

Supplementary figures for “Spatial resolution properties of motion-compensated tomographic image reconstruction methods”

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I. SIMULATION RESULTS

A. Simple phantom with affine motion

Fig. 1 (a) and (b) show that the image intensities around the rings are nonuniform due to the anisotropic and/or non-uniform spatial resolutions of PMC-S and PMC-C. Fig. 1 (c) shows our proposed PMC-P, which approximately achieved the same spatial resolution as the target image in Fig. 1 (d) with isotropic and uniform spatial resolution.

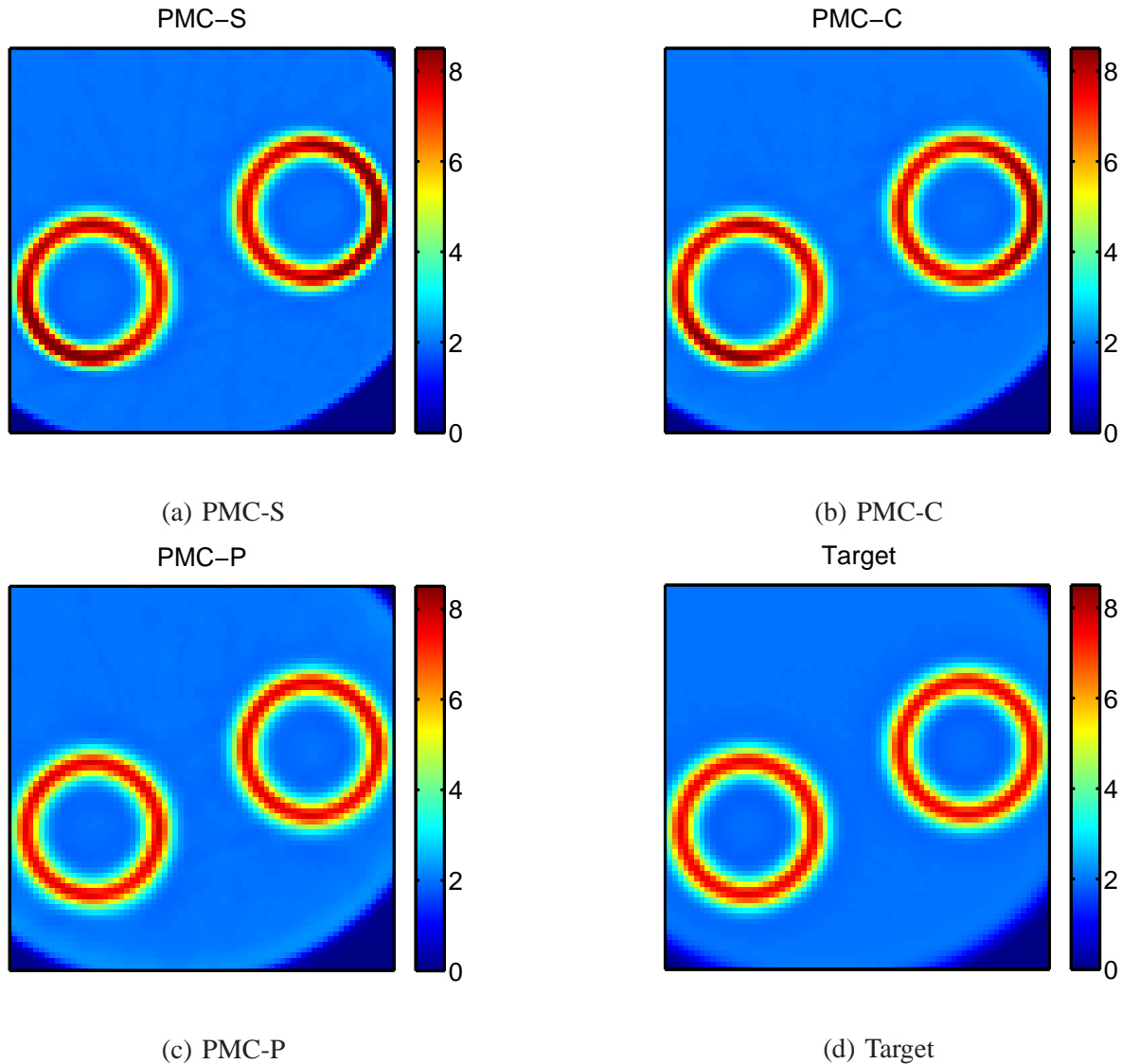


Fig. 1. Reconstructed images of PMC with different spatial regularizers from the noiseless projection data. Nonuniform and/or anisotropic LIRs lead to non-uniform estimation bias in small or narrow structures such as small lesions or rings.

