

Supporting Information File 2 for:

Absolute Affinities from Quantitative Shotgun Glycomics Using Concentration-Independent (COIN) Native Mass Spectrometry

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Mathematical model for mixing of two solutions in nanoESI emitter

To provide a theoretical framework to interpret the experimental results, we consider the idealized one-dimensional problem of diffusion in a long capillary of length L and (constant) diameter d – see Figure S2-1. Mimicking experimental conditions, we allow the solute to be transported both by diffusion and also by advection, though we assume that the latter effect is small in a way to be quantified later. Using subscripts to indicate partial differentiation with respect to time (t) and space (x), the equation governing the spatio-temporal evolution of the solute concentration, c , is

$$c_t + uc_x = Dc_{xx}, \quad (1)$$

where D is the diffusion coefficient and u is the advection velocity, which, for analytical convenience, we assume to be constant. Note that $u = Q/(\pi d^2/4)$ in which Q is the volumetric flow rate of the liquid through the capillary. It is advantageous to non-dimensionalize eq 1 by introducing non-dimensional variables for space ξ ($x = \xi L$) and time τ ($t = \tau L^2/D$). Then we can rewrite eq 1 as

$$(c/c_0)_\tau + \text{Pe}(c/c_0)_\xi = (c/c_0)_{\xi\xi}, \quad (2)$$

in which c_0 is the initial solute concentration as measured in the region $x < \ell$ where the horizontal distance ℓ is defined in Figure S2-1. The Peclet number, Pe , is defined as $\text{Pe} = uL/D$.

Eq 2 makes reference to the non-dimensional concentration c/c_0 , however, it is advantageous to consider the evolution of the non-dimensional concentration deficit, defined as $\sigma = 1 - c/c_0$.

Whereas σ solves the same governing equation as c/c_0 , i.e.

$$\sigma_t + \text{Pe} \sigma_\xi = \sigma_{\xi\xi}, \quad (3)$$

we can transform the above equation into a standard heat equation by applying the transformation

$$\sigma(\zeta, \tau) = \exp\left[\frac{1}{2} \text{Pe} \left(\zeta - \frac{1}{2} \text{Pe} \tau\right)\right] v(\zeta, \tau), \quad (4)$$

such that v satisfies

$$v_\tau = v_{\zeta\zeta} \quad (5)$$

Boundary conditions relevant to the above governing equations are as follows. At $x = 0$,

$\zeta = 0$, i.e. on the left-hand side of the capillary,

$$c(0, t) = c_0 \Rightarrow \sigma(0, \tau) = 0 \Rightarrow v(0, \tau) = 0. \quad (6)$$

At $x = L$, $\zeta = 1$, i.e. on the right-hand side of the capillary,

$$c_x(L, t) = 0 \Rightarrow \sigma_\zeta(1, \tau) = 0 \Rightarrow v_\zeta(1, \tau) + \frac{1}{2} \text{Pe} v(1, \tau) = 0. \quad (7)$$

Also, at $t = 0$, $\tau = 0$,

$$c = c_0 [1 - H(x - l)] \Rightarrow \sigma(\zeta, 0) = H\left(\zeta - \frac{l}{L}\right) \Rightarrow v(\zeta, 0) = \exp\left(-\frac{1}{2} \text{Pe} \zeta\right) H\left(\zeta - \frac{l}{L}\right), \quad (8)$$

where H denotes the Heaviside step function.

