

**S4 Table. Parameters for microstructural fields.**

Parameter	Value	Eq.	Source
$p_{\phi_c, n}$ : rate of collagen deposition for $c = 0$ and $\hat{H}_{\phi_c}$	0.002 1/h	7	Ref. [1]
$\Omega_{\phi_c}^b$ : enhanced $\phi_c$ deposition due to cell proliferation	2.5	7	Selected to match peak in $\phi_c$
$\Omega_{\phi_c}^m$ : enhanced $\phi_c$ deposition due to mechanics	$= \Omega_{\rho}^m$	7	Assumed
$K_{\phi_c, c}$ : saturation of collagen due to inflammation	$10^{-4}$	7	Ref. [1]
$K_{\phi_c, \rho}$ : saturation of collagen due to cell proliferation	1.06	7	Ref. [1]
$d_{\phi_c}$ : decay coefficient for collagen content	0.00292 1/h (0.00291 – 0.00330 1/h)	7	From $\phi_c$ homeostasis ( $\dot{\phi}_c = 0$ )
$d_{\phi_c, \rho, c}$ : rate of collagen degradation due to $\rho$ and $c$	$4.85 \times 10^{-4}$ 1/h	7	Ref. [1]
$p_{\xi_c, \phi_c}$ : natural forward rate of collagen crosslinking	1 1/h	18	Assumed
$K_{\xi_c, \phi_c}$ : saturation of crosslinking in response to $\phi_c$	0.5	18	Assumed
$d_{\xi_c}$ : decay coefficient for collagen crosslinking	0.66326 1/h (0.66288 – 0.66327 1/h)	18	From $\xi_c$ homeostasis ( $\dot{\xi}_c = 0$ )
$d_{\xi_c, \phi_c}^-$ : reduction of crosslinking due to $\phi_c$ depletion	1	18	Assumed
$a$ : nonlinearity of the relation between $k_1$ and $\xi_c$	10	17	Selected to match $k_1$ evolution
$d_{\phi_f^w}$ : decay coefficient for wound fibrin content	$= d_{\phi_c}$	15	Assumed
$d_{\phi_f^w, \rho, c}$ : rate of fibrin degradation due to $\rho$ and $c$	0.00325 1/h	15	To have negligible fibrin by d7
$\tau_{\lambda p}$ : time constant for tissue growth	0.485	8	Ref. [1]

## References

1. Buganza Tepole A. Computational systems mechanobiology of wound healing. Computer Methods in Applied Mechanics and Engineering. 2017;314:46–70.