doi: 10.1111/idj.12394

# Scientific update on nanoparticles in dentistry\*

Gottfried Schmalz<sup>1,2</sup>, Reinhard Hickel<sup>3</sup>, Kirsten L. van Landuyt<sup>4</sup> and Franz-Xaver Reichl<sup>3</sup>

<sup>1</sup>Department of Conservative Dentistry and Periodontology, University Hospital, Regensburg, Germany; <sup>2</sup>Department of Peridontology, University of Bern, Bern, Switzerland; <sup>3</sup>Department of Conservative Dentistry and Periodontology, University Hospital, LMU Munich, Munich, Germany; <sup>4</sup> Department of Oral Health Sciences, KU Leuven Biomat, Leuven, Belgium.

Nanoparticles having a size from 1 to 100 nm are present in nature and are successfully used in many products of daily life. In dental materials, nanoparticles are typically embedded but they may also exist as by-products from milling processes. Possible adverse effects of nanoparticles have gained increased interest, with the lungs being the main target organ. Exposure to nanoparticles in the dental laboratory is addressed by legal regulations. In dental practice, nanoparticles are mainly produced by intra-oral grinding/polishing and removal of materials, by wear of restorations or release from dental implants. Based on worst-case mass-based calculations, the additional risk as a result of exposure to nanoparticles is considered to be low. However, more research is needed, especially on vulnerable groups (patients with asthma or chronic obstructive pulmonary disease). An assessment of risks for the environment is not possible because of lack of data. Exposure-reduction measures mainly include avoidance of abrasive processes (for example, by proper sculpturing), cooling by the use of water spray and sufficient ventilation of treatment areas.

Key words: Nanoparticles, composites, titan, organs, risk assessment

## INTRODUCTION†

Nanomedicine is the controlled use of nanotechnologies/nanoparticles in healthcare, leading to new pathways for the diagnosis and treatment of human diseases<sup>1</sup>. Nanoparticles are present in nature and are used in daily life; for example, in cosmetic products, such as sun screens [in which titanium dioxide  $(TiO<sub>2</sub>)$ ] or zinc oxide (ZnO) particles are added as ultraviolet (UV) light filters], or in toothpastes, in dietary supplements and in sprays used for coating, cleaning and impregnation<sup>2</sup>. Silicon dioxide (SiO<sub>2</sub>), magnesium oxide (MgO) and  $TiO<sub>2</sub>$  are tested and licensed food additives in some countries<sup>3</sup>. Altogether, use of nanotechnology has great potential for improving daily life.

In dentistry, nanoparticles are intentionally embedded into products to improve material properties<sup>4</sup>. Dental materials that intentionally release nanoparticles are rare; such materials include scanning sprays for computer-aided design/computer-aided manufacturing  $(CAD/CAM)^5$  or occlusion indicator foils. On the other hand, nanoparticles can be non-intentional by-products from milling processes for fillers. It has been estimated that nanoparticles are present in about 3,500 dental materials. The aim of this brief survey is to provide some basic information for the dental community on nanoparticles. The original text for this review has been published recently elsewhere<sup>6</sup>; here, we provide a shortened version.

#### **DEFINITIONS**

According to the European Union (EU), nanoparticles have one or more external dimensions in the size range from 1 to 100 nm<sup>7</sup>. More detailed definitions are provided by the International Organization for Standardization (ISO)<sup>8,9</sup>. Nano-sized single particles may, however, arise readily to form clusters, namely aggregates (strongly bonded) and agglomerates (weakly bonded)<sup>8</sup> . The definition of a nanomaterial (e.g. by the  $EU^7$ ) is presently under discussion and

<sup>\*</sup>The original manuscript was prepared for and discussed in the Dental Materials Task Team of FDI and in FDI Science Committee and was published in Dental Materials (Dent. Mater. 2017 Nov; 33 (11):1298–1314). As agreed with the FDI the present shortened version was prepared for the International Dental Journal . Copyright permission was obtained from the Academy of Dental Materials.

<sup>&</sup>lt;sup>†</sup>In this review literal citations e.g. from ISO, EU and other documents are used without quotation marks in each case for better readability; respective references are provided.

may be changed; therefore, in this review only the term nanoparticle (see above) is used.

