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Extracellular Vesicles as an Advanced Delivery Biomaterial for Precision Cancer Immunotherapy

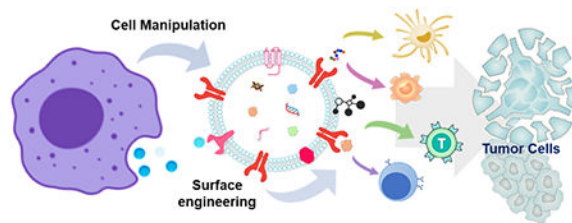
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Abstract

In recent years, cancer immunotherapy has been observed in numerous preclinical and clinical studies for showing benefits. However, due to the unpredictable outcomes and low response rates, novel targeting delivery approaches and modulators are needed for being effective to more broader patient populations and cancer types. Compared to synthetic biomaterials, extracellular vesicles (EVs) specifically open a new avenue for improving the efficacy of cancer immunotherapy by offering targeted and site-specific immunity modulation. In this review, the molecular understanding of EV cargos and surface receptors, which underpin cell targeting specificity and precisely modulating immunogenicity, are discussed. We review unique properties of EVs in terms of their surface markers, intravesicular contents, intrinsic immunity modulatory functions, and pharmacodynamic behavior *in vivo* with tumor tissue models, highlighting key indications of improved precision cancer immunotherapy. Novel molecular engineered strategies for reprogramming and directing cancer immunotherapeutics, and their unique challenges are also discussed to illuminate EV's future potential as a cancer immunotherapeutic biomaterial.

Graphical abstract



Cancer immunotherapy is the game changer in treating cancers. However, only a small population of patients could respond well, which highlights the urgent need of novel immunity modulators. Extracellular vesicles as the natural biomaterial open a new avenue for improving the efficacy of cancer immunotherapy by offering targeted and site-specific immunity modulation.

Keywords

Extracellular Vesicles; Exosomes; Delivery Biomaterials; Cancer Immunotherapy

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Conflict of Interest

The authors declare no conflict of interest.

1. Introduction

Cancer immunotherapy, as a next-generation cancer treatment strategy, is currently attracting great attention[1]. Important breakthroughs within this field, including chimeric antigen receptor T-cell (CAR-T) therapy[2, 3], immune checkpoint blockade therapy [4–6] (e.g. anti-cytotoxic T lymphocyte antigen 4 (CTLA4), anti-programmed cell death 1 (PD-1), and anti-programmed cell death ligand 1 (PD-L1)), have further promoted massive efforts in exploring progressively more efficient immunotherapeutic strategies. However, the major challenge in the development of novel cancer immunotherapy still lies in the limited dosages, constrained by inherent life-threatening side-effects often due to uncontrolled immunity modulation. In particular, rapid elimination and degradation, non-specific distribution, and insufficient antigen uptake or presentation of immunotherapy agents during the delivery process are reported as the key hurdles in immunity activation[7]. Therefore, delivering immunotherapeutic agents to specific tissues or cells for precisely inducing anti-tumor immunity is of great importance in improving efficacious immunotherapy. Biomaterials, including nanoparticles, biodegradable implants, biomaterial scaffolds, and cell-derived extracellular vehicles (EVs), have been widely used for delivering a variety of bioactive cargos and immunotherapeutic agents[8–10]. Increasing interests are centering towards leveraging biomaterials as immunomodulatory agents. Different from synthetic biomaterials, EVs are natural nanovesicles secreted from a variety of cells, which are particularly attractive for dual acting as both delivery platforms and immunomodulatory agents.

EVs are heterogeneous groups of membrane-bound vesicles. These consist of exosomes, microvesicles (MVs), and apoptotic bodies, which all are secreted by most living cells[11]. Among those vesicles, endosome-originated exosomes (30-150nm in diameter) and cytoplasmic membrane-originated MVs (larger than 100nm) have been widely investigated. Due to substantial size overlap, assigning EVs to a specific biogenesis pathway remains extraordinarily challenging. Thus, in this paper, the generic term: EVs, will be used in compliance with the 2018 guidelines from the *International Society of Extracellular Vesicles* (“MISEV”)[12]. Depending on the cell of origin, EVs carry a characteristic composition of bioactive molecules, including proteins, lipids (e.g. cholesterol, ceramides), nucleic acids (e.g. DNAs and RNAs) and metabolites (e.g. amino acids and ATP). EVs can transfer these bioactive molecules from donor cells to recipient cells, acting as a novel mode of intercellular communication[13]. The bioactive molecules effectively alter the biological response and phenotypic features of the recipient cells, thereby playing an important role in numerous physiological and pathological processes, such as immunity regulation, signal transduction, and tumorigenesis[14]. However, successful EV-mediated intercellular communication requires delivery of the bioactive molecules and precise docking onto the target cells. The surface of EVs are enriched with numerous transmembrane proteins, such as tetraspanins, integrin, and intercellular adhesion molecule-1 (ICAM-1), which grant EVs the exceptional ability to target specific cells or tissues[13]. In addition to their intrinsic targeting abilities, EVs offer significant advantages over synthetic biomaterials, including excellent biocompatibility, prolonged circulation time, flexible drug loading abilities, and controllable biological properties, positioning EVs more advantageously for

drug delivery purposes[15]. Thus, EVs demonstrate great potential as drug delivery systems to improve cancer immunotherapy, which has attracted a few review efforts to cover different challenging aspects, such as the tumor cell interaction with immune cell-derived EVs[16], therapeutic delivery[17], isolation and engineering of therapeutic EVs[18, 19], and fundamentals of tumor-derived EVs[20]. However, an in-depth understanding of EV intrinsic immunomodulatory function and their impact on using it as a delivery system has not been discussed, and our review intends to fill up this gap, focusing on the intrinsic role of EVs in immunomodulation, including the active and suppressive role within cancer immunity.

Moreover, EVs that are secreted by specific cells, including cancer cells, immune cells, and other non-immune host cells, may possess immunoregulatory potential while concurrently serving as a drug delivery system[21]. However, the immunoregulatory function of EVs derived from different cell origins are distinct, resulting in antigen presentations for either immune activation, suppression, or immune tolerance. For instance, EVs derived from dendritic cells (DCs) can stimulate the immune response by trafficking functional major histocompatibility complexes (MHC) and co-stimulatory molecules that activate antigen-specific T cell and B cell responses[22, 23]. DC-derived EVs (DEVs) pulsed with tumor peptides are capable of eradicating established murine tumors in a T cell-dependent manner[24]. Meanwhile, using tumor-derived EVs, as a source of neoantigens for internalization by DCs, could cross-prime CD8+ T cells, leading to the rejection of syngeneic and allogeneic murine tumors[25]. Thus, the EVs with immunoregulatory abilities can operate as potent therapeutics to develop cancer immunotherapy. Currently, several EV-based therapies have reached clinical trials, with three completed Phase I clinical trials and one completed Phase II clinical trial as summarized in Table 1.

Although great efforts have been devoted to understanding the intrinsic biological function of EVs, their potential to be leveraged or engineered for advanced cancer immunotherapy remains largely unexplored. In efforts to boost the efficacy of various immunotherapies, while circumventing immunoresistance and reducing off-target side-effects, rational engineering of EVs for advanced cancer immunotherapy is greatly required. In this review, we shed light on the application of EVs as drug delivery systems and immunoregulatory agents for targeting modulation of anti-tumor immunity. We begin with a description of the unique EV properties as a natural biomaterial, discussing resulting advantages over other synthetic biomaterials, such as liposomes and micelle nanoparticles. Secondly, we discuss the intrinsic immunoregulatory function of EVs regarding the immune system corresponding to the tumor microenvironment. We also discuss current strategies for circumventing and/or overcoming the immunosuppressive function, with a summary of published EV markers from the past 20 years, as well as their different sources in cells, for guiding proper selection of modulation targets. Lastly, we highlight several state-of-art applications of EVs in targeted cancer immunotherapy, including modifying and engineering EVs for significantly promoting delivery efficacy and immunostimulatory functions. The future potential and challenges are discussed with manufacturing and clinical translation practices.