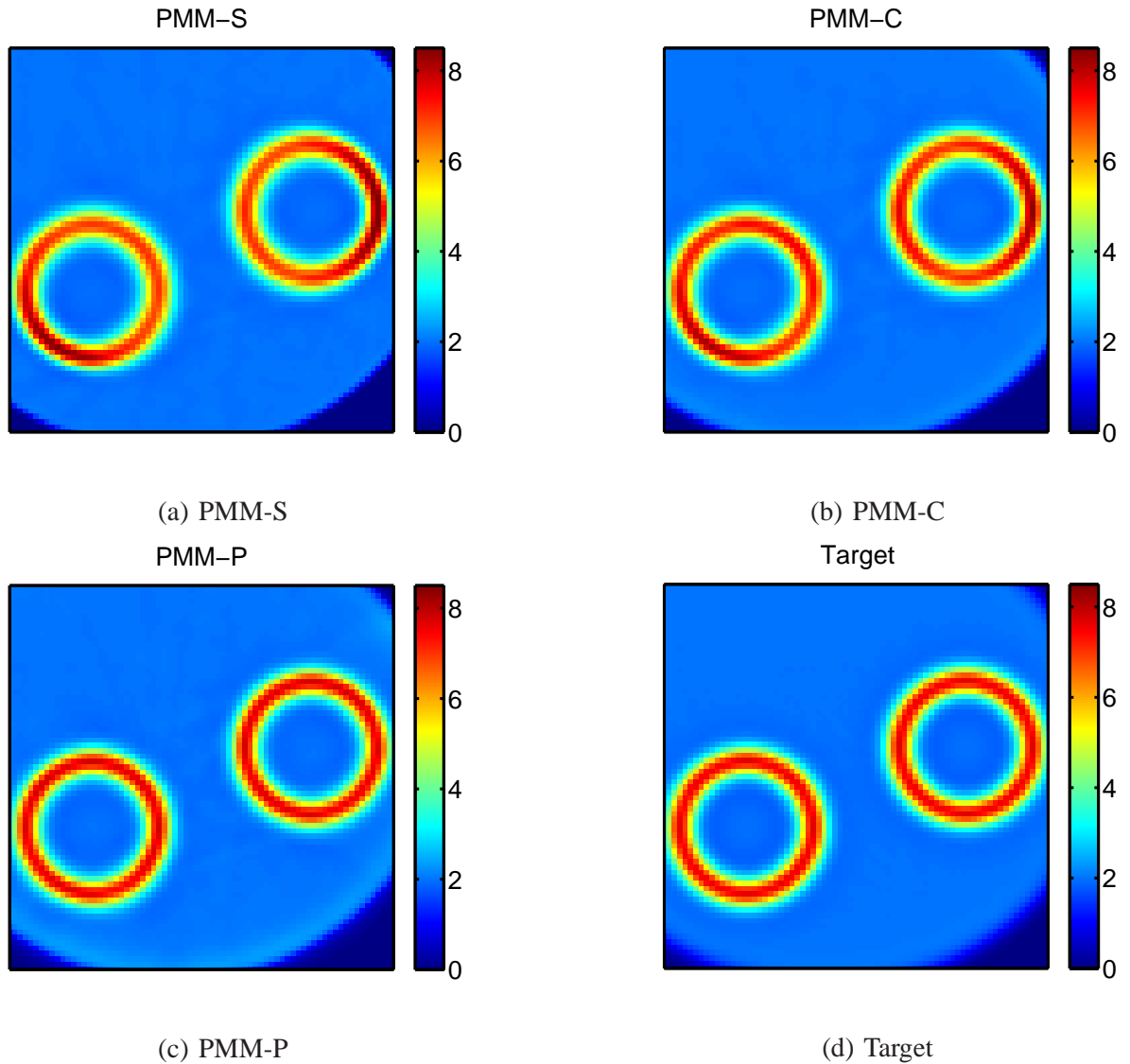


Fig. 2. Reconstructed images of PMM with different spatial regularizers from the noiseless projection data. Nonuniform and/or anisotropic LIRs lead to non-uniform estimation bias in small or narrow structures such as small lesions or rings.

