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## Antibodies with weakly basic isoelectric points minimize trade-offs between formulation and physiological colloidal properties

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### Abstract

The widespread interest in antibody therapeutics has led to much focus on identifying antibody candidates with favorable developability properties. In particular, there is broad interest in identifying antibody candidates with highly repulsive self-interactions in standard formulation conditions (e.g., low ionic strength buffers at pH 5–6) for high solubility and low viscosity. Likewise, there is also broad interest in identifying antibody candidates with low levels of non-specific interactions in physiological conditions (PBS, pH 7.4) to promote favorable pharmacokinetic properties. To what extent antibodies can be systematically identified that possess both highly repulsive self-interactions in standard formulation conditions and weak non-specific interactions in physiological conditions remains unclear and is a potential impediment to successful therapeutic drug development. Here we evaluate these two properties for 42 IgG1 variants based on the variable fragments (Fvs) from four clinical-stage antibodies and complementarity-determining regions from ten clinical-stage antibodies. Interestingly, we find that antibodies with the strongest repulsive self-interactions in a standard formulation condition (pH 6 and 10 mM histidine) display the strongest non-specific interactions in physiological conditions. Conversely, antibodies with the weakest non-specific interactions in physiological conditions display the least repulsive self-interactions in standard formulations. This behavior can be largely explained by the antibody isoelectric point, as highly basic antibodies that are

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#### CONFLICTS OF INTEREST

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highly positively charged at standard formulation conditions (pH 5–6) promote repulsive self-interactions that mediate high antibody stability but also mediate strong non-specific interactions with negatively charged biomolecules at physiological pH, and vice versa for antibodies with negatively charged Fv regions. Therefore, IgG1s with weakly basic isoelectric points between 8–8.5, and Fv isoelectric points between 7.5–9, typically display the best combinations of strong repulsive self-interactions and weak non-specific interactions. We expect that these findings will improve the identification and engineering of antibody candidates with drug-like biophysical properties.

### Keywords

developability; specificity; non-specific; nonspecific; polyreactivity; off-target binding; colloidal stability; self-association; self-interactions; non-specific interactions; Fv net charge; Fv isoelectric point

## INTRODUCTION

Monoclonal antibodies (mAbs) are currently the dominant class of biotherapeutics used for the treatment of indications related to oncology, immune modulation, respiratory disorders, inflammation, and ophthalmology.<sup>1–5</sup> Currently there are over ninety approved antibody therapeutics<sup>6</sup> and their success is attributed to several of their key properties, including their high specificity and affinity, low non-mechanistic toxicity, long half-life and high stability compared to other biologics.<sup>7, 8</sup> Despite this success, attrition rates for mAbs before approval remains significantly high, which strongly contributes to the high cost of therapeutic antibody development. Early identification of antibodies with optimal drug-like properties is essential to reduce the likelihood of failures in the clinic.

Two antibody properties – namely antibody non-specific and self-interactions – are both of significant importance for successful antibody drug development.<sup>9, 10</sup> Antibody non-specific interactions in physiological conditions lead to off-target binding, non-specific cellular uptake, intracellular degradation and/or abnormal interactions with FcRn, which increase the risk for fast antibody clearance and poor efficacy *in vivo*.<sup>11–17</sup> Antibody self-association in standard formulation conditions (low ionic strength formulations at pH 5–6) can lead to poor solubility, opalescence and high viscosity in concentrated antibody formulations, which increases the risk for poorly stable and viscous antibody formulations that are unsuitable for subcutaneous delivery.<sup>10, 18–27</sup>

While it is desirable to identify antibodies with both low non-specific interactions and low self-association, a holistic analysis of previous studies of each individual property suggests that this may be particularly challenging. For example, strongly positively-charged antibodies with high isoelectric points have been shown to display low risk for high self-association, viscosity and opalescence in standard formulation conditions.<sup>20, 28–30</sup> However, the same type of strongly positively-charged antibodies have also been shown to display high risk for non-specific interactions in physiological conditions (pH 7.4, PBS) and fast antibody clearance *in vivo*.<sup>14, 31–40</sup> Likewise, strongly negatively charged antibodies with low isoelectric points have been shown to display high risk for high self-association,

viscosity and opalescence in standard formulation conditions, while the same antibodies display low-to-medium risk for non-specific interactions in physiological conditions and fast antibody clearance *in vivo*.<sup>22, 25–27, 39, 41–43</sup>

Despite these important previous studies, there has been little systematic evaluation of these trade-offs and much remains unknown about how to identify antibodies with optimal combinations of both properties. Here we have sought to directly evaluate trade-offs between antibody non-specific binding (pH 7.4, PBS) and self-association (pH 6, 10 mM histidine) for a panel of antibodies with systematic variation in physicochemical properties of their frameworks and main binding loops (heavy chain CDR3) using the Fv frameworks from four clinical-stage antibodies and the heavy chain CDR3s from ten clinical-stage antibodies (Fig. 1). In particular, we have evaluated the contributions of antibody charge, hydrophobicity, and other physicochemical properties to antibody self-association and non-specific binding. Herein, we report surprisingly strong trade-offs between antibody non-specific binding and self-association, and optimal ranges of antibody physicochemical properties for identifying favorable antibodies with low levels of both non-specific binding and self-association.

## METHODS AND MATERIALS

### Cloning of antibody variants

The heavy ( $V_H$ ) chain variable genes with grafted heavy CDR3 (HCDR3) sequences and the parent antibody heavy and light ( $V_K$ ) chain genes along with the leader sequence were synthesized as gene blocks (IDT technologies). Both  $V_H$  and  $V_K$  gene blocks were cloned using HindIII and EcoRI restriction sites seamlessly with InFusion enzyme mix into pTT5 vectors carrying the IgG1 and kappa constant genes respectively. Sequence confirmed vector constructs of the variant antibodies were scaled up to prepare endotoxin free plasmid DNA for expression in CHO-3E7 (CHO-E) mammalian cell line (L-11992, National Research Council Canada). All the variable genes were designed with codons for optimal mammalian expression.

### Expression and purification of antibody variants

The recombinant antibodies were transiently expressed using optimized methods reported previously.<sup>67</sup> Briefly, CHO-E cells maintained in Glutamax supplemented FreeStyle CHO media at 37 °C, 5% CO<sub>2</sub>, and 150 rpm shake speed were used for transient transfection. Prior to transfection the cells were seeded at a cell density of 2 million cells per mL in 400 mL of BalanCD Transfectory CHO media supplemented with 4 mM L-glutamine. The heavy chain (0.075 mg) and light chain (0.15 mg) plasmids were mixed at 1:2 ratio along with 70% filler DNA (0.525 mg) making it a total of 0.75 mg of DNA into 50 mL of OptiPro media and sterilized by vacuum filtration. Half the volume (0.375 mL) of TransIT-PRO transfection reagent was added to the DNA-OptiPro transfection solution and gently swirled to mix. The DNA-TransIT-Pro complex media was added immediately to the flask containing the cells with gentle swirl. The shake flasks were transferred to orbital shaker at 140 rpm at 37 °C and 5% CO<sub>2</sub>. Four hours post transfection, 50 mL Transfectory Supplement (12.5% culture volume) and 1.0 mL Anti-Clumping agent (Gibco) were added, and the temperature shifted

to 30 °C. Between days 5 to 7 post-transfection, 50 ml of CHO Feed B media was added to the transfected cells to maintain the glucose titer >2 gm/L. The transfected cultures were maintained for 8–9 d and harvested by centrifuging at 4700 rpm, 4 °C for 40 min, followed by sterile filtration through a 0.2 µm filter.

