



Sleep and longitudinal cognitive performance in preclinical and early symptomatic Alzheimer's disease

©Brendan P. Lucey,^{1,2} Julie Wisch,¹ ©Anna H. Boerwinkle,¹ Eric C. Landsness,¹ Cristina D. Toedebusch,¹ Jennifer S. McLeland,¹ Omar H. Butt,¹ Jason Hassenstab,^{1,2,3} John C. Morris,^{1,2,3} Beau M. Ances^{1,2,†} and David M. Holtzman^{1,2,3,†}

[†]These authors contributed equally to this work.

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Sleep monitoring may provide markers for future Alzheimer's disease; however, the relationship between sleep and cognitive function in preclinical and early symptomatic Alzheimer's disease is not well understood. Multiple studies have associated short and long sleep times with future cognitive impairment. Since sleep and the risk of Alzheimer's disease change with age, a greater understanding of how the relationship between sleep and cognition changes over time is needed. In this study, we hypothesized that longitudinal changes in cognitive function will have a non-linear relationship with total sleep time, time spent in non-REM and REM sleep, sleep efficiency and non-REM slow wave activity.

To test this hypothesis, we monitored sleep-wake activity over 4–6 nights in 100 participants who underwent standardized cognitive testing longitudinally, APOE genotyping, and measurement of Alzheimer's disease biomarkers, total tau and amyloid- β_{42} in the CSF. To assess cognitive function, individuals completed a neuropsychological testing battery at each clinical visit that included the Free and Cued Selective Reminding test, the Logical Memory Delayed Recall assessment, the Digit Symbol Substitution test and the Mini-Mental State Examination. Performance on each of these four tests was Z-scored within the cohort and averaged to calculate a preclinical Alzheimer cognitive composite score. We estimated the effect of cross-sectional sleep parameters on longitudinal cognitive performance using generalized additive mixed effects models. Generalized additive models allow for non-parametric and non-linear model fitting and are simply generalized linear mixed effects models; however, the linear predictors are not constant values but rather a sum of spline fits.

We found that longitudinal changes in cognitive function measured by the cognitive composite decreased at low and high values of total sleep time ($P < 0.001$), time in non-REM ($P < 0.001$) and REM sleep ($P < 0.001$), sleep efficiency ($P < 0.01$) and < 1 Hz and 1–4.5 Hz non-REM slow wave activity ($P < 0.001$) even after adjusting for age, CSF total tau/amyloid- β_{42} ratio, APOE $\epsilon 4$ carrier status, years of education and sex. Cognitive function was stable over time within a middle range of total sleep time, time in non-REM and REM sleep and < 1 Hz slow wave activity, suggesting that certain levels of sleep are important for maintaining cognitive function.

Although longitudinal and interventional studies are needed, diagnosing and treating sleep disturbances to optimize sleep time and slow wave activity may have a stabilizing effect on cognition in preclinical or early symptomatic Alzheimer's disease.

- 1 Department of Neurology, Washington University School of Medicine, St Louis, MO 63110, USA
- 2 Hope Center for Neurological Disorders, Washington University School of Medicine, St Louis, MO 63110, USA
- 3 Knight Alzheimer Disease Research Center, Washington University School of Medicine, St Louis, MO 63110, USA

Correspondence to: Brendan Lucey
Washington University School of Medicine
Campus Box 8111, 660 South Euclid Avenue, St Louis, MO 63110, USA
E-mail: luceyb@wustl.edu

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Abbreviations: CDR = Clinical Dementia Rating; DSST = Digit Symbol Substitution Test; FCSRT = Free and Cued Selective Reminding Test; MMSE = Mini- Mental State Examination; NREM = non-REM; PACC = preclinical Alzheimer cognitive composite; p-tau = phosphorylated tau; SWA = slow wave activity; t-tau = total tau

Introduction

Deposition of amyloid- β as insoluble parenchymal plaques and intracellular accumulation of aggregated, hyperphosphorylated tau as neurofibrillary tangles throughout the neuropil are key steps in the pathogenesis of Alzheimer's disease that lead to synaptic and neuronal loss, cognitive dysfunction and eventual dementia.^{1,2} Tau hyperphosphorylation (p-tau) is an early step in tau-mediated neurodegeneration. Amyloid PET scans show deposition of amyloid as insoluble fibrillar amyloid- β deposits (i.e. amyloid-positive). The concentration of amyloid- β_{42} in the CSF decreases with amyloid deposition and is also a marker of amyloid status.³ Amyloid PET scans show increasing amounts of amyloid deposition while an individual is still cognitively normal, although CSF total tau (t-tau) begins to increase.^{4–6} Tau PET scans, which show paired helical filament pathology, only become positive many years after amyloid PET scans become positive, and there are already decreases in CSF amyloid- β_{42} and increases in t-tau and p-tau around the time that clinical symptoms appear.^{7,8} Although soluble amyloid- β_{42} , p-tau and t-tau in human CSF are biomarkers for early (amyloid- β_{42}) and increasing (t-tau and p-tau) amyloid deposition, the CSF t-tau/amyloid- β_{42} ratio is associated with increased amyloid deposition in the brain⁴ and is superior to single biomarkers at predicting the risk of clinical decline and conversion to dementia.⁹

Recent work supports a role for sleep disturbances as markers for and/or potential cause(s) of Alzheimer's disease pathology.¹⁰ The risk of developing both Alzheimer's disease and sleep disturbance increases with age.^{11,12} During normal ageing, multiple measures of sleep change, including decreased sleep efficiency, increased night-time awakenings, decreased sleep spindles and increased time in non-REM (NREM) sleep stage 1 or drowsiness.¹³ Furthermore, sleep measures, such as time spent in NREM stage 3 sleep, change with age and sex,¹³ making their relationships to future Alzheimer's disease risk difficult to define. Sleep disorders, such as obstructive sleep apnoea and restless legs syndrome, result in sleep disturbance and are age-associated.^{14,15} Although controlling for preclinical Alzheimer's disease markedly attenuates the commonly held notion of diminishing cognitive performance as a function of age alone,¹⁶ poor sleep has been associated with worse cognitive performance in older adults.¹⁷

Prior work delving into the relationship between sleep duration and future risk of cognitive performance have shown inconsistent results.^{18–20} For instance, a study of 1844 females aged 70–81 years

who completed baseline cognitive assessments and were retested 2 years later were found to have worse cognitive decline over time if their self-reported sleep duration was ≤ 5 h/night compared to 7 h/night; females who reported sleeping ≥ 9 h/night did not experience cognitive decline.²¹ In contrast, a cross-sectional study of 3212 individuals aged ≥ 60 years found that those individuals who self-reported sleeping ≥ 11 h/night were found to have poor cognitive function compared to participants who reported sleeping 7 h/night.²² Multiple studies have also shown that both shorter and longer sleep duration are associated with decreased cognitive performance.^{23,24} For example, a cross-sectional study of 1115 individuals aged ≥ 60 years found that both self-reported short (< 6 h/night) and long (> 8 h/night) sleep durations were associated with cognitive impairment.²⁵ These studies were performed in older adults with < 10 years of follow-up. Recent work in middle-aged adults followed for up to 25 years found that short sleep duration was associated with an increased risk of dementia.²⁶

