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Feasibility and safety of tethered capsule endomicroscopy in patients with Barrett's esophagus in a multi-center study

Jing Dong^{1,2}, Catriona Grant¹, Barry Vuong^{1,2}, Norman Nishioka^{1,2}, Anna Huizi Gao¹, Matthew Beatty¹, Grace Baldwin¹, Aaron Bailargeon¹, Ara Bablouzian¹, Patricia Grahmann¹, Nitasha Bhat¹, Emily Ryan¹, Amilcar Barrios¹, Sarah Giddings¹, Timothy Ford^{1,2}, Emilie Beaulieu-Ouellet¹, Seyed Hamid Hosseiny¹, Irene Lerman¹, Wolfgang Trasischker^{1,2}, Rohith Reddy^{1,2}, Kanwarpal Singh^{1,2}, Michalina Gora^{1,2,3}, Daryl Hyun¹, Lucille Queneherve^{1,2}, Michael Wallace⁴, Herbert Wolfesen⁴, Prateek Sharma⁵, Kenneth K. Wang⁶, Cadman L. Leggett⁶, John Ponerros⁷, Julian A. Abrams⁷, Charles Lightdale⁷, Samantha Leeds⁷, Mireille Rosenberg^{1,2}, Guillermo Tearney^{1,2,8,9}

¹Wellman Center for Photomedicine, Massachusetts General Hospital, MA

²Harvard Medical School, MA

³ICube Laboratory, CNRS, Strasbourg University, France

⁴Division of Gastroenterology and Hepatology, Mayo Clinic Jacksonville, FL

⁵Department of Gastroenterology, Kansas City Veterans Administration and University of Kansas School of Medicine, MO

⁶Division of Gastroenterology and Hepatology, Mayo Clinic Rochester, MN

⁷Columbia University Irving Medical Center, NY

⁸Department of Pathology, Massachusetts General Hospital, MA

⁹Harvard-MIT Division of Health Science and Technology (HST)

Abstract

Correspondence: Guillermo Tearney, 55 Fruit Street, BHX 604A, Boston, MA. 02114. gtearney@partners.org, Tel: +1 (617) 724-2979, Fax: +1 (617) 726-4103.

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BACKGROUND

Tethered capsule endomicroscopy obtains high resolution images of the entire esophagus. We evaluate the feasibility and safety of OCT-TCE in patients with Barrett's esophagus in a multi-center study.

Background & Aims—Tethered capsule endomicroscopy (TCE) involves swallowing small tethered pill that implements optical coherence tomography (OCT) imaging, procuring high resolution images of the whole esophagus. Here, we demonstrate and evaluate the feasibility and safety of TCE and a portable OCT imaging system in patients with Barrett’s esophagus (BE) in a multi-center (5-site) clinical study.

Methods—Untreated patients with BE as per endoscopic biopsy diagnosis were eligible to participate in the study. TCE procedures were performed in unsedated patients by either doctors or nurses. After the capsule was swallowed, the device continuously obtained 10- μ m-resolution cross-sectional images as it traversed the esophagus. Following imaging, the device was withdrawn through mouth, and disinfected for subsequent reuse. BE lengths were compared to endoscopy findings when available. OCT-TCE images were compared to volumetric laser endomicroscopy (VLE) images from a patient who had undergone VLE on the same day as TCE.

Results—147 patients with BE were enrolled across all sites. 116 swallowed the capsule (79%), 95/114 (83.3%) men and 21/33 (63.6%) women ($p=0.01$). High-quality OCT images were obtained in 104/111 swallows (93.7%) who completed the procedure. The average imaging duration was 5.55 ± 1.92 minutes. A blinded comparison of maximum extent of BE measured by OCT-TCE and EGD showed a strong correlation ($r=0.77-0.79$). OCT-TCE images were of similar quality to those obtained by OCT-VLE.

Conclusions—The capabilities of TCE to be used across multiple sites, be administered to unsedated patients by either physicians or nurses who are not expert in OCT-TCE, and to rapidly and safely evaluate the microscopic structure of the esophagus make it an emerging tool for screening and surveillance of BE patients.

Keywords

Barrett’s esophagus; Optical coherence tomography; Tethered capsule endomicroscopy

INTRODUCTION

Barrett’s esophagus (BE) is a precursor of esophageal adenocarcinoma where normal esophageal squamous mucosa changes to metaplastic columnar mucosa in response to chronic acid reflux. Current standard of care relies on upper endoscopy with biopsy, also known as esophagogastroduodenoscopy (EGD). Since video images obtained by EGD only show the surface of the tissue at a macroscopic scale, targeting biopsies is imprecise and oftentimes diseased tissue is missed. One meta-analysis study with patients who had esophagectomies for high grade dysplasia (HGD) showed that 13 percent of the resection specimens had invasive cancer that was not detected by systematic biopsy¹. Swallowable wireless video capsule endoscopy², unsedated transnasal endoscopy³ and tethered capsule endoscopy⁴ do not require sedation, but like endoscopy, are limited to macroscopic visualization of the mucosal surface. Several advanced imaging techniques, including mucosal staining with vital dyes⁵ (chromoendoscopy), narrow band imaging^{6,7}, magnification endoscopy⁸, and confocal laser endomicroscopy⁹ have been proposed to enhance disease detection. Although these techniques increase the contrast of mucosal

features and increase diagnostic yield¹⁰, they all require sedated endoscopy, which is time consuming, expensive, and unpleasant for many patients.

