Chromatin Hydrodynamics

Robijn Bruinsma,[†]* Alexander Y. Grosberg,[‡] Yitzhak Rabin,[§] and Alexandra Zidovska[¶]

[†]Department of Physics and Astronomy, Department of Chemistry and Biochemistry, University of California at Los Angeles, Los Angeles, California; [‡]Department of Physics and Center for Soft Matter Research, New York University, New York, New York; [§]Department of Physics, and Institute for Nanotechnology and Advanced Materials, Bar Ilan University, Ramat Gan, Israel; [¶]Department of Systems Biology, Harvard Medical School, Boston, Massachusetts; and ^{||}School of Engineering and Applied Sciences, Department of Physics, Harvard University, Cambridge, Massachusetts

ABSTRACT Following recent observations of large scale correlated motion of chromatin inside the nuclei of live differentiated cells, we present a hydrodynamic theory—the two-fluid model—in which the content of a nucleus is described as a chromatin solution with the nucleoplasm playing the role of the solvent and the chromatin fiber that of a solute. This system is subject to both passive thermal fluctuations and active scalar and vector events that are associated with free energy consumption, such as ATP hydrolysis. Scalar events drive the longitudinal viscoelastic modes (where the chromatin fiber moves relative to the solvent) while vector events generate the transverse modes (where the chromatin fiber moves together with the solvent). Using linear response methods, we derive explicit expressions for the response functions that connect the chromatin density and velocity correlation functions to the corresponding correlation functions of the active sources and the complex viscoelastic moduli of the chromatin solution. We then derive general expressions for the flow spectral density of the chromatin velocity field. We use the theory to analyze experimental results recently obtained by one of the present authors and her co-workers. We find that the time dependence of the experimental data for both native and ATP-depleted chromatin can be well-fitted using a simple model—the Maxwell fluid—for the complex modulus, although there is some discrepancy in terms of the wavevector dependence. Thermal fluctuations of ATP-depleted cells are predominantly longitudinal. ATP-active cells exhibit intense transverse long wavelength velocity fluctuations driven by force dipoles. Fluctuations with wavenumbers larger than a few inverse microns are dominated by concentration fluctuations with the same spectrum as thermal fluctuations but with increased intensity.

INTRODUCTION

Nuclei of living cells are places of intense activity (1). DNA-encoded genes are transcribed into messenger RNA strands by RNA polymerases. Helicases provide access for the RNA polymerases to a DNA molecule by unwinding and unzipping it. Topoisomerases control the supercoiling of DNA. The enzymatic activity is fueled by the consumption of free energy obtained from ATP hydrolysis and from other sources. Chromatin serves as a substrate for this activity. Chromatin is composed of centimeter-long DNA molecules wound around spool-like histone octamers, the nucleosomes, comprising the so-called 10-nm fiber. In the less dense regions of the nucleus, referred to as "euchromatin", the 10-nm fiber is packed rather loosely, allowing easy access to DNA for DNA-associating proteins. The more densely packed regions are referred to as "heterochromatin". Genes located inside the heterochromatin regions require local decondensation to allow for gene expression (2). This is facilitated by the covalent modification of the histone proteins through acetylation, methylation, and phosphorylation, which modulates the affinity of nucleosomes for each other. In addition, ATP-consuming chromatin remodeling complexes actively rearrange the positions of nucleosomes (3).

Editor: Gijsje Koenderink.

© 2014 by the Biophysical Society 0006-3495/14/05/1871/11 \$2.00



The content of a cell nucleus is quite complex. The chromatin 10-nm fiber described above is immersed in a viscous liquid, the nucleoplasm, which itself has a very rich composition: it contains not only free proteins, nucleotides, RNAs, small molecules and salts, but also nucleoli and subnuclear bodies such as Cajal bodies and paraspeckles or PML bodies. During interphase-the time in the cell cycle between two cell divisions-the content of the nucleus can, to first approximation, be viewed as a rather concentrated and nonuniform chromatin solution in which 10-nm fiber material, a gigantic polymer, is dissolved in a fluid comprised of much smaller molecules. We will refer to this solvent fluid as "nucleoplasm" (thus ignoring the presence of subnuclear bodies). In this chromatin solution, the chromatin fiber itself may have higher levels of organization, such as the (lately much disputed (4,5)) 30-nm fiber.

Chromatin dynamics has been investigated by high-resolution imaging of fluorescently labeled nuclear proteins and single DNA sites. Early work concluded that, during interphase, chromatin underwent constrained (corralled) diffusive motion with typical diffusion constants of the order of $10^{-4} \ \mu m^2/s$ (6–8). Analysis of three-dimensional tracks of labeled telomeres revealed subdiffusive motion up to timescales of 10–100 s (9). Tracking of labeled lac-operator sites on chromatin showed both ATP and thermally driven dynamics. Long periods of constrained diffusion were observed, followed by short bursts of superdiffusive directed motion (150-nm leaps of ~1 s). Upon ATP depletion, only

Submitted September 12, 2013, and accepted for publication March 19, 2014.

^{*}Correspondence: bruinsma@physics.ucla.edu

localized motion was observed (10). Trajectories of micronsized microinjected particles (11) were found to be constrained within cages of ~250 nm size while ATP-dependent subdiffusion of chromosomal loci was observed in bacterial cells and in yeast cells (12). Interphase chromatin of embryonic stem cells was observed to execute ATP-dependent periodic breathing motion on timescales of 0.1–0.01 s, with amplitudes of ~100 nm (13). This breathing motion is suppressed for differentiated cells while the fraction of condensed chromatin increases. The architectural proteins that maintain the structure of chromatin are hyperdynamic in pluripotent embryonic stem cells but are increasingly immobilized upon differentiation (14).

A microrheology study of the viscoelastic properties of chromatin using 100-nm beads has found predominantly elastic behavior in the frequency range 0.2–5.0 Hz with broadly distributed values of storage and loss moduli (15). Very different values for the moduli were reported in studies of the displacement of a spherical magnetic nanoparticle of 1- μ m diameter (16) and the rotation of a cylindrical magnetic nanoparticle of 1.5- μ m length and 0.2- μ m diameter (17). A macroscopic rheology study using time-dependent deformation of entire cells with fluorescently labeled nuclei has found that nuclei of embryonic stem cells and those of cells lacking A/C lamins were much more deformable than those of differentiated cells (18).

All these studies focused on the tracking of a small number of tracer particles. In a recent study, fluorescently labeled histones were used to map the chromatin movement simultaneously across the entire nucleus (19). The study showed that chromatin motion of human HeLa cells appears to be spatially correlated over length scales ranging from 250 nm to 5 μ m. This is a surprising result: individual events such as gene expression, DNA replication, or DNA repair are presumably highly specific so one would not expect large- scale correlations. The aim of this article is to provide a theoretical framework for the analysis of studies of ATP-driven chromatin dynamics. The basic theoretical assumption of the proposed framework is that the velocity fluctuations inside chromatin can be described within linear response theory applied to a viscoelastic two-fluid model.

