

Deconstructing the role of myosin contractility in force fluctuations within focal adhesions

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ABSTRACT Force fluctuations exhibited in focal adhesions that connect a cell to its extracellular environment point to the complex role of the underlying machinery that controls cell migration. To elucidate the explicit role of myosin motors in the temporal traction force oscillations, we vary the contractility of these motors in a dynamical model based on the molecular clutch hypothesis. As the contractility is lowered, effected both by changing the motor velocity and the rate of attachment/detachment, we show analytically in an experimentally relevant parameter space, that the system goes from decaying oscillations to stable limit cycle oscillations through a supercritical Hopf bifurcation. As a function of the motor activity and the number of clutches, the system exhibits a rich array of dynamical states. We corroborate our analytical results with stochastic simulations of the motor-clutch system. We obtain limit cycle oscillations in the parameter regime as predicted by our model. The frequency range of oscillations in the average clutch and motor deformation compares well with experimental results.

SIGNIFICANCE The large variability in traction force measurements shows that it is imperative to understand the major regulatory parameters that set the magnitude of these forces and properly characterize the cell contractile state. In particular, these measurements in mature focal adhesions (FAs) reveal that individual FAs act autonomously, exhibiting either stable or dynamically fluctuating traction. We show the explicit role of myosin contractility analytically in these force fluctuations, in an experimentally relevant parameter space. With varying contractility, the system exhibits a rich array of dynamical states and shows stable limit cycle oscillations with frequencies comparable with those observed in experiments.

INTRODUCTION

Cellular migration plays a critical role in a host of biological processes starting from embryonic development to the immunological response of the cell as well as wound healing (1–6). The disruption of cellular migration can lead to cancer metastasis and other chronic inflammatory diseases. The process of cell migration involves the sophisticated regulation of the machinery of the actomyosin complex, comprising the actin filaments and the myosin motors, the adaptor proteins, which are linked to the actin, and their subsequent linking to the transmembrane proteins, which connect to the cell microenvironment (7–11). Both in vitro and in vivo experiments have provided in-depth understanding of the role of each of the individual components of this

extensive machinery as well as how they work in unison. In vitro studies on two-dimensional substrates have provided valuable information about how cells interact with the substrate and move on it and how cell speeds are modulated depending on several mechanical and chemical cues. Although the various components of this process are well known, the measurement of the mechanical forces shows significant variability at the cellular level (12–15), making it imperative to decipher the key parameters that regulate them.

The entire molecular assembly involved in cell migration, called the adhesion complex, is highly dynamic with a constant attachment/detachment kinetics between the various elements linking the cytoskeleton to the extracellular matrix. The combined effect of the myosin motors exerting contractile forces and the polymerization of filamentous actin pushing against the cell membrane drives a “retrograde flow” of actin toward the center of the cell. The “molecular clutch” hypothesis posits the focal adhesions (FAs)

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as mechanical clutches that act as dynamic linkages in the transmission of forces between the actin filament and the transmembrane proteins, converting the retrograde flow to forward movement of the cell (16) (Fig. 1 a).

Apart from the *in vitro* and *in vivo* experimental studies, theoretical models have been proposed, which have proved helpful in understanding cell migration both at the cellular and molecular scales. Earlier theoretical studies (17–29) have predominantly looked at the response of the cell to varying substrate rigidity and predict a biphasic relationship between rigidity and force, i.e., forces first increase and then decrease with rigidity. DiMilla et al. (17) combined a viscoelastic-solid model for a cell and adhesion receptor-ligand binding kinetics for the adhesion bonds to predict how the movement of the cell on a rigid substrate can vary with contractility and receptor-ligand kinetics. In certain parameter regimes, the cell speed was shown to be biphasic, with the maxima decided by a balance between contractility and adhesiveness. Using a force-based dynamic approach, Zaman et al. (30) developed a computational model for cell migration in three-dimensional matrices. Similar to the situation in two-dimensional substrates, a biphasic behavior of cell speed with varying adhesivity is predicted. Transmembrane proteins such as integrins have been modeled as Hookean springs with detachment rates increasing with the load force, demonstrating that the clustering of proteins increases with the increase of the stiffness of the substrate. A stochastic motor-clutch model introduced by Chan and Odde (21) was able to describe the load-and-fail characteristic of cellular force transmission, which has been observed experimentally in migrating cells. This model takes the force-velocity relationship of the myosin motors into account, incorporates the load-and-fail dynamics of cellular adhesions, and predicts an optimal stiffness of the substrate when the force transmission is maximal, and the actin retrograde flow is minimal.

Recent experiments using time-lapse traction force microscopy have shown that the local forces exerted by indi-

vidual FAs vary spatiotemporally, suggestive of a repeated tugging of the extracellular matrix/substrate (9,15). Mature FAs exist in two states: a stable state with spatially and temporally invariant traction and a dynamic state in which they fluctuate indicative of a tugging mechanism on the extracellular membrane. These force fluctuations are a possible molecular mechanism for the cell to tightly control cellular movement based on any environmental cues (31,32). The physical understanding of the fluctuations within an integrated cell migration model is an open problem. Myosin contractility is one of the ideal candidates to give rise to these fluctuations since earlier mathematical models have predicted that the collective activity of motors on elastic materials can lead to spontaneous oscillations in the activity of local contractile units (33).

In this paper, we theoretically explore the specific role of myosin II activity in the molecular clutch setting (13,34–43). Activity in myosin II is incorporated via both by its attachment-detachment dynamics with the actin filament, and the velocity of the attached myosin motor proteins (MPs). How does the variation of the activity of these motors affect the dynamical stability of the molecular clutch system? Furthermore, can we quantitatively estimate the local fluctuations resulting from the spontaneous oscillations of these local contractile units? Unlike earlier theoretical models, we focus instead on the stability of the MP-actin-clutch sector only and show that a variation of the activity of myosin motors gives rise to a multitude of dynamical states. Specifically, for a wide range of experimentally accessible parameter space, the system exhibits spontaneous decaying oscillations in a stable spiral region crossing into a stabilized, oscillatory region via a supercritical Hopf bifurcation (44). We also discuss the specific nature of these oscillations and their connection to the traction force fluctuations observed in the experiments. We incorporate stochasticity into the problem and show that the primary features of the model are retained.

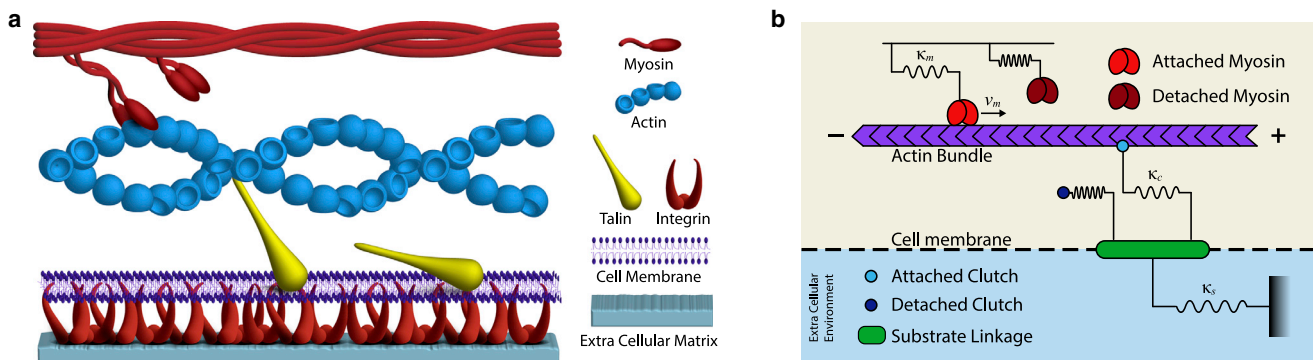


FIGURE 1 (a) Schematic of the cell migration machinery showing the myosin motors and actin bundle that constitute the cytoskeletal network. Adapter proteins (talin) and transmembrane proteins (integrin) form the focal adhesions (FAs) linking the cytoskeletal network to the extracellular matrix/substrate. (b) Motor-clutch model showing the motors and clutches as elastic springs and an inextensible actin bundle with \pm showing the anterograde/retrograde directions. To see this figure in color, go online.

METHODS

Model description

We consider a geometric arrangement consisting of a filamentous actin bundle in the vicinity of myosin II motors and molecular clutches (21–23). The myosin motors are rigidly fixed at one end while the other end attaches to the F-actin bundle and induces a retrograde flow by applying a force on the bundle. Molecular clutches have one end irreversibly attached to a substrate while the other end engages reversibly with the F-actin bundle and resist the retrograde flow. The force that is built up in the attached molecular clutches leads to a traction force that is balanced by the tension and deformation in the substrate as depicted in Fig. 1 b. In our model, we consider the motor-clutch and substrate sector as separate blocks with the substrate deformation solely governed by the dynamical force balance in the motor-clutch sector.