2. EVs as an Advanced Delivery Biomaterial

Due to the intrinsic phospholipid bilayer, EVs are generally stable in maintaining their structural integrity for prolonged periods of time *in vivo*. Sokolova et al. [30] reported that EVs stored in phosphate-buffered saline at $-20\text{ }^{\circ}\text{C}$ were stable for longer times than EVs stored at $4\text{ }^{\circ}\text{C}$ and $37\text{ }^{\circ}\text{C}$, indicating that storage temperature is a key factor in maintaining EV stability. Kalra et al. stored LIM1863 colon cancer cell derived-EVs in plasma at $37, 4, -20$ and $-80\text{ }^{\circ}\text{C}$. The lower storage temperatures ensured higher stability, with the EVs that were stored at $-80\text{ }^{\circ}\text{C}$ exhibiting the greatest stability[31] and retained the clinical usability after 5 months of storage[32]. In addition to EVs' self-stability, EVs also can protect the endogenous or exogenous protein and RNA cargos from enzymatic degradation (e.g., proteases and RNases), which leads to excellent stability of drugs during *in vivo* delivery. For instance, Curcumin self-assembling into the lipid layer of EVs via hydroscopic interactions, result in increased drug stability, solubility and bioavailability[33].

For intravenously administrated EV-based drug delivery systems, the delivery efficiency to the target cells is highly related to the *in vivo* circulation time of the system. Compared to synthetic nanoparticles, EVs with their intrinsic properties are more likely to possess longer circulation times without further optimization or modification. Synthetic nanoparticle delivery systems are limited to rapid clearance and non-specific biodistribution due to rapid opsonization-mediated recognition and phagocytosis by mononuclear phagocyte system (MPS)[34–36]. Several factors, including size, shape, surface charge, and surface property, are reported to play important roles in determining the opsonization, and subsequent MPS capture in these systems[37]. For instance, positively charged nanoparticles are more likely to absorb and aggregate with plasma proteins, contributing to their rapid MPS capture and limited circulation time[38]. In contrast, EVs essentially possess a negative surface charge due to their phospholipid bilayer, which is beneficial in reducing protein absorption, leading to prolonged circulation time[39]. Additionally, EV surface proteins could help evading MPS recognition and clearance[40–43]. An example is CD47, an integrin-associated transmembrane glycoprotein. CD47 plays a critical role in evading macrophage phagocytosis through the interaction of CD47's extracellular domain with CD172a (also known as signal regulatory protein- α , SIRP α) on the macrophages, leading to the activation of the “don't-eat-me” signal transduction pathway[44]. Moreover, isolated EVs can be functionalized with CD47 by specific conjugation strategies, resulting in an increased MPS-escaping ability[45].

Several early clinical trials have evaluated the effects of autologous DC-EVs for cancer immunotherapy and allogeneic mesenchymal stem cell derived EVs for regenerative and anti-inflammatory applications[46]. The majority of these trials reported only mild side effects, indicating that the administration of EVs from these specific cell sources are safe and well tolerated[47]. EVs are also secreted into circulation by all cell phenotypes within the body, leading to an extreme abundance in blood and plasma, with notable concentrations as high as 10^{10} EVs per mL. Amazingly, seriously adverse immune reactions following plasma and blood transfusions were infrequently reported, suggesting these allogeneic EVs are considerably safe[48]. These clinical trial efforts are establishing an excellent biocompatible delivery platform centered on using EVs

3. Intrinsic Immunological Role of EVs

The innate immune system and the adaptive immune system are critical mechanisms for regulating immune responses[49]. They control tumor initiation, progression, and metastasis. Although the intercellular communication between immune cells and tumor cells has been reported by engaging interleukins, chemokines, interferons, and other signaling molecules[50], accumulated studies suggest that EVs secreted from both immune cells and non-immune cells play distinct roles in regulating tumor immunity to form a cancer-immunity cycle (Figure 1), including antigen presentation, antigen transfer, innate and adaptive immune activation, immune suppression, and anti-inflammatory effects[51, 52]. Thus, rationally selecting EV populations with their intrinsic immunomodulatory function is crucial for delivering immunotherapeutic agents, which can further potentiate therapeutic efficacy.

3.1 EVs as Mediators for Innate Immunity

Both tumor cell-derived EVs (TEVs) and immune cell-derived EVs play a positive role in regulating innate anti-tumor immunity. TEVs bearing heat shock protein 70 (HSP70) and other specific antigens can directly activate nature killer cells to promote the production of tumor necrosis factor- α (TNF- α) within macrophages[53, 54]. In addition, TEVs can promote the conversion of immune cells, such as DCs and macrophages, into pro-inflammatory cells at tumor-draining lymph nodes. This conversion leads to an increased production of pro-inflammatory cytokines (i.e. IL-6, IL-12, and interferon (IFN)- γ), while reducing anti-inflammatory cytokines (i.e., IL-10)[55].

Contrastively, EVs derived from natural killer (NK) cells, macrophages, and DCs have been described as pro-inflammatory mediators via paracrine messengers acting on the innate immune system[56]. DC-EVs are reported to express HLA-B-associated transcript 3 (BAT3), TNF superfamily members (TNF, TRAIL, Fas ligand (FasL)) as well as IL-15R, which can bind directly to corresponding surface receptors (NKG2D receptor) on NK cells[55, 57, 58]. The binding affinity of NK cells directly enhances their cytotoxic activity. Macrophage-derived EVs may play multiple roles in regulating innate immunity via either inducing macrophage differentiation or modulating the proliferation of myeloid cells[59]. Moreover, EVs released by pathogen infected macrophages (e.g., *Toxoplasma* or *Mycobacterium tuberculosis*-infected[60], lipopolysaccharide (LPS)-stimulated[61], or oxidized low-density lipoprotein (oxLDL)-stimulated[62]) were reported to induce maturation of DCs, also promoting pro-inflammatory cytokine secretion.

3.2 EVs as Mediators for Adaptive Immunity

To ensure an effectively adaptive anticancer immune response, a series of stepwise cellular events are initiated and expanded iteratively[63, 64] as shown in Figure 1. The cycle of tumor-immune cell interactions was generally considered to be manipulated by immune cells, including antigen presenting cells (APCs) and T cells against tumor cells. Recently accumulated evidence has indicated that immune cell derived EVs may play a similar role in procedurally maintaining the cancer-immunity cycle as their parent cells. TEVs containing various antigens from their parent tumor cells can be taken up by APCs, horizontally

transferring to differently surrounding APCs and subsequently presenting to T cells, thereby activating anti-tumor immune responses[14, 20, 51, 65]. For example, Wolfers et al. first reported that TEVs could effectively cross-prime cancer-specific cytotoxic T lymphocyte (CTL) immunity on syngeneic and allogeneic established mouse tumors[25] during this antigen presentation process.

APC (e.g. DCs and macrophages)-derived EVs were found to express MHC-I, MHC-II, and T cell co-stimulatory molecules (e.g. CD80, CD86) on their surfaces for direct presentation to effector T cells (naïve CD4⁺ T cells or CD8⁺ T cells), establishing immunity activation both *in vitro* and *in vivo*[66, 67]. It is worth mentioning: The efficiency of T cell activation by APC-derived EVs is highly relevant to the maturation status of APCs[68]. For instance, EVs secreted by mature DCs are more effective in inducing T cell activation *in vitro* and *in vivo*, than those secreted by immature DCs[69]. Immature DCs secreted EVs can only induce effector anti-tumor responses when co-injected with adjuvants or pre-loaded into recipient DCs. APC-derived EVs, unlike their parent cells, displayed a limited ability to directly induce T cell priming *in vivo*[23], partially due to an internalization by surrounding APCs through horizontally transferring MHC-antigen complexes. As a consequence, these antigen-bearing APCs can present to specific T cells, acting as an indirect or cross-presentation bearer[70–72].

In addition to APC-derived EVs, B cell-derived EVs are also involved in the presentation of antigenic activation of T cells. Raposo et al. reported that the Epstein-Barr virus-transformed B cells secreted EVs carrying antigen-MHC- II complexes, which could be presented to CD4⁺ T cells for immune-activation[73]. Subsequently, activated antigen-specific T cells will clone, proliferate, and migrate from lymph nodes into the circulatory system, thereby targeting tumors for specific killing. Alternatively, activated effector T cells may also secrete EVs carrying T cell receptors (TCR) to specifically recognize cognate tumor cells, or stimulating autologous resting T cells, further enhancing the immune response[74]. Valadi et al. reported that CD3⁺ T cell-derived EVs were involved in the stimulation and proliferation of resting CD3⁺ T cells, as well as CD8⁺ T cells, when combined with IL-2[75].

