

Biophysical Journal, Volume 98

**Supporting Material**

**A Biophysically-based Mathematical Model for the Kinetics of Mitochondrial Na<sup>+</sup>-Ca<sup>2+</sup> Antiporter**

Ranjan K. Pradhan, Daniel A. Beard, and Ranjan K. Dash

# Supporting Materials for “A Biophysically-based Mathematical Model for the Kinetics of Mitochondrial Na<sup>+</sup>-Ca<sup>2+</sup> Antiporter”

Ranjan K. Pradhan, Daniel A. Beard, and Ranjan K. Dash

Biotechnology and Bioengineering Center and Department of Physiology, Medical College of Wisconsin, Milwaukee, WI-53226

Address for Correspondence: Ranjan K. Dash, Ph.D., Biotechnology and Bioengineering Center, Medical College of Wisconsin, 8701 Watertown Plank Road, Milwaukee, WI 53226-6509, Phone: (414) 955-4497, Fax: (414) 955-6317, E-mail: [rdash@mcw.edu](mailto:rdash@mcw.edu)

## Appendix A: Membrane Potential Dependence of the Kinetic Parameters

The binding of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  to the antiporter and translocation of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  via the antiporter depends on the electrostatic field of the charged membrane. In order to account for this dependency, we assume here that the kinetics parameters  $K_{\text{eq}}$ ,  $K_{\text{Ne}}$ ,  $K_{\text{Nx}}$ ,  $K_{\text{Ce}}$ ,  $K_{\text{Cx}}$ ,  $k_a$  and  $k_b$  depend on the electrostatic potential difference  $\Delta\Psi$  across the membrane. Our approach is similar to that of Metelkin *et al.* (1) on the kinetic modeling of mitochondrial adenine nucleotide translocase (ANT) and Dash *et al.* (2) on the kinetic modeling of mitochondrial  $\text{Ca}^{2+}$  uniporter (CU). This approach is based on biophysical principles as well as laws of thermodynamics, electrostatics, and superposition. In this approach, it is assumed that the total value of the membrane potential is the sum of local electric potentials, each influencing the corresponding stages of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  binding and translocation.

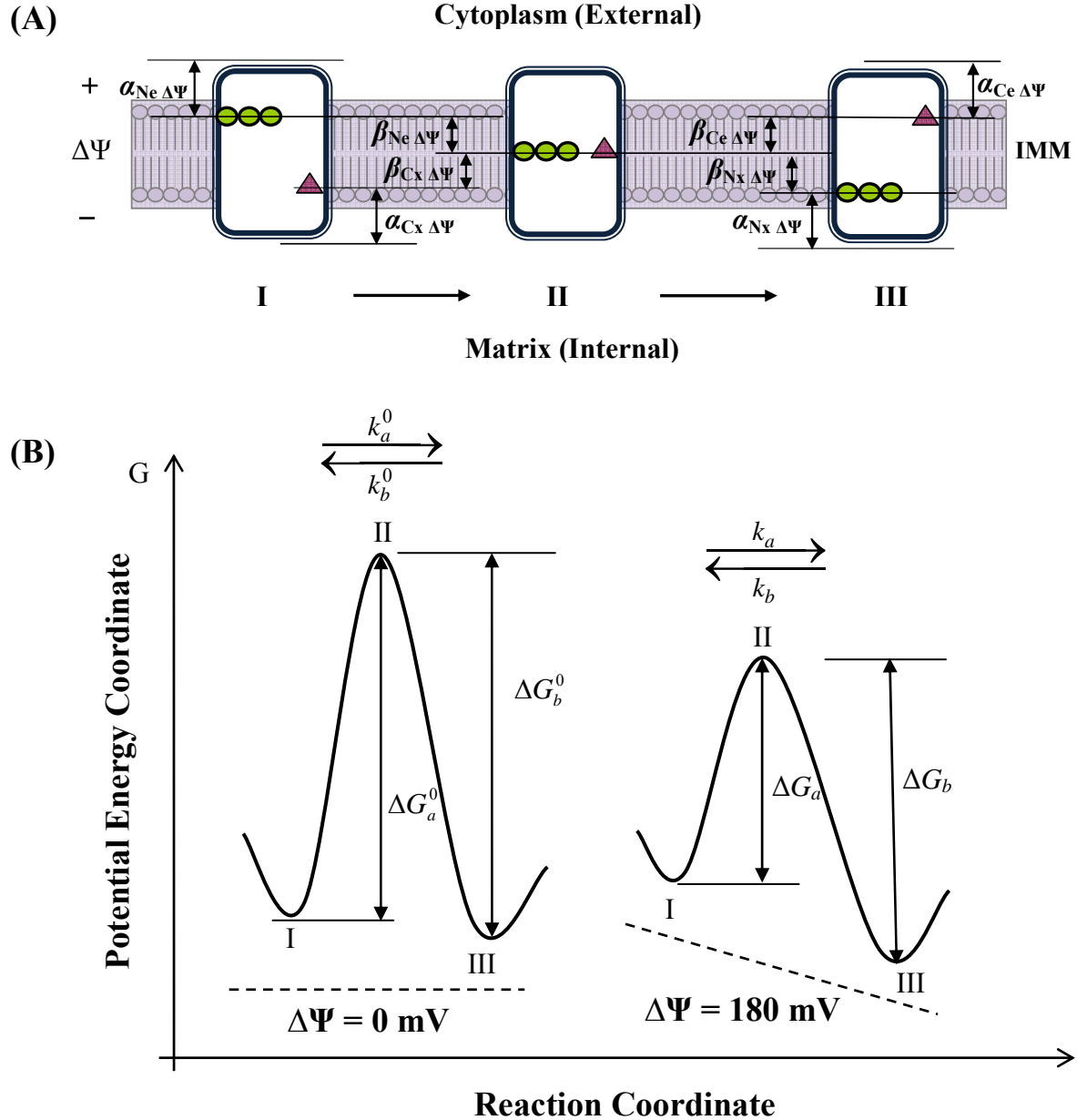
The assumed stages of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  binding to the antiporter and  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  translocation via the antiporter for a  $3\text{Na}^+ : 1\text{Ca}^{2+}$  electrogenic exchange ( $n = 3$ ) are schematized in Figure A1. Every position of  $\text{Na}^+$  or  $\text{Ca}^{2+}$  on the antiporter unit is characterized by an electric potential value. We assume here that the difference in potentials between the adjacent positions of  $\text{Na}^+$  or  $\text{Ca}^{2+}$  is proportional to the total potential difference across the membrane. The sum of potential differences between the consecutive positions of  $\text{Na}^+$  or  $\text{Ca}^{2+}$  is equal to the total potential difference across the membrane. Thus this approach divides the total drop in potential across the membrane into different elementary stages. The scheme described in Figure A1 illustrates the influence of such elementary potential drops on the rate of  $3\text{Na}^+ : 1\text{Ca}^{2+}$  antiporter operation. Values of the potential drops are marked for all elementary stages of the scheme.

**Equilibrium Constant:** As a cycle of antiporter operation for a  $n\text{Na}^+ : 1\text{Ca}^{2+}$  exchange involves translocation of  $n$  elementary positive charges ( $n\text{Na}^+$ ) into the matrix and two elementary positive charges ( $1\text{Ca}^{2+}$ ) out of the matrix, the dependence of the equilibrium constant  $K_{\text{eq}}$  on the membrane potential  $\Delta\Psi$  can be expressed as (Nernst equation)

$$K_{\text{eq}} = \exp[(nZ_{\text{Na}} - Z_{\text{Ca}}) \cdot \Delta\Phi], \quad \Delta\Phi = F\Delta\Psi / RT, \quad (\text{A1})$$

where  $F$ ,  $R$ , and  $T$  denote the Faraday's constant, ideal gas constant, and absolute temperature, respectively;  $Z_{\text{Ca}} = 2$  is the valence of  $\text{Ca}^{2+}$  and  $Z_{\text{Na}} = 1$  is the valence of  $\text{Na}^+$ ;  $\Delta\Phi$  is the non-

dimensional potential difference across the membrane. In the absence of electric field ( $\Delta\Psi = 0$ ), or for a  $2\text{Na}^+ : 1\text{Ca}^{2+}$  electroneutral exchange,  $K_{\text{eq}} = 1$ .



