

Nanozyme and Stimulated Fluorescent Cu-Based Metal–Organic Frameworks (Cu-MOFs) Functionalized with Engineered Aptamers as a Molecular Recognition Element for Thrombin Detection in the Plasma of COVID-19 Patients

Gona K. Ali and Khalid M. Omer*

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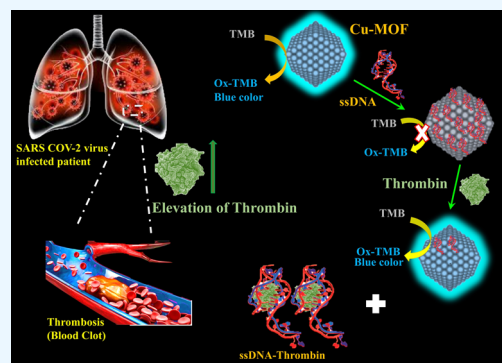
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ABSTRACT: An essential tool in the management and control of the COVID-19 pandemic is the development of a fast, selective, sensitive, and inexpensive COVID-19 biomarkers detection method. Herein, an ultrasensitive and label-free biosensing strategy was described for the colorimetric and fluorimetric detection of thrombin. A dual-mode aptasensing method based on integrating engineered ssDNA with a stimulated fluorescent enzyme-mimetic copper-based metal–organic framework (Cu-MOF) as a molecular recognition element for thrombin was investigated. Cu-MOFs displayed stimulated fluorescence and enzyme-mimetic peroxidase activities that oxidize the chromogenic colorless substance TMB to blue-colored oxTMB. The thrombin-based aptamer (ssDNA) can be immobilized on the Cu-MOF surface to form a functionalized composite, ssDNA/MOF, and quench the stimulated fluorescence emission and the enzymatic activity of the Cu-MOF. Later, addition of thrombin recovers the fluorescence and enzymatic activity of the MOF. Thus, a turn-on colorimetry/fluorimetry aptasensing probe was designed for the detection of thrombin. Based on colorimetric assay, 350 pM was recorded as the lower limit of detection (LOD), while based on the fluorescence mode, 110 fM was recorded as the LOD (when $S/N = 3$). The label-free aptasensing probe was used successfully for the detection of thrombin in COVID-19 patients with satisfactory recoveries, 95–98%. Since the detection time of our aptasensor is relatively rapid (45 min) and due to the low-cost precursors and easy-to-operate characteristics, we believe that it has great potential to be used in point-of-care testing (POCT).



1. INTRODUCTION

Severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2) is an infectious and deadly coronavirus that has killed millions around the world; it was first reported in China in 2019; then, COVID-19 soon became a pandemic illness, and it is now a severe threat to global health.^{1–4} The most prognostic parameters of severe COVID-19 are lymphopenia, thrombocytopenia, leukocytosis, CRP, PCT, LDH, AST, ALT, and D-dimer.^{5,6} Excessive inflammation, hypoxia, immobility, and microvascular damage may all be reasons for thrombosis.^{7–11} In COVID-19 patients, a high thrombin generation capacity that remains within normal values despite heparin therapy and hypofibrinolysis are observed.^{12,13} The coagulopathy linked to coronavirus disease 2019 (COVID-19) is characterized by a prothrombotic condition.¹⁴ Patients with COVID-19 showed high levels of thrombin generation (TG), when they were diagnosed. Intermediate subtherapeutic thromboprophylaxis has reduced TG more successfully.¹⁵

In the literature, there are many methods and techniques to detect thrombin, such as fluorescence, colorimetric, and

electrochemical. Techniques such as immunoassay-based and radioassay-based methods are in use as a benchmark.^{16,17} However, the aforementioned methods are time-consuming, high-cost, and affected by various pHs and temperatures.¹⁸ For instance, immunoassay uses natural antibodies, which are temperature-dependent and suffer from denaturation and a short shelf-life.^{16,19,20} Thus, one should think about stable, robust, selective, and sensitive alternatives with low-cost precursors.

