



Topographical differences in white matter hyperintensity burden and cognition in aging, MCI, and AD

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Received: 21 April 2022 / Accepted: 17 September 2022 / Published online: 13 October 2022
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Abstract White matter hyperintensities (WMHs) are pathological changes that occur with increased age and are associated with cognitive decline. Most WMH research has not examined regional differences and focuses on a whole-brain approach. This study examined regional WMHs between normal controls (NCs), people with mild cognitive impairment (MCI), and Alzheimer’s disease (AD). We also examined whether WMHs were associated with cognitive decline. Participants from the Alzheimer’s Disease Neuroimaging Initiative were included if they

had at least one WMH measurement and cognitive scores examining global cognition, executive functioning, and memory. Only amyloid-positive MCI and AD participants were included. A total of 1573 participants with 7381 timepoints over a maximum period of 13 years were included. Linear mixed-effects models examined group differences in WMH burden and associations between WMH burden and cognition. People with MCI and AD had increased total and regional WMHs compared to NCs. An association between WMHs and cognition was observed for global cognition, executive functioning, and memory in NCs in all regions. A steeper decline (stronger association between WMH and cognition) was observed in MCI compared to NCs for all cognitive domains in all regions. A steeper decline was observed in AD compared to NCs for global cognition in only the temporal region. A strong association is observed between all cognitive domains of interest and WMH burden in healthy aging and MCI, while those with AD only had a few associations between WMH and global cognition. These findings suggest that the WMH burden is associated with changes in cognition in healthy aging and early cognitive decline.

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Keywords Older adults · Mild cognitive impairment · Alzheimer’s disease · Cognitive decline · White matter hyperintensities

Introduction

Increased age is associated with changes in brain structure and function, which may be typical (i.e., normal) or pathological (i.e., abnormal). These changes may result in the development of cognitive decline, including mild cognitive impairment (MCI) or dementia. Declines in cognitive functioning characterize MCI that are not severe enough to interfere with everyday functioning [1]. When the cognitive decline progresses to interfering with everyday functioning, the impairment is then considered dementia [1]. MCI and dementia prevalence increase with aging and is associated with neurodegenerative brain changes [2, 3]. Alzheimer's disease (AD) is the most common form of dementia, accounting for between 60 and 80% of dementia cases [3].

One common pathological brain change seen in the aging population is the increase in white matter hyperintensity (WMH) burden [4–6]. WMHs are measured as a proxy of cerebrovascular disease and are observed as areas of increased signal in T2-weighted or fluid-attenuated inversion recovery (FLAIR) magnetic resonance images (MRIs) [7]. WMHs are observed in clinically healthy older adults [4–6]; however, WMHs may be one of the first pathological changes associated with cognitive decline in cognitively unimpaired older adults (NCs) [8]. High WMH burden is an indicator of future cognitive decline [9] and progression to MCI and dementia [6, 10, 11].

WMH burden is generally increased in each progressive stage of cognitive decline. That is, WMHs are lower in NCs and progressively increase from MCI to AD [6]. Research examining WMH burden tends to measure global WMH burden as opposed to regional WMH burden [9, 12]. The studies that have observed NC and MCI/AD group differences in regional WMH burden have found differences in all regions. For instance, some studies report that the largest NC-AD group difference in WMH volume is observed in the parietal, temporal, or occipital regions [12–14]. However, previous research notes that WMHs are mostly distributed in both the parietal and frontal lobes [14, 15], with MCI and AD patients also showing increased WMHs in frontal regions relative to controls [14]. The regional distribution of WMHs has also been

suggested to correlate with different etiologies, with anterior WMHs linked to physiological aging and posterior WMHs associated with AD [14, 16]. Finally, increases in WMH volumes in both aging and AD have shown associations with future cognitive decline [6, 10, 11].

Studies examining the relationship between WMH and cognition in aging and AD have shown varying results. Many studies have noted an association between declines in executive functioning [17, 18], memory [17, 19, 20], and global cognition [12, 21] with WMH volumes in aging and MCI/AD, while other studies have observed no association between executive functioning [12], memory [12, 22, 23], and global cognition [24] with WMHs in aging and MCI/AD. A recent meta-analysis examined 22 studies that investigated WMH and cognition in MCI and AD [25]. These authors found a small to medium effect size between cognition and WMH. More specifically, the strongest associations between WMH and cognition were observed with attention, executive functioning, and processing speed. These associations were medium-sized in MCI but small in AD. However, the problem with many of the studies in this review is their cross-sectional nature (only 1 was longitudinal). WMHs are known to be more strongly associated with future cognitive decline than immediate cognitive functioning [9]. Therefore, not examining future cognitive decline is a limitation of these studies. Few of the above-mentioned studies have assessed regional changes longitudinally and compared these regional changes to cognition.

The progressive increase in WMH burden from healthy older adults to people with MCI and people with AD is relatively well established in research. However, spatial WMH distributions and regional effects on domain-specific cognition between the groups remains unknown. Also unexplored is how the association between cognitive change over time and WMH burden in MCI and AD differs from that of cognitively healthy older adults. Using data from the Alzheimer's Disease Neuroimaging Initiative (ADNI), the present study will look to answer these questions by investigating the regional accumulation of WMH burden across amyloid-beta positive ($A\beta$ -positive) adults with AD, $A\beta$ -positive adults with MCI (i.e., those on the AD trajectory), and cognitively healthy older adults. The study will

also examine the association between cognition and regional WMH across groups, both at baseline and over time.

Methods

Alzheimer's Disease Neuroimaging Initiative

The data used in the preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (adni.loni.usc.edu). The ADNI was launched in 2003 as a public–private partnership, led by Principal Investigator Michael W. Weiner, MD. The primary goal of ADNI has been to test whether serial magnetic resonance imaging (MRI), positron emission tomography (PET), other biological markers, and clinical and neuropsychological assessment can be combined to measure the progression of mild cognitive impairment (MCI) and early Alzheimer's disease (AD). The study received ethical approval from the review boards of all participating institutions. Written informed consent was obtained from participants or their study partner. Participants were included from all ADNI cohorts (ADNI-1, ADNI-2, ADNI-GO, and ADNI-3).

Participants

Full participant inclusion and exclusion criteria are available at www.adni-info.org. All participants were between 55 and 90 years of age at the time of recruitment and exhibited no evidence of depression. Healthy older adult controls (NCs) had no evidence of either memory decline, as measured by the Wechsler Memory Scale, or impaired global cognition as measured by the Mini-Mental Status Examination (MMSE) or Clinical Dementia Rating (CDR). MCI participants obtained scores between 24 and 30 on the MMSE, 0.5 on the CDR, and exhibited abnormal scores on the Wechsler Memory Scale. AD participants exhibited abnormal memory function on the Wechsler Memory Scale, obtained an MMSE score between 20 and 26 and a CDR of 0.5 or 1.0, and had probable AD according to the National Institute of Neurological and Communicative Disorders and

Stroke and the Alzheimer's Disease and Related Disorders Association criteria [26].

To ensure that the MCI and AD participants included in this study were in fact MCI due to AD, and AD (as opposed to another form of dementia), they were only included if they were amyloid positive. This selection criterion ensured that both MCI and AD participants were actually on the AD trajectory. Both PET and cerebrospinal fluid (CSF) values were used to determine amyloid positivity in people with MCI and AD because some participants had only one measurement available. Amyloid positivity was identified based on the following criteria: (1) a standardized uptake value ratio (SUVR) of > 1.11 on AV45 PET [27], (2) a SUVR of > 1.2 using Pittsburgh compound-B PET [28], (3) a SUVR of ≥ 1.08 for Florbetaben (FBB) PET [29], or (4) a CSF A β 1-42 ≤ 980 pg/ml as per ADNI recommendations.

A total of 977 MCI and 372 AD participants had WMH measurements with 6524 follow-ups. Of those participants, 564 MCI and 259 AD participants were amyloid positive. The amyloid-positive MCI and AD participants were included in this study along with the 750 NCs, for a total of 1573 participants with 7381 follow-up timepoints. Participants were included from all ADNI cohorts including ADNI-3.