The harvested supernatants were subjected to parallel Protein A affinity chromatography using the Protein Maker system (Protein BioSolutions). Sample and buffer lines were cleaned with 0.5 M NaOH to remove any contaminants and equilibrated in DPBS (8.05 mM sodium phosphate, 137 mM NaCl, 1.47 mM potassium phosphate, 2.6 mM potassium chloride, pH 7.2). The column was equilibrated with ten column volumes of DPBS at a speed of 5 mL/min. The supernatant with recombinant antibody was loaded on to a 5 mL HiTrap MabSelect SuRe™ column (GE Healthcare) at a flow rate of 0.5 mL/min overnight and then washed with ten column volumes of DPBS. The column was then subjected to high salt wash using 1 M NaCl followed by another DPBS wash both with ten column volumes at a flow rate of 5 mL/min. Before eluting the antibody, the column was subjected to pre-elution with 3 mL of 30 mM sodium acetate pH 3.5. The bound antibody was then eluted off the column with 5 mL of 30 mM sodium acetate pH 3.5 at a flow rate of 1 mL/min and immediately neutralized with 1% by volume using 3 M sodium acetate pH 9.0 to bring the final formulation to 60 mM sodium acetate pH 5.0. The elution and neutralization steps were repeated two more times to ensure all the bound antibody was eluted off the column. The concentration in the elution fractions were measured by UV280 in a 96 well plate using a DropSense instrument prior to pooling. Pooled neutralized eluted antibody was sterile filtered into a 50 mL Falcon tube by 0.22 µm Millipore Steriflip using vacuum filtration system. The final concentrations were then similarly measured on the DropSense instrument by applying the specific extinction coefficient of each antibody.

As a polishing step, preparative size-exclusion chromatography was also performed (when necessary) to remove large amounts of aggregates to have monomer percentages greater than 95%. Briefly, HiLoad 26/600 Superdex200 preparative grade column was equilibrated with 600 mL of 60 mM sodium acetate pH 5.0 buffer by AKTA system. The Protein A purified antibody sample was loaded onto the column at a flow rate of 1.5 mL/min. Fractions (3 mL) were collected by the fraction collector after approximately one column volume or when the UV280 absorbance reached above the baseline. The fractions containing monomers determined by analytical size exclusion chromatography were pooled and sterile filtered into a 50 mL Falcon tube by 0.22 µm Millipore Steriflip using vacuum filtration system. The concentrations were measured similarly as mentioned before.

### **Analytical size exclusion chromatography**

Purity was evaluated by analytical size exclusion chromatography using a 7.8 × 300 mm TSKgel G3000SWXL HPLC column (GE Healthcare) equilibrated with PBS containing 0.2 mol/L L-arginine (pH 6.8) with a flow rate of 0.5 mL/min PBS containing 0.2 mol/L L-arginine (pH 6.8) using an ACQUITY ultraperformance LC system (Waters, Milford, MA). The monomer and aggregate chromatogram peaks were identified and processed in reference to a molecular weight standard, and % monomer, % low and high molecular

weight species (%LMWS and %HMWS) were determined by calculating the area under the curve of the chromatograms using Empower software (Waters, Milford, MA; Table S1).

#### **Non-specific binding measurements: ELISA #1**

The non-specific binding measurements were performed using an ELISA method reported previously<sup>9, 45</sup> with some modifications. Immulon 2HB plates (3655TS, Thermo Fisher Scientific) were coated separately with six non-antigen reagents (Cardiolipin (50 µg/mL), keyhole limpet hemocyanin (5 µg/mL), lipopolysacchride (10 µg/mL), single and double stranded DNA (1 µg/mL) and insulin at 200 µg/mL) for 1 h at 37 °C. The plates were washed three times with 200 µL/well of PBS containing 0.05% Tween 20 (PBST) using a Biotek plate washer and were not blocked. Then 50 µL of each antibody of interest prepared at 1 µM in PBST was incubated in the wells for 1 h. The plates were washed three times with 200 µL/well of PBST before incubating with 50 µL of the secondary antibody at 10 ng/mL (HRP conjugated goat anti-human IgG antibody, 109-035-008, Jackson Immuno Research) for 1 h. The plates were developed with 50 µL of TMB substrate (TMBS-1000-01, Surmodics) after removal of any unbound secondary antibody with six washes in PBST. Color development was quenched with 50 µL of 2 M sulfuric acid after 5 min. Absorbance values were measured at 450 nm using a Biotek Synergy 2 plate reader. The signals obtained were normalized to adalimumab and bococizumab IgGs in each experiment as negative and positive controls, respectively. Normalized values were calculated as the absorbance for a given mAb minus the absorbance for adalimumab divided by the difference in absorbance for bococizumab and adalimumab.

#### **Non-specific binding measurements: ELISA #2**

The ELISA with baculovirus particles was performed similarly to previously reported method.<sup>38</sup> Briefly, the BVP stock (LakePharma) was first evaluated with reference antibodies to determine the optimal dilution to obtain best signal to noise readouts. Diluted BVP stock (1:100) in sodium carbonate buffer (pH 9.6) was determined to be the optimal dilution. Diluted BVP (50 µL per well) was incubated in Immulon 2HB plates at 4 °C overnight. Unbound particles were aspirated from the wells using Biotek plate washer. The plates were blocked with 200 µL of blocking buffer (PBS with 0.5% BSA) and incubated for 1 h before washing three times with 200 µL of PBS. 50 µL of each antibody, prepared at 1 µM in blocking buffer, was added to the wells and incubated for 1 h followed by six washes with 200 µL of PBS. Next, 50 µL of diluted secondary antibody at 10 ng/mL was added to the wells and incubated for 1 h followed by another six washes. Finally, 50 µL of TMB substrate was added to each well and incubated for 5 min. The reaction was quenched by adding 50 µL of 2 M sulfuric acid to each well. Absorbance values were measured at 450 nm using a Biotek Synergy 2 plate reader. Normalized values were calculated using the same method described for ELISA #1

#### **Non-specific binding measurements: PolySpecificity (PSP) assay**

The assay, including the preparation of soluble membrane protein and ovalbumin reagents, were performed as described in our previous work.<sup>46</sup> Briefly, non-specific binding measurements with soluble membrane proteins (PSP #1) and ovalbumin (PSP #2) were incubated with overnight antibody (15 µg/mL) coated Protein A magnetic beads (10002D,

Invitrogen). The reagent and bead complexes were incubated at 4 °C for 20 min for soluble membrane proteins, while ovalbumin was incubated 3 h at room temperature. The beads were then washed once and incubated with 0.001x streptavidin-AF647 (S32357, Invitrogen) and 0.001x goat anti-human Fc F(ab')<sub>2</sub> AF-488 (H10120, Invitrogen) on ice for 4 min. As a final step, the beads were washed once more and resuspended in PBSB. The samples were analyzed for non-specific binding via flow cytometry to measure their median fluorescent intensities (MFI). Adalimumab and bococizumab (generated using the antibody variable regions from the clinical-stage antibodies on a common IgG1 framework) were analyzed in each experiment as negative (adalimumab) and positive (bococizumab) controls. Polyspecificity scores were calculated as the MFI for a given mAb minus the MFI for adalimumab divided by the difference in MFI values for bococizumab and adalimumab.

### Diffusion interaction parameter ( $k_D$ ) measurements

The antibody samples in acetate buffer were dialyzed into 10 mM histidine HCl (pH 6.0) buffer using 10 kD Slide-A-Lyzer dialysis cassettes (ThermoFisher Scientific) and concentrated to achieve greater than 12 mg/mL mAb. The concentrated sample variants were filtered using 0.2 micron filters before preparing them at six concentrations (10, 9, 7, 5, 2.5 and 1.25 mg/mL), transferred to 384-well plates (Greiner Bio-One) in duplicates, sealed with a film and centrifuged at 1200 rpm for 5 min. The apparent diffusion interaction parameters ( $k_D$ ) were calculated from diffusion coefficients, as a function of antibody concentration, measured using the Wyatt DynaPro Plate Reader II dynamic light scattering instrument. The instrument was set up to measure diffusion coefficients 10 times and each measurement was performed for 5 s. The autocorrelation function was fit using the method of cumulants (Dynamics software, version 7.1) to measure mean diffusion coefficient values. The goodness of the fit was inspected, and any data points with a sum of squares (SOS) values greater than one were removed. The mean diffusion coefficients from triplicate experiments were plotted as a function of antibody concentration to obtain the diffusion interaction parameter values.

### Homology Modeling

The fragment variable region (Fv) sequences were used to build homology models in an automated fashion using the Antibody Modeler feature in Molecular Operating Environment (MOE) Inc., 2019 by Chemical Computing group. The force field was set to Amber10: EHT with the internal and external dielectric values of 4 and 80, respectively. The non-bonded cutoff distances were set to 10 and 12 Å, and the Born solvation was used. Once the homology models were built, the C-termini of the heavy and light variable chains were capped by amidating to neutralize charges. The capped models were prepared for energy minimizations by using the structure preparation feature to remove any errors and protonate the models at pH 6.0 with 0.0001 M ionic strength or pH 7.4 with 0.15 M ionic strength. The prepared structures were subjected to energy minimization to root mean square gradient (RMSG) below 0.00001 kcal/mol/Å<sup>2</sup>.

