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## Blood Pressure Responses During Exercise: Physiological Correlates and Clinical Implications

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### Abstract

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Supplemental Material

- Supplemental Methods
- Tables S1–S4

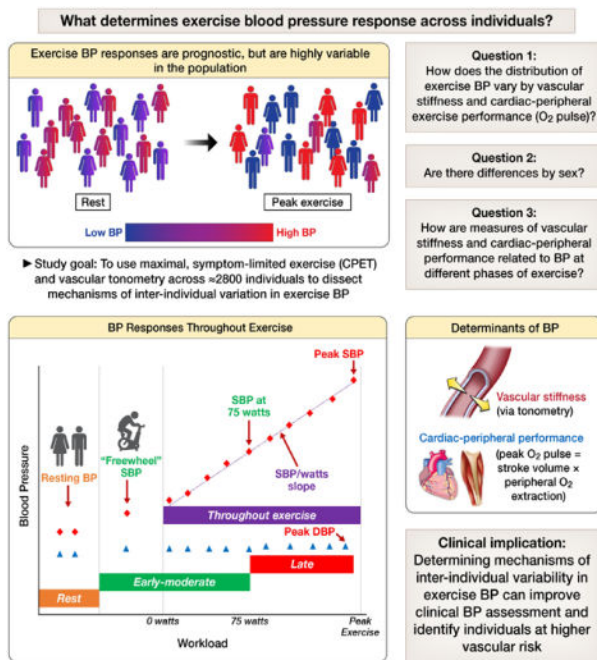
**Background:** Abnormal blood pressure (BP) responses to exercise can predict adverse cardiovascular outcomes, but their optimal measurement and definitions are poorly understood. We combined frequently sampled BP during cardiopulmonary exercise testing (CPET) with vascular stiffness assessment to parse cardiac and vascular components of exercise BP.

**Methods:** CPET with BP measured every two minutes and resting vascular tonometry were performed in 2858 Framingham Heart Study (FHS) participants. Linear regression was used to analyze sex-specific exercise BP patterns as a function of arterial stiffness (carotid-femoral pulse wave velocity; CFPWV) and cardiac-peripheral performance (defined by peak O<sub>2</sub> pulse).

**Results:** Our sample was balanced by sex (52% women) with mean age 54±9 years and 47% with hypertension. We observed variability in CFPWV and peak O<sub>2</sub> pulse across individuals with clinically defined exercise hypertension (peak systolic BP [SBP] in men ≥210 mm Hg; in women ≥190 mm Hg). Despite similar resting SBP and cardiometabolic profiles, individuals with higher peak O<sub>2</sub> pulse displayed higher peak SBP (P = 0.017) alongside higher fitness levels (P<0.001), suggesting that high peak exercise SBP in the context of high peak O<sub>2</sub> pulse may in fact be favorable. While both higher (favorable) O<sub>2</sub> pulse and higher (adverse) arterial stiffness were associated with greater peak SBP (P<0.0001 for both), the magnitude of association of CFPWV with peak SBP was higher in women (sex-CFPWV interaction P<0.0001). In sex-specific models, exercise SBP measures accounting for workload (e.g., SBP during unloaded exercise, SBP at 75 watts, and SBP/workload slope) were directly associated with the adverse features of greater arterial stiffness and lower peak O<sub>2</sub> pulse.

**Conclusions:** Higher peak exercise SBP reflects a complex trade-off between arterial stiffness and cardiac-peripheral performance that differs by sex. Studies of BP responses to exercise accounting for vascular and cardiac physiology may illuminate mechanisms of hypertension and clarify clinical interpretation of exercise BP.

## Graphical Abstract



Abbreviations: CPET, cardiopulmonary exercise testing; BP, blood pressure; SBP, systolic blood pressure; DBP, diastolic blood pressure. In the lower left panel, red diamonds represent systolic blood pressures and blue diamonds represent diastolic blood pressures.

**Subject terms:**

Epidemiology; exercise; hypertension; vascular stiffness

**INTRODUCTION**

Exercise testing unmasks abnormal physiological responses that are not apparent at rest. Over recent decades, exaggerated blood pressure (BP) responses to exercise have been studied in relation to elevated ambulatory BP<sup>1,2</sup> and incident hypertension and cardiovascular disease (CVD)<sup>3-8</sup>. A rapid rise in BP during exercise has been reported to reflect adverse vascular function<sup>4</sup>. However, despite their established relevance for disease prediction and pathophysiology, the use of exercise BP responses in clinical settings is limited by a lack of consensus on the definition of abnormal values<sup>9,10</sup>. While clinical exercise testing recommendations advocate for the use of peak systolic BP (SBP) threshold values ( 210 mm Hg in men, 190 mm Hg in women)<sup>9</sup>, individuals with high fitness levels may achieve higher peak systolic BP as a consequence of greater cardiac and skeletal muscle (peripheral) performance during exercise, which would not necessarily confer higher CVD risk<sup>11,12</sup>. To overcome these limitations, prior observational studies have largely relied on submaximal BP measures<sup>3-8</sup>, but protocols used to derive submaximal BP measures lack standardization. Moreover, prior studies have not examined the physiological contributions of cardiac and vascular function to exercise BP responses

in community-dwelling individuals, which are critical factors in determining the potential adverse cardiovascular consequences of abnormal exercise BP responses.

Here, we quantify BP responses during exercise in a large group of community-dwelling individuals who underwent maximum effort cardiopulmonary exercise testing (CPET) and evaluation of resting arterial stiffness (via tonometry). Combining CPET and vascular function testing allowed us to parse the relations of arterial stiffness and the cardiac-peripheral performance (represented by the peak O<sub>2</sub> pulse, composed of cardiac stroke volume × peripheral O<sub>2</sub> extraction) with BP changes with exercise. Given potential differences among men and women in the epidemiology, physiology, and clinical implications of BP regulation, we evaluated sex differences in exercise BP and its physiological correlates<sup>13,14</sup>. We hypothesized that a high peak exercise SBP would be observed in individuals with either higher arterial stiffness or higher cardiac-peripheral performance and that BP measures that incorporate workload would be more closely associated with adverse vascular characteristics and corresponding CVD risk factors (Graphical Abstract).

## METHODS

### Data sharing

Data used for the present investigation will be made available upon reasonable request. Framingham Heart Study (FHS) data are publicly available through the National Institutes of Health database of genotypes and phenotypes (<https://www.ncbi.nlm.nih.gov/gap/>).

