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# An ultra-sensitive $T_2$ -weighted MR contrast agent based on $Gd^{3+}$ ion chelated $Fe_3O_4$ nanoparticles

 Jing Chen,<sup>a</sup> Hui-Hui Xiang,<sup>ab</sup> Zu-Zhi Zhao,<sup>a</sup> Yun-Kai Wu,<sup>a</sup> Meng-Yu Fei<sup>c</sup> and Meng-Meng Song <sup>\*a</sup>

An ultra-sensitive  $T_2$ -weighted MR imaging contrast agent was prepared based on  $Fe_3O_4$  nanoparticles and  $Gd^{3+}$  ions ( $Fe_3O_4@Gd$ ). Amino modified  $Fe_3O_4$  nanoparticles were conjugated to diethylenetriamine pentaacetic acid, and finally coordinated with  $Gd^{3+}$  ions. The nanoparticles had a uniform morphology with a size of 100 nm and a Gd/Fe mass ratio of 1/110. The  $r_2$  (transverse relaxivity) of the  $Fe_3O_4$  nanoparticles increased from  $131.89\text{ mM}^{-1}\text{ s}^{-1}$  to  $202.06\text{ mM}^{-1}\text{ s}^{-1}$  after coordination with  $Gd^{3+}$  ions. MR measurements showed that the aqueous dispersion of  $Fe_3O_4@Gd$  nanoparticles had an obvious concentration-dependent negative contrast enhancement. Hepatoma cells were selected to test the cytotoxicity and MR imaging effect. The application of  $Fe_3O_4@Gd$  nanoparticles as contrast agents was also exploited *in vivo* for  $T_2$ -weighted MR imaging of rat livers. All the results showed the effectiveness of the nanoparticles in MR diagnosis.

## Introduction

Early and highly accurate diagnosis has great significance in modern medicine.<sup>1</sup> Magnetic resonance imaging (MRI) has been the most powerful and effective diagnostic method due to its many advantages, such as few side effects and non-invasive properties.<sup>2–4</sup> MR contrast agents have played an important role in improving sensitivity by enhancing the contrast between normal tissue and diseased tissue.<sup>5</sup> The commonly used MR contrast agents are divided into  $T_1$ -positive agents, such as Gd chelates, and  $T_2$ -negative agents, such as superparamagnetic iron oxide  $Fe_3O_4$  nanoparticles.<sup>6</sup>

High transversal relaxation is necessary for MR contrast agents. For the past few years, a lot of effort has been devoted to the development of novel ultra-sensitive contrast agents.<sup>5,7,8</sup> Some researchers tried to use materials of high saturation magnetization ( $M_s$ ) as an alternative, such as  $MnFe_2O_4$  and  $CoFe_2O_4$ .<sup>9,10</sup> Because the size, shape and surface modification affected the saturation magnetization of nanoparticles, nanoparticles with cube, octapod, rod and other non-spherical shapes had been also exploited as ultrasensitive contrast agents.<sup>11,12</sup> In addition to the intrinsic materials properties,  $r_2$  enhancement can also be realized by developing aggregates or clusters of magnetic nanoparticles.<sup>13–15</sup> Recently, Huang *et al.* enhanced the transversal relaxation of  $Fe_3O_4$  nanoparticles by using  $Gd^{3+}$ -chelated

mesoporous silica shells.<sup>16</sup> Enlightened by this, we designed a facile strategy to prepare nanoparticles based on  $Fe_3O_4$  nanoparticles and  $Gd^{3+}$  ions. It is well known that  $Gd^{3+}$  ions have well coordination with diethylenetriaminepentaacetic acid (DTPA), so many scientists are working on how to conjugate DTPA to  $Fe_3O_4$  nanoparticles. To achieve this goal, chemicals contain amino group have been used to modify  $Fe_3O_4$  nanoparticles and then coupled to DTPA *via* chemical conjugation or electrostatic interaction, such as (3-aminopropyl)triethoxysilane (APS), dopamine, chitosan and polyethyleneimine (PEI).<sup>16–18</sup> Here amino group modified  $Fe_3O_4$  nanoparticles were hydrothermal synthesized and then the nanoparticles were further modified by DTPA, which enabled the following chelation with  $Gd^{3+}$  ions. Besides, the relaxivity increased from  $131.89\text{ mM}^{-1}\text{ s}^{-1}$  of  $Fe_3O_4$  to  $202.06\text{ mM}^{-1}\text{ s}^{-1}$  of  $Fe_3O_4@Gd$  nanoparticles while the previous publications reported  $Gd^{3+}$  chelated  $Fe_3O_4$  nanoparticles always resulted in a decrease of relaxivity.<sup>19</sup>

The morphology, size and magnetic properties of the formed  $Fe_3O_4@Gd$  nanoparticles were characterized by TEM (transmission electron microscopy), DLS (dynamic light scattering) and VSM (vibrating sample magnetometer). The cytotoxicity and cellular uptake were also investigated by 3-[4,5-dimethylthiazol-2-yl]-2,5-diphenyl tetrazolium bromide (MTT) assay and Prussian blue staining method. The effectiveness of  $Fe_3O_4@Gd$  nanoparticles as MR contrast agents was investigated both *in vitro* and *in vivo*.