**Figure A1: Free-energy barrier formalism for  $\text{Na}^+$  influx/ $\text{Ca}^{2+}$  efflux via the  $3\text{Na}^+ - 1\text{Ca}^{2+}$  antiporter.** (A:I-III) The consecutive states of  $3\text{Na}^+$  (circle) and  $1\text{Ca}^{2+}$  (triangle) bound antiporter functional unit in the process of  $\text{Na}^+ - \text{Ca}^{2+}$  exchange that is used to derive the dependence of the kinetic parameters on the membrane potential  $\Delta\Psi$ ;  $\alpha_{\text{Ne}}$  ( $\alpha_{\text{Ce}}$ ) represents the ratio of potential difference between  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) bound at the site of antiporter facing the external side of the IMM and  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) in the bulk phase to the total  $\Delta\Psi$ ;  $\alpha_{\text{Nx}}$  ( $\alpha_{\text{Cx}}$ ) represents the ratio of potential difference between  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) bound at the site of antiporter facing the internal side of the IMM and  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) in the bulk phase to the total  $\Delta\Psi$ ;  $\beta_{\text{Ne}}$  ( $\beta_{\text{Ce}}$ ) is the displacement of external  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) from the coordinate of maximum potential barrier;  $\beta_{\text{Nx}}$  ( $\beta_{\text{Cx}}$ ) is the displacement of inter-

nal  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) from the coordinate of maximum potential barrier. (B) The potential energy barrier profile along the reaction coordinate that is used to derive the  $\Delta\Psi$ -dependence of the rate constants. The dashed line shows the profile of the potential created by the electric field of the charged membrane. The points I, II, and III correspond to the  $3\text{Na}^+$  and  $1\text{Ca}^{2+}$  bound antiporter states depicted in the upper panel (A). The rate constants  $k_a$  and  $k_b$  are related to the changes in potential energy (Gibbs free energy)  $\Delta G_a$  and  $\Delta G_b$ . In the absence of electric field ( $\Delta\Psi = 0$  mV), the heights of free energy barriers in the forward and reverse directions are equal when the dissociation constants for the binding of external and internal  $\text{Na}^+$  and  $\text{Ca}^{2+}$  to the antiporter are equal:  $\Delta G_a^0 = \Delta G_b^0 = \Delta G^0$  if and only if  $K_{\text{Ne}}^0 = K_{\text{Nx}}^0 = K_{\text{N}}^0$  and  $K_{\text{Cx}}^0 = K_{\text{Ce}}^0 = K_{\text{C}}^0$ .

**Dissociation Constants:** To derive the dependence of the dissociation constants of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  binding to the antiporter on the membrane potential  $\Delta\Psi$ , let us first consider the binding of external  $\text{Na}^+$  and  $\text{Ca}^{2+}$  to the antiporter. The changes in Gibbs free energies for  $n$  binding reactions of external  $\text{Na}^+$  and one binding reaction of external  $\text{Ca}^{2+}$  are given by

$$\begin{aligned}\Delta\mu_{\text{Ne},p} &= \Delta\mu_{\text{Ne},p}^0 + Z_{\text{Na}}\alpha_{\text{Ne}}F\Delta\Psi + RT \ln\left(\frac{[E(p-1)\text{Na}_e^+][\text{Na}^+]_e}{[E p \text{Na}_e^+]}\right); p = 1, 2, \dots, n, \\ \Delta\mu_{\text{Ce}} &= \Delta\mu_{\text{Ce}}^0 + Z_{\text{Ca}}\alpha_{\text{Ce}}F\Delta\Psi + RT \ln\left(\frac{[E][\text{Ca}^{2+}]_e}{[E\text{Ca}_e^{2+}]}\right),\end{aligned}\quad (\text{A2})$$

where  $\Delta\mu_{\text{Ne},p}^0$  and  $\Delta\mu_{\text{Ce}}^0$  are the changes in standard Gibbs free energies of  $p$ th external  $\text{Na}^+$  and one external  $\text{Ca}^{2+}$  binding reactions, respectively. The parameter  $\alpha_{\text{Ne}}$  is the ratio of potential difference between  $\text{Na}^+$  bound to the site of antiporter facing the cytoplasmic side of the IMM and  $\text{Na}^+$  in the bulk phase to the total membrane potential  $\Delta\Psi$  ( $\Delta\Psi = \Psi_e - \Psi_x$ ; outside potential minus inside potential; so  $\Delta\Psi$  is positive). Similarly,  $\alpha_{\text{Ce}}$  is the ratio of potential difference between  $\text{Ca}^{2+}$  bound to the site of antiporter facing the cytoplasmic side of the IMM and  $\text{Ca}^{2+}$  in the bulk phase to the total membrane potential  $\Delta\Psi$ . An assumption inherent in this model is that all  $\text{Na}^+$  binding sites on the antiporter are at equal distance from the bulk medium. At equilibrium ( $\Delta\mu_{\text{Ne},p} = 0$  and  $\Delta\mu_{\text{Ce}} = 0$ ), Eq. (A2) gives

$$\begin{aligned}K_{\text{Ne},p} &= \left(\frac{[E(p-1)\text{Na}_e^+][\text{Na}^+]_e}{[E p \text{Na}_e^+]}\right)_{\text{eq}} = K_{\text{Ne},p}^0 \exp(-Z_{\text{Na}}\alpha_{\text{Ne}}\Delta\Phi); p = 1, 2, \dots, n, \\ K_{\text{Ce}} &= \left(\frac{[E][\text{Ca}^{2+}]_e}{[E\text{Ca}_e^{2+}]}\right)_{\text{eq}} = K_{\text{Ce}}^0 \exp(-Z_{\text{Ca}}\alpha_{\text{Ce}}\Delta\Phi),\end{aligned}\quad (\text{A3})$$

where  $K_{\text{Ne},p}^0 = K_{\text{Ne},p}(\Delta\Psi = 0) = \exp(-\Delta\mu_{\text{Ne},p}^0 / RT)$  and  $K_{\text{Ce}}^0 = K_{\text{Ce}}(\Delta\Psi = 0) = \exp(-\Delta\mu_{\text{Ce}}^0 / RT)$ . This indicates that the dissociation constants associated with the binding of external  $\text{Na}^+$  as well as external  $\text{Ca}^{2+}$  to the antiporter are reduced (i.e., making the association easier) when  $\Delta\Psi > 0$ , provided  $\alpha_{\text{Ne}}$  and  $\alpha_{\text{Ce}}$  are positive.

Similarly, for the binding of internal  $\text{Na}^+$  and  $\text{Ca}^{2+}$  to the antiporter, we have

$$\begin{aligned}K_{\text{Nx},p} &= \left(\frac{[(p-1)\text{Na}_x^+E][\text{Na}^+]_x}{[p\text{Na}_x^+E]}\right)_{\text{eq}} = K_{\text{Nx},p}^0 \exp(+Z_{\text{Na}}\alpha_{\text{Nx}}\Delta\Phi); p = 1, 2, \dots, n, \\ K_{\text{Cx}} &= \left(\frac{[E][\text{Ca}^{2+}]_x}{[E\text{Ca}_x^{2+}]}\right)_{\text{eq}} = K_{\text{Cx}}^0 \exp(+Z_{\text{Ca}}\alpha_{\text{Cx}}\Delta\Phi),\end{aligned}\quad (\text{A4})$$

where  $K_{\text{Nx},p}^0 = K_{\text{Nx},p}(\Delta\Psi = 0) = \exp(+\Delta\mu_{\text{Nx},p}^0 / RT)$  and  $K_{\text{Cx}}^0 = K_{\text{Cx}}(\Delta\Psi = 0) = \exp(+\Delta\mu_{\text{Cx}}^0 / RT)$ ;  $\Delta\mu_{\text{Nx},p}^0$  and  $\Delta\mu_{\text{Cx}}^0$  are the standard changes in Gibbs free energies of  $n$  internal  $\text{Na}^+$  and one internal  $\text{Ca}^{2+}$  binding reactions, respectively. The parameter  $\alpha_{\text{Nx}}$  is the ratio of potential difference between  $\text{Na}^+$  bound at the site of antiporter facing the matrix side of the IMM and  $\text{Na}^+$  in the bulk

phase to the total membrane potential  $\Delta\Psi$ . Similarly,  $\alpha_{\text{Cx}}$  is the ratio of potential difference between  $\text{Ca}^{2+}$  bound at the site of antiporter facing the matrix side of the IMM and  $\text{Ca}^{2+}$  in the bulk phase to the total membrane potential  $\Delta\Psi$ . In contrast to  $K_{\text{Ne},p}$  and  $K_{\text{Ce}}$ , the dissociation constants  $K_{\text{Nx},p}$  and  $K_{\text{Cx}}$  for binding of internal  $\text{Na}^+$  and internal  $\text{Ca}^{2+}$  to the antiporter are increased (i.e., making the association difficult) when  $\Delta\Psi > 0$ , provided  $\alpha_{\text{Nx}}$  and  $\alpha_{\text{Cx}}$  are positive.