Structural MRI acquisition and processing

All participants were scanned consistently using the standardized acquisition protocols provided by the ADNI. Longitudinal MRI data were downloaded from the ADNI public website. For the detailed MRI acquisition protocol and imaging parameters, see <http://adni.loni.usc.edu/methods/mri-tool/mri-analysis/>. T1w scans for each participant were pre-processed through our standard pipeline including noise reduction [30], intensity inhomogeneity correction [31], and intensity normalization into range [0–100]. The pre-processed images were then linearly (9 parameters: 3 translation, 3 rotation, and 3 scaling) [32] registered to the MNI-ICBM152-2009c average template [33]. The quality of the linear registrations was visually verified by an experienced rater (author M.D.), blinded to the diagnostic

group. Only seven scans did not pass this quality control step and were discarded.

WMH measurements

A previously validated WMH segmentation technique that has been extensively tested for the assessment of WMHs in aging and neurodegenerative diseases was used to obtain WMH measurements. This technique uses nonlinear warping (performed within the toolbox) combined with intensity distribution and spatial priors to perform WMH segmentation. This method has been previously employed in other multi-center studies [8, 9, 34] and has also been validated in the ADNI cohort [35]. Automatic segmentation of the WMHs was completed using only the T1w contrasts, along with location and intensity features from a library of manually segmented scans (50 ADNI participants independent of the ones studied here) in combination with a random forest classifier to detect the WMHs in new images [8, 36]. The decision to use only the T1w images for WMH segmentation was made since the ADNI1 study only includes T1w and T2w/PD images, whereas ADNI2/GO includes T1w and axial 2D FLAIR images and ADNI3 includes T1w and sagittal 3D FLAIRs. Since the resolution of the images (i.e., voxel sizes) was very different between T2w/PD ($1 \times 1 \times 3 \text{ mm}^3$) and FLAIRs ($0.5 \times 0.5 \times 5 \text{ mm}^3$ and $1 \times 1 \times 1.2 \text{ mm}^3$), to be able to reliably combine and use WMH volumes from all these studies, we only used the T1w

images for WMH segmentation. We have previously validated the performance of our pipeline in detecting WMHs based on T1w images both in ADNI and another independent dataset and have shown that the T1w-based WMH volumes (1) hold strong correlations with T2w/PD and FLAIR-based WMH volumes and (2) have similar relationships with clinical/cognitive scores [37]. Finally, the quality of all WMH segmentations was visually assessed by M.D. (blinded to clinical diagnosis), and those that did not pass this quality control step were discarded from the analyses ($N=59$). WMH load was defined as the volume of all voxels identified as WMH in the standard space (in mm^3) and were thus normalized for head size (Fig. 1). Regional and total WMH volumes were calculated based on Hammers Atlas [36, 37]. All WMH volumes were also log-transformed to achieve normal distribution.

A previously validated patch-based label fusion segmentation technique was used to segment the ventricles based on T1w images [38, 39]. The training library of the method includes patients with AD, ensuring that the technique is able to accurately segment the larger ventricles in these patients. The segmentations were visually assessed and those that did not pass this quality control step were excluded for the periventricular (PV) WMH and deep WMH analyses ($N=9$). The ventricle mask was dilated by 8 mm and applied to the WMH masks to calculate PV WMH and deep WMH volumes, i.e., all voxels inside the dilated ventricular mask were taken as PV WMH,

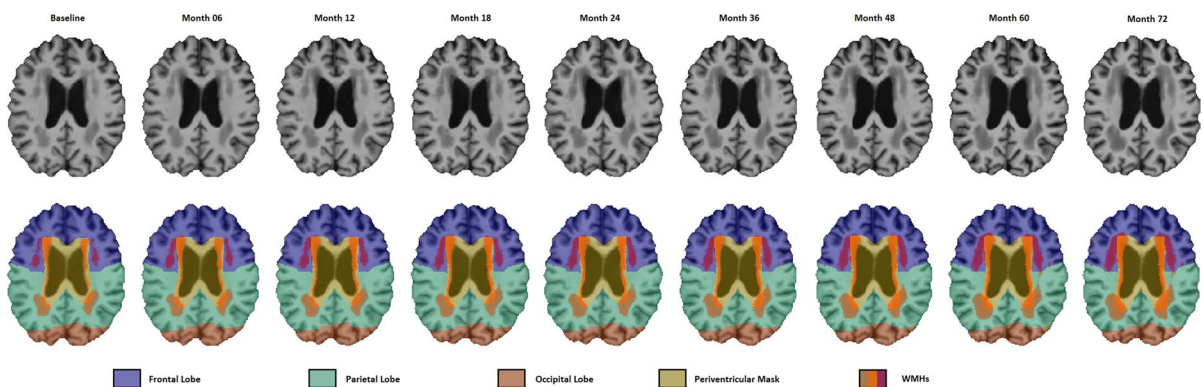


Fig. 1 This image shows the dilated ventricular mask for longitudinal timepoints of one subject (in yellow), overlaid on WMH segmentations. Notes: An example of longitudinally registered T1w images (first row) for a participant with 9 follow-up timepoints (follow-up duration: 72 months). The second row shows the WMHs, dilated ventricle masks, and the lobe masks overlaid on the longitudinally registered images

and all remaining voxels outside the dilated ventricular mask were taken as deep WMH. Figure 1 shows the dilated ventricular mask as well as lobe masks for longitudinal timepoints of one subject (in yellow), overlaid on WMH segmentations.

Cognitive scores

Participant cognitive scores were also downloaded from the ADNI website. The Alzheimer's Disease Assessment Scale-13 (ADAS-13) was included as a measure of global cognitive functioning. Ray's Auditory Verbal Learning test (RAVLT) was included as a measure of episodic memory, and the Trail Making Test Part B (TMT-B) was included as a measure of executive functioning. While other neuropsychological tests were completed throughout ADNI, these three specific tests were included because over 80% of the participants completed these assessments.

Statistical analysis

Baseline assessments

Participant demographic information is presented in Table 1. *T*-tests and chi-square analyses were

performed on the demographic information and corrected for multiple comparisons using Bonferroni correction. The following linear regression models were used to investigate group differences in total, regional, deep, and periventricular WMH loads, including age, sex, years of education, and APOE4 status as covariates

$$\text{Baseline WMH} \sim \text{Age} + \text{Education} + \text{Sex} + \text{Diagnosis} + \text{APOE4} \quad (1)$$

To investigate whether the WMHs were disproportionately distributed across lobes in different diagnostic groups, the lobar WMH volumes (frontal, parietal, temporal, and occipital) were further normalized over the total WMH volume. Similar linear regression models were then completed to investigate whether there were differences in WMH proportions (frontal, temporal, parietal, occipital, total, deep, and periventricular) across groups.

Clinical-anatomical signatures

The partial least squares (PLS) method was used to determine the baseline patterns of association between WMH measures and the cognitive domains in each diagnostic

Table 1 Demographic and clinical characteristics for NCs, MCI, and AD

Demographic information	NC <i>n</i> = 750	MCI <i>n</i> = 564	AD <i>n</i> = 259
Baseline age	73.2 ± 6.2	73.2 ± 7.2	74.2 ± 8.01
Education	16.4 ± 2.6	16.0 ± 2.8 ¹	15.6 ± 2.7 ¹
APOE ε4 +	230 (31%)	349 (62%) ¹	190 (73%) ^{1,2}
Male sex	339 (45%)	332 (59%) ¹	147 (57%) ¹
BMI	26.9 ± 5.1	26.5 ± 4.9	25.6 ± 4.7 ¹
Hypertension	326 (43%)	261 (46%)	130 (50%)
Diabetes	52 (7%)	42 (7%)	19 (7%)
Baseline ADAS13	8.9 ± 4.4	17.3 ± 6.7 ¹	30.6 ± 8.3 ^{1,2}
Baseline TMT-B	81.6 ± 41.2	121.6 ± 68.6 ¹	198.7 ± 85.7 ^{1,2}
Baseline RAVLT-immediate	45.3 ± 9.9	33.0 ± 9.7 ¹	22.4 ± 7.4 ^{1,2}
Baseline RAVLT-learning	6.0 ± 2.4	4.0 ± 2.6 ¹	1.8 ± 1.8 ^{1,2}
Baseline RAVLT-Perc-forgetting	35.6 ± 22.1	64.35 ± 31.1 ¹	88.96 ± 22.1 ^{1,2}