## Materials and methods

### Chemicals and reagents

MTT, iron(III) chloride hexahydrate ( $FeCl_3 \cdot 6H_2O$ ), DTPA, gadolinium(III) nitrate hexahydrate [ $Gd(NO_3)_3 \cdot 6H_2O$ ], *N*-(3-dimethylaminopropyl)-*N'*-ethyl carbodiimide hydrochloride (EDC·HCl)

<sup>a</sup>School of Basic Medical Sciences, Anhui Medical University, 81 Meishan Road, 230032 Hefei, Anhui, PR China. E-mail: songmengmeng@ahmu.edu.cn; Tel: +86-551-6516-1138

<sup>b</sup>Department of CT/MRI, Anhui No. 2 Provincial People's Hospital, 1868 Dangshan Road, North Second Ring Road, 230032 Hefei, Anhui, PR China

<sup>c</sup>The First Affiliated Hospital, Anhui Medical University, 218 Jixi Road, Hefei, Anhui, PR China



and *N*-hydroxysuccinimide (NHS) were purchased from Aladdin (Shanghai, China). HepG2 (liver hepatocellular carcinoma) cells were purchased from the Type Culture Collection of the Chinese Academy of Sciences (Shanghai, China). Sprague-Dawley rats (200–220 g) were purchased from Anhui Experimental Animal Center (Hefei, China).

### Preparation of Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles

Amino modified Fe<sub>3</sub>O<sub>4</sub> nanoparticles are prepared according to Li *et al.*'s publication.<sup>20</sup> Briefly, 6.5 g 1,6-hexanediamine, 2.0 g anhydrous sodium acetate and 1.0 g FeCl<sub>3</sub>·6H<sub>2</sub>O were dissolved in 30 mL glycol and then transferred into a Teflon lined autoclave and kept at 190 °C for 6 h. The products were then washed with ethanol for many times. And then the nanoparticles are reacted with DTPA with the presence of EDC and NHS in MES buffer under room temperature for 72 h. After that, Gd(NO<sub>3</sub>)<sub>3</sub> were added to the mixture and then stirred for another 24 h. Finally, the nanoparticles were collected by centrifugation and rinsed with water for many times.

### Characterization of nanoparticles

The morphology of Fe<sub>3</sub>O<sub>4</sub> nanoparticles and Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles were characterized by TEM (JEOL, JEM-2100F). DLS measurement was determined by Zetasizer (Nano series, Malvern Instruments). The magnetic measurement was carried out using VSM (MPMS SQUIDM, USA). T<sub>2</sub>-weighted MR imaging of Fe<sub>3</sub>O<sub>4</sub> nanoparticles and Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles were measured by an MR scanner at 3.0 T (GE, Milwaukee, USA) as follows: echo time (T<sub>E</sub>) = 20, 40, 60, 80, 100 and 120 ms; repetition time (T<sub>R</sub>) = 3000 ms; field of view (FOV) = 20 mm × 20 mm; slice thickness = 4.0 mm; matrix = 320 × 320. IR characterization was performed by an IR spectrometer (Nicolet iN10, Thermo scientific, USA).

### In vitro study

**Cell culture.** HepG2 cells were cultured in RPMI 1640 medium with 10% fetal bovine serum (FBS), 100 mg mL<sup>-1</sup> streptomycin, and 100 U mL<sup>-1</sup> penicillin at 37 °C under 5% CO<sub>2</sub>.

**Cytotoxicity study.** For MTT study, HepG2 cells were seeded on a 96-well plate at a density of 1 × 10<sup>4</sup> cells per well with. After 24 h, the culture medium was replaced with 100 μL of medium containing 0–40 μg mL<sup>-1</sup> of Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticle. The cytotoxicity was evaluated by determining the cell viability after incubation for 24 h.

**Prussian blue staining.** HepG2 cells (5 × 10<sup>5</sup>) were seeded in 6-well plates and then Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles was added with the concentration range of 0–40 μg mL<sup>-1</sup>. After 24 h, the cells were then treated with 4% formaldehyde for 30 min. Then 5% potassium ferrocyanide and 5% hydrochloric acid was added. Finally, cells were imaged by a microscope (Olympus, IX71).

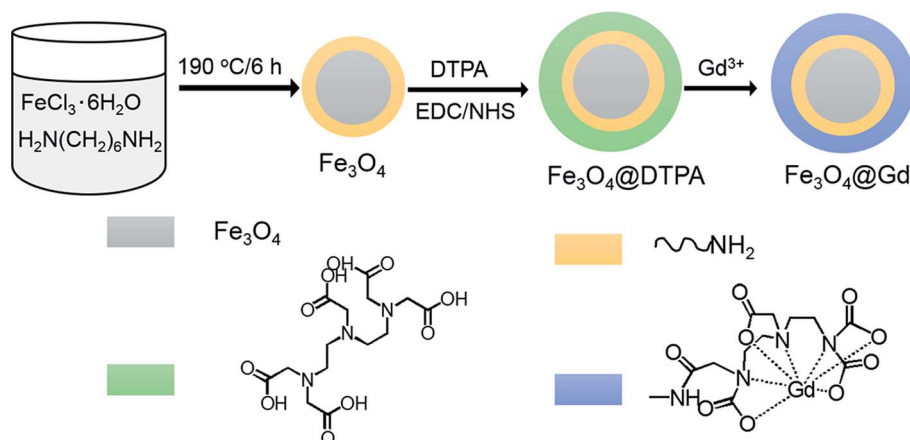
**MRI investigation.** HepG2 cells (5 × 10<sup>5</sup>) were plated in 6-well plates and then Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles were added at a concentration of 0–40 μg mL<sup>-1</sup>. After incubation for 24 h, the cells were collected and re-suspended in 0.5% agarose gel and then imaged by using a 3.0 T MR system (Discovery MR750w, GE Medical Systems, Milwaukee, WI, USA).