In any of the models derived in the paper (Model 1, Model 2, and Model 3), the dissociation constants  $K_{\text{Ne}}$ ,  $K_{\text{Nx}}$ ,  $K_{\text{Ce}}$ , and  $K_{\text{Cx}}$  can be obtained from Eqs. (A3) and (A4) as

$$\begin{aligned} K_{\text{Ne}} &= K_{\text{Ne}}^0 \exp(-\alpha_{\text{Ne}} Z_{\text{Na}} \Delta\Phi), & K_{\text{Nx}} &= K_{\text{Nx}}^0 \exp(+\alpha_{\text{Nx}} Z_{\text{Na}} \Delta\Phi), \\ K_{\text{Ce}} &= K_{\text{Ce}}^0 \exp(-\alpha_{\text{Ce}} Z_{\text{Ca}} \Delta\Phi), & K_{\text{Cx}} &= K_{\text{Cx}}^0 \exp(+\alpha_{\text{Cx}} Z_{\text{Ca}} \Delta\Phi). \end{aligned} \quad (\text{A5})$$

For simplicity and reducing the number of unknown biophysical parameters, we assume here that  $\alpha_{\text{Ne}} = \alpha_{\text{Ce}} = \alpha_e$  and  $\alpha_{\text{Nx}} = \alpha_{\text{Cx}} = \alpha_x$ , that is, the  $\text{Na}^+$  and  $\text{Ca}^{2+}$  binding sites on the antiporter are located at equal distances from the bulk phase on either side of the IMM. Thus, the four dissociation constants  $K_{\text{Ne}}$ ,  $K_{\text{Nx}}$ ,  $K_{\text{Ce}}$  and  $K_{\text{Cx}}$  are fully characterized by six unknown parameters  $K_{\text{Ne}}^0$ ,  $K_{\text{Ce}}^0$ ,  $K_{\text{Nx}}^0$ ,  $K_{\text{Cx}}^0$ ,  $\alpha_e$  and  $\alpha_x$ , increasing the total number of unknown parameters by two. For positive  $\alpha_e$  and  $\alpha_x$ , the dissociation constants of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  binding tend to decrease on the outside and increase on the inside of the IMM. Also note here that  $K_{\text{Ne}}^0$  and  $K_{\text{Ce}}^0$  can be equal to/distinct from  $K_{\text{Nx}}^0$  and  $K_{\text{Cx}}^0$ , respectively (see Case 1 and Case 2 in the paper).

**Rate Constants:** The dependence of the rate constants  $k_a$  and  $k_b$  on the membrane potential  $\Delta\Psi$  during conformational changes of the antiporter complexes  $\text{Ca}_x^{2+}m\text{H}_x^+En\text{Na}_e^+$  and  $n\text{Na}_x^+Em\text{H}_e^+\text{Ca}_e^{2+}$  can be accounted for by using Eyring's free energy barrier theory for absolute reaction rates (3-5). For simplicity, we assume here that the free energy profile for the translocation of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  across the membrane (the limiting stage) is a single barrier (Figure A1B), and the translocation is a jump over the barrier from one potential well to another. We define the reaction coordinate for  $\text{Na}^+$  translocation as the coordinate from  $\text{Na}^+$  bound at the external side to  $\text{Na}^+$  bound at the internal side of the membrane along the direction of  $\text{Na}^+$  translocation. Similarly, the reaction coordinate for  $\text{Ca}^{2+}$  translocation is defined as the coordinate from  $\text{Ca}^{2+}$  bound at the internal side to  $\text{Ca}^{2+}$  bound at the external side of the membrane along the direction of  $\text{Ca}^{2+}$  translocation. The local maximum or peak (State II) of the free energy profile corresponds to the barrier that impedes the  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  translocation, while the local minima (States I and III) corresponds to the  $\text{Ca}_x^{2+}m\text{H}_x^+En\text{Na}_e^+$  and  $n\text{Na}_x^+Em\text{H}_e^+\text{Ca}_e^{2+}$  states on either side of the membrane. The  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  exchange rate is determined by the probability of the antiporter to translocate  $n\text{Na}^+$  for  $1\text{Ca}^{2+}$  from one binding site to the other in opposite direction, which depends on the height of the free energy barrier, which in turn depends on  $\Delta\Psi$ , as shown in Figure A1B.

According to Eyring's free energy barrier theory, the rate ( $k$ ) at which an ion can jump from one binding site to other is given by

$$k = (\kappa_B T / h) \exp(-\Delta G / RT), \quad (\text{A6})$$

where  $\Delta G$  is the height of the free energy barrier;  $k_B$  is Boltzmann's constant;  $h$  is Planck's constant; and  $T$  is the absolute temperature. In this model, the free energy barrier heights (State II to States I and III) can be defined by,

$$\begin{aligned}\Delta G_a &= \Delta G_a^0 - nZ_{\text{Na}}\beta_{\text{Ne}}F\Delta\Psi + Z_{\text{Ca}}\beta_{\text{Cx}}F\Delta\Psi, \\ \Delta G_b &= \Delta G_b^0 + nZ_{\text{Na}}\beta_{\text{Nx}}F\Delta\Psi - Z_{\text{Ca}}\beta_{\text{Ce}}F\Delta\Psi,\end{aligned}\tag{A7}$$

where

$$\begin{aligned}\beta_{\text{Ne}} &= \beta_{\text{Ne}} + \sum_j \frac{\beta_{\text{e},j}Z_j}{nZ_{\text{Na}}}, \quad \beta_{\text{Cx}} = \beta_{\text{Cx}} + \sum_j \frac{\beta_{\text{x},j}Z_j}{Z_{\text{Ca}}}, \\ \beta_{\text{Nx}} &= \beta_{\text{Nx}} + \sum_j \frac{\beta_{\text{x},j}Z_j}{nZ_{\text{Na}}}, \quad \beta_{\text{Ce}} = \beta_{\text{Ce}} + \sum_j \frac{\beta_{\text{e},j}Z_j}{Z_{\text{Ca}}}.\end{aligned}\tag{A8}$$

In Eq. (A7),  $\Delta G_a^0$  and  $\Delta G_b^0$  are the free energy barrier heights in the absence of electric field ( $\Delta\Psi = 0$  mV);  $\beta_{\text{Ne}}$  and  $\beta_{\text{Ce}}$  are the displacements of external  $\text{Na}^+$  and  $\text{Ca}^{2+}$  (State I and State III) from the coordinate of maximum potential barrier (State II);  $\beta_{\text{Nx}}$  and  $\beta_{\text{Cx}}$  are the displacements of internal  $\text{Na}^+$  and  $\text{Ca}^{2+}$  (State III and State I) from the coordinate of maximum potential barrier (State II). Note here that  $\Delta G_a^0 = \Delta G_b^0 = \Delta G^0$  subject to conditions  $K_{\text{Ne}}^0 = K_{\text{Nx}}^0 = K_{\text{N}}^0$  and  $K_{\text{Ce}}^0 = K_{\text{Cx}}^0 = K_{\text{C}}^0$ . For simplicity, the effects of the displacements of other elementary charges that constitute the antiporter on the rate of conformational change has been lumped into the biophysical parameters  $\beta_{\text{Ne}}$ ,  $\beta_{\text{Nx}}$ ,  $\beta_{\text{Ce}}$  and  $\beta_{\text{Cx}}$ , as shown in Eq. (A8). In Eq. (A8), the parameter  $Z_j$  is the valence of the  $j$ th charged species of the antiporter and  $\beta_{\text{e},j}$  and  $\beta_{\text{x},j}$  are the corresponding displacements from the external and internal sides of the antiporter.

