# scientific reports

Check for updates

## **Assessing the external validity OPEN of machine learning‑based detection of glaucoma**

**Chi Li1,4,14, Jacqueline Chua1,2,3,14, Florian Schwarzhans5,6, Rahat Husain1,2, Michaël J.A.Girard1,2,7, Shivani Majithia1 , Yih‑ChungTham1,2, Ching‑Yu Cheng1,2,8, TinAung1,2,8, Georg Fischer5 , ClemensVass9 , Inna Bujor10, Chee Keong Kwoh4 ,**  Alina Popa-Cherecheanu<sup>10,11</sup>, Leopold Schmetterer<sup>1,2,3,6,7,12,13</sup> & Damon Wong<sup>1,3,7,12⊠</sup>

**Studies using machine learning (ML) approaches have reported high diagnostic accuracies for glaucoma detection. However, none assessed model performance across ethnicities. The aim of the study is to externally validate ML models for glaucoma detection from optical coherence tomography (OCT) data. We performed a prospective, cross-sectional study, where 514 Asians (257 glaucoma/257 controls) were enrolled to construct ML models for glaucoma detection, which was then tested on 356 Asians (183 glaucoma/173 controls) and 138 Caucasians (57 glaucoma/81 controls). We used the retinal nerve fbre layer (RNFL) thickness values produced by the compensation model, which is a multiple regression model ftted on healthy subjects that corrects the RNFL profle for anatomical factors and the original OCT data (measured) to build two classifers, respectively. Both the ML models (area under the receiver operating [AUC] = 0.96 and accuracy = 92%) outperformed the measured data (AUC= 0.93; P< 0.001) for glaucoma detection in the Asian dataset. However, in the Caucasian dataset, the ML model trained with compensated data (AUC= 0.93 and accuracy = 84%) outperformed the ML model trained with original data (AUC= 0.83 and accuracy = 79%; P< 0.001) and measured data (AUC= 0.82; P< 0.001) for glaucoma detection. The performance with the ML model trained on measured data showed poor reproducibility across diferent datasets, whereas the performance of the compensated data was maintained. Care must be taken when ML models are applied to patient cohorts of diferent ethnicities.**

Glaucoma is characterized by progressive loss of retinal ganglion cells, leading to visual impairment<sup>1</sup>. Given that visual loss from glaucoma is irreversible, the disease must be detected at an early stage before signifcant visual field (VF) loss has been established so that the risk of vision-related morbidity can be minimized<sup>[2](#page-6-1)</sup>. While the disease is diagnosed based on funduscopic examination and VF testing, optical coherence tomography (OCT) is an efficient approach to support clinicians since it provides quantitative, reproducible measurements which are less patient-dependent<sup>[3](#page-6-2)</sup>.

Recently, machine learning (ML) models have been applied to OCT structural data to assist with glaucoma diagnosis<sup>4</sup>. ML classifiers are computerized systems trained with the capacity to identify the relationship between multiple features and a disease diagnosis. While most have reported high diagnostic accuracies (AUC=0.88–0.98)

<sup>1</sup>Singapore Eye Research Institute, Singapore National Eye Centre, 20 College Road, The Academia, Level 6, Discovery Tower, Singapore 169856, Singapore. <sup>2</sup>Ophthalmology & Visual Sciences Academic Clinical Program, Duke-NUS Medical School, Singapore, Singapore. <sup>3</sup>SERI-NTU Advanced Ocular Engineering (STANCE), Singapore, Singapore. <sup>4</sup>School of Computer Science and Engineering, Nanyang Technological University, Singapore, Singapore. <sup>5</sup>Center for Medical Statistics Informatics and Intelligent Systems, Section for Medical Information Management, Medical University Vienna, Vienna, Austria. <sup>6</sup>Department of Clinical Pharmacology, Medical University Vienna, Vienna, Austria. <sup>7</sup>Institute of Molecular and Clinical Ophthalmology, Basel, Switzerland. <sup>8</sup>Department of Ophthalmology, Yong Loo Lin School of Medicine, National University of Singapore, Singapore, Singapore. <sup>9</sup>Department of Ophthalmology and Optometry, Medical University Vienna, Vienna, Austria. <sup>10</sup>Carol Davila University of Medicine and Pharmacy, Bucharest, Romania. <sup>11</sup>Department of Ophthalmology, Emergency University Hospital, Bucharest, Romania. <sup>12</sup>School of Chemical and Biomedical Engineering, Nanyang Technological University, Singapore, Singapore. 13Center for Medical Physics and Biomedical Engineering, Medical University Vienna, Vienna, Austria. 14These authors contributed equally: Chi Li and Jacqueline Chua. <sup>22</sup>email: damon.wong@ntu.edu.sg

for glaucoma detection<sup>5-9</sup>, none assessed the models with independently sampled data from a different ethnicity group (external test), which limits the generalizability of the models across ethnicities<sup>[10](#page-7-3)</sup>.

