

Appendix: Model Equations

Calcium Input

The model input is a time-varying intracellular calcium concentration, described by the following equation.

$[\text{Ca}^{2+}](t) = \begin{cases} \frac{\text{Ca}_{max}}{2} \left(1 - \cos\left(\frac{\pi t}{T_1}\right)\right) & \text{if } 0 \leq t < T_1 \\ \frac{\text{Ca}_{max}}{2} \left(1 + \cos\left(\frac{\pi(t - T_1)}{T_2 - T_1}\right)\right) & \text{if } T_1 \leq t < T_2 \\ 0 & \text{otherwise} \end{cases}$	(A.1)
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Cardiac Muscle Model

Passive force generated by stretching the muscle unit is given by:

$F_p = K(L - L_0)^5,$	(A.2)
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while active muscle force depends on two main factors: elongation of cross-bridges and concentration of attached cross-bridges. Elongation of cross-bridges is equal to $L - X$, where the return to equilibrium is governed by:

$\frac{dX}{dt} = B(L - X - h_c).$	(A.3)
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Concentration of attached cross-bridges is linked to a chemical reaction network involving four species whose concentrations can be computed by:

$\frac{d[\text{TCa}]}{dt} = Q_b - Q_a$	(A.4)
$\frac{d[\text{TCa}^*]}{dt} = Q_a - Q_r - Q_{d1}$	
$\frac{d[\text{T}^*]}{dt} = Q_r - Q_d - Q_{d2}$	
$Q_a = Y_2 \cdot [\text{TCa}]_{eff} - Z_2 \cdot [\text{TCa}^*]$ $Q_b = Y_1 \cdot [\text{Ca}^{2+}] \cdot [\text{T}] - Z_1 \cdot [\text{TCa}]$ $Q_r = Y_3 \cdot [\text{TCa}^*] - Z_3 \cdot [\text{T}^*] \cdot [\text{Ca}^{2+}]$	(A.5)

$Q_d = Y_4 \cdot [T^*]$ $Q_{d1} = Y_d \cdot \left(\frac{dX}{dt}\right)^2 \cdot [TCa^*]$ $Q_{d2} = Y_d \cdot \left(\frac{dX}{dt}\right)^2 \cdot [T^*]$	
$[TCa]_{eff} = [TCa]e^{-R(L-L_a)^2}$ $[T] = T_t - [TCa^*] - [TCa] - [T^*].$	(A.6)

Finally, force generated by cross-bridges is related to concentration of attached cross-bridges and elongation of cross-bridges by:

$F_b = A([TCa^*] + [T^*])(L - X).$	(A.7)
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Total force generated by the muscle unit is thus:

$F = F_b + F_p.$	(A.8)
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A series elastic element is added to the muscle unit, whose force F_s and length L_s are given by:

$F_s = \alpha(e^{\beta L_s} - 1)$	(A.9)
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$F = F_s$	(A.10)
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$L_t = L + L_s.$	(A.11)
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Ventricular Model

The spherical ventricle model consists of an arrangement of N_c half-sarcomeres on the circumference of a sphere. The number N_c of half-sarcomeres is given by:

$V_{mw} = K_v L_t^3$ $K_v = \frac{N_c^3}{6\pi^2}.$	(A.12)
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The pressure inside the spherical ventricle can be obtained by the following relationship:

$P_{lv} = 5 \frac{F}{L_r} \frac{V_w}{K_v L_t^2}$	(A.13)
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To derive the total length of the muscle unit from the ventricle volume V_{lv} , the following equation is used:

$L_t = \sqrt[3]{\frac{V_w f + V_{lv}}{K_v}}$	(A.14)
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Cardiovascular system model

Pressure in the right ventricle is given by:

$P_{rv} = e(t) E_{rv} V_{rv}$	(A.15)
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with

$e(t) = \sum_{i=1}^3 A_i e^{-B_i(t-C_i)^2}$	(A.16)
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The other elastic chambers are passive, hence

$P_{ao} = E_{ao} V_{ao}$	(A.17)
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$P_{vc} = E_{vc} V_{vc}$	(A.18)
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$P_{pa} = E_{pa} V_{pa}$	(A.19)
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$P_{pu} = E_{pu} V_{pu}$	(A.20)
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Flows between chambers are computed by Poiseuille's law:

$Q_{mt} = r \left(\frac{P_{pu} - P_{lv}}{R_{mt}} \right)$	(A.21)
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$Q_{av} = r \left(\frac{P_{lv} - P_{ao}}{R_{av}} \right)$	(A.22)
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$Q_{sys} = \frac{P_{ao} - P_{vc}}{R_{sys}}$	(A.23)
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$Q_{tc} = r \left(\frac{P_{vc} - P_{rv}}{R_{tc}} \right)$	(A.24)
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$Q_{pv} = r\left(\frac{P_{rv} - P_{pa}}{R_{ap}}\right)$	(A.25)
$Q_{pul} = \frac{P_{pa} - P_{pu}}{R_{pul}}$	(A.26)

where r denotes the ramp function, defined as

$r(x) = \begin{cases} 0, & x < 0 \\ x, & x \geq 0. \end{cases}$	(A.27)
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The volume change in the six chambers can be derived from the continuity equation:

$\frac{dV_{lv}}{dt} = Q_{mt} - Q_{av}$	(A.28)
$\frac{dV_{ao}}{dt} = Q_{av} - Q_{sys}$	(A.29)
$\frac{dV_{vc}}{dt} = Q_{sys} - Q_{tc}$	(A.30)
$\frac{dV_{rv}}{dt} = Q_{tc} - Q_{pv}$	(A.31)
$\frac{dV_{pa}}{dt} = Q_{pv} - Q_{pul}$	(A.32)
$\frac{dV_{pa}}{dt} = Q_{pul} - Q_{mt}$	(A.33)