The response of the chromatin solution to both thermal fluctuations and to active events is determined by the dynamic susceptibility of the two-fluid model. It could be questioned whether a very complex system such as chromatin could be described by any simple theoretical model. Linear hydrodynamic properties of complex systems are in general determined by conservation laws and symmetry. These properties depend on the molecular details of the local structure of the material only insofar as these determine the numerical value of the response moduli of the system. For the case of chromatin, conservation of solvent and conservation of 10-nm fiber material plays such a role. In terms of symmetry, the chromatin solution is treated as a fluid in the sense that the 10-nm fiber is not restrained by any three-dimensional network of covalent cross-links (even if there are higher levels of organization) so the shear modulus at low frequencies should be zero. Moreover, the chromatin solution appears to be relatively isotropic on length scales from tens of nanometers to several microns. We will show that one can similarly classify active events as scalar or vectorial, depending on symmetry considerations.

An important motivation for adopting this methodology was that the hydrodynamic method has been applied with success to active gels such as the actin-myosin system with motor protein activity treated as a distribution of force dipoles. The motor activity produced highly correlated, lowfrequency shear fluctuations through coupling to long-wavelength shear modes of the gel. A recent review summarizes studies of soft materials where large-scale cooperativity and hydrodynamic fluctuations are driven by active force dipoles (20).

We propose that a study of the collective dynamics of chromatin might well be relevant to questions concerning gene expression that are of interest to the life-science community. Collective gene expression events can occur as part of the natural progression through the cell cycle or in response to external signaling cues or environmental challenge. Different forms of collective gene expression could generate different active hydrodynamic fluctuation spectra. If that is the case, then the measurement of the flow spectral densities, as described in this article, could provide a new diagnostic tool for probing collective activity in the nucleus.

THEORY

Two-fluid model

We start with the specification of the linear hydrodynamics of an idealized chromatin solution that is homogeneous and has no sources of free energy consumption. This passive chromatin solution will be treated as a two-fluid model, a viscoelastic fluid composed of a solvent (i.e., the nucleoplasm) and a polymeric material (i.e., the chromatin fiber). The chromatin solution is assumed to have an accessible state of thermodynamic equilibrium with no osmotic or hydrodynamic pressure gradients. Chromatin itself is quite compressible: a change in volume fraction of the chromatin fiber in some region can be compensated by solvent (nucleoplasm) flow in or out of that region. The combined solution composed of polymers (chromatin fiber) plus solvent (nucleoplasm), however, will be treated as incompressible. The polymer volume fraction in this equilibrium state will be denoted by ϕ_0 . Deviations from this equilibrium state are described by the following set of collective hydrodynamic variables:

- 1. Solvent flow velocity \vec{v}^s ;
- 2. Polymer flow velocity \vec{v}^p ;
- 3. Deviation of polymer volume fraction from equilibrium $\delta \phi$;

Chromatin Hydrodynamics

- 4. Hydrodynamic pressure *P*; and
- 5. Osmotic pressure Π .

The linearized hydrodynamic equations of a two-fluid model (21) read as

$$\zeta(\vec{v}^p - \vec{v}^s) = \vec{\nabla} \cdot \overleftrightarrow{\sigma} - \vec{\nabla}\Pi - \phi_0 \vec{\nabla}P, \qquad (1)$$

$$\zeta(\vec{v}^s - \vec{v}^p) = -(1 - \phi_0) \vec{\nabla} P.$$
⁽²⁾

The derivation of these equations, based on general principles of linear response theory (see, e.g., Landau and Lifschitz (22) or Doi (23)) is summarized in Section S1 in the Supporting Material. Equation 1 relates the viscous drag exerted by the solvent on the chromatin polymer to the force per unit volume due to polymer-polymer interactions (first two terms) plus the hydrodynamic force per unit volume exerted on the polymer. The expression $\zeta \sim \eta_0 / \xi^2$ is the inverse of the solvent permeability of chromatin with η_0 the viscosity of the solvent and ξ the typical size of the pores of the chromatin. Next, σ is the (traceless) shear stress tensor of chromatin that is additional to the separately included (minus) gradient of the osmotic pressure Π . Equation 2 relates the viscous drag exerted by the polymers on the solvent with the hydrodynamic force per unit volume exerted on the solvent volume fraction (Darcy's law for porous media); this treatment neglects viscous stresses in the solvent on length scales larger than the mesh size (see Milner (24) for further details). Finally, osmotic pressure variations are related to concentration variations by $\Pi = K\delta\phi$ with K the osmotic modulus of the polymer system.

The hydrodynamics of chromatin will be assumed to be that of a generalized, linear, non-Newtonian, viscoelastic fluid. For such fluids, the shear stress tensor can be expressed as

$$iq_i\sigma_{ij}(\vec{q},\omega) = -E(q,\omega)\left(\frac{1}{3}q_jq_iv_i^p + q^2v_j^p\right).$$
 (3)

Here, $E(q,\omega)$ is a generalized complex shear viscosity of chromatin that depends on both wavevector and frequency. We will not specify the form of $E(q,\omega)$, which must be provided either by microrheological experiments or by a microscopic theory of the chromatin solution. $E(q,\omega)$ is related to the more familiar complex modulus by $G(q,\omega) = -i\omega E(q,w)$.

Our convention for the Fourier transforms in this expression is

$$\phi(\vec{q},\omega) = \int_{\Delta V} \int_{-\infty}^{\infty} \phi(\vec{r},t) e^{i(\omega t - \vec{q} \cdot \vec{r})} d\vec{r} dt, \qquad (4a)$$

$$\phi(\vec{r},t) = \frac{1}{\Delta V} \sum_{\vec{q}} \int_{-\infty}^{\infty} \phi(\vec{q},\omega) e^{i(-\omega t + \vec{q} \cdot \vec{r})} \frac{d\omega}{2\pi}, \qquad (4b)$$

and treated similarly for the other fields. The value ΔV is nucleus volume. Wavevector and frequency are limited by the fact that $q/2\pi$ must be large compared to the inverse of the size of the nucleus and $\omega/2\pi$ must be large compared to the inverse of the duration of the interphase stage.

The condition that the full system of solvent plus chromatin is incompressible can be expressed as

$$\nabla \cdot [(1 - \phi_0)\vec{v}^s + \phi_0\vec{v}^p] = 0, \tag{5}$$

while the linearized continuity equation for polymer material is

$$\partial \phi / \partial t + \phi_0 \vec{\nabla} \cdot \vec{v}^p = 0.$$
 (6)

This completes the hydrodynamic description of passive chromatin as a linear non-Newtonian, viscoelastic fluid. The next step is a description of the active sources. We start with so-called scalar events.

Scalar activity

Activity associated with the local condensation or decondensation of chromatin driven by free energy consumption is termed a "scalar event". Unlike the active force dipoles of the actin-myosin system mentioned in the Introduction, scalar activity is nondirectional. Thermal concentration fluctuations are explicitly excluded from the definition of scalar events. Fig. 1 shows schematically an example of a scalar event.