Anatomic factors such as retinal vessel tree confguration, fovea-disc angle, or optic disc size vary across ethnicities<sup>[11](#page-7-4)[–14](#page-7-5)</sup> and can affect peripapillary retinal nerve fibre layer (RNFL) thickness<sup>[15](#page-7-6)[–21](#page-7-7)</sup>. We have previously developed a compensation model, which is a multiple regression model ftted on healthy subjects that corrects the RNFL profile for factors like ethnicity, disc parameters and age<sup>22</sup>, showing better glaucoma discrimination capability than original OCT data (measured RNFL thickness)<sup>23</sup>. It is likely that ML models trained on compensated data may be more applicable across ethnicities since the classifer would have access to "distilled" information and would not be biased by the anatomic factors.

The objective of this paper was to validate ML models for glaucoma detection from OCT data (Cirrus, Carl Zeiss Meditec, Dublin, CA). We used RNFL thickness values produced by the compensation model and the original Cirrus-generated data (measured) to build two classifers, respectively.

#### **Materials and methods**

**Study population.** Glaucoma patients and controls were enrolled from the Singapore Eye Institute in Singapore and the Department of Ophthalmology, Emergency University Hospital, Bucharest, Romania, respectively. The Asian study was approved by the human ethics boards of Singapore Eye Research Institute and the Caucasian study by the Emergency University Hospital Bucharest Ethics Committee. Both studies were conducted according to the Declaration of Helsinki and written informed consent was obtained from all participants.

For the Asian study, glaucoma cases<sup>24</sup> were enrolled in the Singapore Imaging Eye Network (SIENA) study from July 2018 to July 2019 and controls<sup>[25](#page-7-11)</sup>) from the Singapore Epidemiology of Eye Disease (SEED) program. Briefy, SIENA is a clinical cross-sectional study investigating the efects of vascular abnormalities in participants with primary open-angle glaucoma (POAG) aged 21 years and older, and SEED study is a population-based study comprised of Chinese, Malays and Indians aged 40–80 years living in Singapore<sup>[26](#page-7-12)</sup>. Of the total 569 Asians with glaucoma, 129 had missing variables or poor-quality scans, leaving a fnal sample of 440 glaucoma patients (n=513 eyes), of which 370 were Chinese, 42 Malays and 27 Indians and 1 individual of mixed Asian origin. Of the 3988 Asians with normal eyes, 1289 had missing variables or poor-quality scans, leaving a sample of 2699 controls<sup>[25](#page-7-11)</sup>. For the present analysis, we applied a frequency matching technique based on age- (by 5-year age groups), gender- and race-matchin[g25,](#page-7-11) where one control was randomly selected for each glaucoma participant. Therefore, 430 controls (n=513 eyes) comprising of 348 Chinese, 48 Malays and 34 Indians participants were included for the analysis.

For the Caucasian study, glaucoma cases and controls were enrolled from the Department of Ophthalmology, Emergency University Hospital, Bucharest, Romania from August 2020 to March 2021. From a total of 78 glaucoma patients and 105 controls, 45 with missing or poor-quality scans were excluded, leaving 57 glaucoma patients (n=87 eyes) and 81 controls (n=145 eyes) for the fnal analysis (Supplementary Fig. S1).

Study methodologies were identical for Asians and Caucasians unless otherwise stated. Participants underwent an ocular examination which included measurement of visual acuity using a logarithm of the minimum angle of resolution chart (LogMAR chart, The Lighthouse, NY), auto-refraction-keratometry (Asian: Canon RK-5 Autorefractor Keratometer; Canon Inc., Tokyo, Japan; Caucasian: CHAROPS CRK-7000; Huvitz Co., Ltd, South Korea)<sup>27</sup>, axial length measurement (Asian: IOL Master V3.01, Carl Zeiss Meditec AG, Jena, Germany; Caucasian: IOL Master V5, Carl Zeiss Meditec AG, Jena, Germany), intraocular pressure measurement using Goldmann applanation tonometry, and OCT imaging (see later section). Only glaucoma participants underwent Humphrey Swedish interactive thresholding model SITA standard or SITA fast 24–2 perimetry (Asian: Humphrey VF analyser II; Carl Zeiss Meditec, USA; Caucasian: Zeiss Humphrey Field Analyzer 3, Model 860 Carl Zeiss Meditec, USA). Spherical equivalent (SE) was calculated as the spherical value plus half of the negative cylinder value.

Glaucoma patients were defned during an ophthalmic examination by board certifed ophthalmologists following the criteria: presence of glaucomatous optic neuropathy (defned as loss of neuroretinal rim with a vertical cup: disc ratio of>0.7 or an inter-eye asymmetry of>0.2 and/or notching attributable to glaucoma) with compatible and reproducible VF in standard automated perimetry, and open angles on gonioscopy. Patients with secondary glaucoma or history of retinal operation or laser treatments were excluded from this study. Glaucoma severity was defined on perimetry findings as mild glaucoma (mean deviation (MD) ≥ -6 dB, moderate glaucoma (-6.01 to -12.00 dB), and severe glaucoma (MD <-12 dB)<sup>[28,](#page-7-14)29</sup>. Controls were defined as individuals free from clinically relevant eye conditions and were confrmed to have no sign of glaucoma or other major eye diseases except for mild cataract by an ophthalmic examination. These controls at time of recruitment had intraocular pressure<21 mmHg with open angles, healthy optic nerves, and no family history of glaucoma.