The dose for nanoparticle exposure is often the number of particles<sup>10</sup> or the total surface of applied nanoparticles. There is also a tradition of mass being used for risk assessment (e.g. for dust exposure<sup>11</sup>). Furthermore, the only presently available limit values (e.g. for fine dust exposure) are given as mass values and this is why the present risk analysis used mass.

## BIOLOGICAL RELEVANCE OF NANOPARTICLES - WHY CARE?

Compared with bulk materials, the surface area/volume ratio [volume-specific surface area (VSSA)] of nanoparticles is greatly increased and therefore they are much more reactive compared with larger particles with the same composition. The elution/release of potentially toxic substances may also be enhanced. It is also possible for the passage/translocation of nanoparticles through the intestines into the lymphatic system<sup>12</sup>. As a consequence of cellular uptake of nanoparticles, upregulation of reactive oxygen species, DNA damage and impaired DNA repair have been reported<sup>13</sup>. Contamination of the surface of nanoparticles, for example with endotoxin, is possible<sup>14</sup>.

Fibres play a role, especially in regard to inhalation<sup>10</sup>. Multiwalled carbon nanotubes are carcinogenic to rat  $\text{lungs}^{15}$ . However, the International Agency for Research on Cancer (IARC)<sup>16</sup> did not consider the evidence to be strong enough to alter its evaluations (possibly carcinogenic to humans – Group 2B). Furthermore, chronic inflammation, especially in patients with asthma or chronic obstructive pulmonary disease  $(COPD)^{17}$ , has been reported. There seems to be a significant association between air concentration of the fine dust fraction and increased risk of lung cancer<sup>18</sup>, cardiovascular diseases<sup>19</sup> and allergic reactions in atopic patients<sup>20</sup>. The relevance of these findings in dentistry is unknown.

## NANOPARTICLES IN/FROM DENTAL MATERIALS

Resin-based composites contain anorganic filler particles of different sizes, ranging from supra-micron, to sub-micron and nano-sized<sup>21</sup>. Today, mainly radio-opaque glass-fillers containing, for example, barium, zirconium, strontium or ytterbium with a size between 400 nm and 1  $\mu$ m, or even larger, are used together with nano-sized particles such as pyrogenic silica (SiO<sub>2</sub>) or zirconium dioxide (ZrO<sub>2</sub>)- $SiO<sub>2</sub>$ . The filler particles are embedded in the resin matrix and chemically attached to it through silane coupling.

Zinc phosphate cements contain ZnO or MgO particles in the powder, glass ionomer cements contain finely ground glass particles and some products may contain pyrogenic silica as nanofillers. Hydraulic calcium silicate cements contain different calcium silicates and aluminates $22$  and impression materials contain a variety of fillers (e.g.  $ZnO$  or  $TiO<sub>2</sub>$ ). Filler size is normally in the micrometre range, but nanoparticles can be non-intentional by-products of the milling process.

The above-mentioned materials are delivered as premixed pastes which are cured by light activation within 1 minute or as paste/paste or powder/liquid systems, which have to be mixed and which set in <5 minutes. Nanoparticles on implants are strongly bound ('fixed') to the surface of the implant<sup>10</sup> to prevent infection (e.g. silver nanoparticles) or to improve biocompatibility [e.g. apatite or titanium (Ti) parti $cles^{23}$ . Furthermore, pigments in the form of nanoparticles are used. When grinding resin materials, nanoparticles containing substances of unknown composition derived from the resinous matrix through heat generation<sup>24</sup> may be produced.

## NANOPARTICLES IN/FROM DENTAL MATERIALS – RELEASE AND EXPOSURE

## Occupational exposure

Nanoparticles are released as dust in the dental laboratory. Special legal regulations for occupational safety are available for different countries (e.g. Occupational Safety and Health Administration<sup>25</sup>).

In the dental office, premixed pastes (e.g. resinbased composite pastes) are used and nanoparticles in these pastes are described as 'free' with a high potential for systemic exposure<sup>10</sup>. However, the movement of particles in dental pastes is limited by 'capillary transverse pressure<sup>,26,27</sup>. This keeps wetted particles away from the surface of a paste-like material and thus nanoparticles in dental pastes are normally not available on the surface (K. Dermann, personal communication). The mixing of powder/liquid materials may lead to short-term exposure to particles for the dental personnel, but not for the patient. Actual data on release of nanoparticles from unset dental materials are, however, missing.