3.3 EVs-Mediated Immune Suppression and Evasion

Although TEVs can have indefinite immune-activating potential, conjunctively, they play a critical role in evading immune surveillance and suppressing anti-tumor immune responses: Resulting in pro-tumorigenesis, angiogenesis, and metastasis[76]. Specifically, TEVs carrying NKG2K ligands or transforming growth factor β 1 (TGF- β 1) on their surfaces can reduce NKG2D receptor expression on both NK cells and CD8⁺ T cells, leading to the neutralization of innate immune surveillance and adaptive immune response[77–79]. Other regulatory factors, such as FasL[80], TRAIL (TNF-related apoptosis-inducing ligand)[81, 82], and PD-L1[83–85], are also presented on the surface of TEVs and are involved in inhibiting T-cell proliferation, infiltration, and response by inducing the apoptosis of T cells or accelerating T cell exhaustion. Additionally, TEVs play an important role in promoting regulatory T (Treg) cell expansion by transferring TGF- β , a critical cytokine that mediates the suppression of CD8⁺ T cells and the proliferation of Foxp3⁺ Treg[86]. Moreover, tumor-derived EVs are shown to inhibit the differentiation of myeloid precursors into DCs, while

also promoting the differentiation of myeloid-derived suppressor cells (MDSCs) through the interaction of HSP72 on EVs with TLR2 on MDSCs[87–89]. Similarly, TEVs enriched with miRNA, such as miR-21-3p, miR-125b-5p, and miR-181d-5p, potentially induce the polarization from anti-tumor M1-like tumor-associated macrophages (TAMs) to pro-tumor M2-like TAMs[90]. However, it should be noted that the role of TEVs in suppressing anti-tumor immunity is heterogeneous and highly dependent on cancer type, genomic characteristics, and apparent stage[30]. Apart from TEVs, EVs derived from other cells may also possess the potential to suppress the anti-tumor immune response. For instance, EVs derived from immature DCs have been reported to suppress peripheral immune responses in transplanted models and in mice with autoimmune diseases[91, 92]. EVs derived from T cells[93, 94], MDSCs[95, 96], and M2-like TAMs[97–99] were also shown notably functioning in suppressing the anti-tumor immune response. For example, EVs derived from CD4⁺ T cells inhibited the CD8⁺ CTL response and anti-tumor activity against OVA-expressing B16 melanoma[100]. Further, EVs derived from activated CD8⁺ T cell were reported to express FasL, which could promote the invasion of the murine melanoma cell line B16 and the Lewis lung cancer cell line via Fas signaling pathways[101]. In another study, Xie et al. reported that EVs derived from CD8⁺ T cells can be endocytosed by APCs through MHC-I/TCR interactions, inhibiting DCs mediated antigen-specific CD8⁺ CTL responses[102]. In summary, developing an EV-based delivery system or immunotherapeutic platform requires a deep understanding of EV intrinsic immunomodulatory effects for precise control of their *in vivo* behavior.

EV-mediated immune suppression critically impedes cancer immunotherapy. Especially for TEVs, the robust strategies for overcoming or circumventing the potential immunosuppression might be beneficial for an elevated anti-tumor immunotherapy. It has been reported that blocking PD-L1 can reserve the immunosuppressive effect of PD-L1⁺ TEVs[83] [103]. However, whether the binding of anti-PD-L1 antibodies to PD-L1⁺ TEVs can affect the binding of antibodies to PD-L1 on the tumor cell surface remains unclear. Thus, more precise manipulation in reducing or removing the expression of PD-L1 on TEVs is highly desired. Poggio et al. demonstrated that deleting two important exosomal biogenesis genes (Rab27a and nSMNase2) can suppress exosomal PD-L1 expression, leading to a significant anti-tumor immune response and memory immunization [85]. Furthermore, Li et al. demonstrated that GW4869 and Nexinhib-20, two small molecular inhibitors towards Rab27a and nSMNase2, could also suppress exosomal PD-L1, leading to similar *in vivo* antitumor effects in MC38 models [104]. Such removal of PD-L1⁺ EVs could directly contribute to enhanced antitumor immunity. However, it should be noted that small molecule inhibitors might not guarantee the removal of PD-L1⁺ EVs in all cell lines. Due to robust adaptability, simplicity and efficiency, CRISPR-Cas9 technology has been of great interest for modulating gene-specific immunosuppression[105]. On the other hand, EVs derived from mature DCs have been shown to possess high potency towards priming CTL and inducing anti-tumor immunity, leading to the clinical utility of stimulated DC EVs in cancer immunotherapy [69]. For example, EVs derived from IFN- γ -matured DCs exhibited a stronger antitumor Th1 immune response than those derived from immature DCs, regardless of isolation methods and size[106]. Due to the antitumor function of M1-like TAMs, EVs derived from M1-like TAMs are also reported to potentiate antitumor

immunity [107, 108]. Cheng et al. found that EVs derived from M1-like, not M2-like, enhanced activity of a lipid calcium phosphate nanoparticle-encapsulated Trp2 vaccine, resulting in a stronger antigen-specific cytotoxic T cell response [107].

4. EV Delivery for Tissue and Cell Targeting

EVs have intrinsic tissue and cell-targeting capabilities due to the expression of a broad spectrum of membrane proteins or molecules on their surfaces, such as integrins, tetraspanins, lactadherin, and immune-related molecules[109]. It should be noted that the organotropic and tumor-targeting properties of certain EVs depend on their composition and origin[109, 110]. For instance, Hoshino et al. reported that EVs derived from different tumor cells exhibit different integrin expression profiles, which could mediate tumor metastasis to different organ sites. EVs expressing integrin $\alpha_6\beta_6$ and integrin $\alpha_6\beta_1$ can target lung-resident fibroblasts and epithelial cells. In contrast, EVs expressing integrin $\alpha_v\beta_5$ can specifically target liver-resident Kupffer cells[111]. Tetraspanins are a superfamily of 33 transmembrane proteins, which are also overexpressed on the surface of EVs for cellular targeting. Rana S et al. reported that tetraspanin8 interacts with integrin α_4 to form span8-integrin α_4 complexes, which could drive EVs trafficking towards CD54-expressing endothelial and pancreatic cells[112]. Studies also demonstrated that CD63-expressing EVs specifically bind to neuronal and glial cells, whereas CD63-negative EVs only reside in the dendrites of neurons[112, 113]. In addition, EVs derived from immune or tumor cells are also endowed with insidious capabilities for targeting immune cells: For example, DC EVs carry multiple proteins from the parent cells, including MHC-I, MHC-II, lactadherin, tetraspanins, integrins, ICAM-1, milk fat globule-epidermal growth factor 8 (MFG-E8), and costimulatory and adhesion molecules, such as CD80, CD88, CD83 and CD40[114]. DC EVs have been widely proven to be capable of targeting and presenting antigens to CTLs, leading to the activation of an immune response[72, 115, 116]. DC EVs were also found to transfer these immune-related molecules to cognate DCs for maturation[117]. Similarly, EVs derived from CTLs[75], NK T cells[118], or chimeric antigen receptor T (CAR-T) cells[119] exhibited tumor cell-targeting abilities for precise killing. We summarize the specific EV markers reported from the past 20 years for tissue and cell targeting in Figure 2, which illustrates the exponentially growing interests, particularly in tumor or blood associated EVs with more significant markers identified, such as CD63, TGF- β , and CD9. The more representative EV surface markers specific to disease type and tissue tropism are summarized in Table 2.