### In vivo study

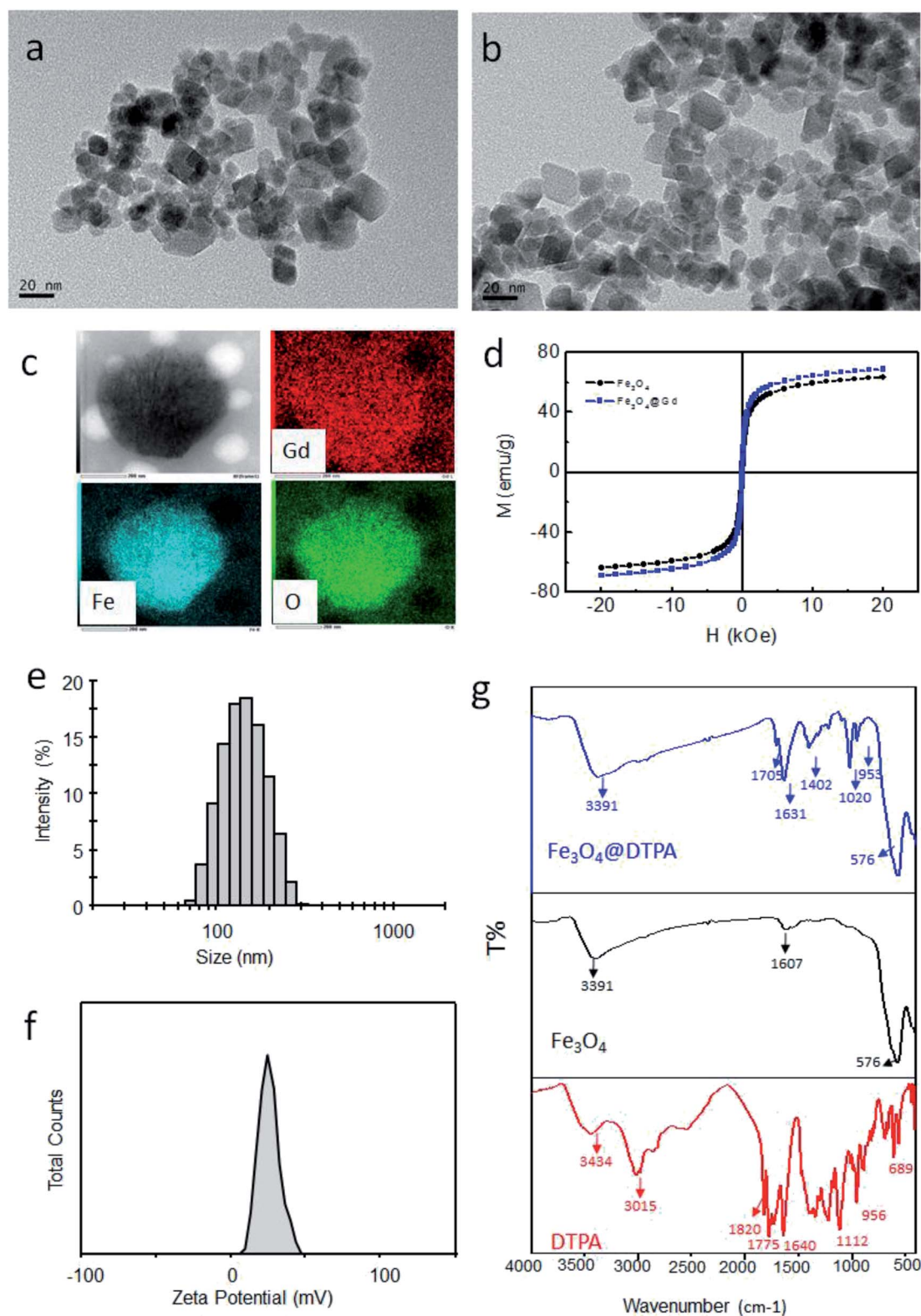
**Animals.** Sprague-Dawley rats (200–220 g) were purchased from the Anhui Experimental Animal Center with the license number "SCXK (Wan) 2011-002". The rats were housed under at 22 °C with a 12 h light/dark cycle and were allowed free access to food and water. All animal procedures were performed in accordance with the Guidelines for Care and Use of Laboratory Animals of Anhui Medical University and approved by the Animal Ethics Committee of Anhui Medical University.