Aptamers are oligonucleotides, single-stranded DNA (ssDNA) or RNA, that were created using the systematic evolution of ligands by exponential enrichment (SELEX) in vitro selection and polymerase chain reaction technique.^{21–25}

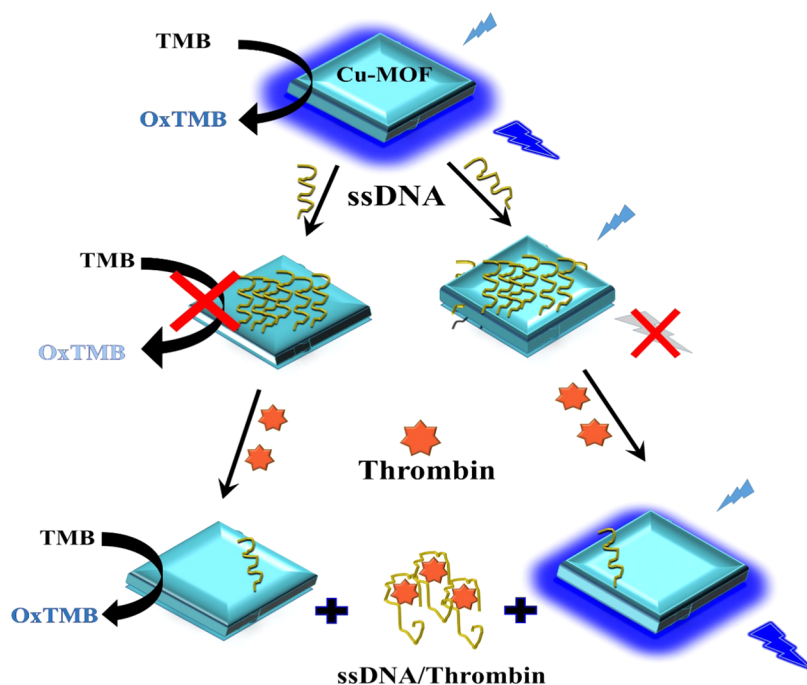
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Scheme 1. Preparation and Detection Mechanisms of Cu-MOF Integrated with the ssDNA Biosensor for Thrombin Detection



They have high affinity and specificity for their targets. As a result, aptamers can be utilized as artificial antibodies.^{26,27} They have unique properties that make them highly promising for biosensing applications, such as high specificity, a wide range of targets, easy synthesis, nonimmunogenicity, stability under various pHs and temperatures, and low cost. Different types of targets can be bound to aptamers, such as organic dyes, bacteria, biomarkers, and proteins.²⁸ This binding is due to changing spatial conformation, stacking aromatic ring interactions, electrostatic forces, and/or hydrogen bonding.^{29,30}

Metal–organic frameworks (MOFs) are crystalline nano-materials made up of metal ions and organic ligands.^{31–33} MOFs are widely used in a variety of fields, including separation,³⁴ gas adsorption,³⁵ energy storage,³⁶ and catalysis,³⁷ due to their huge specific areas, simple synthesis procedures, plentiful functional groups, enzyme-mimetic behavior, and chemical stability.^{38,39} Because of these benefits, MOFs are particularly well-suited for the construction of biosensors with a wide range of applications, particularly in the biomedical domains.^{40–46} Recently, researchers are interested in integrating nucleic acids with MOFs for biosensing.^{47–49} Moreover, the enzyme-mimetic activity or fluorescence emission of some MOFs allows for using this entity in colorimetric or fluorescence assay.^{50–54} To this end, rational selection of MOFs with enzyme-mimetic behavior and fluorescence emission gives the best route toward functionalization with a suitable aptamer.

Aptamer-functionalized MOFs for the detection of thrombin have been reported in the literature. Wang et al.⁵⁵ have prepared and used Fe-MIL-88A for colorimetric detection of thrombin with 10 nM as a LOD. Due to the peroxidase activity of Fe-MIL-88A, they just used this colorimetric property for the detection strategy. Others such as Zhang et al.⁵⁶ used an electrochemical method for aptamer-functionalized Zr-based MOFs for the detection of thrombin. They obtained 0.37 pg mL⁻¹ as a LOD. To this end, we think of a dual-mode sensing

strategy combined with aptamers for the detection of thrombin.

