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Supplementary Materials for

Generalizable and replicable brain-based predictions of cognitive functioning across common psychiatric illness

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	HCP-EP	TCP	CNP
	$(n=145)$	$(n=101)$	$(n=224)$
$Age \ (mean, sd)$	23.41(3.86)	32.21(12.54)	32.59(9.21)
Sex (<i>f, %</i>)	57, 38%	50, 57%	95, 42%
Head motion (mm,	.06(.04)	.09(.05)	.08(.03)
sd)			
Diagnosis			
SZ^*	62	4	37
SZAD	8	\mathfrak{Z}	0
MDD	5	22	0
<i>BD</i>	20	9	40
ANX^*	0	5	0
ADHD	0	0	37
OCD	0	0	0
PTSD	0	7	0
SUD			0
ED	0	2	0
None (HC)	52	48	110

Supplementary Table 1 – Sample demographics

Acronyms: HCP-EP = Human Connectome Project – Early Psychosis, TCP = Transdiagnostic Connectomes Project, $CNP = UCLA$ Consortium for Neuropsychiatric Phenomics, $SZ =$ Schizophrenia, SZAD = Schizoaffective Disorder, MDD = Major Depressive Disorder, BD = Bipolar Disorder, ANX=Anxiety Disorder, ADHD = Attention Deficit Hyperactivity Disorder, $OCD =$ obsessive Compulsive Disorder, PTSD = Post-Traumatic Stress Disorder, SUD = Substance Use Disorder, HC = Healthy Control.

**Includes all Schizophrenia Spectrum Diagnosis, except Schizoaffective Disorder *Includes Generalized Anxiety Disorder and Specific Phobia*

Supplementary Table 2 - Cognitive tests for each clinical dataset and loadings on the first principal component.

HCP-EP	loading	TCP	loading	CNP
nih_picseq_unadjusted	0.230	choice_rt_score*	0.282	cvlt_sd_free_recall
nih_dccs_unadjusted	0.222	cont_concent_score*	-0.028	cvlt_sd_cued_recall
nih_flanker_unadjusted	0.235	digit_symbol_score*	0.474	cvlt_ld_free_recall
nih_tpvt_uss	0.275	fast_react_score*	0.439	cvlt_ld_cued_recall
nih_patterncomp_unadjusted	0.161	matrix_reasonscore*	0.348	cvlt_ld_recognition
nih_lswmt_uss	0.261	read_mind_score*	0.227	wms_vr_immediate_recall
nih_orrt_tbx_reading_score	0.267	recog_emo_score*	-0.011	wms_vr_delayed_recall
nih_fluidcogcomp_unadjusted	0.304	hammer_tot_meanRT^	-0.453	wms_vr_recognition
nih_crycogcomp_unadjusted	0.292	stroop_tot_meanRT^	-0.352	wms_symbol_span
nih_eccogcomp_unadjusted	0.328			wms_digit_span_fwd
nih_totalcogcomp_unadjusted	0.346			wms_digit_span_bwd
wasi_profilesubtest_verbalv	0.248			wms_digit_span_seq
wasi_profilesubtest_performancemr	0.230			wais_letter_number_sequ
wasi_iqscores_full2iq	0.289			wais_vocabulary
				wais_matrix_reasoning
				dkefs_verbal_fluency_engl
				taskswitch_interference
				taskswitch_switch_cost
				taskswitch_residual_switch
				ant_rt_conflict
				color_trail_interference
				cpt_hit_rate
				cpt_false_alarm_rate
				cpt_hits_rt

Supplementary Figure 1 – Model performance and generalizability assessed using Coefficient of Determination (COD). A) Prediction performance (COD between observed and predicted values) using kernel ridge regression (red) and meta-matching (blue) across three transdiagnostic datasets: Human Connectome Project – Early Psychosis (HCP-EP), Transdiagnostic Connectomes Project (TCP) and UCLA Consortium for Neuropsychiatric Phenomics (CNP). Generalizability matrix for the kernel ridge regression (B; KRR) and meta-matching (C; MM) models, showing the prediction performance between the independent samples, where the model is trained in one dataset and then used to make predictions in an independent dataset. The diagonal represents the mean prediction performance within each dataset, which is also represented by the black dots in panel A.

and differences in generalizability between KRR and meta-matching (MM) models (right).

Supplementary Figure 3 – Scatterplots of observed and predicted cognition scores for generalizability of the meta-matching model.

A | Region predictive features classified into 17 networks

B | Region predictive features classified into 7 networks

Supplementary Figure 4 – Regional predictive features classified into 17 (A) and 7 (B) network solutions, as well as aggregated across all three studies (HCP-EP, TCP, CNP) using a 7 network solution (C) and ordered by strongest to weakest mean predictive feature weight.

Supplementary Figure 5 – Edge-level predictive feature weights for each dataset

Supplementary Figure 6 - Model performance after regressing out age, sex and head motion (mean FD)

Supplementary Figure 7 - Correlation between edge-level feature weights for original and covariate adjusted meta-matching models.