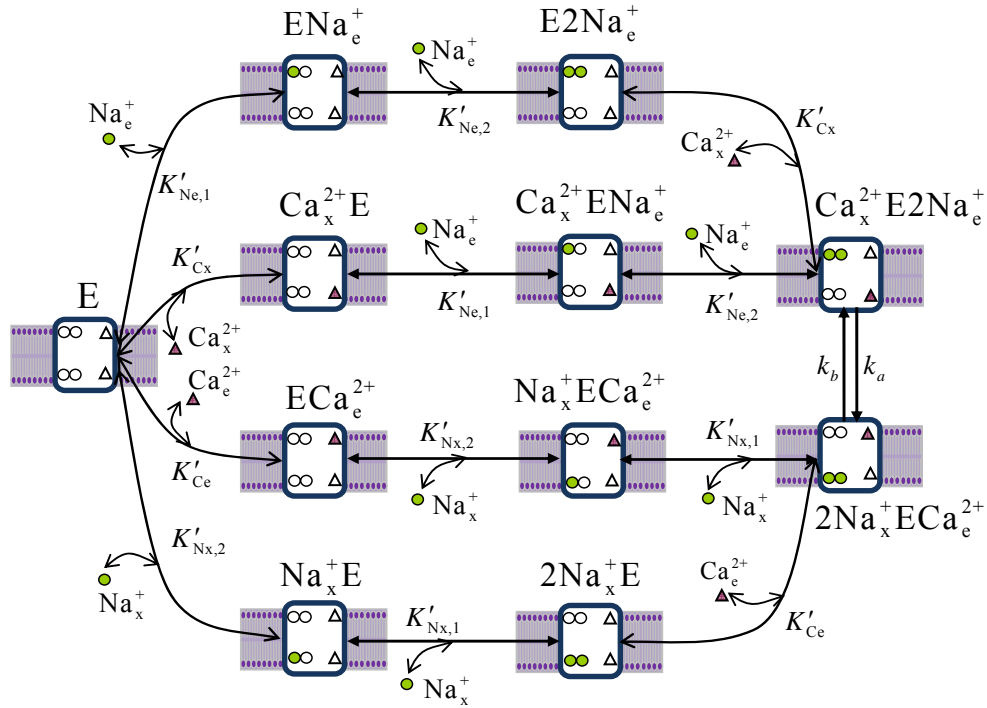
It is evident from Eq. (A7) that the  $\text{Na}^+$  ions tend to decrease the height of the barrier in the inward direction, but increase the height of the barrier in the outward direction, when  $\Delta\Psi > 0$  (see Figure A1B). Similarly, the  $\text{Ca}^{2+}$  ions tend to increase the height of the barrier in the inward direction, but decrease the height of the barrier in the outward direction, when  $\Delta\Psi > 0$ . In other words, it becomes easier for the  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) ions to cross the barrier in the inward (outward) direction, but more difficult for the  $\text{Na}^+$  ( $\text{Ca}^{2+}$ ) ions to exit (enter) the matrix in the presence of a positive membrane potential, measured from outside to inside. Now, substituting Eq. (A7) into Eq. (A6), we obtain the rate constants of  $n\text{Na}^+$  and  $1\text{Ca}^{2+}$  exchange as

$$\begin{aligned}k_a &= k_a^0 \exp[(+n\beta_{\text{Ne}}Z_{\text{Na}} - \beta_{\text{Cx}}Z_{\text{Ca}})\Delta\Phi], \\ k_b &= k_b^0 \exp[(-n\beta_{\text{Nx}}Z_{\text{Na}} + \beta_{\text{Ce}}Z_{\text{Ca}})\Delta\Phi],\end{aligned}\tag{A9}$$

where  $k_a^0 = (\kappa_B T / h) \exp(-\Delta G_a^0 / RT)$  and  $k_b^0 = (\kappa_B T / h) \exp(-\Delta G_b^0 / RT)$  are the forward and reverse rate constants when  $\Delta\Psi = 0$  mV. For simplicity and to reducing the number of unknown biophysical parameters, we assume here that the displacements of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  ions (State I and State III) from the coordinate of maximum potential barrier (State II) are the same on either side of the IMM:  $\beta_{\text{Ne}} = \beta_{\text{Ce}} = \beta_{\text{e}}$  and  $\beta_{\text{Nx}} = \beta_{\text{Cx}} = \beta_{\text{x}}$ . Thus, the two rate constants  $k_a$  and  $k_b$  are fully characterized by four unknown parameters  $k_a^0$ ,  $k_b^0$ ,  $\beta_{\text{e}}$  and  $\beta_{\text{x}}$ , increasing the total number of unknown parameters by two.

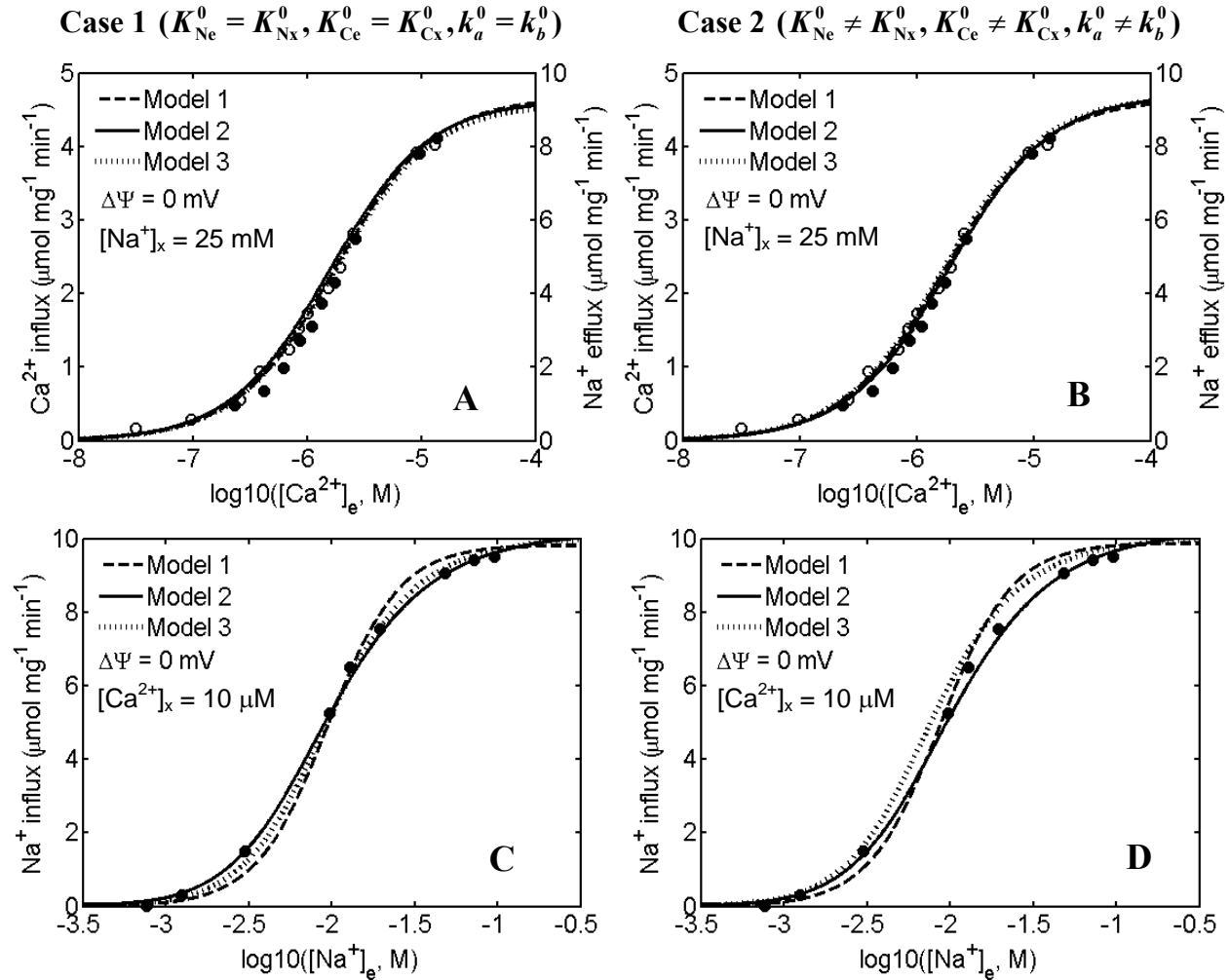
## Appendix B: Model of Mitochondrial $\text{Na}^+$ - $\text{Ca}^{2+}$ Antiporter for $2\text{Na}^+ : 1\text{Ca}^{2+}$ Stoichiometry

This appendix presents three different kinetic models of mitochondrial  $2\text{Na}^+ - 1\text{Ca}^{2+}$  antiporter based on the proposed kinetic mechanism shown in Figure B1. The parameterization of these three kinetic models (Model 1: fully cooperativity, Model 2: partial cooperativity, and Model 3: no cooperativity) under two different model assumptions regarding the magnitudes of the binding constants of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  to the antiporter at the inside and outside of the membrane (Case 1 and Case 2) is done using the experimental data of Paucek and Jaburek (6). The model equations can be easily derived from Eqs. (10-11) with  $n = 2$ , and hence are not shown here. The model specifications and different model assumptions are the same as mentioned in the paper. The fitting of all three models to the experimental data are shown in Figures B2 and B3. The estimated model parameter values are summarized in Table B1.