Values are expressed as mean ± standard deviation or number of participants (percentage %). Statistically significant results were reported if they survived Bonferroni correction. ¹Statistically significant difference from NC. ²Statistically significant difference from MCI. *BMI* body mass index, *APOE ε4 +* number and percentage of people with at least one ε4 allele, *NC* normal control, *MCI* mild cognitive impairment, *AD* Alzheimer's disease, *ADAS13* Alzheimer's Disease Assessment Scale-13, *TMT-B* Trail Making Test-B, *RAVLT* Ray Auditory Verbal Learning Test, *Perc-forgetting* percent forgetting. For baseline ADAS-13, TMT-B, and RAVLT-Perc-forgetting, higher scores represent poor performance. For RAVLT-immediate and RAVLT-learning, lower scores represent poor performance

group. PLS is a singular value decomposition-based multi-variate method that relates two sets of variables to each other, by finding the linear combinations of the variables that maximally covary with each other [40–42]. We entered WMH measures, as well as age, sex, years of education, and APOE4 status as the contributing factors, and the scores for ADAS-13, TMT-B, and RAVLT learning, immediate and percent forgetting as the cognitive domain variables. The 500 bootstraps were performed to calculate the effect sizes and confidence intervals for the loadings of contributing factors and cognitive domains for each latent variable. The p values for each latent variable were calculated using permutations ($N=500$).

Longitudinal assessments

WMH differences between NC, MCI, and AD were investigated using linear mixed-effects models to examine the association between WMH load (frontal, temporal, parietal, occipital, total, deep, and periventricular) and diagnosis. Regional WMH values (i.e., frontal, temporal, parietal, and occipital) were summed across the right and left hemispheres to obtain one score for each region. All results were corrected for multiple comparisons using a false discovery rate (FDR), and p values are reported as raw values with significance and then determined by FDR correction [43].

The categorical variable of interest was diagnosis (i.e., NC, MCI, AD) based on baseline diagnosis, contrasting MCI and AD against the NCs. The model also included age, sex, education, and APOE4 status as covariates. The categorical variable apolipoprotein E (APOE4) was used to contrast subjects with one or two APOE $\epsilon 4$ alleles against those with zero. Participant ID was included as a categorical random effect.

$$WMH \sim Age + Education + Sex + Diagnosis + APOE4 + (1|ID) \quad (2)$$

The following linear mixed-effects model was conducted to examine whether total or regional WMH would influence cognitive scores. The variables of interest were diagnosis (contrasting MCI and AD against the NCs), WMH burden, and their interaction (contrasting the slopes of change in cognition in relation to WMH burden for MCI and AD against the NCs). Cognitive measure represents cognitive scores for global functioning, episodic memory, and executive function

$$\begin{aligned} \text{Cognitive Measure} \sim & Age + Education + Sex + WMH : \text{Diagnosis} \\ & + WMH + \text{Diagnosis} + APOE4 + (1|ID) \end{aligned} \quad (3)$$

For follow-up measurements, 1578 participants had follow-up scores over a maximum period of 13 years. WMHs were examined in both a regional approach and overall. Analyses were completed separately for frontal, temporal, parietal, occipital, total, deep, and periventricular WMHs. The model also included age, sex, education, and APOE4 status as covariates. Participant ID was included as a categorical random effect. All continuous values were z-scored within the population prior to the regression analyses.

All statistical analyses were performed using MATLAB version 2021a. To complete the baseline analysis, we used function fitlm and for longitudinal assessments we used fitlme. All models were repeated including risk factors (diabetes, hypertension, and BMI) as additional covariates.

Results

Demographics and cognitive scores

Table 1 presents demographic information and clinical characteristics of the participants included in the study. NCs had significantly greater education levels than both MCI ($t = 3.32$, $p < 0.001$) and AD ($t = 5.21$, $p < 0.001$), fewer males than both MCI ($\chi^2 = 23.51$, $p < 0.001$) and AD ($\chi^2 = 9.84$, $p = 0.001$), and fewer people with APOE $\epsilon 4 +$ than both MCI ($\chi^2 = 146.44$, $p < 0.001$) and AD ($\chi^2 = 188.62$, $p < 0.001$). There were also fewer APOE $\epsilon 4 +$ positive participants in MCI than in AD ($\chi^2 = 9.84$, $p = 0.001$). These effects remained significant after correction for multiple comparisons.

Baseline cognitive performance decreased with each stage of progressive decline for the ADAS-13 (NC:MCI, $t = -25.84$, $p < 0.001$; MCI:AD, $t = -22.41$, $p < 0.001$), TMT-B (NC:MCI, $t = -12.23$, $p < 0.001$; MCI:AD, $t = -12.05$, $p < 0.001$), RAVLT learning (NC:MCI, $t = -14.32$, $p < 0.001$; MCI:AD, $t = 13.59$, $p < 0.001$), RAVLT immediate (NC:MCI, $t = -22.40$, $p < 0.001$; MCI:AD, $t = -17.26$, $p < 0.001$), and RAVLT percent forgetting (NC:MCI, $t = -17.49$, $p < 0.001$; MCI:AD, $t = -12.95$, $p < 0.001$).

Baseline assessments

Figure 2 shows boxplots of baseline WMHs overall and separately for each lobe. As expected, MCI and AD groups had significantly greater WMH burden than the NC group overall and across all regions ($p < 0.01$, Fig. 2, first row). The normalized WMH loads were not significantly different between diagnostic groups across frontal and occipital lobes, whereas parietal WMHs had a disproportionately higher WMH burden ($t = 2.79$, $p = 0.005$) and the temporal WMHs had a disproportionately lower WMH burden ($t = -3.61$, $p < 0.001$) in the AD group in contrast to NC and MCI (Fig. 2, second row).

Clinical-anatomical signatures

The first latent variables were statistically significant for all diagnostic groups (permuted $p < 0.05$) and accounted for 93.78% of the shared covariance between WMHs and cognitive measures for NC, 85.18% of the shared covariance for MCI, and 52.61% of the shared covariance for AD. Figure 3 shows the loadings of the contributing factors (first row) and cognitive domains (second row) for the first latent variables in each diagnostic group (columns). In the NCs, greater age, male sex, lower education, and greater WMH burden in all lobes were associated with poorer

performance in all 5 cognitive domains (indicated by higher scores in ADAS13, TMT-B, and RAVLT percent forgetting, and lower scores in RAVLT immediate and learning). In MCI, a similar WMH pattern emerged; however, RAVLT percent forgetting was no longer statistically significant. In AD, only parietal WMHs, lower education, and RAVLT immediate significantly contributed to the first latent variable.

Longitudinal assessments

WMH analysis of group differences

Table 2 summarizes the results of the longitudinal linear mixed-effects models for MCI and AD, contrasted against NCs across different lobes. Table 3 summarizes the results of the longitudinal linear mixed-effects models for MCI and AD, contrasted against NCs across different WMH measures (total, PV, and deep). MCI (t belongs to [3.25–5.57], $p < 0.001$) and AD (t belongs to [4.76–7.66], $p < 0.001$) had significantly increased WMH load in all regions compared to NCs. In all regions except temporal, people with AD had increased WMH burden compared to MCI (t belongs to [3.60–12.18], $p < 0.001$). No differences were observed between groups in total deep WMH. MCI ($t = 6.74$, $p < 0.001$) and AD ($t = 7.23$, $p < 0.001$) had significantly increased total PV WMH load compared