There is an increasing recognition that the relationship between cognition, Alzheimer's disease risk factors and biomarkers for Alzheimer's disease is non-linear. For instance, rates of amyloid and tau accumulation in the brain change with both age and apolipoprotein E4 (APOE $\epsilon 4$) allele carrier status. CSF p-tau levels increase in APOE $\epsilon 4$ non-carriers from an age of ~ 55 years and plateau at ~ 75 years, whereas APOE $\epsilon 4$ carriers show a linear increase in CSF p-tau starting at an age of ~ 50 years.²⁷ Another study reported that the relationship between longitudinal memory performance and blood pressure is non-linear and varies with age, depending on the baseline blood pressure.²⁸

The differing results from studies of sleep duration and risk of cognitive impairment may be due to a non-linear relationship between total sleep time and cognition. A meta-analysis of nine cohort studies involving 22 187 participants with longitudinal cognitive assessments and both self-reported sleep duration and that objectively measured with actigraphy found that the relationship between sleep duration and the risk of cognitive dysfunction showed a U-shaped dose-response relationship with the lowest risk of cognitive impairment occurring in those with a sleep duration of 7–8 h/day.²⁹ A second meta-analysis of 11 cross-sectional and seven prospective cohort studies of 97 264 participants also found that both short and long self-reported sleep durations were associated with increased cognitive impairment.³⁰

Sleep has been proposed as a potential marker for Alzheimer's disease pathology that could be non-invasively monitored to assess the risk of future Alzheimer's disease or track responses to

interventions during clinical trials. Since both sleep and Alzheimer's disease risk change with age and potentially interact, a greater understanding of how sleep and cognition change with age and at different stages of Alzheimer's disease pathology is needed. Previous studies have primarily relied on self-reported total sleep time and other sleep measures. Furthermore, measures of sleep quality such as sleep efficiency and NREM slow wave activity (SWA) have been associated with Alzheimer's disease pathology^{31–33} and cognitive function.^{34–36}

Participants in previous studies of sleep and cognition have not been well characterized for Alzheimer's disease biomarkers or genetic risk factors for Alzheimer's disease such as their APOE ϵ 4 carrier status. In this study, we hypothesized that longitudinal changes in cognitive function will have a non-linear relationship with total sleep time, time spent in NREM and REM sleep, sleep efficiency, and NREM SWA. To test this hypothesis, we objectively monitored sleep-wake activity with a single-channel EEG device over 4–6 nights in 100 participants who also underwent standardized annual cognitive testing, genotyping for APOE ϵ 4 status and measurement of CSF Alzheimer's disease biomarkers.

Materials and methods

Participants

Data from 100 community-living participants enrolled in longitudinal studies at the Knight Alzheimer Disease Research Center (ADRC), Washington University in St. Louis, were used. Participants were included if they had completed at least 4 nights of single-channel EEG monitoring, one lumbar puncture for CSF analysis, genotyping for APOE ϵ 4 status and two or more neuropsychological testing visits. All individuals participating in Knight ADRC studies undergo annual clinical and cognitive assessments by a clinician. Clinical Dementia Rating (CDR) is used in longitudinal studies and clinical trials for staging dementia in general and in dementia due to Alzheimer's disease.³⁷ For this analysis, participants were either classified as cognitively normal (CDR 0), or cognitively impaired (CDR > 0). All but one of the cognitively impaired participants were only mildly impaired (CDR 0.5). At the Knight ADRC, the standard protocol is to access the CDR annually. The CDR and other neuropsychological tests have been very stable tools for assessing the stage and degree of impairment in dementia over many years in our cohort.³⁸ This study was approved by the Washington University in St. Louis Institutional Review Board and each participant provided signed informed consent.

Preclinical Alzheimer Cognitive Composite

Individuals completed a neuropsychological testing battery at each clinical visit that included the Free and Cued Selective Reminding Test (FCSRT), the Logical Memory Delayed Recall Test from the Wechsler Memory Scale–Revised, the Digit Symbol Substitution Test (DSST) from the Wechsler Adult Intelligence Scale–Revised and the Mini-Mental State Examination (MMSE). These tests were administered and scored by experienced psychometrists. Performance on each of these four tests was Z-scored within the cohort and averaged in order to calculate a Preclinical Alzheimer Cognitive Composite (PACC) score.³⁹

Sleep monitoring and EEG power analysis

Sleep monitoring was performed as previously described.⁴⁰ To briefly review, sleep was recorded longitudinally in all participants at home for up to 6 nights using sleep logs, actigraphy (Actiwatch 2, Philips Respironics) and a single-channel EEG device worn on

the forehead (Sleep Profiler, Advanced Brain Monitoring). Average total sleep time, time in NREM sleep stages 2 and 3 (time in NREM), time in REM sleep, sleep efficiency and <1 Hz and 1–4.5 Hz NREM SWA were used in all analyses. Sleep efficiency was calculated based on the lights off and lights on times for the single-channel EEG studies and were corroborated with sleep logs. Single-channel EEG sleep studies were visually scored by registered polysomnographic technologists using criteria adapted from the standard American Academy of Sleep Medicine criteria.⁴¹ Nights were excluded if > 10% of the recording was artefactual or if the bed and rise times did not match the sleep log and/or actigraphy. All participants needed at least 4 nights of single-channel EEG monitoring that met these criteria to be included. Time in NREM sleep stages 2 and 3 were combined, because we found this has a higher level of agreement with polysomnography.⁴¹ NREM SWA was calculated for each single-channel EEG study using MATLAB (MathWorks, Natick, MA), and the average NREM SWA was used in the analysis. As previously described,⁴¹ a band-pass (two-way least-squares finite impulse response) filter between 0.5 and 40 Hz was applied to the single-channel EEG data. Spectral analysis was performed in consecutive 5-s epochs (Welch method, Hamming window, no overlap). SWA power was calculated by averaging the power in the frequency bins of 0.5–1.0 Hz and 1.0–4.5 Hz. To semi-automatically remove artefactual epochs, power in the 20–30 and 0.5–4.5 Hz bands for each electrode across all epochs of a recording were displayed. The operator (B.P.L.) then selected a threshold between the 95 and 99.5% threshold of power to remove artefactual epochs. The data were then natural log-transformed to normalize the data.