Maximizing designed targeting efficiency and specificity strategies, EVs can be genetically engineered, post-isolation, to introduce certain tissue- or cell type-specific targeting ligands on their surface at the cellular level[136]. The EV producing cells can be transfected with expression plasmids that encode EV transmembrane proteins, fused with a target of interest (e.g. ligand/homing peptide/signaling peptide). The relevant technique was first reported by Alvarez-Erviti et al to transfect DCs, with the plasmid encoding a lysosome-associated membrane glycoprotein 2 (Lamp-2b) fused with rabies viral glycoprotein (RVG), a central nervous system-specific peptide that can specifically recognize acetylcholine receptors[125]. The external leaflet of the secreted EVs were enriched with Lamp-2b-RVG, these EVs were then loaded with therapeutic siRNA via electroporation after post-isolation. *In vivo* studies

showed that the RVG-carried EVs could efficiently cross the blood-brain barrier (BBB), delivering to neurons and glia cells following intravenous injection, eventually resulting in significantly higher gene silencing than compared to non-targeted EVs [125]. The targeting peptides on EV surfaces, such as EBV glycoprotein 350 for targeting CD19⁺ B cells, has been widely studied since then [126], including the iRGD fused with Lamp-2b for targeting α_v -integrins and neuropilins of tumors [124], and interleukin 3 (IL-3) fused with Lamp-2b for targeting IL3 receptors on chronic myeloid leukaemia cells [127]. In addition to Lamp-2b, other transmembrane proteins have been used, including tetraspanins (CD63, CD9, CD81), glycosyl-phosphatidyl-inositol (GPI), platelet-derived growth factor receptors (PDGFRs), and lactadherin C1C2 domain [136, 137]. Among these, lactadherin's C1C2 domain, which can bind non-covalently to membrane phospholipids, has been widely used as a fusion partner [128]. However, researchers were more interested in using lactadherin's C1C2 domain to fuse with antigens or soluble proteins for targeting immune cells, such as T cells [130–132] and B cells [128].

Apart from EVs intrinsic or engineered targeting traits, intravenously administered EVs may also demonstrate passive targeting mechanisms due to their potential to cluster at tumor sites via the enhanced permeability and retention (EPR) effect. As a consequence, EV-based delivery systems may have the potential to deliver immunoregulatory agents to specific cells within a tumor site. It should be noted that the application of the EPR effect is highly dependent on both the pathological condition of the tumor, such as its neovasculature density, and the physicochemical properties of EVs, including size and shape [138]. The rapid development of tumors is often accompanied by the formation of neovasculatures, which are often immature and irregular, with large intercellular pores being potentially leaky between the endothelial cells (10–1000 nm) [139]. Therefore, near-spherical EVs with a size of 30–150 nm can extravasate from the intercellular pores and diffuse into the interstitial space of the tumor. Meanwhile, the absence of functional lymphatic vessels, in most tumors, contributes to EVs entrapment and retention, referred to as the EPR effect [140]. However, this mechanism has lower cell-targeting specificity and may cause non-specific distribution with unwanted off-target effects. Therapeutic potential when employing the EPR effect can be further improved through rational designs of EV-based delivery systems or combining the EPR effect with active-targeting functionality.

Lymph nodes (LNs) are a primary organ of the immune system, containing a large fraction of immune cells, such as T cells, B cells, and APCs [141]. LNs provide a specialized microenvironment to gather immunogenic information from peripheral tissues, regulating the adaptive immune response of the body [142]. Unsurprisingly, LNs are attractive therapeutic targets for the treatment of a variety of unmet clinical needs, including cancer. One of the most widely used immunotherapies based on LNs-targeting delivery is the conventional vaccine, which can be localized to LNs-resident APCs or lymphocytes after reaching the LNs. Conventional vaccines are usually administered peripherally, in which free antigens and/or adjuvants are transported from interstitial spaces to downstream LNs via lymphatic vessels [143]. However, several challenges, including rapid degradation, limited circulation time, and the unique physiology of LNs may hinder high concentrations of therapeutics from reaching LNs. Encouragingly, EV-based vaccines are a promising alternative due to their improved delivery performance. Similar to the size-dependent EPR

effect for tumor targeting, the delivery of EVs-based vaccines to LNs is also size-dependent. The LNs are more sensitive to the hydrodynamic size of EVs, owing to the unique structure of the lymphatics coupled with its size-restrictive reticular network. It has been reported that small molecules (< 20 kDa) are typically rapidly cleared into the blood following injection, whereas larger molecules (> 20 kDa) and particles (10-100 nm in diameter) drain into the lymphatics from interstitial spaces. Even larger particles, with diameters > 100 nm, are likely to become trapped in the interstitial matrix due to limited lymphatic access[144, 145]. Therefore, particles with diameters of 10-100 nm may ensure efficiently precise delivery to LNs. Considering that the intrinsic size range of EVs are 30-150 nm, which also overlaps with an ideal delivery size range, EV-based vaccines have the potential to be selectively delivered to the LNs in a size-dependent manner. Moreover, as aforementioned, the presence of surface molecules can further affect targeted delivery to cell subtypes within LNs, as well as enhance cellular uptake.

5. EV Delivery for Targeting Immunity Modulation

The immunoregulatory function of EVs derived from different cell origins are distinct, which could result in different *in vivo* behavior, promoting usage as therapeutic agents or delivery platforms. Further molecular engineering of those EVs could reprogram EV functions to develop novel and advanced cancer immunotherapy. The molecular engineering approaches, as well as the five major reprogramming pathways are summarized in Figure 3 and discussed respectively in the subsequent sub-headings.

5.1 DC-derived EVs for immunomodulation

Cancer vaccines using tumor antigens[146], antigenic peptides[147], DNA[148], mRNA[149] or adjuvants[150] have been widely explored as promising options for cancer immunotherapy. However, their clinical outcomes vary, mainly because of limited immunoactivation and poor delivery efficacy[151–153]. Therefore, improving immunity potency and delivery efficacy for developing diverse vaccines is of great importance. Tailoring biomaterials (e.g. liposome, nanoparticle, scaffold) and autologous or allogeneic cells as vaccine delivery platforms has recently been proven to improve the therapeutic benefits[8, 154, 155]. Specifically, DC-based vaccines have emerged as the personalized cancer vaccine[156, 157]. Notably, Sipuleucel-T, an autologous DC therapy, was the first FDA-approved therapeutic cancer vaccine for prostate cancer in 2010[158]. However, the clinical implementation of Sipuleucel-T was hampered due to the manufacturing complexity associated many issues[159, 160]. EVs derived from APCs, especially DCs, have the potential as the therapeutic cell-free vaccines to surrogate their parent DCs, owing to the unique surface molecule composition, as illustrated in Figure 3 pathway 1. Pioneering work by Zitvogel et al. demonstrated that EVs derived from DCs, pulsed with antigen peptides, induced potent anti-tumor CD8⁺ T cell responses in murine mastocytoma P815 and mammary carcinoma TS/A tumor models, resulting in the regression of established tumors[24]. This study illustrates the potential of DC EVs as cell-free delivery platforms for vaccine development, while circumventing the bottleneck currently existing in DCs-based vaccine production. Additionally, preclinical studies also showed that peptides have a higher antitumor efficacy when carried by EVs[121, 123]. However, the antitumor

efficiency of DC-EV-based vaccines are limited in some patients with cancers[26, 28, 29]. The heterogeneity of *ex vivo* expanded DC-EVs combined with the maturation status of parent DCs mainly account for the poor therapeutic benefit of DC-EV-based therapy: Long withstanding challenges include generating highly homogeneous DC-EVs, and obtaining mature parent DCs, of which are usually asynchronously incomplete in maturation.[161]. Furthermore, their small size relates to rapid dispersion caused by Brownian motion, consequently impeding their recognition and docking on T cell receptors. Indeed, enhanced T cell activation can be pursued when EVs are immobilized at high concentrations, such as with latex beads. Additionally, the expression of immune-related molecules, such as MHC-I, MHC-II, CD86, CD80, and cytokines carried by EVs, is much lower than parent cells, which may require a large number of peptide-MHC complexes per EV and/or high-level EVs secretion[14]. These requirements along with designated cargo packaging are still missing reliable supporting techniques.