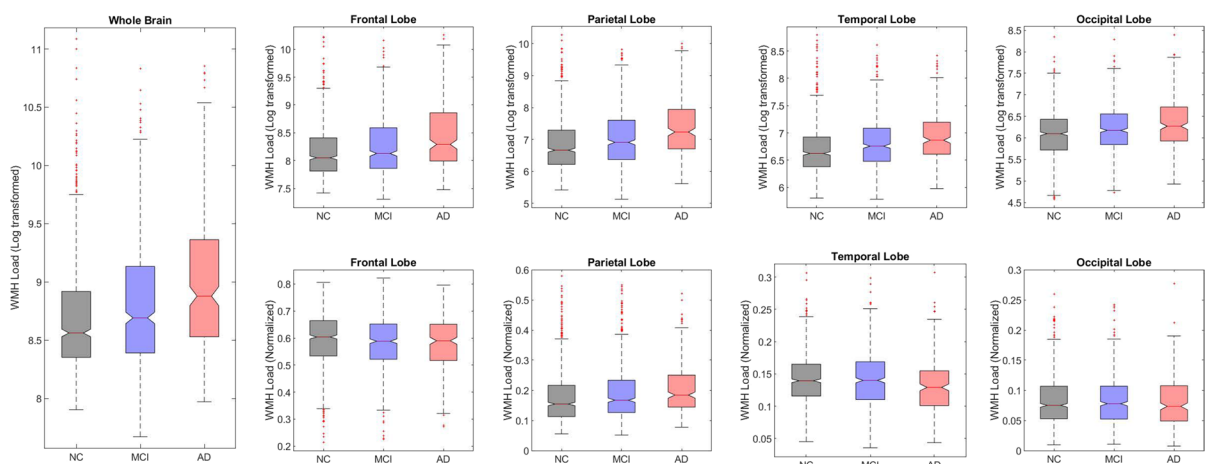


Fig. 2 Boxplots showing baseline WMH distributions. Notes: Baseline WMH distributions (log-transformed and normalized) across diagnostic groups for each lobe. The first row shows the log-transformed WMH loads for each group by lobe. The second row shows the normalized WMH loads for each group by lobe. NC normal controls, MCI mild cognitive impairment, AD Alzheimer's disease, WMH white matter hyperintensity

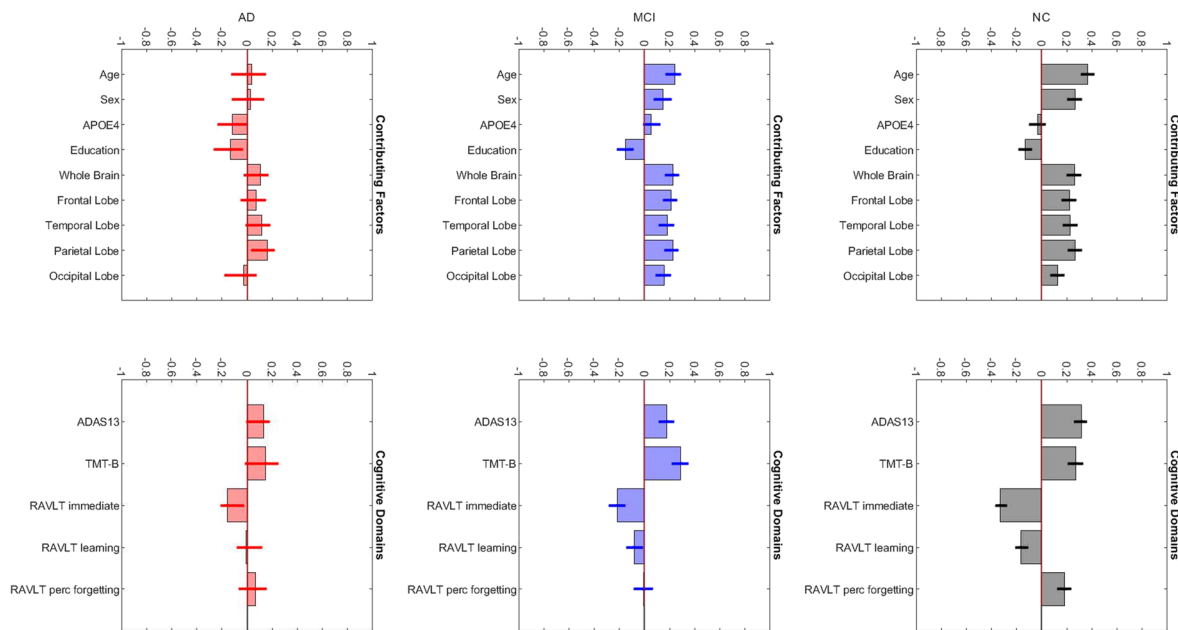


Fig. 3 First latent variables from the parietal least squares analysis. Notes: Each column represents each diagnosis group, Row 1 AD, Row 2 MCI, and Row 3 NC. The first row shows the contributing factors loadings, while the second row shows the cognitive domains for the first latent variables. NC normal controls, MCI mild cognitive impairment, AD Alzheimer’s disease

to NCs. AD ($t=4.65, p=0.03$) had significantly increased total PV WMH load compared to MCI.

Cognition and regional WMH

Table 4 and Fig. 4 summarize the results of the linear mixed-effects models examining the longitudinal relationship between cognitive scores and WMH load. Table 5 summarizes the linear regression model results showing interactions between cognition and total WMH, deep WMH, and PV WMH. For global cognition as measured by ADAS13, there was a significant association with WMH in NC for all regions

except temporal, total deep WMH, and total PV WMH (t belongs to $[3.64–5.33], p<0.001$), demonstrating that increased WMH is associated with increased ADAS13 scores (i.e., worse cognition) in NCs. The interaction between WMH and global cognition was significant for MCI in all regions (t belongs to $[10.45–12.55], p<0.001$), total deep WMH ($t=2.12, p=0.03$), and total PV ($t=8.46, p<0.001$). The interaction between WMH and AD was marginally significant only in the parietal region ($t=2.18, p=0.03$).

For executive functioning as measured by TMT-B, there was a significant association with WMH in

Table 2 Linear regression model results showing differences between NCs, MCI, and AD

	Frontal		Temporal		Parietal		Occipital	
	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>
WMH								
NC vs MCI	5.57	<.001*	4.93	<.001*	5.07	<.001*	3.25	.001*
NC vs AD	7.66	<.001*	5.61	<.001*	6.60	<.001*	4.76	<.001*
MCI vs AD	12.18	<.001*	3.60	.057	7.85	.005*	5.48	.019*

*Results that are significant when uncorrected and bolded values represent those that remained significant after correction for multiple comparisons

Table 3 Linear regression model results showing differences between NCs, MCI, and AD across different WMH measures

	Total WMH		Total deep WMH		Total PV WMH	
	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>
WMH						
NC vs MCI	5.50	<.001*	1.59	0.11	6.74	<.001*
NC vs AD	7.29	<.001*	1.50	0.13	7.23	<.001*
MCI vs AD	10.07	.002*	0.09	0.76	4.65	.03*

*Results that are significant when uncorrected and bolded values represent those that remained significant after correction for multiple comparisons

NC for all regions except total deep WMH, and total PV WMH (*t* belongs to [3.27–6.03], *p* < 0.001, i.e., decreases in executive functioning were associated with increases in WMH burden in all regions). When examining the WMH by diagnosis interaction for executive functioning, there was a significant interaction between MCI and WMH load in all regions

and measures except total deep WMH (*t* belongs to [3.01–6.51], *p* < 0.001), whereas the interactions with AD were not significant in any region (*p* > 0.05). That is, the slopes of changes in executive functioning score associated with WMHs were significantly steeper in MCI (for all regions) but not AD compared to NCs (Fig. 4, second row).

Table 4 Linear mixed model results showing interactions between cognition and WMH at all regions of interest for NCs, MCI, and AD

	Frontal		Temporal		Parietal		Occipital	
	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>
ADAS13								
WMH	4.58	<.001*	1.74	.08	4.68	<.001*	3.64	<.001*
MCI:WMH	12.18	<.001*	10.45	<.001*	11.84	<.001*	12.10	<.001*
AD:WMH	0.86	0.39	1.53	0.12	2.18	0.03*	1.64	0.10
TMT-B								
WMH	5.10	<.001*	3.27	.001*	5.46	<.001*	4.53	<.001*
MCI:WMH	5.96	<.001*	6.23	<.001*	6.41	<.001*	6.51	<.001*
AD:WMH	−1.26	.20	0.36	.71	0.51	.60	1.00	.31
RAVLT-immediate								
WMH	−5.78	<.001*	−3.36	<.001*	−5.98	<.001*	−3.90	<.001*
MCI:WMH	−3.74	<.001*	−3.42	<.001*	−3.78	<.001*	−4.07	<.001*
AD:WMH	2.04	.04	−0.61	.54	1.05	.29	0.25	.79
RAVLT-learning								
WMH	−4.52	<.001*	−3.61	<.001*	−5.81	<.001*	−4.49	<.001*
MCI:WMH	0.77	.43	0.85	.39	1.62	.10	0.91	.36
AD:WMH	2.93	.003*	2.82	.005*	3.35	<.001*	3.53	<.001*
RAVLT-Perc-forgetting								
WMH	5.00	<.001*	3.26	0.001*	5.04	<.001*	4.40	<.001*
MCI:WMH	−0.23	0.81	−0.72	0.47	−1.12	0.26	−0.57	0.56
AD:WMH	−2.21	0.03*	−1.75	0.08	−1.87	0.07	−1.99	0.05