Fig. 2 also shows similar results: PMM-S and PMM-C caused non-uniform estimation bias due to the spatial-variant data statistics and the motion, but PMM-P achieved approximately the same isotropic and uniform spatial resolution as those of the target PULS estimator.

Fig. 3 shows that our proposed spatial regularization method for MTR, denoted MTR-P, approximately achieved the same spatial resolution regardless of ζ , whereas the spatial resolution of MTR-S changes with ζ .

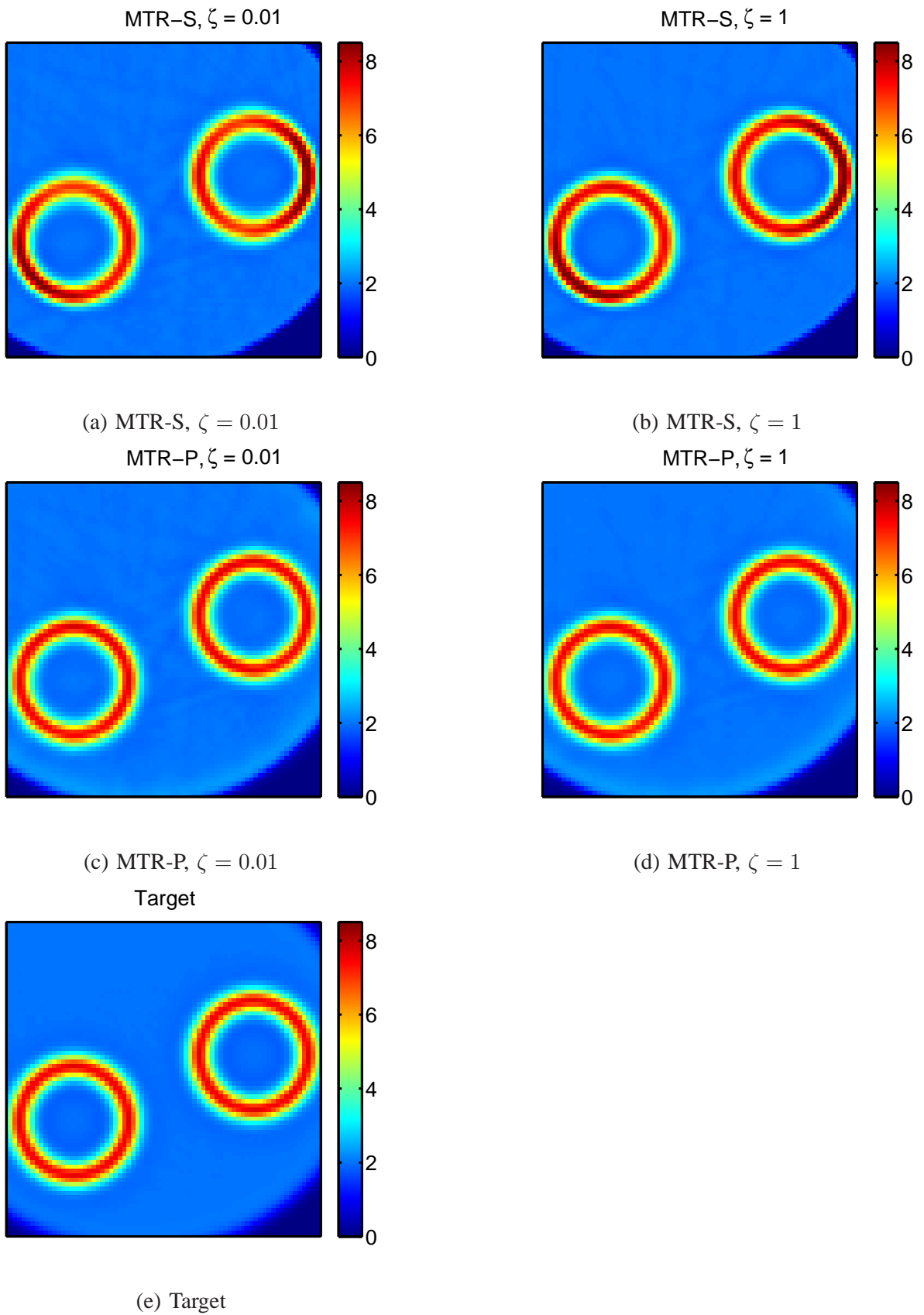


Fig. 3. Reconstructed images of MTR-S, MTR-P with different ζ values from the noiseless projection data. Nonuniform and/or anisotropic LIRs lead to non-uniform estimation bias in small or narrow structures such as small lesions or rings.