**OCT Imaging.** Participants underwent Cirrus (Carl Zeiss Meditec, Dublin, CA) spectral domain-OCT optic disc and macular cube  $(200 \times 200)$  imaging after pharmacological dilation<sup>30</sup>. Trained graders, masked to the participant's characteristics reviewed the quality of OCTs. Only eyes with good quality images (signal strength greater than or equal to 6), no excessive movement artifacts, consistent signal intensity across the scan, circular scan centred at the optic disc, and no segmentation artifact were included in the analysis. Both eyes were included in the study if they met the eligibility criteria. Supplementary Fig. S2 shows two representative OCT images of normal and glaucoma patients.

**Extractions of measured RNFL thickness and other ocular anatomical features.** Peripapillary RNFL thickness measurements were automatically obtained from a 3.46 mm diameter ring around the optic disc using the Cirrus Review Software (software version 11.0.0.29946). The global RNFL thickness was calculated from 12 sector-wise values and used for subsequent comparative analysis.

2

Optic disc and macular OCT images were processed with MATLAB (MathWorks Inc., R2018b, Natick, MA) to extract anatomical features such as the optic disc, fovea, and the retinal vessel tree from the OCT volumes<sup>22</sup>. Optic disc variables including its area, orientation (angle between the horizontal axis and the major axis of the optic disc), and ratio (between major and minor axes) were extracted from the OCT. The optic disc ratio describes how elliptical the optic disc is, where a value closer to 1.0 indicates a more circular optic disc. From the registered optic disc and macula images, the fovea distance (the distance between optic disc and fovea centers) and fovea angle (the angle between a line connecting fovea and optic disc centers and a horizontal line passing through the optic disc center) were calculated.

**Compensation model.** We previously developed a compensation model, which is a multiple regression model ftted on healthy subjects that corrects the RNFL profle for eight factors, namely age, refractive error, optic disc (ratio, orientation, and area), fovea (distance and angle), and retinal vessel density<sup>23</sup>. A compensation model was developed separately for each ethnic group (Chinese, Malay and Indian). It was trained on 1619 healthy Asian patients  $(n=2389 \text{ eyes})$ .

**Machine learning models.** We used the Asian dataset and built two classifers, one using the RNFL thickness values produced by the compensation model and the original Cirrus-generated data (measured) (Supplementary Fig. S1). We used the 12 sectors of RNFL thickness values to build the ML models. The Asian dataset was randomly divided using a 6:4 ratio for the training and test datasets based on the age, gender, and race frequency matching, where the training set consists of 257 glaucoma patients ( $n=307$  eyes) and 257 controls  $(n=307 \text{ eyes})$ , and the internal test set consists of 183 glaucoma patients  $(n=206 \text{ eyes})$  and 173 controls  $(n=206 \text{ eyes})$ eyes; Supplementary Fig. S1). We compared the performance of the ML models on our internal Asian dataset of 356 participants (412 eyes) and the external Caucasian dataset comprising of 138 participants (232 eyes).

We combined four different ML models, logistic regression  $(LR)^{31}$ , support vector machines (SVM)<sup>31</sup>, random forests  $(RF)^{32}$ , and gradient boosting (GB)<sup>[33](#page-7-19)</sup>, using soft voting ensembling (SVE). LR analysis involves fitting a logit function for class prediction, while a SVM classifer works by determining the hyperplane for maximal class separation. In contrast, RF classifers are a collection of decision trees, each constructed by randomly sampling from the training data with replacement in a process known as bagging. GB classifers are decision tree models in which a sequence of decision trees is generated, with each subsequent tree correcting for errors made by prior trees. While each of these ML models may be used for glaucoma detection, SVE balances out the potential weak-nesses of each model by combining their inputs<sup>[34](#page-7-20)</sup>. Class probabilities obtained from each classifier were averaged and the class with the highest averaged probability was used as the output of the SVE.

Grid search fvefold cross-validation is used for fnetuning of the hyperparameters for each specifc classifer. Apart from some pre-determined parameters, like penalty and kernel, the remaining parameters are estimated with GridSearchCV in sklearn.model\_selection. GridSearchCV is a way of iterating through the possible values for target parameter and testing the accuracy through cross validation. The dataset used for model training was frst separated into fve groups. First, the cross validation iterates through the folds and uses one of the fve folds as the validation dataset at each iteration while all remaining folds are used as training dataset. This process is repeated until every fold has been used as a validation dataset for every combination of potential value of the parameters.

**Statistical analyses.** The characteristics between train and test datasets were compared using independent t-test and chi-square for continuous and categorical variables, respectively. Independent *t* test and chi-squared test were conducted in R version 4.0.4 (The R Foundation for Statistical Computing) using functions t.test and chisq.test. The area under the receiver operating characteristics curve (AUC) for glaucoma detection were calculated. To account for the nested structure of dataset, eyes of same patient were clustered in ROC analyses. 1000 bootstrap replicates from the internal and external datasets were drawn to generate the 95% bootstrap percentile intervals. Sensitivity at 95% specificity was also generated. DeLong's test was conducted in R version 4.0.4 (The R Foundation for Statistical Computing), using function roc.test in pROC packages. DeLong's test evaluated the difference between AUCs<sup>35</sup>. Accuracy was defined as the ratio between the number of properly classified samples over the overall number of samples<sup>[36](#page-7-22)</sup>. F1 score was calculated as the harmonic mean of the precision and recall<sup>36</sup>. Spearman's rank correlation coefficients  $(r<sub>s</sub>)$  were used to evaluate the relationship between VF's mean deviation (VFMD) and raw values of structural damage either using measured RNFL or probability score predicted from ML models. A locally weighted scatterplot smoothing (LOWESS) curve was used to visualize the relationship between these variables. In this paper, statistical significance threshold was set at 0.05 as proposed by Fischer<sup>[37](#page-7-23)</sup>. The exact P value for t-test, chi-squared test and DeLong's test was also provided in Tables [1](#page-3-0) and [2](#page-3-1). Data were analyzed with R version 4.0.4 (The R Foundation for Statistical Computing).