For set materials, peak concentrations of respirable dust could be observed when the dentist was finishing/ polishing composite restorations in the front teeth without water coolant<sup>28</sup> and the airborne fraction was mainly nano-sized<sup>29</sup> with concentrations of above  $10^6$ particles/cm<sup>3</sup> in the breathing zone of both patient and dentist. Nanoparticles may also be produced by grinding resin materials, which per se do not contain nanoparticles $^{24}$ .

The risk assessment presented in this review is based on 57 million fillings placed in Germany (in

 $2015$ <sup>30</sup> and 71,425 practicing dentists (in 2015), representing, on average, three fillings per dentist each day with about 80% of fillings being of composite material. As dentists were included who normally do not place fillings, it can be estimated that three to six fillings are placed each day by every dentist who performs such procedures. Taking possible variations into account, for a risk assessment, 10 composite fillings per dentist per day are considered here to represent the worst-case scenario.

#### Exposure of patients

No release of nanoparticles from unset restorative materials is expected. For set materials, risk assessment is based on the above-mentioned figures from Germany for 82,175,684 inhabitants (at 31 December 2015). Thus, 0.67 fillings per inhabitant were placed in 2015. As this calculation also covers patients without teeth, an average exposure of one to two fillings per patient per year can be assumed. Taking possible variations into account, for a risk assessment, five fillings per year are assumed in a worst-case scenario.

Nanoparticles from dental-restorative materials may be generated by wear and swallowed. For resin-based composites, a mean annual occlusal wear of up  $100 \mu m$  was reported in 2006<sup>31</sup>. In more recent studies, after 3 or 5 years in situ<sup>32</sup> annual wear rates of up to 30–40 µm were measured. For amalgam an annual wear rate of 60  $\mu$ m was reported<sup>31</sup>. Wear rates are lower for ceramic materials than for composites<sup>31</sup>. For glass ionomer cements or combinations of resin materials with cements, data on wear are sparse. Generally, the wear for these materials is regarded to be greater than for composites. However, these materials are only recommended for Class I and Class V cavities with reduced wear<sup>33</sup>.

In summary, for all dental-restorative materials a general loss of up to  $50 \mu m$  per year seems a reasonable assumption. However, taking possible variations into account, for a risk assessment, beside 50 lm also 100 lm per year, and based on a recent study<sup>34</sup>, 250  $\mu$ m per 3 years, are taken as the worst-case scenario.

Titanium particles could be observed in periimplant tissues and in newly formed bone<sup>35</sup> and were probably detached during insertion of the implant<sup>36</sup> or were released after insertion $37$ . In a postmortem study<sup>38</sup> the highest Ti content detected in human mandibular bone was found to be  $37,700 \mu g/kg$  of bone weight at a distance of  $556-1,587 \mu m$  from the implants, and the intensity increased with decreasing distance from implants. Particles with sizes of 0.5– 40 lm were found in human jawbone marrow tissues at distances of  $60-700 \mu m$  from dental implants<sup>38</sup>.

Silver nanoparticles (AgNPs) have been applied in different dental materials, but release data are rare. However, materials containing silver ion-implanted fillers had antibacterial effects<sup>39</sup> and metallic implant coatings released  $550 \text{ µg/l}$  of AgNPs after released  $550 \text{ µg/l}$  of AgNPs after  $168$  hours<sup>40</sup>.

## Environment/Waste generation

Nanoparticles created during the removal of dental restorations may end up in the effluent of the dental office and thus in the environment; separators are only available for amalgam waste $41$ . Bisphenol A (BPA) and several resin monomers are eluted from resin-based composites (bulk samples) over a long period of time<sup>42</sup>. From composite dust, up to 970  $\mu$ g/m<sup>3</sup> of triethyleneglycol dimethacrylate (TEGDMA),  $360 \text{ µg/m}^3$  of urethane dimethacrylate (UDMA),  $180$  $\mu$ g/m<sup>3</sup> of bisphenol A glycidylmethacrylate (Bis-GMA) and 1.28  $\mu$ g/m<sup>3</sup> of BPA were eluted into ethanol<sup>43</sup>.

## NANOPARTICLES IN/FROM DENTAL MATERIALS – RISK ASSESSMENT

This risk assessment concentrates on the additional effects of nanoparticles from dental materials. Material-related (mainly chemically induced) biocompatibility effects, such as allergic responses, are not covered here in detail.