In the present work, Cu-MOFs have been prepared that have both stimulated fluorescence and mimetic peroxidase-like enzymatic activity. An engineered thrombin-binding aptamer (ssDNA) has been integrated with Cu-MOFs to combine the mimetic behavior and fluorescence of the MOFs with high affinity of the ssDNA toward thrombin detection (Scheme 1). Combining an aptamer platform with MOFs will enhance the affinity and sensitivity of thrombin detection. Femtomolar detection of thrombin was achieved using our low-cost, robust, and highly stable aptasensor.

2. EXPERIMENTAL SECTION

2.1. Chemicals. A thrombin amine aptamer (ssDNA) was synthesized and purified by Bioneer Co., Ltd. (Daejeon, south Korea) with sequences (5-(NH₂)-(CH₂)₆-CCA-TCT-CCA-CTT-GGT-TGG-TGT-GGT-TGG-3). Dimethylformamide (DMF), 3, 3', 5, 5'-tetramethylbenzidine (TMB), terephthalic acid (TA), and thrombin protein extracted from human plasma were all purchased from Merck-Sigma-Aldrich (Baden-Württemberg, Germany) and used as received. Cu(NO₃)₂·3H₂O and hydrogen peroxide (H₂O₂) 30% were purchased from Biochem chemopharma Co., Ltd. (Biochem, ZA Cosne sur Loire, France). TE buffer (Tris-EDTA, pH 8.0) was purchased from EMB corporation (EMB Co.). Phosphate buffer saline (pH 7) was ordered from (CDH Co., Ltd. Delhi, India).

2.2. Instruments. Field emission scanning electron microscopy (FE-SEM) was used for taking the image of the MOF particles (Germany ZEISS Gemini SEM). UV–vis absorption spectra were recorded on a Cary 60 Spectrophotometer (Agilent technologies). Fluorescence measurements (PL) were recorded on a Cary Eclipse fluorescence Spectrophotometer (Agilent Technologies).

