

S1 Appendix. Literature data for wound biochemistry and mechanobiology.

To perform wide-range calibration of our custom FE model, we derive temporal evolutions of the biochemical fields c , ρ , and ϕ_c from published data on full-thickness excisional wounds in wild type mice (diameter: 3–8 mm). Unless numerical values are explicitly reported, we extract them from published charts using the web-based tool ‘WebPlotDigitizer’ [1]. For studies featuring measurement replicates, we focus on their average at each available time point. When multiple data from different studies are available for the same time point, we quantify and display their average and standard deviation (*cf.* Figs. 5-6 and Fig. A1.1).

To inform the temporal evolution of c , we consider TGF- β 1 as a reliable indicator of the second inflammatory wave progression, owing to its undisputed role as the growth factor with the broadest spectrum of actions on cell activity within wound healing [2]. Focusing on experimental studies reporting the evolution of TGF- β 1 throughout healing and the corresponding baseline values in unwounded tissue [2–5], we obtain the temporal evolutions in Fig. A1.1a.

For the cell content, ρ , we focus on previous studies reporting the number of fibroblasts in wounded and unwounded tissue [3,6], and obtain the temporal evolutions in Fig. A1.1b.

For the collagen content, ϕ_c , we consider measurements of wound hydroxyproline content [7–10] and obtain the corresponding collagen amount per mass of wet tissue according to the relation:

$$\phi_c^* = \frac{4H}{0.13\pi D^2 TP}, \quad (\text{A1.1})$$

where H is the hydroxyproline mass measured in a tissue biopsy of diameter D , thickness T , and density P , while 0.13 is a conversion factor corresponding to the typical percentage of hydroxyproline within collagen [11]; in line with previous measurements, we take $P = 1.1 \text{ mg mm}^{-3}$ [12]. Using a similar approach, we also estimate the average collagen content in unwounded murine skin to be $\phi_c^{*,Skin} = 4.9\%$ [9, 13–18], which is remarkably close to recent experimental measurements (6.39% in wet mass) [19] and leads to the normalized wound collagen contents shown in Fig. A1.1c and in Figs.5,6.

For the dependence of cell activity on tissue deformation, we consider previous *in vitro* data on the proliferation of human patellar tendon fibroblasts under uniaxial

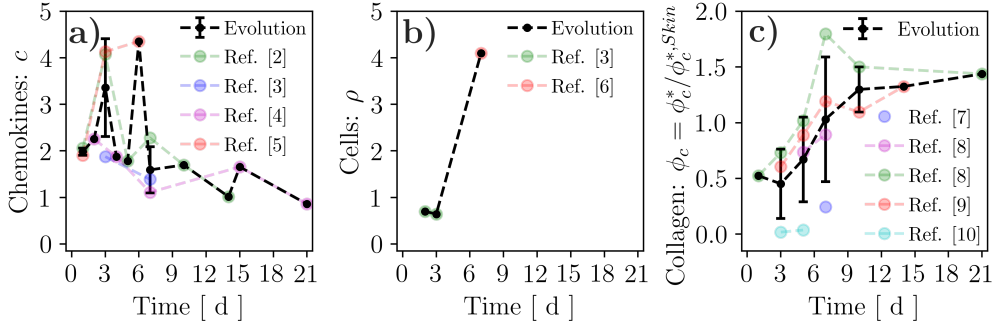


Figure A1.1. Temporal evolution of cytokines, c , cells, ρ , and collagen content, ϕ_c , according to several published studies (colored translucent dots connected by dashed lines showing trends). The data points for comparison with simulations are obtained by averaging information at corresponding time points, as obtained from different studies (black dots and error bars: mean \pm standard deviation; dashed lines show trends).

cyclic stretch of increasing magnitude [20]. For comparability with our study, where we simulate tissue biaxial stretching from a physiological deformation state, we assume that the data in Ref. [20] can be interpreted as representative of fibroblast overproduction induced by a tissue overstretching $\theta^e/\theta^{ph} \sim (\lambda^{over}/\lambda^{ref})^2$, where λ^{over} are the uniaxial stretch values used in Ref. [20] and $\lambda^{ref} = 1$ is the corresponding reference value (no stretch). To determine the overexpression of ρ for an unwounded tissue under stretch, we consider the ODE system comprising Eqs. (5–7) and predict the values of c , ρ , and ϕ_c after 210 days of application of an areal deformation θ^e . Specifically, we set $\alpha = 0$ and select all parameters except for $\Omega^m = \Omega_\rho^m = \Omega_{\phi_c}^m$ according to S3 Table and S4Table. Since we are interested in stretch-mediated mechanosensing, we adopt the definition of \hat{H} in Eq. (10). As shown in Fig. A1.2, increasing/decreasing the tissue stretch around its physiological value results in increased/decreased fibroblast production, in a way that depends on the value of Ω^m . Since values of Ω^m in the range of 0.005 – 0.02 well capture the experimental data in Ref. [20], we select $\Omega^m = 0.01$ as the reference value for this study.

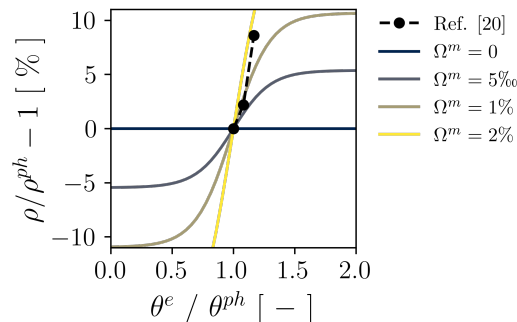


Figure A1.2. Dependence of fibroblast production on tissue stretch for alternative values of the coupling parameter Ω^m , in comparison with experimental data (black dots connected by a dashed line showing trend).

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