

## Supplementary information

### Supplementary Figure S1.

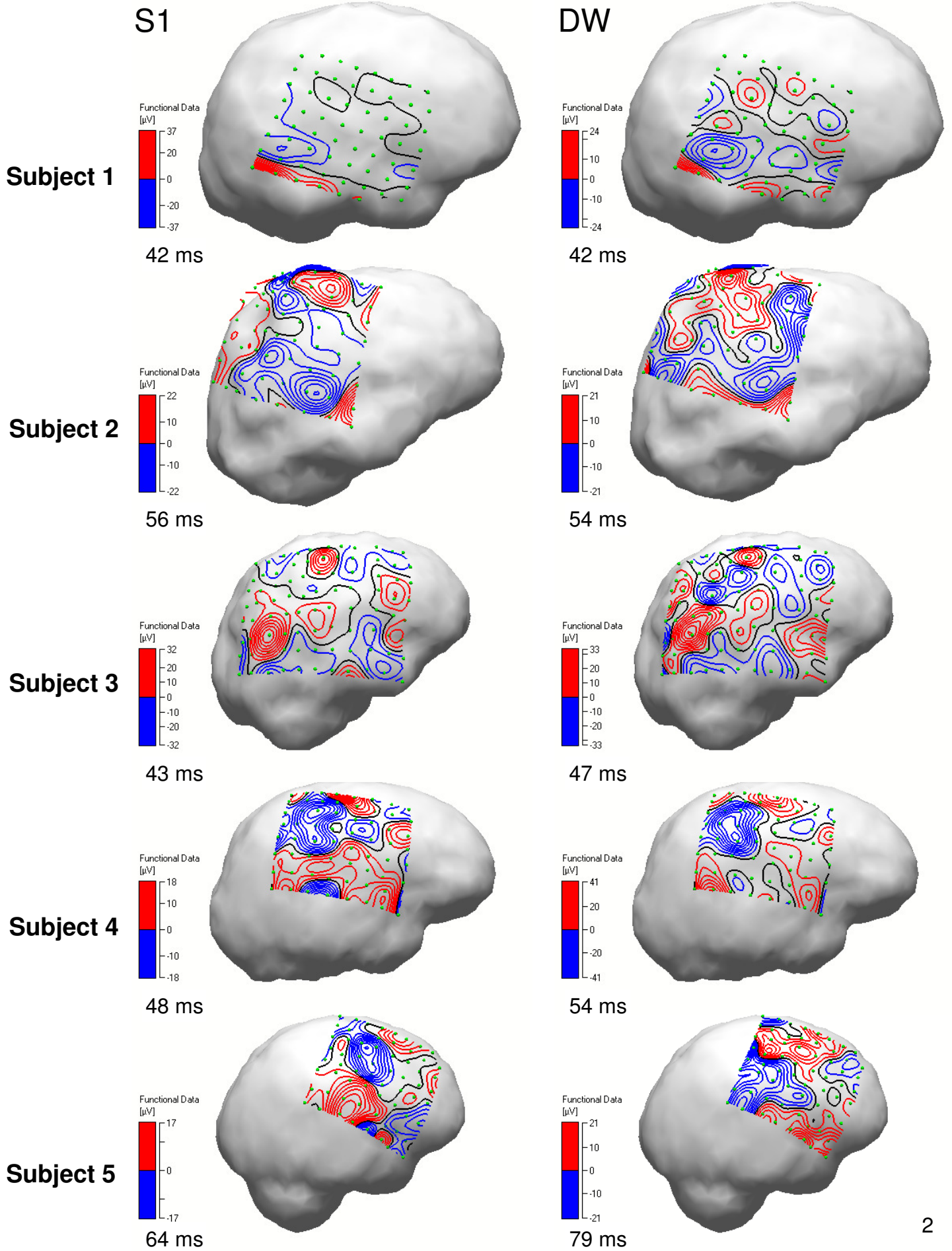
The grid coverage (electrodes shown in green), surface potential maps (negativity in blue and positivity in red) and source reconstruction images from 20 subjects (10-10 grids over lateral surfaces of the right and left hemispheres, respectively) are shown in the following images. Both S1 and DW (difference wave: S1-S2) data are present.

