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Stepping Forward in Antibody-drug Conjugate Development

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Abstract

Antibody-drug conjugates (ADCs) are cancer therapeutic agents comprised of an antibody, a linker and a small-molecule payload. ADCs use the specificity of the antibody to target the toxic payload to tumor cells. After intravenous administration, ADCs enter circulation, distribute to tumor tissues and bind to the tumor surface antigen. The antigen then undergoes endocytosis to internalize the ADC into tumor cells, where it is transported to lysosomes to release the payload. The released toxic payloads can induce apoptosis through DNA damage or microtubule inhibition and can kill surrounding cancer cells through the bystander effect. The first ADC drug was approved by the United States Food and Drug Administration (FDA) in 2000, but the following decade saw no new approved ADC drugs. From 2011 to 2018, four ADC drugs were approved while in 2019 and 2020 five more ADCs entered the market. This demonstrates an increasing trend for the clinical development of ADCs. This review summarizes the recent clinical research, with a specific focus on how the in vivo processing of ADCs influences their design. We aim to provide comprehensive information about current ADCs to facilitate future development.

Keywords

antibody-drug conjugates (ADCs); cancer therapy; clinical research; metabolism

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Recommended readings: For additional background information on ADCs and their metabolism, the following publications are highly recommended: Chen S. Q. & Zhan J. B. (2019). Antibody-drug conjugates and cellular metabolic dynamics. Hangzhou, Zhejiang University Press. (ISBN: 9787308197281) and Ducry L. (2013). Antibody-Drug Conjugates. New Jersey, Humana Press. (ISBN: 9781627035415).

1. Introduction

As early as the mid-20th century, doctors and scientists began to use cytotoxic chemicals to treat patients with advanced cancers (Miller et al., 2010). One of the earliest trials was to apply nitrogen mustard to treat patients with non-Hodgkin's lymphoma (Conrad & Crosby, 1960). After treatment with nitrogen mustard, tumor regression occurred. Even though regression was short and incomplete, it encouraged researchers in this field at that time. In the following decades, alkylating agents (e.g. cyclophosphamide and cisplatin) and anti-metabolites (e.g. methotrexate and fluorouracil) were developed and utilized as cancer treatments (DeVita & Chu, 2008). In the late 20th century, the emergence of monoclonal antibodies (mAb) made it possible to develop more targeted anti-cancer drugs (Liu, 2014; Slamon, et al., 2001). In parallel, a growing number of tumor markers and tumor surface antigens were found and identified, providing targets for antibody therapy (Walts & Said, 1983). When combined to form antibody-drug conjugates (ADCs), the toxic compounds (payloads) provide the tumor cell killing effect, while antibodies provide targeted distribution (Latif et al., 1980).

After decades of time and effort, the first ADC drug, Mylotarg, was approved by the United States Food and Drug Administration (FDA) in 2000 (Norsworthy et al., 2018). It is used to treat patients with relapsed cluster of differentiation (CD) 33 positive acute myeloid leukemia (Zaro, 2015). Although Mylotarg was delisted in the United States for a period of time due to toxicity concerns, it is a milestone of ADC drug development and sets a precedent for ADC-based cancer therapy. In the following ten years, no new ADCs reached clinical approval. After 2011, several new ADC drugs were launched in quick succession. In 2011, Adcetris, targeting CD30, was approved for the treatment of Hodgkin's lymphoma (Leal et al., 2015). In 2013, ado-trastuzumab emtansine (T-DM1) targeting human epidermal growth factor receptor 2 (HER2) was approved for the treatment of HER2-positive breast cancer (Reichert, 2014). In 2017 and 2018, Besponsa and Lumoxiti, respectively, which target CD22, were approved for use in the treatment of acute lymphoblastic leukemia (Kaplon & Reichert, 2018). By 2019, ADC development was on the rise evidenced by the approval of three ADC drugs within the year. Polivy, Padcev and Enhertu were approved by the FDA for treatment of B-cell lymphoma, urothelial tumor and HER2-positive breast cancer, respectively (Kaplon et al., 2020). In the past year, two more new ADC drugs gained approval, Trodelvy for triple-negative breast cancer and Blenrep for relapsed and refractory multiple myeloma (as shown in Table 1 and Figure 1).

At the same time, pharmaceutical companies have made great efforts to overcome technical barriers related to ADCs, including plasma stability, payload dissociation, low blood retention time, minimal tumor penetration, decreased payload efficiency, immunogenicity, off-target toxicity, and drug resistance (Sassoon & Blanc, 2013). In the decade from 2010–2019, more than 60,000 research papers on ADCs were published, while only a few drugs entered the market. Behind the newly launched ADC drugs are a large number of clinical studies on ADCs that have been terminated due to safety or efficacy concerns (Tolcher, 2016). A better understanding of ADCs and their small molecule payloads would improve the likelihood of clinical success. Therefore, this review examines the mechanisms of ADC drugs according to their intended route of in vivo processing. It summarizes several clinical

studies on ADCs over recent years according to different targeted tumor types in order to provide a framework for pre-clinical development of ADCs.

2. The structure of ADCs

An ADC is a complex formed by covalently coupling a small molecule drug (payload) with a monoclonal antibody through a linker. These three parts jointly define the overall physical and chemical properties, efficacy and possible problems of ADC drugs. The typical ADC design is shown in Figure 2.

2.1. Antibodies

Antibodies (Abs) are glycoproteins produced by plasma cells that can specifically bind to a corresponding antigen and generally consist of a variable antigen binding domain (Fab) and a constant domain (Fc) that binds immune cell receptors (Buss et al., 2012). The term immunoglobulins (Ig) refers more generally to Abs and all globulin proteins that have structural similarities to antibodies (Cushley & Owen, 1983). Antibodies can be divided into five categories: IgG, IgA, IgD, IgE and IgM (Kuroda et al., 2010). Among the five types, IgM is a pentamer and although it has high affinity, its molecular weight is too large and penetrability is poor (Shimizu et al., 2004). IgA has a dimer structure and a large molecular weight. IgD is sensitive to protease and is easy to degrade, so its half-life is short. IgE is very rare, only accounting for 0.002% of the total immunoglobulin in human serum. However, IgG can account for 75% ~ 85% of total immunoglobulin in human serum and has a molecular weight of about 150 kilodalton (kDa) (Smith, 1974). Because of its moderate molecular weight, high affinity, long half-life, strong penetrability and easy preparation, IgG has been the first choice in selection of ADC antibodies (Ritchie et al., 2015). There are four subtypes of IgG: IgG1, IgG2, IgG3 and IgG4. IgG1 is easy to prepare and has an intracellularly degradable hinge structure, therefore most ADCs are constructed with an IgG1 scaffold (Rees, 2015). IgG2 and IgG4 have weakly active Fc portions, so their ability to initiate antibody-dependent cellular cytotoxicity and complement-dependent cytotoxicity is weak (Steplewski et al., 1988; Armour et al., 1999), therefore IgG2 and IgG4-based ADCs can reduce side effects of non-target tissue aggregation caused by Fc segments (Aalberse et al., 2010). Some ADCs lacking Fc function have been FDA approved (e.g. Mylotarg and Besponsa) (Sau et al., 2017). Cytotoxic drugs are usually connected to the Fc or constant region, but not to the Fab region to avoid a negative impact on antigen detection and binding (as shown in Figure 2).

As navigation systems for ADC tumor distribution, antibodies used in ADCs need to have weak immunogenicity, high target specificity, high binding affinity, long half-life and good stability in blood circulation (Nejadmoghaddam, et al., 2019). The immunogenicity of antibodies and ADCs is one determinant of their circulation half-life (Hock et al., 2015). Early antibody therapies and ADC studies used mouse mAbs, which could induce a strong, acute immune response (Kuus-Reichel et al., 1994), while at present most ADCs use partially humanized or fully humanized antibodies (Lonberg, 2008). High specificity helps concentrate the cytotoxic agents on tumor sites, so as to achieve a targeted pharmacological effect. ADCs with low specificity are more likely to cause toxicity to normal tissues

(Nejadmoghaddam et al., 2019). ADC antibodies should have high binding affinity and most ADCs have binding affinities in the range of 0.1 to 1.0 nM, also described as the equilibrium dissociation constant or K_d value, but few published data have solved the optimal binding affinity of ADCs. One theory on binding affinity (the binding site barrier theory) explains that the higher the antibody affinity and the higher the antigen density, the more of that antibody binds to the solid tumor surface rather than penetrates to the interior of the tumor tissue (Juweid, et al., 1992). One recent study prepared three ADCs that had different target binding affinities and found almost the same in vitro cytotoxicity among the three ADCs. The three ADCs had equivalent antitumor effects against small BxPC3 tumors. However, for large BxPC3 tumors, the high affinity ADC showed stronger anti-tumor activity relative to the low affinity ADC. In addition, immunofluorescence staining indicated that the high affinity ADC distributed throughout the whole tumor, whereas the low affinity ADC mainly localized close to tumor vessels, suggesting distribution and anti-tumor activity may depend on binding affinity (Tsumura et al., 2018). Kang et al. prepared an ‘acid-switched’ ADC targeting HER2. It had higher affinity at near neutral pH (in plasma and the extracellular microenvironment), but lower affinity at acidic pH (in endosome or lysosome), which allowed more cellular payload release. The antibody showed 250-fold weaker affinity intracellularly compared to outside cells. In xenograft tumor models, compared with T-MD1, the engineered ADC showed increased lysosomal delivery and higher therapeutic efficacy (Kang et al., 2019). In addition, for the same tumor surface antigen, antibodies of ADCs bound to different epitopes have different internalization rates (Rohrer, 2017). Fast internalization can improve efficiency of ADCs. Compared with small molecules, antibodies enter into tissues from plasma more slowly (Schlom et al., 1990). The use of antibodies as a targeting mechanism in ADCs demonstrates substantial benefit for localized delivery of cytotoxic agents.

2.2. Payloads

Payloads, also known as “cytotoxic molecules” or “warheads”, are important factors affecting the properties and activities of ADCs (Damelin, 2018). The mechanisms of cytotoxic molecules determine efficacy and adverse reactions of ADCs. At present, the commonly used cytotoxic molecules are nearly all natural-product based including microtubule inhibitors (such as auristatin, maytansinoids), DNA damaging agents (such as calicheamicin, duocarmycins, anthracyclines, pyrrolbenzodiazepine dimers) and DNA transcription inhibitors (amatotoxin and quinoline alkaloid (SN-38)) (Yaghoubi et al., 2020; Theocharopoulos et al., 2020; Chen et al., 2017a; Gromek & Balunas, 2015). Among nine of the ten approved ADC drugs, six different small molecule payloads are used (shown in Table 1, Figure 1 and Figure 3). Three ADCs deliver monomethyl auristatin E (MMAE), two drugs deliver calicheamicin, and monomethyl auristatin F (MMAF), mertansine (DM1), SN-38 and DXd are also successfully applied. The toxins or toxin skeletons suitable as ADCs payloads (Chen et al., 2017a; Gromek & Balunas, 2015) must have the complex characteristics described in the following paragraphs.

Ultra-high toxicity—The intrinsic potency of a payload must be very high, because the accumulation of payloads in target cells is limited due to the low permeability of mAbs into tumor tissue, limited expression of tumor cell antigens, low cellular internalization and

metabolic decomposition of ADCs in blood circulation (Ducry, 2013). Current payloads can kill tumor cells at sub-nM concentrations (Diamantis & Banerji, 2016). ADC payloads generally act on a small number of cell targets involved in basic cell survival processes, which ensures high cytotoxicity in genetically heterogeneous tumor tissues and prevent cancer cells from escaping through a drug resistance mechanism (Anderl et al., 2013).

Intracellular toxic targets—The target of a typical ADC payload is located within the cell and most ADCs need to enter tumor cells to release their payloads (Chen et al., 2017a). Many highly toxic agents from plants, animals and microorganisms are membrane targeted, blocking ion channels on neurons or causing coagulation disorders. Such toxins are not suitable for use as ADC payloads. At present, intracellular targets for ADCs are focused on nucleic acids or tubulin protein (Yaghoubi et al., 2020).

Payload characteristics—The molecular weight of payloads should be relatively small, so as to reduce the risk of an immunogenic reaction (Birrer et al., 2019). In addition, payloads should have appropriate solubility in a water-based buffer to facilitate antibody coupling. Payloads should contain a functional group suitable for coupling with an antibody through linkers in its structure (Birrer et al., 2019). The payload should also be stable in the low pH environment of the lysosomes. When non-cleavable linkers are used, the toxins should retain their cytotoxicity when degraded into linker residue-payload form, such as thiol derivative forms after breakage of disulfide bonds in tumor cells (Ponziani et al., 2020).

2.3. Linker

The third important component of ADCs is the linker, which functions as a connection between the antibody and payload. The linker needs to be stable in blood to keep the cytotoxic payload attached to the antibody, but once the ADC enters the tumor cell or is transported to lysosomes, the linker should quickly break down to release the payload (Filntisi et al., 2014). The linker impacts many important properties of ADCs, such as drug-to-antibody ratio or DAR value (the number of payloads attached to one antibody), payload release time, therapeutic index (TI) and pharmacokinetics/pharmacodynamics. The stability of the linker in blood is very important. Linkers with limited stability are prone to cause nonspecific cleavage, which leads to wider drug release and off-target toxicity (Excoffier et al., 2016). The stability of linkers used in initial ADCs was limited and the subsequent rapid release of payload led to poor therapeutic indices and side effects that were similar to non-conjugated chemotherapy (Excoffier et al., 2016). After application of new linkers, this situation has improved. Commonly used linkers include the valine-citrulline (VC) linker, N-succinimidyl 4-(2-pyridyldithio)butanoate (SPDB) linker, hydrazone linker, succinimidyl 4-(N-maleimidomethyl)cyclohexane-1-carboxylate (SMCC) linker, maleimidocaproyl (MC) linker, N-succinimidyl-4-(2-pyridyldithio)pentanoate (SPP) linker, thioether linker, tetrapeptide linker and carbonate linker (Tsuchikama & An, 2016; Yao et al., 2016) (Table 1, Figure 2 and Figure 4).