Optical coherence tomography (OCT) is a cross-sectional imaging technique that uses principles of low-coherence interferometry to obtain depth-resolved, microscopic images of human tissue¹¹. A form of OCT called volumetric laser endomicroscopy (VLE)^{12,13}, uses a balloon probe that is inserted to the endoscope's accessory channel. Helically scanning optics¹⁴ obtain contiguous microscopic images of a 6-cm-long segment of distal esophagus^{12,13}. While VLE has the potential to mitigate sampling error, it is used in conjunction with sedated endoscopy.

Tethered capsule endomicroscopy (TCE), is a recently developed form of in vivo microscopy based on OCT technology^{15,16}. Once swallowed, the TCE device obtains three-dimensional microscopic images of the superficial esophageal wall as the capsule descends the organ via gravity/peristalsis or is pulled up towards mouth using the tether. OCT-TCE does not require sedation, obtains microscopic images of the entire esophagus, and is a faster and more convenient procedure. Our group and others have successfully conducted OCT-TCE in pilot, single-center studies^{15–19} showing exemplary images that demonstrate the potential of this technology to improve upper GI tract diagnosis by elevating diagnostic yield, lowering costs, and bettering patient tolerance. Here, we report our experience using a next generation OCT-TCE system and device in BE patients in a multi-center clinical study (Massachusetts General Hospital, Mayo Clinic Jacksonville, Kansas City VA, Mayo Clinic Rochester and Columbia University Medical Center).

MATERIALS AND METHODS

Technology

OCT tethered capsule with a distal scanning micro-motor—The OCT-TCE optics enclosed in the capsule includes a single mode optical fiber, a glass spacer and a distal ball lens fusion spliced together, providing approximately 30 μ m lateral resolution. At the distal end of capsule, a right-angle prism mounted on the shaft of a micro-motor^{20,21} deflects the optical beam to the side of the capsule. Rotation of the shaft effectuates circumferential scanning across esophageal layers. The capsule connects to a 1-mm-diameter, 2.0-m-long, flexible tether that houses an optical fiber and electrical wires to power the micro-motor. The tether contains pad printed distance marks at 5cm intervals. The overall size of the capsule is 11mm (diameter) \times 25mm (length), comparable to the size of a wireless video endoscopy capsule. A photograph of the TCE device is shown in Fig. 1A. TCE devices are multi-use; standard high-level disinfection (HLDI) is conducted between procedures.

Portable OCT imaging system—A picture of the portable OCT imaging system (size of a briefcase) is shown in Fig. 1B. Briefly, the imaging console's laser source consisted of a commercially available swept source-based OCT imaging engine (Axsun Technologies, Inc, Billerica, MA). This OCT laser source provides an axial resolution of approximately 7 μ m (tissue) over a ranging depth of 5mm. The OCT engine also contains an on-board digitizers and digital signal processing electronics, which allows compressed (JPEG2000, compression ratio 7:1) OCT images to be streamed across an Ethernet bus to a mini-PC

with a touchscreen monitor. The portable imaging system provides a motor control signal to the distal micro-motor of the TCE device for rotational beam scanning. Each cross-sectional OCT image consists of 2560 A-lines, acquires at a rotational rate of ~40 Hz, corresponding to a 40 frames/second (fps) cross-sectional imaging rate. The system was designed to be mass produced and easily maintained. This design allowed the imaging consoles to be rapidly manufactured, deployed to the various sites, and serviced.

Clinical study design

Patients—Patients eligible for the study had untreated, newly diagnosed BE or known BE without high grade dysplasia, intramucosal adenocarcinoma, or esophageal adenocarcinoma as per prior endoscopic biopsy diagnosis (within 9 to 15 months of baseline enrollment). Patients were over the age of 18 and capable of giving informed consent. Patients required minimal preparation, including no solid food for 4 hours prior to the procedure, and clear liquids 2 hours prior to the procedure.

Clinical procedure—All 5 sites were provided a portable OCT imaging system and at least 3 tethered capsule devices. Multiple training sessions regarding capsule and system operation, HLDI, and OCT image tissue type identification were provided to each site (See Supplementary Material and Fig. S1 for learning curves). Unsedated patients swallowed the capsule in a sitting position with an optional sip of water to facilitate swallowing the capsule. After the capsule was swallowed, patients were free to talk normally and were asked to occasionally sip water. Patients were given the option to use “Pill Glide Swallowing Spray”, a readily available over-the-counter water-based lubricating spray. When utilized, the spray was applied on the surface of capsule by capsule operator right before handing the capsule to the patient. Patients were also given the option of using an over-the-counter throat numbing spray such as “Cepacol”, “Chloraseptic” or “Topex”. When used, the spray was self-administered with the guidance of the study staff. Patients typically used the spray 5–10 minutes before the start of the procedure.