**Figure B1: Proposed kinetic mechanism of  $\text{Na}^+$ -dependent  $\text{Ca}^{2+}$  efflux from mitochondria via  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporter with a presumed  $2\text{Na}^+ : 1\text{Ca}^{2+}$  stoichiometry.** The antiporter functional unit (E) is assumed to have two binding sites for  $\text{Na}^+$  and one binding site for  $\text{Ca}^{2+}$  facing either side of the inner mitochondrial membrane (IMM). In one process, two  $\text{Na}^+$  ions from the external (cytoplasmic) side of the IMM ( $2\text{Na}_e^+$ ) first cooperatively bind to the unbound antiporter E in two consecutive steps forming the antiporter complex  $\text{E}2\text{Na}_e^+$ . Then, a  $\text{Ca}^{2+}$  ion from the internal (matrix) side of the IMM ( $\text{Ca}_x^{2+}$ ) binds to the complex  $\text{E}2\text{Na}_e^+$  forming the complex  $\text{Ca}_x^{2+}\text{E}2\text{Na}_e^+$ . In another process, a  $\text{Ca}^{2+}$  ion from the matrix side ( $\text{Ca}_x^{2+}$ ) first binds to the unbound antiporter E to form the antiporter complex  $\text{Ca}_x^{2+}\text{E}$ . Then, two  $\text{Na}^+$  ions from the cytoplasmic side ( $2\text{Na}_e^+$ ) cooperatively bind to the complex  $\text{Ca}_x^{2+}\text{E}$  in two consecutive steps to form the complex  $\text{Ca}_x^{2+}\text{E}2\text{Na}_e^+$ . The complex  $\text{Ca}_x^{2+}\text{E}2\text{Na}_e^+$  that is formed via these two distinct processes then un-

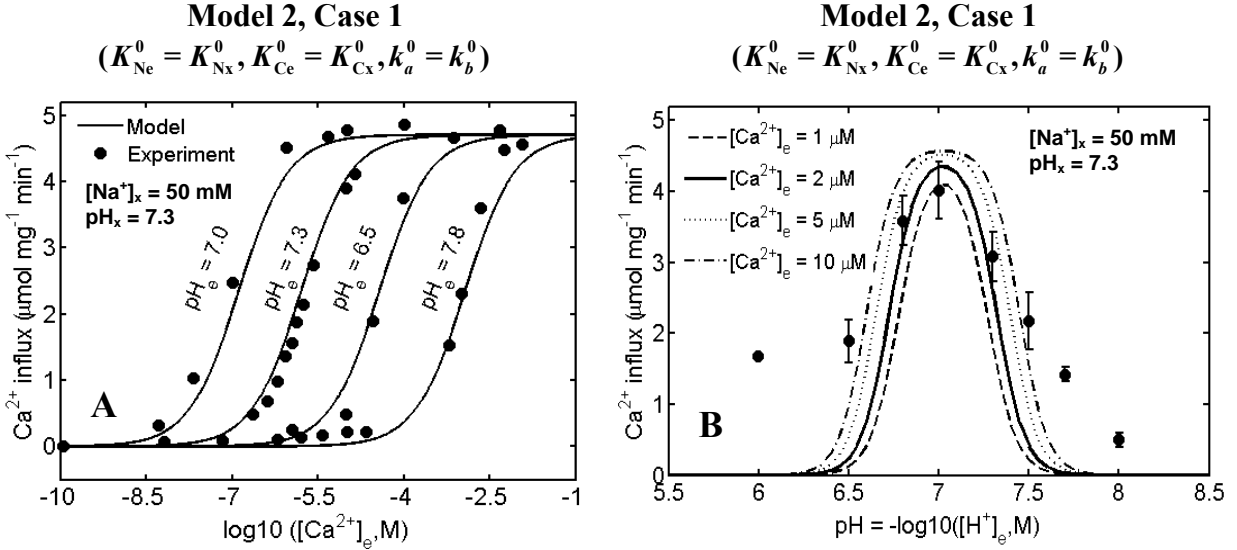
dergoes conformational changes (or flips upside down) to form the complex  $2\text{Na}_x^+\text{E}\text{Ca}_e^{2+}$ . The complex  $2\text{Na}_x^+\text{E}\text{Ca}_e^{2+}$  undergoes the reverse processes, where it dissociates in two distinct processes to form two  $\text{Na}^+$  ions in the matrix side of the IMM ( $2\text{Na}_x^+$ ) and one  $\text{Ca}^{2+}$  ion in the cytoplasmic side of the IMM ( $\text{Ca}_e^{2+}$ ), in addition to the formation of the unbound antiporter E.  $K'_{\text{Ne},1}$ ,  $K'_{\text{Nx},1}$ ,  $K'_{\text{Ne},2}$ ,  $K'_{\text{Nx},2}$ ,  $K'_{\text{Ce}}$  and  $K'_{\text{Cx}}$  are the apparent dissociation constants associated with the binding of external and internal  $\text{Na}^+$  and  $\text{Ca}^{2+}$  to the antiporter. The exchange of  $2\text{Na}^+$  for  $1\text{Ca}^{2+}$  via the interconversion mechanism  $\text{Ca}_x^{2+}\text{E}2\text{Na}_e^+ \leftrightarrow 2\text{Na}_x^+\text{E}\text{Ca}_e^{2+}$  is limited by the forward and reverse rate constants  $k_a$  and  $k_b$  which are independent of IMM potential  $\Delta\Psi$ .



**Figure B2: Comparison of mitochondrial  $2\text{Na}^+-1\text{Ca}^{2+}$  antiporter models (lines) to the experimental data (points) of Paucek and Jaburek (6) on the kinetics of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  fluxes via the antiporter with fixed external pH. Shown are the best fits of three different kinetic models (Model 1, Model 2, and Model 3) under two different model assumptions (Case 1, left panel: A,C and Case 2, right panel: B,D) to the kinetic data of Paucek and Jaburek in which the initial rates of  $\text{Ca}^{2+}$  influx ( $\text{Na}^+$  efflux) with variations in external  $[\text{Ca}^{2+}]$  (internal  $[\text{Na}^+] = 25\text{ mM}$ , external  $[\text{Na}^+] = 0\text{ mM}$ , internal  $[\text{Ca}^{2+}] = 0\text{ }\mu\text{M}$ , internal pH = 7.3, and external pH = 7.3) (A,B:**



upper panel) and the initial rates of  $\text{Na}^+$  influx ( $\text{Ca}^{2+}$  efflux) with variations in external  $[\text{Na}^+]$  (internal  $[\text{Na}^+] = 0$  mM, internal  $[\text{Ca}^{2+}] = 10$   $\mu\text{M}$ , external  $[\text{Ca}^{2+}] = 0$   $\mu\text{M}$ , internal  $\text{pH} = 7.3$ , and external  $\text{pH} = 7.3$ ) (C,D: lower panel) were measured in proteoliposomes reconstituted with purified  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporters of beef heart mitochondria. The models were fitted to the data by setting the membrane potential  $\Delta\Psi = 0$  mV, in consistent with the experimental protocol. The dashed lines are the simulations from Model 1 ( $K'_{\text{Ne},1} \gg 1$   $\mu\text{M}$ ,  $K'_{\text{Ne},2} \ll 1$   $\mu\text{M}$  and  $K'_{\text{Nx},1} \gg 1$   $\mu\text{M}$ ,  $K'_{\text{Nx},2} \ll 1$   $\mu\text{M}$  such that  $K'_{\text{Ne},1}K'_{\text{Ne},2} = K'_{\text{Ne}}{}^2$  and  $K'_{\text{Nx},1}K'_{\text{Nx},2} = K'_{\text{Nx}}{}^2$ ; fully cooperativity), the solid lines are the simulations from Model 2 ( $K'_{\text{Ne},1} = K'_{\text{Ne},2} = K'_{\text{Ne}}$  and  $K'_{\text{Nx},1} = K'_{\text{Nx},2} = K'_{\text{Nx}}$ ; partial cooperativity), and the dotted lines are the simulations from Model 3 ( $K'_{\text{Ne},1} = 2K'_{\text{Ne}}$ ,  $K'_{\text{Ne},2} = K'_{\text{Ne}}/2$  and  $K'_{\text{Nx},1} = 2K'_{\text{Nx}}$ ,  $K'_{\text{Nx},2} = K'_{\text{Nx}}/2$ ; no cooperativity) for both the conditions (Case 1:  $K_{\text{Ne}}^0 = K_{\text{Nx}}^0$ ,  $K_{\text{Ce}}^0 = K_{\text{Cx}}^0$  and  $k_a^0 = k_b^0$  and Case 2:  $K_{\text{Ne}}^0 \neq K_{\text{Nx}}^0$ ,  $K_{\text{Ce}}^0 \neq K_{\text{Cx}}^0$  and  $k_a^0 \neq k_b^0$ ). The model parameter values are as given in Table B1.