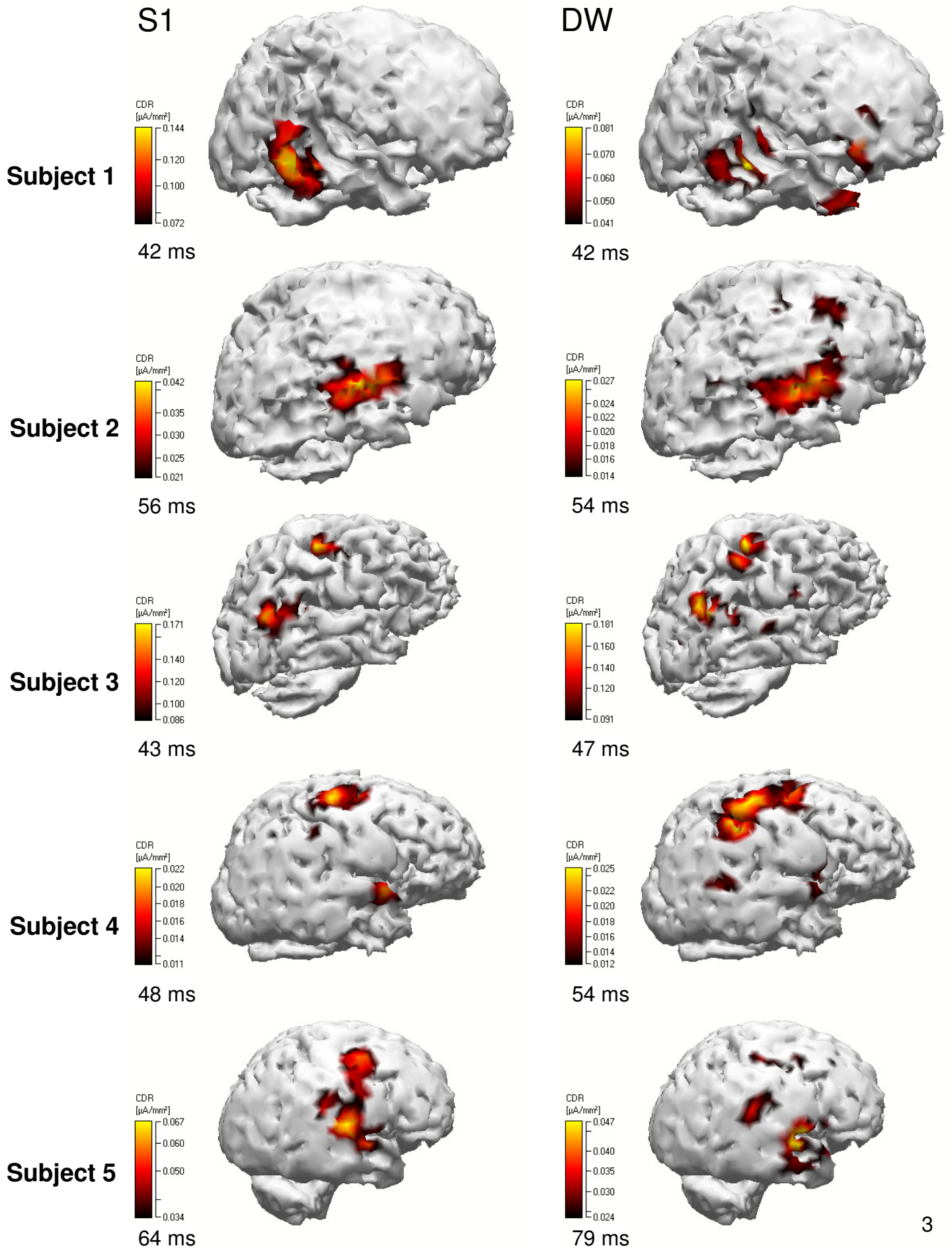
Only data from grids with a sufficient number of electrodes (minimum 64 electrodes) were used for source localization. There were 20 subjects with this arrangement. CURRY software (Neuroscan, Compumedics Ltd.) was used for head modeling and source estimation. The sensor 3D positions were extracted from grids in post-implantation MRIs via identification of four corner electrodes and subsequent linear interpolation of electrode positions for the full array. To allow extended current patterns to be mapped, a weighted minimum-norm technique (LORETA: low resolution electromagnetic tomography) was used to estimate current density distributions from S1 signal P50 potentials and so-called difference waves (S1-S2). LORETA solution is based in the assumption of neighboring sources having similar strengths and allows reconstruction of smooth current distributions. Individual BEM (boundary element model) head models were created from the subjects' MRI data and used to solve the forward problem.