#### **Results**

There mainly were no significant differences between the training dataset and the Asian test dataset (P≥0.174), except for fovea distance ( $P=0.029$ , Table [1](#page-3-0)). However, there were significant differences between the training dataset and the Caucasian test dataset, with participants in the external test dataset being younger (mean ± standard deviation (SD) of 49±17 years), having a larger ratio of females, and more mild and moderate glaucoma eyes (P<0.00[1](#page-3-0), Table 1). The ocular characteristics of normal participants were also significantly different between the training dataset and the Caucasian test dataset, fewer Caucasians having signifcantly shorter fovea distances, smaller foveal angles, less elliptical optic discs (ratio closer to 1.0), and thicker retinal vessel densities (P≤0.009, Table [1\)](#page-3-0). For the glaucoma dataset, Caucasians had signifcantly less elliptical optic discs, higher optic disc



<span id="page-3-0"></span>**Table 1.** Characteristics of the training and testing datasets. Data are number, mean±standard deviation, or number (%). For n (%), the denominator is number of patients or number of eyes (by eye), as applicable. P value was obtained with independent t-tests for continuous variables and with chi-square tests for categorical variables and values in bold indicate statistical signifcance. \* Denotes comparison between Asian training and Asian test dataset whereas † between Asian training and Caucasian test dataset.



<span id="page-3-1"></span>**Table 2.** Comparison of glaucoma detection between measured retinal nerve fbre layer (RNFL), compensated RNFL, and machine learning approaches. Data in parentheses are 95% confdence intervals. Results for sensitivity are expressed as percentages. P value was obtained with DeLong et al. (1988) for paired receiver operating characteristic curves and values in bold indicate statistical signifcance.

4

orientations, thicker retinal vessel densities, were more hyperopic, and had larger RNFL thicknesses (P≤0.001, Table [1\)](#page-3-0).

The values for AUC and sensitivity at 95% specificity for glaucoma detection using the measured RNFL, compensated RNFL, and ML models trained either with measured RNFL or compensated RNFL (Table [2](#page-3-1)). In the Asian test dataset, both the ML models ( $AUC=0.96$ ) outperformed the measured RNFL thickness ( $AUC=0.93$ ;  $P < 0.001$ ) and compensated RNFL thickness (AUC=0.93; P < 0.001) for glaucoma detection. However, in the Caucasian dataset, the ML model trained with compensated data (AUC= 0.93) outperformed the ML model trained with measured RNFL (AUC=0.83; P< 0.001) and measured RNFL thickness (AUC=0.82; P< 0.001). There was no difference in the AUCs between the ML model trained with compensated data and compensated RNFL thickness (AUC =  $0.89$ ; P =  $0.641$ ). At a specificity level of 95%, the sensitivity for detecting glaucoma was highest using ML models (84–85%) and lowest using non-ML approaches (73–76%) in the Asian dataset (Table [2](#page-3-1) and Fig. [1](#page-4-0)). In the Caucasian dataset, the sensitivity for detecting glaucoma was highest using compensated RNFL approaches (64–67%) and lowest using original RNFL (49–52%; Table [2](#page-3-1) and Fig. [1](#page-4-0)). We also included the result of every classifer for every dataset (Supplementary Table S2) and the ML confusion matrix for testing of every dataset (Supplementary Table S3). The findings of Tables S2 and S3 support the overall finding that the use of compensated OCT data in ML achieves better results than measured data.

We next performed a separate sub-analysis on a balanced Caucasian test dataset using 87 normal and 87 glaucoma patients. Our additional fndings were consistent with earlier analysis where the use of compensated data for machine learning (AUC=0.92) is significantly better than measured data (AUC=0.84; P < 0.01; Supplementary Table S1).

We evaluated the relationship between the VFMD and structural damage with the measured RNFL and ML models. Figure [2](#page-5-0) shows the LOWESS plots, suggesting a monotonic relationship between VFMD and all approaches for both the internal test (+1.4 to − 27.3 dB) and external test (+2.5 to − 23.0 dB) datasets. Tis association with the VFMD was statistically signifcant for all approaches (P<0.001). It was the strongest with the ML model trained with the measured RNFL in the Asian dataset  $(r_s = 0.589)$  and Caucasian dataset  $(r_s = 0.446)$ .

We reviewed two glaucoma cases in which there are diferences in the results between the Cirrus-generated RNFL analysis and the ML models (Fig. [3\)](#page-6-3). Case A is an Asian glaucoma patient presenting a normal RNFL probability color code in all quadrants with the Cirrus normative database and ML with compensated RNFL. Only the ML model using measured RNFL correctly predicted an abnormal RNFL probability color code correlated with the VF report. Case B is a Caucasian glaucoma patient, where only the ML using compensated RNFL correctly predicted an abnormal RNFL probability color code, which agrees better with the VF report.