CSF biomarkers

CSF was collected under a standardized protocol.⁴² After fasting overnight, participants underwent a lumbar puncture at 8 a.m., when 20–30 ml of CSF was collected by gravity drip into a 50-ml conical tube using a 22-gauge atraumatic Sprotte spinal needle, gently inverted to disrupt potential gradient effects and centrifuged at low speed to pellet any cellular debris. Samples were aliquoted (500 μ l) in polypropylene tubes and stored at -80°C until analysis. CSF amyloid- β_{42} , t-tau and p-tau 181 were measured as previously described using an automated electrochemiluminescence immunoassay (Elecsys on the cobas e 601 analyzer, Roche).⁴²

Statistical analysis

For demographic variables at the time of sleep monitoring, group differences between cognitively normal (CDR 0) and impaired (CDR > 0) participants were compared using t-tests for continuous variables and chi-square tests for categorical variables. We then used generalized additive mixed effects models^{43,44} to estimate the effect of cross-sectional total sleep time, sleep efficiency, time in NREM sleep, time in REM sleep and <1 Hz and 1–4.5 Hz NREM SWA on longitudinal cognitive performance measured by the PACC scores. Generalized additive models are powerful tools that allow for non-parametric and non-linear model fitting in the context of frequentist statistics. A generalized additive model is simply a generalized linear mixed effects model; however, the linear predictors are not constant values but rather a sum of spline fits. Generalized additive models have been used in sample sizes ≤ 100 ^{45–47} and 100–200^{48–50} to study non-linear relationships in neurodegenerative and cardiovascular diseases. We included an individual participant identifier as a random effect since these were longitudinal data. Generalized additive models implemented in the R Package mgcv⁴⁴ apply basis functions as predictors.

For each of the generalized additive models in this analysis, we fit splines to age at PACC score completion, the sleep parameter of

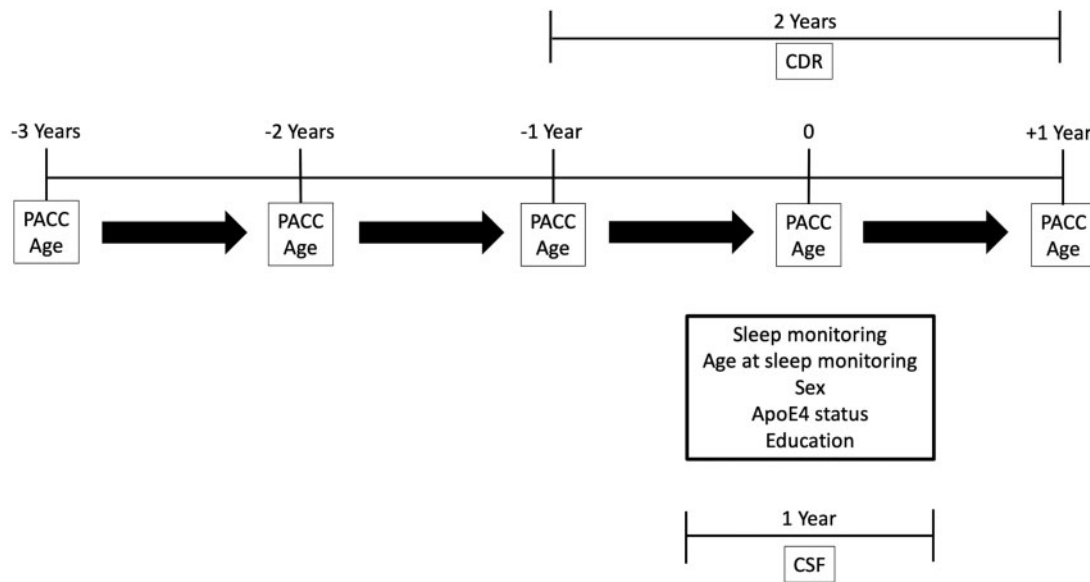


Figure 1 Overview of data collection. Sleep monitoring was performed over 4–6 nights in all participants. CSF was collected within ≤ 1 year of sleep monitoring and CDR measured ≤ 2 years of sleep monitoring. Participants underwent annual cognitive assessments before and after sleep monitoring to generate PACC scores.

Table 1 Participant characteristics

	Cognitively normal CDR = 0 (n = 88)	Cognitively impaired CDR > 0 (n = 12)	P-value
Age at sleep study, years, mean (SD)	75.23 (4.99)	78.27 (5.61)	0.054
Sex, number of males (%)	43 (48.9)	6 (50.0)	1.000
Years of education, mean (SD)	16.67 (2.36)	16.58 (2.07)	0.903
APOE $\epsilon 4$ status: n APOE $\epsilon 4$ + (%)	29 (33.0)	5 (41.7)	0.785
Race			0.431
More than one (%)	1 (1.1)	0 (0.0)	
African American (%)	10 (11.4)	0 (0.0)	
Caucasian (%)	77 (87.5)	12 (100.0)	
Total sleep time, h, mean (SD)	6.32 (0.77)	6.47 (0.84)	0.546
Sleep efficiency, %, mean (SD)	79.33 (8.50)	76.40 (9.60)	0.273
< 1 Hz NREM SWA, $\mu V^2/Hz$, mean (SD)	59.85 (46.4)	66.57 (45.8)	0.651
1–4.5 Hz NREM SWA, $\mu V^2/Hz$, mean (SD)	17.63 (10.80)	18.70 (10.30)	0.757
AHI, number of respiratory events/h of monitoring time (%)			0.156
None (<5)	33 (37.5)	6 (50.00)	
Mild (5–15)	39 (44.3)	5 (41.7)	
Moderate (15–30)	15 (17.0)	0	
Severe (>30)	1 (1.1)	1 (8.3)	
PLMI, number of leg movements/h of monitoring time (%)			0.003
None (<15)	48 (54.5)	1 (8.3)	
Low (15–45)	17 (19.3)	7 (58.3)	
High (>45)	23 (26.1)	4 (33.3)	
T-tau/amyloid- β_{42} ratio, n (%)			0.007
Amyloid-negative ^a	55 (62.5)	2 (16.7)	
Amyloid-positive ^a	33 (37.5)	10 (83.3)	
Years between PACC assessments	1.15	1.12	0.725
Number of PACC assessments (SD)	5.89 (3.00)	4.75 (3.77)	0.236
Years of follow-up (SD)	5.49 (3.37)	4.07 (3.80)	0.180

Comparisons were made by unpaired t-test. AHI = apnoea-hypopnea index; APOE $\epsilon 4$ + = apolipoprotein E $\epsilon 4$ -positive status; PLMI = periodic limb movement index; SD = standard deviation.