Myosin contractility and the resultant force generation is dependent on its attachment-detachment dynamics (45,46). Myosin motors are modeled as stretchable springs, which, due to energy consumption via the hydrolysis of ATP, undergo attachment-detachment dynamics to/from the F-actin bundle. One end of the spring is fixed while the other end attaches (detaches) to (from) the F-actin with rates ω_a and ω_d , respectively. Following well-established theoretical approaches for molecular motors, their detachment rates are considered to increase exponentially with a load force $|f_i|$ as $\omega_d = \omega_d^0 \exp(|f_i|/f_d)$, where f_d sets the force scale and ω_d^0 is the bare detachment rate. Extension y^i of the i -th MP leads to a load force $f_i^j = \kappa_m y^i$, where κ_m is the force constant. Thus the average load force on motors is $f_l = \kappa_m y$, where $y = \frac{1}{n_m} \sum_{i=1}^{n_m} y^i$ denotes the average extension of these MPs. With N_m MPs available on average and n_m of them attached to the actin bundle at time t , the kinetics of the attached MPs is given by

$$\frac{dn_m}{dt} = \omega_a(N_m - n_m) - \omega_d^0 n_m \exp\left(\frac{|f_l|}{f_d}\right). \quad (1)$$

In their attached state, MPs move along the filament bundle with a velocity $v_m(f_i)$, which is dependent on the load force that it experiences, predominantly toward one end of the filament. We model this behavior with the piecewise linear force-velocity relation

$$v_m(f_i) = \begin{cases} v_u & \text{for } f_i \leq 0 \\ v_u \left(1 - \frac{f_i}{f_s}\right) & \text{for } 0 < f_i \leq f_s \\ v_b & \text{for } f_i > f_s \end{cases}, \quad (2)$$

where f_s is the stall force when the MP ceases to move, v_u is the intrinsic motor velocity without load, and v_b is a back velocity.

The motion of the MPs on the actin bundle induces the retrograde motion of the actin. The clutches are also modeled as extensible elastic springs with spring constant κ_c . One end of a clutch is attached to the actin bundle while the other end is attached to an elastic substrate with stiffness k_s (Fig. 1 b). Retrograde motion of the actin bundle due to myosin contractility leads to an extension x_c^i in the i -th attached clutch. The substrate extension, x_s , is determined by an elastic force balance between the total force due to the attached clutches and the spring force due to the substrate. We consider N_c to be the total number of available clutches, n_c as the number of clutches attached at a given time, and $x_c = \frac{1}{n_c} \sum_{i=1}^{n_c} x_c^i$ as the average extension of connected clutches. The dynamics of the average clutch deformation x_c is determined by a mechanical balance of forces in the over-damped limit,

$$\Gamma \frac{dx_c}{dt} = -n_m \kappa_m y - n_c \kappa_c x_c, \quad (3)$$

where the viscous force due to motion of clutches, designated by viscous friction coefficient Γ , is balanced by the total restoring forces of both mo-

tors and clutches. Note that the negative sign in the force expression for the clutches in the above equation is a matter of convention since x_c takes negative values. Within our assumption of treating the motor-clutch sector and substrate sector as separate blocks, the deformation of the substrate can be independently calculated using the force balance $k_s x_s = -n_m \kappa_m y - n_c \kappa_c x_c$. This allows us to focus on the stability of the motor-clutch sector alone.

The rate of mean extension of an attached MP is determined by the active motor velocity v_m on the filament and the rate of average deformation of the attached clutches. This is given as

$$\frac{dy}{dt} = v_m(f_i) + \frac{dx_c}{dt}. \quad (4)$$

Clutches undergo attachment-detachment dynamics with rates k_{on} and k_{off} , respectively. The clutch detachment rate is again assumed to be exponentially increasing with the load force, $k_{off} = k_{off}^0 \exp(|f_l^c|/F_b)$, where F_b is the force scale for bond rupture. Similar to the MPs, the average load force on clutches is $f_l^c = \kappa_c x_c$. The attachment-detachment dynamics of the clutches gives rise to the following rate equation

$$\frac{dn_c}{dt} = k_{on}(N_c - n_c) - k_{off}^0 n_c \exp\left(\frac{|f_l^c|}{F_b}\right). \quad (5)$$

We present a detailed analysis of the stability of the MP-filament-clutch system, emphasizing the effect of the activity of myosin motors both in terms of the motor velocity and attachment/detachment kinetics. The physical parameters used in our model are described in Table 1. Choosing the length, time, velocity, and force scales as $l_0 = (k_b T / \omega_d^0 \Gamma)^{1/2}$, $\tau = 1 / \omega_d^0$, $v_0 = l_0 \omega_d^0$, and $f = (\omega_d^0 \Gamma k_b T)^{1/2}$, respectively, Eqs. 1, 3, 4 and 5 are cast in dimensionless form with $\tilde{\omega} = \omega_a / \omega_d^0$, $\tilde{v}_u = v_u / v_0$, $\tilde{k}_{on} = k_{on} / \omega_d^0$, $\tilde{k}_{off} = k_{off} / \omega_d^0$, $\tilde{x}_c = x_c / l_0$, $\tilde{y} = y / l_0$, $\tilde{\kappa}_c = \kappa_c l_0 / f$, $\tilde{\kappa}_m = \kappa_m l_0 / f$, and $\tilde{f}_s = f_s / f$ (see supporting material: Appendix A). Attachment/detachment dynamics is varied using a turnover ratio defined as $\Omega = \omega_a / (\omega_a + \omega_d^0)$. A dynamical modeling of the system provides us with the basic building blocks of understanding the mechanics of motility in the absence of noise. We proffer a *linear stability analysis* of the system, numerical solutions of the differential equations, illustrate the morphologies, and characterize the detailed dynamics.

Stochastic simulation of a motor-clutch system

We model the actin filament as a rigid string of connected $\sigma = 5.5$ nm segments (45,51). The i -th myosin motor can attach to an actin segment stochastically with the rate ω_a . At the moment of attachment, the extension of the MP, y^i , is zero. Post attachment, the MP moves by a length scale σ toward the plus (minus) end of the actin filament with a velocity v_m , where

TABLE 1 Physical parameters present in the system

Parameter	Symbol	Values
Motor attachment rate	ω_a	40 s ⁻¹ (47)
Motor detachment rate	ω_d^0	350 s ⁻¹ (47)
Total number of motors	N_m	100
Clutch attachment rate	k_{on}	1 s ⁻¹ (21)
Clutch detachment rate	k_{off}	0.1 s ⁻¹ (21)
Back velocity	v_b	0.2256 μ m s ⁻¹ (47)
Stall force	f_s	4.96 pN (47)
Detachment force	f_d	2.4 pN (48)
Clutch bond rupture force	F_b	6.25 pN (22)
Motor spring constant	κ_m	0.3 pN/nm (47)
Clutch spring constant	κ_c	0.03144 pN/nm (49)
Viscous friction coefficient	Γ	893 k _B Ts/ μ m ² (50)

v_m is given by Eq. 2. The total extension of the attached MP, y^i , is determined by the active motor velocity v_m on the filament and the deformation of the attached clutches. The MPs detach from the actin filament with a rate $\omega_d = \omega_d^0 \exp(\kappa_m |y^i| / f_d)$.

The i -th clutch undergoes attachment and detachment dynamics with rates k_{on} and $k_{off} = k_{off}^0 \exp(\kappa_c |x_c^i|)$, respectively. After attachment, the clutch deformation x_c^i is determined from the following stochastic equation

$$\Gamma \dot{x}_c^i = - \sum_{i=1}^{n_m} \kappa_m y^i - \sum_{i=1}^{n_c} \kappa_c x_c^i + \sqrt{2\Gamma k_B T} \eta_T(t), \quad (6)$$

as opposed to Eq. 3. Here, $\eta_T(t)$ is a Gaussian noise with $\langle \eta_T(t) \rangle = 0$ and $\langle \eta_T(t) \eta_T(t') \rangle = \delta(t - t')$. We numerically integrate the above equation using a Euler-Maruyama scheme with time steps small enough that the probability of each event is less than one. The stochastic simulations were performed using programs written in Fortran.

RESULTS

The steady-state solutions, i.e., the fixed points $\tilde{x}_c^0, \tilde{y}_0, n_m^0$, and n_c^0 , of the scaled dynamical equations are obtained as $\tilde{y}_0 = \tilde{f}_s / \tilde{k}_m$, $n_m^0 = \tilde{\omega} N_m / (\tilde{\omega} + \exp(\tilde{f}_s / \tilde{f}_d))$, and $\tilde{x}_c^0 = - n_m^0 \tilde{f}_s / n_c^0 \tilde{k}_c$. Thus, the extension of the clutches in steady state is governed by the ratio of the numbers of attached motors and attached clutches. n_c^0 is determined by solving the transcendental equation,

$$\tilde{k}_{on} (N_c - n_c^0) = \tilde{k}_{off} n_c^0 \exp\left(\frac{n_m^0 \tilde{f}_s}{n_c^0 \tilde{F}_b}\right). \quad (7)$$

This equation, as we shall see, gives rise to a saddle-node bifurcation with two branches—one stable and another unstable.