Segmentation of the MRI data was performed in order to obtain the boundaries on the surface of the brain and inner skull that enclose tissue compartments which are assumed to be homogeneous and isotropic, with known conductivity values (0.33 and 1.79 S/m, respectively). This involved a routine of realistic head modeling in Curry software via high resolution discretisation of the surfaces with approximately 3500 nodes (about 2000 nodes representing the innermost brain compartment and about 1500 nodes for the CSF's BEM surface). As part of the distributed current density reconstructions with LORETA, the source locations were defined in the cortical surface (source space included thousands of locations and was defined by a sufficiently high sampling of the segmented cortical surface). A rotating source type was used instead of fixed source orientations (i.e. cortical surface normals) in order to allow estimation of omnidirectional currents and minimize the effects of nonoptimal surface segmentations. Noise level in the evoked responses was estimated from the pre-stimulus interval (-100 to 0 ms). Current density regularization parameter lambda (controlling the trade-off between data and the model) was optimized so that the residual deviation equaled 1/SNR (signal-to-noise ratio).

The optimal head modeling for intracranial data is still a matter of research. The use of a single-compartment BEM model has been preferred in conjunction with a spatially smoothed source space in order to avoid the issue of whether grid cortical recordings allow one to reliably define source depth. However, if the latter is true, it is unclear what source localization would provide in addition to cortical surface potential maps. Here, we used a two-compartment BEM model including the innermost brain and cerebrospinal fluid (CSF) compartments.

The main purpose of source localization from grid electrodes was to show differences in terms of individual regions that are involved in both or predominantly in one of two studied processes such as stimulus registration during P50 phase and repetition suppression.

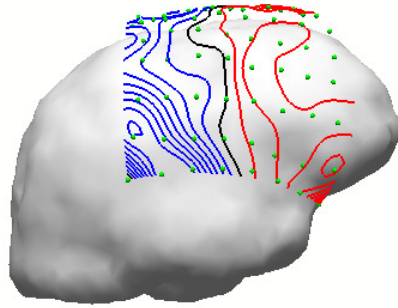
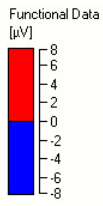




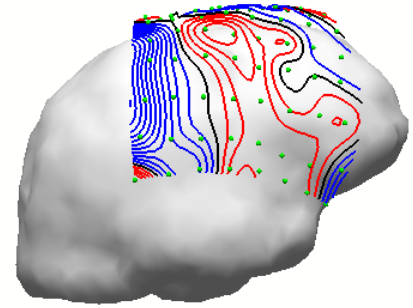
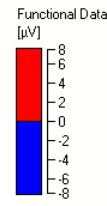
S1

DW

Subject 6

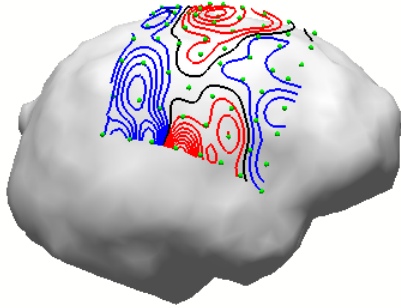
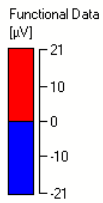


56 ms

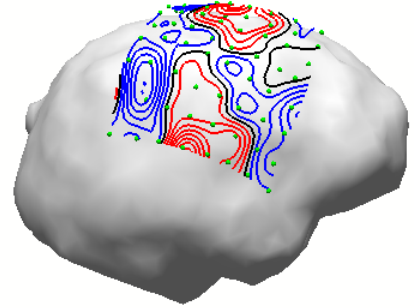
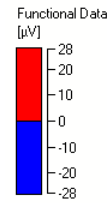


