## Supplemental figures for case (v)

This SI shows results from simulations where the interstitial conductivity is increased by scaling  $K_l$  and  $D_s$  by a factor of 10 for tumor and normal tissue.

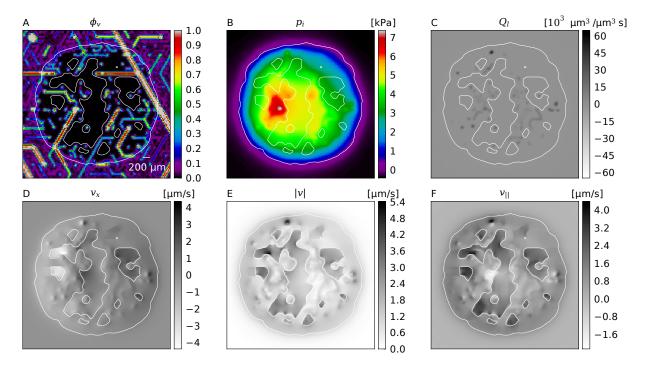


Figure 1: Snapshots of interstitial fluid flow related quantities. Corresponds to Figure 4 in the paper.

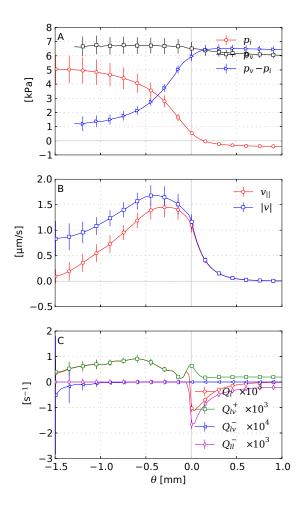


Figure 2: Averages of IF flow quantities vs. distance from tumor surface  $\theta$ . Corresponds to Figure 5 in the paper.

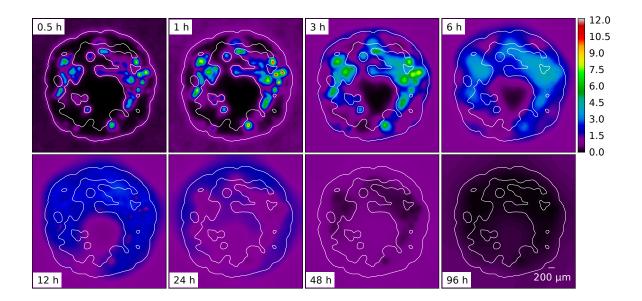


Figure 3: **Drug distribution** s in a series of snapshots. Corresponds to Figure 7 in the paper.

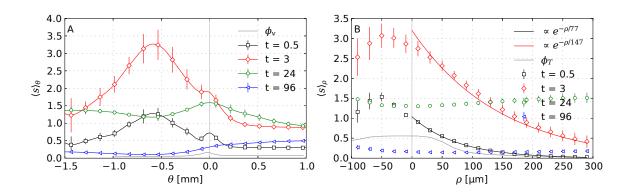


Figure 4: **Drug concentration profiles at different times.** (A) plotted vs.  $\theta$ , and (B) vs. distance from vessels  $\rho$ . Corresponds to Figure 8 in the paper.

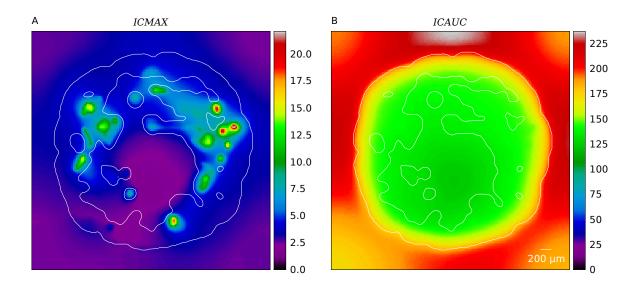


Figure 5: **Spatial distribution of drug exposure metrics.** (A) maximum concentration ICMAX and (B) the AUC ICAUC, taken from a slice through the origin of the system. Corresponds to Figure 9 in the paper.

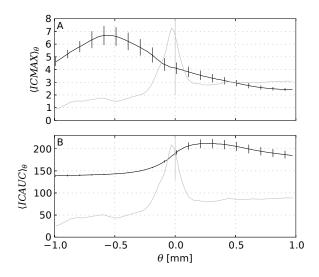


Figure 6: **Drug exposure metrics profiles.** Maximal concentration ICMAX (A) and area under curve ICAUC (B) plotted vs.  $\theta$ . Corresponds to Figure 10 in the paper.

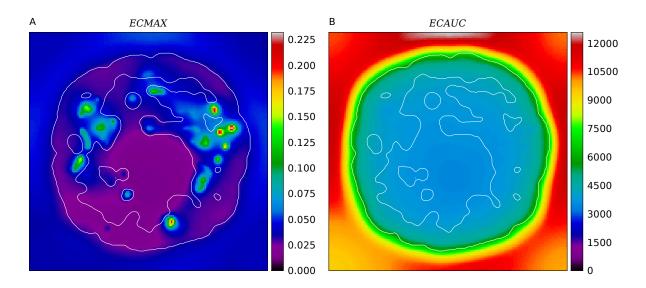


Figure 7: Maximal concentration (A) and area under curve (B) for the concentration in the interstitial compartment.

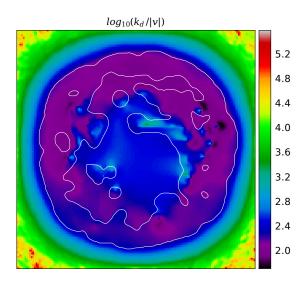


Figure 8: Logarithmic plot of the length scale  $L_{dc}$ . It is defined by  $L_{dc} = k_d/|v|$  following the requirement that the Peclet number equals one, i.e.  $1 = Pe = L_{dc}|v|/k_d$ . The data is scaled logarithmically.