The stability of these fixed points is tested by studying the time evolution of small perturbations away from the steady state. In that vein, the dynamical equations representing the system in terms of MP extension, clutch extension, number of attached motors, and number of connected clutches can be linearized in matrix form, $\frac{d}{dt}[\delta \tilde{x}_c, \delta \tilde{y}, \delta n_m, \delta n_c]^T = \mathbf{J}[\delta \tilde{x}_c, \delta \tilde{y}, \delta n_m, \delta n_c]^T$. Eigenvalues of the 4×4 Jacobian matrix \mathbf{J} (see supporting material: Appendix B), determine the linear stability of the dynamical system. The eigenvalues are calculated by solving the fourth-order characteristic polynomial equation,

$$P(\lambda) = \lambda^4 + \mathcal{A}\lambda^3 + \mathcal{B}\lambda^2 + \mathcal{C}\lambda + \mathcal{D}, \quad (8)$$

where \mathcal{A} , \mathcal{B} , \mathcal{C} , and \mathcal{D} are the coefficients that are given in terms of the scaled parameters (see supporting material: Appendix B).

The nature and properties of the eigenvalues are dependent on the sign of the coefficients \mathcal{A} , \mathcal{B} , \mathcal{C} , and \mathcal{D} . We note that \mathcal{A} is always real positive; however, the other three coefficients can change sign and different combinations of those signed coefficients determine the nature of the roots of the quartic polynomial and related dynamical phases.

With λ_k ($k = 1 \dots 4$) denoting the eigenvalues, we get the following combination: 1) all real negative eigenvalues corresponding to stable nodes where a perturbation decays exponentially with time; 2) two real negative and two real positive—both these combinations correspond to the unstable phase with exponentially growing perturbations; 3) two real negative and two eigenvalues with $\lambda_{3,4} = -\alpha \pm i\beta$ resulting in stable spiral phase with decaying oscillations; and 4) two real negative and two eigenvalues with $\lambda_{3,4} = \alpha \pm i\beta$ corresponding to the unstable spiral phase with growing oscillations. We proceed with determining the closed-form expressions for the possible phase boundaries present in our system. *Wolfram Mathematica* (52) was used to numerically solve the dynamical equations using *Implicit Differential-Algebraic Solver* (53).

Phase boundary separating saddle-node bifurcated stable and unstable branches

The stability of the two branches arising from a saddle-node bifurcation in Eq. 7 can be characterized by checking the sign of its derivative. A negative/positive value will represent a stable/unstable branch of fixed points and the *bifurcation point* can be obtained by solving Eq. 7 while simultaneously setting its derivative with respect to n_c^0 to zero. The derivative equation is computed below,

$$-\tilde{k}_{on} - \left[\tilde{k}_{off} \exp\left(\frac{n_m^0 \tilde{f}_s}{n_c^0 \tilde{F}_b}\right) - \tilde{k}_{off} \frac{n_m^0 \tilde{f}_s}{n_c^0 \tilde{F}_b} \exp\left(\frac{n_m^0 \tilde{f}_s}{n_c^0 \tilde{F}_b}\right) \right] = 0, \quad (9)$$

with trivial algebra, it can be easily shown that this is exactly the same as the phase boundary equation at $D = 0$,

$$n_c^0 \tilde{k}_{on} \tilde{F}_b + \tilde{k}_{off} \exp\left(\frac{n_m^0 \tilde{f}_s}{n_c^0 \tilde{F}_b}\right) (\tilde{F}_b n_c^0 - \tilde{f}_s n_m^0) = 0. \quad (10)$$

The bifurcation point is then calculated and marked in Fig. 2 with a red dot. Using Eq. 7 one can simplify Eq. 10 and attain the following,

$$N_c n_c^0 \tilde{F}_b = n_m^0 \tilde{f}_s (N_c - n_c^0). \quad (11)$$

Confirming the presence of an unstable branch in the $D < 0$ region, we shift our focus on the stable branch, where $D > 0$, and investigate the geometric properties of the quartic polynomial with the change in sign of \mathcal{B} and \mathcal{C} . In the region where N_c is lower than its value at the bifurcation point, due to the absence of fixed points of n_c^0 the system loses stability and remains unstable regardless of v_u . Therefore, this region is marked unstable on the phase diagram in Fig. 3 a. Furthermore, the condition $B > 0$ remains valid throughout the scanned parameter regime. Consequently, the properties of coefficient \mathcal{C} associated with the linear part of the polynomial $P(\lambda)$ mostly governs the nature of the eigenvalues.

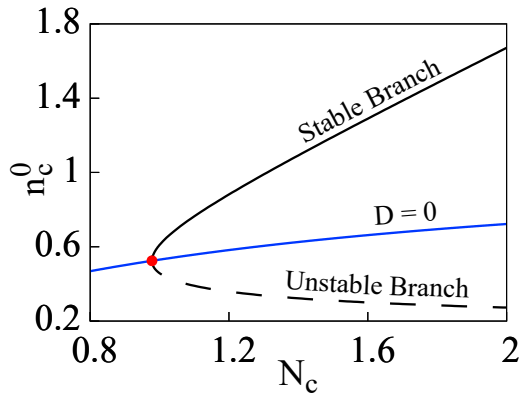


FIGURE 2 Transcendental nature of the n_c^0 equation leads to a saddle-node bifurcation with distinguishable branches—solid black curve representing the stable branch and dashed black line denoting the unstable one. The red point denotes the bifurcation point of the system. To see this figure in color, go online.

Phase boundary between (un)stable nodes and (un)stable spiral phases

The quartic polynomial $P(\lambda)$ is bound from below as the term λ^4 comes with positive sign and has got two minima and one maximum. Sign of C controls the position of the minimum closer to the origin as B remains positive. When P_m , a minimum of $P(\lambda)$ occurring near the origin, with $\lambda = \lambda_m$, crosses the negative λ axis (positive λ axis), it turns two complex conjugate eigenvalues with negative (positive) real parts into real negative (real positive). Therefore, $P_m = 0$ denotes a boundary between phases with either a node or a

spiral (refer to Fig. 3), where $C > 0$ ($C < 0$) provides a sufficient condition for concluding that these fixed points are stable (unstable). A necessary and sufficient condition can be obtained by finding the equation of a second phase boundary which can be derived from the fact that we have two degenerate real roots λ_m at the boundary. Thus comparing the coefficients of various powers of λ with those in Eq. 8, we obtain a closed-form equation of the stability boundary,

$$\begin{aligned} 2AD(-9A^2BC + 2AB^3 + 3AC^2 + 40B^2C) \\ + D^2(27A^4 - 144A^2B + 192AC + 128B^2) \\ + C^2(4A^3C - A^2B^2 - 18ABC + 4B^3 + 27C^2) \\ = 16D(B^4 + 9BC^2 + 16D^2) \end{aligned} \quad (12)$$

Phase boundary between stable spirals and unstable spirals

An oscillation increasing in time appears in the system, switching from decaying oscillation as the parameter values are tuned. It is characterized by a change in complex conjugate eigenvalues from $(-\alpha \pm i\beta)$ to $(\alpha \pm i\beta)$, which is an occurrence of a dynamical transition between stable spiral (SS) and unstable spiral (US). The sign of the real part of the complex conjugate roots α is opposite in either sides of the boundary and, thereupon, $\alpha = 0$ is the condition of the associated phase boundary. Following the prescription of the previous case, we calculate the equation of the boundary as,