Once the capsule was swallowed, cross-sectional microscopic OCT images of the esophagus were obtained and visualized in real-time as the capsule traversed the esophagus. The capsule position was controlled manually via the tether outside of the patient’s mouth by the capsule operator. Operators were instructed to attempt to keep the tether’s translation at a constant velocity. The patient was optionally asked to take additional sips of water during the procedure to assist lower esophageal sphincter opening and capsule passage into the stomach. Typically, four passes of the esophagus were imaged, two during descent to the stomach and two pulling the tether up from the stomach towards the mouth. During each pass, similar to distance measurements that are performed during endoscopy, marks on the tether at the incisors (every 5cm) were recorded along with the real-time cross-sectional image frame number. During pull-back imaging, the TCE device was usually pulled from the gastric cardia to the 20cm tether mark at the incisors. After the imaging part was completed, the capsule operator removed the capsule from the esophagus through the mouth by gently pulling the tether. The procedural duration (the time between when the capsule was handed to the patient and the capsule was removed from patient) was recorded manually with a precision of 1 minute. The imaging duration (the time between

when the capsule was swallowed and the capsule was removed from the mouth) was automatically, computer-recorded with a precision of 1 second. Following imaging, patients who swallowed the capsule successfully were given a questionnaire about the tolerability of the TCE experience and were asked if they would prefer TCE over endoscopy and whether they would recommend the procedure to other patients. If the patient was not able to swallow the capsule after five attempts, the procedure ended, and the patients were provided a separate questionnaire that focused on capsule swallowing difficulties. Capsules were then disinfected prior to reuse.

Data collection

The study was approved by the Partners IRB (IRB 16-P000919) and the IRBs of each of the sites. Each of the four esophageal (2 down and 2 up) OCT imaging sessions were recorded to a separate file. Apart from OCT images, the medical data included patient demographics, medical history, procedure details, post-procedural questionnaires, and endoscopic and pathology reports were collected and managed using REDCap electronic data capture tools hosted at MGH²².

Data analysis

OCT images were only used for research purposes. The OCT files, collected in polar coordinates (distance, angle) were scan converted to cartesian coordinates and saved as 1024×1024 pixel movies after the procedure. OCT images were displayed in inverse gray scale, where black indicated a high OCT signal (high backscattering) and white indicated a low OCT signal (low backscattering). Tether marks and corresponding TCE frame numbers were used to calculate the imaged esophageal length as well as the capsule's velocity throughout each esophageal scan.

Two expert OCT readers (GJT, JD) evaluated the image quality of OCT-TCE images, including ensuring adequate image sensitivity, presence of cardia and esophagus in each run, sufficient tissue in the field of view, and visualization was not hindered by intraluminal contents or other artifacts caused by system or capsule malfunction. To compare the length of BE (maximum extent, Prague M measurement^{23,24}) measured by OCT-TCE and EGD, two readers blinded to the EGD reports identified the proximal and distal margins of BE in OCT-TCE movies with their corresponding frame number. Patients data were included in the analysis if: 1) the length of BE was indicated in EGD report, 2) at least two OCT-TCE datasets included OCT images of the distal esophagus, gastroesophageal junction, and proximal stomach, and 3) The capsule positions (tether marks at the incisors) were recorded along with their corresponding OCT-TCE frame numbers. The length of BE was calculated using the presumed velocity of the capsule, estimated by time stamps of tether mark readings. OCT-TCE images were compared to VLE images from a patient who had undergone TCE and VLE procedures on the same day (See Supplementary Materials, Fig. S3).

All statistical analyses were performed with GraphPad Prism 8 for macOS version 8.3.0 (GraphPad Software, Inc, La Jolla, CA). For datasets with a normal distribution, data were expressed as the mean ± standard deviation; for datasets that were not normally

distributed, data were expressed as median with interquartile range (IQR). The outliers were identified using ROUT algorithm with coefficient of 0.5% ($Q=0.5\%$). The flagged outliers were checked practically before being eliminated for statistical analysis. The association between gender, capsule operator, capsule lubricant or throat numbing spray and capsule swallowing rate were calculated using Chi-square test. The age and BMI difference between capsule swallows and non-swallows was compared with unpaired T-test. The differences in swallowing rates across all sites were compared with the Fisher's exact test. The relationship between BE length determined by EGD and OCT-TCE was calculated using linear regression. P values ≤ 0.05 were considered statistically significant. All authors had access to the study data and reviewed and approved the final manuscript.

RESULTS

To date, a total of 147 patients with BE have been successfully enrolled across all sites (MGH: 60, Mayo Jacksonville: 27, Kansas City VA: 25, Mayo Rochester: 20, Columbia University: 15). The average age was 64.8 ± 9.3 years old (min=33, max=83), and 114 were men (77.6%). The patient characteristics is listed in Table 1.