#### **Discussion**

In this prospective duo-center, cross-sectional diagnostic study, we validated ML models for glaucoma detection, one trained using measured RNFL thickness and the other compensated RNFL thickness, derived from a multiple regression model ftted on healthy subjects that corrects the RNFL profle for factors like ethnicity, disc parameters and age. The results showed a poor reproducibility of the performance with the ML model trained on original RNFL data across diferent datasets. In contrast, the performance of the ML model trained on compensated RNFL seemed to be maintained. To the best of our knowledge, our study is the frst to assess the performance of ML classifers to detect glaucoma between ethnicities. Evaluating the performance of ML models for glaucoma detection using OCT data in new subjects is a crucial step in understanding the model generalizability to other populations.



<span id="page-4-0"></span>**Figure 1.** Receiver operating characteristic curves comparing glaucoma detection on the (**A**) Testing Asian dataset and (**B**) Testing Caucasian dataset using the measured retinal nerve fber layer (RNFL), machine learning models using either measured RNFL thickness or compensated RNFL thickness. Values in brackets indicate the area under the curves (AUC) for the corresponding approaches.



<span id="page-5-0"></span>Figure 2. Scatter plots showing the associations between the visual field mean deviation (VFMD) and measured retinal nerve fber layer (RNFL) thickness for (**A**) Asian and (**D**) Caucasian test datasets. (**B**) and (**E**) show the associations between VFMD, and the probability score generated by a machine learning (ML) model using measured RNFL thickness, where a lower score indicates greater severity of glaucoma. (**C**) and (**F**) show the associations between VFMD, and the probability score generated by a ML model using compensated RNFL thickness, where a higher score indicates greater severity of glaucoma. Spearman's correlation coefficient ρ and LOWESS curves are indicated for the corresponding variables in each plot.

Studies using ML approaches to detect glaucoma have used RNFL thickness data from OCT scans<sup>5-[9](#page-7-2)[,38](#page-7-24)</sup>. While most reported high cross-validated AUCs of 0.88–0.98 (internal validation)<sup>5[,6](#page-7-25),[8,](#page-7-26)[9](#page-7-2)[,38](#page-7-24)</sup>, none assessed the model performance across ethnicities. In the current study, while the performance of ML when using measured RNFL thickness was excellent in the Asian dataset (AUC=0.96), it was less promising in the Caucasian dataset (AUC = 0.83). Instead, the ML model trained on compensated RNFL thickness data (AUC = 0.93; P < 0.01) achieved better glaucoma detection than the traditional ML model (uses original RNFL data; AUC=0.83) in an external dataset. The improvement in AUC is likely because the compensation model "normalizes" the RNFL profle (not biased by anatomic variability of each eye), which enhances the true extent of pathological damage for ML modeling. Most importantly, our study suggests that the anatomical variations may explain the poor generalizability of ML models when tested on datasets they were not trained on. It is well-known that there are considerable diferences in the fundus between Asians and Caucasians. For instance, diferences in optic disc size, shape, and cup-to-disc ratio have been reported across ethnicities/races in healthy individuals $14$ . This is also evident from the current study where the ocular characteristics difered between training and external datasets. These anatomic differences can notoriously affect the RNFL thickness<sup>[15](#page-7-6)-[21](#page-7-7)</sup>. Hence, current ML models trained on measured RNFL data from a specifc patient population may be less applicable across ethnicities. In general, the direct application of the ML model may be the most appropriate for individuals who share multiple characteristics from which the model was derived. In the future, it may be more feasible to use compensated RNFL thickness data to develop an ML classifer rather than using RNFL thickness data from specifc ethnicity. Another reason for the heterogeneous model performance may be the distribution of glaucoma cases. The training Asian dataset had a more signifcant proportion of glaucoma than the testing Caucasian dataset (50 vs. 38%). Furthermore, the percentage of mild glaucoma in the testing Caucasian dataset was higher than in the training Asian dataset (75 vs. 61%). As a result, the higher percentage of mild glaucoma and normal eyes in the testing Caucasian dataset as compared to the training Asian dataset may make discrimination more difficult<sup>39</sup>. Tis can also be seen in the poor diagnostic performance of RNFL thickness in the testing Caucasian dataset compared to the testing Asian dataset.

The compensation model did not improve glaucoma detection compared to the conventional circumpapillary RNFL thickness in the Asian dataset, which was in contrast to our recent study<sup>[23](#page-7-9)</sup>. One potential explanation is that the current study was a race-matched dataset, whereas our previous study<sup>[23](#page-7-9)</sup> was not matched for the race. Significant racial differences in the ocular factors were reported in a multi-ethnic Asian population $30$ . Given that



<span id="page-6-3"></span>**Figure 3.** Representative glaucoma cases showing the diagnostic performances of the measured retinal nerve fber layer (RNFL), machine learning model using measured RNFL thickness, and machine learning model using compensated RNFL thickness. Case (**A)** is an Asian glaucoma patient, while Case (**B**) is a Caucasian glaucoma patient. The Cirrus RNFL thickness maps indicate a reduction in the RNFL thickness in the superior and inferior regions in Case (**A**), while it shows a reduction in the superior regions in Case (**B**). However, the Cirrus quadrant analyses show a normal RNFL probability color code in all quadrants in both cases. The output prediction of both compensation and machine learning approaches are color-coded, where the red circle indicates wrong prediction, and the green circle indicates correct prediction. The machine learning model measured RNFL thickness correctly predicted Case (**A**) with glaucoma while the machine learning model using compensated RNFL thickness correctly predicted Case (**B**) with glaucoma.

race is now matched equally between the training and test dataset, the infuence of anatomical factors on the RNFL thickness is relatively minimal.