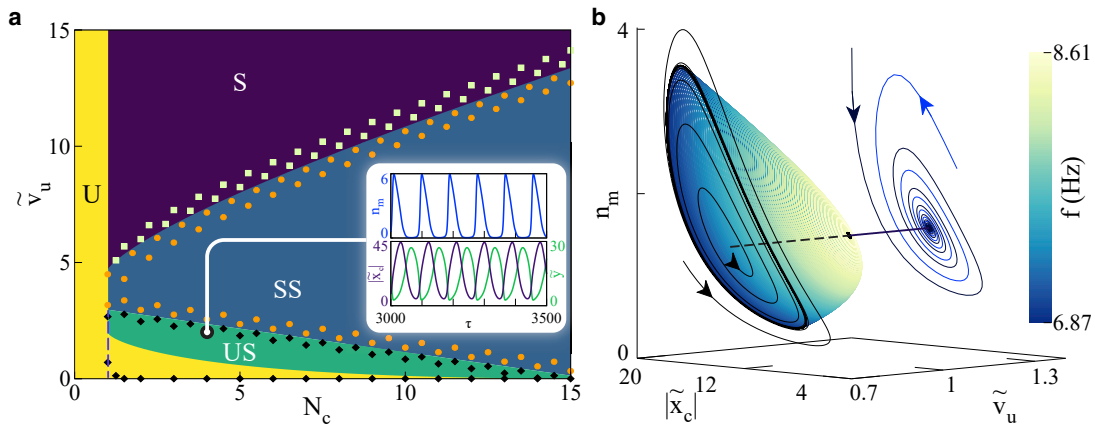


FIGURE 3 (a) Phase diagram depicting dynamical phases in the N_c - \tilde{v}_u plane: phase boundaries predicted by stability analysis and the resultant dynamical phases are portrayed using colored regions with labels—S, stable; SS, stable spirals; US, unstable spirals; and U, unstable. The unstable region consists of two parts—one arising from an absence of fixed points and another from the loss of stability due to $C < 0$. A dashed line is used to separate them. Colored points are obtained by solving the dynamical equations numerically near the phase boundaries—stable (●); and limit cycle oscillations (◆). The range of \tilde{v}_u is equivalent to 0–9 $\mu\text{m/s}$, in physical units. The phase boundary demarking Hopf bifurcation, i.e., between US and SS, is provided by Eq. 13, while the boundaries between U/US and SS/S are governed by Eq. 12. (Inset) Time evolution: at $N_c = 4$ and $\tilde{v}_u = 2$ the system shows stable limit cycle oscillations and corresponding evolution of n_m , \tilde{y} , and $|\tilde{x}_c|$ are shown in panels. The ranges of $|\tilde{x}_c|$ and \tilde{y} are equivalent to 0–80 and 0–53 nm, respectively, in physical units. The time t ranges from 8.5 to 10 s. (b) Supercritical Hopf bifurcation: at $N_c = 10$, the system shows decaying oscillations at higher values of \tilde{v}_u and stable limit cycle oscillations through a supercritical Hopf bifurcation as \tilde{v}_u is lowered. The straight line shows the fixed points in the n_m - $|\tilde{x}_c|$ plane. Solid (dashed) line denotes their stable (unstable) nature. As the limit cycle grows with decreasing \tilde{v}_u , its frequency starts to reduce. Here \tilde{v}_u and $|\tilde{x}_c|$ range from 0.4 to 0.8 $\mu\text{m/s}$ and 7 to 35 nm, respectively, in physical units. To see this figure in color, go online.

$$ABC = A^2D + C^2. \quad (13)$$

SS to US transition is the route through which stable limit cycle oscillation sets in the system via non-linear effects leading to Hopf bifurcation. At the bifurcation boundary, we can work out an expression for the frequency as $f_\omega = (2\pi)^{-1} \sqrt{C/A}$.

Force fluctuations: Regulatory pathway via Hopf bifurcation

To quantify the explicit effect of myosin activity, we present a phase diagram in \tilde{v}_u and N_c plane that illustrates the different dynamical behaviors of the motor-clutch system (Fig. 3 a). As observed earlier, N_c controls the saddle-node bifurcation and v_u regulates the activity of the myosin motors, providing an apt parameter space for the model mechanics. Earlier experimental studies (54–56) have established myosin force-velocity relations and ensemble measurements with unloaded motor velocities. We used the broad range of 0–10 $\mu\text{m/s}$ for v_u in our study. These predictions are evaluated by the numerical solutions of the differential equations over the entire parameter space. The phase boundaries predicted by the linear stability analysis are exact. At high motor velocities, the system is in a stable state. As the motor velocity is reduced, the system moves into a stable spiral state as seen by the inward spiraling curve in the $n_m - x_c$ phase plane (Fig. 3 b). With sufficient number of clutches available, as \tilde{v}_u is lowered, the oscillations in the stable spiral region take gradually increasing amount of time to decay and cross into a stabilized, oscillatory region via a supercritical Hopf bifurcation. This indicates a limit cycle around an unstable fixed point in the $n_m - x_c$ plane. The temporal oscillations of the clutch and motor deformations in the US regime are shown in Fig. 3 a (inset). At sufficiently low motor velocities, \tilde{v}_u , the system moves from a region of instability to US on increasing N_c .

The physical understanding of the stability mechanism in the motor-clutch system is achieved via two balancing acts: stalling of motors with a particular extension given by $\tilde{k}_m \tilde{y}_0 = \tilde{f}_s$ and the force balance $n_m^0 \tilde{f}_s = n_c^0 \tilde{k}_c (-\tilde{x}_c^0)$. The modalities of this mechanism are corroborated by the numerical solutions of the dynamical equations across a range of active velocities in Fig. 4. At high ATP concentrations, motor velocities (v_u) are high (Fig. 4 a), leading to large extensions and hence stalling of motors is quickly established. The clutch extension attains the overall force balance condition and the system becomes stable. With higher number of clutches, stability is attained at higher \tilde{v}_u . At low ATP concentrations (Fig. 4, b and c), with slower moving motors, the forces exerted by motors on the actin filaments result in slow retrograde movement of the filament, which in turn reduces motor deformation \tilde{y} and increases clutch extension \tilde{x}_c . Reduction in \tilde{y} results in an increase in the number of motors

(n_m) with time, resulting in further retrograde movement of the actin filament. Leftward movement of the filament is stopped when n_m reaches its maximum, whereas \tilde{x}_c and n_c are at their near maximum and minimum, respectively. Beyond this point, slow motor velocity results in detachment of motors and the stored energy in the deformed clutch sector ensures the anterograde movement of the filament. Motor detachment continues, and the filament moves toward less and less clutch deformation until it reaches a minimum. \tilde{y} attains maximum and the motor attachment rate takes over its detachment rate as n_m becomes minimum. The cycle continues. At very low ATP concentrations, with the motor velocities (v_u) very small (Fig. 4 d), the deformation \tilde{y} continues to go down with the retrograde movement of the actin filament. However, after reaching force balance, the extremely slow movement of the motors means that the motor extension beyond the point is never realized. The clutches on the other hand are at their highest extension and, with no relief, fail completely, which leads to instability.

In Fig. 5, we vary myosin turnover, Ω , by tuning the attachment rates of myosin. This provides another experimentally tunable mechanism of changing myosin contractility. The phase diagram shows that, with increasing Ω , the phase boundaries between the unstable (U)–US and US–SS shifts toward larger \tilde{v}_u and N_c , and the area enclosed between them expands. This signifies that the MPs that have a higher tendency to attach will also result in more persistent limit cycles over larger areas in the parameter space.

Examining our system with tunable total motor/clutch numbers allows us to probe the dynamic behavior under another important experimentally viable parameter space. Linear stability analysis in this space leads to the same array of dynamic phases seen before. We also test the robustness of predicted phase boundaries by incorporating numerical solutions to the differential equations shown in Fig. 6 a. Time evolutions of motor and clutch extensions at two points of interests on the phase diagram are portrayed in the accompanying plots in Fig. 6 b. We indeed find that, for a given value of the motor velocity, there is a minimum number of motors and clutches required to observe the oscillations.

Simulation output validates the motor-clutch model

To check our results, we first consider the special case where all clutches are attached permanently i.e., $k_{\text{off}} = 0$. To present a comparison between the theoretical model and the numerical simulations, we first present the results from the dynamical equations. We now have three coupled differential equations in the number of attached motors (n_m), the average deformation of a clutch (x_c) and the average deformation of a molecular motor (y). We obtain the steady-state solution of the coupled scaled differential equations as $\tilde{y}_0 = \tilde{f}_s / \tilde{k}_m$, $n_m^0 = \tilde{\omega} N_m / (\tilde{\omega} + \exp(\tilde{f}_s / \tilde{f}_d))$,