*Results that are significant when uncorrected and bolded values represent those that remained significant after correction for multiple comparisons. WMH white matter hyperintensity, MCI mild cognitive impairment, AD Alzheimer’s disease, ADAS13 Alzheimer’s Disease Assessment Scale-13, RAVLT Ray’s Auditory Verbal Learning test, TMT-B Trail Making Test-B, Perc-forgetting percent forgetting

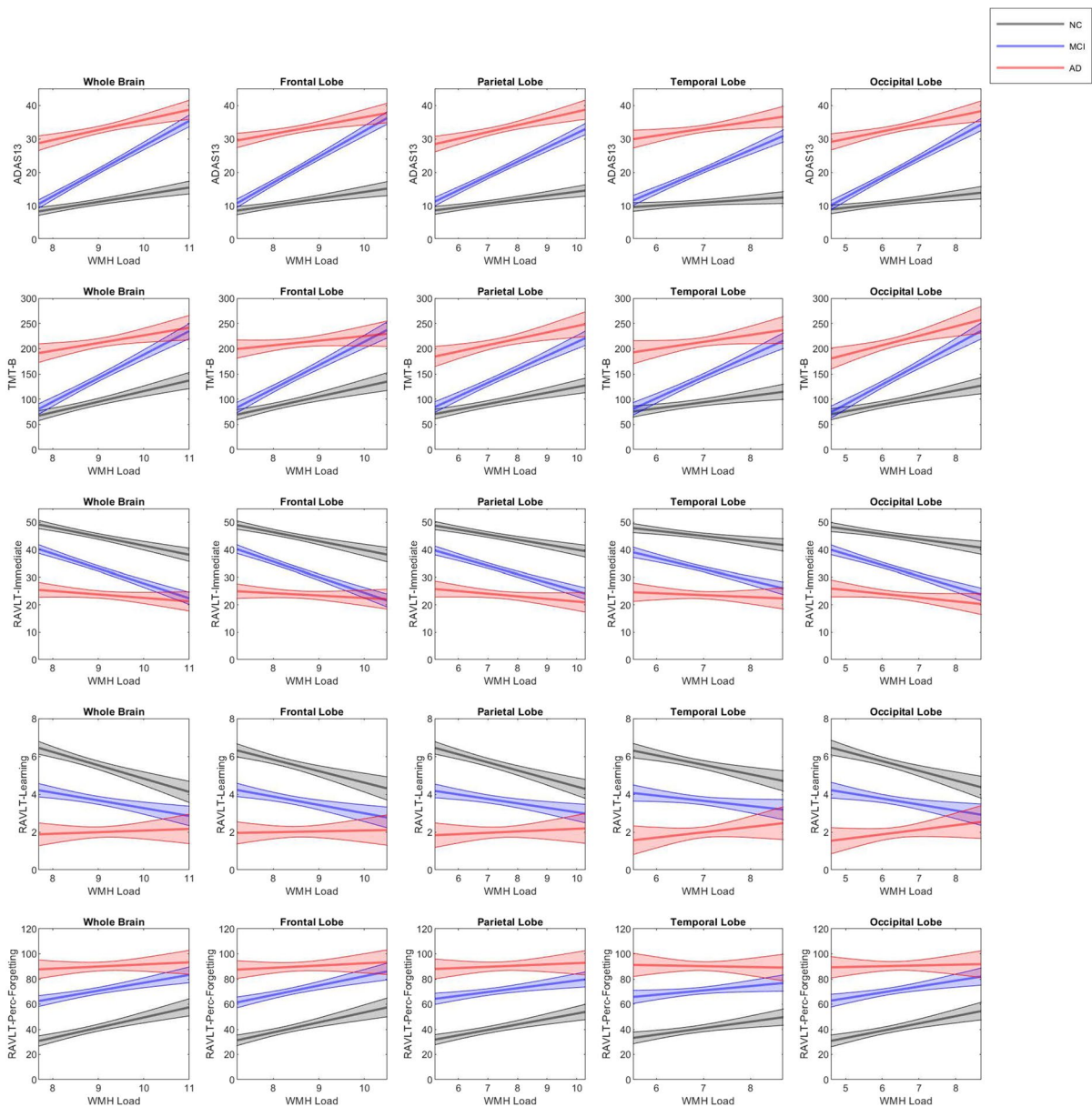


Fig. 4 Figures showing the interactions between cognition and WMH at all regions of interest for NCs, MCI, and AD. Notes: WMH white matter hyperintensity, MCI mild cognitive impairment, AD Alzheimer’s disease, ADAS13 Alzheimer’s Disease Assessment Scale-13, RAVLT Ray’s Auditory Verbal Learning test, TMT-B Trail Making Test-B, Perc-forgetting percent forgetting

For memory, as measured by RAVLT (immediate, learning, and percent forgetting), there was a significant association with WMH in NC for all regions (t belongs to $[-6.43-5.56]$, $p < 0.001$) except total PV WMHs. For NC, increased WMH load was associated with poorer memory performance in all memory

measures. When examining the WMH by diagnosis interaction for RAVLT, there was a significant interaction for MCI and all WMH regions and PV WMHs for RAVLT immediate (t belongs to $[-3.42-4.18]$, $p < 0.001$). For MCI, the slopes of changes in RAVLT immediate were associated with changes in WMH

Table 5 Linear mixed model results showing interactions between cognition and WMH across all measures of interest for NCs, MCI, and AD

	Total WMH		Total deep WMH		Total PV WMH	
	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>	<i>T</i> stat	<i>p</i>
ADAS13						
WMH	5.33	< .001*	1.26	.20	−0.66	.51
MCI:WMH	12.55	< .001*	2.12	.03*	8.46	< .001*
AD:WMH	1.44	.15	−1.04	.29	1.95	.05
TMT-B						
WMH	6.03	< .001*	2.54	.01	0.62	.53
MCI:WMH	6.30	< .001*	0.90	.36	3.01	.002*
AD:WMH	−0.62	.53	−1.61	.10	0.52	.60
RAVLT-immediate						
WMH	−6.43	< .001*	−3.09	.002*	−0.38	.70
MCI:WMH	−3.70	< .001*	0.63	.52	−4.18	< .001*
AD:WMH	1.77	.07	2.92	.003*	−0.70	.48
RAVLT-learning						
WMH	−5.64	< .001*	−3.20	.04	−0.80	.42
MCI:WMH	1.55	.12	2.45	.01*	−0.96	.33
AD:WMH	3.56	< .001*	2.20	.03	1.09	.27
RAVLT-Perc-forgetting						
WMH	5.56	< .001*	2.89	.004*	−1.95	.05
MCI:WMH	−0.95	.38	−1.99	.04	2.40	.01*
AD:WMH	−2.36	.02*	−1.94	.05	0.72	.47

*Results that are significant when uncorrected and bolded values represent those that remained significant after correction for multiple comparisons. *WMH* white matter hyperintensity, *MCI* mild cognitive impairment, *AD* Alzheimer's disease, *ADAS13* Alzheimer's Disease Assessment Scale-13, *RAVLT* Ray's Auditory Verbal Learning test, *TMT-B* Trail Making Test-B, *Perc-forgetting* percent forgetting

that were significantly steeper than NCs in all regions (Fig. 4, third row). For RAVLT learning, there was a significant interaction between MCI and total deep WMHs ($t=2.45$, $p=0.01$) but not for total PV or regional WMHs. For RAVLT percent forgetting, there was a significant interaction between MCI and total PV WMHs ($t=2.40$, $p=0.01$) but not for total deep or regional WMH. AD interaction with WMH burden was not significant in any region ($p>0.05$) for RAVLT immediate. AD significantly interacted with WMH across all regions except total PV WMH measures (t belongs to $[2.82-3.56]$, $p<0.005$) for RAVLT learning, although in the opposite direction, indicating that while WMH burden significantly impacted change in RAVLT learning scores for the NCs, this was not the case in the AD group (note the differences in the slopes in Fig. 4, row 4). For MCI, the slopes of changes in RAVLT learning were associated only with changes in total deep WMH. AD

significantly interacted with WMH in the frontal region ($t=-2.21$, $p=0.03$) and total ($t=-2.36$, $p=0.02$) for RAVLT percent forgetting, but again in the opposite direction, indicating a significantly less steep slope in the AD group compared with the NCs. The less steep slopes for AD in comparison with the NC are likely due to the fact that the AD group has reached the ceiling on poor performance, as reflected in the much higher intercept values for ADAS13, TMT-B, and RAVLT percent forgetting (for which a higher score indicates poorer performance), and lower values for RAVLT immediate and learning (for which a lower score indicates poorer performance).