## Inhalation/Dust

Dust <5 µm and >0.01 µm can penetrate deep into the alveolar region of the lungs<sup>44</sup>. Particles released from composites are in the nanoscale size and thus able to reach the lungs of patients and dental personnel<sup>29</sup>. In spite of efficient macrophage phagocytosis<sup>45</sup>, an overload may lead to an excessive production of inflammatory mediators and sustain inflammation and fibrotic changes. However, in vitro exposure of bronchial epithelial cells to up to 3.3 mg/ml of resinbased composite dust did not result in membrane damage or in the release of interleukin-1beta (IL- $1\beta$ <sup>46</sup>. Metabolic activity of the cells decreased at concentrations of dust particles of  $>660 \mu g/ml$ . In a similar study, alveolar macrophages were exposed to the respirable fraction (i.e. dust particles of size  $\leq$   $\frac{1}{45}$ . They were able to phagocytize the composite dust particles. As they tolerated a comparatively high cell burden (60 pg of dust particles per cell), the cytotoxic potential of respirable composite dust seemed to be low.

To estimate exposure to nanoparticles, the size distribution by number of particles is used, as published by van Landuyt et  $al.^{28}$ . Thus, the nano-fraction corresponds to a concentration of 0.0004–0.0013% (w/ w) of the total dust. This order of magnitude is confirmed by data from Bradna et  $al.^{47}$ .

For the 10 restorations placed per dentist per year (see above), with five fillings in premolars (surface 75 mm<sup>2</sup> ) and five fillings in molars (surface 150 mm<sup>2</sup>), this sums to a total surface of 225 mm<sup>2</sup>. Assuming a vertical removal of 1 mm, this would result in an exposure of  $450,000 \text{ µg}$  of dust. The nano-fraction of this dust (taking the highest calculated w/w concentration) would be 18 µg per day. If about one-third of the 10 restorations are made in anterior teeth (surface  $100 \text{ mm}^2$ ), then dentists are being exposed to approximately 20 µg of dust per day.

The German Agency for Occupational Safety<sup>48</sup> proposed 110–190  $\mu$ g/m<sup>3</sup> as the maximum acceptable nanodust concentration over a working day of 8 hours. For air uptake of 10 m<sup>3</sup> during an 8-hour working day (ISO 10993-17<sup>49</sup>), the daily acceptable intake of nanodust would be  $1,100-1,900$  µg. Background exposure is estimated to be 400 µg of nanoparticles without apparent harm<sup>50</sup>.

Although the present calculations are based on estimates, assumptions for exposure were very conservative and the calculated margins of safety are >20 to >100. This low exposure, together with the low cytotoxicity, indicates that no significant risk for dental personnel is expected. The same is true for patient exposure (of five fillings per year), being around 25 ng of nanodust per day.

It can be concluded that the uptake of nanoparticles after grinding/polishing of composites (and other restorative materials) and the health risks for the dental personnel and patients is low to negligible. However, no data are available for special vulnerable patient groups, like those with severe asthma or COPD.

# Ingestion of nanoparticles

Nanoparticles from wear are swallowed with the prime target organ being the intestines. The following calculations are based on 20 restorations (12 in molars and eight in premolars) with a total surface of 480 mm². Taking 50, 100 or 83 lm as annual vertical loss, this equates to exposure to about 133, 266 or 221 µg of particles per day, per patient. Taking the nano-fraction as outlined above [0.0004–0.0013% (w/w)], it can be assumed that only  $0.2-0.4$  µg are nanoparticles. The normal daily (total) uptake of nanoparticles is about 400  $\mu$ g per day<sup>50</sup>. Therefore, the uptake of nanoparticles abraded from restorations is likely to be low and the health risk in patients is considered to be acceptable.

Ingestion of nanoparticles is also assumed to be the major route of exposure during restoration removal. Assuming removal of five restorations per patient per year, less than 2 ug of nanoparticles per day are ingested. This calculation does not take into account the removal of particles through the high-vacuum suction, together with water cooling. Again, the expected exposure is very low, as is the additional particle-associated risk.