5.2 Targeted Delivery of Nucleic acids for immunomodulation

EVs are also natural carriers of nucleic acids, including message RNAs (mRNA), miRNA, small interfering RNAs (siRNA)[162, 163] and DNA, which are used to relay intracellular signals. The nucleic acids, mostly RNAs carried by EVs, were reported as promising biomarkers significantly interplaying tumor-immunity microenvironment[164]. More importantly, not only are nucleic acids in TEVs found to manipulate the immune response, but those in EVs secreted from immune cells also counteractively mediate tumor responses[164, 165]. In order to modulate the delivery of therapeutic EVs for the purpose of immune regulation, EVs can be engineered with tumor targeting ligands via post-purification: Chemical modifications or cellular surface engineering methods[124, 166–168]. Surface modified EVs can be tailored for targeted delivery of synthetic drugs and exogenous nucleic acids, which significantly reduces the toxicity and avoids the potential degradation or binding to other proteins. Particularly, the therapeutic nucleic acids, such as mRNAs and miRNAs carried by EVs, can effectively mediate development of immune cells. For instance, miR-155 and miR-326 were demonstrated to regulate the differentiation and maturation of CD4⁺ T cells[169, 170], while miR-20, and miR-124 demonstrated anti-tumor T cell responses, while miR-19 showed NF- κ B mediated inflammation[171–173]. Moreover, CpG oligonucleotides, which agonize TLR-9 receptors on B cells, can also be conjugated with EVs to boost anti-tumor immunity[174]. It was also found that streptavidin-lactadherin modified EVs, self-assembled with biotinylated CpG DNA, were internalized into TLR-9 presenting DC2.4 cells, which subsequently contributed to increasing cytokine release, initiating the immune response to adjuvants by dermal-resident APCs *in vivo*[175]. Therapeutic nucleic acids carried by EVs with surface tailored properties for targeted delivery have shown tremendous advantages in gene therapy[176, 177], which also will be an unmatched delivery system for advancing cancer immunotherapy. However, loading nucleic acids into EVs generally require different transfection strategies like electroporation, sonication, chemical transfection, which may potentially cause irreversible damage on EV membranes, and thereby influencing the recognition of EVs by recipient cells. Also, it remains unclear if enzymes carried by EVs can degrade nucleic acids. An unanswered question is if EVs can efficiently escape from lysosomes after cellular uptake through endocytosis or phagocytosis.

5.3 EV Targeting modulation of Tumor-Associated Macrophages

TAMs have been known in M2-like phenotype for promoting tumor growth by inducing immunosuppressive tumor microenvironments[178, 179]. In order to maximize the potential of macrophages for cancer immunotherapy, targeted modulation of TAMs by repolarizing pro-tumoral M2-like TAMs to M1-like TAMs is an emerging strategy, as shown in Figure 3 pathway 2. The EV surface CD47 interaction with SIRP α on the macrophage has been reported as preventing the capture and clearance from MPS[180]. Lv et al. proposed a hybrid nanoparticle, created by fusing CD47-expressing EVs with a thermosensitive liposome, for delivering chemotherapeutics and immunoregulatory agents to metastatic peritoneal cancer cells[181]. The CD47-expressed EVs produced from genetically engineered fibroblasts were capable of efficiently escaping from MPS capture after entering into systemic circulation. The granulocyte-macrophage colony-stimulating factor (GM-CSF) and docetaxel-loaded, genetically engineered EV-thermosensitive liposomes hybrid nanoparticles (G/D-gETL NPs) could preferentially accumulate in tumor sites, via the EPR effect, and release cargos under hypothermia conditions in hyperthermic intraperitoneal chemotherapy (HIPEC)[181]. As a consequence, the release of GM-CSF promoted the repolarization of M2-like TAMs to M1-like TAMs, leading to the improved presentation of antigens to effector T cells. Moreover, CD47 carried by gETL NPs interacted with SIRP α on macrophages, which further improves macrophage-mediated tumor cell phagocytosis. The targeted repolarization of M2-like TAMs into M1-like TAMs could restore the anti-tumor immunity, establishing an essential role in cancer immunotherapy. Although specific engineering ensures a CD47 outer coating, the biodistribution of this smart EVs-based system, after intravenous injection, was still mainly concentrated in liver. Moreover, the enhanced permeability and retention (EPR) effect-based passive targeting delivery of this EVs-based system to tumor site might not guarantee high TAM-targeting specificity when compared to ligand-mediated active targeting. It is highly expected that TAM targeting specificity could be further developed for a more robust and specific immunomodulation.

5.4 EV Dual-Targeting modulation of T Cells and Tumor Cells

Surface engineering EVs to simultaneously express ligands for targeting both T cells and tumor cells can effectively elicit cytotoxicity of T cells towards specific tumor cells. Cheng et al. developed synthetic multivalent antibodies (svFc) tailored EVs by engineering HEK293 cells to secrete EVs carrying svFc specific to T-cell CD3 and epidermal growth factor receptor (EGFR) from tumor cells[167], which can bridge T cellular anti-tumor responses against the EGFR-expressing breast cancer cells. Similarly, engineered EVs carrying svFc specific to CD3 and human epidermal growth factor receptor 2 (HER2) exhibited excellent anti-tumor immunity against HER2⁺ breast cancer cells *in vitro* and *in vivo*[182]. The effectiveness of dual-targeting engineered EVs open up novel possibilities for designing EVs to re-direct T cell cytotoxicity towards specific tumor cells, which could improve targeted cancer immunotherapy and reduce off-target effects, as illustrated in Figure 3 pathway 3. However, the *in vivo* efficiency of these EVs with dual-targeting functionality to bridge together T cells and tumor cells needs further investigation. Also, if the effector T cells were dysfunctional or apoptotic, their enrichment around tumor cells may impede the function of other activated effector T cells like immune recognition and subsequent response. Therefore, a more specific engineering strategy ensuring targeting activated

effector T cells is highly recommended. Furthermore, to realize clinical applications, in-depth characterization of exosomal composition may be required for developing therapeutic EVs with improved efficacy and reduction in side effects.

5.5. Engineering T-cell Derived EVs for Targeted Immunomodulation

The most common strategies for engineering EVs with intravesicular cargos are exogenous and endogenous loading[18, 183]. Endogenous loading functions through genetical modification of their parental cells for specific cargo packaging into the EV secretory pathway. Reports showing exogenous loading was mostly performed by co-incubating cargos with isolated EVs under chemical transfection, electroporation, sonication, or freeze/thaw cycles[15, 163]. Genetically engineered T cells expressing a chimeric antigen receptor (CAR) or T-cell receptor (TCR) are rapidly emerging as promising treatment options for a broad range of cancers, especially CD19⁺ B cell malignancies[184–187]. However, the associated life-threatening toxicity is significant, such as high fever, hypertension, hypoxia, and/or multiorgan toxicity, and CAR-T-related encephalopathy syndrome (CRES)[188]. Thus, CAR-T or TCR-T cells derived EVs are catching great attentions as alternatives to their parent cells. Lentiviral vectors can be used to transfect primary human T cells with Cetuximab scFv (termed CAR-T-CTX) or Trastuzumab svFv (CAR-T-TTZ), with results demonstrating that CAR-T CTX or CAR-T TTZ could efficiently lyse EGFR⁺ cancer cells or HER2⁺ cancer cells[189]. By isolating EVs from these engineered T cells using ultracentrifugation, it was found that EVs carry parent CARs on their surface, mostly in the form of exosomes. Similar to CAR-T cells, these CAR-EXO-CTX or CAR-EXO-TTZ notably expressed perforin or granzyme B, which is crucial for cytolytic activity[189]. The CAR-EXO-CTX or CAR-EXO-TTZ also demonstrated strong cytotoxic effects on EGFR-expressing cells or HER2-expressing cells respectively. Most importantly, the CAR EVs specifically targeted EGFR⁺ or HER2⁺ tumor cells after intravenous injection, inhibiting tumor growth in a dose-dependent manner[189]. Given that tumor cells may inactivate CAR-T cells via a variety of immunosuppressive signaling pathways, such as PD-L1/PD-1, an *in vivo* study was conducting, by adding recombinant PD-L1 to CAR exosomes which showed no significant influence on cytolytic activity, indicating the rare expression of PD-1 on these CAR exosomes. There was very limited CRS side effect observed. EVs derived from genetically engineered T cells abstract functionality from their parent cells, cytotoxically affecting cancer cells, and are less vulnerable to suppression.