It should also be noted that all models were repeated including risk factors (diabetes, hypertension, and BMI) as additional covariates and we obtained similar results in terms of effect size and significance. We thus opted to include results from the models that do not include the risk factors.

Discussion

The relationship between WMH and future cognitive decline in aging and cognitive impairment is well established. However, the association between cognitive changes and WMH in specific regions is relatively unexplored and inconsistent. Furthermore, whether cognitive changes are influenced differently by WMHs in aging vs MCI/AD is relatively unknown. The current study was designed to (1) investigate the regional accumulation of WMH burden in cognitively healthy older adults, adults with MCI, and adults with AD and (2) examine the relationship between change in WMH burden and change in cognitive functioning in each group. The study also investigated the impact of regional WMH on cognition across groups. The findings from the present study show that MCI and AD had significantly more WMH burden in all regions compared to NCs. In contrast to NCs, smaller changes in WMH burden in all regions result in a higher impact on declines in global functioning, executive functioning, and RAVLT immediate scores in MCI, as reflected by the steeper slopes observed in MCI.

Compared with the NCs, MCI and AD had increased WMH load in all regions as well as in the whole brain analysis. Research has similarly shown an increase in WMH burden at each progressive stage of cognitive decline [6, 10, 11]. These findings suggest that an increase in widespread WMH pathology occurs in MCI and AD. When examining group WMH differences regionally, studies have typically observed increased WMH in MCI and AD compared to NC in all regions [6, 10, 11]. In line with previous reports, we found a disproportionately greater prevalence of normalized WMHs in the parietal lobe for the AD group. A larger parietal difference is to be expected because parietal WMHs are reflective of AD pathology as opposed to frontal WMHs which are more reflective of normal aging changes [14, 16, 44].

Several previous studies have observed an association between cognitive functioning and WMH burden in aging, cognitive decline, MCI, and AD. However, the results of these studies have been inconsistent and most examine total instead of regional WMH burden [12, 17, 19–21, 23, 24]. Our results show that change in cognition (global functioning, executive functioning, and memory) for NCs was associated with total, frontal, temporal, parietal, and occipital WMH

burden. People with MCI had an increased change in cognition, which was associated with WMHs, that was above what was observed in NC for all cognitive domains, except two components of memory (i.e., RAVLT learning and RAVLT percent forgetting). That is, MCI had increased slopes compared to NC, for all regions and all domains except RAVLT learning and percent forgetting. When examining people with AD, there were fewer interactions between cognition and WMHs.

The results also showed a greater regional association between cognitive functioning and WMH burden. Compared to NCs, AD only had steeper slopes (i.e., increased change in cognition associated with WMHs) for ADAS-13 in the parietal region. For RAVLT percent forgetting and learning, AD exhibited a less steep slope than NCs (in only total and frontal regions) (Fig. 4). The less steep slope observed in AD compared to NCs was not unexpected, because the trajectories inevitably flatten out when the performance of all the participants in the AD group falls in the saturation range of the cognitive scores (see the estimated trajectories for RAVLT percent forgetting as an example — last row in Fig. 4 — for which the AD group started from an average baseline score of 88.96 — Table 1, without much further range remaining to detect worsening performance). That is, the AD participants perform so poorly that the ceiling is reached at baseline; therefore, there is less change in scores over time. This interpretation could explain why other studies have observed minimal associations in AD between cognition and WMHs [12, 22, 23]. These findings suggest WMHs are associated with increased cognitive decline in early aging and prodromal AD (MCI), but only slightly related to changes in AD as detectable by the cognitive batteries currently used. Another potential interpretation that would explain the differences in slopes across the three groups pertains to the presence and impact of other pathologies (i.e., amyloid, tau, and hippocampal neurodegeneration) which may be more strongly related with cognitive deterioration in participants with AD than WMHs. In other words, increased WMH burden contributes to early cognitive decline in aging, but the acceleration in cognitive deterioration, associated with smaller volumetric increases in WMHs, experienced by AD participants, could be driven by

other pathological changes in the brains, which are superimposed to the WMHs.

To examine the influence of hippocampal atrophy, we repeated these analyses adding hippocampal volume as a covariate. The current results obtained did not change to reflect the influence of neurodegeneration; therefore, these results here likely reflect ceiling effects in AD performance. The AD group had a smaller sample size than the NC and MCI. To ensure that the findings were not impacted by sample size differences between the three groups, we repeated the analyses, down sampling the two larger groups to the same sample size as the smallest group, and obtained similar results (in terms of significance of the findings as well as model estimates).

Future research should further explore the limitations of this study. Participants in the ADNI dataset have relatively high education levels and thus may have high cognitive reserve compared to other populations. Future research should aim to examine the influence of WMHs in a population with lower education to determine whether high education levels are protective against cognitive decline caused by WMH burden. The AD participants were in the saturation range of the cognitive scores, and therefore, the memory test employed here (RAVLT) was not able to capture further worsening of this groups' cognition. Future research should employ other cognitive batteries that can better capture cognitive change in those with AD. Several other cognitive tests and domains should be examined to better understand the associations between WMH and cognitive change. For example, the Montreal Cognitive Assessment (MoCA) which is sensitive to cognitive changes in MCI and AD [45] may provide additional insight into the relationship between global cognition and WMHs. However, over 50% of our sample was missing MoCA scores and thus MoCA could not be examined in this study.

In addition to these limitations, there are a few strengths of this study that should also be noted. The image processing tools used to analyze the data in this study were previously designed and validated for use in multi-center and multi-scanner studies. These methods have been extensively used to examine neurodegeneration changes in aging, MCI, and dementia [9, 46]. The sample size used in this study is very large, with an average of 4.7 follow-up timepoints per participant. The large sample size and follow-up periods improve our statistical power and confidence that the

results observed here are an accurate representation of the association between WMH changes with cognition. Finally, our study limited the MCI and dementia patients to those who had confirmed amyloid positivity (using either PET or CSF). This approach is important to show that the dementia participants had an AD diagnosis and that those with MCI were on the AD trajectory. This approach of focusing on only those on the AD trajectory may also explain why some of our results do not match other studies.

Conclusion

The findings from this study show a strong relationship between WMH burden changes and cognition in aging and MCI, with fewer results in AD. WMHs were associated with global cognition, executive functioning, and memory in aging and MCI. A greater prevalence of WMH burden was observed in people with AD in the parietal region. Furthermore, increased change in global cognition associated with WMH burden was also observed for AD (compared to NC), but only in the parietal region. These findings suggest that regional and total WMHs may be a sensitive measure of progressive changes in global cognition, executive functioning, and memory in aging and prodromal AD but not in late-stage AD. The regional association between global cognition in AD suggests that the parietal lobe may be a more specific marker for progressive WMH change in AD. Future work is needed to determine if WMHs can predict cognitive decline in healthy older adults and conversion to AD.

