

Supporting Information

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SI Text

SI Methods Cell isolation and culture. Ovine tissues from animals weighing 20–25 kg and 8–10 mo of age were obtained under approved guidelines for animal experimentation at Children's Hospital, Boston. Primary cultures of mitral valve endothelial cells (MVECs) from ovine mitral valve leaflets were prepared and plated as single cells in 96-well plates as described previously (1–3). Briefly, clonal populations were isolated from MVECs at passage 2 by suspending in endothelial basal medium (EBM; Lonza), 10% heat-inactivated FBS (GIBCO), 1% L-glutamine-penicillin-streptomycin sulfate (GPS; GIBCO), and 2 ng/mL basic fibroblast growth factor (bFGF; Roche) at 3.3 cells per milliliter and plating 100 μ L per well of a 96-well plate. When the colonies covered two-thirds of the well, cells were passaged into 24-well dishes. Cells were passaged 1:3 or 1:4 every 6–14 d and used between passages 6 and 14.

Microcontact printing and valve thin films. Fibronectin (BD Biosciences) was microcontact printed as described before (4) onto either regular elastomer stretcher membranes (Specialty Manufacturing, Inc.; 0.010" NRV) or onto valvular thin films (vTFs) in order to create either an isotropic or anisotropic tissue. For anisotropic tissue, fibronectin was microcontact printed in 20- μ m-wide lines of 50 μ g/mL concentration separated by 20- μ m-wide gaps of 5 μ g/mL concentration to provide cellular alignment cues. In isotropic tissue, fibronectin was microcontact printed with a flat polydimethylsiloxane (PDMS) stamp at 50 μ g/mL concentration. Valvular thin films were constructed as outlined before (5) by spin-coating poly(*N*-isopropylacrylamide) (PIPAAm) (Polysciences) onto a prestretched elastomer membrane (SMI 0.010" NRV) then spin-coating PDMS (Sylgard 184) doped with 0.2- μ m diameter fluorospheres (Invitrogen) on the PIPAAm. The construct was then cured at 65 °C for 4 h before being microcontact printed.

Cyclic stretcher experiments. MVECs were seeded on 5.5 \times 8 cm elastomeric membranes within 20 cm² silicone reducer rings at a density of 25,000 cells per cm². A custom-built cyclic stretcher apparatus was used to subject samples to either 10% (Movie S1) or 20% strain (Movie S2) at 1 Hz, which is the normal resting heart rate of sheep. Stretching was started 30 min after seeding in order to allow the cells to form strong focal adhesions with the underlying substrate (Fig. S1). The device used a direct current motor (Maxon Precision Motors, Inc.) to displace the membrane a total of 5.5 mm (10% strain) or 11 mm (20% strain). Control samples were maintained unstretched (0% strain). The deformation was measured by marking the membrane with dots recording the deformation at 100 frames per second. The strain field of the membrane was then validated using an in-house three-point strain algorithm. We asked if cyclic stretch induced apoptosis and conducted a TUNEL assay of the stretched tissues, revealing no significant difference between conditions (Fig. S1D). Thus, our experimental model does not appear to be traumatic to the cells within the tissue.

Valve thin film contractile stress measurements. Valve thin film tissue stresses were calculated as previously published (5). Briefly, prior to the experiment, the tissues were cultured at 37 °C. At the time of the experiment, culture media was exchanged with Tyrode's buffer solution and the tissue and PDMS layers of the construct were cut into rectangular strips and the buffer was allowed to cool below 32 °C, dissolving the PIPAAm layer. The free-floating vTFs