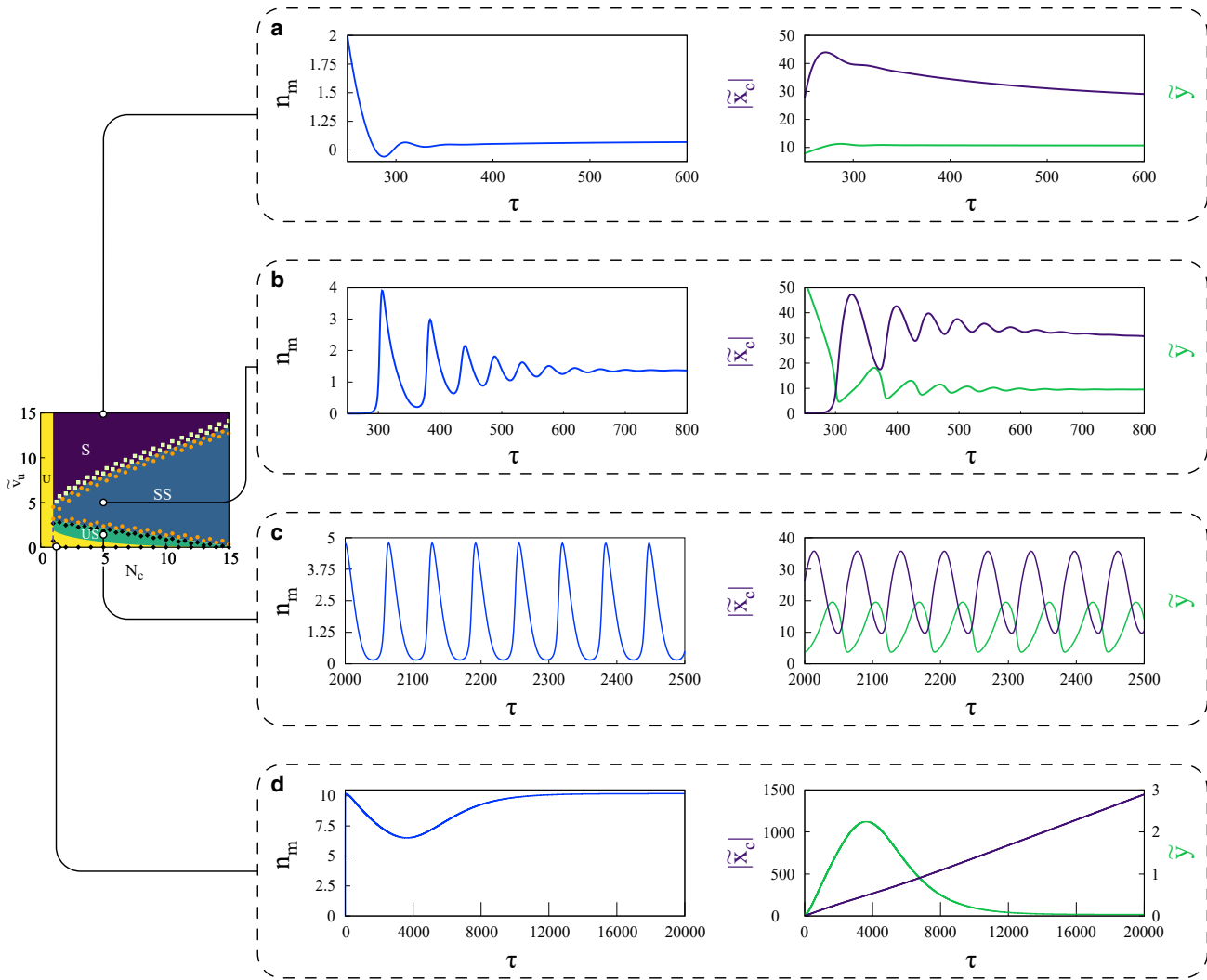


FIGURE 4 Dynamics of the active system: numerical solutions of the dynamical equations at different points in the $N_c - \tilde{v}_u$ phase plane elucidate the dynamical phases predicted by linear stability analysis. The range of \tilde{v}_u is equivalent to 0–9 $\mu\text{m/s}$, in physical units. At high \tilde{v}_u region (a), the system is quickly stabilized as it reaches steady-state solutions, while relatively lower \tilde{v}_u at (b) ensures that the system follows a path of decaying oscillations. It is at (c) that the system showcases self-sustaining limit cycle oscillations after crossing the supercritical Hopf bifurcation boundary. As predicted by linear stability analysis, critically low values of \tilde{v}_u and N_c ensure that the system is unstable, as evident by runaway clutch deformation. The range of extensions are equivalent to 0 to 70–88 nm in the first three plots. In (d), x_c ranges within 0–2,650 nm, while y remains between 0 and 5 nm. Ranges of time in physical units are 0.6–1.7 s in (a), 0.6–2.3 s in (b), 5.7–7.1 s in (c), and 0–57 s in (d). To see this figure in color, go online.

and $\tilde{x}_c^0 = -n_m^0 \tilde{f}_s / N_c \tilde{\kappa}_c$. The transcendental equation in n_c^0 is now replaced by the constant N_c , as all the clutches are now bound. We perform a linear stability analysis by studying the time evolution of small perturbations away from the steady state. This leads to a third-order characteristic polynomial equation in the eigenvalues λ as $P'(\lambda) = \lambda^3 + A'\lambda^2 + B'\lambda + C'$, where A' , B' , and C' are the new coefficients given in terms of scaled parameters (see [supporting material](#): Appendix D for details).

The coefficients determine the dynamical behavior of the system, which has four different phases characterized by the different combinations of the three eigenvalues: 1) all three eigenvalues real negative that result in stable nodes; 2) one negative and two real positive giving rise to a linearly unsta-

ble phase; 3) one real negative and two complex conjugate with negative real part, characterizing a stable spiral phase with decaying oscillations; and 4) one real negative and two complex conjugate roots with positive real part characterizing an US phase with oscillations of growing amplitude. We can determine the different phase boundaries analytically as before. However, to show the comparison with numerical simulations that incorporate stochasticity as described above we concentrate on the phase boundary between the SS and US phases. The condition for the phase boundary is $C' - A'B' = 0$. Using numerical simulations we show how the growing amplitudes of the oscillations in the US phase are stabilized by non-linearities into stable limit cycle oscillations.

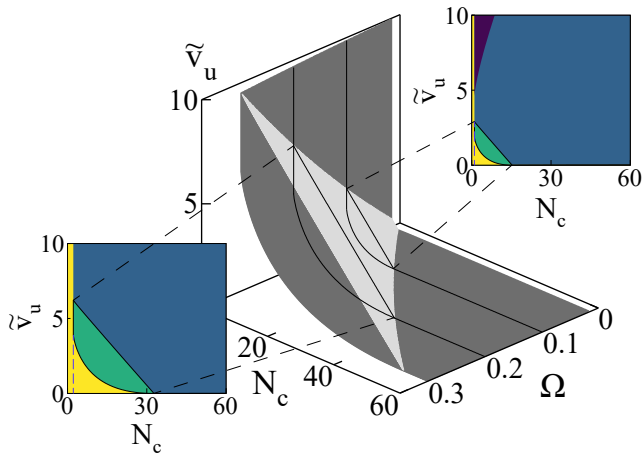


FIGURE 5 Evolution of phase boundaries with varying active velocity \tilde{v}_u and myosin turnover Ω : increasing both the active velocity and motor attachment rates result in growth of areas enclosed by the phase boundaries, namely the boundaries separating U and US phases (dark gray) and the Hopf bifurcation boundaries (light gray). We focus on two slices obtained at duty ratios 0.1 and 0.2, respectively. The enclosed areas (green) in the resulting phase diagrams clearly establish this expansion. The range of \tilde{v}_u is equivalent to 0–6 $\mu\text{m/s}$, in physical units. To see this figure in color, go online.

In Fig. 7 a, we present the phase diagram of the system in the $\tilde{v}_0 - \tilde{f}_d$ plane. As we can observe, there are four phases, with two being of particular interest: 1) corresponding to the stable spiral phase SS characterized by decaying oscillations, and 2) corresponding to the unstable spiral phase US characterized by stable limit cycle oscillations. We also plot the phase boundary as obtained from our analytical estimates, which shows reasonable agreement with the simulations. In the inset of Fig. 7 a, we show the dynamical behavior of the scaled clutch deformation \tilde{x}_c and the scaled motor extension \tilde{y} in the stable limit cycle phase. The slow

extension and the rapid decay of the clutch deformation is reminiscent of the rapid detachment of MPs. The parametric plot in Fig. 7 b, shows a stable limit cycle as expected. The spread in the trajectories underlines the stochastic nature of the simulations.

Having established the simulation model, we advanced to verify the results for the situation where the clutches are free to attach/detach to/from the actin filament. In Fig. 8 a, we show the phase diagram obtained using the equations as described in methods. As before, we see the five different phases with the different phase boundaries. In Fig. 8 b, we show a comparison of the limit cycle oscillations between the theoretical calculations and numerical simulations incorporating stochasticity arising from different sources—attachment/detachment of MPs and clutches to/from the actin filament, stochastic extension of attached clutches and MPs, and finally the Gaussian noise. As we can observe, we do recover stable limit cycle oscillations in the given parameter regime as predicted by our theoretical study.

DISCUSSION

The variability of cell traction force measurements suggests that a mere readout of these forces may not be optimal in understanding the processes that regulate force generation and subsequent transmission (12–15). It also points to the possibility that a large part of the mechanical work due to actomyosin contractility is dissipated. Therefore there is a need to discern the role of individual parameters in deciphering the mechanisms that regulate force generation. In this work, we have established the explicit role of myosin activity in generating rich dynamics within individual focal adhesion complexes, focusing our attention on a subset of the force regulation machinery involving the MPs and

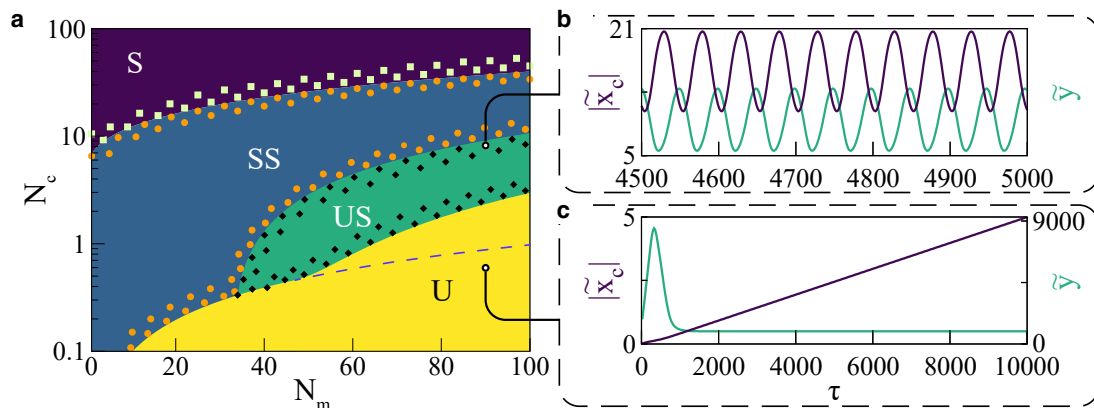


FIGURE 6 (a) Phase diagram in the $N_m - N_c$ plane: tuning total numbers of motors and clutches simultaneously at a fixed $\tilde{v}_u = 1$ leads to a phase diagram with dynamical phases discussed before—S, stable; SS, stable spirals; US, unstable spirals; and U, unstable. A dashed line is used to separate the two unstable regions discussed previously. The colored points are used following the convention from Fig. 3 to test the robustness of the phase boundaries predicted by linear stability analysis. Time evolution of the system at two different points are depicted in (b). The upper point is below the Hopf bifurcation boundary and exhibits limit cycle oscillations as expected, while the lower point is well inside the unstable region, and a runaway $|\tilde{x}_c|$ establishes the predicted instability. The length scales in (b) and (c) range between 8.8–37 and 0–8.8 nm, respectively. Time scales for these figures range between 12.9–14.2 and 0–28.6 s, respectively. To see this figure in color, go online.