### Study sample

Enrollment and characteristics of the FHS Generation Three, Omni Generation Two, and New Offspring Spouse cohorts have been reported<sup>15,16</sup>. Briefly, these three cohorts were enrolled together and attended their first study visit in 2002–2005 and their second study visit in 2008–2011. At the third study visit (2016–2019), 3117 of 3521 participants (89%) consented to undergo maximum effort CPET, as described<sup>17,18</sup>. Only information from the third study visit was used for the present investigation. From individuals who performed CPET, we excluded those with missing gas exchange measures (N=13), sub-maximum volitional effort (peak respiratory exchange ratio [RER] <1.05; N=139), missing tonometry measures (N=56), or missing blood pressure measures or covariates (N=51), yielding 2858 individuals eligible for the present analysis. Institutional Review Boards at Boston University and Massachusetts General Hospital approved all study protocols. All participants provided written informed consent.

### Exercise testing and BP quantification

CPET methods have been reported previously and are reproduced below for fidelity of scientific communication<sup>19</sup>. Participants were encouraged to fast overnight (including caffeinated beverages) prior to the CPET and arterial tonometry assessments and to not perform exercise prior to arrival at the study visit. CPET assessment and arterial tonometry were performed primarily during the mornings in the context of a ≈four-hour study visit<sup>19</sup>. Maximal effort CPET was performed on a cycle ergometer (Lode, Netherlands) using one

of two incremental ramp protocols (15 and 25 watts/minute). Participants were assigned to a specific ramp protocol by study staff based on an estimate of the predicted peak watts after considering age, sex, weight, height, and physical activity level<sup>19</sup>. The CPET assessment was conducted in a separate room with an adjustable air conditioner unit to avoid high temperatures during exercise. The exercise protocol consisted of three minutes of unloaded (“freewheel”) exercise followed by incremental ramp exercise. We obtained breath-by-breath gas exchange measures (MedGraphics, St. Paul, MN) throughout exercise<sup>17,18</sup>. Heart rate was monitored continuously during exercise with wireless electrocardiogram (ECG) equipment (Mortara, Milwaukee, WI). Peak oxygen uptake ( $\text{VO}_2$ ) was assessed as the highest 30-second median during the final minute of exercise and peak  $\text{O}_2$  pulse was calculated as the peak  $\text{VO}_2$  divided by the peak heart rate<sup>17,18</sup>. The percent predicted peak  $\text{VO}_2$  was calculated using the Wasserman-Hansen equations (equations included in the Supplemental Material)<sup>20</sup>. BP was measured every two minutes during exercise using a manual sphygmomanometer. Peak BP was measured immediately after termination of loaded exercise. BP measures used for this analysis include the following: (1) resting systolic and diastolic BP while the participant was seated on the cycle immediately prior to exercise (without a specified resting period); (2) unloaded exercise (turning the pedals with no added resistance) systolic BP (SBP), measured at minute 2 of the unloaded period; (3) SBP at 75 watts (occurring at minute 3 for the 25 watts/minute and minute 5 for the 15 watts/minute ramp protocols); and, (4) the “SBP/W slope”, calculated as (peak SBP – rest SBP)/peak workload. Participants were encouraged to exercise until exhaustion and testing was only stopped early for safety criteria (including chest pain with ECG changes, complex ectopy or high-degree atrioventricular block, symptomatic fall in SBP >20 mm Hg, marked exercise hypertension [SBP >240 mm Hg, diastolic BP (DBP) >120 mm Hg], oxygen desaturation, neurologic compromise, or at the discretion of the supervising clinician). To account for sex differences in workload, we multiplied the SBP/W slope by the sex-specific 1-standard deviation change in workload. Resting hypertension was defined, using the average of two measurements taken while the participant was seated in a chair following a five-minute period of rest prior to exercise, as SBP  $\geq$  130 mm Hg, DBP  $\geq$  80 mm Hg, or use of BP lowering medications<sup>21</sup>. An exaggerated SBP response to exercise was defined as systolic BP  $\geq$  210 in men and  $\geq$  190 mm Hg in women, consistent with published recommendations<sup>3,9,22</sup>.

### Vascular stiffness assessment

Applanation tonometry was performed on the right brachial, femoral, and carotid arteries on supine participants after a five-minute resting period using a custom transducer and data acquisition system (NIHem Hemodynamic Workstation, Cardiovascular Engineering, Inc., Norwood, MA), as previously described<sup>23</sup>. Arterial waveforms were signal-averaged using the electrocardiographic R wave as the fiducial point. Signal-averaged brachial artery waveforms were calibrated with systolic and diastolic auscultatory BP and integrated to derive mean arterial pressure. Carotid-femoral pulse wave velocity (CFPWV) was calculated as carotid-femoral transit distance (measured as the difference in body surface measurements from the suprasternal notch to the femoral and carotid sites) divided by carotid-femoral transit time delay (measured using the foot of the carotid and femoral waveforms). The augmentation index was calculated as the difference between the first

systolic inflection point and the peak waveform (i.e., the augmentation pressure) divided by the total pulse pressure and multiplied by 100. Central pressure and flow waveforms were used to perform time domain waveform separation analysis in order to obtain forward and backward pressure waveforms<sup>23</sup>. Forward wave amplitude was defined as the amplitude of the forward pressure wave. Characteristic impedance was calculated in the time domain by dividing the pressure increase by the flow increase up to 95% of peak flow<sup>23</sup>.

### Covariate assessment

Prevalent CVD was defined as a history of myocardial infarction, stroke, or heart failure, or by self-report of taking medications for heart failure, angina or chest pain, atrial fibrillation/heart rhythm abnormality, stroke, peripheral arterial disease, or claudication. Diabetes was defined by fasting blood glucose  $\geq 126$  mg/dL, non-fasting blood glucose  $\geq 200$  mg/dL, or use of glucose lowering medications. Smoking was defined by self-report as current smoking (within the 1-year period preceding the study visit) vs. former or never smoking. The physical activity index was calculated based on the reported time spent performing specific activities<sup>24</sup>.

### Statistical analysis

Baseline characteristics, exercise responses, and vascular stiffness measures were summarized and tabulated. Peak O<sub>2</sub> pulse was natural log-transformed for analysis to reduce skewness. CFPWV was inverse transformed to reduce heteroscedasticity and skewness and multiplied by  $-1000$  to convert units (ms/m) and restore directionality (i.e., expressed as  $-1000/\text{CFPWV}$  for analysis), consistent with prior work<sup>4,25</sup>. Distributions of rest/exercise BP measures and physiological correlates (CFPWV and peak O<sub>2</sub> pulse) were examined separately in men and women. Baseline and exercise measures were compared according to categories of CFPWV and peak O<sub>2</sub> pulse using two sample t-tests for continuous variables and chi-square tests for categorical variables.