A total of 116 of 147 patients (79%) successfully swallowed the capsule (MGH: 82%, Mayo Jacksonville: 78%, Kansas City VA: 76%, Mayo Rochester: 70%, Columbia University: 87%). For data pooled across sites, sex was the only variable that was associated with statistically significant differences in swallowing rates (83.3% male, 63.6% female, $p=0.01$). No statistically significant associations between capsule swallowing rate and operator, the usage of capsule lubricant, or the use of throat numbing were found ($p=0.20$, 0.29 and 0.32 , respectively). The average age and BMI of capsule swallows was 64.8 ± 9.0 years old and 28.8 ± 4.6 kg/m², respectively, while for non-swallows it was 64.8 ± 10.3 years old and 29.2 ± 4.7 kg/m², respectively. There was no statistically significant age or BMI difference between capsule swallows and non-swallows ($p=0.98$ and 0.69 , respectively). The average length of BE diagnosed by endoscopy was 3.52 ± 2.56 cm based on 72 endoscopic reports of positive swallows where the length of BE segment was indicated, including 1 patient with a BE segment length smaller than 1cm, 44 patients between 1 to 3cm, and 27 patients greater than 3cm. 46/116 (39.7%) patients were diagnosed with a hiatal hernia. The TCE procedure was completed in 111 cases. 5 cases were terminated early because of technical issues, including 3 cases of capsule malfunction, and 2 cases of a wrong system setting. High-quality OCT images were obtained in 104 of 111 (93.7%) cases among the patients who completed the procedure, which was defined as acquiring at least one complete analyzable full scan during the procedure that typically showed distal esophagus, gastroesophageal junction, and proximal stomach. OCT-TCE images were not analyzable in 7 cases, including 6 cases of insufficient length of esophagus captured and 1 case where food particles prevented clear visualization of the esophagus.

A summary of the results from procedure and post procedural questionnaires is provided in Table 2. There were no adverse events associated with TCE procedure. The results showed that the majority (85.2%) stated that they likely preferred TCE over endoscopy, and 96.6% of patients would recommend TCE if it was approved for clinical use. The reusable TCE device was used 4.2 ± 3.8 times averaged across all participating sites. Histograms of capsule

number of swallow attempts, procedural duration, imaging duration, and post procedural questionnaire results are shown in Fig. S2.

Factors that interfered with the ability to swallow the capsule was assessed for patients who could not swallow the capsule. The major factors included the capsule size (n=22) and the presence of a tether (n=19). 13 non-swallowers reported an extraordinary strong gag reflex and 11 patients stated that fear of gagging also interfered with their ability to swallow the capsule. 5 patients stated that the throat numbing was insufficient, and 1 patient stated that the lubrication of the capsule was inadequate.

After the procedures, all datasets were sent to the study coordinating center (MGH), where the quality of the OCT-TCE images were assessed by readers who were experts in OCT. Images acquired had an average of 95.5% (95% CI: 94.1–96.8%) visible esophageal mucosa in the field of view based on OCT-TCE movies from 15% randomly selected patients who swallowed the capsule. Figure 2 shows example OCT-TCE images of healthy squamous of esophagus obtained from a study patient. The full thickness esophageal architecture including the epithelium, lamina propria/muscularis mucosa (LP/MM), submucosa (SM), muscularis propria (MM), myenteric plexus (MYP) and adventitia were seen.

Representative OCT-TCE images of BE without dysplasia are shown in Fig. 3(A,B). Images of non-dysplastic BE were devoid of squamous layering or pit and crypt architecture, had an irregular mucosal surface, and heterogeneous backscattering, consistent with previously published BE diagnostic criteria^{25,26}. Figure 3(C,D) depicts OCT-TCE images of dysplastic BE; dysplasia was confirmed by histology of biopsies obtained in their subsequent EGD procedures. OCT-TCE images of dysplastic BE showed glandular atypia (Fig. 3C), lack of epithelial surface maturation (Fig. 3D), also consistent with previously validated OCT criteria for dysplastic BE²⁷.

OCT-TCE provided data that was consistent with that obtained by consecutive endoscopy. We assessed BE length (maximum extent) from 40 BE patients who had analyzable OCT-TCE datasets and EGD reports. OCT-TCE and EGD measurements of BE extent showed a strong correlation ($r=0.77-0.79$, Fig. 4), which is comparable with OCT-TCE results previously published from a single-center study ($r=0.77-0.78$)¹⁸. TCE interobserver correlation was very strong ($r=0.91$). Of the 104 patients in this study who had analyzable OCT-TCE datasets, 1 patient had a biopsy with LGD and 1 patient had a biopsy showing focal HGD. Both patients with biopsy-proven dysplastic BE had OCT features consistent with dysplasia²⁷, as determined by OCT-TCE readers blinded to biopsy results. An additional 6 patients had biopsies that were read as IND. Of these patients, 4 showed OCT-TCE evidence of dysplasia²⁷.

DISCUSSION

In this paper, we have demonstrated the feasibility, safety, and patient tolerability of OCT-TCE in a multi-center clinical study. The device was customized for external multi-site use by making the imaging system robust and portable, and by including a micro-motor inside the capsule to scan the OCT light beam. Findings showed that this TCE technology

can be effectively used across multiple sites to evaluate the esophagus, retaining all of the advantages seen previously in other TCE pilot studies. Results, including BE length and dysplasia, were consistent with those obtained on subsequent EGD. In this multi-center study, after a comprehensive training tutorial, the TCE procedure was performed equally well in the hands of physicians and nurses. This feature may mitigate some of the cost and time associated with other procedures that require physician operation. The device is also reusable; the average number of times the capsule was used here (4.2 ± 3.8) was similar to that reported in a previously published single center study (4 ± 3 times)¹⁸.