^aT-tau/amyloid- β_{42} cut-point for amyloid status = 0.211.⁴²

interest (total sleep time, time in NREM sleep, time in REM sleep, sleep efficiency or NREM SWA) and the individual random effect where the PACC score was the dependent variable of interest. In

these analyses, we included APOE $\epsilon 4$ status, sex (referenced to female), years of education, age at sleep study participation, estimated Alzheimer’s disease pathology measured by the CSF t-tau/

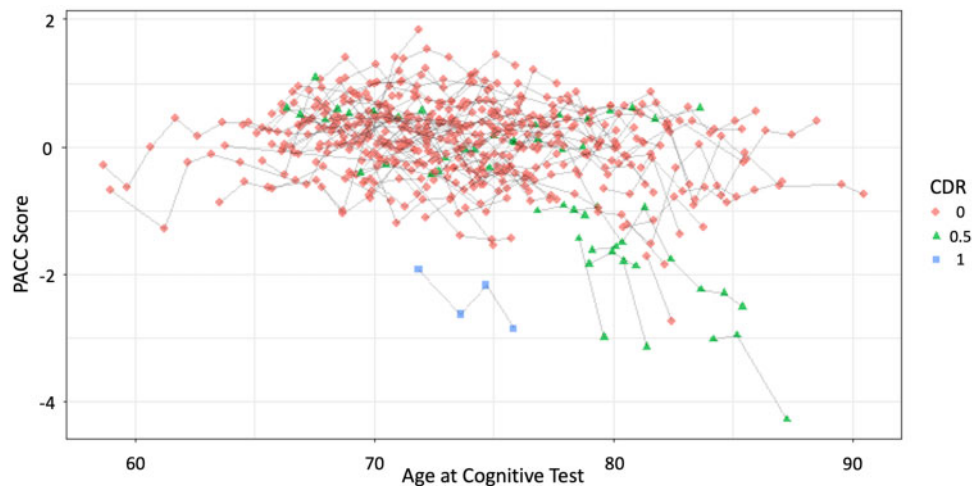


Figure 2 Distribution of longitudinal PACC scores by age. Spaghetti plots of the PACC scores are shown for each participant at the age when testing was performed. Overall, cognitive performance on the PACC was relatively stable between -1 and 1 for the majority of participants. A subset of participants who were >70 years of age at baseline showed more rapid decline in PACC performance.

CSF amyloid- β_{42} ratio within 1 year of sleep monitoring and CDR within 2 years of sleep monitoring as covariates. An overview of the timing of data collection is shown in Fig. 1. The CDR was included in the model, because it is the gold standard for overall clinical and cognitive status in patients with Alzheimer's disease and allows for overall stage of Alzheimer's disease to be controlled for in the models. Moreover, the CDR does not use cognitive scores and is the marker often used as the primary outcome in clinical trials. Although the CDR is the gold standard for clinical and cognitive status, the use of biomarkers and neuropsychological testing helps to supplement the diagnosis. The CSF t-tau/amyloid- β_{42} ratio is a marker for amyloid pathology and future risk of cognitive impairment, because once an individual starts to accumulate amyloid and the ratio increases, they will eventually progress to symptomatic Alzheimer's disease.^{4,51} A generalized form of this model is shown as Equation 1, where $s()$ indicates that a spline fit was applied. The distributions of both age at PACC and sleep parameter of interest were assumed to be Gaussian.

$$\begin{aligned} \text{PACC} \sim & s(\text{Age at PACC}) + s(\text{Sleep Parameter}) \\ & + s(\text{Individual Random Effect}) + \text{APOE}\epsilon 4 \text{ status} + \text{Sex} \\ & + \text{Years of Education} + \text{Age at Sleep Study} \\ & + \text{CSF} \frac{\text{t-tau}}{\text{Amyloid-}\beta_{42}} + \text{CDR} \end{aligned} \quad (1)$$

The maximum number of knots for each spline fit was limited to four to minimize overfitting. The number of knots specifies the dimension of the basis function used to represent the smoothing parameter and was selected using an iterative backfitting algorithm. Cyclic cubic regression splines were used for smoothing the age at PACC and sleep parameter predictors, and ridge penalties were used for smoothing random effects. We used generalized cross-validation for smoothing parameter estimation. We also performed generalized linear models with the same covariates as used in the generalized additive models: sleep parameter, CDR, CSF t-tau/amyloid- β_{42} , age at sleep study, age at PACC, APOE $\epsilon 4$ status, sex and education. Generalized linear models account for the dependencies among the longitudinal measurements. All model variables were treated as fixed effects with random intercepts and slopes to accommodate individual variation. All analyses were performed using R.

Data and material availability

All of the data that support the findings of this study are available from the corresponding author upon reasonable request. All code associated with this analysis is freely available from the corresponding author upon reasonable request.

Results

Participant characteristics

Table 1 shows the demographic and clinical characteristics of cognitively normal (CDR 0) and cognitively impaired (CDR > 0) participants at the time of sleep study monitoring. There were no significant differences in the CDR 0 and CDR > 0 groups with regard to age, sex, years of education, APOE $\epsilon 4$ status, race, total sleep time, sleep efficiency, NREM SWA, apnoea-hypopnoea index (measure of sleep apnoea), years between PACC assessments, number of PACC assessments, or years of follow-up. CDR > 0 participants had significantly more participants with a periodic limb movement index > 15 (measure of periodic leg movements during sleep) than CDR 0 participants. Twelve individuals (12%) had a baseline CDR of 0.5 or greater. A single individual had a baseline CDR of 1.0. No individuals progressed from CDR 0 to 0.5 or from 0.5 to 1.0 during the follow-up window, and participants had on average 4–5 years of follow-up (Table 1) with a range of 2–12 years (Supplementary Fig. 1). Most participants (78%) underwent cognitive assessments that crossed the date of sleep monitoring, 22% undertook these before the date of sleep monitoring, while none underwent them after the date of sleep monitoring. A detailed comparison between the baseline and final PACC scores, including individual component assessments, can be found in Supplementary Tables 1 and 2. As expected, a greater percentage of CDR > 0 participants showed greater evidence of Alzheimer's disease pathology as measured by the CSF t-tau/amyloid- β_{42} ratio. The unadjusted relationship between PACC scores and age is shown in Fig. 2. The change in longitudinal PACC scores was in the range -1 to 1 for the majority of participants, but a subset of participants >70 years of age showed greater decreases in PACC performance over time.