We investigated the relations of peak SBP (dependent variable) with CFPWV and peak O<sub>2</sub> pulse (independent variables) using linear models adjusted for age, sex, resting (pre-exercise) SBP, and hypertension medication use. Due to differences noted in the distributions of BP indices in men and women, we evaluated for effect modification by sex on the associations of CFPWV and peak O<sub>2</sub> pulse with peak SBP using multiplicative interaction terms (i.e., sex-CFPWV and sex-peak O<sub>2</sub> pulse interaction terms were added to separate models including covariates above). Based on evidence of effect modification and different distributions of CFPWV, peak O<sub>2</sub> pulse, and peak SBP by sex, all subsequent models were conducted separately in men and women. Accordingly, we evaluated sex-specific models relating peak SBP to CFPWV and peak O<sub>2</sub> pulse adjusting for age, resting SBP, and hypertension medication use. These models were used to estimate the marginal means of peak SBP across the 5th to 95th percentile values of (non-transformed) CFPWV and peak O<sub>2</sub> pulse separately in men and women (*emmeans* package in R). Peak SBP estimation was performed using transformed variables ( $-1000/\text{CFPWV}$  and the natural logarithm of peak O<sub>2</sub> pulse) and joint effects plots were shown on the original scale for CFPWV and peak O<sub>2</sub> pulse for interpretability.



Next, we evaluated the cross-sectional associations of vascular stiffness measures (independent variables) with BP measures during exercise (dependent variables) in sex-specific linear models adjusted for age, hypertension treatment, and resting SBP. In an additional model, we also adjusted for potential confounders of body mass index (BMI), smoking, and menopause status (in women). In models with peak DBP as the dependent variable, we substituted resting DBP for resting SBP as a covariate. All independent and dependent variables were mean-centered and standardized to unit variance within each sex to facilitate comparison and interpretation. In sensitivity analyses, associations of BP responses with vascular stiffness measures were evaluated after excluding individuals with hypertension. A Bonferroni-adjusted P-value threshold of 0.01 (0.05/5 dependent or “outcome” variables) was used to determine statistical significance and control for multiple hypothesis testing. All analyses were performed using R version 4.1.3 (R project, [www.rproject.org](http://www.rproject.org)).

## RESULTS

### Clinical characteristics

Study participants had a mean age of 54±9 years and BMI of 28.1±5.3 kg/m<sup>2</sup>, with 52% women and 9.2% nonwhite individuals (Table 1). Peak VO<sub>2</sub> was 21.0±5.9 ml/kg/min (98% predicted) in women and 26.1±6.8 ml/kg/min (93% predicted) in men. Nearly half (47%) of participants had resting hypertension. Resting and exercise BP measures differed substantially in men and women with men demonstrating higher values for all BP measures except for the SBP at 75 watts. Peak O<sub>2</sub> pulse and CFPWV were also higher in men versus women (Table 1 and Figure 1).

### Distributions and relations of physiological correlates of peak SBP

The distribution of peak SBP across resting SBP measures demonstrated that ≈25% of men and women had peak SBP above clinical thresholds for elevated exercise SBP; however, these individuals exhibited varied levels of resting SBP and did not necessarily demonstrate lower peak workloads or peak O<sub>2</sub> pulse (Figure 2). To further explore the relations of peak O<sub>2</sub> pulse and CFPWV with peak SBP, we examined individual characteristics according to categories defined by low versus high values for peak O<sub>2</sub> pulse and CFPWV (Table S1). Despite higher BMI and similar resting SBP and cardiometabolic risk profiles, individuals with lower CFPWV (below sex-specific median) but higher peak O<sub>2</sub> pulse (above sex-specific median) displayed higher mean peak SBP (P<0.001 for both men and women) and higher peak fitness levels (peak VO<sub>2</sub>; P<0.001 for men and women) than individuals with lower CFPWV and lower peak O<sub>2</sub> pulse. Similarly, individuals with higher CFPWV and higher peak O<sub>2</sub> pulse demonstrated higher peak SBP than individuals with higher CFPWV and lower peak O<sub>2</sub> pulse (P<0.001 in women, P=0.017 in men) despite similar resting SBP (P>0.05 in women and men). Notably, the workloads were markedly higher (P<0.001) in individuals with higher O<sub>2</sub> pulse, suggesting that the higher SBP observed in these individuals was consistent with greater external work performed. Collectively, these findings support the notion that a higher peak SBP may not solely reflect adverse vascular function and can be observed in the setting of either higher achieved workload and cardiac-peripheral performance (O<sub>2</sub> pulse) or higher arterial stiffness (CFPWV).

### Joint relations of arterial stiffness and peak O<sub>2</sub> pulse with peak SBP

We next examined joint relations of resting CFPWV and peak O<sub>2</sub> pulse (independent variables) with peak SBP (dependent variable) using multivariable modeling. A linear model that included CFPWV, peak O<sub>2</sub> pulse, age, sex, resting SBP, and hypertension treatment explained 47% of the variability in peak exercise SBP, and CFPWV and peak O<sub>2</sub> pulse were both directly related to peak SBP (Table S2). Effect modification by sex on the relation of CFPWV with peak SBP was observed ( $P < 0.0001$ ). By contrast, the sex interaction with peak O<sub>2</sub> pulse was not significant ( $P = 0.61$ ). Given the different distributions of CFPWV, peak O<sub>2</sub> pulse, and peak SBP in men and women and the significant interaction observed by sex, we then elected to construct all subsequent models separately in men and women (Table S2). Similar relations of higher peak O<sub>2</sub> pulse with greater peak SBP were observed in women and men, consistent with lack of a significant sex interaction. However, the magnitude of association of peak SBP with CFPWV was higher in women (75% higher regression coefficient in women; Table S2 and Figure 3A). We specified model-estimated marginal means for peak SBP across CFPWV and peak O<sub>2</sub> pulse to visualize their relations with peak SBP (Figure 3B). A higher peak SBP was observed with higher CFPWV and with higher peak O<sub>2</sub> pulse. Adjusted for resting SBP, at the same peak O<sub>2</sub> pulse, a given increment in CFPWV was associated with a higher increment in peak SBP in women versus men.