**Prussian blue staining.** Liver, heart, spleen, kidney and lung tissues freshly removed from Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles treated rat were fixed in 4% paraformaldehyde and processed routinely into paraffin, sectioned at a thickness of 3 μm, brain sections were then stained with Prussian blue and counterstained with eosin. Finally, the sections were imaged by a microscope (Olympus, IX71).

**MRI investigation.** For *in vivo* MR investigation, SD rats were tail vein injected with Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles (1 mL, 10 mg per kg of rat body weigh). The rats were imaged before and at 0.5 h, 1 h, and 24 h post injection. T<sub>2</sub>-weighted MR images were



Scheme 1 Schematic illustration of the formation of Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles.



**Fig. 1** Characterization of nanoparticles. (a) TEM image of  $\text{Fe}_3\text{O}_4$  nanoparticles; (b) TEM image of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles; (c) EDX mapping images of one nanoparticle; (d) the magnetic hysteresis loops of  $\text{Fe}_3\text{O}_4$  and  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles at room temperature; (e) size distribution of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles; (f) zeta potential of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles; (g) IR spectra of  $\text{Fe}_3\text{O}_4@\text{DTPA}$  nanoparticles,  $\text{Fe}_3\text{O}_4$  nanoparticles and DTPA.

obtained with a matrix size of  $256 \times 256$ , slice thickness of 2 mm, and field of view of  $60 \text{ mm} \times 60 \text{ mm}$ . The signal intensity was also measured.

## Results

### Materials characterization

$\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles were fabricated by three steps (Scheme 1). First, amino group modified  $\text{Fe}_3\text{O}_4$  nanoparticles were hydrothermal synthesized. Second, DTPA were conjugated to amino group through amide bond. Finally,  $\text{Gd}^{3+}$  ions were chelated with DTPA to form  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles. Fig. 1a and b showed the TEM images of  $\text{Fe}_3\text{O}_4$  nanoparticles and  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles, respectively. There was no obvious change between the morphology of the two samples, which had a size ranging from 10–50 nm. To confirm the element composition, energy-dispersive X-ray (EDX) element mapping was performed on a single nanoparticle (Fig. 1c). The results suggested that Gd element is present in the nanoparticle. Inductively coupled plasma atomic emission spectroscopy (ICP-AES) analysis was employed to quantify Fe and Gd content and the results showed the mass ratio of Gd/Fe is 1 : 110. According to the ICP analysis results, each nanoparticles have conjugated to  $1.48 \times 10^4$  DTPA molecules.

The magnetic properties of the nanoparticles were measured at room temperature. As shown in Fig. 1d, the saturation magnetization value of  $\text{Fe}_3\text{O}_4$  and  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles are  $63.35 \text{ emu g}^{-1}$  and  $68.65 \text{ emu g}^{-1}$ , respectively. After chelated with  $\text{Gd}^{3+}$  ions, the saturation magnetization increased. Besides,

both the values were lower than that of bulk  $\text{Fe}_3\text{O}_4$ , which was reasonable because the particle size decreased.<sup>20</sup> The remanence and coercivity of both the samples were nearly zero, suggesting the superparamagnetic property of the nanoparticles.

DLS measurements were carried out to measure the size and zeta potential values of the obtained nanoparticles. The hydrodynamic diameter histogram and the zeta potential distribution were presented in Fig. 1e and f. It was noticed that the hydrodynamic size of the nanoparticles was kept around 130 nm, which was larger than that obtained from TEM observation. This might be explained that the small nanoparticles aggregated slightly. However, the aggregates still had a proper size less than 200 nm, which was still proper for bio-applications. It was also worth mentioned that the obtained nanoparticles possessed a zeta potential of +17 mV, which was critical for formation of stable dispersions.

Fig. 1g shows the IR spectra of  $\text{Fe}_3\text{O}_4$  nanoparticles before and after conjugated to DTPA and free DTPA. It can be see clearly that all the peaks of DTPA are appeared in the spectrum of the conjugated nanoparticles ( $\text{Fe}_3\text{O}_4@\text{DTPA}$ ) with suppressed intensity. The adsorption peak at around  $576 \text{ cm}^{-1}$  was the characteristic absorption of Fe–O bond. Besides, there is a new peak at  $1704 \text{ cm}^{-1}$ , which is ascribed to C=O group of the formatted amide bond. All of these confirmed that DTPA is successfully conjugated to the surface of  $\text{Fe}_3\text{O}_4$  nanoparticles *via* amide bond.