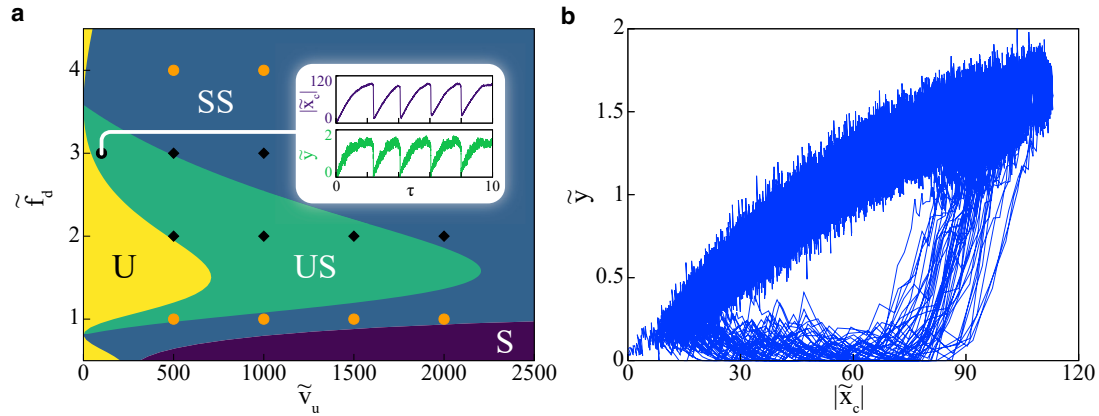


FIGURE 7 (a) Phase diagram portraying permanently bound state of clutches ($k_{\text{off}} = 0$) in the $\tilde{v}_u - \tilde{f}_d$ plane, for fixed $\tilde{\omega} = 5, \tilde{f}_s = 6.58815, N_m = 100, N_c = 10, \tilde{\kappa}_m = 2.191$, and $\tilde{\kappa}_c = 0.2296$. Following the previous convention, colored regions with labels indicate—S, stable; SS, stable spirals; US, unstable spirals; and U, unstable dynamical phases. Stochastic simulations were run at the points, confirming two phases characterizing decaying oscillations (●) and limit cycle oscillations (◆). In physical units, v_u and f_d range between 0 and $2.75 \mu\text{m/s}$ and 0 and 3.75 pN , respectively. (Inset) Time evolution At $\tilde{v}_u = 100, \tilde{f}_d = 3$, the system produces a stable limit cycle and the analogous stochastic time evolution of clutch displacement $|\tilde{x}_c|$ and mean MP extension \tilde{y} are presented in the panel. In physical units, $|\tilde{x}_c|$ and \tilde{y} range between 0–660 and 0–11 nm, respectively. (b) Limit cycle: a parametric plot of the $|\tilde{x}_c(\tau)|$ and $\tilde{y}(\tau)$ showing stable limit cycle oscillations. The length scales here are same as in the inset figures. To see this figure in color, go online.

clutches while ignoring the substrate elasticity. While applicable over a broad experimentally relevant parameter space, our model reproduces stick-slip type behavior at lower active velocities and successfully demonstrates self-sustaining oscillations known to occur within FAs (15,31). Stochastic simulations of the system validate the existence of dynamical phases predicted by our model.

The coupled ordinary differential equations capture a coarse-grained picture of the biomechanical processes at play and act as a modular mechanism of traction force generation that can be joined together to devise complex actomyosin networks which partake in durotaxis. Force fluctuations within FAs and concurrent oscillations in stress fibers (molecular motors) have been observed in experi-

mental setups. Earlier theoretical models predicted the spontaneous directed motions of MPs (57) and subsequently a stick-slip type dynamics with the motor-clutch paradigm (21,23). These models either assumed that the forces exerted by the stress fibers on FAs are constant (19,21) or did not take the roles of myosin contractility and attachment-detachment dynamics into account (22). Our model produces a rich array of dynamical phases for a wide range of biologically relevant parameters, not directly accessible from these earlier models.

Furthermore, an *in vitro* experimental setup by Plaças et al. (58) of a minimal actomyosin system was shown to give rise to spontaneous oscillations under elastic loading. In this setup, a single actin filament was attached to a

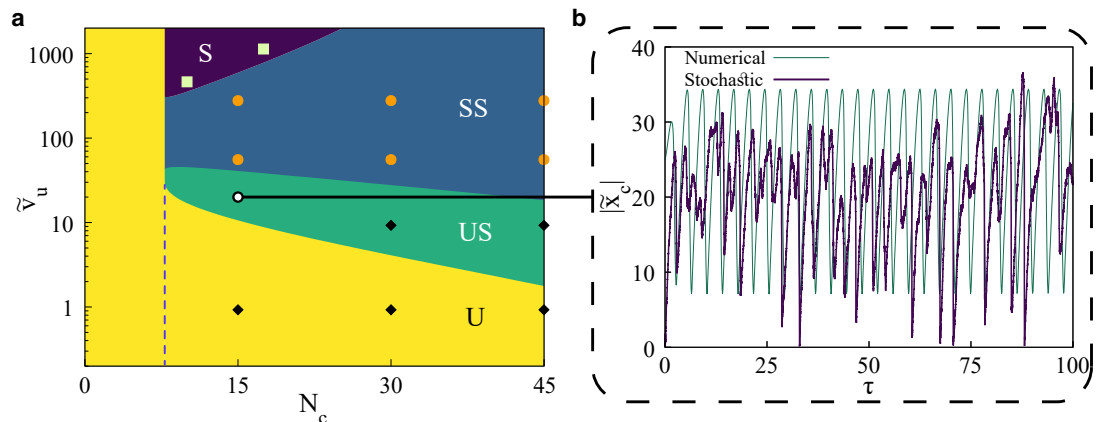


FIGURE 8 (a) Phase diagram depicting dynamical phases in the $N_c - \tilde{v}_u$ plane for fixed $\tilde{\kappa}_m = 2.191, \tilde{\omega} = 1, \tilde{f}_s = 6.58815, N_m = 100$, and $\tilde{\kappa}_c = 0.2296$. Convention wise, colored regions with labels indicate—S, stable; SS, stable spirals; US, unstable spirals; and U, unstable dynamical phases. A dashed line is used to separate the two unstable regions discussed previously. Stochastic simulations at the indicated points confirmed the existence of stable phase (●), decaying oscillations (●), and limit cycle oscillations (◆). (b) Comparison of limit cycle oscillations in the clutch deformation from numerical solution of the differential equations and the stochastic simulations. In physical units, x_c ranges from 0 to 220 nm. To see this figure in color, go online.

micron-sized bead optically trapped while its other end interacts with myosin motors attached to a glass substrate. The system shows spontaneous oscillations for a set of parameters, such as the density of motors and the stiffness of the optical trap. This experiment directly corresponds to the special case of the permanently bound clutch that we have discussed in Fig. 7, the n_c bound clutches giving rise to an effective elastic loading as discussed in the experiment.

Our choice to focus on the role of myosin stems from experimental evidence of its role in the specific context of force fluctuations in individual FAs and in regulating migration and mechanosensing (31,40,59). Our attempt to recognize the key components that considerably influence the force fluctuations in FAs has resulted in a significant model simplification over that of Wu et al. (31) without sacrificing experimentally accessible parameters and results. The explicit role of myosin II in traction peak oscillations, emerges as a natural consequence of the interaction between the motor and clutch sectors of the cellular migration machinery. In Fig. 9 a, we have plotted the frequencies and amplitude of limit cycle oscillations for a small number of clutches at intermediate MP velocity in physical units for the parameter values chosen in our study. With myosin II motor velocity varying in the range of 0.5–2 $\mu\text{m/s}$, the oscillations in the average MP and clutch deformations vary in the range of 1 – 10 Hz, which is an order of magnitude higher than the typical oscillation frequencies in individual FAs observed experimentally. However, the myosin detachment rates (ω_d) that we considered in our study serve as an upper bound. The mechanochemical cycle in myosin II motors broadly consists of ATP hydrolysis followed by actin-binding, subsequent ADP release, and finally myosin detachment. Reduction in the ADP release rate or lower

ATP concentrations significantly affects the bare detachment rate of myosin (60). In Fig. 9 b we look at the change in the oscillation frequency for varying dissociation rates and for different values of the active velocity (all expressed in real units). We observe that the frequency for all values of the active velocity increases with increasing dissociation rate. There is a large range of dissociation rates and active velocities for which the frequency is in the range 0 – 1 Hz, consistent with experimental and microscopic modeling results (31). In Fig. 9 c, we provide an example of an oscillation in the clutch extension at experimentally observed values.