The shift is assumed to be due to a number of isolated events at different sites of the chromatin. In Section S1 in

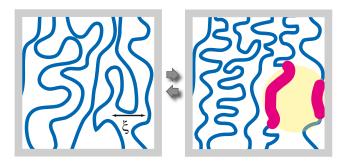


FIGURE 1 Example of a scalar event. (*Left panel*) Equilibrium state of chromatin. The length scale ξ indicates the average spacing between adjacent sections of the 10-nm fiber. (*Right panel*, *yellow region*) Localized region where 10-nm fiber has been chemically altered, with respect to the equilibrium state, by (de)acetylation and/or (de)methylation of the histones. Sections of the 10-nm fiber that have been chemically altered are shown (*red*). Neither the nucleosomes nor the enzymes that produce the alterations are shown. The chemical alteration causes a local change in the solubility of the 10-nm fiber, causing influx or efflux of solvent. (Also in *right panel*) Increased solubility of localized decondensation of the chromatin. (*Gray arrows*) These changes are reversible. (*Gray frame*) Field of view. To see this figure in color, go online.

the Supporting Material, it is shown that, in linear response theory, scalar activity can be included as a shift in the osmotic pressure of the form

$$\Pi(\vec{r},t) = K\delta\phi(\vec{r},t) - \alpha(\vec{r},t),$$

where

$$\alpha(\vec{r},t) = \sum_{k} s_k \delta(\vec{r} - \vec{R}_k) g(t - t_k)$$
(7)

is the activity function. Here, s_k indicates the sign and strength of the condensation or decondensation event at location \vec{R}_k at some time t_k . The dimensionless function g(t) is zero for negative arguments whereas for positive arguments it decays with time. A simple choice for g(t)would be

$$\theta(t)\exp(-t/\tau_a),$$

with τ_a the typical duration of such an event and $\theta(t)$ the step function, which equals 1 for positive arguments and 0 for negative arguments.

Single scalar event

Assume that only one scalar event takes place, at the origin at time t = 0. The linearized force-balance equation is then

$$\zeta(\vec{v}^p - \vec{v}^s) = \vec{\nabla}\vec{\sigma} - K\vec{\nabla}\delta\phi - \phi_0\vec{\nabla}P + s\vec{\nabla}\delta(\vec{r})g(t).$$
(8)

In a few lines of algebra, this yields

$$\frac{\partial \delta \phi}{\partial t} = D \nabla^2 \delta \phi - \tilde{s} \nabla^2 \delta(\vec{r}) g(t) - \frac{\left(1 - \phi_0\right)^2}{\zeta/\phi_0} \vec{\nabla} \cdot \left(\vec{\nabla} \, \vec{\sigma}\right), \ (9)$$

with

$$D = K \frac{(1-\phi_0)^2}{\zeta/\phi_0}$$

and

$$\tilde{s} = s \frac{\left(1 - \phi_0\right)^2}{\zeta/\phi_0}.$$

We can identify D as a collective diffusion constant. This equation can be viewed as defining a Green's function for scalar events. In Section S2 in the Supporting Material, we solve this equation for the special case of a Newtonian fluid. It is found to describe a localized change in polymer concentration at the origin plus a transient collective diffusion pulse that travels radially outwards from the origin. The volume integral over the concentration variation is 0: no new material is introduced by the localized change in solubility.

Distributed scalar events

For the general case of a spatial and temporal distribution of scalar events, the concentration profile induced by the scalar events can be shown to be given by the linear response equation

$$\delta\phi(\vec{q},\omega) = \chi(q,\omega)\alpha(\vec{q},\omega), \qquad (10)$$

where

$$\chi(q,\omega) = \frac{iq^2\phi_0}{\omega\left[\frac{\zeta}{(1-\phi_0)^2} + \frac{4}{3}E(q,\omega)q^2\right] + iq^2K\phi_0}$$
(11)

is the dynamic susceptibility; see Section S3 in the Supporting Material for the derivation. In the limit of zero frequency, $\chi(q,\omega = 0)$ reduces to the static osmotic susceptibility 1/K. The dynamic susceptibility has pole singularities in the lower-half of the complex frequency plane that correspond to the collective modes of the system. In Section S7 in the Supporting Material, as a matter of a mathematical example, we work out the calculations for the artificial case when passive chromatin is assumed to have the rheological properties of the Maxwell fluid. Two collective modes are present in that case, corresponding to hybridized collective diffusion and stress relaxation.

Ensemble averaging of scalar events

Assume a sequence of scalar events is observed, e.g., the initiation or termination of the expression of a specific sequence of genes, DNA replication, or repair, etc. Because only a limited amount of data may be obtainable in a particular experiment on a given cell, strong statistical variations are to be expected. To reduce the effect of statistical variability, the experiment could be repeated for different cells at the same stage of the cell cycle and under the same stimulus conditions. The magnitude of the ensemble-averaged source activity $\langle \alpha(\vec{q}, \omega) \rangle$ then depends on the degree of correlation between different cells. If this ensemble average is nonzero, then according to the linear response theory there should be a nonzero ensemble-averaged longitudinal flow velocity pattern of the form

$$\left\langle v_{\parallel}^{p}(\vec{q},\omega) \right\rangle = \frac{\omega}{\phi_{0}q} \chi(q,\omega) \langle \alpha(\vec{q},\omega) \rangle.$$
 (12)

On the other hand, if $\langle \alpha(\vec{q}, \omega) \rangle$ averages to zero due to lack of correlation, one can still measure the ensemble-averaged second moment of the velocity fluctuations.

Assume an ensemble of cell nuclei at the same stage of the cell cycle and under the same external conditions for the case that gene expression is highly stochastic so that after ensemble averaging, the first moment is $\langle \alpha(\vec{q}, \omega) \rangle = 0$. If active events are locally correlated in space and in time, then the correlation should depend mainly on the time difference t - t' between events—assumed small compared with the characteristic timescale of the cell cycle—and on the distance $\vec{r} - \vec{r}'$ between events, assuming neither \vec{r} nor \vec{r}' are located close to the nuclear envelope. The second moment for stochastic active scalar events is defined as

$$\langle \alpha(\vec{q},\omega)\alpha^*(\vec{q}',\omega')\rangle = \Delta T \Delta V (\alpha^2)_{\vec{q},\omega} \delta_{\omega,\omega'} \delta_{\vec{q},\vec{q}'}, \qquad (13)$$

where the asterisk denotes complex conjugation. Wavevectors are discretized in the usual way by boundary conditions imposed at the surface of the volume ΔV of the nucleus (which do not need to be specified for $q \gg 1/\Delta V^{1/3}$). The Kronecker delta notation $\delta_{\vec{q},\vec{q}'}$ means that the two vectors \vec{q} and \vec{q}' must be equal. Frequency is discretized as well with a frequency interval $2\pi/\Delta T$. The timescale ΔT will be set to infinity at the end. In that limit, the Kronecker delta $\delta_{\omega,\omega}$ in the frequency domain reduces to a delta function as

$$rac{2\pi}{\Delta T}\delta(\omega-\omega')$$

If we denote the total number of active scalar events in the time interval ΔT by \mathcal{M}_s , then the number of scalar events $\rho_s = \mathcal{M}_s / \Delta T \Delta V$ per unit time per unit volume—the scalar event density—will be assumed to be finite in the limit that ΔT goes to infinity.