### Relations of arterial stiffness and peak O<sub>2</sub> pulse with exercise BP measures at different phases of exercise

Given the higher peak workload we observed in individuals with higher peak O<sub>2</sub> pulse (Table S1), we next sought to index SBP measures during exercise to workload and examine their relation to arterial stiffness (Figure 4). We defined the “freewheel” SBP (during unloaded [0 watt] exercise), SBP at 75 watts, and SBP-to-workload slope (SBP/W, as defined in Methods). With these measures, the opposing directionality of association became evident: peak O<sub>2</sub> pulse was negatively associated with each workload-indexed BP measure, and CFPWV was positively associated. Highest effect estimates were observed for the association of CFPWV with the SBP/W slope. We observed minimal relations between augmentation index and exercise BP measures. On the other hand, characteristic impedance (reflecting the pulsatile load) was directly related to SBP measures that accounted for workload (SBP at 75 watts, SBP/W slope). Forward wave amplitude was related to exercise SBP responses at all stages of exercise, including peak SBP. These relations were largely consistent with additional covariate adjustment (Table S3), or when restricted to a subsample of individuals free of hypertension (Table S4).

## DISCUSSION

We assessed BP responses to exercise in a large FHS sample in conjunction with measures of cardiac-peripheral performance and vascular function to characterize physiological and clinical correlates of exercise BP. Our primary result was that arterial stiffness and peak O<sub>2</sub> pulse (reflecting cardiac and skeletal muscle performance during exercise) were jointly associated with peak exercise SBP. In effect, individuals could “achieve” a high peak SBP via mechanisms of greater cardiac stroke volume and O<sub>2</sub> extraction in peripheral tissues (higher peak O<sub>2</sub> pulse; a physiologically “positive” state) or via higher arterial stiffness



(a physiologically “deleterious” state). Importantly, relations of arterial stiffness with peak SBP differed by sex. While the associations of peak O<sub>2</sub> pulse with peak SBP were similar in women and men, CFPWV had a higher strength of association (as evident by the magnitude of the regression coefficient) with peak SBP in women. These observations argue against the use of a single peak SBP cut-point that does not account for stroke volume or workload to identify a hypertensive responses to exercise. Accordingly, SBP responses that incorporate workload (e.g., SBP at 75 watts, SBP/workload slope) were more closely related to adverse vascular function metrics (versus peak SBP). Collectively, these findings suggest that the magnitude of BP elevation during exercise must be interpreted in the context of its physiological contributors to clarify its clinical relevance as a reflection of adverse vascular function.

The BP response to exercise is determined in part by dynamic responses of the cardiac, peripheral (e.g., redistribution of blood flow to exercising skeletal muscle), and vascular systems<sup>26</sup>. With optimal coordination and function, the increased metabolic demands of exercise are met by an increase in cardiac output, reduction in peripheral vascular resistance, and increase in skeletal muscle O<sub>2</sub> uptake to support increased aerobic respiration. These responses are expected to result in a rise in SBP and a minimal change in DBP<sup>26</sup>. Prior clinical and epidemiological studies in individuals without overt CVD have found that exaggerated BP responses to exercise are associated with incident hypertension<sup>7,27,28</sup> and atherosclerotic vascular events<sup>5,6,29–32</sup>. Together with the observation that higher BP response to submaximal exercise is related to higher vascular stiffness and adverse endothelial function<sup>4</sup>, the foregoing findings may suggest that higher SBP during exercise is a reflection of adverse vascular function and attendant vascular risk. According to this reasoning, selected peak SBP thresholds are used by clinical guidelines to define a “hypertensive response to exercise” that serves as a universal marker of CVD risk<sup>9</sup>.

By incorporating a broad range of exercise BP, arterial stiffness, and fitness levels, the current study indicates that underlying heterogeneity in the physiologic determinants of elevated exercise SBP may complicate this interpretation. We observed that SBP values above the single cut-point clinical thresholds endorsed by exercise testing guidelines<sup>9</sup> could be achieved by individuals with lower arterial stiffness in the setting of greater cardiac-peripheral performance. Moreover, across categories of arterial stiffness, a higher peak SBP was observed in individuals with higher peak O<sub>2</sub> pulse and favorable metabolic responses to exercise despite similar cardiometabolic profiles. These observations suggest that higher peak SBP in the context of greater cardiac-peripheral performance may largely be a consequence of augmentation in stroke volume to accommodate higher workloads. By contrast, when workload was accounted for, higher values of exercise BP measures (e.g., SBP at 0 watts of resistance, SBP at 75 watts, and SBP/watts slope) were more closely related to measures of arterial stiffness in men and women and were consequently associated with lower cardiac-peripheral performance (peak O<sub>2</sub> pulse). The opposing direction of association for cardiac peripheral performance (peak O<sub>2</sub> pulse) with peak SBP and SBP measures incorporating workload reflect the ability of workload-indexed SBP measures to account for the expected augmentation in cardiac stroke volume. Use of SBP measures incorporating workload therefore restore directional concordance of the relations

of exercise BP measures and cardiac-peripheral performance/arterial stiffness in support of the traditional notion that a higher SBP response to exercise is adverse.

Importantly, of the exercise BP measures assessed, the SBP/watts slope exhibited the highest effect sizes in relation to higher arterial stiffness and lower O<sub>2</sub> pulse across sex and hypertension status. Although submaximal BP measures, such as SBP at 75 watts, might be easier to obtain, inter-individual variation in the response to a given workload may complicate interpretation. For example, we observed higher SBP measures in men versus women for all exercise BP responses except SBP at 75 watts, as this workload usually represents a higher proportion of the peak workload in women versus men.

We related exercise BP responses to four different physiological measures of arterial stiffness in this study. Directions of association and effect sizes were similar for the relations of exercise BP responses with higher (adverse) CFPWV (the most widely used noninvasive correlate of arterial stiffness), forward wave amplitude (which reflects proximal arterial geometry and stiffness) and characteristic impedance (integrating pulsatile and non-pulsatile arterial load)<sup>33</sup>. However, the augmentation index, which assesses the relative contribution of reflected waves to pulse pressure, was not associated with exercise BP measures in our study. While traditionally considered a measure of higher arterial stiffness, augmentation index has complex determinants throughout the life-course and often demonstrates divergent associations with CFPWV<sup>34</sup>.