### $T_2$ MR relaxometry

To investigate the possibility of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles as  $T_2$ -weighted contrast agents, MRI investigation were carried. Fig. 2

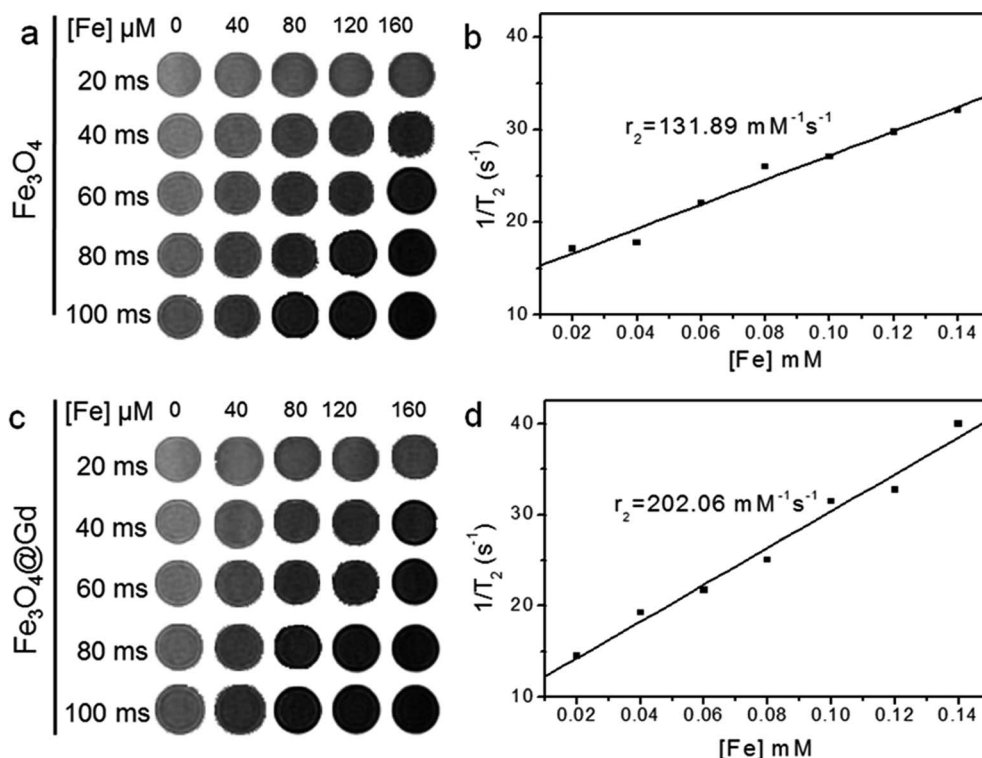


Fig. 2  $T_2$ -weighted MR images at different Fe concentration in 0.5% agarose gel at different TE time and the analysis of relaxation rate vs. Fe concentration. (a and b)  $\text{Fe}_3\text{O}_4$  nanoparticles. (c and d)  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles.

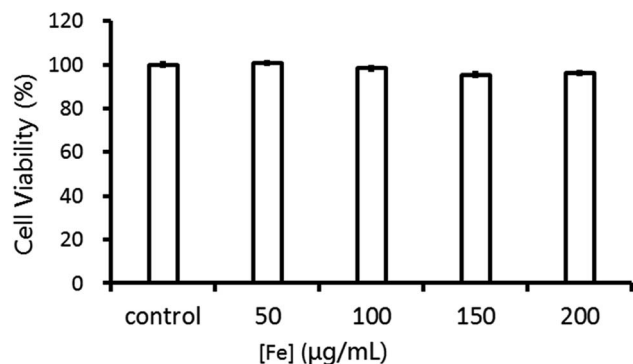


Fig. 3 Cell viability of HepG2 cells incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles at various Fe concentrations.

showed the  $T_2$ -weighted MR images of  $\text{Fe}_3\text{O}_4$  and  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles with various Fe concentrations under different TE time. We observed that the  $T_2$ -weighted MR signal decreased with the increase of Fe concentration.  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles exhibited much higher  $T_2$ -negative contrast than  $\text{Fe}_3\text{O}_4$  nanoparticles. The scatter diagram of relaxation rate *vs.* concentration was linear fitted and the slope was equal to the transverse relaxivities  $r_2$ . The  $r_2$  value of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles was measured to be  $202.06 \text{ mM}^{-1} \text{ s}^{-1}$ , higher than that of  $\text{Fe}_3\text{O}_4$  nanoparticles without  $\text{Gd}^{3+}$  ions coordination.

#### Cytotoxicity and cellular uptake studies

The biocompatibility is a critical parameter for materials in biomedical application. MTT assay was performed to evaluate

the cell viability of HepG2 cells incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles. As shown in Fig. 3, there was no obvious concentration-effect observed in [Fe] range of  $50\text{--}200 \mu\text{g mL}^{-1}$ . After co-incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles for 24 h, the cell viability with the highest concentration up to  $200 \mu\text{g mL}^{-1}$  had no significant difference. This suggested that  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles were very low toxic at the tested concentration range, which is beneficial for the further bio-medical applications.

To study the cellular uptake of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles, HepG2 cells incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles with various concentrations were stained by Prussian blue and Eosin. Iron can be stained by Prussian blue and show blue color. As shown in Fig. 4a, HepG2 cells incubated with DMEM exhibited pink color. After incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles, blue color were observed because of the internalized nanoparticles. The blue color also showed concentration-effect, as the concentration increased, the blue color became stronger. It was noteworthy that the blue color was located in the cytoplasm instead of nucleus, which suggested the internalized  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles were mainly distributed in cytoplasm.