The quantity

 $\left(\alpha^2\right)_{\vec{q},\omega}$

will be referred to as the "power spectral density" (PSD) of active scalar events. To compute this quantity, we will take the definition of the scalar source term Eq. 7, multiply it by complex conjugate, and take an ensemble average. In the resulting double sum over event numbers k and k', only the k = k'terms are assumed to be nonzero under circumstances where the event strengths s_k are statistically independent from one another and from the event onset times and locations. Under these assumptions, the PSD of scalar events reduces to

$$(\alpha^2)_{\vec{q},\omega} \simeq \rho_s \langle s^2 \rangle |g(\omega)|^2.$$
 (14)

Similar spectral densities can be defined for the concentration and longitudinal velocity fields. Using the linear response relation Eq. 10, the PSDs of the concentration and the longitudinal velocity fields are related to the PSD of scalar events by

$$\left(\delta\phi^2\right)_{\vec{q},\omega} = |\chi(q,\omega)|^2 \left(\alpha^2\right)_{\vec{q},\omega},\tag{15a}$$

$$\left(v_{\parallel}^{2}\right)_{\vec{q},\omega} = \frac{\omega^{2}}{q^{2}\phi_{0}^{2}} |\chi(q,\omega)|^{2} (\alpha^{2})_{\vec{q},\omega}.$$
 (15b)

If the active events are uncorrelated, an explicit form can be given as

It is useful to compare these results with the spectrum of thermal concentration fluctuations of the passive fluid. The PSD of thermal fluctuations is determined by the fluctuation-dissipation theorem

$$\left(\delta\phi^2\right)_{\vec{q},\omega} = \frac{2k_{\rm B}T}{\omega} {\rm Im}[\chi(q,\omega)],$$
 (17)

which, in this case, reduces to

$$\left(\delta\phi^{2}\right)_{\vec{q},\omega} = \frac{2q^{2}\phi_{0}^{2}k_{\mathrm{B}}T\left(\frac{\zeta}{(1-\phi_{0})^{2}} + \frac{4}{3}\operatorname{Re}[E(q,\omega)]q^{2}\right)}{\left|\omega\left(\frac{\zeta}{(1-\phi_{0})^{2}} + \frac{4}{3}E(q,\omega)q^{2}\right) + iq^{2}K\phi_{0}\right|^{2}}.$$
 (18)

A comparison of the active (Eq. 16) and the passive (Eq. 18) PSD shows that, although they have the same denominator, the two expressions behave differently in long-wavelength limit. The active PSD, Eq. 16, goes to zero as q^4 at $q \rightarrow 0$ whereas the passive PSD, Eq. 18, is proportional to q^2 . That means that the ratio of the active and passive PSDs vanishes in the long wavelength limit. The extra q^2 factor in the active PSD arises from the fact that the active sources only enter through gradients in the equations of motion. Physically, because $\langle s \rangle = 0$, condensation and decondensation events balance each other over large distances. The active PSD also contains a factor

$$1/((\omega\tau_a)^2+1),$$

which reflects the sudden onset of a condensation/decondensation event. Because the ratio of the active and passive PSDs is q- and ω -dependent, and arising from fundamental physics constraints, it is, in general, not possible to define an effective noise-temperature for active scalar events. It should be noted that the power spectrum for the passive thermal concentration fluctuations has a subleading q^4 term, similar to the active power spectrum, whereas an active source stirring the solvent—not considered in this article—would produce a q^2 term, similar to the passive power spectrum. The difference between the q^4 and q^2 terms thus should not be viewed as reflecting a fundamental difference between active and passive fluctuations.

Vector activity

In the Introduction, we mentioned that many active softmatter systems are characterized by the production of force-dipoles. Because force generation by active proteins must obey the condition that there is no net momentum or angular momentum transfer to the chromatin, the total force and total torque must be zero. It follows also that, in this case, active force generation should be represented as a distribution of collinear force dipoles. Fig. 2 shows possible examples of active events in chromatin where a dipolar pair of collinear, opposing forces is produced. (See also Narlikar et al. (25).)

In Section S4 in the Supporting Material, we show that such a distribution of vector events can be included in our formalism as a contribution to the divergence of the active part of the stress tensor,

$$\vec{\nabla} \cdot \vec{\sigma}^{(\mathrm{ac})}(\vec{r},t) = fa \sum_{k=1}^{\mathcal{M}_{v}} \widehat{n}_{k} (\widehat{n}_{k} \cdot \vec{\nabla}) \delta(\vec{r} - \vec{R}_{k}) g(t - t_{k}),$$
(19)

with \mathcal{M}_{ν} the number of vector events in the time interval Δt . Each force dipole is composed of a pair of collinear opposing forces $f\hat{n}_k$ and $-f\hat{n}_k$ separated by a microscopic distance *a*. Here \hat{n}_k is a unit vector along the force direction. For the case of nucleosome rearrangement events, *a* would have the typical size of a spacer length between nucleosomes.

Single vector event

A single active vector event at the origin at time t = 0 induces a transverse velocity flow field given by

$$\vec{v}_{\perp}(\vec{q},\omega) = ifag(\omega) \frac{\vec{P}(\vec{q}) \cdot \hat{n}(\hat{n} \cdot \vec{q})}{q^2 E(q,\omega)}.$$
 (20)

Here, $P_{ij}(\vec{q}) = \delta_{ij} - \hat{q}_i \hat{q}_j$ is the transverse projection operator defined with $\hat{q} = \vec{q}/q$ and $\hat{q}_i = q_i/q$. The equation for the transverse flow field is obtained by applying this projection operator to Eqs. 1 and 2. The transverse polymer and solvent flow velocities are the same in this case (and hereon indicated as the flow field, itself). The inverse Fourier transform can be viewed as the Green's function for vector events. For the special case of a Newtonian fluid, the flow field can be obtained explicitly, as discussed in Section S5 in the Supporting Material. The pattern of flow lines is that of extensional flow oriented along the force direction.

