Optical-Fiber Based Fluorescence Detection System

An optical fiber based fluorescence detection system was developed to measure the concentration of FITC-BSA in the abluminal chamber in real-time. This cost-effective and compact system used a light emitting diode (LED) as excitation light source and an ultra sensitive photodiode as photon detector. The design was based on similar systems used in previous studies as described by Novak et al. (24), DeMaio et al. (9), Yang et al. (34) and in (26).

Fig. S6 is the schematic of the light path. Excitation lights from a high power blue LED (MBLED, peak wave length 470 nm, 625 mW, Thorlabs) were collimated by a plano-convex lens (f=25.4 mm, surface coated for 350-650 nm wavelength light transmission, Thorlabs). Blue excitation light was then filtered by a narrow bandpass filter (470 nm/10 nm, central wavelength/ full width at half maximum, Thorlabs), and reflected by a long pass dichroic mirror (Q505LP, Chroma) placed at 45 degree to the light path. Excitation light was finally focused by another plano-convex lens (f=25.4 mm, Thorlabs) to one end of the polymer clad multimode silica fiber (numerical aperture 0.48, 1 mm core diameter, Thorlabs). The other end, the measurement end, of the optical fiber was immersed in the abluminal solution. Both ends of the fiber were polished by 5 μm, 3 μm and 1 μm aluminum oxide polishing sheet (Thorlabs) sequentially to achieve the best transmission efficiency.

The emitted fluorescence light was collected by the same optical fiber and collimated by the same lens. The fluorescence light passed through the dichroic mirror, filtered by an emitter filter (530 nm/ 10 nm, Thorlabs) and was finally focused by another

plano-convex lens (f=25.4 mm, Thorlabs) to the sensor of an ultra-sensitive femtowatt photoreceiver (PDF10A, Thorlabs). The photoreceiver combines a low noise silicon photodiode with a built-in ultra low noise transimpedance amplifier with a high gain of 10^{12} V/A. All the optical components were enclosed in lens tubes (Thorlabs) and a mirror holder was used to secure the dichroic mirror precisely at the 45 degree position. Thus, the entire optical path, except for the measurement end of the fiber, was shielded from stray light. The controllers of the LED and photoreceiver were connected to a DAQ board (NI PCI-6221, National Instruments) through BNC cables. The LED was turned on only during the measurement time to minimize photo bleaching. The output of the LED was controlled by a rectangular voltage signal at 20 Hz generated by the DAQ. The average excitation intensity can be modulated by altering either the duty cycle or peak voltage of the control signal. The DC voltage output from the photoreceiver was also transmitted to the computer via the DAQ board. A LabView (National Instruments) program was used for the LED control and data acquisition.

To increase the detection sensitivity and minimize the noise from stray light that enters the measurement end of the fiber, a virtual lock-in amplifier was implemented in the LabView program (1). The fluorescence signal had a frequency of 20 Hz due to the frequency of the excitation lights. An internal sinusoidal waveform of 20 Hz was generated virtually in the LabView program. The virtual lock-in amplifier then acted as a narrow bandpass filter around the reference signal frequency, thus only amplifying the signal at 20 Hz. The fluorescence measurement can be performed inside a conventional cell incubator without the effect of the ambient light. During each measurement cycle,

the LED was turned on for only 6 seconds. Two seconds after the LED was switched on and when the LED output was stable, the fluorescence signal was acquired for 4 seconds. Fluorescence measurements were fully automated, and the tracer concentration can be measured every minute to obtain $\Delta {\sf C_s}/\Delta t$ for the permeability calculation.

Fig. S7 shows the measurements of a series dilution of FITC-BSA solution from 100 ng/ml to 1 μg/ml using three different excitation intensities. The peak voltages of the LED control signal were set to 0.5, 1.0 and 1.5V, respectively. The detection system demonstrated a good sensitivity and the R values of the linear regressions are greater than 0.998. Although 1.5V offered the best linearity and sensitivity, the high excitation intensity can lead to greater photobleaching and fluorescence signal saturation at lower concentrations, which limits the dynamic range of the measurements. Thus, the voltage of 1.0 V was used to control the LED output in the following experiments.

Figure S1: Schematic of the flow circuit for permeability measurement.

Figure S2: Schematic and 3D design of the permeability apparatus

Figure S3: Schematic of flow circuit for transcriptional studies.

Figure S4: Real-time PCR validates the microarray results of the magnitude step-up experiments. Left: microarray measurements; Right: real-time PCR measurements. n=4 for each data point. Expression values were normalized by the pre step-up controls, and error bars indicates the standard error of the mean. *: p<0.05, one-way t-test against zero.

Figure S5: Matrix of scatter plots to compare the global expression profiles between different time points. Each panel compares transcriptional profile between two time points. Each gene is plotted as one data point, where x-axis is the expression value at one time point and y-axis is the expression value at the other time point.

Figure S6: GeneGo identified pathways that are sensitive to the elevated shear stress magnitude. Top ten canonical pathways were listed. * indicates the false discovery rate < 5%.

Figure S7: Schematic of the light path of the fluorescence detection system.

Figure S8

Figure S8: Measurement of a series dilution of FITC-BSA solution. X: concentrations of the FITC-BSA solution. Y: output voltages of the fluorescence detector. Excitation lights at three different intensity levels were generated by applying different driving voltage to the LED.

Table 51, THIRTS for Teal-third qualiticative-TCR		
Gene	3' Primer	5' Primer
GAPDH	5'-GTC TTC TGG GTG GCA GTG AT-3'	5'-GGG CAT GAA CCA TGA GAA GT-3'
eNOS	$5'$ -AGC ACA GC AGG TTG ATT TC-3'	5'-GGC TGG TAC ATG AGC ACA GA-3'
KLR2	5'-CAA AAT GCC ACC TGT CTT CC-3'	5'-AGC CCA CCG GGT CTA CAC TA-3'
Interluekin- 1α	5'-CAT CAT TCA GGA TGC ACT GG-3'	5'-CAA GGA CAG TGT GGT GAT GG-3'

Table S1: Primers for real-time quantitative-PCR

Table S2: List of genes identified at different time points after shear step-up at false discovery rate controlled at 10%. The expression values were normalized to the pre step-up controls, and were presented in log2 scale.

Table S3: The expression of *a-priori* **selected genes in response to the elevated shear stress. Red: p<0.05; blue: p<0.1. The expression values after shear step-up were normalized to the pre step-up (preconditioned) controls. The expression of preconditioned cells were normalized to the static cells. Literature discussing the function and shear response of each selected gene is cited in the table. LSS: laminar shear stress, DSS: disturbed shear stress.**

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