The higher effect size in women versus men for arterial stiffness in regression with peak SBP is consistent with accumulating evidence that greater arterial stiffness may partially account for a higher prevalence of heart failure with preserved ejection fraction (HFpEF) in women<sup>14</sup>. Higher peripheral vascular resistance and an exaggerated rise in BP that is not accompanied by increases in stroke volume (referred to as “ventricular-vascular uncoupling”) are commonly observed in HFpEF and may limit cardiac output augmentation and reinforce impaired exertional tolerance<sup>35–38</sup>. Women with HFpEF display higher vascular stiffness than men, a finding that is associated with a steeper rise in left ventricular heart filling pressures with exercise<sup>14</sup>. Additionally, sex-based differences in BP regulation occur before the onset of CVD: women without overt CVD experience a steeper increase in SBP after midlife than men<sup>13</sup>, have higher proximal aortic stiffness<sup>39</sup>, and demonstrate a rise in exercise peak SBP throughout the life-course, whereas peak SBP in men often plateaus in the fifth decade<sup>3</sup>. Our findings provide physiologic insights into these clinical observations and suggest that consideration of the mechanisms underlying high peak SBP may prove useful for refining HFpEF risk assessment, especially in women.

Notably, exercise on a cycle ergometer, which was performed by all participants in our study, has been previously demonstrated to lead to higher excursions in SBP and lower peak VO<sub>2</sub> values when compared with other forms of exercise (e.g., treadmill)<sup>40</sup>. We therefore would caution against drawing conclusions about specific threshold values for use with other exercise modalities from this work. On the other hand, mean peak SBP values observed in our study sample (172 mm Hg in women, 191 mm Hg in men) were comparable to those reported for similar age groups in a large multi-center consortium of individuals undergoing treadmill exercise tests (174 mm Hg in women, 192 mm Hg in men)<sup>3</sup>. In



by sex, but an alternative strategy in which sex interaction terms are included for model estimation across the entire dataset could also be employed. In addition, our arterial stiffness assessment took place at rest. While recent work has demonstrated that different trajectories of arterial stiffness with exercise may also be relevant to CVD and HFpEF risk<sup>46</sup>, noninvasive assessment of changes in arterial stiffness with exercise is complex and may vary across different vascular beds<sup>47</sup>. Finally, our sample had a relatively high prevalence of individuals with hypertension. While we performed sensitivity analyses excluding individuals with hypertension, it is possible that the high prevalence influenced our findings.

In conclusion, our findings complicate the clinical interpretation of peak exercise SBP: both high (adverse) arterial stiffness and high (beneficial) cardiac-peripheral performance were associated with peak exercise SBP. Benchmarking SBP response to workload “restored” an adverse association of higher arterial stiffness and lower cardiac performance with SBP. Arterial stiffness appeared to have a higher effect on peak SBP responses in women. Future investigations of exercise BP responses that are sensitive to sex-based differences, workload, and vascular and cardiac physiology may illuminate mechanisms of hypertension and clinical interpretation of exercise BP.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

## Sources of Funding:

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## Disclosures:

Dr. Nayor has received speaking honoraria from Cytokinetics. Dr. Shah is supported in part by grants from the National Institutes of Health and the American Heart Association. In the past 12 months, Dr. Shah has served as a consultant for Myokardia (ongoing) and Best Doctors (ongoing), receives research funding from Amgen (concluded), had minor stock holdings in Gilead, and has current stock holdings in Pfizer. Dr. Shah is a co-inventor on a patent for ex-RNAs signatures of cardiac remodeling. Dr. Shah’s spouse works for UpToDate (Wolters Kluwer). Dr. Murthy owns stock in Amgen, General Electric and Cardinal Health. He has received speaking honoraria from, serves as a scientific advisor for, and owns stock options in Ionetix. He has received research funding and speaking honoraria from Siemens Medical Imaging. He has served as a scientific advisor for Curium and has received expert witness fees from Jubilant Draximage. He has received a speaking honorarium from 2Quart Medical. He has received non-financial research support from INVIA Medical Imaging Solutions. Dr. Lewis has research funding from the National Institutes of Health and the American Heart Association as well as Amgen, Cytokinetics, Applied Therapeutics, AstraZeneca, Sonivie in relation to projects and clinical trials investigating exercise capacity that are distinct from this work. He has served as a scientific advisor for Pfizer, Merck, Boehringer-Ingelheim, Novartis, American Regent, Relypsa, Cyclorion, Cytokinetics, and Amgen and receives royalties from UpToDate for scientific content authorship related to exercise physiology. Dr. Mitchell is owner of Cardiovascular Engineering, Inc., a company that designs and manufactures devices that measure vascular stiffness. The company uses these devices in clinical trials that evaluate the effects of diseases and interventions on vascular stiffness. He also serves as a consultant to and receives grants and honoraria from Novartis, Merck, Bayer, Servier, Philips and deCODE genetics.

## NON-STANDARD ABBREVIATIONS AND ACRONYMS

<b>BP</b>	blood pressure
<b>CVD</b>	cardiovascular disease
<b>SBP</b>	systolic blood pressure
<b>CPET</b>	cardiopulmonary exercise test
<b>FHS</b>	Framingham Heart Study
<b>RER</b>	respiratory exchange ratio
<b>ECG</b>	electrocardiogram
<b>VO<sub>2</sub></b>	oxygen uptake
<b>DBP</b>	diastolic blood pressure
<b>CFPWV</b>	carotid-femoral pulse wave velocity
<b>BMI</b>	body mass index