73 ms

Subject 7

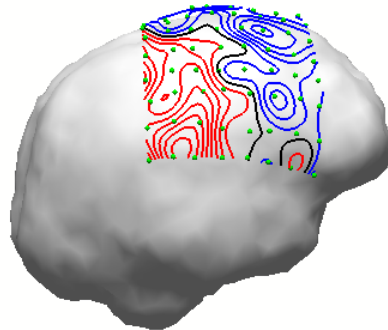
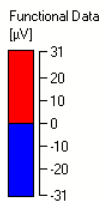


51 ms

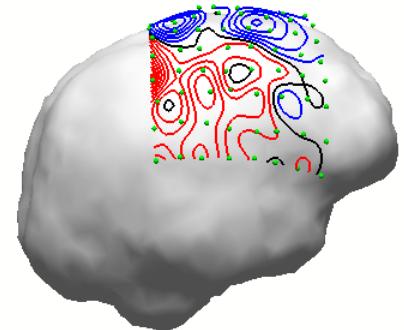
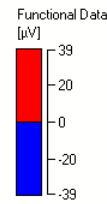


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Subject 8

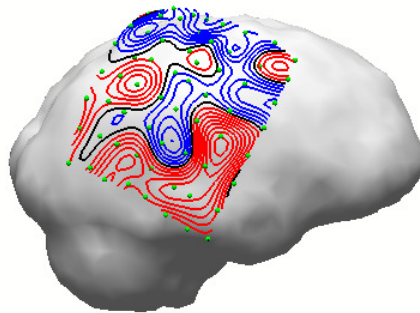
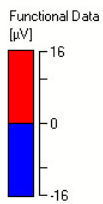


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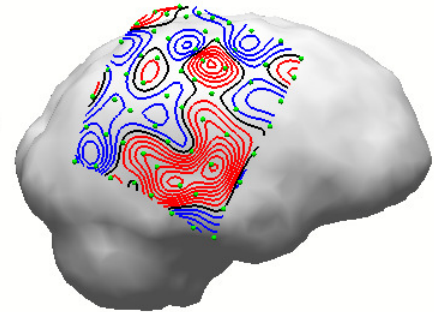
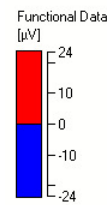


58 ms

Subject 9

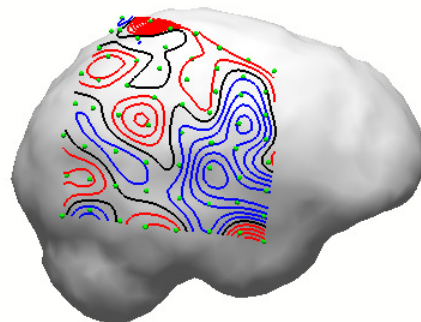
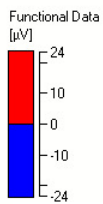


73 ms

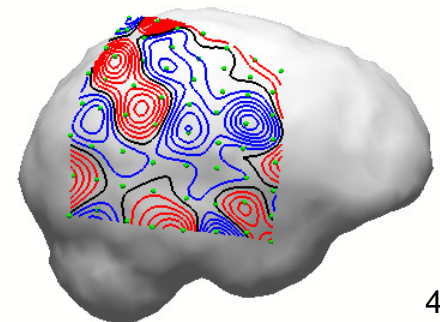
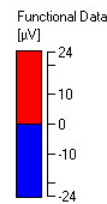


78 ms

Subject 10



58 ms

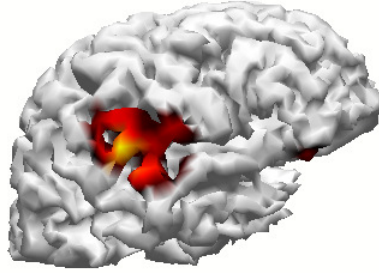
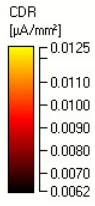


63 ms

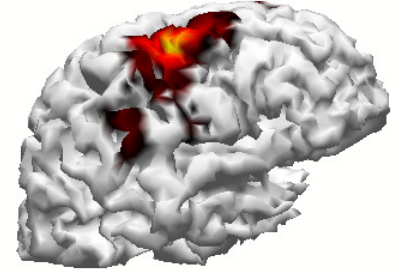
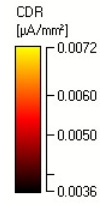
S1