### Sequence and structure based molecular property calculations

The heavy and light chain sequences were used to calculate net charge of all 6 CDRs, V<sub>L</sub>, V<sub>H</sub> and Fv at pH 6 and pH 7.4 and also isoelectric points of Fv and IgG. The homology

models of Fv were used to calculate stability, charge and hydrophobic properties for the CDRs and Fv regions at both pH 6 and pH 7.4 using the property calculation feature in MOE 2019.

## RESULTS

### Design and production of clinical-stage antibody frameworks with HCDR3 sequence variation

Toward our goal of evaluating how CDR sequences impact antibody self-association and non-specific binding, we first chose four clinical-stage antibodies for analysis, namely lebrizumab, siltuximab, trastuzumab and humanized OKT3 (hOKT3).<sup>9, 44</sup> These four antibodies have variable regions with a range of physicochemical properties and germlines (Table 1 and Fig. S1). The fragment variable (Fv) regions of the antibodies differ significantly in terms of their charges (−1.9 to +9.2 at pH 7.4) and isoelectric points (pIs of 5.4 to 9.3; Table 1). To generate additional diversity in heavy chain CDR3 (HCDR3) for the four antibodies, we selected a set of ten naturally occurring HCDR3s, each of which is ten residues long and differs in its physicochemical properties (Table 2). The ten different HCDR3s were grafted onto the V<sub>H</sub> regions to generate a set of 42 IgG1 antibodies with diverse properties. This is less than the expected 44 antibodies because two of the HCDR3s (trastuzumab and hOKT3) were used for CDR grafting. Given that trastuzumab has an 11-residue HCDR3, the grafted trastuzumab variants have a tryptophan at the N-terminus of HCDR3 to keep the loop length constant (11 residues).

The antibodies were expressed as IgG1/kappa antibodies in mammalian cells and purified by Protein A. The quality of the purified variants was assessed by analytical size-exclusion chromatography (Table S1). Antibodies that were <90% monomer were further purified by size-exclusion chromatography. The purification yields were relatively high for the four scaffolds, including 29–124 mg/L for the lebrizumab variants, 82–203 mg/L for the siltuximab variants, 99–151 mg/L for the trastuzumab variants and 24–187 mg/mL for the hOKT3 variants.

### Antibody variants display trade-offs between specificity and colloidal stability

To evaluate potential trade-offs between different types of antibody colloidal interactions, we next evaluated non-specific binding at physiological conditions (pH 7.4, PBS) for the panel of antibody variants using two previously reported ELISAs and two forms a flow cytometry assay [PolySpecificity Particle (PSP) assay].<sup>9, 38, 45, 46</sup> First, we used an ELISA (referred to ELISA #1) for evaluating antibody non-specific interactions with six non-antigen reagents, namely cardiolipin, lipopolysaccharide (LPS), keyhole limpet hemocyanin (KLH), insulin, single and double stranded DNA (Fig. 2A). The parent antibodies (open circles in Fig. 2A) generally displayed relatively low levels of non-specific binding, although the higher pI parent antibodies (hOKT3 and trastuzumab) displayed modestly higher levels of non-specific binding relative to the lower pI antibodies (siltuximab and lebrizumab). Interestingly, the grafted CDR variants generally displayed higher to much higher levels of non-specific binding than the parent antibodies. For the high pI antibodies (hOKT3 and trastuzumab), the positively charged HCDR3s (triangles) generally displayed higher levels

of non-specific binding than those with negatively charged HCDR3s (circles). For the lower pI antibodies (siltuximab and lebrizumab), it is notable that the few antibody variants that display relatively high levels of non-specific interactions have positively charged HCDR3s.

We also evaluated non-specific binding for the antibody panel using a second ELISA (referred to as ELISA #2) with immobilized baculovirus particles that present a range of proteins, glycans and lipids (Fig. 2B). Overall, the results were generally similar between the two ELISAs. The high pI antibody variants (hOKT3 and trastuzumab) displayed the highest levels of non-specific binding, while the lower pI antibodies (siltuximab and lebrizumab) displayed the lowest levels of non-specific binding. Moreover, the effect of HCDR3 charge was less significant on the non-specific binding measurements by ELISA #2 than observed for ELISA #1 (Fig. 2A), although the trends were similar (Fig. 2A and 2B).

We next evaluated the antibody variants for their levels of non-specific interactions via a complementary flow cytometry-based assay, namely the PolySpecificity Particle (PSP) assay,<sup>46</sup> using two polyspecificity reagents (Fig. 2C–2D). These reagents included a complex mixture of soluble membrane proteins (SMP) isolated from CHO cells (Fig. 2C) and ovalbumin (OVA, Fig. 2D). Overall, the PSP assays revealed that OKT3 has the highest levels of non-specific binding, while most of the other antibody variants display low levels of non-specific binding. However, the siltuximab variants unexpectedly display a wide range of levels of non-specific binding to soluble membrane proteins, including levels that were similar to or higher than those for OKT3 (Fig. 2C).

Given the strong impact of Fv charge and HCDR3 sequence on antibody non-specific binding in physiological conditions (pH 7.4, PBS), we also evaluated the impact of these properties on antibody self-association in a standard formulation condition (pH 6.0, 10 mM histidine; Figs. 3 and S2). This formulation condition was chosen because it is a consensus pH and buffer system for mAb therapeutics,<sup>10</sup> and pH 6 is within the most common range of pHs (e.g., pH 5.5–6.2) of most approved antibody therapeutics since 2015.<sup>47</sup> We evaluated antibody self-association by measuring the diffusion interaction parameter ( $k_D$ ), which is the slope of the mutual diffusion coefficient as a function of protein concentration. Values of  $k_D > -8.2$  to  $-8.9$  mL/g generally are linked to repulsive antibody self-interactions, while smaller (more negative) values are generally to attractive self-interactions.<sup>21, 48</sup> Interestingly, all antibody variants displayed repulsive self-interactions, as judged by their positive  $k_D$  values. Moreover, the high pI antibodies (hOKT3 and trastuzumab) displayed the most repulsive self-interactions. The hOKT3 grafted variants displayed reduced repulsion relative to the parental antibody regardless of the HCDR3 charge. Conversely, the antibodies with lower pIs (siltuximab and lebrizumab) displayed weakly-to-moderately repulsive self-interactions, and the variants with the most repulsive self-interactions had positively charged HCDR3s (Fig. 3). We also observe similar  $k_D$  values for the four parental antibodies at pH 5.5 and 6.5 (Fig. S3), suggesting the general patterns of behavior are weakly impacted by pH in this range of pH values (pH 5.5–6.5) that are relevant to many mAb therapeutic formulations.<sup>10</sup>



To evaluate potential trade-offs between antibody non-specific binding in physiological conditions (PBS, pH 7.4) and self-association in a standard formulation condition (pH 6.0, 10 mM histidine), we plotted them against each other (Fig. 4). For reference, antibodies with  $k_D$  values  $>20$  mL/g in standard formulation conditions (vertical dotted line in Fig. 4) are particularly desirable because they have been shown to have a low likelihood of viscous or opalescent behavior when formulated at high concentrations ( $>100$  mg/mL) for subcutaneous delivery.<sup>10</sup> Likewise, antibodies with low levels of non-specific interactions, such as the levels for the prototypical antibody trastuzumab, are desirable to minimize off-target interactions *in vivo* that can lead to fast antibody clearance. For simplicity, the normalized value of trastuzumab non-specific interactions in each assay is indicated with a dotted horizontal line. Interestingly, most of the antibody variants either displayed both highly repulsive self-interactions and high levels of non-specific binding or both weakly repulsive self-interactions and low levels of non-specific binding. None of the antibody variants displayed as low of levels of non-specific binding as trastuzumab in all assays while displaying highly repulsive self-interactions ( $k_D > 20$  mL/g). The two types of colloidal interactions (self- and non-specific interactions) are thus positively correlated but with opposite implications (Fig. S4). ELISA #2 exhibits a stronger correlation with  $k_D$  (Spearman's  $\rho$  of 0.76) than observed for ELISA #1 (Spearman's  $\rho$  of 0.49). The correlations were weaker between  $k_D$  and the PSP assays [Spearman's  $\rho$  of 0.21 (PSP #1, SMP) and 0.48 (PSP #2, OVA)].