Drug-to-antibody ratio (DAR)—The drug-to-antibody ratio describes the average number of drug molecules conjugated to the antibodies. In general, interchain disulfide bridges and surface-exposed lysine and cysteine residues are the most commonly used

linker modification sites on antibodies (Dimasi et al., 2017). The hydroxyl on glycosylation groups and other residues on antibodies are rarely used as conjugation sites (Nolting, 2013). Most of the clinical ADCs adopt hetero-coupling technology and carefully control average modification to achieve a DAR value in range of 2 to 8, which often results in mixtures of ADCs with different DAR values (Su et al., 2018; Yao et al., 2016). At present, a number of site-specific linker methods (homologous conjunction technologies) are under investigation to control DAR value and prepare better stability and low aggregation ADCs (Panowski et al., 2014; Tsuchikama & An, 2016).

Based on the cleavage properties of linkers within tumor cells, linkers can be divided into two types: cleavable and non-cleavable (stable) (Tsuchikama & An, 2016). ADCs with cleavable linkers can release payloads quickly in tumor cells through linker cleavage, while ADCs with stable linkers release payloads only after entering the lysosomes of tumor cells where the antibody is fully degraded by proteases (Dan et al., 2018). Cleavable linkers have higher metabolism in circulation, which can contribute to off-target toxicity (Tumey & Han, 2017). The metabolites produced by the two linker types are also different. ADCs with cleavable linkers can release intact cytotoxic molecules, while ADCs with stable linkers release payloads that are linked to amino acids (Bargh et al., 2019). Generally, ADCs with stable linkers have longer half-lives and lower clearance rates than those with cleavable linkers (Tumey & Han, 2017). In addition, ADCs with cleavable linkers can release their payload even if the internalization process is not smooth (Bargh et al., 2019).

Cleavable linkers—Cleavable linkers can be cleaved by a number of mechanisms, including hydrolysis of acid labile bonds, enzymatic cleavage of amide or ester bonds, or reductive cleavage of disulfide bonds (Mueller et al., 1990). These mechanisms may operate in primary and late endosomes of tumor cells, and there are no strict requirements for lysosomes (Klussman et al., 2004). Cleavable linkers are sensitive to the intracellular environment. For example, acid cleavable linkers are usually stable in blood, but rapidly cleaved in the low pH lysosomal environment (such as Besponsa and Mylotarg). Disulfide linkers release payloads through intracellular glutathione (GSH) reduction reactions (Mueller et al., 1990). If the released payloads can cross tumor cell membranes, they can kill nearby cancer cells- this is referred to as the bystander effect (Bargh et al., 2019; Kovtun et al., 2006). For example, the cleavable ADC DS-8201a releases its membrane permeable payload DXd, which kills HER2-positive cells surrounding the targeted cancer cells, but not more distant cells. This is beneficial for treatment of HER2 heterogeneous tumors (Ogitani et al., 2016). However, cleavable linkers do not always enable the bystander effect, rather it depends on membrane-penetrability and charge properties of the released payload (Chari et al., 2014). The bystander effect is advantageous for tackling heterogeneous tumors and for penetrating deeper into solid tumors which are less accessible to the conjugate. At the same time there are disadvantages such as killing normal cells or immune cells nearby the intended target tumor cells (Chari et al., 2014).

Non-cleavable linkers—Non-cleavable linkers are composed of structures that have enzyme-resistant properties and are stable in blood (Filntisi et al., 2014). Representing non-cleavable linkers are thioether and MC linkers (Dorywalska et al., 2015). Their payloads

can be released only after the ADCs are transported to lysosomes and broken down into amino acids (Lu et al., 2016). The advantages of stable linkers include minimal payload release outside of cells, thus reducing off-target toxicity and improving therapeutic index, but the disadvantages include lower release efficiency and the need for a good internalization process (McCombs & Owen, 2015; Gianolio et al., 2012). In addition, stable linkers do not achieve bystander effects because the metabolized payload form (lysine or cysteine residue-linker-payload form) possesses a charge, restricting its diffusion (Bargh et al., 2019).

3. Mechanism and in vivo processing to activate ADCs

3.1. First step - ADCs enter blood through IV injection and distribute to tissues

3.1.1. Tissue distribution of ADCs—ADCs are usually administered by intravenous (IV) injection to ensure rapid whole body distribution and avoid degradation (Dan et al., 2018). After injection, ADCs are initially distributed to organs with rich blood flow (Xu, 2015) (shown in Figure 5, step 1). Barrier systems of some organs and tissues, such as the blood-testis barrier and blood-brain barrier reduce tissue entry of ADCs (Pardridge, 2015). With time, ADCs gradually enter interstitial space of organs and tissues which decreases blood concentration and increases distribution volume (Boswell et al., 2011). During the process, the ADC reaches the tumor epitope and the antibody portion binds the target antigen (Schneider et al., 2017).

The distribution characteristics of ADCs are mainly determined by the antibody, which accounts for more than 95% of the whole ADC molecular weight (Chen & Zhan, 2019). ADCs show similar PK characteristics as antibodies, such as low clearance rate, long half-life, low volume of distribution, poor oral bioavailability, nonlinear distribution and elimination, and immunogenicity (Chen & Zhan, 2019). The molecular weight of IgG is about 150 kDa and its radius is about 15 nm (Bournazos & Ravetch, 2017). The half-lives of antibodies such as IgG can reach 21 days boosted by neonatal Fc receptor (FcRn) mediated IgG recycling (Pernille et al., 2017; Roopenian & Akilesh, 2007). The Fc segment of IgG can specifically bind FcRn of the major histocompatibility complex family to form an IgG-FcRn complex, which can be internalized into cells with high binding affinity under the acidic conditions of endosomes (Wang et al., 2014; Gurbaxani et al., 2013). Then the IgG-FcRn complex can be recycled back to the cell membrane surface and exposed to low alkaline pH, which decreases the affinity of the complex and releases the antibody into circulation (Maas & Cao, 2018). In this way, the half-life of IgG is significantly prolonged. In addition, when an ADC, as a biological macromolecule, enters the human body, it may stimulate humoral immunity and cause an anti-ADC immune response, thus accelerating the inactivation or elimination of the ADC and preventing its tissue distribution (Waldmann, 2019; Petkova et al., 2006).

The kinetics of ADCs in circulation are also affected by payloads and linkers, altering charge distribution and hydrophilicity of the antibody, thus changing the aggregation and sedimentation characteristics of the antibody in circulation (Kamath & Iyer, 2015). Due to the difference in the DAR and the payload distribution heterogeneity, ADCs show structure diversity, resulting in heterogeneous dissociation, which is different from simple antibody

drugs. The actual DAR values of ADCs generally fluctuate in the range of 0 to 8 (the average value is generally 3 to 5), making PK studies more difficult (Tang et al., 2019).

3.1.2. Assessment of ADC in tissue distribution—Since an ADC is composed of an antibody, a linker and a payload, the three parts need to be considered as a whole to study absorption and distribution. At the same time, because ADCs may degrade in vivo, distribution and metabolism analysis of the three parts individually is also important, which can be used to examine the consequences of potential degradation of an ADC before it reaches its target (Kamath & Iyer, 2015).

Radioisotope labeling is a common method applied to study ADC distribution (Pimm et al., 1987). Radioisotopes, such as ^3H , ^{131}I and ^{89}Zr , can be used to label antibodies and small molecule drugs at the same time or separately (Pimm et al., 1987). After IV administration, the distribution of whole ADCs or individual antibodies and payloads after release can be monitored in real time (Terwisscha et al., 2017). In blood or tumor tissue, antibodies and drug molecules labeled with different radioisotopes can be counted to determine the distribution and cleavage of ADCs. Simultaneously, an isotope-labeled ADC can be compared to an isotope-labeled antibody to study distribution differences caused by addition of the payload. Liquid scintillation counting of blood samples can be used to analyze drug distribution parameters after administration (Fand et al., 1986; Schmidt et al., 2002). In recent years, whole body quantitative autoradiography has also been applied to study distribution of ADCs (McEwen & Henson, 2015).

Before binding to the tumor surface antigen, linker cleavage and ADC metabolism could happen within circulation. This is one of the focal points in ADC development and clinical research. DAR variation impacts decomposition of ADCs (Roberts et al., 2013) as it determines drug loading and reflects safety and effectiveness of ADCs. For ADCs in blood circulation, DAR analysis mainly examines molar concentration changes in the ratio of total drug molecules and antibody molecules in ADCs with respect to administration time. The main analytical method is liquid chromatography-mass spectrometry (LC-MS), which has high sensitivity, resolution and accuracy (Mou et al., 2018). Moreover, the absolute molecular weight of ADC molecules with varying DAR values is different, so the DAR can be analyzed by electrospray ionization or matrix assisted laser desorption MS. The ADCs with different DAR values can be identified by individual mass charge ratio peaks on the mass spectrum, and then the relative contents (i.e. the distribution of DAR) can be obtained according to calculation of peak areas (Chen et al., 2016). The latest high-resolution mass analyzers, such as time of flight mass and orbital ion trap analyzer (orbitrap), combined with deconvolution calculation of intelligent software, make MS analysis of ADCs more convenient and accurate (Beck et al., 2019; Chen et al., 2016; Lanshoeft et al., 2016).

3.1.3 Problems of ADC tissue distribution and strategies for improvement—The biological distribution of ADCs enables their therapeutic effects (Lambert & Berkenblit, 2018). Very early clinical dosimetric studies of patients with radiolabeled antibodies showed that only ~0.1% of the antibody dose could be located in solid tumor mass 24 hours after infusion, regardless of tumor type or antibody target (Mach et al., 1980; Sedlacek et al., 1992). On the bright side, antibodies including ADCs as a high molecular weight

agent can extravasate from leaky tumor vessels and sinusoidal vessels in the liver, bone marrow, or lymphoid organs, but not from other normal vessels, known as the enhanced permeability and retention (EPR) effect (Yasunaga, 2020). The EPR effect or enhanced vascular permeability can sustain an adequate supply of nutrients and oxygen for rapid tumor growth, which also provides accumulations of both endogenous and exogenous proteins larger than 60 kDa, benefiting macromolecule-based solid tumor therapy (Maeda et al., 2000). However, characteristics such as increased hydrostatic pressure and blockage of tumor lymphatic channels and blood vessels are reported to obstruct ADCs outside tumor tissues (Dahlgren & Lennernäs, 2020). Different from direct binding with hematological tumors, four steps occur for ADCs to bind solid tumors: reaching tumor blood vessels, exuding the blood vessel, distributing to tumor tissue and binding with the tumor target (Thurber et al., 2008). The best drug effect with limited cytotoxic molecules depends on tumor uptake of the ADC, tumor vascular density, membrane permeability and other rate limiting steps (Sapra et al., 2011). In addition, the affinity between the ADC and FcRn, the charge and physiochemical properties of the ADC, and the internalization of target will affect the distribution of ADCs (Maas & Cao, 2018).

In circulation, the toxicity and/or side effects caused by early payload release or ADC binding to normal tissue are problems that cannot be ignored (Bander, 2013). Non-target tissues and organs can capture ADCs, especially in tissues with large blood flow and strong phagocytic function (such as intestine and liver) (Maas & Cao, 2018). For example, liver cells phagocytize a number of ADC molecules and their rich metabolic enzymes decompose these ADCs where the released payloads then experience first and second phase metabolism resulting in drug inactivation (Tumey et al., 2015; Bumbaca et al., 2011).

Dispersion of ADCs in target-expressing normal cells can also lead to side effects or treatment failure (Bander, 2013). For example, treatment with epidermal growth factor receptor (EGFR)-targeted ADC (depatuxizumab mafodotin) for recurrent glioblastoma caused side effects including corneal abnormalities (Goss et al., 2018). When HER2-targeted ADC (trastuzumab emtansine (T-DM1)) was used for treatment of HER2-positive breast cancer the side effects of nodular regenerative hyperplasia and corneal abnormalities were observed (Lepelley et al., 2018; Tsuda et al., 2016). A folate receptor α -targeted ADC (mirvetuximab soravtansine) also showed corneal abnormalities following treatment of platinum-resistant ovarian cancer patients (Lepelley et al., 2018; Tsuda et al., 2016). Treating non-Hodgkin's lymphoma patients with CD79b-targeted ADC (polatuzumab vedotin) resulted in 70% of patients showing peripheral neuropathy (Lu et al., 2017).

Additionally, off-target toxicity based on the Fc domain has been reported. An ADC antibody that lacked terminal galactose caused receptor mediated endocytosis by the mannose receptor (Gorovits & Krinos-Fiorotti, 2013). The mannose receptor is a lectin that specifically binds and internalizes antibodies with specific agalactosylated Fc-segments which has been found on the surface of endothelial cells and immune cells in hepatic and splenic sinusoids.