The MR imaging ability of  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles was first performed *in vitro*. HepG2 cells were incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles with various concentrations for 24 h and then collected for MR scanning. As shown in Fig. 5a, HepG2 cells after incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles displayed a negative enhancement. The MR images of HepG2 cells darkened gradually as Fe concentration increased. HepG2 cells exposed to  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles exhibited an obvious signal decrease even at the lowest concentration  $5 \mu\text{g mL}^{-1}$

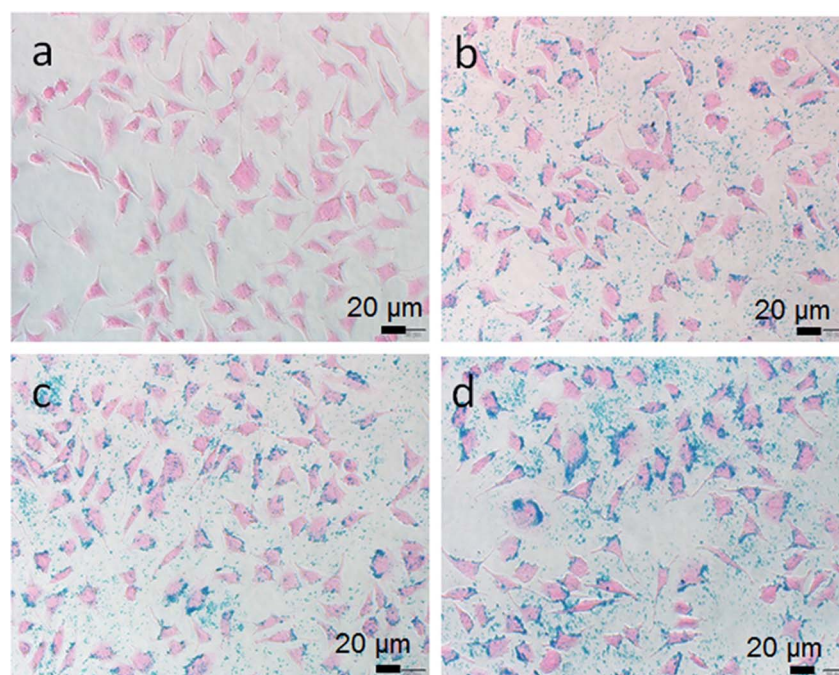


Fig. 4 Prussian blue staining images of HepG2 cells incubated with  $\text{Fe}_3\text{O}_4@\text{Gd}$  nanoparticles at various iron concentration ((a) – control, (b) –  $10 \mu\text{g mL}^{-1}$ , (c) –  $20 \mu\text{g mL}^{-1}$ , (d) –  $30 \mu\text{g mL}^{-1}$ ).

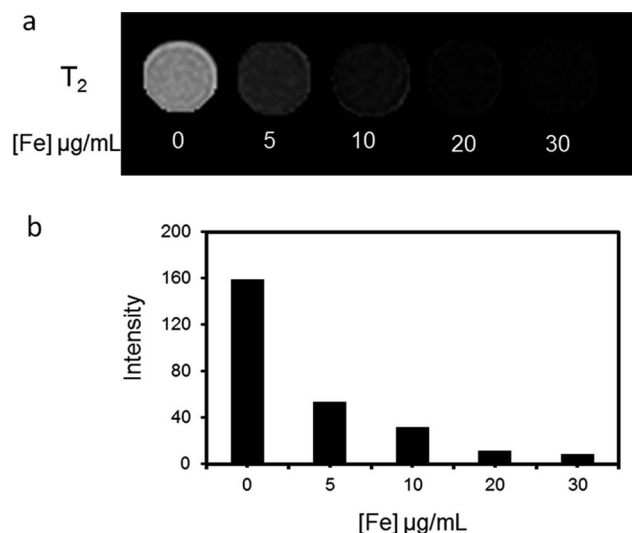


Fig. 5 MR investigation *in vitro*. (a)  $T_2$ -weighted MR images of HepG2 cells incubated with Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles with iron concentration ranging from 0–30 µg mL<sup>-1</sup> and (b) the corresponding analysis of MR signal intensity.

compared with control cells. When iron concentration greater than 20 µg mL<sup>-1</sup>, the signal intensity was almost keep stable. This demonstrated that the uptake of Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles of HepG2 cells was nearly saturated.

### MR investigation

High  $r_2$  relaxivity, low toxicity and good imaging effect *in vitro* encouraged us to explore there *in vivo*  $T_2$ -weighted MR imaging capability. 10 mg Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles (1 mL, 10 mg per kg of rat body weight) were injected into the SD rat *via* tail vein. After vein tail injection of our nanoparticles, MR scanning was performed. Fig. 6 showed  $T_2$ -weighted MRI images of rat liver collected from different time. After injection 30 min, MR images of liver showed slightly changes. The signal intensity of the corresponding  $T_2$ -weighted images was plotted in Fig. 6e. As long prolonged, the  $T_2$  MR signal intensity of liver darkened gradually compared with that before injection. At 24 h post injection, the rat liver showed the lowest signal intensity in  $T_2$ -weighted MR images. This result demonstrated that the negative enhancement of MRI could be achieved by using our Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles as contrast agents.