### Molecular properties correlated with non-specific binding and colloidal stability

Given the strong apparent impact of Fv charge on both antibody self-interactions and non-specific binding, we next evaluated correlations for both biophysical measurements with Fv charge and IgG isoelectric point (Table 3). As expected, the correlations were strong (Spearman's  $\rho$  values of 0.75–0.89) and highly significant ( $p$ -values  $<10^{-7}$ ).

We also evaluated correlations between antibody non-specific interactions and self-association for several other sequence- and structure-based antibody properties (Table 3). Many of the charge properties, calculated either based on sequence or structure, displayed strong positive correlations with non-specific interactions and self-association. Interestingly, CDR net charge was much more strongly correlated with the average measurements of the four non-specific binding assays ( $\rho$  of 0.69,  $p$ -value  $<0.0001$ ) than with the measurements of self-interactions ( $\rho$  of 0.49,  $p$ -value of  $<0.05$ ). Structure-based calculations revealed significant correlations between the average of the non-specific interactions assays and the total area of positively charged patches in the CDRs and Fv region ( $\rho$  of 0.75–0.82,  $p$ -values  $<0.00001$ ).

The structure-based calculations also identified strong positive correlations between Fv hydrophilic surface area due to polar residues (including charged residues) and both non-specific and self-interactions ( $\rho$  of 0.52–0.6; Table 3). This is likely due to the dominant contributions of positively charged residues, which are included in the hydrophilic area calculations, to each of the biophysical properties. The calculations of hydrophobicity reveal weaker and more complex correlations, as hydrophobic surface and patch areas are negatively correlated with each property, while measures of the distribution of

hydrophobic residues (hydrophobic moment and imbalance) are positively correlated with these properties.

The dominant role of antibody charge in mediating both non-specific interactions and repulsive self-association suggests that there may be ranges of antibody isoelectric points that are best at balancing the competing demands of high antibody colloidal stability (high levels of repulsive self-interactions) in formulation conditions with the high antibody specificity (low levels of non-specific binding) in physiological conditions. Therefore, we plotted both biophysical properties against each other and highlighted ranges of Fv isoelectric points (Fig. 5). Notably, IgG1s with Fv isoelectric points between 7.5–9 displayed the best combinations of these properties, as seen for the average ELISA (Fig. 5A) and PSP (Fig. 5B) measurements. In particular, the antibodies in these groups generally displayed strongly repulsive self-interactions with low-to-moderate levels of non-specific interactions. Conversely, antibodies with higher isoelectric points displayed high levels of non-specific interactions, while those with lower isoelectric points displayed weaker repulsive self-interactions. Interestingly, the Fv regions from most (61%) of 79 approved antibody drugs have isoelectric points between 7.5–9, suggesting this range of antibody charge properties may be particularly attractive for therapeutic development (Fig. 6A). Human antibody repertoires (14037 mAbs<sup>49, 50</sup>) display similar but slightly higher Fv isoelectric points, as only 49% of such antibodies have isoelectric points between 7.5–9 (Fig. 6B). This may reveal a modest bias toward Fv isoelectric points with intermediate values of 7.5–9 during therapeutic antibody development, although the differences between the two distributions are not statistically significant.

## DISCUSSION

Our studies demonstrate natural trade-offs between two key molecular properties of antibody therapeutics, namely non-specific binding in physiological conditions (pH 7.4, PBS) and self-association in a standard formulation condition (pH 6, 10 mM histidine). Moreover, we demonstrate for the first time, at least to our knowledge, that intermediate ranges of antibody isoelectric point (Fv pIs of 7.5–9, corresponding to IgG1 pIs of 8–8.5) are best for balancing the competing requirements of high colloidal stability in formulation conditions and low non-specific binding in physiological conditions.

While it is obvious that such simple rules of thumb will fail in cases where non-electrostatic interactions play a key role in either type of biophysical property [e.g., see<sup>51</sup> for examples of mutations that cannot be entirely explained by these rules of thumb], it is interesting that this finding is generally consistent with a surprisingly large number of previous observations. For example, several studies have evaluated the self-association behavior of antibody variants in formulation conditions that are either the same or similar to those studied in this work (pH 5–6 and low ionic strength).<sup>10, 20, 26</sup> One notable example, namely omalizumab, displays abnormally high viscosity when concentrated to >100 mg/mL (pH 6, histidine, 15 mM ionic strength), and it has a theoretical Fv pI of 5.8.<sup>20</sup> Notably, introducing mutations into the CDRs that increases the Fv pI to 7.9 significantly reduces self-association and viscosity, which is consistent with our finding that antibodies display highly repulsive self-interactions at Fv pIs between 7.5–9.

More generally, a recent study demonstrated that antibodies with IgG isoelectric points  $>8$  typically displayed favorable viscoelastic and opalescent behavior when concentrated to 150 mg/mL in the same formulation condition evaluated in this work,<sup>10</sup> which is also consistent with our findings that IgG1s with pIs in the range of 8–8.5 display repulsive self-interactions. Our findings also agree with several other studies that high pI antibodies typically display strongly repulsive self-interactions and/or low viscosities, and low pI antibodies typically display stronger self-association and/or increased viscosity in standard formulation conditions.<sup>21–23, 26, 28, 42, 51, 52</sup> Finally, it is important to note that increasing the ionic strength in weakly basic formulations (e.g., pH 6) will, in some cases, reduce antibody self-association,<sup>18, 20, 53, 54</sup> and should be investigated further in the future in relation to our findings.

Our findings are also consistent with several other studies on the molecular determinants of antibody non-specific interactions in physiological conditions. For example, several studies report that increased positive charge in the CDRs or Fv in general promotes antibody non-specific binding,<sup>14, 35, 55–59</sup> as we observed for high pI antibodies in this work. One of the most striking examples of this is the cationization of polyclonal IgGs using chemical derivatization, which shifts the pI of the IgG antibody mixture from a pI range of 5.9–9 to 8.7–10.3, and increases non-specific cellular uptake several fold.<sup>59</sup> Conversely, multiple studies report that increased negative charge in the CDRs or Fv in general are linked to reduced non-specific binding.<sup>35, 60, 61</sup> Moreover, we evaluated three sets of previously reported non-specific binding data for clinical-stage antibodies<sup>9</sup> and found that antibodies with Fv pIs  $\geq 8.7$  display significantly higher levels of non-specific binding than antibodies with lower Fv pIs ( $p$ -values of 0.0001–0.01 for  $2 \times 2$  contingency table analysis), which is also consistent with our findings in this study.

It also notable that reducing IgG pI has been reported to reduce antibody clearance *in vivo*,<sup>31, 33, 37, 62</sup> which is likely due to reduced non-specific interactions along with other contributing factors. Notably, a previous study predicted that Fv charge  $<+6.2$  (and  $>0$ ) at pH 5.5 was optimal for promoting favorable antibody pharmacokinetics.<sup>42</sup> This range of Fv charges corresponds to antibodies with Fv pIs of 4.9–8.7, which is consistent with our rule of thumb that antibodies with Fv pIs  $<9$  have low-to-moderate levels of non-specific interactions.

Our findings motivate the development of phenomenological models, rather than overly simple rules of thumb, that can better predict antibodies with Fv properties that balance the competing demands of low self-association in formulation conditions and low non-specific binding in physiological conditions. This will require much larger and more diverse datasets, including those with antibody framework and CDR diversity. Additionally, in this study we only focus on the human IgG1 subclass because it represents the largest proportion (~two thirds) of the approved antibody therapeutics. Future work will be required to further expand our analysis to other subclasses such as IgG2 and IgG4 to test the generality of our findings. To enable the generation of such large datasets, it will be critical to use methods that can evaluate antibody non-specific and self-interactions at ultra-dilute concentrations (~0.001–0.01 mg/mL). Two assays that are particularly well suited for this challenge are the PSP assay, which was used this study, for measuring non-specific interactions in physiological

conditions and the CS-SINS assay,<sup>63</sup> a refined version of AC-SINS<sup>64–66</sup> that was reported after this study was completed, for measuring self-interactions in standard formulation conditions (pH 6 and 10 mM histidine). The combination of these two assays holds great potential for generating large datasets (hundreds to thousands of mAbs) for developing models that can predict both antibody non-specific and self-interactions, which we believe are critical to advance the identification of therapeutic antibodies with drug-like colloidal properties and increased likelihood of success in clinical development.