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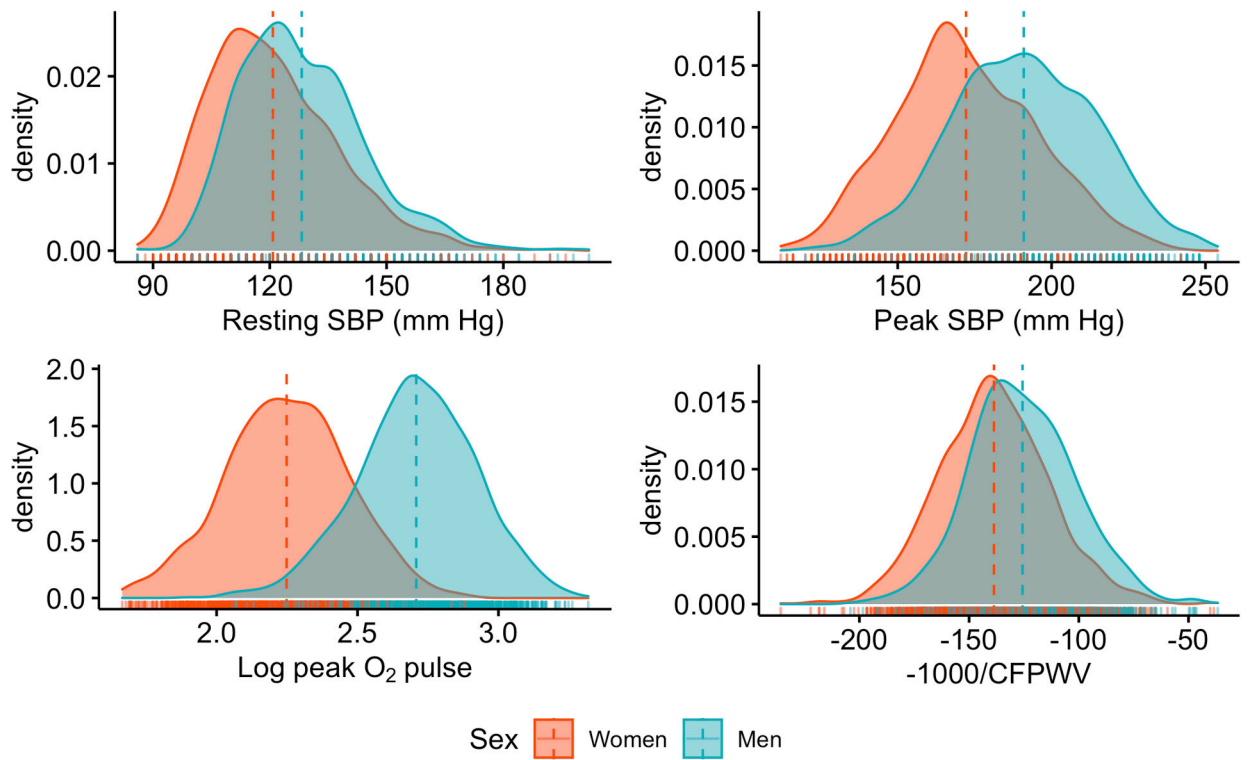
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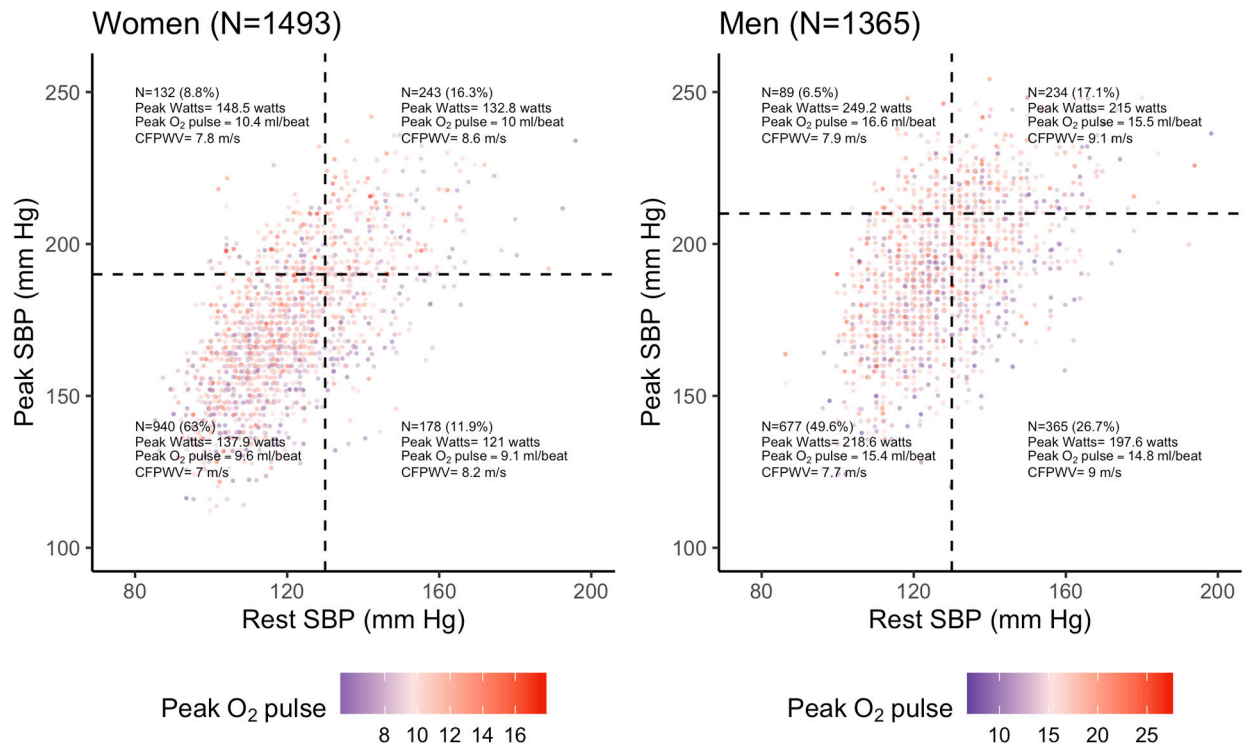
### HIGHLIGHTS

- While abnormal blood pressure responses to exercise have been linked to poorer cardiovascular outcomes and adverse arterial function, their definitions and determinants are incompletely defined.
- We sought to parse the relations of cardiac and vascular function to different measures of exercise blood pressure using maximal effort cardiopulmonary exercise tests and resting arterial tonometry.
- In 2858 Framingham Heart Study participants, an elevated peak exercise systolic blood pressure was observed in individuals with either higher (beneficial) cardiac-peripheral performance (as assessed by the peak O<sub>2</sub> pulse) or higher (adverse) arterial stiffness, with a higher magnitude of association for arterial stiffness with peak systolic blood pressure in women versus men.
- Exercise blood pressure measures incorporating workload (such as the slope of the change in systolic blood pressure during exercise/peak workload) restored directional consistency with higher values corresponding to greater arterial stiffness and poorer cardiac-peripheral performance.
- Cardiac and vascular physiological measures help to clarify the complex determinants of peak systolic blood pressure and indicate that exercise blood pressure measures incorporating workload may be preferable for clinical assessment.