### *In vivo* biodistribution

Prussian blue staining was used to investigate the *in vivo* bio-distribution of the Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles. At 24 h post-injection, different organs including heart, liver, spleen, lung, and kidney were harvested and then stained by Prussian blue and Eosin (Fig. 7). As shown Fig. 7a and magnified Fig. 7b, it is obvious that large amounts of nanoparticles distributed in the liver, which suggested large amount of Fe<sub>3</sub>O<sub>4</sub>@Gd uptake in the liver. A relatively small amount of Fe<sub>3</sub>O<sub>4</sub>@Gd uptake can also be

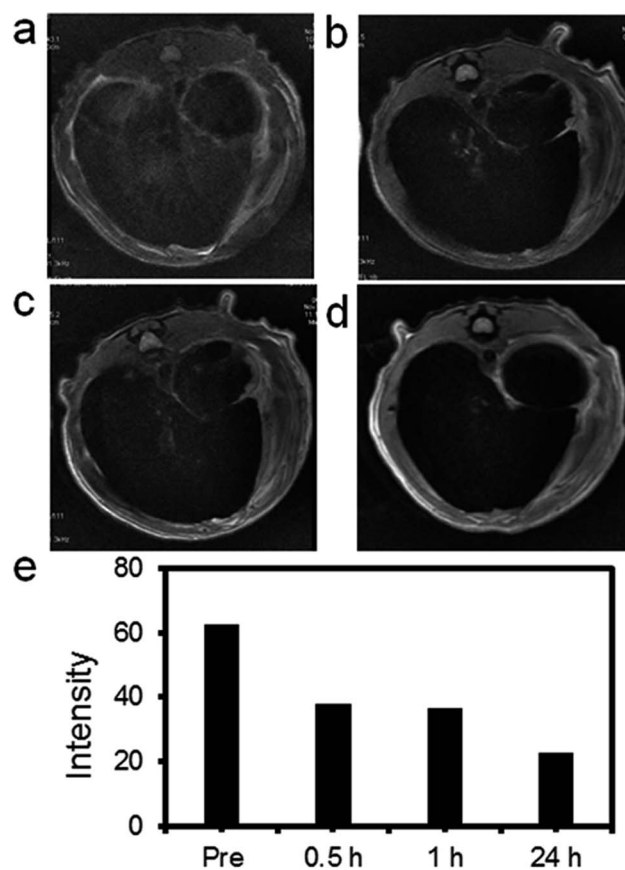


Fig. 6 MR images of rat liver before and after vein tail injection of Fe<sub>3</sub>O<sub>4</sub>@Gd nanoparticles (10 mg kg<sup>-1</sup>). (a) Pre-injection; (b) 30 min after injection; (c) 60 min after-injection; (d) 24 h after injection; (e) the corresponding  $T_2$ -weighted MR signal intensity of the liver.

found in the other organs, such as lung and kidney. There is almost no Fe<sub>3</sub>O<sub>4</sub>@Gd uptake in heart and lung.

## Discussion

Here we prepared Gd<sup>3+</sup> ions chelated Fe<sub>3</sub>O<sub>4</sub> nanoparticles as contrast agent for  $T_2$ -weighted MR imaging. Between the two components, one is  $T_1$  positive contrast agent and the other is  $T_2$  negative contrast agent. For the previous publications, the integration of these two components for MR contrast agents is mainly utilized as  $T_1$ - and  $T_2$ -dual mode MR contrast agent.<sup>21–23</sup> For instance, Bae, *et al.* reported a dual mode contrast agent Gd(DTPA) labelled IONP has  $r_2$  value of 30.32 mM<sup>-1</sup> s<sup>-1</sup> and  $r_1$  value of 11.17 mM<sup>-1</sup> s<sup>-1</sup> at 3.0 T with similar size.<sup>19</sup> Thorat *et al.* reported a multifunctional gadolinium-doped iron oxide nanoparticles for targeted magnetic hyperthermia, chemotherapy and  $T_1$ - $T_2$  dual-model magnetic resonance (MR) imaging with  $r_2$  value of 50.47 mM<sup>-1</sup> s<sup>-1</sup> and  $r_1$  value of 1.55 mM<sup>-1</sup> s<sup>-1</sup> at 3.0 T.<sup>24</sup>

A similar formulation based on Fe<sub>3</sub>O<sub>4</sub> and Gd<sup>3+</sup> has also been reported, Gd<sup>3+</sup> ions were introduced *via* three different methods including direct complex formation, covalent attachment and electrostatically and the results indicated only the nanoparticles