In conclusion, our studies resolve some existing conflicts in the field that report seemingly contradictory findings as to whether low or high pI antibodies have optimal physicochemical properties for antibody development. The fact that neither extreme is desired naturally leads to the conclusion that intermediate pI antibodies are generally best at balancing the competing demands of antibody colloidal properties in formulation and physiological conditions. It will be important in the future to identify more refined predictors of antibodies with the best combinations of *in vitro* (formulation) and *in vivo* (bioavailability) properties, which will require accounting for other types of charge (e.g., dipole-dipole) and non-charged (e.g., hydrophobic) interactions. These modelling efforts hold great potential for improving antibody candidate selection and protein engineering at early stages of drug development to reduce the risk for problems that may emerge later in drug development and clinical trials.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

## ACKNOWLEDGEMENTS

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## SUPPORTING INFORMATION

The supporting figures include: i) a summary of the antibody amino acid sequences used in this study, measurements of diffusion interaction parameters ( $k_D$ ) for all of variants at pH 6 (10 mM histidine) and for a subset of the parent mAbs at pH 5.5–6.5 (10 mM histidine); and ii) a comparison of colloidal interactions in physiological (PBS, pH 7.4) and formulation (10 mM histidine, pH 6) conditions. The supporting tables include: i) monomer quality assessment by analytical size exclusion chromatography; and ii) thermal melting temperature (midpoint of unfolding) of the purified antibody variants.

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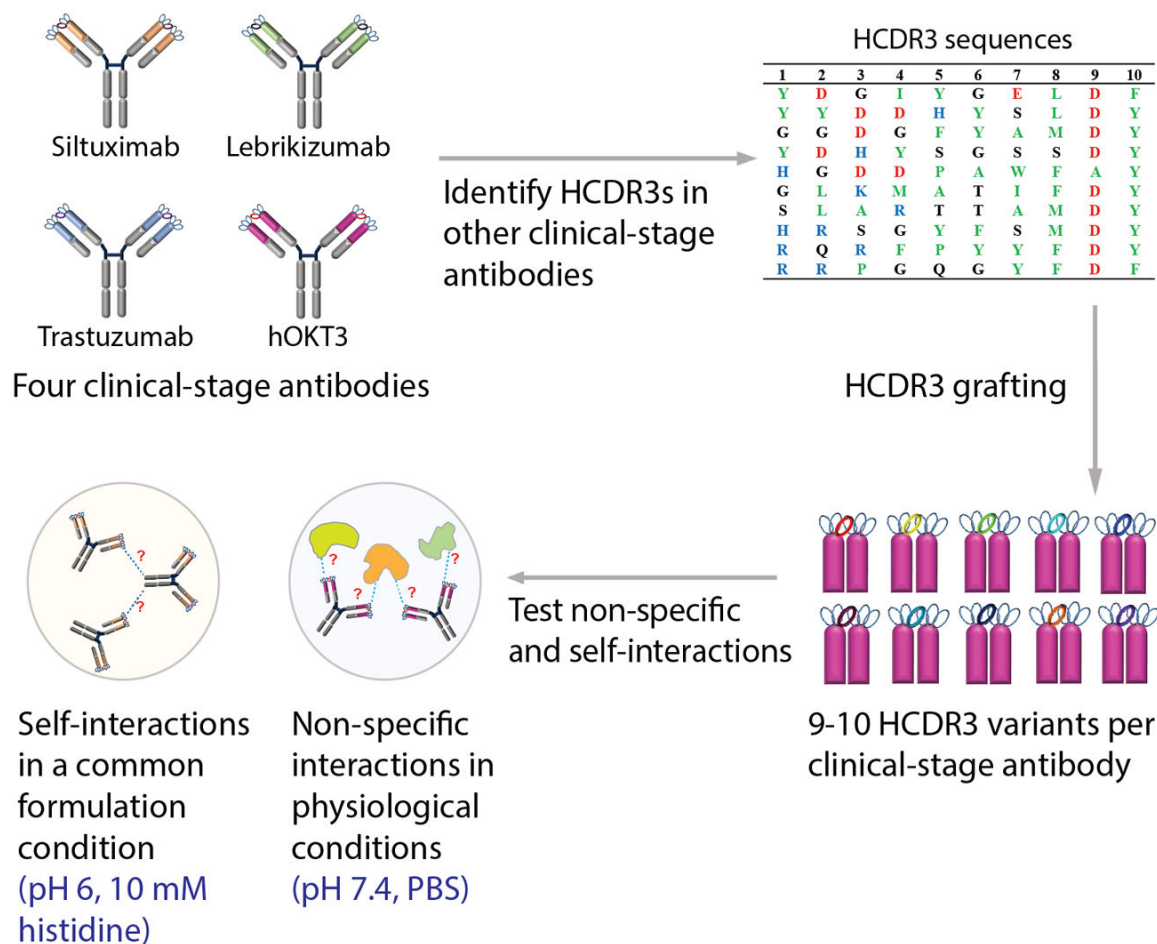
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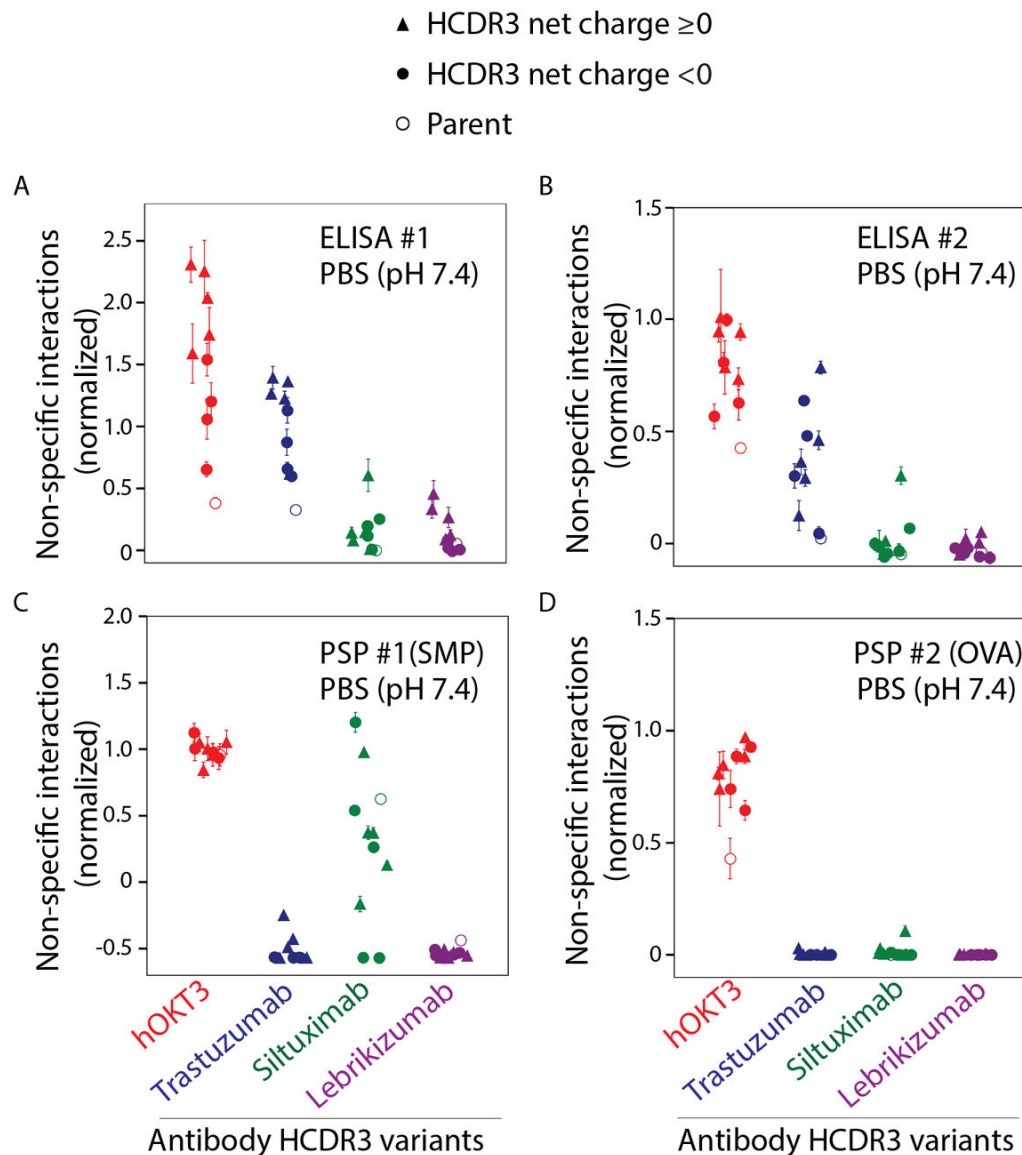
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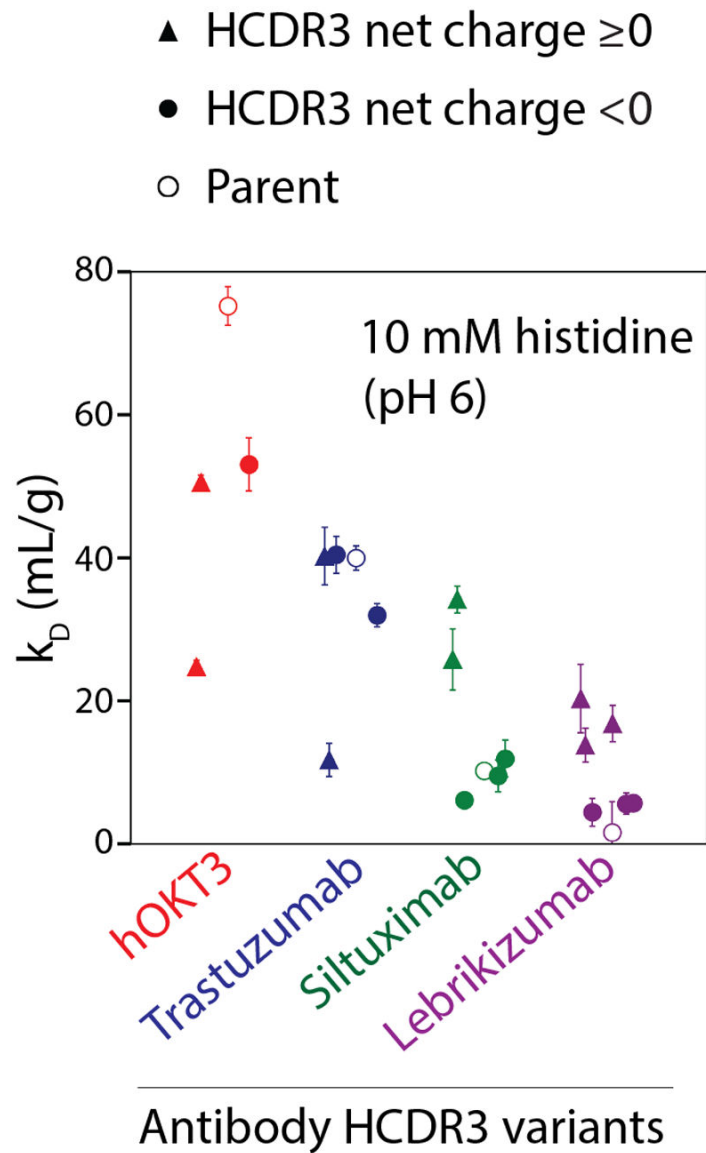
**Figure 1. Design of a panel of antibody variants based on four clinical-stage antibodies with grafted heavy chain CDR3s.**