Distributed vector events

The flow field produced by a distribution of vector events is obtained by the superposition of the flow fields of individual sources. The activity function for a distribution of vector events is the linear superposition of individual events of the form of Eq. 20:

$$\vec{\beta}(\vec{q},\omega) = ifag(\omega) \sum_{k=1}^{M_{\nu}} \vec{P}(\vec{q}) \cdot \hat{n}_{k}(\hat{n}_{k} \cdot \hat{q}) e^{i\left(\vec{q} \cdot \vec{R}_{k} + \omega t_{k}\right)}.$$
 (21)

The associated flow field can be obtained by a simple linear response relation

$$\vec{v}_{\perp}(\vec{q},\omega) = \frac{1}{qE(q,\omega)}\vec{\beta}(\vec{q},\omega).$$
(22)

If, as for the scalar case, the ensemble-averaged flow field is very small, then the PSD of the velocity fluctuations is

$$\left(\vec{v}_{\perp}^{2}\right)_{\vec{q},\omega} = \left|\frac{1}{qE(q,\omega)}\right|^{2} \left(\vec{\beta}^{2}\right)_{\vec{q},\omega},\tag{23}$$

where the PSD for vector sources, $(\vec{\beta}^2)_{\vec{q},\omega}$, is defined as in Eq. 13 for the scalar PSD.

To compare this expression with the PSD for transverse thermal equilibrium fluctuations, we use again the fluctuation-dissipation theorem:

$$\left(\vec{v}_{\perp}^{2}\right)_{\vec{q},\omega} \simeq \frac{4k_{\rm B}T}{q^2} \operatorname{Re}\left[\frac{1}{E(q,\omega)}\right].$$
 (24)

This should be compared with the full Landau-Lifshitz expression for thermal hydrodynamic fluctuations in a Newtonian fluid (see, e.g., Lifshitz and Pitaevskii (26)),

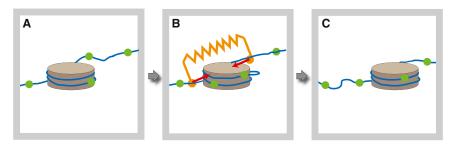
$$\left(\vec{v}_{\perp}^{2}\right)_{\vec{q},\omega} = k_{\rm B}T \frac{4\eta q^2}{\left(\omega\rho\right)^2 + \eta^2 q^4},\tag{25}$$

with ρ the mass density. For frequencies small compared to $\eta q^2 / \rho$, the two expressions agree if one sets $E = \eta$.

Comparing the spectrum of active fluctuations with that of transverse equilibrium thermal fluctuations, one sees

FIGURE 2 Example of a vector event. (A) The figure shows two steps of the translocation of one nucleosome (shown as a *disk*) along DNA. The dots (in *green*) along the DNA are position markers as a guide to the eye. In the first step (B), a chromatin remodeling enzyme binds to the nucleosome and applies equal but opposite forces on the DNA on opposite sides of the nucleosome. The enzyme is not shown, but its action is indicated by the spring (in *orange*). It leads to an excess of DNA wound around the nucleosome, which promotes formation of DNA loops that can diffuse along

the nucleosome. In the second step (C), the enzyme detaches, and the extra DNA is released by the nucleosome, resulting in nucleosome translocation. (*Gray frame*) Limited field of view. For other illustrations of the production of force dipoles in chromatin, see Fig. 2 in Narlikar et al. (25) or Fig. 2 in Racki and Narlikar (3). Many other types of events in the nucleus are associated with generation of localized force dipoles including—but not limited to—the action of RNA polymerases, helicases, topoisomerases, etc. To see this figure in color, go online.



that—unlike the scalar case—active vectorial events are not reduced by a factor q^2 as compared to the equilibrium fluctuation spectrum. If active events have a long lifetime, then the active spectrum carries again an extra factor $1/\omega^2$. In that case, active vector events should dominate at low frequencies.

Nematic order parameter

Ensemble averaging for vectorial events can be discussed conveniently by introducing a nematic order parameter field. A force dipole source, Eq. 19, (locally) breaks rotational symmetry at the site of the force dipole event while maintaining inversion symmetry $\hat{n} \leftrightarrow -\hat{n}$ as reflected by Eq. 21. If the orientations of different force dipoles across the chromatin are correlated, then rotational symmetry could be broken on larger length scales. To examine the development of nematic order, we define the density $\rho_{v}(\vec{r},t)$ of vector events and the nematic order parameter as

$$\rho_{\nu}(\vec{r},t) = \sum_{k} \delta(\vec{r} - \vec{R}_{k}) \delta(t - t_{k}), \qquad (26a)$$

$$Q_{ij}(\vec{r},t) = \sum_{k} \delta\left(\vec{r} - \vec{R}_{k}\right) \delta(t - t_{k}) \left[\widehat{n}_{i}^{(k)} \widehat{n}_{j}^{(k)} - \frac{1}{3} \delta_{ij}\right].$$
(26b)

A similar formulation, in terms of fields instead of individual events, can be found in MacKintosh and Levine (27). In terms of the force dipole distribution, a chromatin solution would be a uniaxial or biaxial nematic if the spatial and temporal average $\langle Q_{ij} \rangle$ of $Q_{ij}(\vec{r}, t)$ would be nonzero. In terms of the event density and the nematic order parameter field, Eq. 19 then reads as

$$\vec{\nabla} \cdot \vec{\sigma}^{(\mathrm{ac})}(\vec{r},t) = fa \int d^{3}\vec{r}' dt'g(t-t') \\ \times \left[\overleftrightarrow{Q}(\vec{r}',t') + \frac{1}{3}\overrightarrow{I}\rho(\vec{r}',t') \right] \cdot \vec{\nabla}\,\delta(\vec{r}-\vec{r}').$$
(27)

An ensemble-averaged activity function for vectorial events $\langle \vec{\beta}(\vec{q},\omega) \rangle$ can be defined in analogy to the ensemble-averaged activity function $\langle \alpha(\vec{q},\omega) \rangle$ for scalar activity. In terms of the nematic order parameter:

$$\left\langle \vec{\beta}(\vec{q},\omega)\right\rangle = ifag(\omega)\vec{P}(\vec{q}) \cdot \left\langle \vec{Q}(\vec{q},\omega)\right\rangle \cdot \hat{q}.$$
 (28)

The nucleus could have a broken rotational symmetry of the nematic type either because the orientations of the different force dipoles are correlated due to the intrinsic structural organization of the nucleus (which may or may not be related to the liquid-crystalline ordering possible in the suspensions of nucleosome particles (28)). Another, and even more interesting, possibility is that the symmetry-breaking is dynamic. The hydrodynamic backflow of active force dipoles produces the aligning torques on neighboring dipoles. Spontaneous nematic symmetry-breaking of this type has been invoked as a possible mechanism for the convective flows observed in oocytes (29).