**Figure B3: Comparison of mitochondrial  $2\text{Na}^+$ - $1\text{Ca}^{2+}$  antiporter models (lines) to the experimental data (points) of Paucek and Jaburek (6) on the kinetics of  $\text{Na}^+$  and  $\text{Ca}^{2+}$  fluxes via the antiporter with varying external pH.** Shown are the best fits of the best kinetic model (Model 2, Case 1) to the kinetic data of Paucek and Jaburek in which the initial rates of  $\text{Ca}^{2+}$  influx ( $\text{Na}^+$  efflux) with (A) variations in external  $[\text{Ca}^{2+}]$  at four different levels of external pH (internal  $[\text{Na}^+] = 50$  mM, external  $[\text{Na}^+] = 0$  mM, internal  $[\text{Ca}^{2+}] = 0$   $\mu\text{M}$ , internal  $\text{pH} = 7.3$ , and external  $\text{pH} = 7.0, 7.3, 6.5$  and  $7.8$ ), and (B) variations in external pH and fixed external  $[\text{Ca}^{2+}]$  (internal  $[\text{Na}^+] = 50$  mM, external  $[\text{Na}^+] = 0$  mM, internal  $[\text{Ca}^{2+}] = 0$   $\mu\text{M}$ , external  $[\text{Ca}^{2+}] = 2$   $\mu\text{M}$ , and internal  $\text{pH} = 7.3$ ) were measured in proteoliposomes reconstituted with purified  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporters of beef heart mitochondria. Also shown in plot B are the model simulations of the initial rates of  $\text{Ca}^{2+}$  influx ( $\text{Na}^+$  efflux) with variations in external pH at four different levels of external  $[\text{Ca}^{2+}]$  (1, 2, 5 and 10  $\mu\text{M}$ ) with other experimental conditions remaining the same. The model specifications for Model 2 and model assumptions for Case 1 are the same as in Figure B2. The model was fitted to the data by setting the membrane potential  $\Delta\Psi = 0$  mV, in consistent with the experimental protocol. The model parameter values are given in Table B1.

**Table B1:** The estimated parameter values in the kinetic models of mitochondrial  $2\text{Na}^+ - 1\text{Ca}^{2+}$  antiporter from the experimental data of Paucek and Jaburek (6). The kinetic parameters satisfy the constraint:  $(k_a^0/k_b^0)(K_{\text{Ce}}^0/K_{\text{Cx}}^0)(K_{\text{Nx}}^0/K_{\text{Ne}}^0)^2 = 1$ . The biophysical parameters are chosen as  $\alpha_e = \alpha_x = \alpha = 0$  and  $\beta_e = \beta_x = \beta = 0.5$ . The rate constants are in the units of  $\mu\text{mol}/\text{mg}/\text{min}$  and the dissociation constants are in the units of molar (M). Reference ‘r1’ corresponds to Figure B2 (A,B) and reference ‘r2’ corresponds to Figure B2 (C,D).

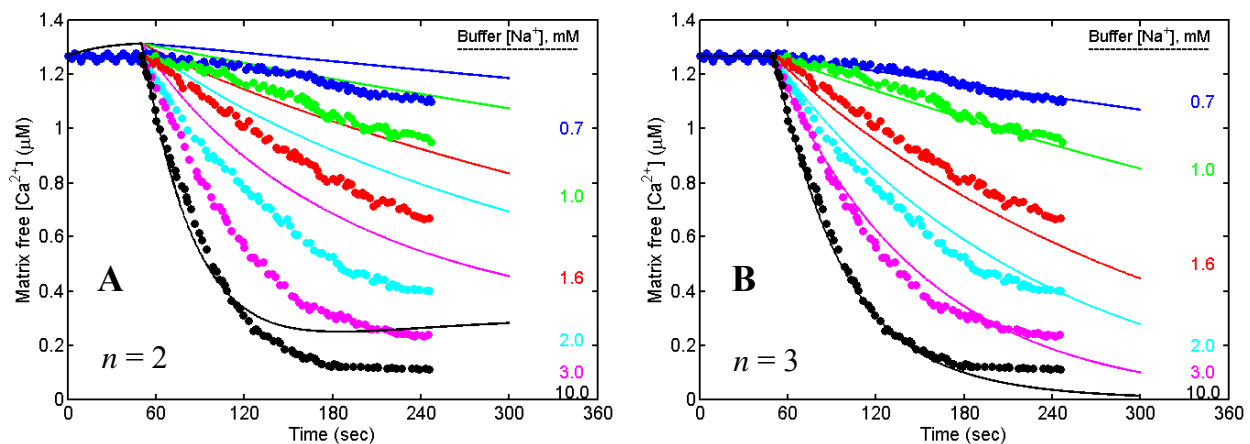
Parameter	Values for Model 1		Values for Model 2		Values for Model 3		Refer- ence
	Case 1 ( $K_{\text{Ne}}^0 = K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 = K_{\text{Cx}}^0$ )	Case 2 ( $K_{\text{Ne}}^0 \neq K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 \neq K_{\text{Cx}}^0$ )	Case 1 ( $K_{\text{Ne}}^0 = K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 = K_{\text{Cx}}^0$ )	Case 2 ( $K_{\text{Ne}}^0 \neq K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 \neq K_{\text{Cx}}^0$ )	Case 1 ( $K_{\text{Ne}}^0 = K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 = K_{\text{Cx}}^0$ )	Case 2 ( $K_{\text{Ne}}^0 \neq K_{\text{Nx}}^0$ , $K_{\text{Ce}}^0 \neq K_{\text{Cx}}^0$ )	
$k_a^0$	5.2, 5.75	5.1, 5.71	5.9, 5.9	5.81, 6.0	5.8, 5.9	5.3, 5.83	r1, r2
$k_b^0$	5.2, 5.75	5.2, 5.82	5.9, 5.9	5.90, 6.1	5.8, 5.9	5.4, 5.94	r1, r2
$K_{\text{Ne}}^0$	$8.86 \times 10^{-3}$	$8.20 \times 10^{-3}$	$5.61 \times 10^{-3}$	$5.89 \times 10^{-3}$	$7.10 \times 10^{-3}$	$5.76 \times 10^{-3}$	r1, r2
$K_{\text{Nx}}^0$	$8.86 \times 10^{-3}$	$7.93 \times 10^{-3}$	$5.61 \times 10^{-3}$	$5.60 \times 10^{-3}$	$7.10 \times 10^{-3}$	$5.56 \times 10^{-3}$	r1, r2
$K_{\text{Ce}}^0$	$2.29 \times 10^{-9}$	$2.29 \times 10^{-9}$	$2.27 \times 10^{-9}$	$2.26 \times 10^{-9}$	$2.10 \times 10^{-9}$	$2.30 \times 10^{-9}$	r1, r2
$K_{\text{Cx}}^0$	$2.29 \times 10^{-9}$	$2.10 \times 10^{-9}$	$2.27 \times 10^{-9}$	$2.01 \times 10^{-9}$	$2.10 \times 10^{-9}$	$2.10 \times 10^{-9}$	r1, r2
$K_{\text{Ce}}^{\prime 0}$ (pH=7.0)	$1.37 \times 10^{-7}$	$1.38 \times 10^{-7}$	$1.30 \times 10^{-7}$	$1.45 \times 10^{-7}$	$1.34 \times 10^{-7}$	$1.42 \times 10^{-7}$	r1, r2
$K_{\text{Ce}}^{\prime 0}$ (pH=7.3)	$1.70 \times 10^{-6}$	$1.70 \times 10^{-6}$	$1.56 \times 10^{-6}$	$1.88 \times 10^{-6}$	$1.68 \times 10^{-6}$	$1.71 \times 10^{-6}$	r1, r2
$K_{\text{Ce}}^{\prime 0}$ (pH=6.5)	$3.92 \times 10^{-5}$	$4.00 \times 10^{-5}$	$3.76 \times 10^{-5}$	$4.16 \times 10^{-5}$	$3.94 \times 10^{-5}$	$4.23 \times 10^{-5}$	r1, r2
$K_{\text{Ce}}^{\prime 0}$ (pH=7.8)	$1.22 \times 10^{-3}$	$1.22 \times 10^{-3}$	$1.18 \times 10^{-3}$	$1.37 \times 10^{-3}$	$1.22 \times 10^{-3}$	$1.23 \times 10^{-3}$	r1, r2
$K_{\text{Cx}}^{\prime 0}$ (pH=7.3)	$1.70 \times 10^{-6}$	$1.56 \times 10^{-6}$	$1.56 \times 10^{-6}$	$1.67 \times 10^{-6}$	$1.68 \times 10^{-6}$	$1.56 \times 10^{-6}$	r1, r2
$K_{\text{H1}}$	$6.47 \times 10^{-8}$	$6.45 \times 10^{-8}$	$6.51 \times 10^{-8}$	$6.39 \times 10^{-8}$	$6.37 \times 10^{-8}$	$6.39 \times 10^{-8}$	r1, r2
$K_{\text{H2}}$	$1.40 \times 10^{-7}$	$1.40 \times 10^{-7}$	$1.38 \times 10^{-7}$	$1.43 \times 10^{-7}$	$1.42 \times 10^{-7}$	$1.40 \times 10^{-7}$	r1, r2