2.3. MOF Synthesis. A Cu-metal–organic framework (Cu-MOF) was prepared based on reports in the literature with

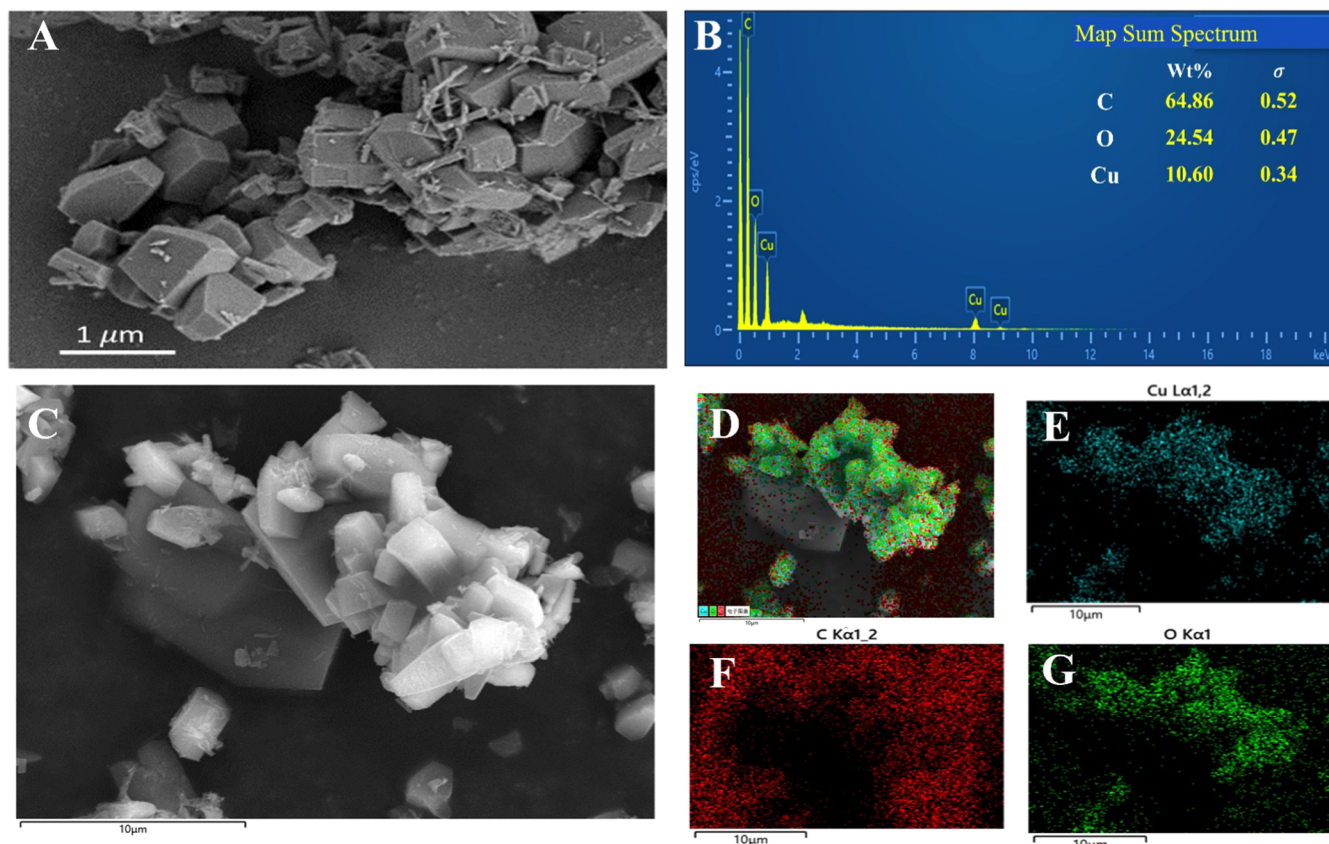


Figure 1. (A) FE-SEM of the Cu-MOF; (B) EDX mapping spectra, and (C–G) EDX distribution of the Cu-MOF at the 10 μm scale bar.

minor modifications.⁵⁷ In brief, 0.97 g of $\text{Cu}(\text{NO}_3)_2 \cdot 3\text{H}_2\text{O}$ and 0.67 g of TA (terephthalic acid) were first dissolved in 20 mL of DMF. The resulting solution was then transferred to a 50 mL Teflon-lined stainless-steel autoclave for reaction at 150 °C for 3 h. Blue crystals were collected by centrifugation and rinsed with adequate ethanol and deionized water alternately. To prepare a stock solution ($100 \mu\text{g}\cdot\text{mL}^{-1}$) of Cu MOF in water, 10 mg of the Cu-MOF was dispersed in 100 mL of deionized water.

2.4. Colorimetric Assay. For the colorimetric assay protocol, 150 μL of $100 \mu\text{g}\cdot\text{mL}^{-1}$ Cu-MOF solution was mixed with 100 μL of ssDNA solution ($1.6 \mu\text{M}$) and then incubated for 5 h at 35 °C. The ssDNA with the presence of different amounts, 0.0–7.0 nM, of thrombin was stirred for 15 min in PBS buffer, followed by addition of 150 μL ($100 \mu\text{g}\cdot\text{mL}^{-1}$) of the Cu-MOF to it with stirring for 5 h. Peroxidase enzymatic activity was measured by taking 100 μL from every solution mixed with 100 μL of 5 mM TMB as a substrate with 100 μL of 30 mM H_2O_2 solution; then, the volume was calibrated to 1.0 mL using a buffer, pH 4. The color change was observed and recorded after 45 min.

2.5. Fluorimetric Assay. For the fluorescence-based assay, 150 μL of $100 \mu\text{g}\cdot\text{mL}^{-1}$ Cu-MOF solution was mixed with 100 μL of ssDNA ($1.6 \mu\text{M}$) and then stirred for 5 h at 35 °C. Recovery response was obtained with addition of different amounts, 0.0–7.0 nM, of thrombin and stirring for 15 min in PBS buffer, with 100 μL of 30 mM H_2O_2 solution added and then incubated for 8 h in room temperature. The fluorescence spectra were recorded at 320 nm excitation wavelength.