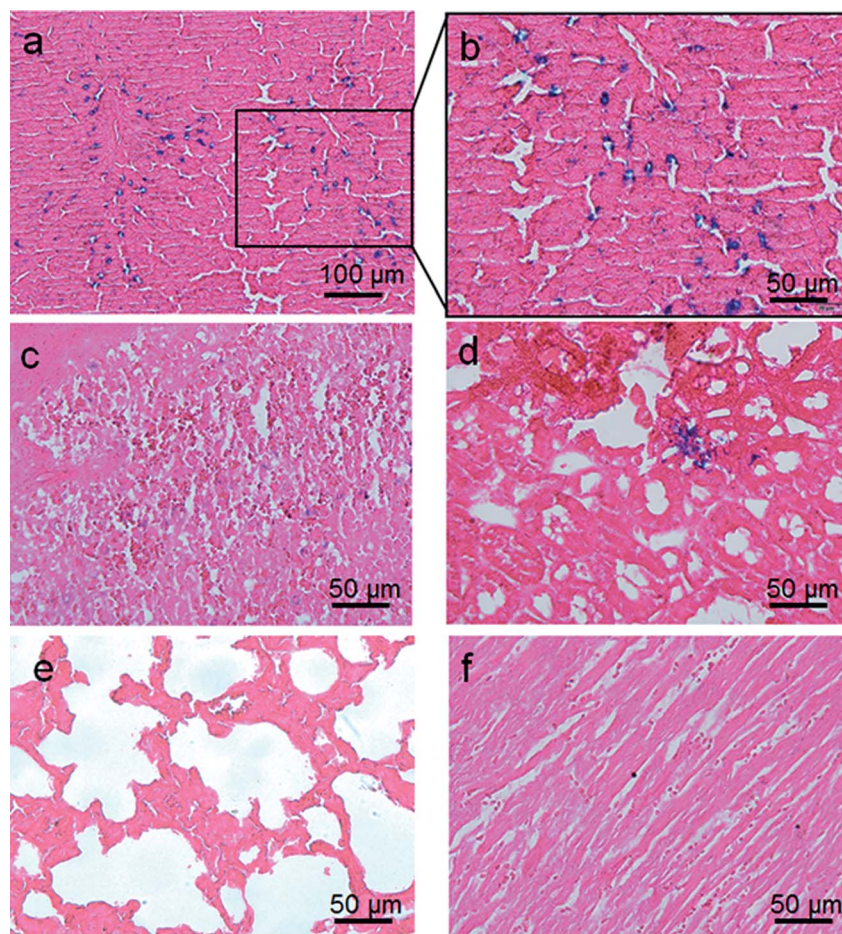


Fig. 7 Prussian blue staining images of the major organs of SD rats ((a and b) – liver, (c) – spleen, (d) – kidney, (e) – lung and (f) – heart). The sections were acquired from rat at 24 h after intravenous injection of  $10 \text{ mg kg}^{-1} \text{ Fe}_3\text{O}_4\text{@Gd}$  nanoparticles.

obtained by the following two methods work effective.<sup>25</sup> Here  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles were prepared by a very facile conjugate method. Amino modified  $\text{Fe}_3\text{O}_4$  nanoparticles were prepared by one-pot hydrothermal synthesis method and then coupled to DTPA and further chelated with  $\text{Gd}^{3+}$  ions. The  $r_2$  of  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles ( $202.06 \text{ mM}^{-1} \text{ s}^{-1}$ ) is higher than that of  $\text{Fe}_3\text{O}_4$  nanoparticles ( $131.89 \text{ mM}^{-1} \text{ s}^{-1}$ ). However, the introduction of  $\text{Gd}^{3+}$  has no obvious contribution for the enhancement of longitudinal relaxivity  $r_1$ , which is only  $1 \text{ mM}^{-1} \text{ s}^{-1}$ . This may be explained by the low content of Gd in our nanoparticles. This different influence of  $\text{Gd}^{3+}$  to longitudinal relaxivity and transverse relaxivity are also found by Huang *et al.*<sup>16</sup> Recently, some scientists proposed to classify a contrast agent with  $r_2/r_1 > 10$  as  $T_2$  agents.<sup>26</sup> Therefore, we named the  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles as  $T_2$  contrast agents. The reason why transverse relaxivity increased are not clear.

There are many factors affect the relaxivities, such as particle size, aggregation and surface modification. Therefore it is difficult to compare our nanoparticle to other formulation. However, the  $r_2$  relaxivity of  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles is higher than that of commercialized Feridex  $r_2$  ( $148.95 \text{ mM}^{-1} \text{ s}^{-1}$ ),<sup>19</sup> suggesting their  $T_2$  contrast effect was strong enough to be qualified as  $T_2$ -weighted MR contrast agents.

It is important to understand the biodistribution of the fabricated  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles for their bio-medical applications. The particles are mainly distributed in the liver without further modification, which is accordant with the imaging results *in vivo* MR. Besides, the nanoparticles are also found in spleen and kidney. The presence of  $\text{Fe}_3\text{O}_4\text{@Gd}$  nanoparticles in the kidney may suggest the nanoparticles could be cleared by kidney. Further pharmacokinetic studies of the nanoparticles at different time are necessary for a full understanding of the biodistribution.

## Conclusions

A new kind of  $T_2$ -weighted MR imaging contrast agents based on  $\text{Fe}_3\text{O}_4$  nanoparticles and  $\text{Gd}^{3+}$  ions were prepared. The introduction of  $\text{Gd}^{3+}$  increased the transverse relaxation rate of  $\text{Fe}_3\text{O}_4$  nanoparticles but still maintained their good biocompatibility. Both *in vitro* and *in vivo* studies showed the nanoparticles had an obvious MR enhancement.

## Conflicts of interest

The authors declare no conflict of interest.

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