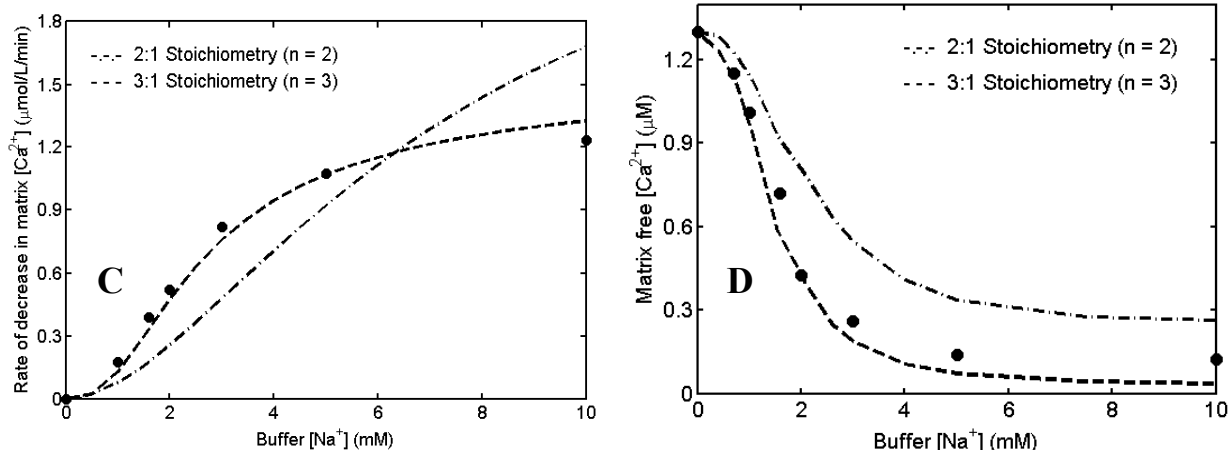
## Appendix C: Integrated Modeling of Mitochondrial Bioenergetics and $\text{Ca}^{2+}$ Handling

In spite of large number of kinetic studies (6-10), the stoichiometry of mitochondrial  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporter is not well established. Furthermore, the antiporter function under pathophysiological conditions (e.g., myocardial ischemia) is not well known. In a step towards understanding these aspects, the proposed model of mitochondrial  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporter and our recently developed model of mitochondrial  $\text{Ca}^{2+}$  uniporter (2) is integrated to our existing model of mitochondrial bioenergetics and  $\text{Ca}^{2+}$  handling (11). The integrated model is then applied to characterize the stoichiometry of the antiporter as well as to predict the antiporter function with varying levels of external (cytosolic) pH that occur during pathophysiological conditions.

### Characterization of the Stoichiometry of the $n\text{Na}^+$ - $1\text{Ca}^{2+}$ Antiporter:

This section presents the application of the proposed kinetic model of mitochondrial  $n\text{Na}^+$ - $1\text{Ca}^{2+}$  antiporter to characterize the stoichiometry of the antiporter. For doing this, the best model of the antiporter (Model 2, Case 1;  $n = 2$  or 3) is integrated into our recently developed computational model of mitochondrial bioenergetics and  $\text{Ca}^{2+}$  handling (11). The resulting integrated model is further modified by incorporating our recently developed biophysical model of mitochondrial  $\text{Ca}^{2+}$  uniporter (2), while keeping the other model components and equations the same, as reported in the previous Supplementary Material (11). The integrated model (with  $n = 2$  and 3) is then applied to simulate the experimental data of Cox and Matlib (12) in which the time course of matrix free  $[\text{Ca}^{2+}]$  in purified respiring mitochondria from rabbit hearts with addition of varying levels of  $\text{Na}^+$  to the extra-matrix buffer medium with the activity of mitochondrial  $\text{Ca}^{2+}$  uniporter blocked by ruthenium red. The result of this analysis is summarized in Figure C1. The integrated model with  $3\text{Na}^+$ - $1\text{Ca}^{2+}$  antiporter successfully describes the data, while the integrated model with  $2\text{Na}^+$ - $1\text{Ca}^{2+}$  antiporter deviates significantly from the data. This further validates our previous hypothesis that the stoichiometry of mitochondrial  $\text{Na}^+$ - $\text{Ca}^{2+}$  antiporter is 3:1 (i.e., an electrogenic exchange of  $3\text{Na}^+$  for  $1\text{Ca}^{2+}$  via the antiporter).