Compared to prior studies that had successful TCE swallowing rates between 85% to 92%¹⁶⁻¹⁸, we found the overall successful swallowing rate of this study (79%) was slightly lower. Unlike the single center studies that were done in a small number of subjects by investigators who had developed the technology, here we sent the devices to sites that were naïve to TCE development and operation. Additionally, previously published studies¹⁶⁻¹⁸ included healthy volunteers and other types of subjects, which may also affect the overall swallowing rate. Swallowing rates were lower in some sites whereas in others they were higher (range 70%–87%), and the differences in swallowing rates between sites were not statistically significant ($p=0.75$). Nonetheless, averaged over all sites, the swallowing rate was near 80%, and the procedure was widely accepted and well tolerated by BE patients. In the questionnaire from non-swallowers, feedback indicated that the capsule size and the existence of a tether were the two major factors that interfered with swallowing. Reducing the capsule size and changing the material/diameter of the tether may improve swallowing rates and comfort.

Identification of BE tissue and dysplasia has been previously validated by OCT histopathologic correlative studies²⁵⁻²⁷. Using these same criteria, we were able to identify healthy squamous and BE tissues in the OCT-TCE images. One limitation of the current study is a lack of biopsy confirmation for the TCE findings. Such a study could be facilitated by incorporating TCE-based laser cautery marking (similar to VLE real-time targeting²⁸) that has been recently reported²¹ and uses the same imaging and capsule technology described here. Future studies are merited to validate this technology using standard endoscopic and histologic findings.

Other tethered capsule devices have recently been developed that detect BE using a sponge that collect cells scraped off the esophageal mucosal surface of unsedated patients, these cells are then sent off for molecular analysis that detects biomarkers indicative of BE or dysplasia²⁹⁻³¹. The format of these devices is similar to OCT-TCE technology described here and thus patient preparation, case utilization, and procedural times are comparable. Devices differ in interpretation, as the cells from sampling sponges are sent to clinical pathology labs, providing a gold standard result³². Sampling sponges are further along in their validation, with multiple studies showing good sensitivities/specificities compared to endoscopic biopsy^{31,33,34}. In contrast, OCT-TCE images are currently interpreted by expert readers, which is a limited resource. Thus, it is critical to develop automated image analysis algorithms to diagnose BE from OCT-TCE images in real time and this research is ongoing³⁵⁻³⁷. Studies with other forms of OCT^{12,13} have shown good sensitivity and specificity for BE^{13,38}, but the accuracy of OCT-TCE has not yet been

directly demonstrated. Both technologies offer analysis of the entire relevant portion of the esophagus, but OCT-TCE has the additional advantage of being able to localize BE anatomically, which may be useful for follow up treatment or to assess features such as the extent of BE (Fig. 4) or dysplasia. In addition, OCT-TCE provides information below the mucosal surface, thus allowing the detection of BE/dysplasia depth³⁹ or other anomalies such as buried BE and submucosal BE extension^{40,41}.

This study describes the extensibility of this technology to be utilized in multiple sites that are not expert in OCT-TCE, providing an understanding of the feasibility of OCT-TCE for broader utilization beyond the expert labs and for screening in general. Our experience with OCT-TCE technology in this multi-center clinical study demonstrates that this technology is safe and feasible for depth-resolved microscopic imaging of the entire esophagus in BE patients. High quality microscopic images of the entire esophageal wall were obtained in majority of the cases (93.7%) across the different sites, which is consistent with that reported in prior TCE studies^{16–18}. The high image quality, lack of sedation, ease of use, short procedure time, and patient acceptance of OCT-TCE procedure suggest that this technology has the potential to become a useful surveillance and screening tool for BE.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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FINDINGS

OCT-TCE is a safe and feasible procedure to be performed across multiple sites for rapidly obtaining depth-resolved microscopic images of the entire esophagus. It is capable of being administered to unsedated patients by either physicians or nurses, and has high patient acceptance.

Abbreviations:

BE	Barrett's esophagus
BMI	body mass index
CI	confidence interval
EGD	esophagogastroduodenoscopy
GERD	gastroesophageal reflux disease
HGD	high grade dysplasia
HLDI	high-level disinfection

IND	indefinite for dysplasia
IQR	interquartile range
Kansas City VA	Kansas City Veterans Administration
LGD	low grade dysplasia
LP	lamina propria
MGH	Massachusetts General Hospital
MM	muscularis mucosa
MP-ICL	inner circular layer of muscularis propria
MP-OLL	outer longitudinal layer of muscularis propria
MYP	myenteric plexus
OCT	optical coherence tomography
PPI	proton pump inhibitors
SM	submucosa
TCE	tethered capsule endomicroscopy
VLE	volumetric laser endomicroscopy

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IMPLICATIONS FOR PATIENT CARE

Owing to the merits of lack of sedation, ease of use, short procedure time, better patient comfort and high quality images, OCT-TCE technology is an emerging tool for screening and surveillance of BE patients.