Antibody variants were designed using the variable regions of four clinical-stage antibodies, namely humanized OKT3 (hOKT3), trastuzumab, siltuximab and lebrikizumab, that were grafted onto a common IgG1 scaffold. The heavy chain CDR3 (HCDR3) loops from ten clinical-stage antibodies (carlumab, muromonab, trastuzumab, bapineuzumab, farletuzumab, seribantumab, tocilizumab, girentuximab, lenzilumab and ustekinumab) were grafted onto each of the four clinical-stage antibody scaffolds. The panel of grafted antibodies was evaluated in terms of antibody self-association in a standard formulation condition (pH 6, 10 mM histidine) and physiological conditions (pH 7.4, PBS) to evaluate potential trade-offs between these two properties. The muromonab HCDR3 contains a cysteine residue that was mutated to serine in this study.

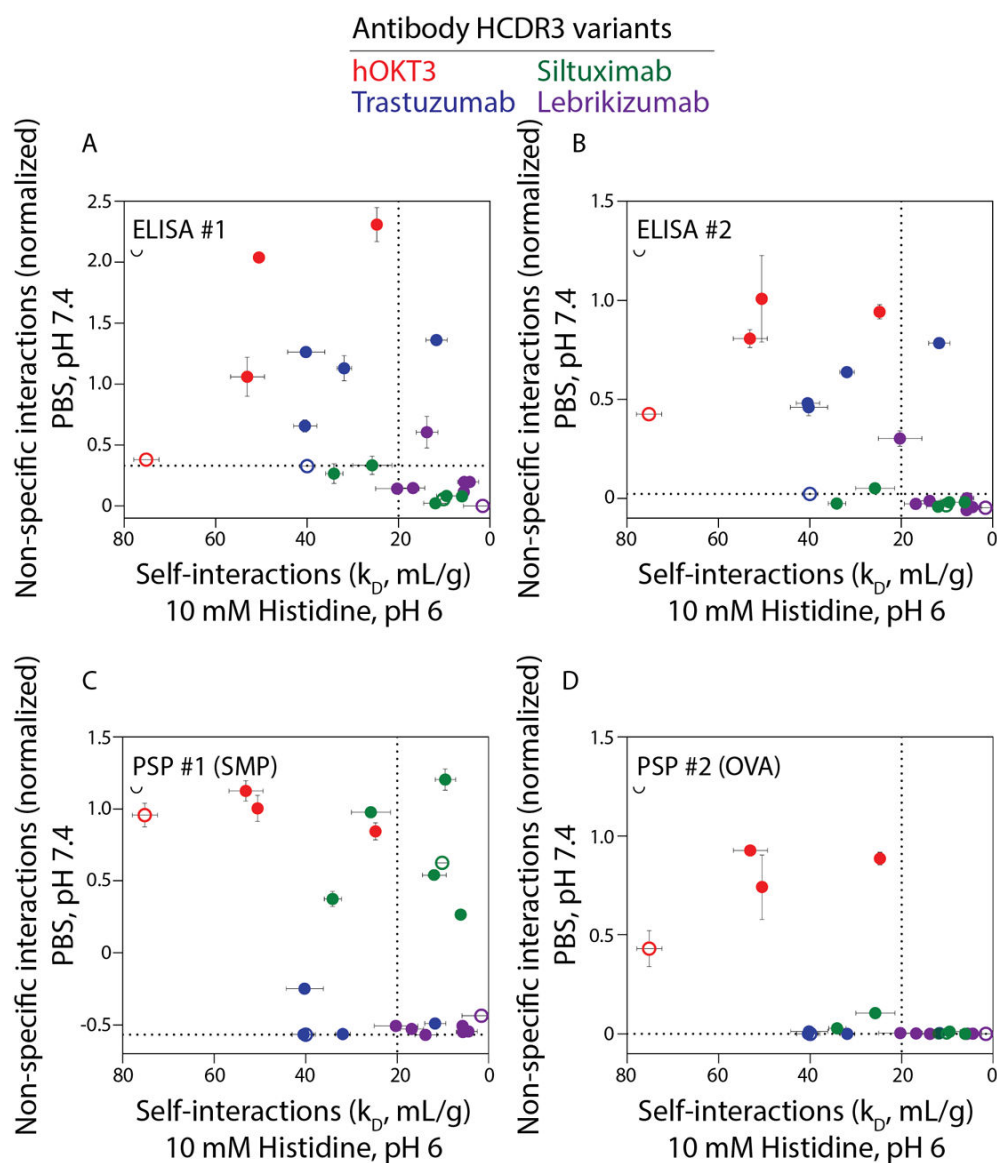


**Figure 2. Evaluation of non-specific interactions for grafted antibody variants in physiological conditions (pH 7.4, PBS).**

The antibody variants were evaluated using two ELISAs (#1 and #2), one with (A) with six different reagents (cardiolipin, LPS, KLH, ssDNA, dsDNA and insulin) and the second assay with (B) baculovirus particles (BVP). The variants were also evaluated using two flow cytometry (Polyspecificity Particle, PSP) assays, one with (C) soluble membrane proteins (SMP, PSP #1) and second one with (D) ovalbumin (OVA, PSP#2). ELISA and PSP assay values were normalized on a scale of 0 to 1 using adalimumab and bococizumab as negative and positive controls for nonspecific binding, respectively. The parental antibodies are indicated in open circles, while the negatively charged HCDR3s are indicated in filled circles and the positively charged HCDR3s are indicated in filled triangles. The values reported are averages for three independent experiments, and the error bars are standard deviations.