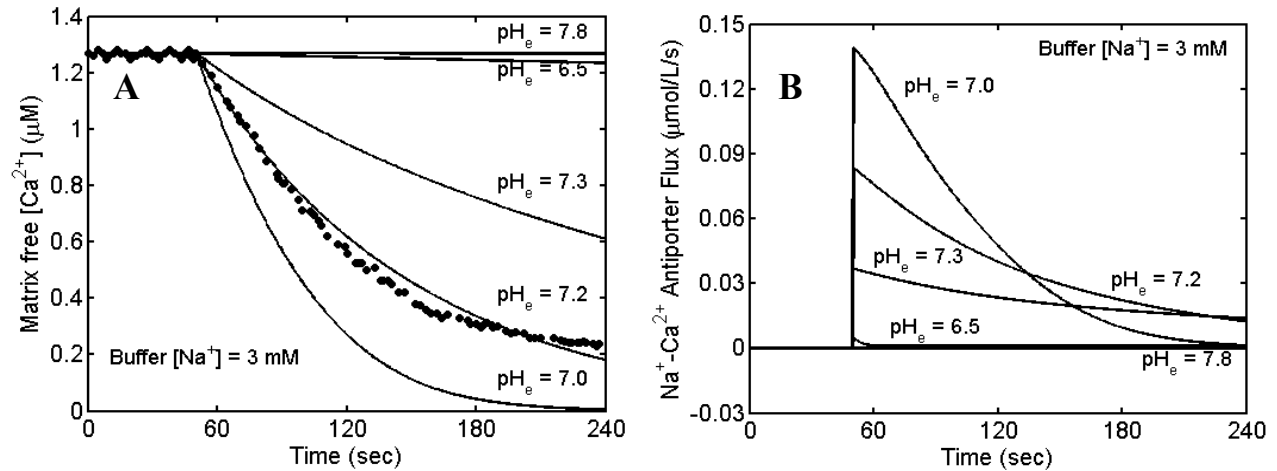




**Figure C1: Characterization of the stoichiometry of mitochondrial  $n\text{Na}^+-1\text{Ca}^{2+}$  antiporter.** Shown are the comparisons of the integrated model predictions (lines) to the experimental data (points) of Cox and Matlib (12) with both (A,C,D)  $2\text{Na}^+-1\text{Ca}^{2+}$  and (B,C,D)  $3\text{Na}^+-1\text{Ca}^{2+}$  antiporter models. The total buffer  $[\text{Ca}^{2+}]$  was fixed at  $20\ \mu\text{M}$ , corresponding to a free buffer  $[\text{Ca}^{2+}]$  of  $0.15\ \mu\text{M}$  with  $50\ \mu\text{M}$  of EGTA in the external buffer medium (external  $\text{pH} = 7.2$ ). The antiporter model uses the same parameter values for  $K_{\text{Ce}}$ ,  $K_{\text{Cx}}$ ,  $K_{\text{H1}}$ ,  $K_{\text{H2}}$ ,  $\alpha$  and  $\beta$  as estimated before (Tables 1 and B1), while the rate constants  $k_a$  and  $k_b$  and the dissociation constants  $K_{\text{Ne}}$  and  $K_{\text{Nx}}$  are varied to obtain the best fit of the model to the data on the dynamic of matrix free  $[\text{Ca}^{2+}]$  (Plots: A,B). The parameters  $K_{\text{Ne}}$  and  $K_{\text{Nx}}$  are found to be  $1.6\ \text{mM}$  for  $3\text{Na}^+-1\text{Ca}^{2+}$  antiporter model and  $4.4\ \text{mM}$  for  $2\text{Na}^+-1\text{Ca}^{2+}$  antiporter model. The rate constants  $k_a$  and  $k_b$  are found to be  $7.8\ \text{nmol of Ca}^{2+}/\text{L}/\text{sec}$  for  $3\text{Na}^+-1\text{Ca}^{2+}$  antiporter model and  $650\ \text{nmol of Ca}^{2+}/\text{L}/\text{sec}$  for  $2\text{Na}^+-1\text{Ca}^{2+}$  antiporter model. Plot C shows the comparisons of integrated model simulations to the initial rates of decrease of matrix free  $[\text{Ca}^{2+}]$  following addition of different levels of  $\text{Na}^+$  to the external buffer medium, using both  $2\text{Na}^+-1\text{Ca}^{2+}$  and  $3\text{Na}^+-1\text{Ca}^{2+}$  antiporter models. Plot D shows the corresponding comparisons on the levels of matrix free  $[\text{Ca}^{2+}]$  after 3 min of  $\text{Na}^+$  addition to the buffer medium.

### Mitochondrial $\text{Ca}^{2+}$ Dynamics during Pathophysiological Conditions:

In order to predict the effect of  $3\text{Na}^+-1\text{Ca}^{2+}$  antiporter on mitochondrial  $\text{Ca}^{2+}$  regulation during pathophysiological states (high and low pH), the integrated model of mitochondrial bioenergetics and  $\text{Ca}^{2+}$  handling is used to simulate the dynamics of matrix free  $[\text{Ca}^{2+}]$  based on the experimental protocol of Cox and Matlib (12) with fixed external  $[\text{Na}^+]$  of  $3\ \text{mM}$  and different external pH ( $\text{Ca}^{2+}$  uniporter blocked) which is shown in Figure C2 (A). The corresponding dynamics of  $\text{Na}^+$  influx ( $\text{Ca}^{2+}$  efflux) via the antiporter is shown in Figure C2 (B). The simulations with different external  $[\text{Na}^+]$  and fixed external pH of  $7.2$  is shown above in Figure C1 (B). These simulations show that the model is able to adequately predict the experimental data with external  $\text{pH} = 7.2$ , and the antiporter function is optimal at  $\text{pH} \approx 7.0$ . However, at high and low pH (i.e., for  $\text{pH} < 6.5$  and  $\text{pH} > 7.5$ ), the model significantly deviates from the data. At these levels of pH, the  $\text{Na}^+-\text{Ca}^{2+}$  antiporter flux is significantly reduced due to the inhibition of the antiporter function by protons, resulting in significantly higher matrix free  $[\text{Ca}^{2+}]$  compared to pH around  $7.0$ .



**Figure C2: Effect of extra-matrix buffer pH variations on the dynamics of matrix free  $[Ca^{2+}]$  and  $Ca^{2+}$  efflux ( $Na^+$  influx) via the  $3Na^+:1Ca^{2+}$  antiporter.** (Plot A) Shown are the integrated model simulations (lines) of the dynamics of matrix free  $[Ca^{2+}]$  at different levels of external pH (6.5, 7.0, 7.2, 7.3, 7.8) based on the experimental protocol of Cox and Matlib (12) in which the time course of matrix free  $[Ca^{2+}]$  were measured (points) following addition of varying levels of  $[Na^+]$  to the external buffer medium (external EGTA = 50  $\mu M$ , external total  $[Ca^{2+}] = 20$   $\mu M$ , internal free  $[Ca^{2+}] = 1.27$   $\mu M$ , external pH = 7.2) in purified respiring mitochondria from rabbit hearts with the activity of  $Ca^{2+}$  uniporter blocked by ruthenium red (also see Figure C1). The data and corresponding model simulations are shown only for external  $[Na^+] = 3$  mM. (Plot B) Shown are the integrated model simulations of the dynamics of  $Na^+-Ca^{2+}$  fluxes via the antiporter at different levels of external pH with the simulation protocol the same as in Plot A. The simulations are conducted by exclusively integrating the best  $3Na^+:1Ca^{2+}$  antiporter model (Model 2, Case 1) to our previous model of mitochondrial bioenergetics and  $Ca^{2+}$  handling (11).

## REFERENCES

1. Metelkin, E., I. Goryanin, and O. Demin. 2006. Mathematical modeling of mitochondrial adenine nucleotide translocase. *Biophys J* 90(2):423-432.
2. Dash, R.K., F. Qi, and D.A. Beard. 2009. A biophysically based mathematical model for the kinetics of mitochondrial calcium uniporter. *Biophys J* 96(4):1318-1332.
3. Keener, J.P., and J. Sneyd. 1998. *Mathematical Physiology*. Springer, New York.
4. Lauger, P. 1973. Ion transport through pores: a rate-theory analysis. *Biochim Biophys Acta* 311(3):423-441.
5. Woodbury, J.W. 1971. Eyring rate theory model of the current-voltage relationship of ion channels in excitable membranes. In *Chemical Dynamics: Papers in Honor of Henry Eyring*. Hirschfelder J, editor. John Wiley and Sons Inc., New York.
6. Paucek, P., and M. Jaburek. 2004. Kinetics and ion specificity of  $Na^+/Ca^{2+}$  exchange mediated by the reconstituted beef heart mitochondrial  $Na^+/Ca^{2+}$  antiporter. *Biochim Biophys Acta* 1659(1):83-91.

7. Brand, M.D. 1985. The stoichiometry of the exchange catalysed by the mitochondrial calcium/sodium antiporter. *Biochem J* 229(1):161-166.
8. Wingrove, D.E., and T.E. Gunter. 1986. Kinetics of mitochondrial calcium transport. II. A kinetic description of the sodium-dependent calcium efflux mechanism of liver mitochondria and inhibition by ruthenium red and by tetraphenylphosphonium. *J Biol Chem* 261(32):15166-15171.
9. Baysal, K., D.W. Jung, K.K. Gunter, T.E. Gunter, and G.P. Brierley. 1994. Na<sup>+</sup>-dependent Ca<sup>2+</sup> efflux mechanism of heart mitochondria is not a passive Ca<sup>2+</sup>/2Na<sup>+</sup> exchanger. *Am J Physiol* 266(3 Pt 1):C800-808.
10. Jung, D.W., K. Baysal, and G.P. Brierley. 1995. The sodium-calcium antiport of heart mitochondria is not electroneutral. *J Biol Chem* 270(2):672-678.
11. Dash, R.K., and D.A. Beard. 2008. Analysis of cardiac mitochondrial Na<sup>+</sup>-Ca<sup>2+</sup> exchanger kinetics with a biophysical model of mitochondrial Ca<sup>2+</sup> handling suggests a 3:1 stoichiometry. *J Physiol* 586(13):3267-3285.
12. Cox, D.A., and M.A. Matlib. 1993. A role for the mitochondrial Na<sup>+</sup>-Ca<sup>2+</sup> exchanger in the regulation of oxidative phosphorylation in isolated heart mitochondria. *J Biol Chem* 268(2):938-947.