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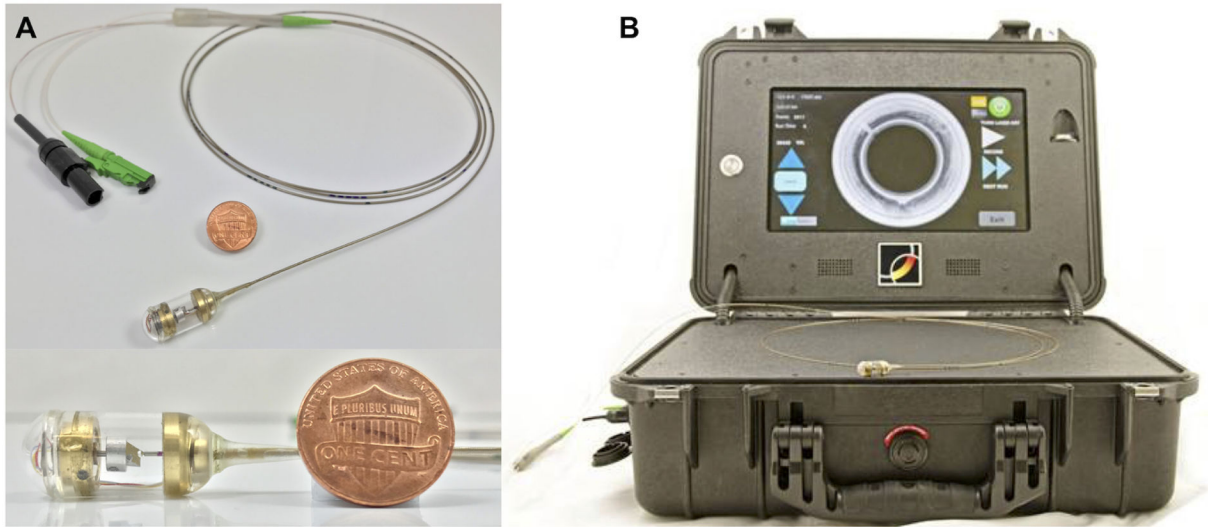


Figure 1. Photographs of (A) the OCT-TCE capsule with a micro-motor for distal scanning and (B) the custom-built, portable OCT imaging system.

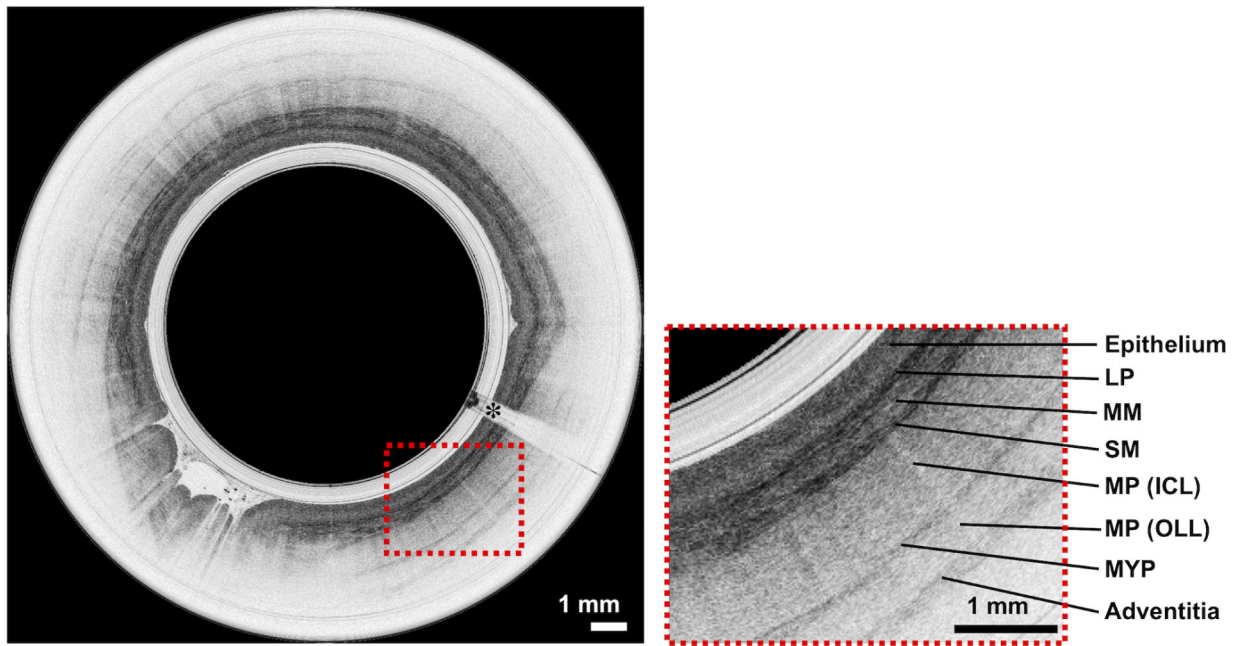


Figure 2. Representative surface and subsurface OCT-TCE microscopic images of esophagus obtained by TCE, showing layered tissue structure in the esophageal wall. Esophageal TCE images show epithelium, LP/MM, SM, inner circular layer of muscularis propria (MP-ICL), outer longitudinal layer of muscularis propria (MP-OLL), myenteric plexus (MYP) and adventitia. Scale bars, 1 mm. The asterisks indicate the image shadows caused by electrical wires that power up the distal micro-motor.