Table 2 Generalized additive models of the relationship between longitudinal PACC scores and total sleep time, sleep efficiency, NREM stage 2 and stage 3 and REM sleep

Generalized additive models									
	Total sleep time			Sleep efficiency		NREM stages 2 and 3		REM	
	EDF			EDF		EDF		EDF	
Spline fit	2.377 ^{***}			2.808 ^{**}		2.6100674 ^{***}		1.6478 ^{***}	
Sleep parameter	2.836 ^{***}			2.821 ^{***}		2.8406516 ^{***}		2.7936 ^{***}	
Age at PACC	1.118×10^{-3}			9.09×10^{-2}		4.752×10^{-4}		0.2533	
Participant ID									
Covariate	Estimate	95% CI	Estimate	95% CI	Estimate	95% CI	Estimate	95% CI	
CDR	-1.592 ^{***}	-1.903, -1.281	-1.551 ^{***}	-1.880, -1.222	-1.589 ^{***}	-1.913, -1.266	-1.423 ^{***}	-1.744, -1.101	
CSF t-tau/amyloid- β_{42}	-1.171 ^{***}	-1.500, -0.843	-1.047 ^{***}	-1.386, -0.708	-1.140 ^{***}	-1.476, -0.804	-1.108 ^{***}	-1.445, -0.770	
Age at sleep study	0.038 ^{***}	0.022, 0.055	0.025 ^{**}	0.008, 0.042	0.037 ^{***}	0.019, 0.054	0.026 ^{**}	0.009, 0.042	
APOE $\epsilon 4+$	0.146 [†]	0.027, 0.266	0.135 [†]	0.011, 0.258	0.167 ^{**}	0.048, 0.287	0.179 ^{**}	0.059, 0.299	
Sex (male effect)	-0.236 ^{***}	-0.343, -0.129	-0.181 ^{**}	-0.290, -0.073	-0.177 ^{**}	-0.288, -0.066	-0.231 ^{***}	-0.338, -0.123	
Education (years)	0.006	-0.018, 0.030	0.012	-0.014, 0.038	0.007	-0.018, 0.032	0.008	-0.017, 0.033	
Intercept	-2.600 ^{***}	-3.938, -1.261	-1.593 [†]	-3.023, -0.163	-2.537 ^{***}	-3.927, -1.147	-1.658 [†]	-3.033, -0.284	

n = 100; dependent variable = PACC. EDF = effective degrees of freedom.

[†]P < 0.05, ^{**}P < 0.01, ^{***}P < 0.001.

Table 3 Generalized additive models of the relationship between longitudinal PACC scores and <1 Hz NREM SWA and 1–4.5 Hz NREM SWA

Generalized additive models									
	Ln (<1 Hz NREM SWA)					Ln (1–4.5 Hz NREM SWA)			
	EDF					EDF			
Spline fit	2.55368 ^{**}					2.8279655 ^{**}			
Sleep parameter	2.84824 ^{***}					2.8507198 ^{***}			
Age at PACC	0.06847					2.473×10^{-4}			
Participant ID									
Covariate	Estimate	95% CI	Estimate	95% CI	Estimate	95% CI	Estimate	95% CI	
CDR	-1.384 ^{***}	-1.702, -1.065	-1.365 ^{***}	-1.681, -1.048	-1.365 ^{***}	-1.681, -1.048	-1.365 ^{***}	-1.681, -1.048	
CSF t-tau/amyloid- β_{42}	-0.879 ^{***}	-1.224, -0.534	-0.925 ^{***}	-1.269, -0.581	-0.925 ^{***}	-1.269, -0.581	-0.925 ^{***}	-1.269, -0.581	
Age at sleep study	0.026 ^{**}	0.009, 0.043	0.023 ^{**}	0.006, 0.040	0.023 ^{**}	0.006, 0.040	0.023 ^{**}	0.006, 0.040	
APOE $\epsilon 4+$	0.131 [†]	0.011, 0.252	0.155 [†]	0.035, 0.274	0.155 [†]	0.035, 0.274	0.155 [†]	0.035, 0.274	
Sex (male effect)	-0.240 ^{***}	-0.360, -0.121	-0.223 ^{***}	-0.343, -0.103	-0.223 ^{***}	-0.343, -0.103	-0.223 ^{***}	-0.343, -0.103	
Education, years	0.001	-0.024, 0.026	-0.007	-0.032, 0.018	-0.007	-0.032, 0.018	-0.007	-0.032, 0.018	
Intercept	-1.635 [†]	-3.006, -0.263	-1.272	-2.639, 0.094	-1.272	-2.639, 0.094	-1.272	-2.639, 0.094	

n = 100; dependent variable = PACC. EDF = effective degrees of freedom.

[†]P < 0.05, ^{**}P < 0.01, ^{***}P < 0.001.

Sleep and longitudinal cognitive performance are non-linear

To assess the relationship between sleep and longitudinal changes in cognitive performance, we performed generalized additive models of total sleep time, sleep efficiency, time in NREM stage 2 and 3, time in REM, <1 Hz and 1–4.5 Hz NREM SWA with longitudinal PACC scores, age at the time of cognitive testing, age at the time of sleep monitoring, sex, CDR score within 2 years of sleep monitoring, APOE $\epsilon 4$ status, CSF t-tau/amyloid- β_{42} ratio and years of education. We found that the longitudinal PACC performance varied with the value of each sleep parameter. For total sleep time, sleep efficiency, time in NREM stage 2 and 3, time in REM, and NREM SWA, both the sleep parameter and age at PACC were found to have significant spline fits in the fully adjusted model. CDR, CSF t-tau/amyloid- β_{42} ratio and sex (male effect) showed a significant inverse relationship with longitudinal PACC scores for all models. Age at the sleep study visit and APOE $\epsilon 4+$ status had positive linear relationships with PACC scores in all models. Years of education was not significant in any model (Tables 2 and 3, Figs 3A, C, E, F and 4A and C).

The estimated spline functions for total sleep time, sleep efficiency, time in NREM, time in REM, and NREM SWA showed bimodal distributions. For instance, total sleep times of <4.5 h and >6.5 h were associated with worse cognitive performance over time (Fig. 3B). However, there was no change in PACC after adjusting for the model covariates in between these total sleep durations (i.e. the 95% confidence intervals are not above or below zero change in PACC performance over time). Although sleep efficiency was non-linearly related to longitudinal PACC performance, the 95% confidence intervals crossed zero (i.e. no significant change in PACC scores over time) except between 60–65% where PACC performance decreased ~ 0.1 (Fig. 3D). Both time in NREM and time in REM sleep showed an inverse U-shaped relationship with change in PACC scores over time (Fig. 3F and H). NREM SWA (1–4.5 Hz) was similar to sleep efficiency with 95% confidence intervals crossing zero, but low and high <1 Hz NREM SWA was related with worsening PACC performance of ~ 0.2 (Fig. 4B and D). These findings suggest that total sleep time, time in NREM, time in REM, and <1 Hz NREM SWA are more sensitive measures for longitudinal PACC performance than sleep efficiency or 1–4.5 Hz NREM SWA.