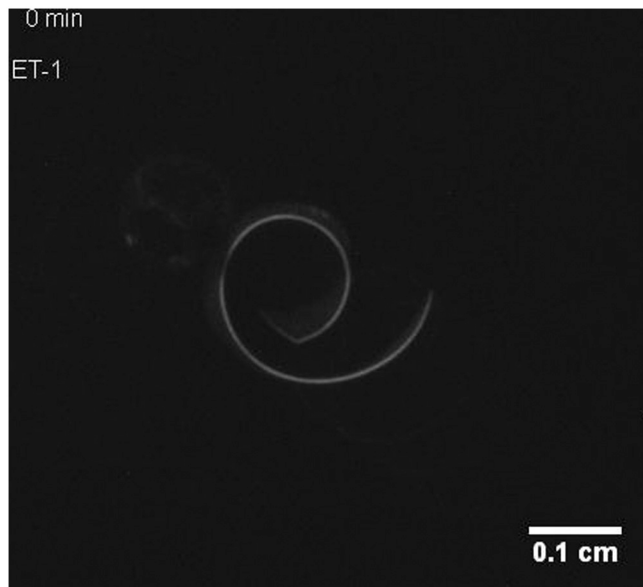
are then attached to polytetrafluoroethylene posts in a separate dish for stress measurement. The vTFs were maintained at 37 °C in a bath of Tyrode's solution. The vTFs were stimulated serially with 50 nM endothelin-1 (ET-1), 100 mM KCl, and 100 μ M of the rho-kinase inhibitor HA-1077. The radius of curvature was measured under a stereomicroscope in both brightfield and fluorescence. The tissue stress was calculated by assuming that the vTF is a two-layered beam with one passive layer (PDMS) and one active layer (valve cells). The serial stimulation allows measurement of the basal contractile tone, or contraction stress prior to any stimulation, and the induced contraction or relaxation due to added compounds. The PDMS and tissue layer thickness needed to calculate vTF stress were measured using stylus profilometry (Dektak 6M; Veeco Instruments, Inc.) and confocal microscopy (Fig S3), respectively. Optimum concentration for ET-1 was based on dose curve experiments (Fig. S4).

Immunocytochemistry. After 48 h of culture, tissues were fixed in a solution of 4% paraformaldehyde (PFA) for 15 min and permeabilized with ice-cold methanol for 2 min. Samples were washed 3 \times with PBS solution (GIBCO) and then blocked using 1% BSA in PBS with 0.05% Tween-20 for 1 h at room temperature. Samples were then incubated with antibodies against α -smooth muscle actin (α -SMA, 1:1000; Sigma), phosphorylated-smad-2/3 (p-smad-2/3, 1:100; Santa-Cruz), β -catenin (1:500; Sigma), and VE-cadherin (1:25; Santa-Cruz) for 2 h at room temperature. Samples were subsequently washed 3 \times with PBS and then stained with appropriate secondary antibodies and DAPI (Sigma) for 1 h at room temperature, and coverslipped using Prolong Gold antifade reagent (Invitrogen). Confocal image stacks were captured with an LSM 510 Live (Zeiss) line scanning confocal microscope using a 40 \times objective.

Quantification of cell geometry parameters. After 24 h of culture, tissues were stained for their nuclei (DAPI), F-actin filaments (phalloidin), and cell membrane (VE-cadherin, 1:25; Santa-Cruz) as outlined above. Actin orientational order parameter (OOP) was calculated from phalloidin staining as previously published by us (6, 7). Briefly, the OOP was computed from the pixel-based orientation vectors of the actin images. The OOP was developed for the study of organization of liquid crystals (8) and adapted for biological applications (9). The parameter ranges from zero in isotropic systems to one in perfectly aligned systems. Nuclear eccentricity was calculated by thresholding the DAPI image, fitting an ellipse to each individual nucleus, and measuring the major and minor dimensions of the ellipse (10). Eccentricity is a measure of the shape of an ellipse and is in the range of [0,1]; a circle has an eccentricity of zero, and a more elongated shape is associated with a higher value of eccentricity. Cell aspect ratio and perimeter were also similarly calculated by fitting an ellipse to each individual cell around the border of the cell membrane, fitting an ellipse and calculating the ratio of major and minor lengths. A value of one corresponds to a circular shape, with larger values for cell aspect ratios indicating a more elongated shape. Phalloidin-stained images were also used for tissue thickness measurements (Fig. S4). Confocal stacks were first deconvolved (Fig. S4 A and B) using Imaris bitplane software (IMARIS) and an in-house MATLAB (Mathworks) code was used to calculate tissue thickness (Fig. S4 C–E). Tissue thickness data were utilized to calculate vTF contractile stresses (5). All geometric parameters were quantified based on at least 12 image



Movie S2. Representative video showing stretchers on our cyclic stretcher device subject to 20% strain.
[Movie S2 \(AVI\)](#)



Movie S3. Representative vTF during serial stimulation with 50 nM ET-1, 100 mM KCl, and 100 μ M HA-1077.
[Movie S3 \(AVI\)](#)

Table S1. List of gene primers used in this study.

Gene name	Forward primer (5'-3')	Reverse primer (5'-3')
TGF- β 1	TAACACGCTTCAAGTGGACA	TCCGGAAGTCAATGTAGAGC
WNT1	CAGCATAGAGCCGGGCAAG	AGGAGAGTGCTCCCTGGGGC
VEGF	ATTTCAAGCCGTCTGTGT	CCTCGGCTTGTCACATTTT
ACTB	CAAGGAGAAGCTCTGCTACG	TAGAGGTCTTTGCGGATGTC