Our study had several limitations. First, the ground truth of glaucoma was defned clinically based on glaucomatous structural damage and corresponding VF abnormalities, which can be contentious even among expert observer[s40.](#page-7-28) Even though glaucoma diagnosis was made by board-certifed ophthalmologists for both Asians and Caucasians, misclassifcations as a result of this subjective assessment cannot be entirely ruled out, particularly in diferentiating patients with early glaucoma. Second, our ML model was trained on Asians of Chinese, Malay, and Indian ethnicities and validated on Caucasians. The results reported herein apply to the sample and ML classifiers investigated and should be extrapolated to other populations or models with caution. In this study, we cannot investigate whether the diferent performances are still observed when the model was trained using a Caucasian training dataset. Glaucoma imaging was introduced recently in Caucasians, and recruitment is ongoing.

#### **Conclusion**

In conclusion, although  $ML^{5-9,38}$  $ML^{5-9,38}$  $ML^{5-9,38}$  has been suggested as a potential solution for accurately and quickly identifying glaucomatous damage on diagnostic tests compared to subjective ocular examination and other traditional methods, their predictive performance can be variable across datasets.

#### **Data availability**

Data in this study cannot be shared publicly due to regulations of local ethical committees (Sing-Health Centralised Institutional Review Board, R1500/83/2017) and (Emergency University Hospital Bucharest Ethics Committee, 11285). Data might be made available to researchers who meet the criteria (to be provided once all data are available) for access to confdential data and upon Institutional Review Board's approval; requests for access to Asian dataset can be made to Prof. Leopold Schmetterer (leopold.schmetterer@seri.com.sg) and Caucasian dataset to Prof. Alina Cherecheanu (alina\_cherecheanu@yahoo.com).

Received: 19 August 2022; Accepted: 9 January 2023

#### **References**

- <span id="page-6-0"></span>1. Weinreb, R. N., Aung, T. & Medeiros, F. A. Te pathophysiology and treatment of glaucoma: A review. *JAMA* **311**, 1901–1911. <https://doi.org/10.1001/jama.2014.3192>(2014).
- <span id="page-6-1"></span>2. Ramulu, P. Glaucoma and disability: Which tasks are afected, and at what stage of disease?. *Curr. Opin. Ophthalmol.* **20**, 92–98. <https://doi.org/10.1097/ICU.0b013e32832401a9> (2009).
- <span id="page-6-2"></span>3. Weinreb, R. N. *et al.* Primary open-angle glaucoma. *Nat. Rev. Dis. Primers* **2**, 16067. <https://doi.org/10.1038/nrdp.2016.67> (2016).