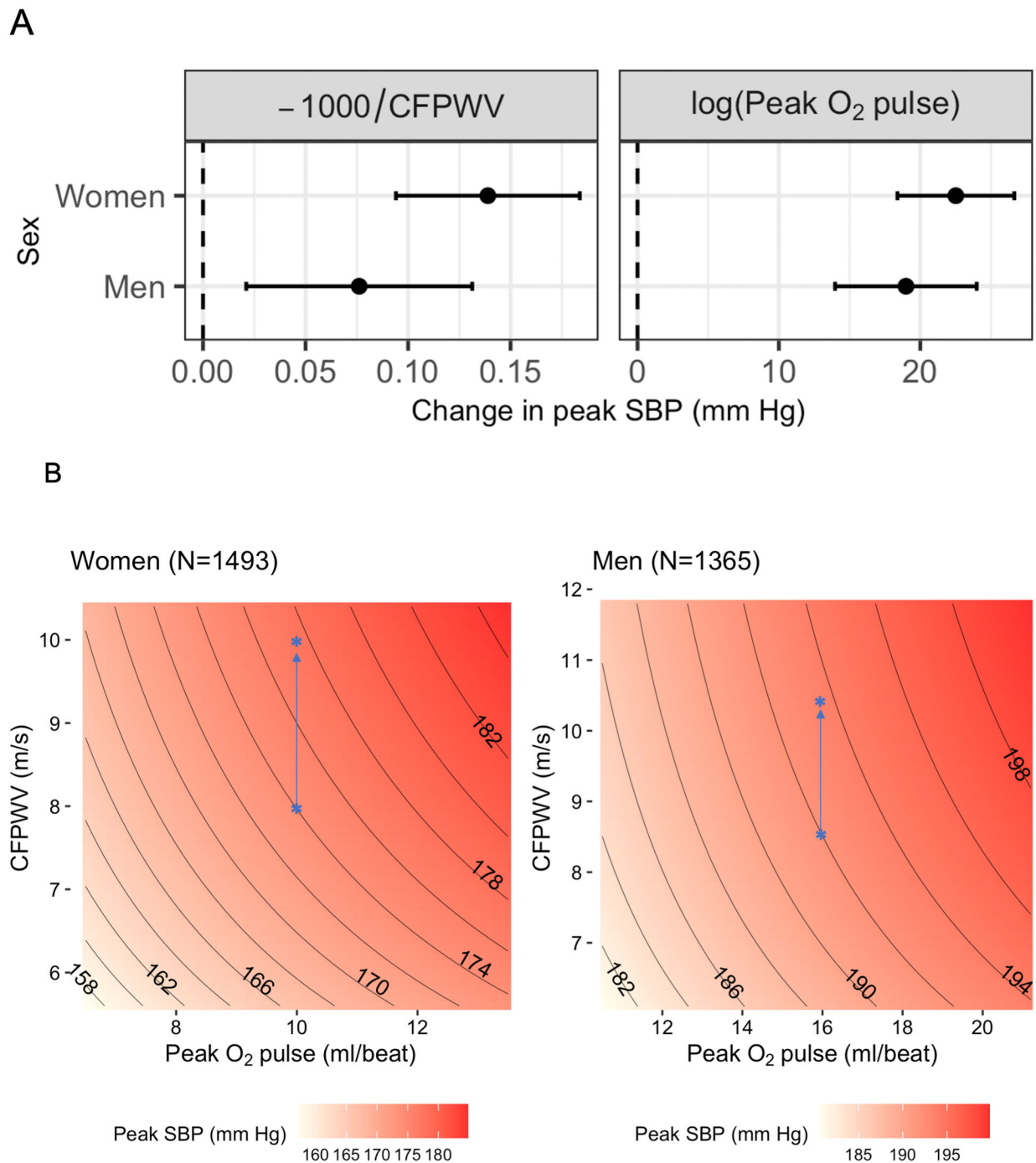
**Figure 1. Distributions of rest and exercise blood pressure measures and their physiological correlates in men and women.**

The probability density functions are plotted for men and women separately for resting systolic blood pressure (SBP), peak exercise SBP, natural log (peak O<sub>2</sub> pulse), transformed carotid-femoral pulse wave velocity ( $-1000/\text{CFPWV}$ ). Dotted lines represent sex-specific mean values.



**Figure 2. The distribution of peak systolic blood pressure across ranges of resting systolic blood pressure.**

Rest and peak exercise systolic blood pressure (SBP) were plotted for each participant separately in men and women. Points are colorized by the peak O<sub>2</sub> pulse achieved. Dotted lines were placed at 130 mm Hg to denote elevated rest SBP and 210 mm Hg for men and 190 mm Hg for women to denote elevated peak SBP. The N and mean workload (“peak watts”), peak O<sub>2</sub> pulse, and carotid-femoral pulse wave velocity are displayed for each quadrant.

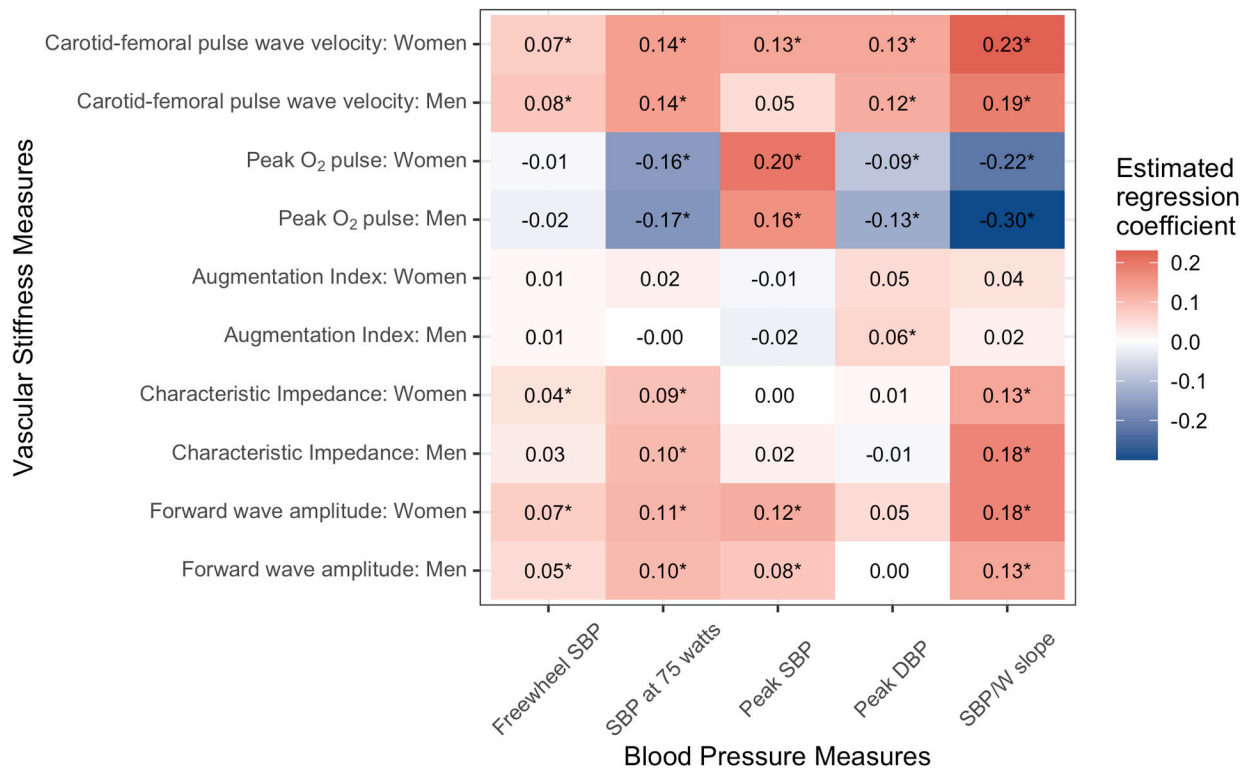


**Figure 3. Joint associations of peak  $\text{O}_2$  pulse and carotid-femoral pulse wave velocity with peak systolic blood pressure.**