2.6. Stirring Time Effect of Cu-MOF/ssDNA. This study has been done by mixing $15 \text{ ng}\cdot\text{mL}^{-1}$ MOF with 160 nM

aptamer in PBS; then, 100 μL has been taken from the mixture solution in different periods of time, 0.5, 1, 3, 5, and 24 h; then, 0.5 mM TMB substrate was added and 100 μL of 30 mM H_2O_2 solution was added; the volume was calibrated to 1 mL using a buffer (pH 4); then, the color change was observed and recorded after 45 min.

3. RESULTS AND DISCUSSION

3.1. Characterizations. Based on FE-SEM, the Cu-MOF product forms polydisperse decahedral crystals in the micrometer-to-sub-micrometer range (Figure 1A). EDS elemental mapping and spectra were characterized and are shown in Figure 1B–G. As one can notice, the crystals are made of C, O, and Cu elements, confirming the formation of the Cu-MOF.

3.2. Enzymatic Activity and Stimulated Fluorescence of the Cu-MOF. The Cu-MOF showed a peroxidase-mimetic enzyme activity with the appearance of a clear blue color via oxidation of the colorless TMB substrate to blue oxidized TMB in the presence of H_2O_2 . When amine-terminated ssDNA was added, it adsorbed on the surface of Cu-MOFs via the π – π interaction, and the enzymatic activity of the Cu-MOF was inhibited.⁵⁸ However, when thrombin protein was added, the enzymatic activity of the Cu-MOF was shown again and the blue color recovered due to the selective binding of the ssDNA with the thrombin protein (Figure 2A). The high affinity of NH_2 -ssDNA binding with thrombin led to a sensitive colorimetric probe for the detection of the thrombin protein. Interestingly, due to the stimulated fluorescence of Cu-MOFs with H_2O_2 ($\lambda_{\text{emission}}$ 410 when $\lambda_{\text{excitation}}$ at 320 nm), the emission of Cu-MOFs was quenched after adding thrombin ssDNA and recovered after addition of the thrombin