7

- <span id="page-7-0"></span>4. Wu, J. H., Nishida, T., Weinreb, R. N. & Lin, J. W. Performances of machine learning in detecting glaucoma using fundus and retinal optical coherence tomography images: A meta-analysis. *Am. J. Ophthalmol.* <https://doi.org/10.1016/j.ajo.2021.12.008>(2021).
- <span id="page-7-1"></span>5. Wang, P. *et al.* Machine learning models for diagnosing glaucoma from retinal nerve fber layer thickness maps. *Ophthalmol. Glaucoma* **2**, 422–428. <https://doi.org/10.1016/j.ogla.2019.08.004> (2019).
- <span id="page-7-25"></span>6. An, G. *et al.* Glaucoma diagnosis with machine learning based on optical coherence tomography and color fundus images. *J. Healthc. Eng.* **2019**, 4061313. <https://doi.org/10.1155/2019/4061313> (2019).
- 7. Kim, S. J., Cho, K. J. & Oh, S. Development of machine learning models for diagnosis of glaucoma. *PLoS ONE* **12**, e0177726. [https://](https://doi.org/10.1371/journal.pone.0177726) [doi.org/10.1371/journal.pone.0177726](https://doi.org/10.1371/journal.pone.0177726) (2017).
- <span id="page-7-26"></span>8. An, G. *et al.* Comparison of machine-learning classifcation models for glaucoma management. *J. Healthc. Eng.* **2018**, 6874765. <https://doi.org/10.1155/2018/6874765>(2018).
- <span id="page-7-2"></span>9. Oh, S., Park, Y., Cho, K. J. & Kim, S. J. Explainable machine learning model for glaucoma diagnosis and its interpretation. *Diagnostics* <https://doi.org/10.3390/diagnostics11030510>(2021).
- <span id="page-7-3"></span>10. Ramspek, C. L., Jager, K. J., Dekker, F. W., Zoccali, C. & van Diepen, M. External validation of prognostic models: What, why, how, when and where?. *Clin. Kidney J.* **14**, 49–58.<https://doi.org/10.1093/ckj/sfaa188> (2021).
- <span id="page-7-4"></span>11. Rochtchina, E., Wang, J. J., Taylor, B., Wong, T. Y. & Mitchell, P. Ethnic variability in retinal vessel caliber: A potential source of measurement error from ocular pigmentation?–the Sydney Childhood Eye Study. *Investig. Ophthalmol. Vis. Sci.* **49**, 1362–1366. <https://doi.org/10.1167/iovs.07-0150>(2008).
- 12. Seider, M. I. *et al.* Optic disk size variability between African, Asian, white, Hispanic, and Filipino Americans using Heidelberg retinal tomography. *J. Glaucoma* **18**, 595–600.<https://doi.org/10.1097/IJG.0b013e3181996f05> (2009).
- 13. Bourne, R. R. Ethnicity and ocular imaging. *Eye (Lond.)* **25**, 297–300.<https://doi.org/10.1038/eye.2010.187> (2011).
- <span id="page-7-5"></span>14. Girkin, C. A., McGwin, G. Jr., McNeal, S. F. & DeLeon-Ortega, J. Racial diferences in the association between optic disc topography and early glaucoma. *Investig. Ophthalmol. Vis. Sci.* **44**, 3382–3387.<https://doi.org/10.1167/iovs.02-0792>(2003).
- <span id="page-7-6"></span>15. Jonas, R. A. *et al.* Optic disc—Fovea angle: Te Beijing eye study 2011. *PLoS ONE* **10**, e0141771. [https://doi.org/10.1371/journal.](https://doi.org/10.1371/journal.pone.0141771) [pone.0141771](https://doi.org/10.1371/journal.pone.0141771) (2015).
- 16. Resch, H. *et al.* Infuence of disc-fovea angle and retinal blood vessels on interindividual variability of circumpapillary retinal nerve fbre layer. *Br. J. Ophthalmol.* **100**, 531–536.<https://doi.org/10.1136/bjophthalmol-2015-307020> (2016).
- 17. Budenz, D. L. *et al.* Determinants of normal retinal nerve fber layer thickness measured by Stratus OCT. *Ophthalmology* **114**, 1046–1052. <https://doi.org/10.1016/j.ophtha.2006.08.046>(2007).
- 18. Ho, H. et al. Retinal nerve fiber layer thickness in a multi-ethnic normal Asian population: The Singapore Epidemiology of Eye Diseases (SEED) Study. *Ophthalmology* <https://doi.org/10.1016/j.ophtha.2018.11.031>(2018).
- 19. Choi, J. A., Kim, J. S., Park, H. Y., Park, H. & Park, C. K. Te foveal position relative to the optic disc and the retinal nerve fber layer thickness profle in myopia. *Investig. Ophthalmol. Vis. Sci.* **55**, 1419–1426.<https://doi.org/10.1167/iovs.13-13604> (2014).
- 20. Yamashita, T. *et al.* Relationship between position of peak retinal nerve fber layer thickness and retinal arteries on sectoral retinal nerve fber layer thickness. *Investig. Ophthalmol. Vis. Sci.* **54**, 5481–5488. <https://doi.org/10.1167/iovs.12-11008>(2013).
- <span id="page-7-7"></span>21. Hood, D. C. *et al.* Blood vessel contributions to retinal nerve fber layer thickness profles measured with optical coherence tomography. *J. Glaucoma* **17**, 519–528.<https://doi.org/10.1097/IJG.0b013e3181629a02> (2008).
- <span id="page-7-8"></span>22. Pereira, I. *et al.* Multivariate model of the intersubject variability of the retinal nerve fber layer thickness in healthy subjects. *Investig. Ophthalmol. Vis. Sci.* **56**, 5290–5298.<https://doi.org/10.1167/iovs.15-17346> (2015).
- <span id="page-7-9"></span>23. Chua, J. *et al.* Multivariable normative comparison, a novel method for improved use of the retinal nerve fber layer thickness to detect early glaucoma. *Ophthalmol. Glaucoma* <https://doi.org/10.1016/j.ogla.2021.10.013>(2021).
- <span id="page-7-10"></span>24. Chua, J. *et al.* Diagnostic ability of individual macular layers by spectral-domain OCT in diferent stages of glaucoma. *Ophthalmol. Glaucoma* **3**, 314–326. <https://doi.org/10.1016/j.ogla.2020.04.003> (2020).
- <span id="page-7-11"></span>25. Chua, J. *et al.* Age-related changes of individual macular retinal layers among Asians. *Sci. Rep.* **9**, 20352. [https://doi.org/10.1038/](https://doi.org/10.1038/s41598-019-56996-6) [s41598-019-56996-6](https://doi.org/10.1038/s41598-019-56996-6) (2019).
- <span id="page-7-12"></span>26. Majithia, S. et al. Cohort profile: The Singapore Epidemiology of Eye Diseases study (SEED). Int. J. Epidemiol. 50, 41-52. [https://](https://doi.org/10.1093/ije/dyaa238) [doi.org/10.1093/ije/dyaa238](https://doi.org/10.1093/ije/dyaa238) (2021).
- <span id="page-7-13"></span>27. Chua, J. et al. Ethnic differences of intraocular pressure and central corneal thickness: The Singapore Epidemiology of Eye Diseases study. *Ophthalmology* **121**, 2013–2022.<https://doi.org/10.1016/j.ophtha.2014.04.041> (2014).
- <span id="page-7-14"></span>28. Mills, R. P. *et al.* Categorizing the stage of glaucoma from pre-diagnosis to end-stage disease. *Am. J. Ophthalmol.* **141**, 24–30. <https://doi.org/10.1016/j.ajo.2005.07.044>(2006).
- <span id="page-7-15"></span>29. Spaeth, G. L. & Shields, M. B. Te stages of glaucoma. *Am. J. Ophthalmol.* **141**, 147–148.<https://doi.org/10.1016/j.ajo.2005.08.026>  $(2006)$ .
- <span id="page-7-16"></span>30. Chua, J. *et al.* Compensation of retinal nerve fbre layer thickness as assessed using optical coherence tomography based on anatomical confounders. *Br. J. Ophthalmol.* **104**, 282–290. <https://doi.org/10.1136/bjophthalmol-2019-314086> (2020).
- <span id="page-7-17"></span>31. Pochet, N. L. & Suykens, J. A. Support vector machines versus logistic regression: Improving prospective performance in clinical decision-making. *Ultrasound Obstet. Gynecol.* **27**, 607–608. <https://doi.org/10.1002/uog.2791> (2006).
- <span id="page-7-18"></span>32. Breiman, L. Random forests. *Mach. Learn.* **45**, 5–32.<https://doi.org/10.1023/A:1010933404324>(2001).
- <span id="page-7-19"></span>33. Friedman, J. H. Greedy function approximation: A gradient boosting machine. *Ann. Stat.* **29**, 1189–1232 (2001).
- <span id="page-7-20"></span>34. Rokach, L. Ensemble-based classifers. *Artif. Intell. Rev.* **33**, 1–39.<https://doi.org/10.1007/s10462-009-9124-7>(2010).
- <span id="page-7-21"></span>35. DeLong, E. R., DeLong, D. M. & Clarke-Pearson, D. L. Comparing the areas under two or more correlated receiver operating characteristic curves: A nonparametric approach. *Biometrics* **44**, 837–845 (1988).
- <span id="page-7-22"></span>36. Chicco, D. & Jurman, G. The advantages of the Matthews correlation coefficient (MCC) over F1 score and accuracy in binary classifcation evaluation. *BMC Genom.* **21**, 6.<https://doi.org/10.1186/s12864-019-6413-7> (2020).
- <span id="page-7-23"></span>37. Fisher, R. A. *Statistical methods for research workers*. 11th edn, (Oliver and Boyd, 1950).
- <span id="page-7-24"></span>38. Burgansky-Eliash, Z. *et al.* Optical coherence tomography machine learning classifers for glaucoma detection: A preliminary study. *Investig. Ophthalmol. Vis. Sci.* **46**, 4147–4152. <https://doi.org/10.1167/iovs.05-0366> (2005).
- <span id="page-7-27"></span>39. Wong, D. *et al.* Factors afecting the diagnostic performance of circumpapillary retinal nerve fbre layer measurement in glaucoma. *Br. J. Ophthalmol.* **105**, 397–402.<https://doi.org/10.1136/bjophthalmol-2020-315985>(2021).
- <span id="page-7-28"></span>40. Azuara-Blanco, A. *et al.* Clinical agreement among glaucoma experts in the detection of glaucomatous changes of the optic disk using simultaneous stereoscopic photographs. *Am. J. Ophthalmol.* **136**, 949–950. [https://doi.org/10.1016/s0002-9394\(03\)00480-x](https://doi.org/10.1016/s0002-9394(03)00480-x) (2003).