3.2. Second step - ADCs bind to target antigens on tumor cell surfaces

3.2.1. Interactions of ADCs with tumor surface antigens—After sufficient time in blood circulation, ADCs can spread throughout the body and reach tumor tissue (Nejadmoghaddam et al., 2019). An ADC that reaches tumor tissue can bind to its target antigen on the surface of tumor cells using the antigen-binding site of the antibody (shown in Figure 5, step 2). The target antigen-ADC complex can then undergo receptor-mediated endocytosis, which will transfer the ADC into tumor cells for subsequent transport and processing (Ritchie et al., 2013). Typically, target tumor cells should have moderate antigen expression level on the cell surface (10^5 /cell) (Chari et al., 2014),

Selection of tumor target proteins is a good starting point for ADC design. It determines the type of tumor that the ADC will target, and can predict problems that may be encountered in clinical trials (Bander, 2013). In recent years, many targets have been evaluated in the development process of ADCs (De Stefano et al., 2018). Most of these targets are tumor surface antigens (Ishii, 1995). Tumor surface antigens can be divided into two types, tumor associated antigens (TAA) and tumor specific antigens (TSA) (Butterfield, 2015; Trail et al., 2003). Among them, TAAs are proteins with high expression in tumor cells, but low expression in normal cells (Li et al., 2010). TAAs are often growth factor receptors, carcinoembryonic antigens or leukocyte differentiation antigens, which can be used in clinical diagnosis and classification of tumors (Li et al., 2010). For example, HER2 is a growth factor receptor expressed on the cell membrane (Nemeth et al., 2017) with high expression in breast cancer, gastric cancer and other cancer cells. At present, the ADCs targeting HER2 are Fam-trastuzumab deruxtecan (Enhertu) and Ado trastuzumab emtansine (Kadcyla) (Meric-Bernstam et al., 2019). Alternatively, CD30 is a leukocyte differentiation antigen which is widely overexpressed on the surface of various types of Hodgkin's lymphoma cells (Pierce & Mehta, 2017). Brentuximab vedotin (Adcetris) targets CD30 and is used to treat lymphoma (Pierce & Mehta, 2017).

TSAs only exist on the surface of tumor cells, but not normal cells, so they can be used as markers to distinguish tumor tissue from normal cells. TSAs are unique antigens and generated by mutations. The external environment of physical factors such as radiation, chemical factors such as carcinogens, and biological factors such as viruses can also induce the production of TSAs (Rammensee et al., 2002). When cells expressing TSAs die or tumor tissue expressing TSAs undergo necrosis, the TSAs will be released into the blood, which can be detected and identified (Stauss, 2003). TSAs have the potential to be used as an antibody target to develop corresponding ADC drugs. At present, most targets of ADCs in clinical trials are TAAs, but many ADCs targeting TSAs are undergoing clinical or preclinical studies (Chen & Zhan, 2019). Therefore, ADCs targeting TSAs may be approved in the future, which have potential to reduce the off-target side effects caused by ADCs.

3.2.2. Research on tumor marker detection—For clinical use of ADC drugs, patient stratification is very important (Goutsouliak et al., 2020). Some cancer patients can express tumor antigens corresponding to ADC targets, while some patients do not. For the latter group, other treatment schemes are necessary. For example, Trastuzumab-DM1 is approved for treatment of breast cancer patients. The target is HER2, but ~75% of breast

cancer patients are HER2 negative (Nemeth et al., 2017). Detection of tumor markers in patients is particularly important. Tumor markers are substances produced by tumor cells and related to the formation and occurrence of tumors (Hong et al., 2018). These substances originally exist in the nucleus, cytoplasm, membrane, or cell fluid of tumor cells. With tumor development, expression of the markers is elevated.

Radioimmunoassay and enzyme-linked immunosorbent assay (ELISA) are traditional identification methods of tumor markers (Marsigliante et al., 1993). At present, automatic immunochemical analysis instruments are commonly used detectors, which can rapidly and accurately measure serum tumor markers (Bi et al., 2009). The detection mechanism is based on the antigen-antibody interaction. Generally, luciferase-labeled antibodies specifically bind tumor markers and emit light following addition of a luminescent agent (Webster et al., 1990). In detection of the chemical reactions, some chemical groups are oxidized to form excited states and emit photons of a certain wavelength while returning to the ground state. This is a highly sensitive analytical method combining chemical reaction with immune response, also known as photomultiplier technique (Min et al., 2018). An automated instrument makes the experimental process very simple; obtained blood samples can be directly added to the chemiluminescent immunoassay system for detection and subsequent output to analyze results (Bi et al., 2009).

The above detection methods are serological detection methods, which are generally used in preliminary identification (Holdenrieder, 2016). The detection of tumor markers in tumor tissue is more important for ADC treatment selection. Histological detection of tumor markers can show the quantity, distribution and uniformity of tumor marker expression in tumor tissues (Shi et al., 1991). In addition, the study of tumor antigen regulatory factors, such as tumor marker renewal rate and heterogeneity, are important elements for consideration (Bander, 2013).

3.2.3. Problems and strategies for ADC target selection

Specificity and expression level: Target specificity and expression level are the core of target selection in ADC design. High specificity means one antigen is highly expressed on tumor cells with corresponding low or non-existent expression on normal cells. An antigen with a high expression level means this antigen is present in much larger numbers on the tumor cell surface or tumor tissue when compared to expression levels of the same antigen on either normal cells or other tumor cell types (Bander, 2013). High specificity and high expression level of the antigen can increase ADC recruitment to tumor tissues and decrease delivery to normal tissues.. Most of the selected targets are those with high specificity and high expression levels in tumors and their metastases (Wang et al., 2011). Although uncommon, if a tumor antigen that is also expressed in normal tissue is selected as the target, the expression in normal tissue should be limited to a small region or the normal tissue should have regenerative ability to minimize toxicity of the ADC towards the healthy tissue (Ducry, 2013).

Internalization: Most current payloads have intracellular targets, thus internalization is particularly important for cytotoxic activity (Bander, 2013). As internalization is determined

by the properties of the target antigen, target internalization should be understood before ADC preparation. Moreover, successful recycling or replenishment of cell surface antigen is also essential (Collins et al., 2019). A cell surface antigen that can be quickly replenished can accumulate more ADC into the cell, thus improving payload delivery and the possibility of tumor cell death (Ducry, 2013). However, antigens that are quickly replenished can also deplete ADCs from the tumor tissue surface and prevent interior tumor penetration.

Heterogeneity: Heterogeneity of targets can be found between tumor cells or between patients. With respect to breast cancer, HER2 positive breast cancer patients can benefit from HER2 targeted ADCs, but the remaining patients would not benefit from them. The heterogeneity within tumor cells means that for instance not all tumor cells in a given HER2 positive breast cancer patient express HER2 (Ducry, 2013). The larger the proportion of target-negative cells, the weaker the therapeutic effect of ADCs (Ducry, 2013). Accordingly, for tumor heterogeneity, combination treatment with two or more ADCs may be efficacious and worth investigating (Hamilton, 2015).

Tumor stroma as target: At present, most ADCs are designed to target tumor surface antigens, which is endocytosis dependent. However, ADCs targeting tumor matrix (which is endocytosis independent) are getting increasing attention (Joubert et al., 2017). Cancer-related microenvironments from different cancer types can share many common features, so this approach may eventually extend applications of ADC therapy beyond strict selection of antigen positive patients (Ahmed et al., 2008). Moreover, most solid tumors have abundant stroma that hinders the distribution of high molecular weight agents, which functions as a barrier that prevents ADCs from attacking cancer cells (Yasunaga et al., 2011). Stromal targeted ADCs can release payload after binding to tumor stromal cells through mechanisms like extracellular plasmin or other proteolytic cleavage (Matsumura, 2020; Gébleux et al., 2017). The released small molecule payload can readily enter into and kill cancer cells across the stromal obstacle.

3.3. Third step – ADCs enter tumor cells through receptor-mediated endocytosis

3.3.1. Endocytosis pathways of ADCs—After circulation in the blood, ADCs reach tumor tissues and bind to target antigens on the surface of tumor cells (Damelin, 2018). Upon forming an antigen-antibody complex, the complex will undergo receptor-mediated endocytosis to transport the ADC to lysosomes for payload release (Kalim et al., 2017) (shown in Figure 5, step 3). According to the mechanism of action, endocytosis of ADCs can be divided into four types: clathrin-mediated endocytosis, cell membrane cave-like invagination also known as caveolae-mediated endocytosis, macropinocytosis, and clathrin- and caveolin-independent endocytosis (Kalim et al., 2017). Usually, ADCs enter cells through the clathrin-mediated endocytosis pathway (Chalouni & Doll, 2018).

Clathrin-mediated endocytosis: The clathrin-mediated endocytosis pathway is the most important receptor-dependent endocytosis pathway for biomacromolecule internalization (Swan, 2013). The clathrin pathway exists in mammalian cells to intake nutrients, regulate cell surface receptor levels, and transmit cell-cell signaling (Kalim et al., 2017). There are four steps in clathrin-mediated endocytosis: assembly of clathrin coats, membrane

invagination and coated pit maturation, constriction of pit and fission of vesicle, and uncoating of vesicles (Kaksonen & Roux, 2018). Clathrin (190 kDa) can coat the antigen-ADC complex to form a 100–150 nm diameter vesicle (Chalouni & Doll, 2018). After formation of the complex, clathrin and adaptor protein 2 will be recruited to cell membranes, encapsulating the antigen-ADC complex then invaginating into cells to form clathrin capsule vesicles (Chen & Zhan, 2019). Dynein, a GTPase, will be recruited to the junction site between the cell membrane and vesicle, and forms a ring to separate the vesicle from the cell membrane allowing the vesicle to enter the tumor cell (Chalouni & Doll, 2018). Subsequently, the vesicle will transform into early endosomes with a pH of 5.9 to 6.0. Early endosomes can either transport the antigen-ADC complex back to the cell surface, or transform into late endosomes and transport the complex to the lysosomes. Late endosomes (also known as polyvesicular bodies) with a lower pH value are gradually formed in the early endosome (Chen & Zhan, 2019). The late endosome then fuses with the lysosome to release the ADC (Kalim et al., 2017). From endocytosis to degradation, this process takes several hours (Thurber et al., 2008), during which the payload accumulates in the tumor cells.

Caveolin-mediated endocytosis: Like clathrin-mediated endocytosis, endocytosis mediated by caveolin is generally receptor-dependent (Sargiacomo et al., 1995). Caveolae are a lipid raft structure (55–80 nm diameter) with complex cholesterol and are formed by polymerization of caveolin (21 kDa) (Chalouni & Doll, 2018). Caveolae can mediate cave-like invagination to encapsulate the antigen-ADC complex for internalization, the content and volume of which is smaller than those of clathrin-mediated endocytosis (Chen & Zhan, 2019). Caveolae are dynamic endocytic carriers. Caveolae buds and fuses back to the plasma membrane within one second (Chalouni & Doll, 2018). This is a dynamic cycle of caveolae budding from the plasma membrane, some of which fuse with plasma membranes in an apparent futile cycle, whereas others transform into early endosomes and then return to the plasma membrane. Caveolin-1 was shown to promote T-DM1 internalization and enhance drug sensitivity (Chung et al., 2018). In addition, one study showed that caveolae-mediated endocytosis was a novel T-DM1 resistance mechanism, internalizing T-DM1 and then expelling it out of the cell (Sung, et al., 2018).

Macropinocytosis: Macropinocytosis is a spontaneous endocytosis pathway (Bauer et al., 2016). It can also be induced by the engagement of growth factor, chemokine, or toll-like receptors (Mitrenga et al., 1975). This pathway, like phagocytosis, is actin-mediated. Additionally, microtubules and microfilaments play important roles in membrane ruffling and macropinosome closure (Marques et al., 2017). After extending a certain length, the plasma membrane forms about 50–100 microvilli-like structures (about 0.5 μm to 5 μm), which can encapsulate the ADC (Chalouni & Doll, 2018). This vesicle is called the macropinosome. The existence time of macropinocytosis in the cell is short (about 5–20 minutes). This process transports encapsulated contents to lysosomes (Bauer et al., 2020; Bauer et al., 2016). For normal tissues, macropinocytosis can function in clearing apoptotic cells, participating in an immune response, mediating the invasion of some pathogens and renewing the cell membrane (Marques et al., 2017). Macropinocytosis provides an effective way for non-selective endocytosis of extracellular nutrients and liquid macromolecules. In

tumor cells, mutated genes such as v-Src or K-Ras can enhance macropinocytosis. There are a large number of dead cells (70–80%) in the center of tumor tissues due to a lack of nutrient supply (Jayashankar & Edinger, 2020). Surrounding living tumor cells can absorb the biomacromolecules and nutrients from dead cells through macropinocytosis, greatly improving the utilization rate of cell resources (Jayashankar & Edinger, 2020).

3.3.2. Research methods for intracellular transport and localization of ADCs

—For the evaluation of ADC endocytosis, the rate and intracellular localization are the most important aspects (Harper et al., 2013). Determining the mechanism of endocytosis can offer valuable information including the proportion of ADCs in the tumor environment that enter into tumor cells and the time necessary for ADC internalization of the target antigen or target cancer cells. These determinants can be used to select the best target cancer cells, target antigen and optimal ADC composition. Intracellular localization of ADCs can offer information such as the proportion of ADC excreted outside of tumor cells after endocytosis, the rate limiting step in lysosome transport, the drug release rate in tumor cells, and the stability of different linkers throughout transport.

Flow cytometry is often used as a method for determining endocytosis of ADCs (Marder et al., 1987). At 4°C ADCs can specifically bind to the cell surface target antigen, but will not be endocytosed. At 37°C, cells can mediate endocytosis to intake ADCs from the cell surface. Thus the endocytosis rate of an ADC can be calculated indirectly by comparing the fluorescence intensity changes of cell surface at 4°C with that after incubation at 37°C (Harper et al., 2013; Chen & Zhan, 2019).

The use of confocal microscopy allows visualization of ADCs after endocytosis (Harper et al., 2013). This technique uses different fluorophores to label the ADC, payload, cell membranes, and organelles including lysosome-associated membrane protein-1, clathrin heavy chain and caveolin-1 (Donaldson, 2015; Chen & Zhan, 2019). The localization of the ADC in the cells at different times is observed directly by a high-resolution confocal microscope (Kalim et al., 2017; Harper et al., 2013).