## Ti nanoparticles from dental implants

Titanium is one of the most biocompatible metallic materials as a result of its ability to form a stable and insoluble protective oxide layer  $(TiO<sub>2</sub>)$  on its surface<sup>51</sup>. Ti is preferentially used for endosseous dental  $implants<sup>51</sup>$  and the properties of Ti implants can be improved by using nanostructured Ti-containing particles or Ti nanoparticles  $(T_i-NPs)^{52}$ . However, a recent *in vitro* study<sup>53</sup> demonstrated a size-dependent cytotoxicity and DNA damage of Ti particles. Genotoxic effects of Ti particles have also been detected, such as induction of apoptosis in mesenchymal stem cells<sup>54</sup>. It was claimed that peri-implantitis can arise by exposure to  $TiO<sub>2</sub>$ , even in the absence of bacteria<sup>55</sup>. Furthermore, a previous postmortem study investigating metal particles released from implants showed bone marrow fibrosis<sup>38</sup>. In a clinical study,  $0.6\%$  of 1,500 patients were found to exhibit allergic reactions to  $Ti<sup>56</sup>$ 

The highest Ti content detected in human mandibular bone was  $37,700$  µg/kg of bone<sup>38</sup>. Assuming that all Ti in the bone is Ti nanoparticles and that 1 kg bone equals 1 l of fluid, a Ti nanoparticles concentration of 37 µg/ml can be calculated. The half-maximal effective concentration  $(EC_{50})$  for Ti nanoparticles in human cells is  $2,800 \text{ µg/ml}^{53}$ . Therefore, it is assumed that Ti nanoparticles released from dental implants might have no toxicologically clinical effects.

# Silver nanoparticles

Heinlaan et  $al$ .<sup>57</sup> described that AgNPs were very toxic to Daphnia magna (OECD202) (48-hour  $EC_{50}$ : 1–5.5  $\mu$ g of Ag/l), as well as to Danio rerio (OECD236) (96-hour EC<sub>50</sub>: 8.8–61 µg of Ag/l), embryos. These  $EC_{50}$  values are 10–100 times lower than the Ag(nano)particle concentrations measured after release from metallic implant coatings. There are also clinical problems associated with AgNPs, such as colour change<sup>58</sup> or impairment of the polymerization process of resin-based materials, which then leads to increased release of substances (e.g. monomers)<sup>59</sup>. The actual risk of the inclusion of AgNPs into resin-based composites is presently difficult to estimate. However, the potential of adverse biological effects of resinbased composites when adding AgNPs seems to be increased.

#### Risk for the environment

It can be assumed that particles from resin-based composites reach the environment and that included residual monomers will be released. However, in the 2014 EU report [Scientific Committee on Health and Environmental Risks  $(SCHER)|^{60}$  it is stated that the information available on the mercury (Hg)-free alternatives to amalgam does not allow a sound risk assessment for the environment to be performed.

#### CONCLUSIONS/RECOMMENDATIONS

Available data on possible adverse reactions derived from nanoparticles in dental materials or by processing dental materials dealing with additional particle-related risks are sparse and more research is  $n$ ecessary<sup>10</sup>.

In the dental laboratory, technicians are exposed to nanoparticles as dust, and must follow available relevant national/international safety regulations. In dental practice, virtually no exposure to nanoparticles occurs when handling unset materials. Dental personnel are mainly exposed to nanoparticle dust produced by grinding/polishing set dental materials, irrespective of the presence of nanoparticles in the material. The lungs are the prime target organ. Actual risk assessment has shown that for the materials used at present, the additional particle-associated health risk for dental personnel after inhalation of nanoparticles as dust is likely to be low. Although no data on the long-term exposure of dental personnel to (dental) nanoparticles are available, such personnel have been exposed to nanoparticles for many decades already and there are so far no indications for an increased rate of nonallergic lung diseases.

Patients are exposed to nanoparticle dust or debris, but to a much lesser extent than dental personnel. Actual risk assessment has shown that the particleassociated health risk of materials used at present, for patients for both inhalation of nanoparticles and ingestion from wear, is likely to be low. Available information is limited, especially concerning the influence of dental material nanoparticles on special vulnerable patient groups, such as those with asthma or COPD. A risk assessment for the environment is presently not possible because of lack of data.

In any case, the amount of dust generated should be kept to a minimum by properly sculpturing the restoration. Cooling with water spray and effective suction whenever possible, when grinding and polishing intra-orally, are recommended. Effective local ventilation at treatment areas is also recommended, as is the use of encapsulated powder/liquid systems. Protective measures, such as wearing a mask, may limit exposure of dental personnel to small particles.