#### **Author contributions**

J.C., D.W. and L.S. conceived and designed the study. All authors collected, analyzed, and interpreted the data. J.C., L.C., D.W. and L.S. wrote the main manuscript text. All authors reviewed the manuscript.

#### **Funding**

This work was funded by grants from the National Medical Research Council (CG/C010A/2017\_SERI; OFLCG/004c/2018-00; MOH-000249-00; MOH-000647-00; MOH-001001-00; MOH-001015-00;

MOH-000500-00; MOH-000707-00), National Research Foundation Singapore (NRF2019-THE002-0006 and NRF-CRP24-2020-0001), A\*STAR (A20H4b0141), the Singapore Eye Research Institute & Nanyang Technological University (SERI-NTU Advanced Ocular Engineering (STANCE) Program), and the SERI-Lee Foundation (LF1019-1) Singapore. The funders had no role in the design and conduct of the study; collection, management, analysis, and interpretation of the data; and preparation, review, or approval of the manuscript; and decision to submit the manuscript for publication.

### **Competing interests**

The authors declare no competing interests.

#### **Additional information**

Supplementary Information The online version contains supplementary material available at [https://doi.org/](https://doi.org/10.1038/s41598-023-27783-1) [10.1038/s41598-023-27783-1](https://doi.org/10.1038/s41598-023-27783-1).

**Correspondence** and requests for materials should be addressed to D.W.

**Reprints and permissions information** is available at [www.nature.com/reprints.](www.nature.com/reprints)

**Publisher's note** Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional afliations.

**Open Access** Tis article is licensed under a Creative Commons Attribution 4.0 International  $\odot$ License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit<http://creativecommons.org/licenses/by/4.0/>.

 $© The Author(s) 2023$