3.3.3. Problems and methods to improve ADC endocytosis efficiency—

Most current ADCs in development and all marketed ADCs target tumor cell surface antigens and depend upon internalization to release payloads, which emphasizes the importance of studying ADC endocytosis and methods for improving endocytosis efficiency (Nejadmoghaddam et al., 2019). The endocytosis efficiency of an ADC is related to endocytosis characteristics of antigens, antibody binding sites on antigens and tumor cell type (Birrer et al., 2019). The antibody internalization rate, internalization time, recycling and intracellular drug accumulation are all key parameters to measure and estimate ADC endocytosis efficacy (Birrer et al., 2019; Muhammad et al., 2017). Durbin et. al. evaluated the endocytosis effectiveness of an ADC against EGFR-overexpressing cancer cell lines. They found that the same ADC (Ab033) has an internalization rate of 0.047/minute for A431 cells and 0.15/minute for H441 cells. In addition, they found up to 45% of internalized Ab033 returned to the cell surface. Fortunately, despite the recycling after 24 hours, about 5×10^6 free toxic drug molecules accumulated in a single tumor cell. Based on the same antibody, Ab033, they prepared ADCs with either cleavable or non-cleavable linkers. Ab033

ADC with a cleavable linker showed high payload accumulation compared with the non-cleavable linker Ab033 ADC (Durbin et al., 2018). This suggests that many different conditions occurring at the same time affect the endocytosis efficiency and therapeutic efficacy of ADCs.

The structure of the antibody can be modified to improve the endocytosis efficiency (Thakur et al., 2018). Bispecific antibodies (those that bind two targets) and biseptide antibodies (those that bind two locations on one target) are two developing strategies to improve ADC endocytosis efficiency (Chiu & Gilliland, 2016).

Bispecific antibody: Bispecific antibodies can bind two target antigens at the same time (the applicable target tumor cells should express both of the two antigens on their surface). The antigen with high endocytosis efficiency can internalize the ADC regardless of a low endocytosis efficiency of the other antigen (normally a low endocytosis antigen is a tumor marker, while a high endocytosis antigen does not have to be a tumor antigen) (Pegram et al., 2020; Andreev et al., 2017). For example, when antibodies targeting the fast-internalized epithelial cell kinase A2 (EphA2) and non-internalized high expression activated leukocyte cell adhesion molecule (ALCAM) are combined to form a bispecific ADC, the number of bispecific antibodies entering tumor cells exceeds that of a single mAb or a mixture of two antibodies, showing a bispecific-dependent amplification effect (Lee et al., 2019). The anti-ALCAM binding domain provides tumor-specific binding sites, and the anti-EphA2 binding domain can promote endocytosis. A small amount of internalized antigen EphA2 induces a large number of internalized ALCAM. On this basis, the bispecific ADC was constructed. Results demonstrate the killing effect of the bispecific ADC on tumor cells in vitro and in vivo were better than that of a single specific ADC (Lee et al., 2019), though it is unclear whether this strategy might negatively impact tumor specificity.

Biseptide antibody: Dual epitope (or biseptide) ADCs do not target two kinds of antigens, but target different epitopes of one target through two Fab fragments of the antibody (Robert et al., 1999). At present, a dual epitope ADC targeting HER2, a poor internalization antigen after antibody binding, has undergone clinical studies (Pegram et al., 2020). Li et al. prepared a bivalent biparatopic antibody targeting two non-overlapping epitopes on HER2 and subsequently prepared an ADC that coupled the biseptide antibody and microtubule inhibitor. They found that the biseptide antibody induced HER2 receptor clustering and brought robust internalization, lysosomal trafficking, and degradation. In vivo studies showed superior anti-tumor activity over T-DM1 (Li et al., 2019).

3.4. Fourth step – ADCs release payloads within target cells

3.4.1 Lysosomal treatment of ADCs—The late endosomes carrying ADCs fuse with lysosomes and transport ADCs for degradation, thereafter releasing the payload (Howard, 2017) (shown in Figure 5, step 4). Lysosomes maintain an acidic environment of pH 4.5 to 5.0 through continuous proton input via H⁺-ATPase (Chalouni & Doll, 2018). They are also rich in proteolytic enzymes, such as cathepsin and collagenase. When ADCs enter tumor cells, the antibody part of the ADC has completed its mission. Part of the antibody will be hydrolyzed by proteases in the cell and broken down into amino acids (Ritchie et al., 2013).

From endocytosis to degradation, this process takes several hours (Thurber et al., 2008). During this time, the payload will be released and accumulate in the cytoplasm. The release mechanism is determined by the type of linker (Staudacher & Brown, 2017).

The first approved ADC, Mylotarg, uses hydrazone linker technology. Hydrazone linkers are chemically unstable linkers, which are joined to the lysine residues of antibodies and release the payload as a result of environmental differences between the plasma and cytoplasm (Lu et al., 2016). Hydrazone linkers break at acidic pH. In general, they are stable at the neutral pH (7.3 to 7.5) of blood, where their degradation rate is only ~6% in 24 hours. After entering tumor cells, ADCs in late endosomes (pH 5.0 to 6.5) and lysosomes (pH 4.5 to 5.0) rapidly release their payloads. The 24-hour degradation can be up to 97% (Nolting, 2013).

Disulfide bond-based linkers are also a type of chemically unstable linker (Lu et al., 2016). The disulfide bond is stable in plasma. After entering tumor cells, it contacts with the strong reductive environment of the cytoplasm and releases the payload. Disulfide linker reduction requires sulfhydryl cofactors, such as reductive glutathione (GSH), or disulfide isomerase (Nolting, 2013). On average, the concentration of GSH in cells ranges from 0.5 to 10 mmol/L, while in blood GSH is very low at about 5 μ mol/L (Tsuchikama & An, 2016).

Enzyme catalyzed linkers are more stable than disulfide and hydrazone linkers (Tumey & Han, 2017). Peptide linkers are a typical enzyme-catalyzed linker, which can better control the release of the ADC payload. Due to the neutral pH of blood and endogenous inhibitors, the activity of protease in blood is very low, which ensures the stability of peptide linkers in blood (McCombs & Owen, 2015). The half-life of a peptide linker is generally 7–10 days (Nolting, 2013). After an ADC enters a tumor cell and is transported to the lysosome, its peptide linker will break down gradually by protease degradation and release the payload. In addition, the β -glucuronide linker is a type of enzyme-cleavable linker which is cleaved by β -glucosidase (Jeffrey et al., 2010). This enzyme is overexpressed in some types of tumors, and its activity is very low in the extracellular environment. An advantage of the β -glucuronide linker is its hydrophilicity, which can reduce ADC aggregation.

At present, the most common non-cleavable linker in ADCs is the thioether linker, which is obtained by reaction of maleimide and mercaptan (Lu et al., 2016). After degradation of the thioether linker in lysosomes, the lysine-containing payload is released (Walles et al., 2017). Generally, a thioether linker has a half-life of about 7 days, which is close to that of a cleavable linker (Alley et al., 2008). For example, the marketed ADC T-DM1 applies a non-cleavable thioether linker, designed to retain the payload inside the tumor cells (Lambert & Chari, 2014). Additionally, the marketed ADC Blenrep applies a non-cleavable maleimidocaproyl linker connecting belantamab and MMAF.

3.4.2. Research on linker technology—Research on linker technology mainly focuses on linker stability determination, optimization of old linkers, development of new linker strategies and mapping of coupling kinetic models (Nolting, 2013). The determination of ADC stability in vivo is key in evaluating the linker (Lu et al., 2016). The most important detection methods are ELISA and LC-MS (Chen et al., 2016). The lysine residues on the antibody surface contain amino groups, which can be used as coupling sites due to their

strong nucleophilicity (Nolting, 2013). In the simplest coupling reaction, the active ester (O-succinimide or N-hydroxythiosuccinimide) can react directly with lysine residues to form stable amide bonds (Behrens et al., 2015). Other active esters such as hydroxybenzotriazole, fluorobenzene or nitrobenzene derivatives can also be used to form linkers (Yao et al., 2016). This coupling method is widely used for non-cleavable linkers.

Alternatively, a two-step coupling method can be used to couple antibodies and payloads (Chih et al., 2011). In this method, lysine residues of the antibody are modified, the linker is added, and then payloads are coupled to the linker (Gandhi et al., 2018). The second coupling reaction usually uses a sulfhydryl group in the payload (Chih et al., 2011). For example, T-DM1 is linked to the antibody by using SMCC as its linker (Wakankar et al., 2010). After preparation, DAR determination and structure characterization of the ADC are needed. The available detection methods of ADCs include UV-Vis spectroscopy, hydrophobic interaction chromatography (HIC) and LC-MS (D'Atri et al., 2018; Ouyang, 2013).

3.4.3. Problems and strategies related to linkers—There are, on average, 40 lysine sites on a typical antibody that can be used to couple payloads, giving $\sim 10^6$ forms of the ADC, theoretically (Chen & Zhan, 2019). IgG1 contains only four inter-chain disulfide bonds, which have higher reactivity than intra-chain disulfide bonds and can be used for modification (Badescu et al., 2014). After disulfide bond breaking, eight cysteine residues are produced as potential junction sites. However, the use of cleaved cysteine as a payload binding site will affect stability of the antibody (Dimasi et al., 2017). Some of the early ADCs were constructed using glycosyl groups on the antibody surface as junction sites, with the advantage of being able to connect large numbers of payloads (Tumey & Han, 2017). However, the disadvantage lies in the inability to control the junction site and DAR, leading to the junction site covering the antibody specific recognition sites. As a result, part of these ADCs cannot bind to the target antigen, or alternatively, the excessive connections can enhance the hydrophobicity of the ADC resulting in hydrophobic aggregation and precipitation (Panowski et al., 2014). Early development of Mylotarg used lysine on antibodies to couple payloads. Due to a relatively large amount of lysine on the antibody, the DAR is as high as 14, which makes inter-batch consistency and ADC diversity of Mylotarg difficult to control. At present, research has focused on reducing heterogeneity of ADCs (Sochaj et al., 2015; Behrens et al., 2015).

Site-specific coupling technology is used to couple a certain number of payload molecules to specific sites of the antibody, ensuring consistency of the prepared ADC, with the benefit of improving efficacy and reducing toxicity (Dan et al., 2018). Enzyme based coupling is an important example of this technology. Enzymatic modification of antibodies can produce completely homogeneous ADCs through enzyme-specific substrate catalysis. The commonly used enzymes are glycosyltransferase, glutamine transferase and β -galactosidase (Yamada & Ito, 2019). The Fc segment of all IgG subtypes has a pair of N-glycosylated aspartates (Asn297), which can be used for glycosyltransferase modification to introduce linker and payload (Kubizek et al., 2017). Specifically, β -N-acetylglucosaminidase is used to break oligosaccharides on N-glycosylated aspartate to expose active sites for modification (the original oligosaccharide has unfixed length and lacks a payload conjugating site).

Then β -N-acetylglucosaminidase mutants are used to add oligosaccharides with azide-based payload binding sites. Following this addition, payloads can be attached onto the oligosaccharide by azides through biorthogonal reactions (Manabe & Yamaguchi, 2021). In one study the authors designed a β -galactosidase-cleavable linker for ADCs. A galactoside linker, monomethyl auristatin E (MMAE) and cysteine-reactive trastuzumab were conjugated to form an ADC. Evaluation of the ADC, both in vitro and in vivo, found superior therapeutic efficacy in mice compared to trastuzumab emtansine (Kolodych, et al., 2017).

During antibody preparation, unnatural amino acids can be added into the antibody through genetic engineering (Axup et al., 2012). The biggest advantage of introducing unnatural amino acids is that the prepared antibody can easily complete specified chemical reactions at these residues to connect a payload (Liang et al., 2019). The most common method is to change a stop codon into a coded codon (Axup et al., 2012). This method also requires synthetic tRNA and tRNA synthetase. Additionally, the strategy of converting amino acid residues in a non-antigen-recognition region of an antibody into cysteine by genetic engineering has also been reported (Dimasi et al., 2017). This method can be used to modify a disulfide bond in the antibody chain to couple payloads without destroying inter-chain disulfide bonds or affecting the stability of the antibody (Dimasi et al., 2017).

3.5. Fifth step – cytotoxic ADC payloads inhibit tumor cell growth

3.5.1. ADC payload mechanism of action and toxicity—Once ADCs are degraded in lysosomes, their payloads are released into the cytoplasm to engage their corresponding targets (Casi & Neri, 2012). Typically, for moderately potent payloads, accumulation over 10^6 molecules/cell will kill one tumor cell (Chari et al., 2014). The most common targets are DNA in the nucleus and microtubules in the cytoplasm. Drugs targeting nuclear DNA include adriamycin, duocarmycin and pyrrole benzodiazepines (PBDs) (Fu & Ho, 2018). These drugs embed into small grooves on the double helix structure of DNA, breaking the DNA apart and leading to cellular apoptosis (Fu & Ho, 2018). There are two kinds of ADC payloads targeting microtubules: auristatin derivatives (including MMAE and MMAF) and maytansine derivatives (including DM1 and DM4) (Akaiwa et al., 2020). More than 60% of ADCs in clinical trials employ microtubule inhibitors as their payloads (Fu & Ho, 2018). Compared to payloads that target DNA, these drugs better limit cell growth. They mainly target microtubules of rapidly dividing cells, blocking the cell cycle and leading to apoptosis. After degradation of the ADC, the small molecules released into the cytoplasm can cross cell membranes, enter adjacent cells and inhibit proliferation (Staudacher & Brown, 2017). The bystander effect is helpful to inhibit tumor cells with weak or no expression of TSA in heterogeneous tumors (Staudacher & Brown, 2017) (shown in Figure 5, step 5), though at the same time it could have negative consequences if neighboring normal cells are affected.