Supplementary Figure 8 –Feature weights associated with 67 health, demographic and behavioral variables using the stacking component of the meta-matching model.

Supplementary Figure 9 – Model performance (Top) and feature weights (bottom) associated with 64 health, demographic and behavioral variables using the stacking component of the metamatching model (after removing age, sex, and gene PC1 from the meta-matching model).

SFig10 – Leave-One Out -Cross Validation (LOO-CV) results. Points colored by diagnosis, sex, and age. F=Female; M=Male; Anx=Anxiety Disorder; BD=Bipolar Disorder; ED=Eating Disorder; HC=Healthy Control; MDD=Major Depressive Disorder; SUD=Substance Use Disorder; SZ=Schizophrenia; SZAD=Schizoaffective Disorder; ADHD=Attention Deficit Hyperactivity Disorder. See 'Control Analyses' for further details of sub-group analysis.

Supplementary Figure 11 – All FDR-corrected network level feature weights.

Supplementary Figure 12 – Cross-dataset generalizability after removing schizophrenia patients from CNP dataset.

SFig 13 – A) Model performance after removing all heathy control participants from each sample. Generalizability of meta-matching (B) and KRR (C) models after removing all heathy control participants from each sample. $* = p < 0.05; ** =$ $p<0.001$; *** = $p<0.0001$; ns= $p>0.05$) and black ^ denotes statistically significant difference between models.

Additional Information on TCP dataset

The MRI data for the Yale University and McLean Hospital sites are collected at the FAS Brain Imaging Center and McLean Hospital Brain Imaging Center, respectively. The purpose of this study is to collect brain imaging and behavioral data from a transdiagnostic cohort of patients with common psychiatric diagnoses, as well as control participants. An open release of the TCP dataset is planned for 2024 (NDA ID: 3552). Participants are recruited from the community via flyers, online advertisements and through patient referral from clinicians. All participants complete a clinical interview and an MRI scanning session. Participants were eligible for the study if they 1) were aged between of 18-65, 2) had no MRI contraindications, 3) were not colorblind, and 4) had no neurological abnormalities. All participants underwent Structured Clinical Interview for DSM-5 to determine psychiatric diagnosis. As a result, recruitment included both healthy individuals and individuals with a diverse set of clinical presentations, including affective and psychotic psychopathology.

Additional Information on MRI processing and denoising

For the UK Biobank, we used the processed volumetric rs-fMRI data from the first imaging $visit(1)$. Each fMRI dataset was spatially normalised to MNI152 2-mm template space and FMRIB's ICA-based X-noiseifier ((FSL-FIX; *2*)) was trained on holdout set of participants and applied to the remaining participants to denoise the data. The mean global signal was extracted using a whole-brain mask and was regressed out of each dataset. A detailed outline of the processing, denoising and quality control of these data has been previously reported (*1*).

For the CNP data set, *fmriprep* v1.1.1(*3*) was used. During this standardised and automated pipeline, each T1-weighted (T1w) volume was corrected for intensity non-uniformity using N4BiasFieldCorrection(*4*) and skull-stripped using antsBrainExtraction.sh. Brain surfaces were reconstructed using recon-all from [FreeSurfer](https://www.sciencedirect.com/topics/medicine-and-dentistry/freesurfer) v6. Spatial normalization to the MNI152 Nonlinear Asymmetrical template version 2009c was performed through nonlinear registration with ANT_s(5), using brain-extracted versions of both T1w volume and template. Brain-tissue segmentation of tissue classes was performed on the brain-extracted T1w using FSL FAST(*6*). Functional MRI data were slice-time corrected using AFNI(*7*) and realigned to a mean reference image using mcflirt(*8*). Susceptibility distortion correction was performed by co-registering the functional image to the intensity-inverted T1w image with an representative EPI distortion atlas(*9*). This was followed by co-registration to the corresponding T1w using boundary-based registration, implemented using FreeSurfer's BBRegister. The motion-correcting transformations, fielddistortion-correcting warp, BOLD-to-T1w transformation, and T1w-to-MNI warp were concatenated and applied in a single step using ANTS. ICA-based Automatic Removal Of Motion Artifacts (AROMA) was used to generate signal and noise and signal regressors for use in the nonaggressive variant of the method(*10*). Regressors were calculated on the spatially smoothed output 6 mm FWHM kernel) and then applied to the unsmoothed pre-processed file. Following ICA-AROMA, we extracted mean time courses from eroded masks of the WM and CSF and regressed these signals out of the ICA-AROMA denoised data. Finally, each dataset was detrended with a 2nd order polynomial and high-pass filtered at 0.005 Hz using AFNI's 3dTproject. The mean

global signal was extracted using a whole-brain mask and was regressed out of each dataset. Further details on processing, denoising and quality control, please see are reported elsewhere(*11*).

