

Experimental model for stimulation of cultured human osteoblast-like cells by high frequency vibration

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Abstract

Reliable and reproducible experimental methods for studying enhancement of osteoblast proliferation and metabolic activity *in vitro* provide invaluable tools for the research of biochemical processes involved in bone turnover *in vivo*. Some of the current methods used for this purpose are based on the ability of the osteoblasts to react metabolically to mechanical stimulation. These methods are based on the hypothesis that intracellular metabolic pathways could be influenced by the excitation of cytoskeletal components by mechanical cell deformation. Based on the same assumptions we developed a new experimental approach of biomechanical stimulation of cultured osteoblast-like cells by vibration. This method is based on the use of a specially designed vibration device that consists of an electric shaker with horizontally mounted well plate containing cell cultures. We used a first passage explant outgrowth of human osteoblast-like cell cultures, originating from samples of cancelous bone, collected from femoral necks of six donors during surgical arthroplasties of osteoarthritic hips. Well plates with replicates of cultured cells were exposed to a sine shaped vibration protocol in a frequency range of 20–60 Hz with displacement amplitude of 25 (\pm 5) μ m. We found that vibration at a distinct set of mechanical
parameters of 20 Hz frequency and peak to peak acceleration of 0.5 \pm 0.1 m/sec² is optimal for cel easily reproducible experimental model should improve and simplify further research on the interactions between mechanical stimuli and intracellular biochemical pathways in osteoblasts.

hancing factors influencing osteoblast metabolism of cultured osteoblast-like cells. The method is based (Boppart et al. 1998; Duncan and Turner 1995; Neidl- on the application of external vibration directly to a inger-Wilke et al. 1994). Current research methods in cell culture plate. The vibration should cause methis field are based on the ability of cultured osteob- chanical deformation of the cells adherent to the lasts to react metabolically to mechanical stimulation. culture plate surface. The deforming force should be Stretching of cultured cells on elastic membranes and uniformly transferred to all cultured cells. This relaexposure of osteoblast cultures to a controlled fluid tively simple method of osteoblast stimulation *in vitro* flow are the most popular models for this purpose can provide a reproducible experimental tool for (Neidlinger-Wilke et al. 1994; Banes 1999; Sejima research on cellular mechanotransduction pathways. 1999). Both of these methods are based on the hy- For determination of the optimal vibration paramepothesis that intracellular metabolic pathways are ters we have investigated the cellular response to influenced by the excitation of cytoskeletal compo- vibration at infrasonic frequencies which are in the

Introduction nents by mechanical cell deformation (Burger and Klein-Nulend 1998). Here we describe a different Mechanical stimulation is one of the important en- experimental approach to biomechanical stimulation

Hz (Nigg 1998). Vibration peak to peak displacements streptomicin at 37 $^{\circ}$ C in humidified atmospheric enof 20–30 μ m, which are in the range of the osteob- vironment of 95% air with 5% CO, [v:v] for 20–30 last's cell diameter (Liu and Kalu 1990), were chosen days. Human osteoblast-like cells grew out from the empirically and have been confirmed by preliminary chips as adherent to the plastic tissue culture plates. experiments (Levy et al. 1999). This set of vibration The human bone cell cultures obtained by this method parameters has been chosen to investigate conditions have been shown previously to express osteoblast-like that are equivalent to the upper limit of the normal characteristics (Gundle et al. 1998). These cells were vibration environment of bone cells *in vivo* (Nigg passaged into 24 - well plates. Each well was seeded 1998). The impetus to investigate the response of with 2×10^4 cells. Six replicate wells from each donor osteoblasts to vibration in this specific range of me- were prepared for each vibration condition. Following chanical parameters came from previous *in vivo* passage the cells were incubated in DMEM with 20 studies that suggested an existence of positive in- mM HEPES buffer, 5% heat-inactivated fetal calf fluence of 20 Hz vibration on the bone mass mainte-
serum, 2 mM L-glutamine, 50 U ml-ml penicillin and nance (Rubin et al. 1995). 150 μ ml-ml streptomicin. Lower fetal calf concen-

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Donors

Samples of cancellous bone were collected from the *Vibration device* (*Figures* ¹ *and* 2) femoral necks of six donors during total hip replacements of osteoarthritic hips. The bone samples used Well plates containing the cell cultures were conare usually disposed after removal. The donors were nected to a horizontally oriented shaker [Mini-shaker in the age range of $55-77$ years, one man and five Type 4810- Bruel & Kjaer, Denmark]. The amplitude,

100 mM ascorbate-2-phosphate, 10 nM dex- was measured by a LVDT [Linear Variable Displace-

range of a physiologic vibromyogram, e.g. about 20 ametasone, 50 U ml-ml penicillin, 150 μ ml-ml trations were used at this stage in order to minimize its component's effect on cells.