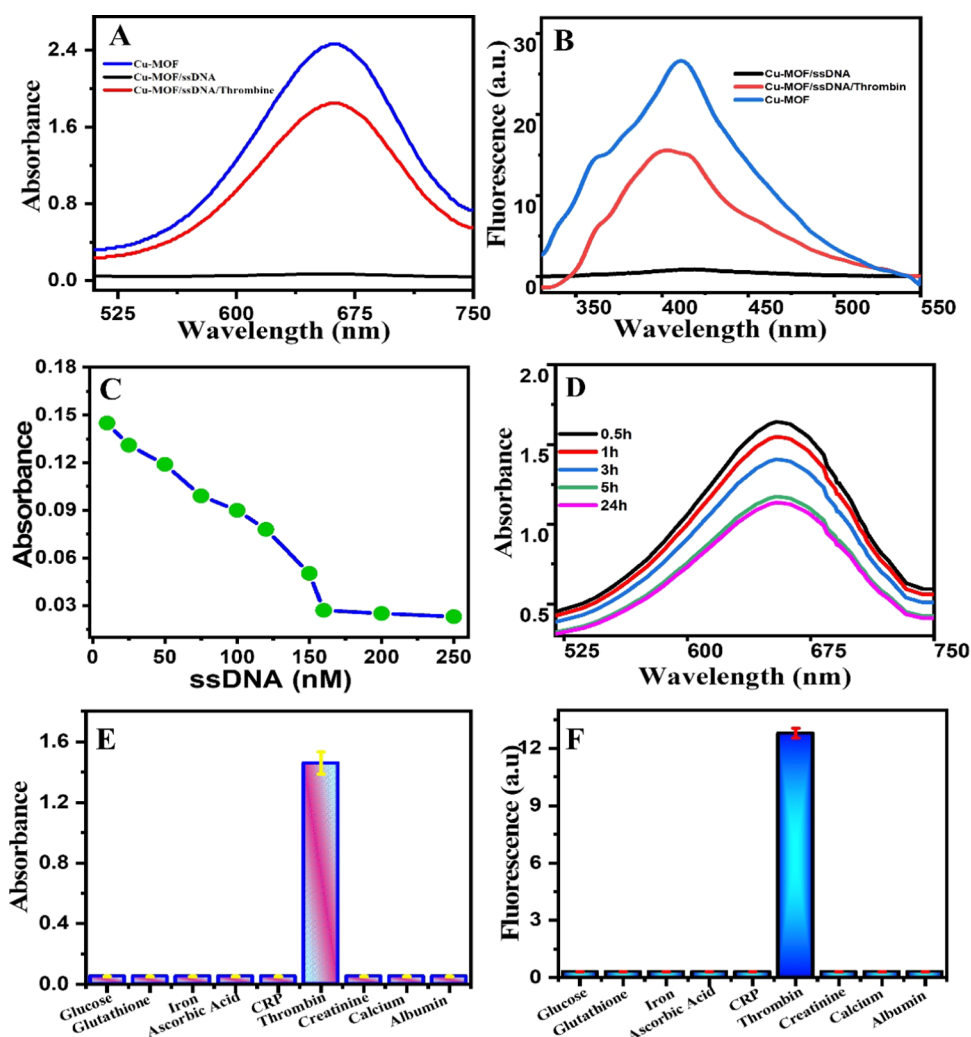


Figure 2. Aptamer-based assay responses on the Cu-MOF after addition of thrombin. (A) Colorimetry-based assay. (B) Fluorescence-based assay. (C) Optimum ssDNA concentration. (D) Stirring time effect on the adsorption capacity of the ssDNA on the Cu-MOF ($15 \text{ ng}\cdot\text{mL}^{-1}$), ssDNA (160 nM). (E, F) Selectivity study of the proposed biosensor, Cu-MOF ($15 \text{ ng}\cdot\text{mL}^{-1}$), ssDNA (160 nM), and thrombin (5 nM), and the concentrations of other interferences are all 500 nM . (E) Colorimetric assay and (F) fluorescence assay response.

protein. Thus, we designed a fluorescence-based probe in parallel with colorimetric assay exploiting the fluorescence and enzymatic behaviors of the Cu-MOFs (Figure 2B).

3.3. Optimizations. To obtain the best catalytic activity, variable experimental parameters were optimized, such as stirring time and ssDNA concentrations. Figure 2C shows the effect of stirring time of the Cu-MOF with ssDNA on the enzymatic activity. With increasing time of stirring, the enzymatic activity of the Cu-MOF decreases gradually until 5 h, due to adsorption of ssDNA on the MOF surface. Beyond 5 h and until 24 h, there were very slight changes in the enzymatic activity, which indicates that 5 h is the optimum time for stirring. The concentration of ssDNA was also optimized as shown in Figure 2D. At 160 nM , the whole catalytic activity of the Cu-MOF was totally inhibited, suggesting that 160 nM is the best concentration of ssDNA to start with for an off–on experiment.

3.4. Selectivity Study. To evaluate the selectivity of our aptamer-based sensor, common ions, biomolecules, and proteins that usually coexist with thrombin in the serum matrix were tested. Interferences such as glucose, glutathione, ascorbic acid, iron, C-reactive protein (CRP), creatinine,

albumin, and calcium were selected for this study. The concentration of all of them in selective experiments was 100 times that of thrombin. As shown in Figure 2E,F, the corresponding absorbance and fluorescence intensity of thrombin were much greater than those of the other proteins and metals. These results indicate that the Cu-MOF/ssDNA sensor has high selectivity for the detection of thrombin, which makes the Cu-MOF/ssDNA sensor a good probe for the real serum fluid sample.