Tubulin inhibitors: Tubulin polymerization is essential for a variety of cellular processes, including intracellular transport, mitosis, and structural integrity maintenance (Chen et al., 2017a). Microtubules have at least five known binding sites, including vinca alkaloid, colchicine, paclitaxel, meticin and lauramide binding sites. Microtubule-targeting agents

block separation of the mitotic spindle, resulting in unstable cytoskeleton structure, which induces cell cycle arrest in the G2/M phase leading to cell death. The structure of microtubules can be influenced by the binding of β -subunit or α - β heterodimer of tubulin (Chen et al., 2017a; Haider et al., 2019). Maytansines can bind to the extended microtubules and inhibit formation of microtubules by blocking the tubulin heterodimer formation (Steinmetz & Prota, 2018). Drugs with this mechanism are suitable for rapidly proliferating cells. Therefore, microtubule inhibitors are particularly cytotoxic to cancer cells, because cancer cells divide and grow faster than most normal cells (Steinmetz & Prota, 2018). This can also reduce the off-target killing of normal tissues and cells. However, early release of microtubule inhibitors can kill some rapidly dividing normal cells, resulting in adverse side effects (Gébleux et al., 2015). In addition, static and undifferentiated cancer cells, such as cancer stem cells or tumor initiating cells, are less sensitive to microtubule inhibitors, thus avoiding killing and producing drug resistance (Takebe et al., 2015). It should be noted that most mouse xenotransplantation models contain tumors that grow much faster than normal human tumors (Morton et al., 2016). Therefore, drugs that exhibit strong tumor killing activity in animal experiments may not necessarily show the same efficacy in human clinical trials.

Maytansines are cytotoxins similar in structure to rifamycin, geldanamycin and cladospirin, which have a common nineteen membered macrolide structure (Elliott & Fried, 1976; Erickson et al., 2006). Maytansine and its derivatives are potent inhibitors of microtubule assembly. They can induce mitotic arrest of poisoned cells by binding to tubulin at the vinblastine binding site, therefore, the mechanism of maytansines is similar to that of vinblastine (Huang et al., 1985). At low concentrations, microtubule dynamic instability and cell migration are inhibited; at higher concentrations, microtubule assembly and cell division are inhibited. These effects result in antiproliferative activity during mitosis (Su et al., 2018). The ED₅₀ (effective dose) of maytansine ranges from 10⁻⁵ μ g/ml to 10⁻⁴ μ g/ml (Cassady et al., 2004). Premature release of maytansines can lead to side effects such as neurotoxicity, gastrointestinal toxicity, weakness, nausea, vomiting and diarrhea (Kowalczyk et al., 2017).

DNA damaging agents: DNA damaging agents have a long history of application to cancer chemotherapy (Hartley & Hochhauser, 2012). These molecules exert their cytotoxic role by binding to the DNA double helix. According to their mechanisms of action against DNA, they are divided into four types: double strand break agents (such as doxorubicin), alkylating agents (such as PBDs), intercalating agents (such as calicheamicins) and crosslinking agents (such as cisplatin) (Hartley & Hochhauser, 2012). DNA damage agents have two advantages as ADC payloads relative to microtubule targeting agents: (1) DNA damaging agents (pM IC₅₀ values) have more potent cytotoxicity than microtubule targeting agents (nM IC₅₀ value), which enables ADCs to kill cancer cells at lower doses, including cancer cells with low expression of target antigens; (2) DNA damaging agents kill tumor cells regardless of their cell cycle stages (dividing or non-dividing cells) (Bander, 2013). This can produce cytotoxic activity against less proliferative cancer cells, such as cancer stem cells (Takebe et al., 2015). In addition, calicheamicins can insert into the minor DNA groove and induce cell apoptosis. The cytotoxicity of calicheamicin is more than 100 times that of standard

chemotherapy drugs (Ricart & D., 2011). Among the ADC drugs currently on the market, Mylotarg and Besponsa both use calicheamicin as their payload.

3.5.2. Metabolism studies of ADCs—Payloads released from ADCs in the lysosome kill tumor cells. Research in this area mainly focuses on the metabolism of the ADC, the toxicity mechanism of the payload, and the adverse reactions of the ADC (Sarrut et al., 2016). As an ADC enters circulation, payloads are slowly released, and the average DAR value will decrease with time until reaching zero (Hedrich et al., 2018). The change rate of DAR can reflect the release rate of payloads from the antibody. At the same time, the molar concentration of cytotoxic molecules in circulation will increase, which affects efficacy and safety. The metabolism of ADCs includes: (1) the study of small molecules and their metabolites and (2) the study of antibodies and their metabolites (Malik et al., 2017). These studies help uncover the toxicity mechanism and metabolic process of ADCs, to understand more about these molecules to optimize their design and achieve a better curative effect.

ELISA is a typical ligand binding assay for qualitative and quantitative analysis of antibody molecules in ADCs (Shah & Maghsoudlou, 2016) (Li et al., 2016). The ADC and its metabolism can be measured conveniently and accurately by this method. A downfall of this assay is that it only measures the ADC antibody, but not released payloads. Additionally, it is only suitable for the detection of known metabolites, not unknown metabolites (Li et al., 2016).

LC-MS can be used to detect small-molecule payloads. With the improvement of analytic methods and instrument sensitivity, LC-MS can be used to analyze the DAR of ADCs and the metabolism of toxic small molecules (Zhu et al., 2020). This method is quite beneficial especially because it is capable of identifying new metabolites (Huo et al., 2015). The connection sites and the number of connections of the payload on the ADC can be obtained (Yu et al., 2010).

3.5.3. Problems with ADC payloads

Effects of payloads on ADCs: Often times, cytotoxic small molecule drugs used as ADC payloads are hydrophobic in nature (Adair et al., 2012; Anderl et al., 2013). The hydrophobicity of the payload affects physical and chemical properties of the ADC (Lyon et al., 2015). Excessive hydrophobic cytotoxic molecules coupling to the ADC structure make ADCs easy to aggregate and become unstable. This is not only due to the hydrophobicity, but also because of changes in antibody secondary and tertiary structures and the resulting impact on conformation stability (Lyon et al., 2015). For example, the serum half-life of the ADC T-DM1 (3.94 days) is far shorter than its antibody trastuzumab (18.3 days) (Pegram et al., 2020). In addition, differences in conjugation sites and the DAR also affect pharmacokinetic (PK) properties of ADCs leading to ADC heterogeneity and characterization difficulties (Lyon et al., 2015). In contrast, hydrophilic payloads decrease ADC aggregation, but also decrease ADC membrane permeability and bystander effect. The off-target effects and metabolism of payloads directly impact the function of ADCs. Payloads that are substrates, inhibitors or inducers of metabolic enzymes such as

cytochrome P450 isozymes or even transporters (such as P-glycoprotein) likely impact ADC metabolism as well (Lynch & Price, 2007; Shen et al., 2012).

Limit adverse reactions: One of the key research points of ADC development is to limit off-target toxicity. This toxicity of the ADC is mainly driven by prematurely released payload or payload released in normal cells (Mahalingaiah et al., 2019). In blood, the ADC linker may break (especially cleavable linker), which can lead to toxicity. ADCs collected by normal cells through nonselective endocytosis also produce toxicity (Su et al., 2018). In addition, some ADCs will bind non-tumor cells that also express the target antigen. Ocular toxicity has been reported in more than a dozen ADCs targeting a variety of antigens, most of which have limited expression in the eyes (Su et al., 2018). These adverse reactions include blurred vision, abnormal cornea, or dry eyes (Masters et al., 2018). Most of the ADCs involved contain MMAF or DM4 indicating that there is a relationship between these tubulin inhibitory payloads and the development of ocular side effects (Wolska-Washer & Robak, 2019). It is speculated that this effect, at least in part, is a result of damage to stem cells living in the limbus (Parrozzani et al., 2020). Compared with MMAF, ADCs containing MMAE have less ocular toxicity (Akaiwa et al., 2020). However, most MMAE based ADCs have toxic effects such as neutropenia and peripheral neuropathy (Masters et al., 2018). These are also common side effects of various microtubule inhibitors. As mature neurons do not actively divide, neuronal cell death is not related to mitotic blockade (Masters et al., 2018). In contrast, peripheral neuropathy is thought to be caused by damage to microtubule-dependent transport pathways. The development of vadastuximab talirine (SGN-CD33A) based on PBDs was suspended by the FDA due to its severe hepatotoxicity (Saber et al., 2019). In one study the authors carried out a meta-analysis of 70 publications to obtain clinical toxicity information of ADCs. In the analysis, anemia, neutropenia, and peripheral neuropathy were found for MMAE ADCs, where thrombocytopenia and hepatic toxicity were evident for DM1, and ocular toxicity followed MMAF (Masters et al., 2018). In another example, T-DM1 can bind to HER2 in hepatocyte cell surfaces, thus leading to hepatic toxicity (Pegram et al., 2020). Additionally, T-DM1 can internalize into megakaryocytes via a Fc γ RIIa-dependent manner, resulting in diminished megakaryocytes. Platelets are produced by megakaryocytes, so T-DM1 treatment can lead to thrombocytopenia (Pegram, et al., 2020). ADCs that extravasate into a normal lung have the potential to cause interstitial pneumonia as a severe adverse effect. EGFR-targeted therapy causes dermatitis in some patients, and while the mechanism is unknown, it is observed in both EGFR-high and -low tumors (Lenz, 2006). These adverse reactions are concluded as off-target toxicities and related to payloads. Overall, it is necessary to study new compounds as potential payloads for ADCs that reduce the risk of adverse reactions and off-target toxicity, while providing the same or better tumor cell killing.

4. Current ADC clinical landscape

Use of ADCs for tumor therapy is promising for the treatment of a number of cancer types. So far, at least ten ADC drugs have been approved by the FDA (shown in Table 1). Among them, six ADCs treat hematological malignancies. Compared with solid tumors, target antigens of hematological malignancies are more easily contacted by circulating

ADCs. Lymphoma and breast cancer are two of the most researched cancers. There are three ADCs approved for breast cancer and another two for lymphoma. The antigens in these ten approved ADCs (e.g., CD33, CD30, CD22) are tumor cell surface molecules with highly restricted distribution patterns, which avoid ADCs targeting hematopoietic tissues and pluripotent stem cells, providing better specificity and tolerance.

The number of ADCs in clinical trials is increasing rapidly. At present, there are more than 280 ADC-related clinical trials at different stages studying about 138 different ADCs to treat roughly 60 kinds of cancer (<https://clinicaltrials.gov>). Pharmaceutical companies around the world have contributed to the vigorous development of ADCs in clinical research, which brings new hope to the fight against cancer. Table 2 summarizes some of the ADCs in clinical trials in the most recent years, focusing on tumor types, payloads, linker type, sponsors, and clinical status.

Of the clinically used agents, Mylotarg was first approved by the FDA in May 2000. In 2010, Pfizer withdrew Mylotarg from the market due to the side effect of veno-occlusive disease causing the early death of patients (Cohen et al., 2002; Norsworthy et al., 2018). In 2014, analysis of data from five randomized clinical trials found that low-dose Mylotarg improved patient survival compared with supportive treatment. Based on these data, in September 2017, the FDA again approved it for treatment of adult patients with newly diagnosed acute myeloid leukemia expressing CD33 antigen (Norsworthy et al., 2018).

Adcetris was initially approved for Hodgkin's lymphoma (HL) and systemic anaplastic large cell lymphoma (sALCL) in 2011 (Scott, 2017). Additionally, it was approved as a first-line treatment in November 2018 for treating adult patients with CD30 positive peripheral T-cell lymphoma (PTCL) ([NCT01777152](#), [NCT01578499](#) and [NCT01100502](#)). Around HL, sALCL and PTCL, Adcetris has obtained six treatment indications, demonstrating a rapid indication expansion (van der Weyden et al., 2019).

Kadcyla was approved for use in treating HER2-positive breast cancer in 2013. Currently, it is the only ADC approved as a monotherapy drug in 104 countries (including the United States and EU Member States) for HER2-positive metastatic breast cancer patients who have previously received Herceptin and/or paclitaxel chemotherapy (Lambert & Chari, 2014; Phillips et al., 2016) ([NCT00829166](#)).

Besponsa is the second ADC from Pfizer. Launched in 2017, it targets CD22 for the treatment of relapsed/refractory B-cell precursor acute lymphoblastic leukemia ([NCT01564784](#)). Besponsa uses the same acid-unstable hydrazone linker as Mylotarg. Lumoxiti (Moxetumomab pasudotox) was approved in September 2018 for the treatment of patients with hairy cell leukemia. Eighty percent of patients (64) achieved complete remission of tumors over 180 days after treatment ([NCT01829711](#)). The most common adverse reactions were tissue edema and renal failure (Kreitman & Arons, 2018).

Polivy (polatuzumab vedotin) was approved in June 2019 for patients with B-cell lymphoma who had received at least two other prior treatments (Deeks, 2019). It was approved because of good therapeutic outcome in clinical trial ([NCT02257567](#)). Padcev (enfortumab vedotin) was approved in December 2019 for treatment of locally advanced or metastatic urothelial

carcinoma (Hanna, 2020). In a clinical trial involving 125 patients, Padcev brought 44% objective response rate (ORR), 12 complete responses and 7.6 months in median duration response contributing to its approval (NCT03219333). The most common side effects were hyperglycemia, peripheral neuropathy and eye diseases. Enhertu (trastuzumab deruxtecan) was approved in December 2019 for patients with HER2-positive breast cancer who had received at least two other previous treatments (Keam, 2020). In the clinical trial, 60.3% ORR reflected significant tumor regression, and median relapse free time of 14.8 months supporting approval (NCT03248492). The common adverse reactions of Enhertu were neutropenia and left ventricular dysfunction. Severe adverse reactions included interstitial lung disease and embryo-fetal toxicity (Keam, 2020).

Trodelvy (sacituzumab govitecan) was approved by the FDA in April 2020 for patients with advanced triple negative breast cancer who had received at least two other prior treatments. In the clinical study (NCT01631552), 33.3% ORR and a median relapse free time of 7.7 months. The most common adverse reactions include nausea and vomiting, neutropenia, diarrhea, and fatigue. Blenrep (bellantamab mafodotin) was approved by the FDA in August 2020 for the treatment of recurrent multiple myeloma. In its clinical study (NCT03525678), good outcomes were observed with 31% ORR and 73% patients showing no recurrence for more than six months. The most common adverse reactions include corneal disease (corneal epithelial changes on ophthalmic examination), vision loss and nausea (Kaplon et al., 2020). These clinical studies and patents outline successful applications of ADCs and meanwhile suggest some drawbacks of current ADCs.