If the fluctuations in chromatin are sufficiently strong that the ensemble-averaged nematic order parameter is zero, then—as in the scalar case—the PSD for nematic fluctuations can be expressed in the form of a two-point correlation function. In terms of the nematic order parameter field:

$$\left(\vec{\beta}^{2}\right)_{\vec{q},\omega} = f^{2}a^{2}|g(\omega)|^{2} \\ \times \frac{\left\langle \hat{q} \cdot \overleftrightarrow{Q}^{*}(\vec{q},\omega) \cdot \widecheck{P}(\vec{q}) \cdot \overleftrightarrow{Q}(\vec{q},\omega) \cdot \widehat{q} \right\rangle}{\Delta V \Delta T}.$$
(29)

Similar to the formula in Eq. 14, the PSD of vector events simplifies if the directions of the force dipoles are statistically independent of each other and of the event positions. In that case, only the k = k' terms survive in the double summation over event pairs implicit in the formula of Eq. 29, which results in

$$\left(\vec{\beta}^{2}\right)_{\vec{q},\omega} = \rho_{v}f^{2}a^{2}|g(\omega)|^{2}\left\langle \left(\widehat{q}\cdot\widehat{n}\right)^{2} - \left(\widehat{q}\cdot\widehat{n}\right)^{4}\right\rangle, \quad (30)$$

where ρ_{ν} is the average of $\rho_{\nu}(\vec{r},t)$. If the force dipoles are distributed isotropically, then

$$\left\langle \left(\widehat{q} \cdot \widehat{n}\right)^2 - \left(\widehat{q} \cdot \widehat{n}\right)^4 \right\rangle = 2/15.$$

RESULTS AND COMPARISON WITH EXPERIMENT

This section provides a preliminary comparison of the theoretical framework of the previous sections with the observational study of collective dynamics in chromatin that motivated our work. The observational study applied displacement correlation spectroscopy (DCS), which is based on time-resolved image correlation analysis as a means for the measurement of the velocity fluctuation spectra (19). DCS uses algorithms of particle image velocimetry to measure direction and magnitude of local movements simultaneously across the entire nucleus and over the entire duration of the experiment (19). Fluorescently-labeled histones are used to visualize chromatin movement. A camera records subsequent exposures to pulses of laser light. The frames are split into a large number of interrogation areas, or windows. For each interrogation window a local displacement vector between two time points, separated by time interval Δt , is obtained by cross-correlation between pairs of images; all experimentally accessible values of Δt were sampled. If the displacement over a time interval Δt is measured, then the mean velocity

$$[\vec{r}(t+\Delta t)-\vec{r}(t)]/\Delta t$$

can be obtained. The spatial Fourier transform $\vec{F}(\vec{q}, \Delta t)$ of the mean flow velocity is given by

$$\vec{F}(\vec{q},\Delta t) = \sum_{j}^{N} \frac{\vec{r_{j}}(t+\Delta t) - \vec{r_{j}}(t)}{\Delta t} e^{i\vec{q}\cdot\vec{r}_{j}(t)}, \qquad (31)$$

with *N* the number of tracer particles. The flow spectral density (FSD) $S(q,\Delta t)$ is defined as

$$\left\langle \left| \vec{F}(q,\Delta t) \right|^2 \right\rangle / N.$$

In Section S6 in the Supporting Material we show that this measured FSD is related to the computed velocity PSD by,

$$S(q,\Delta t) \simeq c \int \frac{1 - \cos \omega \Delta t}{\left(\omega \Delta t\right)^2} \left(\bar{v}^2\right)_{\vec{q},\omega} \frac{d\omega}{\pi},$$
 (32)

with $c = N/\Delta V$ the tracer concentration.

In the study, the time-dependent displacements of labeled chromatin sites,

$$\vec{r}_i(t+\Delta t)-\vec{r}_i(t),$$

were measured for interphase HeLa cells both with and without ATP consumption (19). From these data, we calculated the FSD using the method described above. Fig. 3 shows the measured FSD as a function of the wavenumber q for different values of Δt .

We fitted the data to the form

$$S(q,\Delta t) = A(q)/\Delta t^2 + B(q)/\Delta t.$$
(33)

The motivation for this fitting function was twofold. In the limit that the wavenumber q is larger than the inverse of the mean separation between the tracer particles, the FSD should be proportional to $1/\Delta t^2$ for localized tracer particles

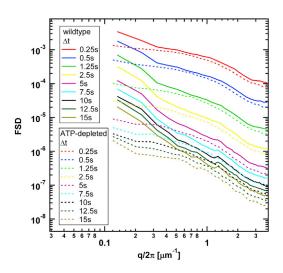


FIGURE 3 Flow spectral densities of the chromatin of wild-type and ATP-depleted nuclei of interphase HeLa cells as a function of the wavenumber q for several values of the fixed measurement time interval Δt . To see this figure in color, go online.

Biophysical Journal 106(9) 1871-1881

and proportional to $1/\Delta t$ for diffusing tracer particles (see Section S6 in the Supporting Material). We will discuss below that this is also a natural fitting form for general qwhen a simple model for the $E(q,\omega)$ value of chromatin is adopted.

The result of a fit to the passive data (ATP-depleted nuclei) is shown in Fig. 4. The best fit is $A(q) \propto 1/q^{1.6}$ whereas B(q) is statistically very close to zero for the $q/2\pi$ value in excess of an inverse micron. The inset of Fig. 4 shows the FSD multiplied by Δt^2 as a function of Δt for fixed q. Because B(q) is statistically almost zero, this should be practically a horizontal straight line for the fitting procedure to be meaningful. This appears to be the case. Recall that in terms of tracer dynamics, a Δt^2 dependence would indicate localization.

The next step should be a comparison between the measured FSD and the FSD computed for a generalized complex shear viscosity $E(q,\omega)$ obtained either from a microrheological study or a microscopic theory of chromatin rheology. As neither is available at this point, we will assume

$$E(\omega) = \frac{\eta}{1 - i\omega\tau}$$

independent of wavenumber as a simple illustrative example. This form is the generalized viscosity of the Maxwell fluid (MF). Based on the Tseng et al. (15), Celedon et al. (17), Pajerowski et al. (18), and Dahl et al. (30), our best estimates are for τ to be in the range of a few seconds and for η/τ to be in the range of 1.5–200 Pa. In Section S7 in the Supporting Material, it is shown that the FSD of a passive MF is the sum of a longitudinal velocity term

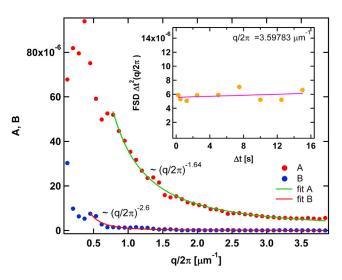


FIGURE 4 Fit coefficients A(q) and B(q) of the fitting form of Eq. 33 for the case of ATP-depleted cells. B(q) is practically zero for $q/2\pi$ greater than an inverse micron; that means that the FSD at constant q should be proportional to $1/\Delta t^2$. (*Inset*) Passive FSD multiplied by Δt^2 for fixed q as a function of Δt ; linear regression (*pink line*), very nearly horizontal. To see this figure in color, go online.

(approximately) proportional to $1/(q^2\Delta t^2)$ for Δt large compared to the inverse of the relaxation rates of the MF, and a transverse velocity term proportional to $1/(q^2\Delta t)$. In terms of a comparison with the MF, our results would seem to rule out transverse velocity fluctuations as the source of the observed equilibrium FSD because of the Δt dependence. However, the q dependence of the FSD deviates somewhat from the MF $1/q^2$ dependence; the heterogeneity of chromatin could be a contributing factor in this regard (because the local chromatin concentration varies throughout the nucleus in a living cell significantly), or it could indicate that a q dependence must be included in the MF expression for the generalized viscosity. It should be noted that the viscosity of the nucleoplasm is known to be time-dependent (31) but this takes place over timescales that are much longer than the duration of the experiment (~25 s).