4. DUAL-MODE COLORIMETRIC AND FLUOROMETRIC ASSAY

In the colorimetric assay, the intensity of blue color increased as the amount of thrombin increased (Figure 3A) due to removal of the immobilized ssDNA on the surface of the Cu-MOF. Hence, the enzymatic activity will be restored. A linear relationship was constructed from 0.7 to 7.0 nM (Figure 3B) with a lower limit of detection (LOD) as small as 360 pM being calculated. Regarding the fluorescence-based assay, different concentrations of thrombin were added to the Cu-MOF/ssDNA solutions and the fluorescence recovery was observed, as shown in Figure 3C. A dynamic linear relationship

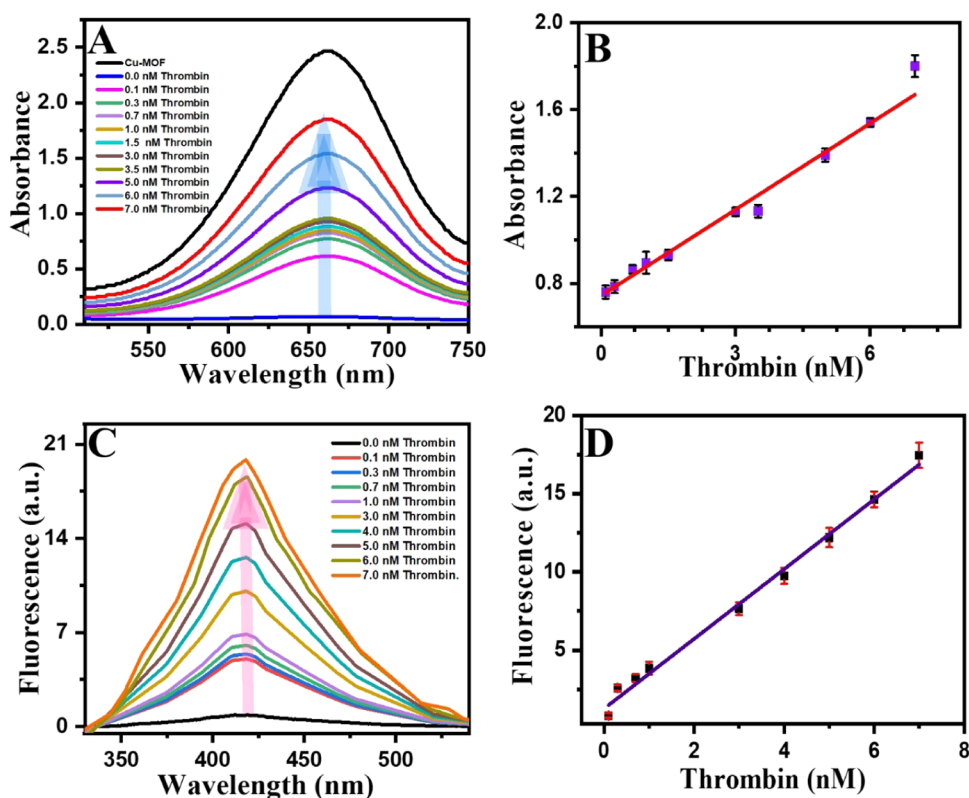


Figure 3. Thrombin concentration-dependent response profiles; (A, C) Colorimetric and fluorescence spectra, respectively. (B, D) Calibration curves of thrombin using colorimetry and fluorescent aptamer-based assays, respectively. Error bars are for $n = 3$.

was obtained as the thrombin concentration increased ($R^2 = 0.998$), and a LOD as small as 110 fM was calculated (Figure 3D). The LOD and LOQ were determined according to $S/N = 3$ and $S/N = 10$ criteria, respectively (S was estimated to SD ($n = 10$) obtained from the current intensity of the lowest concentration of thrombin in the calibration 0.7 nM). Such a small LOD is attributed to the synergistic effect of the luminescence of the Cu-MOF with high affinity of ssDNA toward thrombin. Both LODs are much lower than the normal level of thrombin in normal adults and in patients with COVID-19. Our proposed biochemical sensor showed excellent LODs and a dynamic range in both assays, colorimetric and fluorimetry modes. Table 1 shows a comparison between common MOF-based methods for the detection of thrombin. As one can notice, our results showed very low LODs compared with those of others.

In general, fluorimetric assays are more sensitive and selective than colorimetric assays. Dynamic ranges are broader and LODs are lower in fluorescence-based assays. Thus, fluorescence-based methods are more favorable for trace

analysis. However, colorimetric-based assays are simple requiring low-cost instruments for the analysis.