Acknowledgements Data collection and sharing for this project were funded by the Alzheimer's Disease Neuroimaging Initiative (ADNI) (National Institutes of Health Grant U01 AG024904) and DOD ADNI (Department of Defense award number W81XWH-12-2-0012). ADNI is funded by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, and through generous contributions from the following: AbbVie, Alzheimer's Association; Alzheimer's Drug Discovery Foundation; Araclon Biotech; BioClinica, Inc.; Biogen; Bristol-Myers Squibb Company; CereSpir, Inc.; Cogstate; Eisai Inc.; Elan Pharmaceuticals, Inc.; Eli Lilly and Company; EuroImmun; F. Hoffmann-La Roche Ltd and its affiliated company Genentech, Inc.; Fujirebio; GE Healthcare; IXICO Ltd.; Janssen Alzheimer Immunotherapy Research & Development, LLC.; Johnson & Johnson Pharmaceutical Research & Development LLC.; Lumosity; Lundbeck; Merck & Co., Inc.; Meso Scale Diagnostics, LLC.; NeuroRx

Research; Neurotrack Technologies; Novartis Pharmaceuticals Corporation; Pfizer Inc.; Piramal Imaging; Servier; Takeda Pharmaceutical Company; and Transition Therapeutics. The Canadian Institutes of Health Research is providing funds to support ADNI clinical sites in Canada. Private sector contributions are facilitated by the Foundation for the National Institutes of Health (www.fnih.org). The grantee organization is the Northern California Institute for Research and Education, and the study is coordinated by the Alzheimer's Therapeutic Research Institute at the University of Southern California. ADNI data are disseminated by the Laboratory for Neuro Imaging at the University of Southern California.

Data used in the preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (adni.loni.usc.edu). As such, the investigators within the ADNI contributed to the design and implementation of ADNI and/or provided data but did not participate in the analysis or writing of this report. A complete listing of ADNI investigators can be found at http://adni.loni.usc.edu/wp-content/uploads/how_to_apply/ADNI_Acknowledgement_List.pdf

Funding Dr. Morrison is supported by a postdoctoral fellowship from the Canadian Institutes of Health Research, Funding Reference Number: MFE-176608. Dr. Dadar reports receiving research funding from the Healthy Brains for Healthy Lives (HBHL), Alzheimer Society Research Program (ASRP), and Douglas Research Centre (DRC). Dr. Kamal is supported by a postdoctoral scholarship from the Quebec Bio-Imaging Network.

Declarations

Conflict of interest The authors declare no competing interests.

References

- Peterson RC, Caracciolo B, Brayne C, Gauthier S, Jelic V, Fratiglioni L. Mild cognitive impairment: a concept in evolution. *J Intern Med*. 2014;275(3):214–28. <https://doi.org/10.1111/joim.12190>.
- Petersen RC. Mild cognitive impairment. *CONTINUUM: Lifelong Learning in Neurology*. 2016;22(2 Dementia):404. <https://doi.org/10.1002/9781118656082.ch6>.
- Alzheimers Association. What is Alzheimer's disease, (2022). <https://www.alz.org/alzheimers-dementia/what-is-alzheimers>. Accessed Apr 2022.
- Kloppenborg RP, Nederkoorn PJ, Geerlings MI, van den Berg E. Presence and progression of white matter hyperintensities and cognition: a meta-analysis. *Neurology*. 2014 10;82(23):2127–38. <https://doi.org/10.1212/WNL.0000000000000505>.
- Lampe L, Kharabian-Masouleh S, Kynast J, Arelin K, Steele CJ, Löffler M, Witte AV, Schroeter ML, Villringer A, Bazin PL. Lesion location matters: the relationships between white matter hyperintensities on cognition in the healthy elderly. *J Cereb Blood Flow Metab*. 2019;39(1):36–43.
- Yoshita M, Fletcher E, Harvey D, Ortega M, Martinez O, Mungas DM, Reed BR, DeCarli C. Extent and distribution of white matter hyperintensities in normal aging, MCI, and AD. *Neurology*. 2006; 26;67(12):2192–8. <https://doi.org/10.1212/01.wnl.0000249119.95747.1f>.
- Raman MR, Kantarci K, Murray ME, Jack Jr CR, Vemuri P. Imaging markers of cerebrovascular pathologies: pathophysiology, clinical presentation, and risk factors. *Alzheimer's Dement. Diagnosis, Assess. Dis. Monit*. 2016;1;5:5–14. <https://doi.org/10.1016/j.dadm.2016.12.006>.
- Morrison C, Dadar M, Villeneuve S, Collins DL. White matter lesions may be an early marker for age-related cognitive decline. *NeuroImage: Clinical*. 2022;35:103096. <https://doi.org/10.1016/j.nicl.2022.103096>.
- Dadar M, Camicioli R, Duchesne S, Collins DL, Alzheimer's Disease Neuroimaging Initiative. The temporal relationships between white matter hyperintensities, neurodegeneration, amyloid beta, and cognition. *Alzheimer's Dement Diagn Assess Dis Monit* 2020;12(1):e12091. <https://doi.org/10.1002/dad2.12091>.
- Bangen KJ, Preis SR, Delano-Wood L, Wolf PA, Libon DJ, Bondi MW, Au R, DeCarli C, Brickman AM. Baseline white matter hyperintensities and hippocampal volume are associated with conversion from normal cognition to mild cognitive impairment in the Framingham Offspring Study. *Alzheimer Dis Assoc Disord*. 2018;32(1):50. <https://doi.org/10.1097/WAD.0000000000000215>.
- Kim S, Choi SH, Lee YM, Kim MJ, Kim YD, Kim JY, Park JH, Myung W, Na HR, Han HJ, Shim YS. Periventricular white matter hyperintensities and the risk of dementia: a CREDOs study. *Int Psychogeriatrics*. 2015;27(12):2069–77. <https://doi.org/10.1017/S1041610215001076>.
- Garnier-Crussard A, Bougacha S, Wirth M, Dautricourt S, Sherif S, Landeau B, Gonneaud J, De Flores R, de la Sayette V, Vivien D, Krolak-Salmon P. White matter hyperintensity topography in Alzheimer's disease and links to cognition. *Alzheimer's Dement*. 2021:422–423. <https://doi.org/10.1002/alz.12410>.
- Lee S, Viqar F, Zimmerman ME, Narkhede A, Tosto G, Benzinger TL, Marcus DS, Fagan AM, Goate A, Fox NC, Cairns NJ. White matter hyperintensities are a core feature of Alzheimer's disease: evidence from the dominantly inherited Alzheimer network. *Ann Neurol*. 2016;79(6):929–39.
- Brickman AM. Contemplating Alzheimer's disease and the contribution of white matter hyperintensities. *Curr Neurol Neurosci Rep*. 2013;13(12):1–9. <https://doi.org/10.1007/s11910-013-0415-7>.
- Gootjes L, Teipel SJ, Zebuhr Y, Schwarz R, Leinsinger G, Scheltens P, Möller HJ, Hampel H. Regional distribution of white matter hyperintensities in vascular dementia, Alzheimer's disease and healthy aging. *Dement Geriatr Cogn Disord*. 2004;18(2):180–8. <https://doi.org/10.1159/000079199>.
- Habes M, Erus G, Toledo JB, Bryan N, Janowitz D, Doshi J, Völzke H, Schminke U, Hoffmann W, Grabe HJ, Wolk DA. Regional tract-specific white matter hyperintensities are associated with patterns of aging-related brain atrophy via vascular risk factors, but also