In panel (A), the estimated beta coefficients and 95% confidence intervals are displayed for carotid-femoral pulse wave velocity (CFPWV, transformed) and for peak  $\text{O}_2$  pulse (natural log transformed) separately in men and women. Estimated regression coefficients were calculated in sex-stratified linear models with peak systolic blood pressure (SBP) as the dependent variable and transformed CFPWV,  $\log(\text{peak O}_2 \text{ pulse})$ , age, hypertension



treatment, and resting SBP as independent variables. Panel **(B)** displays estimated marginal means for peak SBP (using the models described above) as a function of CFPWV and peak O<sub>2</sub> pulse (5<sup>th</sup>-95<sup>th</sup> percentiles of non-transformed values) using a joint effects plot. These plots demonstrate a “trade-off” between CFPWV and peak O<sub>2</sub> pulse in relation to peak SBP. The magnitude of effect of CFPWV on peak SBP is higher in women than men. Overlaid in blue are two illustrative examples. For a woman with CFPWV of 8 m/s and peak O<sub>2</sub> pulse of 10 ml/beat, the predicted peak SBP is 174 mm Hg. An increase in CFPWV of 2 m/s (with no change in peak O<sub>2</sub> pulse) would correspond to a  $\approx 3.5$  mm Hg higher predicted peak SBP. By contrast, in a man with a CFPWV of 8.5 m/s and a peak O<sub>2</sub> pulse of 16 ml/beat, the predicted peak SBP is 192 mm Hg. A 2 m/s increase in CFPWV (with no change in peak O<sub>2</sub> pulse) would result in a  $\approx 1.7$  mm Hg increase in predicted peak SBP.



**Figure 4. Associations of blood pressure responses during exercise with different measures of vascular stiffness.**

All variables shown were mean-centered and standardized for regression. Beta coefficients represent the change in BP measures (dependent variables) for a 1-standard deviation higher value of the vascular stiffness measures or peak O<sub>2</sub> pulse. Models were adjusted for age, hypertension treatment, and resting SBP and separate models were constructed for men and women. In models with peak DBP as the dependent variable, we substituted resting DBP for resting SBP as a covariate. A Bonferroni-adjusted P-value threshold of 0.01 was used to determine statistical significance and values below this threshold are marked with an “\*”.

**Table 1.**

## Characteristics of the study sample

Variable	Overall (N=2858)	Women (N=1493)	Men (N=1365)	P-value
Age, years	54±9	53±9	54±9	0.13
Nonwhite race, N (%)	263 (9.2)	137 (9.2)	126 (9.2)	1.00
Height, in	66.8±3.7	64.3±2.5	69.5±2.7	<0.001
Body mass index, kg/m <sup>2</sup>	28.1±5.3	27.1±5.6	29.1±4.7	<0.001
Hypertension medication use, N (%)	599 (21)	256 (17)	343 (25)	0.001
AV nodal blocking medication use, N(%)	230 (8.0)	98 (6.6)	132 (9.7)	0.003
Hypertension, N (%)	1349 (47)	540 (36)	809 (59)	<0.001
Prevalent cardiovascular disease, N (%)	104 (3.6)	37 (2.5)	67 (4.9)	0.85
Diabetes, N (%)	206 (7.2)	69 (4.6)	137 (10.0)	<0.001
Current smoking, N (%)	164 (5.7)	84 (5.6)	80 (5.9)	<0.001
Total Cholesterol, mg/dL	191±36	196±35	184±36	<0.001
HDL Cholesterol, mg/dL	60±19	68±19	51±15	<0.001
Physical activity index	34±6	33±4	35±7	<0.001
SBP at rest, mm Hg	119±14	116±14	123±13	<0.001
SBP during freewheel exercise, mm Hg	130±17	127±18	134±16	<0.001
SBP at 75 watts, mm Hg	153±21	154±22	152±19	0.06
SBP at peak, mm Hg	181±25	172±23	191±23	<0.001
SBP/workload slope, mm Hg/watts	0.3±0.1	0.4±0.2	0.3±0.1	<0.001
DBP at rest, mm Hg	79±8	78±8	82±8	<0.001
DBP at peak, mm Hg	84±10	82±9	87±10	<0.001
Resting heart rate, beats/min	71.9±12.0	74.0±11.9	69.6 ±11.6	<0.001
Peak heart rate, beats/min	152.1±18.7	152.5± 18.2	151.6 ±19.3	0.18
Peak O <sub>2</sub> pulse, ml/beat	12.4±3.9	9.7±2.1	15.3±3.2	<0.001
Carotid-femoral pulse wave velocity, m/s	7.9±1.9	7.5±1.7	8.3±2.0	<0.001
Forward wave amplitude, mm Hg	48±12	47±12	48±12	0.02
Characteristic impedance	207 (70)	222 (75)	190 (60)	<0.001
Augmentation index, %	16.6±11.8	20.9±10.9	11.9±10.9	<0.001
Peak respiratory exchange ratio	1.23±0.09	1.21±0.09	1.24±0.09	<0.001
Peak workload, watts	173±60	136±35	214±54	<0.001
Peak VO <sub>2</sub> , ml/kg/min	23.4±6.8	21.0±5.9	26.1±6.8	<0.001
Percent predicted peak VO <sub>2</sub> , %	96 (20)	98 (21)	93 (18)	<0.001

Values are displayed as mean ± SD for continuous variables and N (%) for categorical variables. Abbreviations: SBP, systolic blood pressure; DBP, diastolic blood pressure; VO<sub>2</sub>, oxygen uptake. P-value reflects a comparison of men and women using two sample t-tests for continuous variables and chi-square tests for categorical variables.