At the next stage, we repeated the analysis for the case of wild-type HeLa cells, which are ATP-active. For values of $q/2\pi$ larger than an inverse micron, the passive (ATPdepleted) and active (wild-type, ATP-active) spectra appear to be quite similar, apart from the roughly doubled overall intensity (see Fig. 3). The simplest interpretation is that in this high q regime the FSD still is dominated by thermal fluctuations but that ATP activity has reduced the osmotic modulus by a factor of approximately one-half. In principle, it is also possible that large q active fluctuations have the same form as thermal fluctuations, but with an effective noise-temperature that is twice the actual temperature.

For $q/2\pi$ less than an inverse micron, the active and passive spectra are different: the FSD of the active system increases rapidly, as compared to the passive data (Fig. 3). Equation 33 still can be used as a fitting form. This is demonstrated in the inset in Fig. 5, which shows a plot of the FSD multiplied by $(\Delta t)^2$ for a fixed q roughly corresponding to the crossover between large and small q regimes (where passive and active data are very similar and very different, respectively). It is seen that the FSD multiplied by Δt^2 is approximately linear in Δt (the linear regression fit is shown as a solid straight line). Having justified the fitting from Eq. 33, we analyzed the coefficients A(q) and B(q) obtained from the fitting procedure. The data for large q regime are shown in Fig. 5. Just as for the passive case, B(q) is very small for $q/2\pi$ that is larger than an inverse micron. On the other hand, in the low q range, B(q) grows so rapidly that it has to be plotted on a different vertical scale (see Fig. S2 in the Supporting Material).

The inset in Fig. 5 that demonstrates linear dependence would be consistent with a FSD that is inversely proportional to $1/\Delta t$. In turn, this would be consistent with diffusive tracer dynamics. In terms of a comparison between the FSD of active cells and that of MF rheology, we show in Section S7 in the Supporting Material that the contribution to the FSD coming from active transverse velocity fluctuations is proportional to $1/q^2\Delta t$, just as it was for thermal

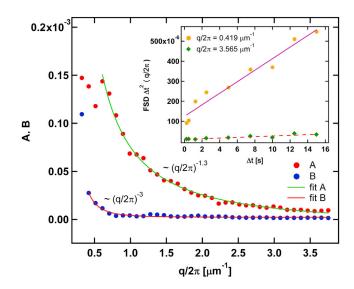


FIGURE 5 Fit coefficients A(q) and B(q) of the fitting form of Eq. 33 for the case of ATP-consuming cells. (*Inset*) FSD multiplied by Δt^2 of wildtype (ATP-consuming) cells for two particular fixed values of q as a function of Δt ; (*solid* and *dashed lines*) linear regression fits. To see this figure in color, go online.

fluctuations. The contribution coming from active longitudinal fluctuations is either independent of q or goes to zero in the small q limit, depending on whether Δt is small or large compared to the duration of the active events. In either case, the longitudinal FSD would be proportional to $1/\Delta t$, which is not consistent with the observed Δt dependence. The interpretation of these results in terms of the MF would be that, for ATP-consuming cells, transverse active fluctuations dominate in the small q limit whereas longitudinal thermal fluctuations dominate for larger q.

CONCLUSIONS

To summarize, we have presented a framework for the analysis of large-scale studies of chromatin dynamics using particle-tracking methods. It is based on the assumption that the response of chromatin to equilibrium thermal fluctuations, active concentration fluctuations, and active force dipoles can be described by linearized hydrodynamics. The proposed method was illustrated by applying it to the results of a recent DCS study of global chromatin dynamics. If the results are interpreted in terms of single-particle dynamics, they indicate a crossover from localized dynamics in ATP-depleted cells to diffusive dynamics in ATP-active cells. This is consistent with some of the single-particle tracking studies (e.g., Levi et al. (10)). In terms of an interpretation based on the MF, thermal fluctuations of ATPdepleted cells are dominated by concentration fluctuations. For ATP-active cells, small wavelength fluctuations (i.e., wavenumbers larger than a few inverse microns) are still dominated by concentration fluctuations. The increase of the intensity of the fluctuations could be due to a simple reduction of the osmotic modulus in the presence of ATP hydrolysis. Longer wavelength fluctuations appear to be associated with transverse velocity fluctuations generated by force-dipole activity.

It should be pointed out that boundary effects associated with the nuclear membrane are likely to play an important role for fluctuations with a wavelength comparable to the size of the nucleus. Large-scale concentration fluctuations should be suppressed by a rigid boundary. Indeed, on the timescales relevant for the experiments discussed above $(\leq 10 \text{ s})$, the nuclear membrane is effectively rigid (19) (see also Hinde et al. (13) and Talwar et al. (32)). Coupling between nuclear envelope breathing and internal chromatin dynamics in embryonic stem cells on timescales upwards of ~ 100 s was examined in Talwar et al. (32) and would have to be included for the theory to be extended into this frequency range. Based on the results of a recent study of the convective dynamics driven by active force dipoles inside a sphere as a model for cytoplasmic streaming (33), active transverse flow fluctuations with q in the range of the inverse of the nucleus are not expected to be suppressed, although they may be scattered by the concentration inhomogeneities that characterize chromatin. One interesting possibility is that coupling of the dipoles through the medium leads to a form of nematic order.

Another open question concerns the actual form of the generalized complex viscosity $E(q,\omega)$. Studies of the local topology of chromatin have concluded that it has a fractal structure, specifically that of a crumpled globule (34–36). Theoretical studies of the rheological properties of polymer melts (in which polymers have the fractal geometry of Gaussian chains) indicate that even in this simple case $E(q,\omega)$ does not have the MF form (37). Understanding the connection between the fractal structure of chromatin and its rheological properties poses an interesting theoretical challenge.

Finally, we would like to put our work in the broader context of complex materials and systems. To the best of our knowledge, the possibility of active scalar events has not been considered in the literature. However, sequences of force-dipole events have been discussed in relation to punctuated stress relaxation phenomena in amorphous media, such as glasses or foams (see, e.g., Chattoraj et al. (37)). An interesting possibility would be to apply the PSD/FSD measurement method discussed here to other active systems, such as a suspension of actively swimming microorganisms (38–40).

SUPPORTING MATERIAL

Two figures, 55 equations, and additional supplemental information, are available at http://www.biophysj.org/biophysj/supplemental/S0006-3495(14) 00340-3.

The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health. R.B. and Y.R. acknowledge the hospitality of the Center for Soft Matter Research of NYU where part of this research was carried out. A.Y.G. acknowledges the hospitality of the Aspen Center for Physics where part of this work was done.