$\gamma\delta$ -T cells are innate-like T cells with lytic activities that are not restricted by MHCs[190]. The V δ 1 type T cells are mainly located in mucosal and epithelial tissues, while V δ 2-T cells exist in the peripheral blood and lymphoid organs[191]. As reported, either the adoptive transfer of *ex vivo* phosphoantigens-expanded V δ 2-T cells or the direct administration of phosphoantigens to active V δ 2-T cells *in vivo*, could efficiently control Epstein-Barr virus (EBV)-induced B cell lymphoproliferative disorder (EBV-LPD)[192]. It has been hypothesized that V δ 2-T cell-derived EVs may possess the potential to inhibit tumor proliferation. Wang et al. reported that EVs derived from phosphoantigen-expanded V δ 2-T cells carry death-inducing ligands (FasL and TRAIL), an activating receptor for nature killer cells (NKG2D), and other immune-related molecules (e.g. MHC class I and II, CD80 and CD86)[193]. *In vivo* studies demonstrated that, after intraperitoneally injection into

mice for 24 h, V δ 2-T derived exosomes targeted EBV-transformed B lymphoblastoid cell lines (EBV-LCL) with much higher levels of accumulation than control exosomes. More importantly, the anti-tumor effect of V δ 2-T-Exos using an EBV-induced B cell lymphoma model was also shown as significantly reducing the incidence of tumors. Interestingly, it observed that antitumor effect of V δ 2-T-Exos was mediated by activating FasL and TRAIL signal pathways, as well as by inducing EBV antigen-specific CD4⁺ and CD8⁺ T cell expansion, indicating EVs derived from activated $\gamma\delta$ -T cells hold great promise in modulating antitumor immune responses. Compared with cell-based therapy, cell-free EVs-based therapy has several advantages in clinical applications. CAR-EVs may have a lower risk of toxicities compared to parent CAR-T cells, such as cytokine release syndrome (CRS), which is characterized by high fever hypotension, hypoxia and/or multiorgan toxicity[194, 195]. Another advantage, EVs-based immunotherapy may be more resistive to the immunosuppressive tumor microenvironment[196]. The manufacturing process of these cell-free vesicles is also safer than that of living CAR-T cells. However, it is still difficult to compare the killing efficiency between CAR-T cells and CAR-EVs, because they possess different natural mechanisms even though they have a similar function. Different from CAR-T cell-based treatment, the exact number of CAR-EVs normalized in equivalent protein content is controversial based on current methods[197]. Moreover, the efficiency of V δ 2-T-EVs was only evaluated in the context of EBV-associated cancers; whether V δ 2-T-EVs would be effective in other cancers remains to be determined. These aforementioned engineering strategies are tailorable and applicable for investigation of a variety of ligand-receptor pathways in immunomodulation, further unlocking the effective targeting ability of T cell derived EVs.

6. Challenge and Prospective

EVs are emerging as promising drug delivery biomaterials, involving extensive applications ranging from gene therapy, regenerative medicine, to immunotherapy and cancer vaccines. By harnessing the power of EVs, scientists have made tremendous strides in modulating the immune response for improving therapeutic outcomes. However, the majority of recent research investigations on EVs are from either animal models or 2D planar cell cultures. Given that 3D culture systems are recognized as more advanced in physiologically relevance than 2D culture systems, a growing body of studies are highlighting the distinct profiles of EVs secreted from 3D culture systems which are more accurately reflect the *in vivo* situation[198]. Increased secretion of EVs, upregulation of microRNAs, and downregulation of proteins was observed in 3D spheroid models composed of human gastric cancer cell lines (MKN45 and MKN74) in comparison to 2D conditions[199]. These results reveal the effect of cellular architecture on the release and content of EVs[200, 201]. Similarly, Thippabhotla et al. also demonstrated that EV miRNAs derived from 3D cervical cell culture displayed a 96% similarity to *in vivo* circulating EVs derived from cervical cancer patient plasma, while only a 80% similarity was observed in 2D culture[202]. Beyond just content and concentration, Kim et al. also conducted a comparative study on EVs-mediated immunomodulatory functions using 2D- and 3D-cultured mesenchymal stem/stromal cell-derived extracellular vesicles (MSC-EVs)[203]. *In vitro* analysis identified that EVs, derived from 3D cultured MSCs, performed better on restraining the secretion of pro-inflammatory

cytokines (IFN- γ and IL-6) while stimulating the production of immunoregulatory cytokines (TGF- β 1 and IL-10)[204]. Taken together, EV production is highly sensitive to their secretion-by-cell-culture system and apparent conditions implemented. EV sources also could introduce significant variables. Therefore, such variables pose substantial challenges in EV manufacturing and purification.

Currently, there is no standardized isolation and purification methods for preparing homogeneous EVs yet. Although ultracentrifugation, polymer precipitation, or column filtration isolation methods can provide high recovery yield of EV, such yields are irrelevant to homogenous or highly specific EV molecular components. Highly specific isolation methods are much more advanced in terms of isolation precision to EV subtypes and specificity to pathogenesis-relevant markers, such as filtration combined with SEC[205], immunoaffinity capture-based techniques[206], and microfluidics-based isolation techniques[207–209]. The ideal isolation technique is desired with homogenous molecular cargos, reproducible, high-yielding and throughput, and scale up capability. Thus, careful considerations should be taken while choosing an isolation method with the cell sources and the nature of molecular cargos in mind.

Due to the constraints from the above EV isolation methods, the clinical translation of EV-based drug delivery and therapies is hampered consequently. Several attempts have been made to develop production and purification using GMP standard protocols, as well as characterization procedures of GMP-grade EVs[32, 210–212], which requires sterilized manufacturing process in producing EVs with sufficient and consistent therapeutic payloads. The batch-to-batch variation is the focal point, requiring rigorous validation. Currently, amounts of efforts are contributed to a more ideal strategy meeting all the criteria for large-scale GMP-grade EVs manufacturing in pursuit of good scalability, reproducibility, safety, potency, and purity of EVs for precision cancer immunotherapy. As shown in Table 2, including three completed Phase I clinical trials and one completed Phase II clinical trial, there is no approved EV-based therapy yet for clinical use, possibly due to the nature of heterogeneity within the production of EVs and intra-exosomal compositions. Particularly, in light of COVID-19 pandemic needs, two clinical trials were registered on March 2020 for investigating mesenchymal stem cell secreted EVs as therapy for reducing pulmonary inflammation and their safety ([ClinicalTrials.gov Identifier: NCT04276987](https://clinicaltrials.gov/ct2/show/study/NCT04276987) and [NCT04313647](https://clinicaltrials.gov/ct2/show/study/NCT04313647)). Despite this significant progression, timely large-scale manufacturing in meeting emerging clinical needs is still challenging, mainly due to the complication on isolation and purification of heterogeneous EVs from a tremendous upscale, attempting to consistently output a production of population-based dosages. Therefore, to further translate EVs to the bedside applications, more multidisciplinary technologies and collaborations are highly expected in the near future.