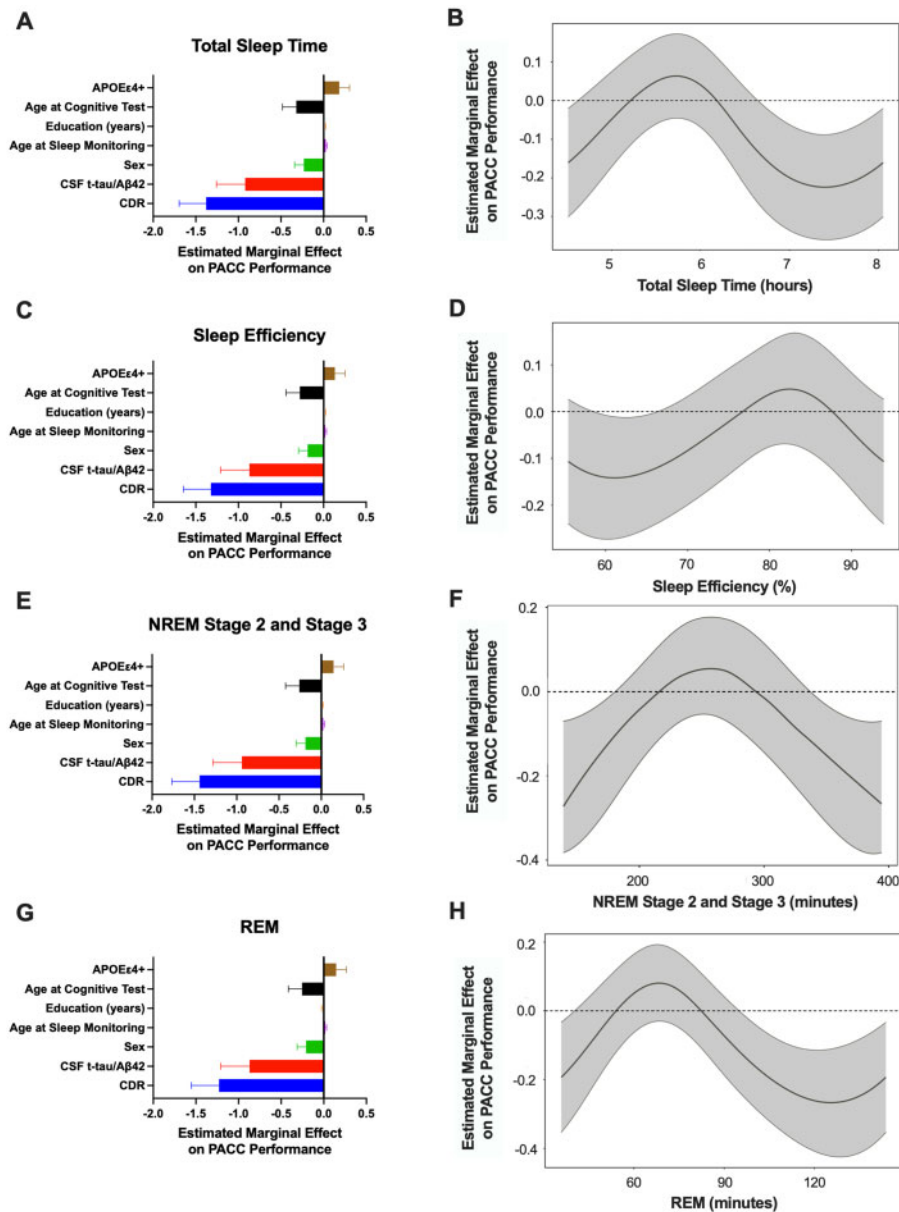


Figure 3 Longitudinal PACC performance and sleep time are non-linearly related. In 100 participants, generalized additive models found that the association of longitudinal PACC performance with total sleep time, sleep efficiency, time in NREM stage 2 and stage 3 sleep, and time in REM sleep was non-linear after adjusting for APOE ϵ 4-positive status, age at cognitive test, age at sleep monitoring, education, sex (male effect), CSF t-tau/amyloid- β ₄₂ and CDR. For the models of total sleep time (A), sleep efficiency (C), time in NREM stage 2 and 3 sleep (E), and time in REM sleep (G), the estimated marginal effect on longitudinal PACC performance (i.e. change in PACC score over time) is shown for each of the covariates. The estimated smoothed spline function of total sleep time in the fully adjusted model shows that a total sleep time <4.5 h and >6.5 h was associated with worse PACC performance over time (B). For sleep efficiency (D), PACC performance was generally unchanged over time. Time spent in NREM stage 2 and 3 (F) and in REM sleep (H) showed inverse U-shaped relationships with longitudinal PACC performance.

To test if generalized additive models best fit our data, we used linear mixed effects models adjusted for the same covariates to test if a linear function describes the relationship between longitudinal PACC and total sleep time, sleep efficiency, time in NREM stage 2 and 3, time in REM, and <1 Hz and 1–4.5 Hz NREM SWA. Total sleep time was found to have an inverse relationship with longitudinal PACC (Supplementary Table 3). In addition to total sleep time, CDR, CSF t-tau/amyloid- β ₄₂ ratio, and sex (male effect) were also significant. Sleep efficiency, time in NREM stage 2 and 3, time in REM, <1 Hz NREM SWA, and 1–4.5 Hz NREM SWA, however, were not significant using a generalized linear model although

CDR, CSF t-tau/amyloid- β ₄₂ ratio, and sex remained significant (Supplementary Tables 3 and 4).

To understand how each of the four cognitive tests that comprise the PACC change with two representative sleep measures (total sleep time and <1 Hz NREM SWA), we included the MMSE, FCSRT, DSST, and Logical Memory tests as the dependent variable in our generalized additive models (Supplementary Tables 5–8). Total sleep time showed a similar association with the MMSE, FCSRT, and Logical Memory Test as with the PACC, but the DSST did not. NREM SWA <1 Hz was also significantly related to the FCSRT, DSST, and Logical Memory Test but not the MMSE. To test