Addition of AgNPs may increase toxicity of the materials. For patients with Ti implants, the general risk of Ti nanoparticles is likely to be  $low^{53}$ . Possible micromovements between implant and abutment should be avoided by ensuring a tight connection.

#### Acknowledgement

The authors would like to thank Dr Christof Högg for publication assistance. There was no financial support for this publication.

#### Conflict of interest

The authors declare no conflict of interest.

#### **REFERENCES**

- 1. ETPN Association. Nanomedicine European Nanotechnology Platform. 2017. Available from: [http://www.etp-nanomedicine.e](http://www.etp-nanomedicine.eu) [u](http://www.etp-nanomedicine.eu). Accessed on May 2017.
- 2. Chaudhry Q, Scotter M, Blackburn J et al. Applications and implications of nanotechnologies for the food sector. Food Addit Contam Part A Chem Anal Control Expo Risk Assess 2008 25: 241–258.
- 3. Kohlhuber M, Winterhalter R, Dietrich S et al. Nanomaterialien in Lebensmitteln und Verbraucherprodukten Anwendungsbereiche, Analytik, rechtliche Rahmenbedingungen. Bayerisches Landesamt für Gesundheit und Lebensmittelsicherheit (LGL); 2012.
- 4. Besinis A, De Peralta T, Tredwin CJ et al. Review of nanomaterials in dentistry: interactions with the oral microenvironment, clinical applications, hazards, and benefits. ACS Nano 2015 9: 2255–2289.
- 5. Rupf S, Berger H, Buchter A et al. Exposure of patient and dental staff to fine and ultrafine particles from scanning spray. Clin Oral Investig 2015 19: 823–830.
- 6. Schmalz G, Hickel R, van Landuyt KL et al. Nanoparticles in dentistry. Dent Mater 2017 33: 1298–1314.
- 7. European Commission. Definition of a nanomaterial. 2017. Available from: [http://ec.europa.eu/environment/chemicals/nan](http://ec.europa.eu/environment/chemicals/nanotech/faq/definition_en.htm) [otech/faq/definition\\_en.htm.](http://ec.europa.eu/environment/chemicals/nanotech/faq/definition_en.htm) Accessed on May 2017.
- 8. ISO/TR 10993-22:2016 Biological evaluation of medical devices - Part 22: Guidance on nanomaterials. International Organization for Standardization.
- 9. ISO/TS 80004-1:2010 Nanotechnologies Vocabulary Part 1: Core terms. International Organization for Standardization.
- 10. Scientific Committee on Emerging and Newly Identified Health Risks (SCENIHR). Opinion on the guidance on the determination of potential health effects of nanomaterials used in medical devices. European Commission; 2015.
- 11. Ausschuss für Gefahrstoffe (AGS). Technische Regeln für Gefahrstoffe (TRGS) Arbeitsplatzgrenzwerte 900. Gemeinsamen Ministerialblatt (GMBl) 2017 20: 368–370.
- 12. Moghimi SM, Hunter AC, Murray JC. Long-circulating and target-specific nanoparticles: theory to practice. Pharmacol Rev 2001 53: 283–318.
- 13. Carriere M, Sauvaigo S, Douki T et al. Impact of nanoparticles on DNA repair processes: current knowledge and working hypotheses. Mutagenesis 2017 32: 203–213.
- 14. Li Y, Boraschi D. Endotoxin contamination: a key element in the interpretation of nanosafety studies. Nanomedicine (Lond) 2016 11: 269–287.

Schmalz et al.