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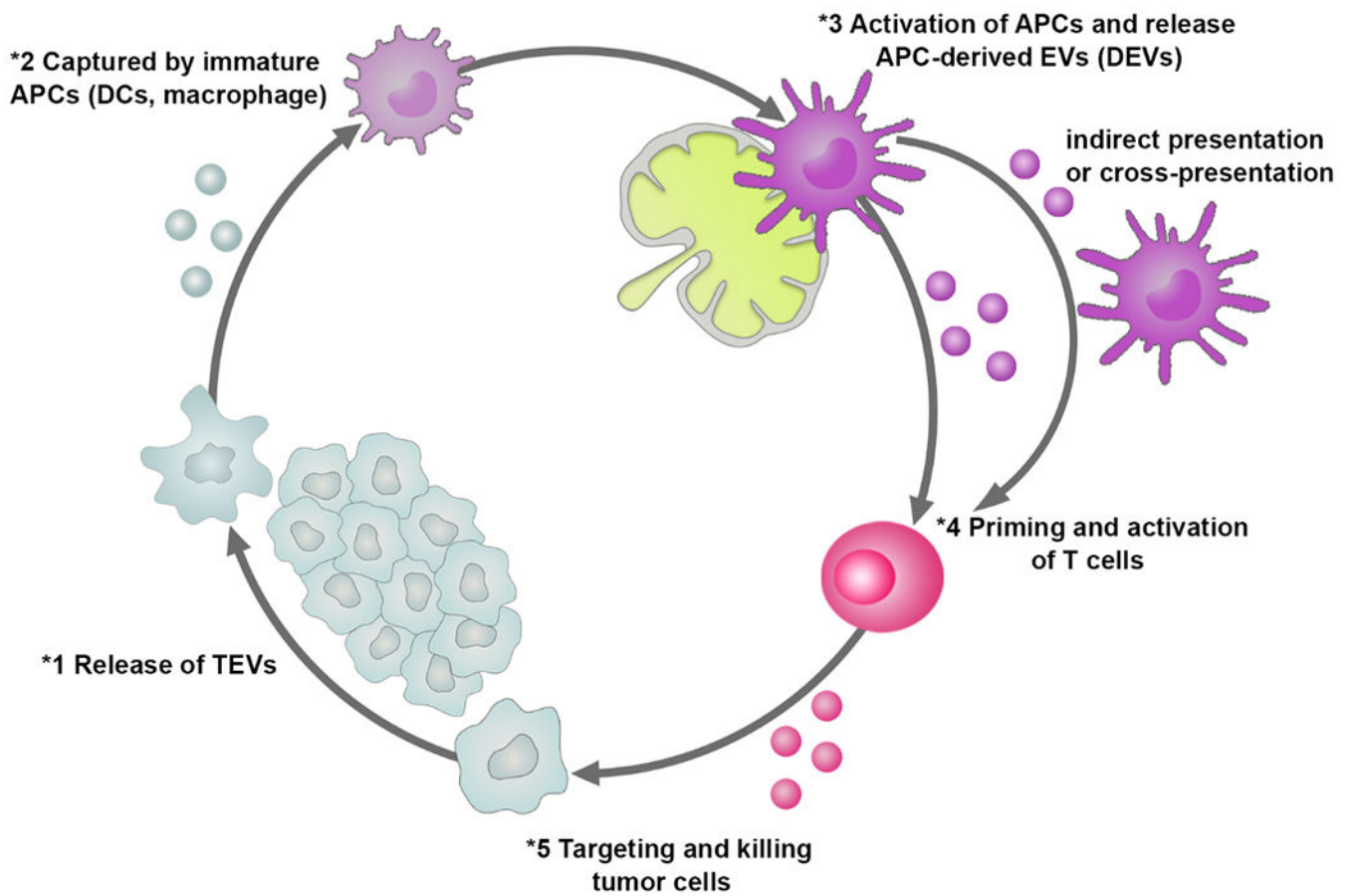


Figure 1.
The role of EVs derived from either tumor cells or immune cells in regulating cancer-immunity cycle.

The Explosive Growth of Exosomal Research

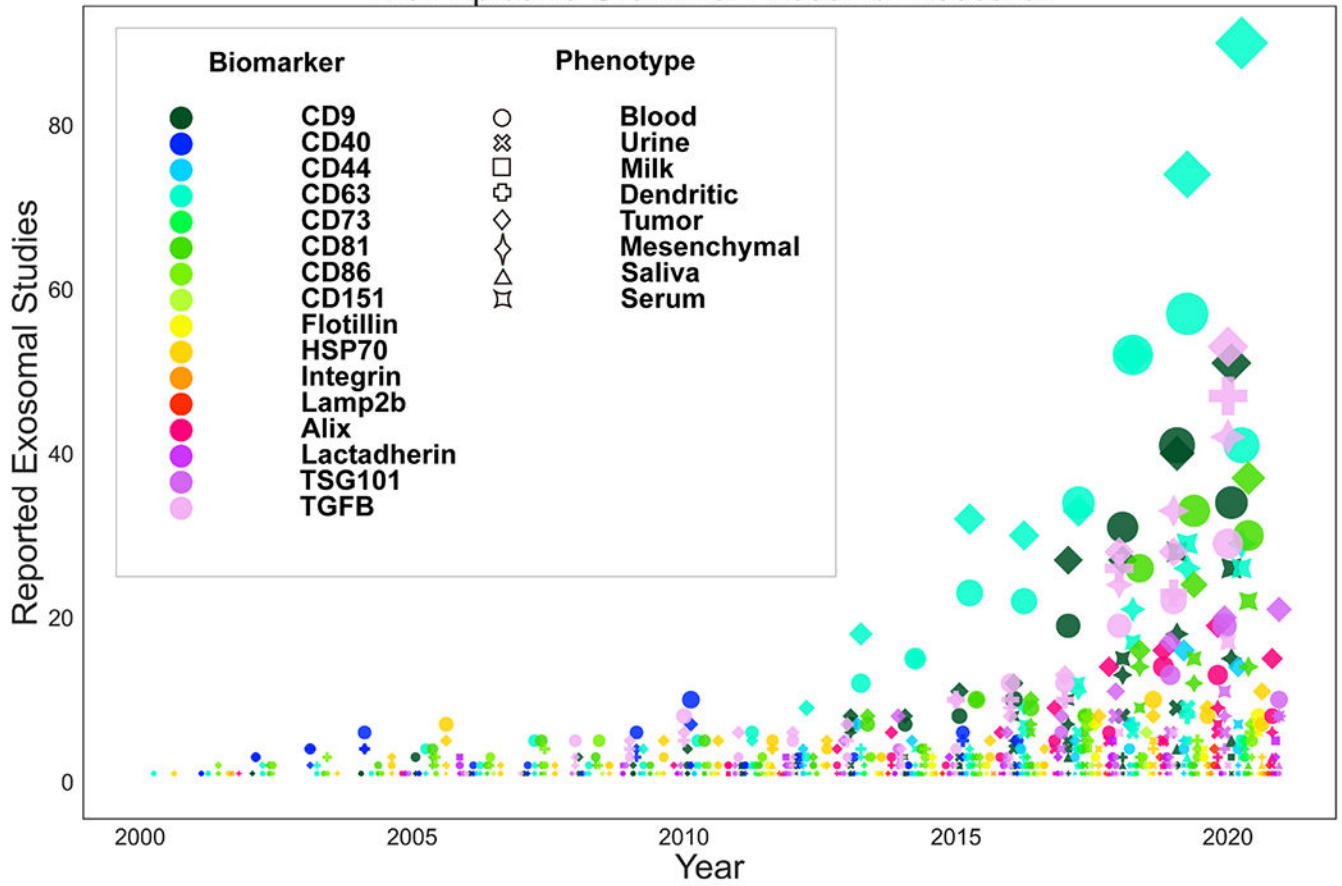


Figure 2. Summary of published EV markers in past 20 years from different sources in cell and tissue targeting.

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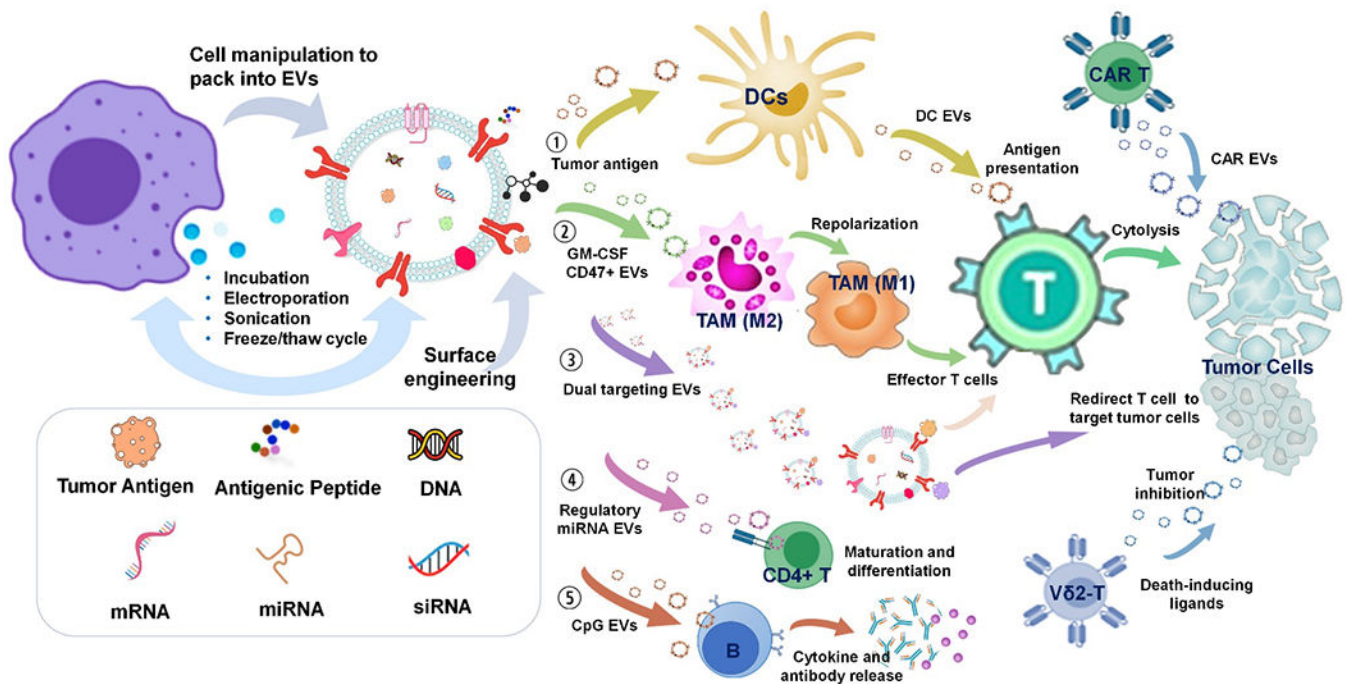