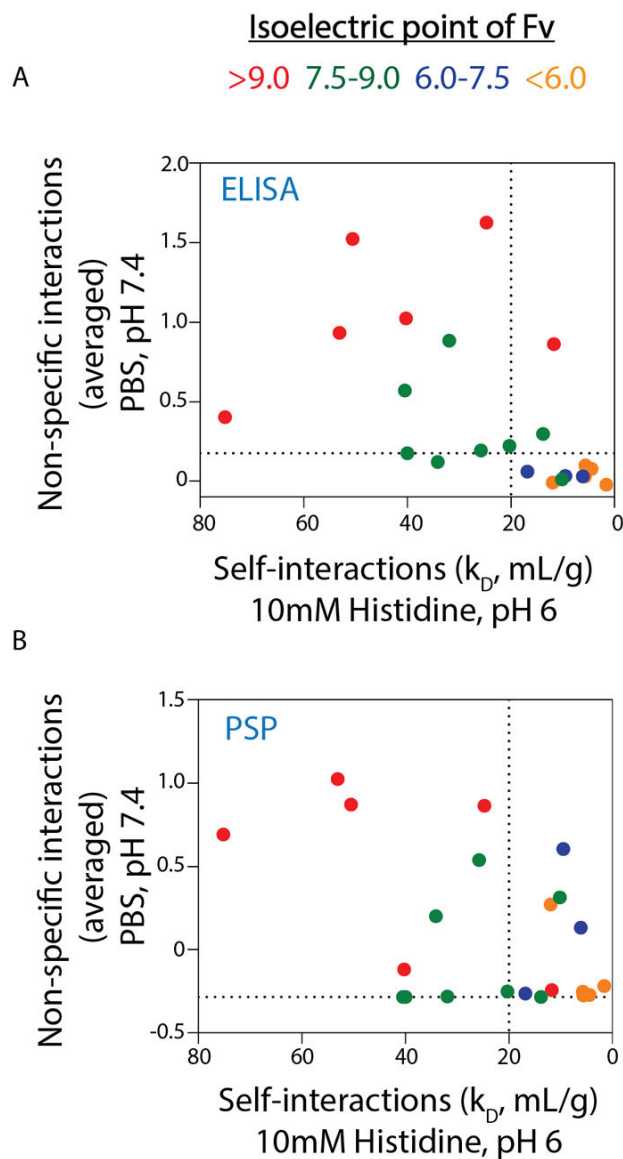


**Figure 3. Evaluation of self-interactions for grafted antibody variants in a standard formulation condition (pH 6, 10 mM histidine).** The antibody variants were evaluated using dynamic light scattering to measure diffusion interaction parameters ( $k_D$ ). The parental antibodies are indicated in open circles, while the negatively charged HCDRs are indicated in filled circles and the positively charged HCDR3s are indicated in filled triangles. The values reported are averages for three independent experiments, and the error bars are standard deviations.



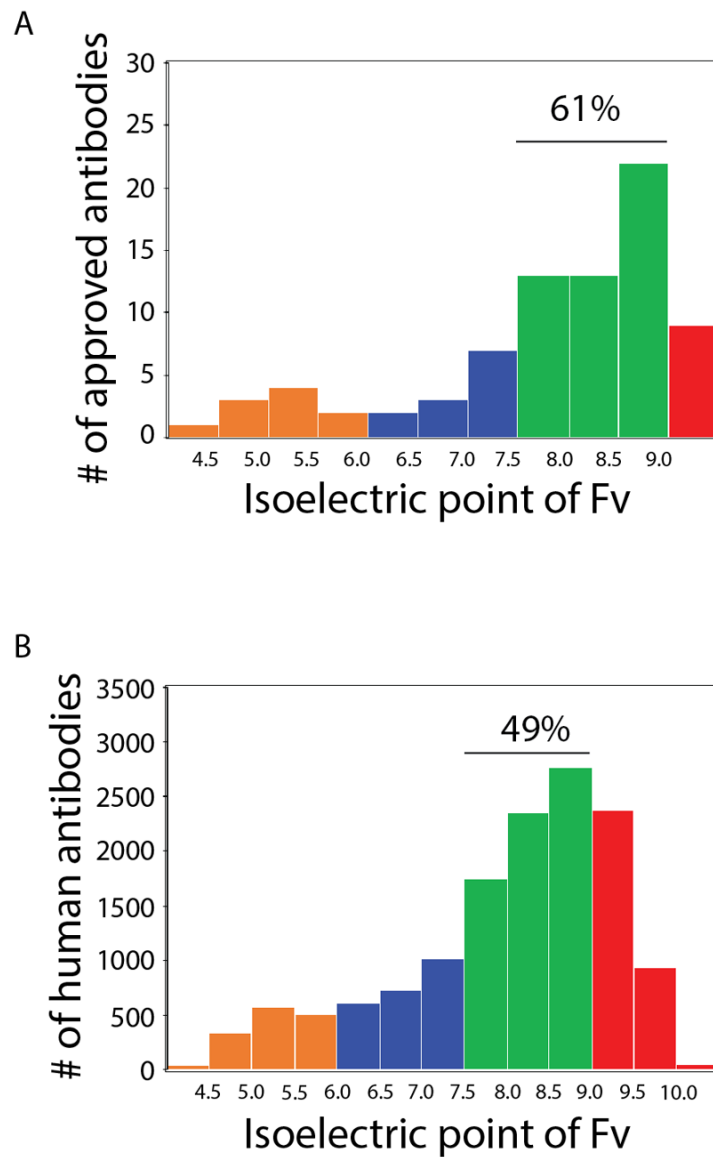
**Figure 4. Trade-offs between antibody non-specific interactions in physiological conditions and self-interactions in a standard formulation condition.**

Comparison of antibody self-interactions ( $k_D$ , diffusion interaction parameter) and nonspecific binding using (A) ELISA #1, (B) ELISA #2, (C) PSP #1 and (D) PSP #2. The dotted line at a  $k_D$  value of 20 mL/g indicates a previously reported threshold for strongly repulsive self-interactions corresponding to desirable viscoelastic and opalescent properties for concentrated antibody formulations.<sup>10</sup> The dotted line is the normalized non-specific binding value for trastuzumab, which is used as a threshold for low levels of non-specific binding in each assay. The parental antibodies are indicated in open circles. Notably, antibodies with low non-specific binding generally also display low levels of repulsive self-interactions (small  $k_D$  values). Conversely, antibodies that generally display highly repulsive self-interactions (large  $k_D$  values) also generally display high levels of non-specific binding.



**Figure 5. Antibodies with intermediate Fv isoelectric points display the best combination of formulation and physiological colloidal properties.**

Antibodies with low isoelectric points display low levels of non-specific interactions in physiological conditions but weakly repulsive self-interactions in formulation conditions. Conversely, antibodies with high isoelectric points display highly repulsive self-interactions in formulation conditions but high levels of non-specific interactions in physiological conditions. Intermediate isoelectric points of 7.5–9 for Fv provide an attractive balance of strongly repulsive self-interactions in formulation conditions and low-to-moderate levels of non-specific binding in physiological conditions. Y-axes represents the average values from the two (A) ELISA and (B) PSP assays used to evaluate non-specific interactions. The dotted lines are defined in Fig. 4.



**Figure 6. Distributions of Fv isoelectric for approved antibody drugs and human antibodies in general.**  
Distribution of Fv isoelectric points for (A) 79 approved antibodies (median pI of 8.14) and (B) 14037 human antibodies (median pI of 8.34).