It is worthwhile to discuss the effect of introducing modifications in our model based on experimental observations. Both myosin and multiple components of the adhesion clutch (e.g., integrins, talin, and vinculin) have been shown to display catch-bond behavior, i.e., an increase in bond lifetime with increasing load for a specific range of force (61,62). For example, force applied to integrins has been shown to increase bond lifetimes by nearly an order of magnitude. Recent experiments have also suggested a direction-dependent catch-bond behavior in the binding of vinculin (63), which is a component of both cadherin and integrin-based adhesion complexes, to actin filaments. Myosin II isoforms have also shown catch-bond behavior, with the detachment rates of myosin varying accordingly (45,64). These results emphasize the need to incorporate catch bond in the detachment rates of both motor and clutch. Although we do not expect the mechanosensitivity of force generation to be affected by the catch-bond kinetics, we do expect the oscillation frequencies to be sensitive to such behavior. The presence of an external force or a substrate could change the timescales of attachment/detachment of motor and clutch proteins.

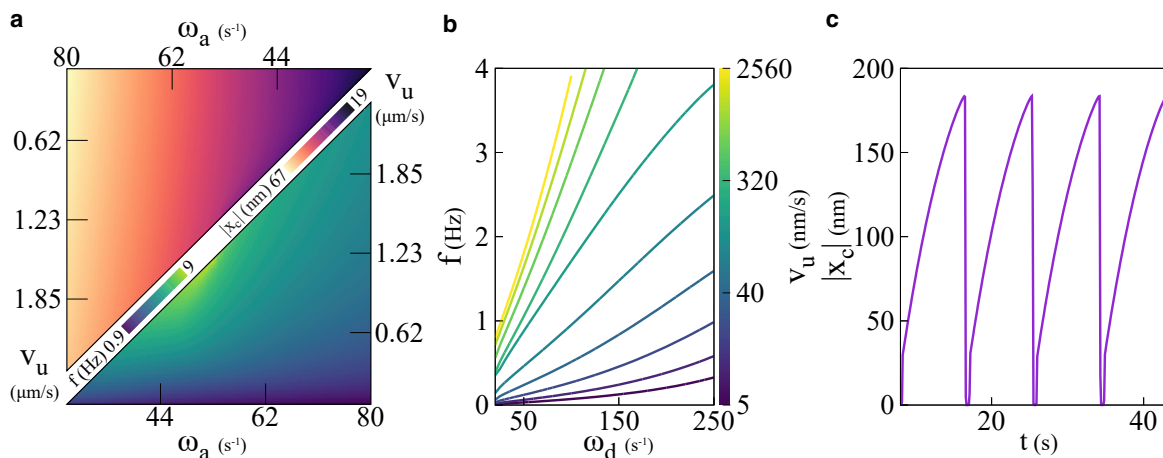


FIGURE 9 Density plots characterizing limit cycle oscillations: with $N_c = 10$, the upper and lower triangles in (a) delineate the amplitudes and frequencies f of stable limit cycle oscillations in clutch extension x_c , respectively. The areas of these triangles are demarcated by the Hopf bifurcation boundary at their hypotenuse. Dependence on motor detachment rate: with $N_m = 65$ and varying bare detachment rates, frequencies increase with rising v_u within a range of 0–4 Hz, as seen in (b). The oscillations in clutch extension at $\omega_a = \omega_d$, and $v_u = 0.025\mu\text{m/s}$, displays a frequency below 0.2 Hz in (c), conforming previous studies. To see this figure in color, go online.

Substantially more critical is the effect of MP activity on the substrate deformation, both by varying myosin velocity and attachment/detachment dynamics. Most theoretical studies which focus on force transmission in clutch models where substrate rigidity is tuned, show a biphasic relationship between substrate rigidity and force. This is understood in terms of a loading rate, which is the speed at which forces in the clutches build when they are engaged and is directly controlled by the rigidity of the substrate (8). Experimental observations suggest that force transmission is maximized for a specific value of rigidity or loading rate. Inhibiting myosin would lead to a decrease in the loading rate and therefore would require a higher rigidity of the substrate to reach the optimal value. Thus, although myosin inhibition leads to a reduction in myosin contractility, force transmission is enhanced for a range of rigidity. This counterintuitive result has been shown experimentally (16) using myosin inhibitor blebbistatin. Our model allows us to tune the myosin activity specifically via the myosin detachment rate and velocity, therefore providing a direct route to verify this counterintuitive result and predict an experimentally tunable parameter range to probe the mechanosensitivity of the molecular clutch.

SUPPORTING MATERIAL

Supporting material can be found online at <https://doi.org/10.1016/j.bpj.2022.03.025>.

AUTHOR CONTRIBUTIONS

A.C. designed the research. D.G. and S.G. performed the research and analyzed the data. D.G. performed all numerical studies. D.G., S.G., and A.C. wrote and edited the manuscript.

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REFERENCES

- Petrie, R. J., A. D. Doyle, and K. M. Yamada. 2009. Random versus directionally persistent cell migration. *Nat. Rev. Mol. Cell Biol.* 10:538–549.
- De Rooij, J., A. Kerstens, ..., C. M. Waterman-Storer. 2005. Integrin-dependent actomyosin contraction regulates epithelial cell scattering. *J. Cell Biol.* 171:153–164.
- Paszek, M. J., N. Zahir, ..., V. M. Weaver. 2005. Tensional homeostasis and the malignant phenotype. *Cancer Cell.* 8:241–254. <http://www.sciencedirect.com/science/article/pii/S1535610805002680>.
- Yamaguchi, H., J. Wyckoff, and J. Condeelis. 2005. Cell migration in tumors. *Curr. Opin. Cell Biol.* 17:559–564. <http://www.sciencedirect.com/science/article/pii/S0955067405001055>, cell-to-cell contact and extracellular matrix.
- Schwarz, U. S., and S. A. Safran. 2013. Physics of adherent cells. *Rev. Mod. Phys.* 85:1327.
- Paluch, E. K., I. M. Aspalter, and M. Sixt. 2016. Focal adhesion-independent cell migration. *Annu. Rev. Cell Dev. Biol.* 32:469–490.
- Case, L. B., and C. M. Waterman. 2015. Integration of actin dynamics and cell adhesion by a three-dimensional, mechanosensitive molecular clutch. *Nat. Cell Biol.* 17:955–963.
- Elosegui-Artola, A., X. Trepast, and P. Roca-Cusachs. 2018. Control of mechanotransduction by molecular clutch dynamics. *Trends Cell Biol.* 28:356–367.
- Plotnikov, S. V., and C. M. Waterman. 2013. Guiding cell migration by tugging. *Curr. Opin. Cell Biol.* 25:619–626.
- Blanchoin, L., R. Boujemaa-Paterski, ..., J. Plastino. 2014. Actin dynamics, architecture, and mechanics in cell motility. *Physiol. Rev.* 94:235–263.
- Charras, G., and E. Sahaï. 2014. Physical influences of the extracellular environment on cell migration. *Nat. Rev. Mol. Cell Biol.* 15:813–824. <https://doi.org/10.1038/nrm3897>.
- Kurzawa, L., B. Vianay, ..., M. Théry. 2017. Dissipation of contractile forces: the missing piece in cell mechanics. *Mol. Biol. Cell.* 28:1825–1832.
- Meili, R., B. Alonso-Latorre, ..., J. C. Lasheras. 2010. Myosin II is essential for the spatiotemporal organization of traction forces during cell motility. *Mol. Biol. Cell.* 21:405–417.
- Rape, A. D., W.-h. Guo, and Y.-l. Wang. 2011. The regulation of traction force in relation to cell shape and focal adhesions. *Biomaterials.* 32:2043.
- Plotnikov, S. V., A. M. Pasapera, ..., C. M. Waterman. 2012. Force fluctuations within focal adhesions mediate ECM-rigidity sensing to guide directed cell migration. *Cell.* 151:1513–1527.
- Elosegui-Artola, A., R. Oria, ..., P. Roca-Cusachs. 2016. Mechanical regulation of a molecular clutch defines force transmission and transduction in response to matrix rigidity. *Nat. Cell Biol.* 18:540–548.
- DiMilla, P., K. Barbee, and D. Lauffenburger. 1991. Mathematical model for the effects of adhesion and mechanics on cell migration speed. *Biophysical J.* 60:15–37.
- Macdonald, A., A. R. Horwitz, and D. A. Lauffenburger. 2008. Kinetic model for lamellipodal actin-integrin-clutch dynamics. *Cell Adhes. Migrat.* 2:95–105.
- Sabass, B., and U. S. Schwarz. 2010. Modeling cytoskeletal flow over adhesion sites: competition between stochastic bond dynamics and intracellular relaxation. *J. Phys. Condens. Matter.* 22:194112.
- Schwarz, U. S., and M. L. Gardel. 2012. United we stand—integrating the actin cytoskeleton and cell–matrix adhesions in cellular mechanotransduction. *J. Cell Sci.* 125:3051–3060.
- Chan, C. E., and D. J. Odde. 2008. Traction dynamics of filopodia on compliant substrates. *Science.* 322:1687–1691.
- Bangasser, B. L., S. S. Rosenfeld, and D. J. Odde. 2013. Determinants of maximal force transmission in a motor-clutch model of cell traction in a compliant microenvironment. *Biophysical J.* 105:581–592.
- Bangasser, B. L., and D. J. Odde. 2013. Master equation-based analysis of a motor-clutch model for cell traction force. *Cell Mol. Bioeng.* 6:449–459.
- Danuser, G., J. Allard, and A. Mogilner. 2013. Mathematical modeling of eukaryotic cell migration: insights beyond experiments. *Annu. Rev. Cell Dev. Biol.* 29:501–528.
- Sens, P. 2013. Rigidity sensing by stochastic sliding friction. *Europhys. Lett.* 104:38003.
- Bangasser, B. L., G. A. Shamsan, ..., D. J. Odde. 2017. Shifting the optimal stiffness for cell migration. *Nat. Commun.* 8:1–10.
- Craig, E. M., J. Stricker, ..., A. Mogilner. 2015. Model for adhesion clutch explains biphasic relationship between actin flow and traction at the cell leading edge. *Phys. Biol.* 12:035002.