5. Conclusions and future directions

ADCs are considered to be exciting and promising treatments for cancer (Tsuchikama & An, 2016). The number of ADCs registered in clinical trials continues to grow. This is closely related to the expansion of ADC antibody target ranges, optimization of linker technologies and innovation of new payloads (Damelin, 2018). The research of ADCs is undergoing a transition period. The old conjugation methods are giving way to newer point-specific modification methods, lower toxicity payloads are giving way to super-high toxicity payloads, mouse derived antibodies are giving way to fully humanized antibodies, and so on (Bander, 2013). A better understanding of all aspects of in vivo processing of ADCs and lessons from 20 years of clinical experience are vital to developing more effective ADCs (Damelin, 2018; Tolcher, 2016). With the approval of three ADCs in 2019, they have attracted worldwide attention. In fact, we are in the era of an ADC boom, as a large number of new and emerging ADCs are under development or in clinical trials (Theocharopoulos et al., 2020; Tolcher, 2016). It is worth noting that the addition of ADCs in clinics, clinical trials and research environments not only reflects the growing interest and confidence of doctors and pharmaceutical companies in this field, but also highlights the value and benefits that ADCs provide to cancer patients (Howard, 2017). Currently, ten ADCs have demonstrated effectiveness as therapeutic agents and gained approval by the FDA for treatment of cancers. (Table 1). In the future, more ADC drugs are expected to be approved for marketing to treat additional types of cancer (such as those in Table 2).

ADCs have the distinct advantage of transporting cytotoxic drugs into cancer cells specifically reducing the toxicity of these drugs to healthy tissues (Anderl et al., 2013; Sedlacek et al., 1992). Earlier studies tried a number of natural toxins as payloads for ADCs (Walts & Said, 1983). However, the cytotoxic activity of these toxins was not strong enough and lacked effectiveness in both animal and clinical trials. In the past 20 years, great efforts have been devoted to the development of super toxins, especially those for intracellular targets (Anderl et al., 2013). At present, many super toxins and their derivatives have been developed. These usually target microtubules or DNA. Tubulin inhibitors, such as auristatin and maytansine, are widely used in ADC development and selectively targets rapidly dividing cancer cells and induces less damage to non-dividing healthy cells (Akaiwa et al., 2020; Saber et al., 2019). DNA damaging agents, such as calicheamicins and PBDs, can induce apoptosis in all cells, including non-dividing cancer cells (Saber et al., 2019). However, despite the progress made in payload effectiveness, alternative types of payload skeletons for ADCs has not increased, and most cytotoxic agents are derivatives of former core skeletons (Yaghoubi et al., 2020). Therefore, in the next generation of ADCs, it is necessary to develop new scaffolds of high-efficiency payloads with diversified targets, mechanisms of action, and decreased side effects (Masters et al., 2018). We expect complex natural product libraries will continue to be an excellent source of novel cytotoxic molecules for use as ADC payloads.

A central difficulty within ADC development lies in the linker technology. The traditional linker technique usually couples drugs through an antibody disulfide bond utilizing cysteine or lysine residues (Tsuchikama & An, 2016). The approximately 20 potential joinable lysine residues and randomly conjugation lead to production of millions of different ADC forms (Bargh et al., 2019; Birrer et al., 2019; Tsuchikama & An, 2016). The PK properties of the heterogeneous ADCs in vivo vary greatly and as a result, industrial production faces great challenges to ensure sample consistency between batches (Tsuchikama & An, 2016). This heterogeneity in ADCs is an obstacle in gaining approval by the FDA (Birrer et al., 2019). Therefore, many companies producing ADCs are developing site-specific linker technology (White et al., 2019). Site-specific linker technology can ensure a fixed number of drug molecules coupled to specific sites of the antibody, which can ensure drug homogeneity and batch production stability to a large extent (Panowski et al., 2014). In addition, it can accurately control DAR values at 2 to 4 (Behrens et al., 2015). Presently, site-specific ADC technologies mainly rely on engineering modification of cysteine, modification of unnatural amino acids, selenocysteine replacement or site-specific enzyme catalysis (Nolting, 2013; Panowski et al., 2014). Looking toward the future, innovative and low-cost methods for coupling cytotoxicity payloads to antibodies will undoubtedly attract attention.

What are the current challenges facing the field of ADC development? Although it has been more than 35 years since the initial development of ADCs (Deguchi et al., 1986; Garnett et al., 1983), the FDA has only approved ten ADC drugs to date. Several ADCs have exhibited great potential in preclinical research, but did not perform well in clinical trials (Nejadmoghaddam et al., 2019). Toxicity and incomplete characterization data are the two main factors contributing to these failures (Hinrichs & Dixit, 2015). The nature of ADCs is more complex than mAbs, and requires additional data to support clinical trials (Lansita et al., 2015). This includes 1) complete ADC structure data: different characterizations of

ADCs between batches (MS, peptide map, glycosylation, circular dichroism, differential scanning calorimetry, etc.), DAR values, coupling site, cytotoxin distribution uniformity, etc.; 2) efficacy of ADC: antigen-binding affinity, time required for internalization, timing and localization of ADC in blood circulation, intracellular ADC entry ratio, effect of ADC in different cancers and effect of combination therapy with other drugs; 3) analysis of adverse reactions: causes and severity of side effects, toxicity to normal tissues with low expression of target antigen, adverse reactions caused by premature cleavage of linker (early release of toxin) and toxicity caused by non-specific endocytosis in non-tumor tissues (Masters et al., 2018; Roberts et al., 2013).

What are the possibilities for the future of ADC development? A large number of ADC technologies developed over the past decade have created a wide range of opportunities for designing ADCs specific to a given target (Nejadmoghaddam et al., 2019; White, et al., 2019). In combination with the approval of novel ADCs, new technologies may be able to shine in the coming years. These areas for development may include: 1) ADCs targeting tumor microenvironments. Several characteristics and targets in the tumor microenvironment are common regardless of tumor types, which can greatly broaden the therapeutic window of ADCs and improve their antitumor activity. 2) New forms of ADCs, such as X-drug conjugate (XDC, such as peptides and small molecules). Many publications in recent years reveal novel attempts on ADC-like peptide-drug conjugates, small molecule-drug conjugates, and nanoparticle-drug conjugates. 3) Recombinant DNA technology and other interdisciplinary and multidisciplinary methods that can bring low-cost site-specific payload coupling (Birrer et al., 2019; Chen & Zhan, 2019). 4) Payloads without direct cytotoxicity, such as those that may guide the immune system to target the cancerous cells. On the whole, decades of time has been spent on ADC development, thousands of papers on ADCs have been published and importantly ten ADCs have been approved up to now, all of which predict a prosperous future for ADCs.

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Abbreviations

Abs	Antibodies
ADC	Antibody-drug conjugate
ALCAM	Activated leukocyte cell adhesion molecule
BCMA	B-cell maturation antigen
CD	Cluster of differentiation
DAR	Drug-to-antibody ratio
DM1	Mertansine 1

ED	Effective dose
EGFR	Epidermal growth factor receptor
ELISA	Enzyme linked immunosorbent assay
EphA2	Epithelial cell kinase A2
EPR	Enhanced permeability and retention
Fab	Antigen binding fragment
Fc	Constant domain fragment
FcRn	Neonatal Fc receptor
FDA	Food and Drug Administration
GO	Gemtuzumab ozogamicin
GSH	Glutathione
HER2	Human epidermal growth factor receptor 2
HIC	Hydrophobic interaction chromatography
HL	Hodgkin's lymphoma
Ig	Immunoglobulin
IV	Intravenous
kDa	kilodalton
LC	Liquid chromatography
mAb	Monoclonal antibody
MC	Maleimidocaproyl
MMAE	Monomethyl auristatin E
MMAF	Monomethyl auristatin F
MS	Mass spectrometry
ORR	objective response rate
PBD	Pyrrole benzodiazepines
PK	Pharmacokinetics
PTCL	Peripheral T-cell lymphoma
sALCL	systemic anaplastic large cell lymphoma
SGN-35	Brentuximab vedotin

SMCC	Succinimidyl 4-(N-maleimidomethyl)cyclohexane-1-carboxylate
SPDB	N-succinimidyl 4-(2-pyridyldithio)butanoate
SPP	N-succinimidyl-4-(2-pyridyldithio)pentanoate
TAA	Tumor associated antigens
T-DM1	Ado-trastuzumab emtansine
TSA	Tumor specific antigens
VC	Valine citrulline

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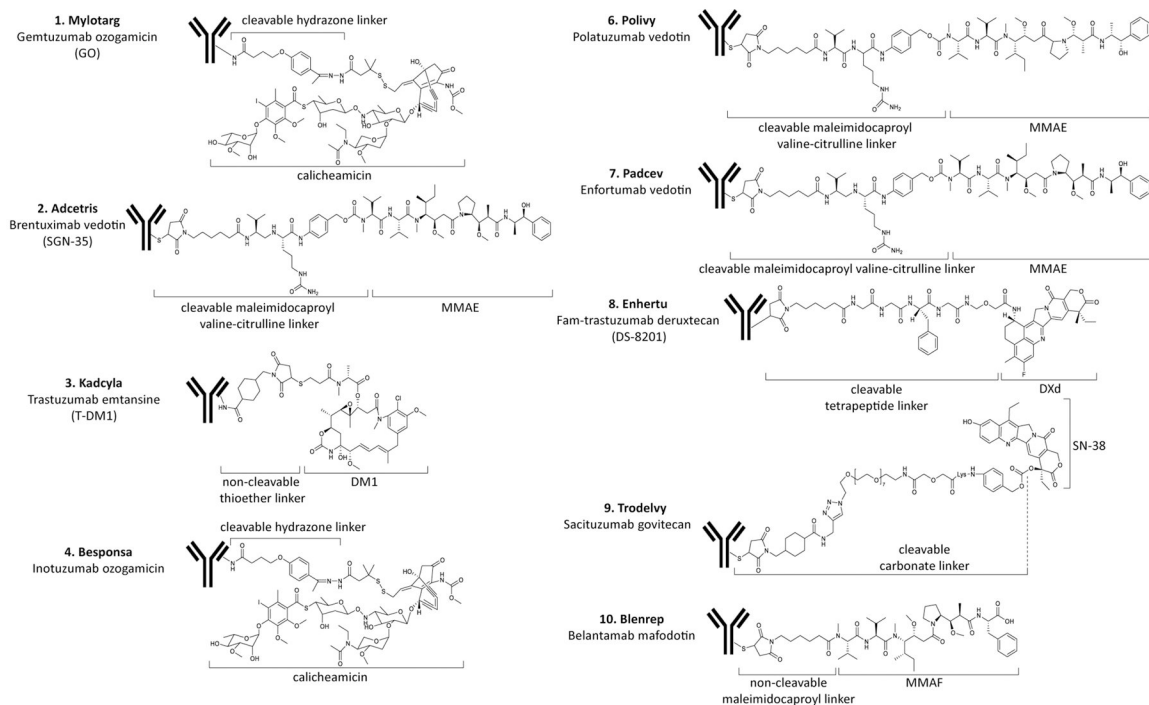


Figure 1.
Structures of the approved ADC drugs listed in Table 1.

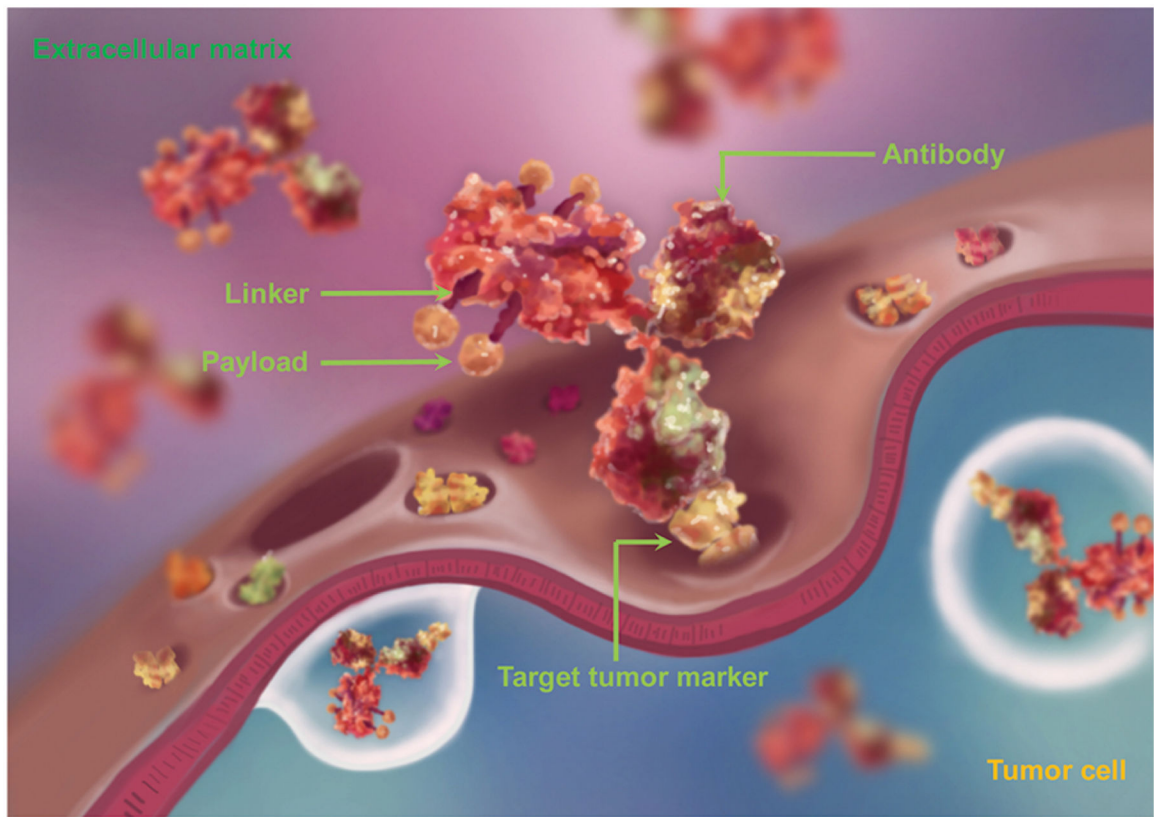


Figure 2. Structure of ADCs.