- 15. Suzui M, Futakuchi M, Fukamachi K et al. Multiwalled carbon nanotubes intratracheally instilled into the rat lung induce development of pleural malignant mesothelioma and lung tumors. Cancer Sci 2016 107: 924–935.
- 16. IARC Working Group. IARC Monographs on the Evaluation of Carcinogenic Risks to Humans; volume 111 - Some Nanomaterials and some Fibres. Lyon, France: International Agency for Research on Cancer (IARC); 2017.
- 17. MacNee W, Donaldson K. Mechanism of lung injury caused by PM10 and ultrafine particles with special reference to COPD. Eur Respir J Suppl 2003 40: 47s-51s.
- 18. Roller M. Carcinogenicity of inhaled nanoparticles. Inhal Toxicol 2009 21(Suppl 1): 144–157.
- 19. Seaton A, MacNee W, Donaldson K et al. Particulate air pollution and acute health effects. Lancet 1995 345: 176–178.
- 20. Steerenberg PA, van Amelsvoort L, Lovik M et al. Relation between sources of particulate air pollution and biological effect parameters in samples from four European cities: an exploratory study. Inhal Toxicol 2006 18: 333–346.
- 21. Albers HF. Tooth-Colored Restoratives: Principles and techniques, 9th ed. London, UK: BC Decker Inc; 2002.
- 22. Camilleri J, Pitt Ford TR. Mineral trioxide aggregate: a review of the constituents and biological properties of the material. Int Endod J 2006 39: 747–754.
- 23. Kawaguchi H, Ogawa T, Shirakawa M et al. Ultrastructural and ultracytochemical characteristics of multinucleated cells after hydroxyapatite implantation into rat periodontal tissue. J Periodontal Res 1992 27: 48–54.
- 24. Bogdan A, Buckett MI, Japuntich DA. Nano-sized aerosol classification, collection and analysis–method development using dental composite materials. *J Occup Environ Hyg* 2014 11: 415–426.
- 25. Occupational Safety and Health Administration (OSHA), U.S. Department of Labor. Laboratory Safety Guidance - OSHA 3404-11R; 2011. Available from:<http://www.osha.gov>. Accessed 1 November 2017.
- 26. Heumann T, Dermann K. On the existence of a transverse pressure in capillaries filled with liquid, Part I. Z Metallkde 1979 70: 281–285.
- 27. Heumann T, Dermann K. On the existence of a transverse pressure in capillaries filled with liquid, Part II. Z Metallkde 1979 70: 286–292.
- 28. Van Landuyt KL, Yoshihara K, Geebelen B et al. Should we be concerned about composite (nano-)dust? Dent Mater 2012 28: 1162–1170.
- 29. Van Landuyt KL, Hellack B, Van Meerbeek B et al. Nanoparticle release from dental composites. Acta Biomater 2014 10: 365–374.
- 30. Arbeitsgemeinschaft der Deutschen Zahnärztekammern<br>(BZÄK). Statistisches Jahrbuch 2015/2016. Bun-(BZAK). € Statistisches Jahrbuch 2015/2016. Bundeszahnärztekammer; 2016.
- 31. Heintze SD. How to qualify and validate wear simulation devices and methods. Dent Mater 2006 22: 712–734.
- 32. Palaniappan S, Elsen L, Lijnen I et al. Three-year randomised clinical trial to evaluate the clinical performance, quantitative and qualitative wear patterns of hybrid composite restorations. Clin Oral Investig 2010 14: 441–458.
- 33. Folwaczny M, Mehl A, Kunzelmann KH et al. Determination of changes on tooth-colored cervical restorations in vivo using a three-dimensional laser scanning device. Eur J Oral Sci 2000 108: 233–238.
- 34. Castilho GA, Martins MD, Macedo WA. Surface characterization of titanium based dental implants. Braz J Phys 2006 36: 1004–1008.
- 35. Franchi M, Bacchelli B, Martini D et al. Early detachment of titanium particles from various different surfaces of endosseous dental implants. Biomaterials 2004 25: 2239–2246.
- 36. Flatebo RS, Hol PJ, Leknes KN et al. Mapping of titanium particles in peri-implant oral mucosa by laser ablation inductively coupled plasma mass spectrometry and high-resolution optical darkfield microscopy. J Oral Pathol Med 2011 40:  $412 - 420$ .
- 37. Jacobs JJ, Gilbert JL, Urban RM. Current concepts review-corrosion of metal orthopaedic implants. J Bone Joint Surg 1998 80: 268–282.
- 38. He X, Reichl FX, Wang Y et al. Analysis of titanium and other metals in human jawbones with dental implants - A case series study. Dent Mater 2016 32: 1042–1051.
- 39. Yamamoto K, Ohashi S, Aono M et al. Antibacterial activity of silver ions implanted in SiO2 filler on oral streptococci. Dent Mater 1996 12: 227–229.
- 40. Gosau M, Haupt M, Thude S et al. Antimicrobial effect and biocompatibility of novel metallic nanocrystalline implant coatings. J Biomed Mater Res B Appl Biomater 2016 104: 1571– 1579.
- 41. ISO 11143:2008 Dentistry Amalgam separators. International Organization for Standardization.
- 42. Sevkusic M, Schuster L, Rothmund L et al. The elution and breakdown behavior of constituents from various light-cured composites. Dent Mater 2014 30: 619–631.
- 43. Cokic SM, Duca RC, Godderis L et al. Release of monomers from composite dust. J Dent 2017 60: 56–62.
- 44. Klaassen CD. Casarett and Doull's Toxicology: The Basic Science of Poisons, 7th ed. USA: The McGraw-Hill Companies, Inc.; 2008.
- 45. Van Landuyt KL, Cokic SM, Asbach C et al. Interaction of rat alveolar macrophages with dental composite dust. Part Fibre Toxicol 2016 13: 62.
- 46. Cokic SM, Hoet P, Godderis L et al. Cytotoxic effects of composite dust on human bronchial epithelial cells. Dent Mater 2016 32: 1482–1491.
- 47. Bradna P, Ondrackova L, Zdimal V et al. Detection of nanoparticles released at finishing of dental composite materials. Monatshefte für Chemie - Chemical Monthly 2017 148: 531–537.
- 48. Bundesanstalt für Arbeitsschutz und Arbeitsmedizin (BAuA), Ausschuss für Gefahrstoffe (AGS) Geschäftsführung. Beurteilungsmaßstab NanoGBS - Beurteilungsmaßstab für technisch gezielt hergestellte ultrafeine Stäube aus alveolengängigen granulären biobeständigen Stäuben ohne bekannte signifikante spezifische Toxizität (nanoskalige GBS) (A-Staub). 2015. Available from: [http://www.baua.de.](http://www.baua.de) Accessed 1 November 2017.
- 49. ISO 10993-17:2002 Biological evaluation of medical devices - Part 17: Establishment of allowable limits for leachable substances, Annex A. International Organization for Standardization.
- 50. Terzano C, Di Stefano F, Conti V et al. Air pollution ultrafine particles: toxicity beyond the lung. Eur Rev Med Pharmacol Sci 2010 14: 809–821.
- 51. Elias C, Lima J, Valiev R et al. Biomedical applications of titanium and its alloys. JOM 2008 60: 46–49.
- 52. Valiev RZ, Semenova IP, Latysh VV et al. Nanostructured titanium for biomedical applications. Adv Eng Mater 2008 10: B15–B17.
- 53. He X, Hartlieb E, Rothmund L et al. Intracellular uptake and toxicity of three different Titanium particles. Dent Mater 2015 31: 734–744.
- 54. Wang ML, Tuli R, Manner PA et al. Direct and indirect induction of apoptosis in human mesenchymal stem cells in response to titanium particles. J Orthop Res 2003 21: 697–707.
- 55. Pettersson M, Kelk P, Belibasakis GN et al. Titanium ions form particles that activate and execute interleukin-1beta release