DW

Subject 6

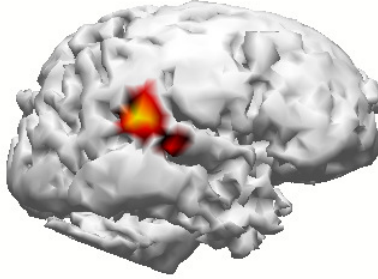
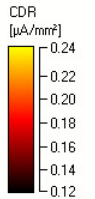


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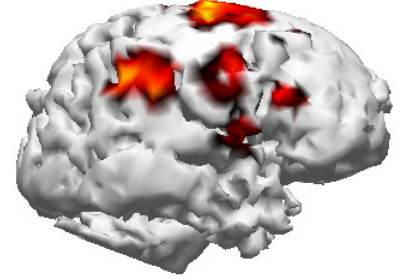
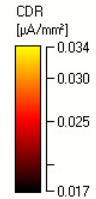


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Subject 7

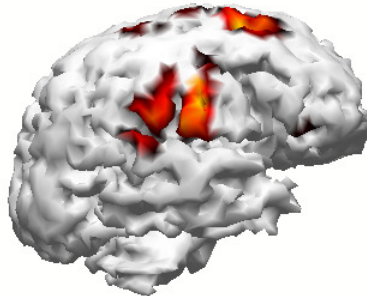
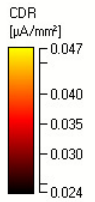


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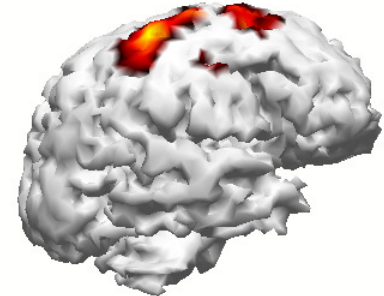
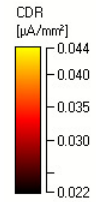


60 ms

Subject 8

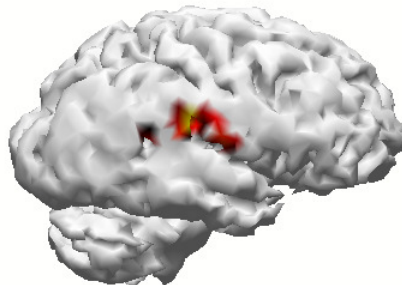
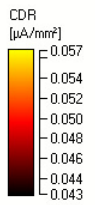


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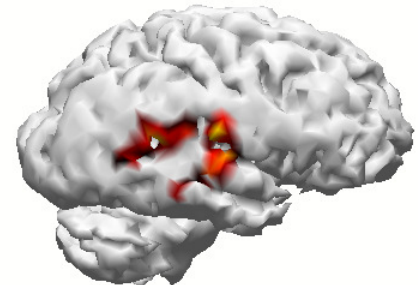
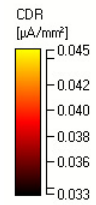


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Subject 9

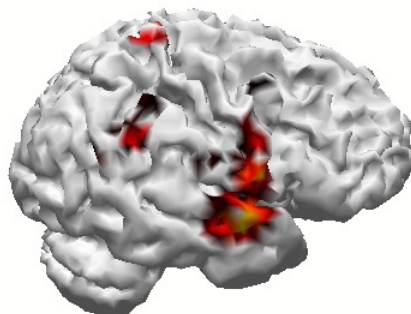
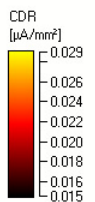


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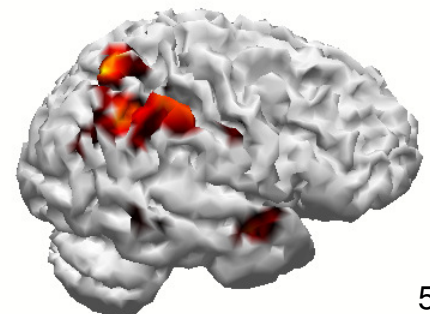
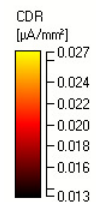


78 ms

Subject 10



58 ms



63 ms