5. APPLICATIONS

Plasma samples of patients with COVID-19 were taken for thrombin analysis from Shahid-Hemn Hospital (Sleman City, Kurdistan Region, Iraq). The plasma sample collection was done following the guidelines of the ethical committee at the hospital, and the patients were informed and before collecting blood, permission was acquired. The samples were collected from the emergency and intensive care units of the hospital. Plasma samples were 1000-fold diluted with double-deionized water (to convert the thrombin range to our biosensor's linearity range) and then spiked with 1.0 and 3.5 nM standard thrombin solution. Table 2 shows various colorimetric and fluorescence results using our proposed biosensor. Spike recoveries were very satisfactory, ranging from 86 to 94% for colorimetric assay and from 88 to 98% for fluorescence assay. Thus, a quantitative thrombin COVID-19 biomarker in real serum was achieved. In one word, Cu-MOF/ssDNA already demonstrated its utility in clinical diagnosis as a novel biochemical assay. For the intra-assay, the precision (repeatability) reached a RSD of 4% ($n = 3$) for the same day, and the interassay precession (reproducibility) reached 6% ($n = 3$) for different days.

6. CONCLUSIONS

A dual-mode and label-free aptasensor based on integration of ssDNA with a stimulated fluorescent peroxidase Cu-MOF was developed for the detection of thrombin. The biosensor enabled femtomolar detection of thrombin based on the fluorescence mode and picomolar detection based on the

Table 1. MOF-Based Aptasensors Using MOFs as Signal Probes

type of MOFs	LOD	detection method	references
MIL-101	15 pM	fluorescence assay	59
Zr-NMOF	0.40 $\mu\text{g}\cdot\text{mL}^{-1}$	electrochemical	56
ZIF-8	0.8 fM	electrochemical	60
Fe-MIL-88A	10 nM	colorimetric	55
Cu-MOF	110 fM	fluorescence	this work
Cu-MOF	360 pM	colorimetric	this work

Table 2. Various Colorimetric and Fluorescence Recoveries with RSDs, Number of Replications, $n = 3$

sample	unspiked (nM)	added (nM)	spiked (nM)	recovery %	RSD %
Colorimetric Assay					
1	1.15 ± 0.02	1	2.01 ± 0.01	86.00 ± 1.52	1.71
	1.64 ± 0.021	3.5	4.94 ± 0.02	94.35 ± 1.03	1.33
2	3.03 ± 0.01	1	3.91 ± 0.03	88.00 ± 2.07	0.51
	5.35 ± 0.20	3.5	8.64 ± 0.02	94.08 ± 1.95	0.34
Fluorometric Assay					
1	1.17 ± 0.02	1	2.10 ± 0.01	93.00 ± 2.16	0.72
	1.40 ± 0.02	3.5	4.50 ± 0.03	88.00 ± 1.38	0.33
2	2.95 ± 0.02	1	3.89 ± 0.02	94.20 ± 2.46	1.53
	3.21 ± 0.01	3.5	6.65 ± 0.07	98.34 ± 2.63	0.22

colorimetry mode. The detection limits by both modes, colorimetry and fluorimetry, were much lower than the physiological thrombin level in human serum. The colorimetric and fluorometric assays were successfully evaluated, and satisfactory results were obtained for the detection of thrombin in the serum of COVID-19 patients. This label-free aptasensor will pave the way toward designing more functionality-sensitive fluorescent nanozymes.

AUTHOR INFORMATION

Corresponding Author

Khalid M. Omer – Department of Chemistry, College of Science and Center for Biomedical Analysis, Department of Chemistry, College of Science, University of Sulaimani, Slemani City 46002 Kurdistan Region, Iraq; orcid.org/0000-0002-6866-4116; Email: khalid.omer@univsul.edu.iq

Author

Gona K. Ali – Department of Chemistry, College of Science, University of Sulaimani, Slemani City 46002 Kurdistan Region, Iraq

Complete contact information is available at: <https://pubs.acs.org/10.1021/acsomega.2c05232>

Notes

The authors declare no competing financial interest.

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