#### Scientific Update on Nanoparticles in Dentistry

from lipopolysaccharide-primed macrophages. J Periodontal Res 2017 52: 21–32.

- 56. Sicilia A, Cuesta S, Coma G et al. Titanium allergy in dental implant patients: a clinical study on 1500 consecutive patients. Clin Oral Implants Res 2008 19: 823–835.
- 57. Heinlaan M, Muna M, Knobel M et al. Natural water as the test medium for Ag and CuO nanoparticle hazard evaluation: an interlaboratory case study. Environ Pollut 2016 216: 689–699.
- 58. Chladek G, Mertas A, Barszczewska-Rybarek I et al. Antifungal activity of denture soft lining material modified by silver nanoparticles-a pilot study. Int J Mol Sci 2011 12: 4735–4744.
- 59. Durner J, Stojanovic M, Urcan E et al. Influence of silver nanoparticles on monomer elution from light-cured composites. Dent Mater 2011 27: 631–636.

60. Scientific Committee on Health and Environmental Risks (SCHER). Opinion on the environmental risks and indirect health effects of mercury from dental amalgam (update 2014). European Commission; 2014.

> Correspondence to: Prof. Dr Franz-Xaver Reichl, Department of Conservative Dentistry and Periodontology, University Hospital, LMU Munich, Goethestr. 70, 80336 Munich,Germany. Email: reichl@lmu.de