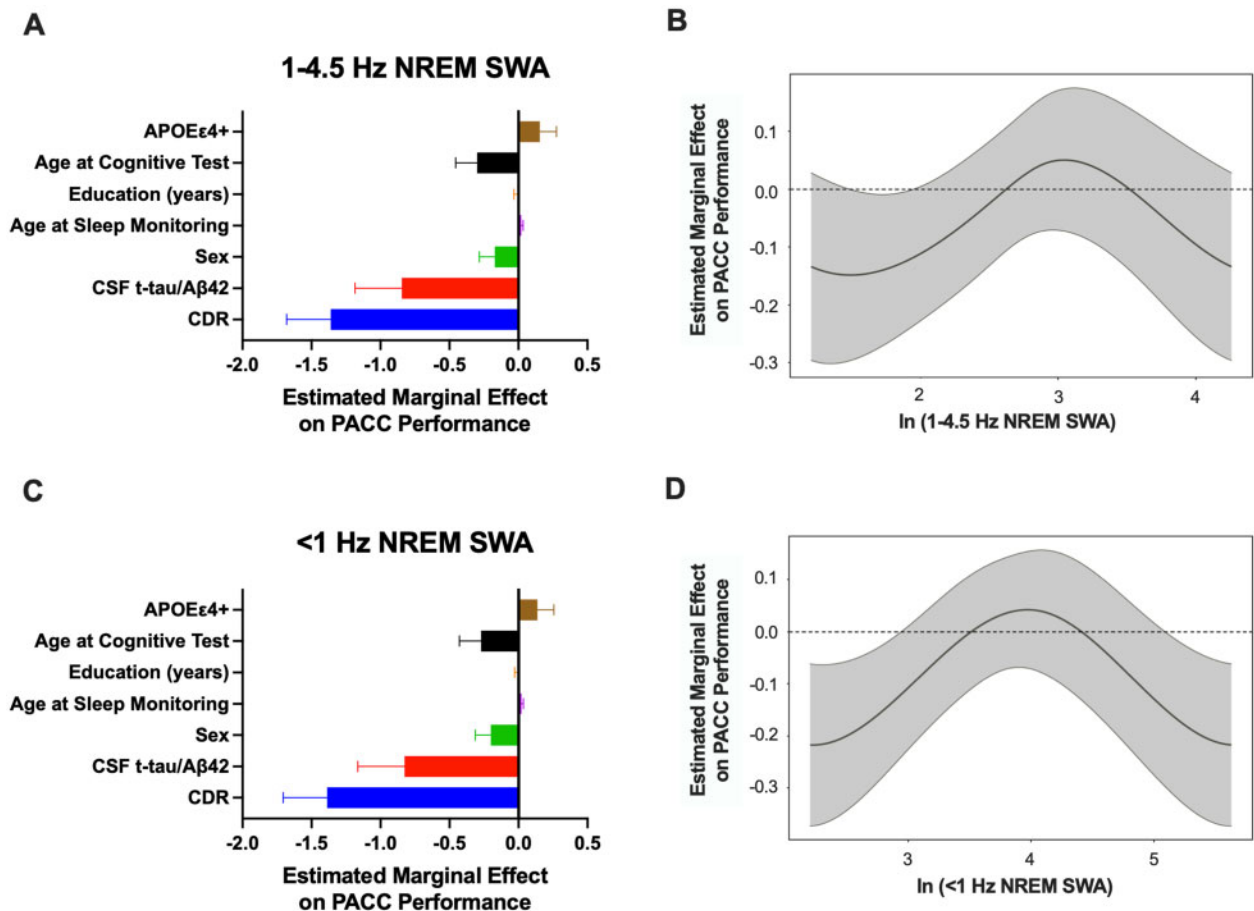


Figure 4 Longitudinal PACC performance and NREM SWA are non-linearly related. In 100 participants, generalized additive models found that the association of longitudinal PACC performance with NREM SWA was non-linear after adjusting for APOE ϵ 4-positive status, age at cognitive test, age at sleep monitoring, education, sex (male effect), CSF t-tau/amyloid- β ₄₂ and CDR. For the models of 1–4.5 Hz NREM SWA (A) and < 1 Hz NREM SWA (C), the estimated marginal effect on longitudinal PACC performance (i.e. change in PACC score over time) is shown for each of the covariates. The estimated smoothed spline function of ln (1–4.5 Hz NREM SWA) in the fully adjusted model shows a non-linear relationship with PACC performance generally unchanged over time (B). Ln (< 1 Hz NREM SWA) showed inverse U-shaped relationships with longitudinal PACC performance (D).

if the four cognitive tests that make up the PACC are linearly associated with sleep, we included the MMSE, FCSRT, DSST, and Logical Memory tests as the dependent variable in our generalized linear models (Supplementary Tables 9–12). We found that the total sleep time was inversely related to FCSRT and Logical Memory tests, but not MMSE or DSST; <1 Hz NREM SWA was not linearly associated any individual cognitive test.

Discussion

In this study, we observed that the relationship between cross-sectional measures of total sleep time, time in NREM stage 2 and 3, time in REM, and <1 Hz NREM SWA and cognitive function over time, as assessed by the PACC, was non-linear. This relationship was seen even after adjusting for multiple potential confounders that can affect sleep and cognition, including age, CSF markers of Alzheimer’s disease pathology, APOE ϵ 4 allele carrier status, years of education and sex. These findings have important implications for using sleep to track the risk of developing cognitive impairment in the clinic or in response to an intervention in a clinical trial. Furthermore, these results support the suggestion that sleep measures have an optimal middle range where PACC scores are stable and suggest targets for sleep interventions to help maintain

cognitive function in individuals at risk of developing Alzheimer’s disease. We also found that the Logical Memory Test, a story memory test, was significantly associated with both total sleep time and <1 Hz NREM SWA. The MMSE, a general cognitive test, was associated with total sleep time while the DSST, a test of multiple cognitive functions, was associated with <1 Hz NREM SWA. The FCSRT, a word list test of episodic memory, was associated with both total sleep time and <1 Hz NREM SWA. Further research is needed to determine if specific sleep measures are associated with longitudinal changes on specific neuropsychological tests.

Our study supports previously reported associations between increased risk of cognitive impairment and both short and long total sleep time. Furthermore, time spent in both NREM and REM sleep showed similar non-linear relationships suggesting that the relationship between total sleep time and cognitive function is not due to increases or decreases in specific sleep stages. However, future studies are needed to test this hypothesis. Unlike prior studies that used self-reported total sleep time, we objectively assessed total sleep time over multiple nights using a single-channel EEG device that compares favourably to polysomnography.⁴¹ Comparing our findings to previous work for cut-offs of short and long total sleep time must account for different methods used to measure sleep duration. We have recently shown in our cohort that self-reported total sleep time is ~1 h longer than that measured by the single-channel

EEG device on the same night.⁵² Fewer studies have investigated the relationship between cognitive performance and sleep duration measured by polysomnography.^{53–55} In those studies, participants were monitored with polysomnography for only 1 night in either a sleep lab or at home, which may not have represented a typical night of sleep. In contrast, all participants in our study had sleep-wake activity measured by single-channel EEG for 4–6 nights at home, which more likely represented how each participant typically sleeps. The single-channel EEG is recorded from electrodes placed on the forehead, however, and provides more limited monitoring of sleep-wake activity compared with polysomnography.