Figure 3. The schematic illustration of EVs for reprogramming tumor immunity. Number 1-5 indicate the five major EV reprogramming pathways in regulating tumor immunity.

Table 1.

The summary of clinical trials of EVs-based cancer therapies in recent five years.

Disease	Phase/Number of Patients	EV Sources	Manipulation	Therapeutic Outcomes
Completed Trials				
Metastatic Melanoma[26]	Phase I/ n = 15	imDCs, autologous	Pulsed with MAGE3 peptides	Safe, well tolerated; 2 stable disease, 1 minor response, 1 partial response, 1 mixed response
Colon cancer[27]	Phase I/ n = 40	Ascites, autologous	Loaded with CEA± GM-CSF	Safe, well tolerated, 1 stable disease, 1 minor response
NSCLC[28]	Phase I/ n = 4	imDC, autologous	Pulsed with MAGE-A3, -A4, -A10, -3DP04 peptides	Safe, well tolerated, 9 completed therapy, 2 with initial progression, 2 without progression for >12 months
NSCLC[29] [NCT01159288]	Phase II/ n = 41	mDCs, autologous	Pulsed with MAGE-A1, -A3, NYESO-1, MAGE-A3-DP04, EBV peptides	22 completed therapy, 7 with stable disease (>4 months), primary endpoint (50%) not reached
Ongoing Trials				
Malignant ascites and pleural effusion [NCT02657460]	Phase II/ n = 90	Malignant pleural effusion	Loaded with methotrexate	Recruiting
Malignant ascites and pleural effusion [NCT01854866]	Phase II/ n = 30	Tumor derived	Loaded with chemotherapeutics	Unknown status
Malignant ascites [NCT03230708]	Phase 1/2/ n = 18	Erythrocytes, autologous	Loaded with methotrexate	Unknown status
Colon cancer	Phase I/ n = 35	Plant derived	Loaded with Curcumin	Active, not recruiting
Metastasis pancreatic cancer [NCT0368631]	Phase I/ n = 28	MSCs, allogeneic	KrasG12D siRNA (iExosomes)	Recruiting
Malignant pleural effusion	N/A/ n = 248	Not reported	Loaded with methotrexate	Recruiting

Notes: CEA: Carcinoembryonic antigen; NSCLC: Non-small cell lung cancer

Table 2.

Selected example list of reported EV surface markers corresponding to tissue tropism in different diseases.

Disease	Cell/Tissue tropism	EV Surface Biomarkers
Melanoma	Heterogenous Tumor	FasL, Perforin, CD63, Alix[118]
	DCs	A2/MART 1 Tetramer, CD11c, i-A, CD80, CD86, CD40 and H-2D, MA2.1, Integrin $\alpha\beta3/\alpha\beta5$, Lactadherin, OVA, LFA-1/CD54, CCR7, DEC205, TLR4, TLR9, MyD88, DC-Sign[120–122]
	T, B cell / Spleen	OVA/SHINFEKL, CD9, 54, 81, 80, 86[23]
	DCs / Spleen	Cyclophosphamide, MART1[123]
	NK Cells, DCs	MAGE 3 A1/B35, MAGE3.247-258DPO4[26]
	Liver, Spleen, Breast	Lamp-2b/ αv specific iRGD peptide[124]
Pancreatic Adenocarcinoma	BMC/Lung, Tissue, Kidney, Pancreas	Clusterin, GDF15, Neuropilin, Beta Actin, Thrombosposin CD9, CD151, CD49e, CD63, Tspan8 and B4, CD49f, CD621, CD104, CD54[112]
Neuroblastoma	Glial cells, Neuronal Soma	CTF, GAL4, CD63, Flot-1, APP[113]
Plasmacytoma	DCs	MFG-E8/Lactadherin, MAC-1a/b, CD9, MHC1/II, CD86, CD80, CD88, CD83, CD40, ICAM-1, Lamp2b, Syntenin, Gi2a, Alix, TPx, 14-3-3, Galectin-3, Hsc73, Hsp84, RabGDI, Rap1B, Rab7, Annexins, I,II,IV,V,VII, Gag, EF1a, Actin, Tubulin, Cofilin, Profilin I, EIF-4a[114]
HIV-1	DCs (CD11 ⁺)	HLA-DR1, CD1b, CXCR4- or CCR5- cells, CD9, CD63[115]
Unspecific	DCs	ICAM-1, LFA1, I-Ab/HY Peptide[117]
Lymphatic Leukemia	CD4+ and CD8+ w/ IL-2	CD3, IL-2, CD9, CD63, CD81[75]
	Brain, Kidney, Liver	Lamp2b, RVG, MSP, FLAG[125]
	Malignant B-cells, T-cells	EBV-gp350+, CD154, CD21, B1FNR1, CD154, HSP70, TSG101, CD63, GM1[126]
Chronic Myeloid Leukemia	Liver, Spleen, Kidney, Tumor	IL-3/CD-123, ALIX, CD81, TSG101[127]
T-cell Lymphoma	B-cells	HLA, pMAGE-A33, Lactadherin[128]
Mouse Lymphoma	NK Cells, Liver, Lung, Spleen	α -Galactosylceramide, OVA, CD-1d[129]
T-cell hybridoma	Tumor	MFG-E8, OVA, Lactadherin, HSC70, TSG101, CD9[130]
Breast Cancer	Tumor Xenografts	Dicer/Actin, CD9, CD63, CD81, Flotillin-1, TSG101[49]
	Lung, Colon, Tumor Xenografts	Oncolytic Adenovirus fused to CD40L, Paclitaxel TSG101, CD63, CD9[109]
Hepatocarcinoma	Liver, Spleen, Breast	Lamp-2b fused with an αv integrin iRGD peptide[124]
	DCs	Human HER2, nt 1-1953/nt 1-2025/AAV, Lactadherin[131]
Unspecified	Unspecified	Lamp-2b fused with an $\alpha\beta$ integrin iRGD peptide[124]
Prostate Cancer	Tumor Tissue	Lactadherin[132]
Fibrosarcoma	Tumor	MFG-E8, OVA, Lactadherin, HSC70, TSG101, CD9[130]
Pancreatic Ductal Adenocarcinoma	Tumor, liver, skin, kidneys, lungs	Oxaliplatin and Galactin, Lactadherin, Annexin V, CD63, Alix, HSP70, CD81[133]
Acute Lung Inflammation / LPS Septic Shock	Liver, Lung, Kidney, Spleen, CD11b ⁺ Gr-1 ⁺ cells	TGS101, CD81[134]
Chronic Acute Inflammation	Spleen, Liver, DCs, Macrophages, Kupffer cells,	IL-4, FasL, CD11b, CD71, CD86, CD178[135]
Lung Cancer	NK cells	MAGE-A3 and MAGE-A4, MAGE-3DPO4, MHC1/2, CD1a-d, CD86, CD9, C37, CD53, CD81, CD82[28]