An ADC consists of three parts: an antibody, a linker and a payload (not to scale). The payloads are covalently coupled to the monoclonal antibody using linkers. This figure is based on a figure from www.adcreview.com.

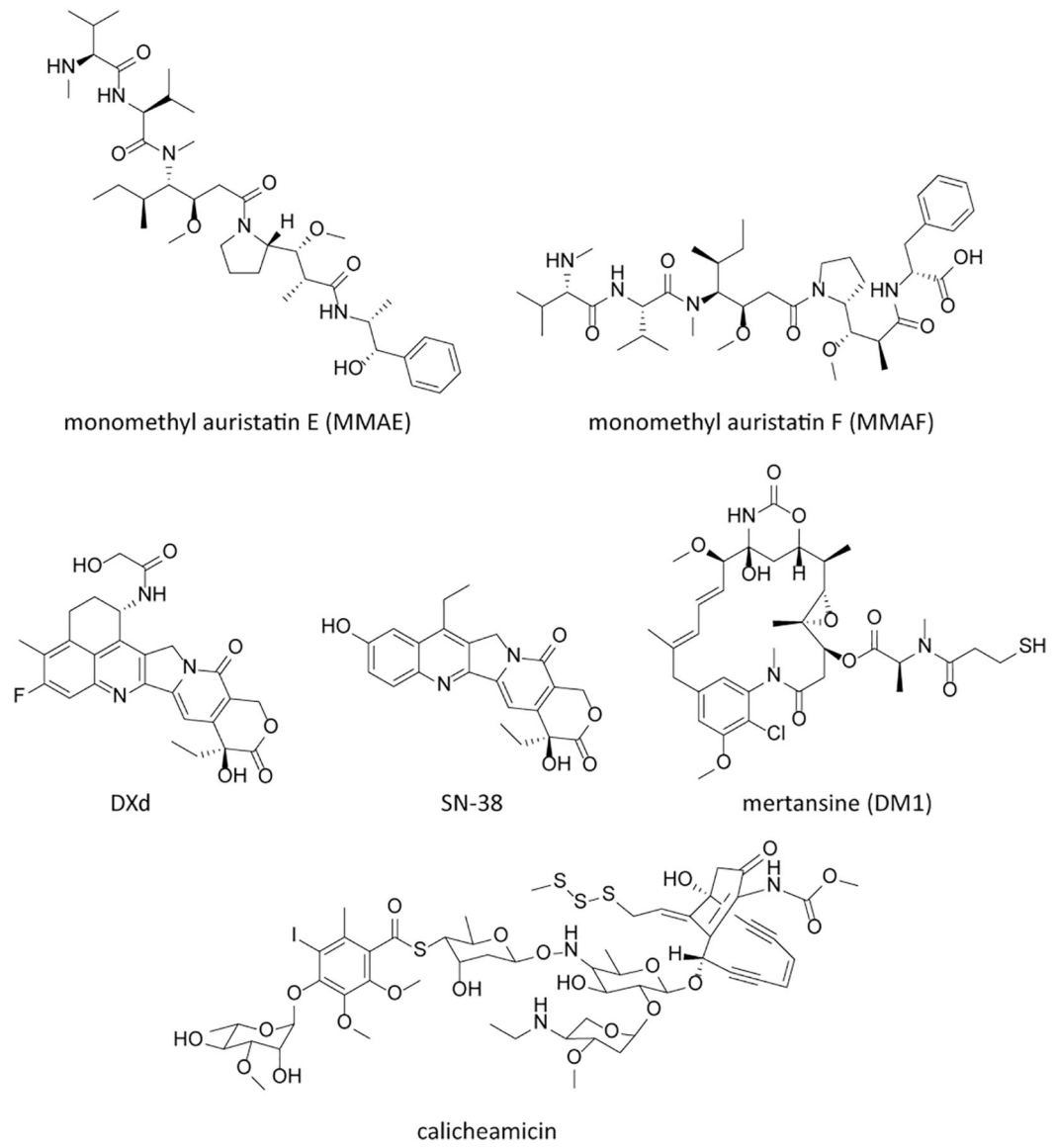


Figure 3.
Chemical structures of clinical ADC payloads.

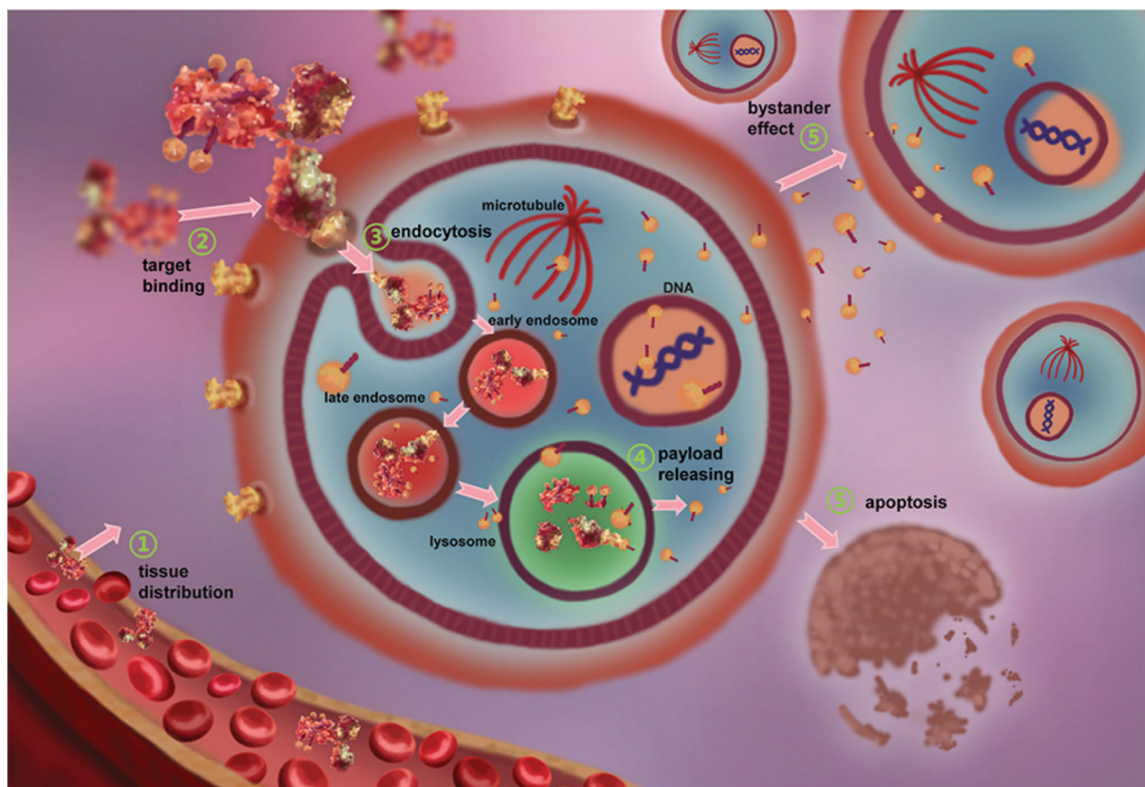


Figure 5. In vivo processing of a typical antibody drug conjugate.

(1) The ADC enters blood circulation through IV injection and then distributes throughout the body over time. (2) The ADC binds to targeted antigen on tumor cell surfaces by antigen-antibody specific binding. (3) The ADC is internalized into tumor cells via receptor-mediated endocytosis and then is transported to the lysosome. (4) Within the lysosome, cytotoxic payloads are released after ADC proteolysis or linker split. (5) Cytotoxic payloads destroy the tumor cell and nearby tumor cells through the bystander effect. The figure is based on figures in (Birrer et al., 2019) and (Lambert & Berkenblit, 2018).

Table 1.

ADC drugs approved by FDA (up to December 2020)

	ADC name	Brand name	Tumor target Antibody	Linker	Payload DAR	Indication	Pharmaceutical companies	Launch date
1	Mylotarg	Gemtuzumab ozogamicin (GO)	CD33 Humanized IgG4	Cleavable hydrazone linker	Calicheamicin 3–5	CD33 positive acute myeloid leukemia	Pfizer	5/2000/2017*
2	Adcetris	Brentuximab vedotin (SGN-35)	CD30 Chimeric IgG1	Cleavable maleimidocaproyl valine-citrulline linker	MMAE 4	Hodgkin's lymphoma	Seattle Genetics/ Takeda	8/2011
3	Kadcyla	Trastuzumab emtansine (T-DM1)	HER2 Humanized IgG1	Non-cleavable thioether linker	DM1 3–4	HER2 positive breast cancer	Roche	2/2013
4	Besponsa	Inotuzumab ozogamicin	CD22 Humanized IgG4	Cleavable hydrazone linker	Calicheamicin 6	B-cell acute lymphoblastic leukemia	Pfizer	8/2017
5	Lumoxiti	Moxetumomab pasudotox	CD22 Recombinant murine immunoglobulin variable domain	Fusion protein (antibody and payload)	Pseudomonas exotoxin	Hairy cell leukemia	AstraZeneca	9/2018
6	Polivy	Polatuzumab vedotin	CD79b Fully humanized IgG1κ	Cleavable maleimidocaproyl valine-citrulline linker	MMAE 3–4	Diffuse large B-cell lymphoma	Roche	6/2019
7	Padcev	Enfortumab vedotin	Nectin-4 Fully humanized IgG1κ	Cleavable maleimidocaproyl valine-citrulline linker	MMAE 3–4	Urothelial carcinoma	Seattle Genetics/ Astellas	12/2019
8	Enhertu	Fam-trastuzumab deruxtecan (DS-8201)	HER2 Fully humanized IgG1κ	Cleavable maleimide tetrapeptide linker	DXd 8	HER2 positive breast cancer	AstraZeneca/ Daiichi Sankyo	12/2019
9	Trodelyv	Sacituzumab govitecan	Trop-2 Humanized IgG1κ	Cleavable carbonate linker	SN-38 7–8	Triple-negative breast cancer	Immunomedics	4/2020
10	Blenrep	Belantamab mafodotin	BCMA Humanized IgG1κ	Non-cleavable maleimidocaproyl linker	MMAF 4	Relapsed and refractory multiple myeloma	GlaxoSmithKline	8/2020

* Mylotarg was first approved in 2000, withdrawn in 2010 and relaunched in 2017.

Table 2.

ADCs under clinic trials in the most recent years

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
Targeted cancer							
1. Multiple kinds of tumors							
Trastuzumab deruxtecan	HER2 Humanized antibody	Deruxtecan (camptothecin)	Cleavable	Phase I	NCT02564900 Daiichi Sankyo Co, Ltd.	Advanced breast and gastric or gastro-esophageal tumors	(Doi et al., 2017)
Lifastuzumab vedotin (LIFA)	NaPi2b (SLC34A2) Humanized IgG1 monoclonal antibody (MNB2126A)	MMAE	Cleavable VC linker	Phase I	NCT01911598 Genentech, Inc.	Non-small cell lung cancer or platinum-resistant ovarian cancer	(Gerber et al., 2020)
Anetumab ravtansine (BAY 94-9343)	Mesothelin Fully human IgG1 monoclonal antibody	DM4 3-4	Cleavable disulfide linker	Phase I	NCT01439152 Bayer HealthCare Pharmaceuticals	Advanced or metastatic solid tumors	(Hassan et al., 2020)
PF-06664178 (RN927C)	Trop-2 Humanized IgG1	Aur0101 (auristatin derivative) 2	Cleavable C-terminus of heavy chain via an enzymatic process	Phase I	NCT02122146 Pfizer	Advanced or metastatic solid tumors	(King et al., 2018)
IMGN853 Mirvetuximab soravtansine	Folate receptor α	DM4		Phase I	NCT01609556 ImmunoGen, Inc.	Solid tumors	(Moore et al., 2017a)
ABT-414	EGFR Humanized recombinant antibody	MMAF	Non-cleavable MC linker	Phase I/II	NCT01741727 AbbVie	Advanced solid tumors	(Munasinghe et al., 2017)
Telisotuzumab Vedotin (ABBV399)	c-Met Humanized monoclonal antibody	MMAE	Cleavable VC linker	Phase I	NCT02099058 AbbVie Inc.	Advanced solid tumors	(Strickler et al., 2018)
PF-06647263	EFNA4	Calicheamicin		Phase I	NCT02078752 Pfizer	Advanced solid tumors	(Garrido-Laguna et al., 2019)
PF-06263507	5T4 Humanized IgG1 antibody	MMAF 4	Cleavable MC linker	Phase I	NCT01891669 Pfizer	Advanced solid tumors	(Shapiro et al., 2017)
Depatuxizumab mafodotin (ABT-414)	EGFR	MMAF 3-4	Non-cleavable MC linker	Phase I/II	NCT01800695 AbbVie	Advanced solid tumors likely to overexpress EGFR	(Goss et al., 2018)
Enfortumab vedotin (EV)	Nectin-4 Fully humanized IgG1 κ monoclonal antibody	MMAE 3-4	Cleavable maleimidocaproyl VC linker	Phase I	NCT02091999 Astellas Pharma and Seattle Genetics	Nectin-4-positive solid tumors	(Rosenberg et al., 2020)
Brentuximab vedotin	CD30 Chimeric IgG1 antibody	MMAE	Cleavable	Phase II	NCT01461538 Seattle Genetics, Inc.	CD30-expressing solid tumors	(Sharman et al., 2019)
Aprutumab Ixadotin (BAY 1187982)	Fibroblast Growth Factor Receptor 2 (FGFR2) fully human monoclonal antibody	Auristatin W	Non-cleavable	Phase I	NCT02368951 Bayer Healthcare	Advanced FGFR2 positive solid tumors	(Kim et al., 2019)

