinase catalytic subunit;  $\gamma$ -H<sub>2</sub>AX: phosphorylation of H<sub>2</sub>AX at Ser139; GAPDH: glyceraldehyde-3-phosphate dehydrogenase; SD: standard deviation; ns: not significant.

### Compliance with ethics guidelines

Xin WEN, Hui QIU, Zhiying SHAO, Guihong LIU, Nianli LIU, Aoxing CHEN, Xingying ZHANG, Xin DING, and Longzhen ZHENG declare that they have no conflict of interest.

This article does not contain any studies with human or animal subjects performed by any of the authors.

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### Supplementary information

Materials and methods