Methods The passaged cells were incubated for 24 h and subsequently exposed four times for periods of 120 s *Outline* to the different vibration parameters at 24 h intervals. • Culture of a confluent layer of osteoblast-like cells The exposure to vibration was done outside the cell from cancellous bone samples were taken from culture incubator at ambient room conditions $[25 \text{ °C}]$. femoral necks of donors during osteoarthritic hip The control replicates, kept in static conditions, were replacements. placed at the same distance from the vibrating shaker • Following a first passage, replicates of equal num- as the replicates exposed to the vibration protocol, and ber of cultured cells were submitted to different for the same time duration at the same time intervals vibration conditions using a specially designed to eliminate the possible influence of the electrovibration device. The magnetic fields and/or high frequency sound on the vibration device. • On completion of exposure to different controlled cultured osteoblasts. Twenty four h after the fourth vibration protocols the total DNA content and exposure to vibration, all the replicates were washed alkaline phosphatase activity of all cultured cells by phosphate buffer solution and dissolved in Triton replicates were measured and statistically com- $X - 100 (0.1 %)$ solution. All replicates were frozen pared to control replicates kept under static con-
at -20 °C and thawed twice for complete DNA ditions. recovery. Each replicate was then assayed for total DNA content and alkaline phoshatase activity.

wave shape and frequency of the vibration provided by the shaker were controlled by an amplifier and *Cell cultures* pulse generator [Farnell, Function Generator – FG3]. Vibration peak-to-peak acceleration was measured Bone chips of cancellous bone, $2-3$ grams in total, with a piezoelectric accelerometer [4383 V- Bruel & were incubated in DMEM [Dulbecco's Modified Kjaer, Denmark] and displayed on a Vibration Eagles Medium] with heat-inactivated fetal calf serum Measuring Amplifier [Type 2525 - Brüel & Kjaer, (10%), 20 mM HEPES buffer, 2 mM L-glutamine, Denmark]. The displacement of vibration movement

Figure 1. Experimental setup for vibration of cultured osteoblast-like cells-Schematic presentation.

ment Transducer - sensitivity 78.16 mV/V/mm, Solat- the range of $25 \pm 5 \mu$ m. An additional six replicates

Vibration protocol

Sine shaped vibration at 20, 30, 40 and 60 Hz was applied to well plates containing six replicates of cultured cells from each of the six donors. The vi- was measured fluorometrically using the Hoechst bration displacement in all experiments was kept in 33258 dye fluorescence enhancement method with

ron] and displayed on an oscilloscope. of cell cultures from every donor were kept under static conditions and served as controls.

DNA assay

The total content of DNA in each replicate culture

Figure 2. Photograph of the shaker with well plate ready for vibration experiment.

excitation at 355 nm and emission at 450 nm using a luminescence spectrometer [Model LS30 - Perkin Elmer] (Labarca and Paigen 1980). For calibration, standard solutions of salmon testes DNA in the range of 100–1000 ngr were used.

Alkaline phosphatase assay

Alkaline phosphatase activity was determined in dissolved cell culture replicates, after incubation with P-nitrophenyl phosphate substrate, by 410 nm wavelength spectrophotometry (Bessey et al. 1946).

Statistical analysis

The values of DNA content and Alkaline phosphatase
activity/DNA Figure 3. DNA contet of osteoblast-like cell cultures following
activity per cell [alkaline phosphatase activity/DNA vibration at frequencies of 20–60 Hz rela content] in replicates exposed to each vibration profile were compared to the values of the static controls by t
test, after a normal distribution of values had been
confirmed by the Kolmogorov-Smirnov test. If a normal distribution was not confirmed values were compared by the Mann-Whitney Rank Sum Test. P **Discussion** values of less than 0.05 indicated a significant difference between the compared groups. The results are
expressed as means with standard deviation distribu-
tion.
Steoblast-like cells. The rationale for this is that high
tion.

All the cultured cell replicates survived the exposure to the vibration protocol at the frequency range of 20–60 Hz. On microscopic examination of the cells after completion of the vibration protocol, normal morphological appearance of cells was verified in all replicates.

Exposure to vibration applied at 20 Hz frequency increased the DNA content significantly in cultures from five of six donors (Figure 3).Vibration at higher frequencies, from 30 to 60 Hz, showed either no change or decreased DNA content per well.

After exposure to vibration at 20 Hz frequency, alkaline phosphatase activity was significantly lower in 5 donors and without change in one additional donor when compared to static controls. Alkaline phosphatase activity gradually increased in cultures exposed to vibration with higher frequencies in the *Figure 4.* Alkaline phosphatase activity in cultured osteoblast-like range from 30 to 60 Hz (Figure 4). At 60 Hz fre-
cells following vibration at frequencies of 20–60 Hz relative to quency cultured replicates from four donors showed a static controls.