**Table 1.**

Summary of the four clinical-stage antibodies evaluated in the study. The most homologous human germlines for the V<sub>H</sub> and V<sub>L</sub> domains are noted. The antibodies display a range of net charges and isoelectric points. Antibody charge values were calculated at pH 7.4 using values of -1 for Asp and Glu, +1 for Arg and Lys, and +0.1 for His.

Antibody framework	pI			Net charge (pH 7.4)			Closest human germline	
	V <sub>H</sub>	V <sub>L</sub>	Fv	V <sub>H</sub>	V <sub>L</sub>	Fv	V <sub>H</sub>	V <sub>L</sub>
<b>hOKT3</b>	9.2	9.2	9.3	5.2	4	9.2	IGHV1-46	IGKV3-20
<b>Trastuzumab</b>	8.0	8.6	8.6	1.1	2.1	3.1	IGHV3-66	IGKV1-39
<b>Siltuximab</b>	6.5	7.9	7.8	-1	1	0	IGHV3-23	IGKV3-11
<b>Lebrikizumab</b>	7.9	4.9	5.4	1	-2.9	-1.9	IGHV2-70	IGKV4-1

**Table 2.**

Summary of the heavy chain CDR3 (HCDR3) sequences used for CDR grafting in this work. The HCDR3 sequences from clinical-stage antibodies possess differences in net charge and sequence composition consisting of negatively charged (red), positively charged (blue), hydrophobic (green) and polar (black) residues. The net charges of the HCDR3 and Fv regions (pH 7.4) are calculated as described in Table 1. The muromonab HCDR3 contains a cysteine that was mutated to serine in this study.

HCDR3 #	HCDR3 amino acid sequences											Origin of HCDR3	HCDR3 net charge (pH 6)	HCDR3 net charge (pH 7.4)	Fv net charge of variants (pH 7.4)			
	hOKT3	Tras.	Silt.	Lebr.														
1	Y	D	G	I	Y	G	E	L	D	F	Carlumab	-3	-3	9.1	2.2	-2	-2.9	
2	Y	Y	D	D	H	Y	S	L	D	Y	Muromonab*	-2.5	-2.9	9.2	2.3	-1.9	-2.8	
3	G	G	D	G	F	Y	A	M	D	Y	Trastuzumab	-2	-2	10.1	3.2	-1	-1.9	
4	Y	D	H	Y	S	G	S	S	D	Y	Bapineuzumab	-1.5	-1.9	10.2	3.3	-0.9	-1.8	
5	H	G	D	D	P	A	W	F	A	Y	Farletuzumab	-1.5	-1.9	10.2	3.3	-0.9	-1.8	
6	G	L	K	M	A	T	I	F	D	Y	Seribantumab	0	0	12.1	5.2	1	0.1	
7	S	L	A	R	T	T	A	M	D	Y	Tocilizumab	0	0	12.1	5.2	1	0.1	
8	H	R	S	G	Y	F	S	M	D	Y	Girentuximab	0.5	0.1	12.2	5.3	1.1	0.2	
9	R	Q	R	F	P	Y	Y	F	D	Y	Lenzilumab	1	1	13.1	6.2	2	1.1	
10	R	R	P	G	Q	G	Y	F	D	F	Ustekinumab	1	1	13.1	6.2	2	1.1	



**Table 3.**

Evaluation of antibody molecular properties that are most strongly correlated with non-specific interactions in physiological conditions (PBS, pH 7.4) and self-association in formulation conditions (10 mM histidine, pH 6). The sequence-based charge features were calculated as described in Table 1. The ELISA/PSP results are for the average measurements from the four assays. The structure-based features were evaluated from Fv homology models using Molecular Operating Environment software.

Molecular Property	Region	Descriptors	ELISA #1 (pH 7.4)		ELISA #2 (pH 7.4)		PSP #1 SMP (pH 7.4)		PSP #2 OVA (pH 7.4)		ELISA/PSP (pH 7.4)		kD, mL/g (pH 6)		
			Spearman's correlation	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value
Sequence Based	Electrostatic	HCDR3	Net charge	0.34	*	0.25	ns	0.09	ns	0.34	*	0.26	ns	0.12	ns
		CDR	Net charge	0.80	****	0.76	****	0.29	ns	0.55	***	0.69	****	0.49	*
		V <sub>L</sub>	Net charge	0.78	****	0.79	****	0.50	**	0.46	**	0.87	****	0.76	***
		V <sub>H</sub>	Net charge	0.77	****	0.81	****	0.32	*	0.59	****	0.68	****	0.62	*
		Fv	Net charge	0.88	****	0.89	****	0.42	**	0.55	***	0.88	****	0.86	****
		Fv	Cross charge (V <sub>H</sub> x V <sub>L</sub> )	0.82	****	0.75	****	0.53	**	0.53	***	0.86	****	0.63	*
		Fv	pI	0.86	****	0.83	****	0.48	*	0.56	***	0.88	****	0.84	****
		IgG	pI	0.85	****	0.84	****	0.48	*	0.56	***	0.89	****	0.84	****
Structure Based (Fv)	Stability	Fv	Buried SA (V <sub>H</sub> /V <sub>L</sub> interface); Å <sup>2</sup>	-0.53	**	-0.50	**	0.26	ns	0.14	ns	-0.32	*	-0.18	ns
		Fv	Interaction energy (V <sub>H</sub> /V <sub>L</sub> interface); Å <sup>2</sup>	0.59	***	0.56	**	-0.15	ns	-0.07	ns	0.40	**	0.22	ns
		Fv	Hydrophilic SA; Å <sup>2</sup>	0.76	****	0.73	****	0.04	ns	0.16	ns	0.60	****	0.52	*
	Electrostatic	Fv	Positive patch SA; Å <sup>2</sup>	0.82	****	0.77	****	0.37	*	0.38	*	0.82	****	0.71	**
		Fv	Negative patch SA; Å <sup>2</sup>	-0.09	ns	0.01	ns	0.02	ns	0.11	ns	-0.16	ns	-0.20	ns
		CDR	Positive patch SA near CDR; Å <sup>2</sup>	0.84	****	0.82	****	0.28	ns	0.40	**	0.75	****	0.60	*
		CDR	Negative patch SA near CDR; Å <sup>2</sup>	-0.08	ns	0.01	ns	0.24	ns	0.23	ns	-0.01	ns	-0.02	ns
		Fv	Dipole moment (Debye)	0.26	ns	0.30	Ns	0.27	ns	0.48	**	0.22	ns	-0.06	ns
		CDR	Net charge	0.72	****	0.67	****	-0.12	ns	0.15	ns	0.48	**	0.48	*
		Fv	Net charge	0.81	****	0.79	****	0.57	****	0.63	****	0.88	****	0.75	***
Fv	pI	0.84	****	0.81	****	0.53	***	0.62	****	0.89	****	0.82	****		

Molecular Property	Region	Descriptors	ELISA #1 (pH 7.4)		ELISA #2 (pH 7.4)		PSP #1 SMP (pH 7.4)		PSP #2 OVA (pH 7.4)		ELISA/PSP (pH 7.4)		kD, mL/g (pH 6)	
			Spearman's correlation	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$	p-value	$\rho$
<b>Hydrophobic</b>	Fv	Zeta potential (mV)	0.81	****	0.79	****	0.57	****	0.63	****	0.88	****	0.75	***
	Fv	Hydrophobic SA; Å <sup>2</sup>	-0.49	**	-0.48	*	-0.11	ns	-0.05	ns	-0.48	**	-0.65	*
	Fv	Hydrophobic SA; Å <sup>2</sup>	-0.35	*	-0.37	*	-0.20	ns	-0.36	*	-0.32	*	-0.20	ns
	CDR	Hydrophobic patch SA near CDR; Å <sup>2</sup>	-0.67	****	-0.65	****	-0.47	**	-0.42	**	-0.77	****	-0.69	**
	Fv	Hydrophobic moment	0.56	**	0.51	*	-0.27	ns	-0.14	ns	0.31	*	0.31	ns
	Fv	Hydrophobic imbalance	0.51	**	0.48	*	0.15	ns	0.00	ns	0.57	****	0.42	*

Spearman's  $\rho$  and p-values are reported, the latter which are indicated as values <0.0001 (\*\*\*\*), <0.001 (\*\*\*), <0.01 (\*\*), 0.01 to 0.05 (\*), and >0.05 (ns). Surface area is referred to as SA.