- independently. *Alzheimer's Dement Diagn Assess Dis Monit* 2018;10:278–84. <https://doi.org/10.1016/j.dad.2018.02.002>.
17. Cees De Groot J, De Leeuw FE, Oudkerk M, Van Gijn J, Hofman A, Jolles J, Breteler MM. Cerebral white matter lesions and cognitive function: the Rotterdam Scan Study. *Ann Neurol*. 2000;47(2):145–51.
 18. O'Brien JT, Wiseman R, Burton EJ, Barber B, Wesnes K, Saxby B, Ford GA. Cognitive associations of subcortical white matter lesions in older people. *Ann N Y Acad Sci*. 2002;977(1):436–44.
 19. Baune BT, Roesler A, Knecht S, Berger K. Single and combined effects of cerebral white matter lesions and lacunar infarctions on cognitive function in an elderly population. *J Gerontol A Biol Sci Med Sci* 2009;64(1):118–24. <https://doi.org/10.1093/gerona/gln004>.
 20. Kaskikallio A, Karrasch M, Rinne JO, Tuokkola T, Parkkola R, Grönholm-Nyman P. Domain-specific cognitive effects of white matter pathology in old age, mild cognitive impairment and Alzheimer's disease. *Aging Neuropsychol Cogn* 2020;27(3):453–70. <https://doi.org/10.1080/13825585.2019.1628916>.
 21. Tabei KI, Kida H, Hosoya T, Satoh M, Tomimoto H. Prediction of cognitive decline from white matter hyperintensity and single-photon emission computed tomography in Alzheimer's disease. *Front Neurol*. 2017;8:408. <https://doi.org/10.3389/fneur.2017.00408>.
 22. Bracco L, Piccini C, Moretti M, Mascali M, Sforza A, Nacmias B, Cellini E, Bagnoli S, Sorbi S. Alzheimer's disease: role of size and location of white matter changes in determining cognitive deficits. *Dement Geriatr Cogn Disord*. 2005;20(6):358–66. <https://doi.org/10.1159/000088562>.
 23. Gao FQ, Swartz RH, Scheltens P, Leibovitch FS, Kiss A, Honjo K, Black SE. Complexity of MRI white matter hyperintensity assessments in relation to cognition in aging and dementia from the Sunnybrook Dementia Study. *J Alzheimer's Dis*. 2011;26(s3):379–88. <https://doi.org/10.3233/JAD-2011-0058>.
 24. Shenkin SD, Bastin ME, Macgillivray TJ, Deary IJ, Starr JM, Rivers CS, Wardlaw JM. Cognitive correlates of cerebral white matter lesions and water diffusion tensor parameters in community-dwelling older people. *Cerebrovasc Dis*. 2005;20(5):310–8. <https://doi.org/10.1159/000087930>.
 25. Van Den Berg E, Geerlings MI, Biessels GJ, Nederkoorn PJ, Kloppenborg RP. White matter hyperintensities and cognition in mild cognitive impairment and Alzheimer's disease: a domain-specific meta-analysis. *J Alzheimer's Dis*. 2018;63(2):515–27. <https://doi.org/10.3233/JAD-170573>.
 26. Tierney MC, Fisher RH, Lewis AJ, Zoritto ML, Snow WG, Reid DW, Nieuwstraten P. The NINCDS-ADRDA Work Group criteria for the clinical diagnosis of probable Alzheimer's disease: a clinicopathologic study of 57 cases. *Neurology*. 1988;38(3):359–64. <https://doi.org/10.1212/wnl.38.3.359>.
 27. Landau SM, Lu M, Joshi AD, Pontecorvo M, Mintun MA, Trojanowski JQ, Shaw LM, Jagust WJ, Alzheimer's Disease Neuroimaging Initiative. Comparing positron emission tomography imaging and cerebrospinal fluid measurements of β -amyloid. *Ann Neurol* 2013;74(6):826–36. <https://doi.org/10.1002/ana.23908>.
 28. Villeneuve S, Rabinovici GD, Cohn-Sheehy BI, Madison C, Ayakta N, Ghosh PM, La Joie R, Arthur-Bentil SK, Vogel JW, Marks SM, Lehmann M. Existing Pittsburgh Compound-B positron emission tomography thresholds are too high: statistical and pathological evaluation. *Brain*. 2015;138(7):2020–33. <https://doi.org/10.1093/brain/awv112>.
 29. Landau S, Koeppel R, Jagust W, Alzheimer's Disease Neuroimaging Initiative. Florbetaben processing and positivity threshold derivation. Alzheimer's Disease Neuroimaging Initiative. 2011. https://adni.bitbucket.io/reference/docs/UCBERKELEYFBB/UCBerkeley_FBB_Methods_04.11.19.pdf. Accessed Apr 2022.
 30. Coupé P, Yger P, Prima S, Hellier P, Kervrann C, Barillot C. An optimized blockwise nonlocal means denoising filter for 3-D magnetic resonance images. *IEEE Trans Med Imaging*. 2008;27(4):425–41. <https://doi.org/10.1109/TMI.2007.906087>.
 31. Sled JG, Zijdenbos AP, Evans AC. A nonparametric method for automatic correction of intensity nonuniformity in MRI data. *IEEE Trans Med Imaging*. 1998;17(1):87–97. <https://doi.org/10.1109/42.668698>.
 32. Dadar M, Fonov VS, Collins DL, Alzheimer's Disease Neuroimaging Initiative. A comparison of publicly available linear MRI stereotaxic registration techniques. *Neuroimage*. 2018;174:191–200. <https://doi.org/10.1016/j.neuroimage.2018.03.025>.
 33. Fonov V, Evans A, Botteron K, Almli C, McKinstry R, Collins D. BDCG. Unbiased average age-appropriate atlases for pediatric studies. *NeuroImage*. 2011;54(1). <https://doi.org/10.1016/j.neuroimage.2010.07.033>.
 34. Dadar M, Fereshtehnejad SM, Zeighami Y, Dagher A, Postuma RB, Collins DL. White matter hyperintensities mediate impact of dysautonomia on cognition in Parkinson's disease. *Mov Disord Clin Pract*. 2020;7(6):639–47. <https://doi.org/10.1002/mdc3.13003>.
 35. Dadar M, Maranzano J, Ducharme S, Collins DL, Alzheimer's Disease Neuroimaging Initiative. White matter in different regions evolves differently during progression to dementia. *Neurobiol Aging*. 2019;76:71–9. <https://doi.org/10.1016/j.neurobiolaging.2018.12.004>.
 36. Dadar M, Maranzano J, Misquitta K, Anor CJ, Fonov VS, Tartaglia MC, Carmichael OT, Decarli C, Collins DL, Alzheimer's Disease Neuroimaging Initiative. Performance comparison of 10 different classification techniques in segmenting white matter hyperintensities in aging. *NeuroImage*. 2017;157:233–49. <https://doi.org/10.1016/j.neuroimage.2017.06.009>.
 37. Dadar M, Maranzano J, Ducharme S, Carmichael OT, Decarli C, Collins DL, Alzheimer's Disease Neuroimaging Initiative. Validation of T1w-based segmentations of white matter hyperintensity volumes in large-scale datasets of aging. *Hum Brain Mapp*. 2018;39(3):1093–107. <https://doi.org/10.1002/hbm.23894>.
 38. Coupé P, Manjón V, Fonov V, Pruessner J, Robles M, Collins DL. Patch-based segmentation using expert priors: application to hippocampus and ventricle segmentation. *Neuroimage*. 2011;54:940–54.

39. Manera A, Dadar M, Collins DL, Ducharme S. Ventricular features as reliable differentiators between bvFTD and other dementias. *NeuroImage Clin.* 2022;33. <https://doi.org/10.1016/j.nicl.2022.102947>.
40. Abdi H, Williams LJ. Principal component analysis. *Wiley Interdiscip Rev: Comput Stat.* 2010;2(4):433–59.
41. McIntosh AR, Mišić B. Multivariate statistical analyses for neuroimaging data. *Annu Rev Psychol.* 2013;64:499–525.
42. McIntosh AR, Lobaugh NJ. Partial least squares analysis of neuroimaging data: applications and advances. *Neuroimage.* 2004;23:S250–63.
43. Benjamini Y, Hochberg Y. Controlling the false discovery rate: a practical and powerful approach to multiple testing. *J Roy Stat Soc: Ser B (Methodol).* 1995;57(1):289–300.
44. Brickman AM, Zahodne LB, Guzman VA, Narkhede A, Meier IB, Griffith EY, Provenzano FA, Schupf N, Manly JJ, Stern Y, Luchsinger JA. Reconsidering harbingers of dementia: progression of parietal lobe white matter hyperintensities predicts Alzheimer's disease incidence. *Neurobiol Aging.* 2015;36(1):27–32. <https://doi.org/10.1016/j.neurobiolaging.2014.07.019>.
45. Nasreddine ZS, Phillips NA, Bédirian V, Charbonneau S, Whitehead V, Collin I, Cummings JL, Chertkow H. The Montreal Cognitive Assessment, MoCA: a brief screening tool for mild cognitive impairment. *J Am Geriatr Soc.* 2005;53(4):695–9. <https://doi.org/10.1177/0891988716666381>.
46. Dadar M, Gee M, Shuaib A, Duchesne S, Camicioli R. Cognitive and motor correlates of grey and white matter pathology in Parkinson's disease. *NeuroImage Clin.* 2020;27:102353. <https://doi.org/10.1016/j.nicl.2020.102353>.

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