To solve eq 5, we assume a separable solution of the form

$$v(\zeta, \tau) = X(\zeta)T(\tau). \quad (9)$$

Substitution of eq 9 into eq 5 shows that

$$X_n(\zeta) = A_n \cos \lambda_n \zeta + B_n \sin \lambda_n \zeta, \quad (10)$$

where λ_n is the sequence of eigenvalues with $n = 1, 2, 3$ and A_n and B_n are integration constants. Subsequent application of the left- and right-hand side boundary conditions confirm that $A_n = 0$ whereas the eigenvalues satisfy a transcendental equation of the form

$$\tan \lambda_n = -\frac{\lambda_n}{\frac{1}{2} \text{Pe}} \quad (11)$$

The first (trivial) root of eq 11 is $\lambda_1 = 0$ whereby $\sin \lambda_1 \zeta = 0$. Thereafter, and to good approximation for small Pe,

$$\lambda_2 \approx \frac{\pi}{2} \quad \lambda_3 \approx \frac{3\pi}{2} \quad \lambda_4 \approx \frac{5\pi}{2}. \quad (12)$$

In the interests of maintaining an orthogonal set of basis functions, we consider as a generic solution for X_n :

$$X_n(\zeta) = B_n \sin \left[\left(n - \frac{1}{2} \right) \pi \zeta \right], \quad n = 1, 2, 3, \dots, \quad (13)$$

such that

$$T_n(\tau) = C_n \exp \left[- \left(n - \frac{1}{2} \right)^2 \pi^2 \tau \right]. \quad (14)$$

Combining eq 13 and eq 14 and using superposition yields the small-Pe solution for v

$$v(\zeta, \tau) = \sum_{n=1}^{\infty} b_n \sin \left[\left(n - \frac{1}{2} \right) \pi \zeta \right] \exp \left[- \left(n - \frac{1}{2} \right)^2 \pi^2 \tau \right] \quad (15)$$

where the Fourier coefficients b_n satisfy

$$b_n = 2 \int_0^1 \exp\left(-\frac{1}{2} \text{Pe} \zeta\right) \sin\left[\left(n - \frac{1}{2}\right) \pi \zeta\right] \text{H}\left(\zeta - \frac{l}{L}\right) d\zeta. \quad (16)$$

Using the above solution for v , eq 4 can be solved for σ and the normalized concentration $c/c_0 = 1 - \sigma$ can be found.

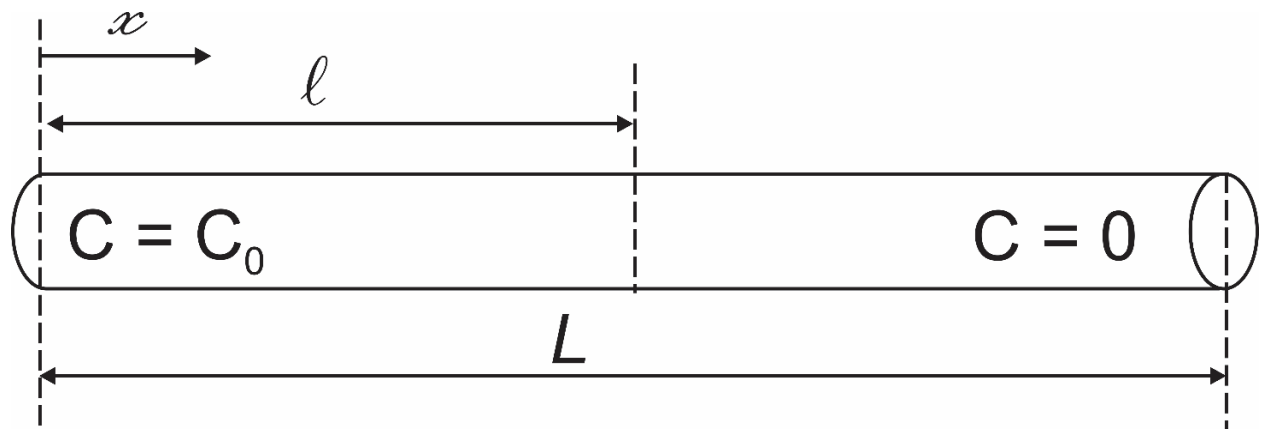


Figure S2-1. Capillary tube schematic. We assume that the solute (whose initial concentration in the region $x < l$ or $\xi < l/L$ is c_0) is transported by a combination of diffusion and (slow) left-to-right advection.