* - P < 0.05 [compared to static controls]

frequency vibration has been shown to increase bone formation *in vivo* (Rubin et al. 1995) and that this type **Results Results Results of mechanical stimulation is likely to be experienced**

The mechanism whereby osteoblasts respond to vi- cal deformation is required. It was designed to overbration *in vivo* is not known. We therefore propose to come the technical difficulties of non uniform strains use this newly developed model to study in detail provided by the use of elastic membranes (Banes proliferation, differentiation and signaling responses 1999) and the relative complicity of their mainte-

studies demonstrating the responses of different cell replicates. The use of a controlled vibration force types, especially bone-derived cells, to mechanical applied to a cell culture dish meets these objectives. stimulation. However the large number of distinct Thus a new technical design has been developed, experimental methods used has made it difficult to adapted from that previously described for the incompare data. Most studies have used cyclic me- vestigation of the influence of vibration on cultured chanical stimulation applied to stretchable membranes lymphocytes (Khalil and Qassem 1996). to which the cells were attached. This stimulation We have chosen to investigate the *in vitro* influence should be characterized by its displacement, fre- of vibration parameters in the range otherwise known quency and acceleration [or wave shape of the applied to be produced by the natural muscular vibration [in force], but from most of these studies neither this infrasonic range of frequencies] to which bone should information nor common optimal stimulation parame- be exposed *in vivo* (Nigg 1998). There appear to be no ters for osteoblast-like cells activation are apparent previous *in vitro* studies in this range, although the (Table 1). Yet though these previous data do not effectiveness of this range of vibration parameters has provide a clear indication of the different mechanical been already presented as effective for bone mass factors required for osteoblast activation they do improvement in whole body vibration studies (Rubin demonstrate that cellular deformation affects the in- et al. 1995; Smith and Gilligan 1996). Because our tra-cellular cytoskeletal scaffold, which results in the hypothesis is that a gradually changing acceleration activation of a cascade of secondary messengers that should be less distractive to the cultured cells and stimulate an active metabolic or proliferative response therefore optimal for cellular response, we have used (Reich et al. 1997; Jacobs et al. 1998). These two a sine wave acceleration pattern of the applied viresponses appear not to be capable of being activated bration. simultaneously (Stanford et al. 1995) and distinct The present results support our initial assumptions. intra-cellular messengers seem to mediate each re- First passage adult human osteoblast-like cells response. Spond to vibration. Proliferation was optimally stimu-

perimental method for mechanical activation, our of 20–30 μ m and peak to peak acceleration of 0.5 intention was to build a device that provides a re- (± 0.1) m/sec². Metabolism was more effective at 60 producible means of delivering a controlled cyclic Hz frequency, displacement of 20–30 μ m and peak to movement, defined by its displacement, frequency peak acceleration of 1.3 (\pm 1) m/sec². Thus proliferand acceleration, in order to activate cultured osteob- ation and metabolism are probably stimulated by last-like cells. This method was based on the assump- distinct mechanical stimuli.

in bone as a result of muscle vibration (Nigg 1998). tion that cytoskeletal activation by cellular mechaniin human osteoblasts. The nance is nance. It was also designed to apply a uniform de-During the last two decades there have been many forming force to a large number of cultured cell

For these reasons when designing the current ex-
lated at a frequency of 20 Hz, displacement amplitude

Table 1. Optimal parametric data of mechanical induction of proliferation of osteoblast like cells *in vitro* in different studies.

Reference	Frequency Hz	Displacement mm	Acceleration mm/sec ²	Time hours	Wave shape	Cells	Origin	Parameters investigated
Buckley et al. (1988)	0.05	$0.009^{\rm a}$	0.00089 ^b	48	square	Osteoblasts	chicks	DNA.Cell No.
Tjandrawinata et al. (1997)	$20 - 2000$	NI	50000	0.12	sine	MC3T3E1	rat	mRNA:c-fos,c-myc
Neidlinger-Wilke et al. (1994)		0.0003^{a}	0.0112^{b}	1.2	NI	Osteoblasts	human	Cell No.
Jones et al. (1991)		0.0003^{a}	0.0112^{b}	0.07	NI	Osteoblasts	bullock	Cell No.
Stanford et al. (1995)	0.5	0.003^{a}	0.03°	6	square	MC3T3E1	rat	DNA
Present study	20	0.025	450-550	0.13	sine	Osteoblasts	human	DNA

NI - not indicated

average displacement estimated from strains applied to cells, assuming that the diameters of osteoblasts are in the range of $20-40 \mu m$. **b** calculated with approximation to sine shaped vibration.

as a result of this study. There is no information on the actual pattern of the mechanical deformation of cells
actual pattern of the mechanical deformation of cells
and at what extent the media flow shearing forces and
ac well plate movement contribute to it. There is also no Bone 23: 409-415. information on the interactions between the cell cyto-
skeleton activation by the presumed cell deformation Jordan R. et al. 1988. Osteoblasts increase their rate of division Skeleton activation, by the presumed cell deformation, Jordan R. et al. 1988. Osteoblasts increase their rate of division and the intracellular secondary messengers that activated and align in response to cyclic, mechanica and the intracellular secondary messengers, that acti-
vate the observed proliferation and metabolic re-
sponses. These key questions will be addressed in
the and sense in the mechanosensitivity. Bone 22: 127S-130S. future studies on the development of this experimental Duncan R.L. and Turner C.H. 1995. Mechanotransduction and

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the surface of a 24 well plate. The values of Jacobs C.R., Yellowley C.E., Davis B.R., Zhou displacement, frequency and acceleration can be ontrolled and recorded.

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