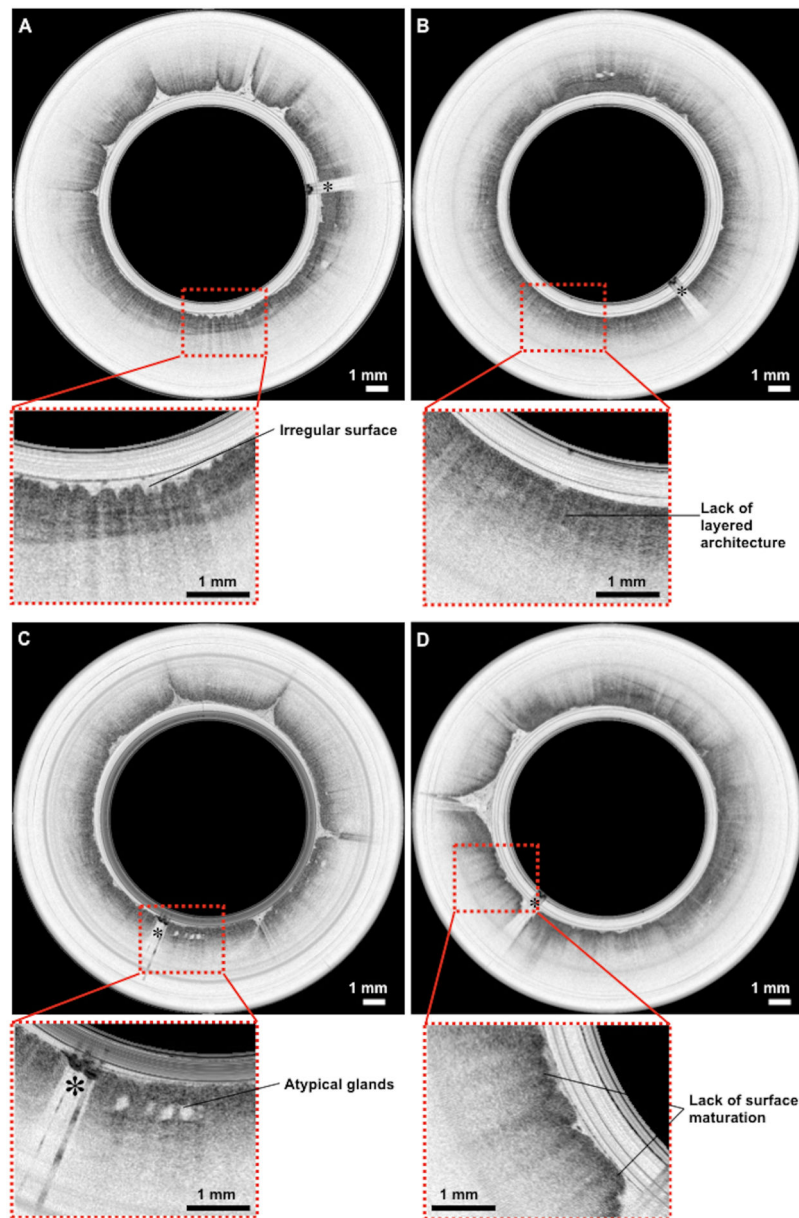


Figure 3. Representative OCT-TCE images of biopsy proven BE with and without dysplasia from different patients. OCT-TCE features consistent with non-dysplastic BE included an irregular surface (A) and a lack of layered squamous architecture or pit and crypt pattern, and heterogeneous scattering (B)^{25,26}. For dysplastic BE, OCT-TCE features were consistent with previously published criteria²⁷, including glandular architectural atypia (C) and lack of epithelial surface maturation (D), manifested as high superficial backscattering. Scale bar, 1 mm. The asterisks indicate the image shadows caused by electrical wires that power the distal micro-motor.