28. Leoni, M., and P. Sens. 2017. Model of cell crawling controlled by mechanosensitive adhesion. *Phys. Rev. Lett.* 118:228101.
29. Bressloff, P. C. 2020. Stochastic resetting and the mean-field dynamics of focal adhesions. *Phys. Rev. E.* 102:022134.
30. Zaman, M. H., R. D. Kamm, ..., D. A. Lauffenburger. 2005. Computational model for cell migration in three-dimensional matrices. *Biophysical J.* 89:1389–1397.
31. Wu, Z., S. V. Plotnikov, A. Y. Moalim, ..., J. Liu. 2017. Two distinct actin networks mediate traction oscillations to confer focal adhesion mechanosensing. *Biophysical J.* 112:780–794. <http://www.sciencedirect.com/science/article/pii/S0006349516343417>.
32. Gardel, M. L., I. C. Schneider, ..., C. M. Waterman. 2010. Mechanical integration of actin and adhesion dynamics in cell migration. *Annu. Rev. Cell Dev. Biol.* 26:315–333.
33. Grill, S. W., K. Kruse, and F. Jülicher. 2005. Theory of mitotic spindle oscillations. *Phys. Rev. Lett.* 94:108104.
34. Escribano, J., M. Sánchez, and J. García-Aznar. 2014. A discrete approach for modeling cell–matrix adhesions. *Comput. Part. Mech.* 1:117–130.
35. Labouesse, C., A. B. Verkhovsky, ..., B. Vianay. 2015. Cell shape dynamics reveal balance of elasticity and contractility in peripheral arcs. *Biophysical J.* 108:2437–2447.
36. Thomas, D. G., A. Yenepalli, ..., T. T. Egelhoff. 2015. Non-muscle myosin IIB is critical for nuclear translocation during 3D invasion. *J. Cell Biol.* 210:583–594.
37. Barnhart, E., K.-C. Lee, ..., A. Mogilner. 2015. Balance between cell-substrate adhesion and myosin contraction determines the frequency of motility initiation in fish keratocytes. *Proc. Natl. Acad. Sci. U S A.* 112:5045–5050.
38. Barnhart, E. L., J. Allard, ..., A. Mogilner. 2017. Adhesion-dependent wave generation in crawling cells. *Curr. Biol.* 27:27–38.
39. Kobb, A. B., T. Zulueta-Coarasa, and R. Fernandez-Gonzalez. 2017. Tension regulates myosin dynamics during *Drosophila* embryonic wound repair. *J. Cell Sci.* 130:689–696.
40. Greenberg, M. J., G. Arpağ, ..., E. M. Ostap. 2016. A perspective on the role of myosins as mechanosensors. *Biophysical J.* 110:2568–2576.
41. Jung, W.-H., K. Elawad, ..., Y. Chen. 2019. Cell–cell adhesion and myosin activity regulate cortical actin assembly in mammary gland epithelium on concaved surface. *Cells.* 8:813.
42. Recho, P., T. Putelat, and L. Truskinovsky. 2013. Contraction-driven cell motility. *Phys. Rev. Lett.* 111:108102.
43. Wilson, C. A., M. A. Tsuchida, ..., J. A. Theriot. 2010. Myosin II contributes to cell-scale actin network treadmill through network disassembly. *Nature.* 465:373–377.
44. Lavi, I., M. Piel, ..., N. S. Gov. 2016. Deterministic patterns in cell motility. *Nat. Phys.* 12:1146–1152.
45. Stam, S., J. Alberts, ..., E. Munro. 2015. Isoforms confer characteristic force generation and mechanosensation by myosin II filaments. *Biophysical J.* 108:1997–2006.
46. Koenderink, G. H., and E. K. Paluch. 2018. Architecture shapes contractility in actomyosin networks. *Curr. Opin. Cell Biol.* 50:79–85.
47. Walcott, S., D. M. Warshaw, and E. P. Debold. 2012. Mechanical coupling between myosin molecules causes differences between ensemble and single-molecule measurements. *Biophysical J.* 103:501–510.
48. Schnitzer, M. J., K. Visscher, and S. M. Block. 2000. Force production by single kinesin motors. *Nat. Cell Biol.* 2:718–723.
49. Dembo, M., D. Torney, ..., D. Hammer. 1988. The reaction-limited kinetics of membrane-to-surface adhesion and detachment. *Proc. R. Soc. Lond. Ser. B. Biol. Sci.* 234:55–83.
50. Lansky, Z., M. Braun, ..., S. Diez. 2015. Diffusible crosslinkers generate directed forces in microtubule networks. *Cell.* 160:1159–1168. <https://www.sciencedirect.com/science/article/pii/S0092867415001294>.
51. Veigel, C., J. E. Molloy, ..., J. Kendrick-Jones. 2003. Load-dependent kinetics of force production by smooth muscle myosin measured with optical tweezers. *Nat. Biol.* 5:980–986.
52. Wolfram Research, Inc. Mathematica, version 12.3.1. <https://www.wolfram.com/mathematica>. Champaign, IL, 2021.
53. Hindmarsh, A., and A. Taylor. 1999. User Documentation for IDA: A Differential-Algebraic Equation Solver for Sequential and Parallel Computers. Lawrence Livermore National Laboratory report, UCRL-MA-136910.
54. Harris, D., and D. Warshaw. 1993. Smooth and skeletal muscle myosin both exhibit low duty cycles at zero load in vitro. *J. Biol. Chem.* 268:14764–14768. <https://www.sciencedirect.com/science/article/pii/S0021925818823985>.
55. Debold, E. P., J. B. Patlak, and D. M. Warshaw. 2005. Slip sliding away: load-dependence of velocity generated by skeletal muscle myosin molecules in the laser trap. *Biophysical J.* 89:L34–L36. <https://www.sciencedirect.com/science/article/pii/S0006349505729301>.
56. Debold, E. P., M. A. Turner, ..., S. Walcott. 2011. Phosphate enhances myosin-powered actin filament velocity under acidic conditions in a motility assay. *Am. J. Physiology-Regulatory, Integr. Comp. Physiol.* 300:R1401–R1408. <https://doi.org/10.1152/ajpregu.00772.2010>.
57. Jülicher, F., and J. Prost. 1995. Cooperative molecular motors. *Phys. Rev. Lett.* 75:2618.
58. Plaçaïs, P.-Y., M. Balland, ..., P. Martin. 2009. Spontaneous oscillations of a minimal actomyosin system under elastic loading. *Phys. Rev. Lett.* 103:158102.
59. Pasapera, A. M., S. V. Plotnikov, ..., C. M. Waterman. 2015. Rac1-dependent phosphorylation and focal adhesion recruitment of myosin IIA regulates migration and mechanosensing. *Curr. Biol.* 25:175–186.
60. Wang, F., M. Kovács, ..., J. R. Sellers. 2003. Kinetic mechanism of non-muscle myosin IIB: functional adaptations for tension generation and maintenance. *J. Biol. Chem.* 278:27439–27448.
61. Sokurenko, E. V., V. Vogel, and W. E. Thomas. 2008. Catch-bond mechanism of force-enhanced adhesion: counterintuitive, elusive, but... widespread? *Cell Host Microbe.* 4:314–323.
62. Thomas, W. E., V. Vogel, and E. Sokurenko. 2008. Biophysics of catch bonds. *Annu. Rev. Biophys.* 37:399–416.
63. Rothenberg, K. E., D. W. Scott, ..., B. D. Hoffman. 2018. Vinculin force-sensitive dynamics at focal adhesions enable effective directed cell migration. *Biophysical J.* 114:1680–1694.
64. O’Connell, C. B., M. J. Tyska, and M. S. Mooseker. 2007. Myosin at work: motor adaptations for a variety of cellular functions. *Biochim. Biophys. Acta.* 1773:615–630.