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
2. Hodgkin's lymphoma							
Brentuximab vedotin	CD30 Monoclonal antibody	MMAE	Cleavable	Phase III	NCT01712490 Millennium Pharmaceuticals and Seattle Genetics	Stage III or IV Hodgkin's lymphoma	(Suri et al., 2019)
Brentuximab vedotin	CD30	MMAE		Phase II	NCT01569204 Takeda Pharmaceuticals	Advanced classical Hodgkin's lymphoma	(Eichenauer et al., 2017)
3. Non-Hodgkin lymphoma							
IMGN529	CD37 Humanized monoclonal antibody	DM1		Phase I	NCT01534715 ImmunoGen, Inc.	Relapsed/refractory B-cell non-Hodgkin lymphoma	(Stathis et al., 2018)
Pinatuzumab vedotin	CD22 Monoclonal antibody	MMAE	Cleavable	Phase I	NCT01209130 Genentech, Inc.	Relapsed or refractory B-cell non-Hodgkin lymphoma	(Advani et al., 2017)
Coltuximab ravtansine (SAR3419)	CD19 Monoclonal antibody	DM4	Cleavable hindered disulfide bond	Phase II	NCT01472887 Sanofi	Relapsed/refractory diffuse large B-cell lymphoma	(Trněný et al., 2018)
Inotuzumab ozogamicin (InO)	CD22 Humanized antibody	Calicheamicin	Cleavable	Phase III	NCT01232556 Pfizer Inc.	Relapsed/refractory aggressive B-cell non-Hodgkin lymphoma	(Dang et al., 2018)
SGN-CD70A	CD70	PBD	Cleavable	Phase I	NCT02216890 Genetics, Inc.	CD70-positive diffuse large B cell lymphoma and mantle cell lymphoma	(Phillips et al., 2019)
Brentuximab vedotin	CD30	MMAE		Phase II	NCT01421667 Genetics, Inc.	Diffuse large B-cell lymphoma	(Bartlett et al., 2017)
Brentuximab vedotin	CD30	MMAE		Phase I/II	NCT02581631 Bristol-Myers Squibb and Seattle Genetics	Relapsed/refractory primary mediastinal large B-cell lymphoma	(Zinzani et al., 2019)
4. Lung cancers							
Rovalpituzumab tesirine (SC16LD6.5)	DLL3 Humanized IgG1 monoclonal antibody	SC-DR002	Cleavable	Phase I	NCT01901653 Stemcentrx Inc.	Small-cell lung cancer	(Rudin et al., 2017)
Sacituzumab govitecan	Trop-2 Humanized antibody	SN-38		Phase I	NCT01631552 Immunomedics, Inc.	Small-cell lung cancer	(Gray et al., 2017)
Lorvotuzumab mertansine (IMGN901)	CD56 Humanized monoclonal antibody	DM1	Cleavable disulfide linker	Phase I/II	NCT01237678	Small-cell lung cancer	(Socinski et al., 2017)
Sacituzumab govitecan	Trop-2 Humanized antibody	SN-38		Phase I/II	NCT01631552	Advanced non-small-cell lung cancer	(Heist et al., 2017)
Trastuzumab emtansine (T-DM1)	HER2	DM1	Non-cleavable thioether linker	Phase II		HER2-positive non-small cell lung cancer	(Hotta et al., 2018)

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
Rovalpituzumab tesirine	DLL3 Humanized IgG1 monoclonal antibody	PBD	Cleavable	Phase I	NCT03086239 AbbVie Inc.	Advanced, recurrent small cell lung cancer	(Udagawa et al., 2019)
Ado-Trastuzumab emtansine (T-DM1)	HER2	DM1	Non-cleavable thioether linker	Phase II	NCT02675829 Genentech	HER2-mutant lung cancer	(Li et al., 2018)
5. Cancers in esophagus, stomach or intestine							
Trastuzumab deruxtecan	HER2 Fully humanized IgG1κ monoclonal antibody	DXd 8	Non-cleavable maleimide tetrapeptide linker	Phase II	NCT03329690 Daiichi Sankyo, Inc. and AstraZeneca	HER2-positive gastric cancer	(Shitara et al., 2020)
TAK-264 (MLN0264)	Guanylyl cyclase C Human mAb	MMAE	Cleavable	Phase II	NCT02202759 Millennium Pharmaceuticals Inc.	Metastatic or recurrent adenocarcinoma of the stomach or gastroesophageal junction	(Almhanna et al., 2017a)
Ado-Trastuzumab Emtansine (T-DM1)	HER2 Humanized monoclonal antibody	DM1	Non-cleavable thioether linker	Phase I	NCT01641939 Roche Ltd, and Genentech, Inc.	HER2-positive advanced gastric cancer	(Chen et al., 2017b)
6. Pancreatic adenocarcinoma							
LMB-100	Mesothelin (MSLN) Humanized Fab	Pseudomonas exotoxin A (PE)		Phase I/II	NCT02810418 Bayer AG, Aduro BioTech, and Morphotek Inc.	Advanced pancreatic adenocarcinoma	(Alewine et al., 2020)
TAK-264 (MLN0264)	Guanylyl cyclase C Human monoclonal antibody	MMAE	Cleavable	Phase II	NCT02202785 Millennium Pharmaceuticals, Inc.	Advanced or metastatic pancreatic adenocarcinoma	(Almhanna et al., 2017b)
7. Colorectal cancer							
Labetuzumab Govitecan (IMMU-130)	Carcinoembryonic antigen-related cell adhesion molecule 5 (CEACAM5) (CD66e) Humanized antibody	SN-38 (camptothecin)		Phase I/II	NCT01605318 Immunomedics, Inc.	Refractory or relapsing metastatic colorectal cancer	(Dotan et al., 2017)
8 Breast cancer							
Trastuzumab deruxtecan (T-DXd)	HER2 Humanized antibody	Exatecan derivative (a topoisomerase I inhibitor)	Cleavable peptide linker	Phase Ib	NCT02564900 Daiichi Sankyo, Inc.	HER2-low-expressing advanced breast cancer	(Modi et al., 2020)
Sacituzumab govitecan (IMMU-132)	Trop-2	SN-38		Phase I/II	NCT01631552 David M. Goldenberg	Metastatic triple-negative breast cancer	(Bardia et al., 2017)
Trastuzumab emtansine	HER2 Humanized monoclonal antibody	DM1		Phase III	NCT00829166 Genentech.	HER2-positive advanced breast cancer	(Diéras et al., 2017)
9. Ovarian cancer							
Mirvetuximab soravtansine (IMGN853)	Folate receptor α Humanized antibody	DM4	Cleavable disulfide linker	Phase Ib	NCT02606305 ImmunoGen, Inc.	Sensitive ovarian cancer (in combination)	(Moore et al., 2018a;

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
						with carboplatin); FRα-positive, platinum-resistant ovarian cancer (in combination with bevacizumab)	O'Malley et al., 2020)
Mirvetuximab soravtansine (IMGN853)	Folate receptor α Humanized antibody	DM4	Cleavable	Phase I	NCT01609556 ImmunoGen.	Relapsed epithelial ovarian cancer	(Martin et al., 2017)
Lifastuzumab vedotin (DNIB0600A)	NaPi2b Humanized IgG1 monoclonal antibody	MMAE		Phase II	NCT01991210 Genentech, Inc.	Platinum-resistant ovarian cancer	(Banerjee et al., 2018)
Mirvetuximab Soravtansine IMGN853	Folate receptor α Humanized monoclonal antibody	DM4	Cleavable	Phase I	NCT01609556 ImmunoGen.	Platinum-resistant ovarian, fallopian tube, or primary peritoneal cancer	(Moore et al., 2017b)
Mirvetuximab soravtansine (IMGN853)	Folate receptor α Humanized monoclonal antibody	DM4 3-4	Cleavable disulfide linker	Phase III	NCT02631876	Platinum-resistant ovarian cancer	(Moore et al., 2018b)
10. Cervical cancer							
Tisotumab Vedotin	Tissue factor (TF) Fully human monoclonal antibody	MMAE	Protease-cleavable linker	Phase I/II	NCT02001623 Genmab A/S	Recurrent or metastatic cervical cancer	(Hong et al., 2020)
11. Renal cell carcinoma							
AMG 172	CD27L Fully human IgG1κ monoclonal antibody	DM1 5	Non-cleavable 4-[N-maleimidomethyl] cyclohexane-1-carb oxylate conjugated to lysine residues	Phase I	NCT01497821 Amgen Inc.	Relapsed/refractory renal cell carcinoma	
AGS-16M8F and AGS-16C3F	ENPP3 Fully human IgG2a antibodies	MMAF	Non-cleavable	Phase I	NCT01114230 NCT01672775 Agensys, Inc.	Advanced refractory renal cell carcinomas	(Thompson et al., 2018)
SGN-CD70A	CD70	PBD	Cleavable	Phase I	NCT02216890 Genetics, Inc.	CD70-positive metastatic renal cell carcinoma	(Pal et al., 2019)
12. Prostate cancer							
PSMA ADC	Prostate-specific membrane antigen (PSMA) Fully human IgG1 monoclonal antibody	MMAE 4	Cleavable VC linker	Phase I	NCT01414283 Progenics Pharmaceuticals, Inc.	Chemotherapy-refractory prostate cancer	(Petrylak et al., 2019)
DSTP3086S	Six-transmembrane epithelial antigen (STEAP1) Humanized IgG1 monoclonal antibody	MMAE	Cleavable	Phase I	NCT01283373 Genentech, Inc.	Metastatic castration-resistant prostate cancer	(Danila et al., 2019)
ASG-5ME	SLC44A4 Fully human IgG2κ	MMAE	Cleavable MC-VC linker	Phase I	NCT01228760 NIH/NCI Cancer Center	Metastatic castration-	(McHugh et al., 2019)

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
PSMA ADC	monoclonal antibody PSMA Fully human IgG1 monoclonal antibody	MMAE	Cleavable VC linker	Phase II	NCT01695044 Progenics Pharmaceuticals, Inc	resistant prostate cancer Progressive metastatic castration-resistant prostate cancer	(Petrylak et al., 2020)
13. Epithelial cancers							
Sacituzumab govitecan (IMMU-132)	Trop-2 Humanized antibody	SN-38 (camptothecin)		Phase I/II	NCT01631552 Immunomedics, Inc.	Diverse epithelial cancers	(Ocean et al., 2017)
14. Melanoma							
Glembatumumab vedotin	Glycoprotein NMB Fully human IgG2 monoclonal antibody	MMAE	Cleavable VC linker	Phase II	NCT02302339 Celldex Therapeutics, Inc.	Advanced melanoma	(Ott et al., 2019)
15. Myeloma							
AMG 224	BCMA Human IgG1 antibody	DM1	Non-cleavable	Phase I	NCT02561962 Amgen Inc.	Relapsed or refractory multiple myeloma	(Lee et al., 2021)
DFRF4539A	FcRH5 Humanized IgG1 monoclonal antibody	MMAE	Cleavable MC-VC-PABC linker	Phase I	NCT01432353 Genentech, Inc.	Relapsed or refractory multiple myeloma	(Lee et al., 2021)
GSK2857916	B-cell Maturation antigen Humanized IgG1 monoclonal antibody	MMAF	Non-cleavable Protease-resistant MC linker	Phase I	NCT02064387 Glaxo SmithKline.	Relapsed or refractory multiple myeloma (BMA117159)	(Trudel et al., 2018; Trudel, et al., 2019)
Lorvotuzumab Mertansine (IMGN901)	CD-56	DM1	Cleavable disulfide linker	Phase I	NCT00346255	Relapsed and/or Refractory CD-56-positive multiple myeloma	(Ailawadhi et al., 2019)
16. Osteosarcoma							
Glembatumumab vedotin (CDX-011)	Glycoprotein non-metastatic B Fully human IgG2 monoclonal antibody	MMAE		Phase II	AOST1521 NCT02487979	Recurrent osteosarcoma	(Kopp et al., 2019)
17. Leukemia							
Camidanlumab tesirine	CD25 Humanized antibody	PBD dimer (SG3199)	Cleavable Cathepsin-valine-alanine linker	Phase I	NCT02588092 Therapeutics SA	Acute myeloid leukemia or acute lymphoblastic leukemia	(Goldberg et al., 2020)
Vadastuximab talirine (SGN-CD33A)	CD33 Monoclonal antibody	PBD dimer	Cleavable MC-VC linker	Phase I	NCT01902329 Genetics, Inc.	CD33-positive acute myeloid leukemia	(Stein et al., 2018)
Azacitidine and Gemtuzumab ozogamicin (GO)	CD33 Humanized IgG4 antibody	Calicheamicin		Phase I/II	NCT00766116 Celgene, Inc.	Relapsed acute myeloid leukemia	(Medeiros et al., 2018)
18. Glioma							
AMG 595	EGFRvIII Fully human	DM1 3-4		Phase I	NCT01475006 Amgen Inc.	Recurrent malignant	(Rosenthal et al., 2019)

ADC name	Tumor target Antibody	Payload DAR	Linker type	Clinical status	ClinicalTrials Identifier Sponsor	Indication	Reference
	monoclonal antibody					glioma expressing EGFRvIII	
Depatuxizumab mafodotin (ABT-414)	EGFR monoclonal antibody	MMAF	Non-cleavable MC linker	Phase I	NCT01800695 AbbVie	EGFR-amplified recurrent glioblastoma	(van den Bent et al., 2017)
ABT-414	EGFR Humanized recombinant IgG1κ monoclonal antibody	MMAF	Non-cleavable MC linker	Phase I	NCT02573324 NCT02343406 AbbVie	Glioblastoma	(Reardon et al., 2017)

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