The estimated marginal effect of total sleep time, time in NREM, and time in REM on PACC performance was approximately –0.2 to –0.3 at the shortest and longest sleep times. In the generalized additive model, this was less than the estimated marginal effect of CDR and CSF t-tau/amyloid- β_{42} (–1.0 to –1.5), greater than the effects of APOE $\epsilon 4$ status and education, but similar to age and sex. Although longitudinal PACC scores and total sleep time had a significant inverse relationship with the simpler linear model, we think a non-linear model better explains findings reported in the literature.

The estimated marginal effect of low and high <1 Hz NREM SWA on longitudinal PACC performance was approximately –0.2, less than the effect of CDR (–1.5) and CSF t-tau/amyloid- β_{42} (–0.5 to –1.0) in our model but comparable to age and sex. Longitudinal PACC scores and NREM SWA were not significantly associated in the linear model, suggesting that the non-linear model more accurately represents these relationships. The 1–4.5 Hz NREM SWA had a smaller marginal effect on PACC performance than the <1 Hz NREM SWA, supporting the suggestion that <1 Hz slow oscillations as a critical marker of cognitive function.

Decreased NREM SWA is correlated with poor cognitive performance³⁴ and Alzheimer's disease pathology.^{32,33} Increased SWA may be a marker of cortical dysfunction in Alzheimer's disease. Disturbed neuronal activity in early preclinical Alzheimer's disease, resulting in excitation/inhibition imbalance with neuronal hyperexcitability and hypersynchrony, is hypothesized to connect structural Alzheimer's disease brain pathology with cognitive dysfunction.^{56–58} For instance, resting EEG studies have shown increases in SWA within individuals with cognitive impairment and early Alzheimer's disease^{59,60} and resting state theta-delta hypersynchrony has also been correlated with both amyloid and tau pathology.⁶¹ Although our participants showed no evidence of seizure activity, clinically silent focal interictal discharges and seizures in the hippocampus have been reported in mildly impaired patients with Alzheimer's disease.⁶² Patients with focal epilepsy and evidence of neuronal hyperexcitability (e.g. interictal spikes, seizures) have increased NREM SWA and reduced daytime learning compared to control participants.⁶³ This example suggests how occult hyperexcitability may increase NREM SWA and decrease cognitive performance. Moreover, individuals with REM sleep behaviour disorder, a parasomnia that predicts later occurrence of synucleinopathies such as Parkinson's disease, have increased NREM SWA compared to controls,⁶⁴ suggesting that similar findings may be seen in the early stages of other neurodegenerative diseases. Future studies with high density EEG are needed in individuals at different stages of Alzheimer's disease to characterize sleep's effect on longitudinal cognitive performance, including assessment of sleep spindles, <1 Hz NREM slow waves, slow oscillation-spindle coupling that have been shown to decouple with age⁶⁵ and Alzheimer's disease⁶⁶ and regional differences.

Decreased sleep efficiency is a marker of poor sleep quality and is associated with worse cognitive function.^{35,36} Higher sleep efficiency is consistent with higher sleep quality. The estimated marginal effect of sleep efficiency on longitudinal PACC scores was minimal and suggested that sleep efficiency <65% was associated with minimally decreased cognitive performance. These are minor

effects compared to total sleep time and NREM SWA. Longitudinal PACC scores and sleep efficiency were not significantly associated in the linear model.

Our cohort is richly characterized for genetic risk factors and biomarkers for Alzheimer's disease that were not available for previous studies and thus allow us to compare the effect of total sleep time, sleep efficiency, time in NREM stage 2 and 3, time in REM, <1 Hz and 1–4.5 Hz NREM SWA on cognitive performance relative to other factors such as CDR or CSF t-tau/amyloid- β_{42} . These results suggest that a certain range of total sleep time and <1 Hz NREM SWA are important for maintaining cognitive function. Participant cognitive performance on the PACC decreased outside of this middle or optimal range. The clinical significance of this cognitive change is unclear. A recent paper compared PACC performance in amyloid-negative and amyloid-positive cognitively normal participants enrolled in three large Alzheimer's disease cohort studies.⁶⁷ Based on the separation between cognitively unimpaired individuals and early mild cognitive impairment, the authors concluded that 1 SD on the PACC (i.e. one point of additional decline in amyloid-positive participants compared to amyloid-negative participants) could be taken as an approximate benchmark for clinically meaningful decline for interventional trials involving preclinical or presymptomatic Alzheimer's disease (e.g. cognitively normal amyloid-positive). Given that our cohort is 88% cognitively unimpaired and there are known practice effects with the PACC,⁶⁸ a marginal effect of sleep on PACC performance ranging from –0.2 to –0.3 is clinically significant; further, this estimated marginal effect is comparable to age in our models, the greatest risk factor for Alzheimer's disease. The effect of sleep efficiency is small, however, and is likely not clinically significant. An exciting possibility from this study is that diagnosing and treating sleep disturbances, such as sleep apnoea or insomnia, to optimize sleep duration and NREM SWA may have a stabilizing effect on cognition in preclinical or early symptomatic Alzheimer's disease.

However, many unanswered questions remain. We need to understand if there are differences in the optimal characteristics of sleep needed to preserve cognitive function and the optimal characteristics of sleep needed to prevent Alzheimer's disease pathology, and if these relationships change with stage of Alzheimer's disease. Also, colinear or linked factors may affect both sleep and cognitive decline. We have already discussed that sleep changes with age and sex, but this is likely an issue with other Alzheimer's disease risk factors. For example, APOE $\epsilon 4$ has been associated with increased duration of NREM stage 3 sleep in cognitively normal older adults.⁶⁹ Yet, APOE $\epsilon 4$ is also associated with increased risk of amyloid pathology that is associated with decreased sleep efficiency.³¹ A major limitation of this study is that cognitive assessments were longitudinal and preceded the cross-sectional sleep monitoring in 22% of participants. Both interventional studies and observational studies with longitudinal sleep and cognitive assessments are needed to see how the trajectories of different sleep parameters, especially total sleep time and <1 Hz NREM SWA, are related to the trajectory of cognitive performance.

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Competing interests

B.P.L. consults for Merck and Eli Lilly; J.W. is currently employed at Bayer; J.C.M. is funded by NIH grants P30 AG066444; P01AG003991; P01AG026276 and U19 AG032438. Neither J.C.M. nor his family owns stock or has equity interest (outside of mutual funds or other externally directed accounts) in any pharmaceutical or biotechnology company. D.M.H. co-founded and is on the scientific advisory board of C2N Diagnostics. D.M.H. consults for Genentech, Idoria, Merck and Denali. Washington University receives research grants to the laboratory of D.M.H. from C2N Diagnostics and NextCure. J.H. is an advisory board member for Roche, Lundbeck and Takeda. A.H.B., E.C.L., C.D.T., J.S.M., O.H.B. and B.M.A. declare that they have no competing interests.

Supplementary material

Supplementary material is available at *Brain* online.

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