Both the HCP-EP and TCP datasets were acquired use the Human Connectome Project (HCP) MRI acquisition parameters. We therefore implemented the Minimal Processing Pipeline which was developed and optimized for HCP data(*12*). The pipeline adapts steps from FMRIB Software Library ((FSL; *13*)) and FreeSurfer to account for greater spatial and temporal resolution and HCPdata related distortions resulting from acquisition choices such as multiband acceleration, while aiming to remove the least amount of data necessary. During this pipeline, brain surfaces were reconstructed using recon-all from FreeSurfer v6. Skull stripped T1w and fMRI data were aligned using FSL Linear Image Registration Tool (FLIRT). Spin Echo EPI Field Maps with opposite phase encoding directions were used to estimate spatial distortion, using FSL topup and FLIRT was used to correct the scans for such distortions. This process was fine-tuned and optimised using FreeSurfer's BBRegister. Functional MRI data realigned to a mean reference image using mcflirt(*8*). Lastly, non-linear registration of Functional MRI data, aligned to individual's structural volume space into standard MNI152 space was done using FLIRT and FMRIB's nonlinear image registration tool (FNIRT). To denoise the fMRI data, ICA-FIX was implemented. During ICA-FIX, the fMRI data is decomposed into spatially independent components using Multivariate Exploratory Linear Optimized Decomposition into Independent Components (MELODIC). The resulting components are then classified as noise or signal. While ICA-AROMA uses a set of fixed rules depending on the time-course and frequency of each component, ICA-FIX uses a machine-learning based classifier. Here we used the pre-trained HCP_hp2000 classifier provided with ICA-FIX(*2*), as the acquisition parameters of the fMRI data this classifier was train on are identical to those of the HCP-EP and TCP datasets. A temporal high-pass filter of 2000 was applied and a lenient threshold component labelling in FIX $(t=10)$ was used. Finally, the mean global signal was extracted using a whole-brain mask and was regressed out of each dataset.

The steps described above resulted in processed and denoised fMRI dataset in MNI152 volume space for each individual. For each fMRI dataset, the time series were averaged within each of the 400 cortical(*14*) and 19 subcortical(*15*) parcels and pairwise Pearson's correlations were computed to generate a 419×419 functional connectivity matrix, after which correlation values were zscored and the upper-triangle of this matrix which consisted of 87,571 unique functional connectivity estimates were entered into the prediction models.

Meta-matching DNN variable selection procedure

To obtain the final set of 67 phenotypes we followed the exact procedure outlined in (*16*), and began by extracting all 3,937 unique phenotypes available under UK Biobank resource application 25163. We then performed three stages of selection and processing:

Stage 1: we removed non-continuous and non-integer data fields (date and time converted to float), except for sex, brain MRI phenotypes (category ID 100), first repeat imaging visit (instance 3), first two instances (instances 0 and 1) if first imaging visit (instance 2) exists and first imaging visit (instance 2) if participants were more than double of participants from instances 0 or 1, first instance (instance 0) if only the first two instances (instances 0 and 1) exist and instance 1 participants were more than double of participants from instance 0, phenotypes for which fewer than 2,000 participants had RSFC data, behaviors with the same value for more than 80% of participants. After the first stage of filtering, we were left with 701 phenotypes.

Stage 2: It is likely that not all phenotypes are predictable using FC. Therefore, in the second stage, our goal was to remove phenotypes that could not be predicted accurately even with a large number of participants. Therefore, we randomly selected 1,000 participants from 37,848 participants. These 1,000 participants were completely excluded from the main experiments. Using these 1,000 participants, KRR was used to predict each of the 701 phenotypes using RSFC. To ensure robustness, we performed 100 random repeats of training, validation, and testing (60%, 20%, and 20%, respectively). For each repeat, KRR was trained on the training set, and hyperparameters were tuned on the validation set. We then evaluated the trained KRR on the test set. Phenotypes with an average test prediction performance (Pearson's correlation) less than 0.1 were removed. At the end of this second stage, 265 phenotypes were left. See (*16*)for a list of selected and removed UK Biobank phenotypes.

Stage 3: Many of the remaining phenotypes were highly correlated. PCA was performed separately on each subgroup of highly similar phenotypes in the 1,000-participant sample. Similarity was evaluated based on the UK Biobank-provided categories of item sets (that is, items under the same category were considered highly similar). PCAs were not applied to 18 phenotypes (out of 265 phenotypes), which were not similar to other phenotypes. For the purpose of carrying out PCA, missing values were filled in using the expectation–maximization algorithm. For each PCA, we kept enough components to explain 95% of the variance in the data or six components, whichever was lower. Overall, the PCA step reduced the 247 phenotypes (out of 265 phenotypes) to 93 phenotypes. We then repeated the previous step (stage 2) on these 93 phenotypes, resulting in 49 phenotypes with prediction performance (Pearson's correlation) larger than 0.1. Adding back the 18 phenotypes that were not processed by PCA, we ended up with 67 phenotypes used in this manuscript.

The final list of the phenotypes and a brief description of each variable can be found in in Supplementary Table 3.

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