Maximum BE extent in EGD vs OCT-TCE

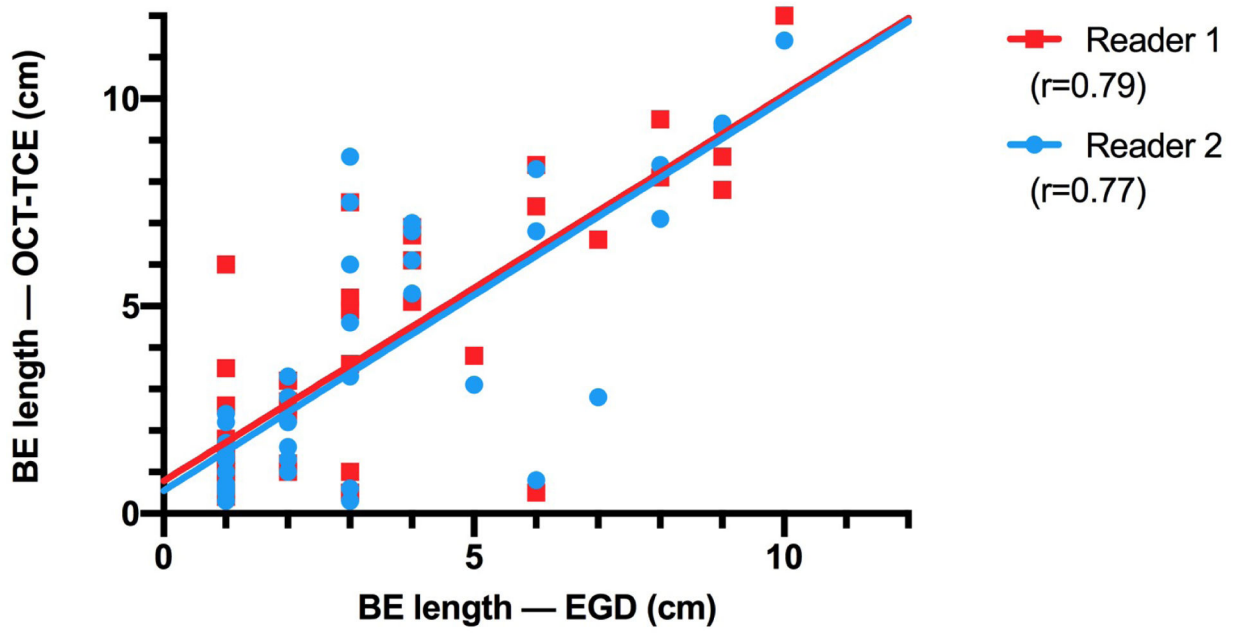


Figure 4. Scatter plot of maximum BE extent measured by EGD vs OCT-TCE.

Table 1.

Patient demographic characteristics and medical history

Characteristics	Number of patients	Mean \pm SD or %	Range
<i>Age at enrollment (years)</i>	147	64.8 \pm 9.3	33 – 83
<i>Gender</i>			
<i>Female</i>	33	22.4%	
<i>Male</i>	114	77.6%	
<i>Height (inches)</i>	147	68.6 \pm 3.5	60 – 76.5
<i>Weight (pounds)</i>	147	193.7 \pm 37.7	123 – 333.3
<i>Body mass index (BMI, kg/m²)</i>	147	28.9 \pm 4.6	19.6 – 43.3
<i>Ethnicity</i>			
<i>Hispanic</i>	5	3.4%	
<i>Non-Hispanic</i>	142	96.6%	
<i>Race</i>			
<i>Asian</i>	1	0.7%	
<i>African American</i>	1	0.7%	
<i>Caucasian</i>	145	98.6%	
<i>Smoking history</i>			
<i>Current smoker</i>	10	6.8%	
<i>Former smoker</i>	69	46.9%	
<i>Never smoked</i>	68	46.3%	
<i>History of GERD</i>			
<i>Yes</i>	125	85.0%	
<i>No</i>	22	15.0%	
<i>Use of proton pump inhibitors (PPI)</i>			
<i>Yes</i>	125	85.0%	
<i>No</i>	22	15.0%	

Table 2.

Summary of results of procedure and post procedural questionnaire.

Procedural results	No. of patients	%	Comments
<i>Operator</i>			
<i>Physicians</i>	75	51.0%	
<i>Registered Nurses</i>	72	49.0%	
<i>Usage of capsule lubricant</i>	142	96.6%	
<i>Usage of throat numbing spray</i>	55	42.0%	Of 131 patients who were provided throat numbing spray option
<i>Capsule swallower</i>	116	79%	
<i>Completed OCT image acquisition</i>	111	95.7%	Of 116 capsule swallowers
<i>High quality analyzable OCT images</i>	104	93.7%	Of 111 completed image acquisition
	Median	Interquartile range	Comments
<i>No. of capsule swallowing attempts</i>	1	1 – 2	
	Mean ± SD	Lower 95% CI of mean	Upper 95% CI of mean
<i>Procedural duration (min)</i>	7.98 ± 2.93	7.40	8.56
<i>Imaging duration (min)</i>	5.55 ± 1.92	5.17	5.93
<i>Length of esophagus imaged (cm)</i>	21.69 ± 5.90	21.12	22.27
<i>Average traverse speed (mm/s)</i>	4.16 ± 2.31	3.93	4.38
Post procedural questionnaire	Median	Interquartile range	Scale
<i>Overall level of discomfort</i>	2	1 – 4	0 = none 10 = severe
<i>Would you prefer it over endoscopy</i>	1	1 – 2	1 = extremely likely 2 = somewhat likely 3 = somewhat unlikely 4 = extremely unlikely
<i>Would you recommend it if it is approved for clinical usage</i>	1	1 – 1	1 = definitely 2 = probably 3 = probably not 4 = definitely not