R.B. thanks the national Science Foundation for support under Division of Materials Research grant No.1006128. The work of A.Y.G. and Y.R. was supported in part by a grant from the US-Israel Binational Science Foundation. Y.R.'s research was supported by the I-CORE Program of the Planning and Budgeting Committee and The Israel Science Foundation. A.Z.'s research reported in this publication was supported by the Damon Runyon Cancer Research Foundation under Award No. DRG 2040-10 and by the National Institute of General Medical Sciences of the National Institutes of Health under Award No. K99GM104152.

REFERENCES

- 1. Alberts, B., A. Johnson, ..., P. Walter. 2008. Molecular Biology of the Cell. Garland Science, New York.
- Cremer, T., and C. Cremer. 2001. Chromosome territories, nuclear architecture and gene regulation in mammalian cells. *Nat. Rev. Genet.* 2:292–301.
- Racki, L. R., and G. J. Narlikar. 2008. ATP-dependent chromatin remodeling enzymes: two heads are not better, just different. *Curr. Opin. Genet. Dev.* 18:137–144.
- Hansen, J. C. 2012. Human mitotic chromosome structure: what happened to the 30-nm fiber? *EMBO J.* 31:1621–1623.
- Dekker, J., and B. van Steensel. 2013. Chapt. 7: The spatial architecture of chromosomes. *In* Handbook of Systems Biology: Concepts and Insights. M. Walhout, M. Vidal, and J. Dekker, editors. Elsevier, New York, pp. 137–151.
- Marshall, W. F., A. Straight, ..., J. W. Sedat. 1997. Interphase chromosomes undergo constrained diffusional motion in living cells. *Curr. Biol.* 7:930–939.
- Bornfleth, H., P. Edelmann, ..., C. Cremer. 1999. Quantitative motion analysis of subchromosomal foci in living cells using four-dimensional microscopy. *Biophys. J.* 77:2871–2886.
- Heun, P., T. Laroche, ..., S. M. Gasser. 2001. Chromosome dynamics in the yeast interphase nucleus. *Science*. 294:2181–2186.
- Bronstein, I., Y. Israel, ..., Y. Garini. 2009. Transient anomalous diffusion of telomeres in the nucleus of mammalian cells. *Phys. Rev. Lett.* 103:018102.
- Levi, V., Q. Ruan, ..., E. Gratton. 2005. Chromatin dynamics in interphase cells revealed by tracking in a two-photon excitation microscope. *Biophys. J.* 89:4275–4285.
- Hameed, F. M., M. Rao, and G. V. Shivashankar. 2012. Dynamics of passive and active particles in the cell nucleus. *PLoS ONE*. 7:e45843.
- Weber, S. C., A. J. Spakowitz, and J. A. Theriot. 2012. Nonthermal ATP-dependent fluctuations contribute to the in vivo motion of chromosomal loci. *Proc. Natl. Acad. Sci. USA*. 109:7338–7343.
- 13. Hinde, E., F. Cardarelli, ..., E. Gratton. 2012. Tracking the mechanical dynamics of human embryonic stem cell chromatin. *Epigen. Chromatin.* 5:20.
- Meshorer, E., D. Yellajoshula, ..., T. Misteli. 2006. Hyperdynamic plasticity of chromatin proteins in pluripotent embryonic stem cells. *Dev. Cell.* 10:105–116.
- Tseng, Y., J. S. H. Lee, ..., D. Wirtz. 2004. Micro-organization and visco-elasticity of the interphase nucleus revealed by particle nanotracking. J. Cell Sci. 117:2159–2167.
- de Vries, A. H. B., B. E. Krenn, ..., J. S. Kanger. 2007. Direct observation of nanomechanical properties of chromatin in living cells. *Nano Lett.* 7:1424–1427.
- Celedon, A., C. M. Hale, and D. Wirtz. 2011. Magnetic manipulation of nanorods in the nucleus of living cells. *Biophys. J.* 101:1880–1886.

- Pajerowski, J. D., K. N. Dahl, ..., D. E. Discher. 2007. Physical plasticity of the nucleus in stem cell differentiation. *Proc. Natl. Acad. Sci. US*
- Sci. USA. 104:15619–15624.
 19. Zidovska, A., D. A. Weitz, and T. J. Mitchison. 2013. Micron-scale coherence in interphase chromatin dynamics. *Proc. Natl. Acad. Sci.* USA. 110:15555–15560.
- Marchetti, M., J. Joanny, ..., R. A. Simha. 2013. Hydrodynamics of soft active matter. *Rev. Mod. Phys.* 85:1143–1189.
- Doi, M., and A. Onuki. 1992. Dynamic coupling between stress and composition in polymer solutions and blends. J. Phys. II (France). 2:1631–1656.
- Landau, L. D., and E. M. Lifshitz. 1980. Statistical physics, part 1. *In* Course of Theoretical Physics, Vol. 5, 3rd Ed. Butterworth-Heinemann, Oxford, UK.
- 23. Doi, M. 2013. Soft Matter Physics. Oxford University Press, Oxford, UK.
- Milner, S. T. 1993. Dynamical theory of concentration fluctuations in polymer solutions under shear. *Phys. Rev. E Stat. Phys. Plasmas Fluids Relat. Interdiscip. Topics.* 48:3674–3691.
- Narlikar, G. J., R. Sundaramoorthy, and T. Owen-Hughes. 2013. Mechanisms and functions of ATP-dependent chromatin-remodeling enzymes. *Cell*. 154:490–503.
- Lifshitz, E. M., and L. P. Pitaevskii. 2002. Statistical physics, part 2: theory of the condensed state. *In* Course of Theoretical Physics, *Vol.* 9. Butterworth-Heinemann, Oxford, UK.
- MacKintosh, F. C., and A. J. Levine. 2008. Nonequilibrium mechanics and dynamics of motor-activated gels. *Phys. Rev. Lett.* 100:018104.
- Mangenot, S., A. Leforestier, ..., F. Livolant. 2003. Phase diagram of nucleosome core particles. J. Mol. Biol. 333:907–916.
- Ganguly, S., L. S. Williams, ..., R. E. Goldstein. 2012. Cytoplasmic streaming in *Drosophila* oocytes varies with kinesin activity and corre-

lates with the microtubule cytoskeleton architecture. *Proc. Natl. Acad. Sci. USA*. 109:15109–15114.

- Dahl, K. N., A. J. Engler, ..., D. E. Discher. 2005. Power-law rheology of isolated nuclei with deformation mapping of nuclear substructures. *Biophys. J.* 89:2855–2864.
- Liang, L., X. Wang, ..., W. R. Chen. 2009. Noninvasive determination of cell nucleoplasmic viscosity by fluorescence correlation spectroscopy. J. Biomed. Opt. 14:024013.
- Talwar, S., A. Kumar, ..., G. V. Shivashankar. 2013. Correlated spatiotemporal fluctuations in chromatin compaction states characterize stem cells. *Biophys. J.* 104:553–564.
- 33. Woodhouse, F. G., and R. E. Goldstein. 2012. Spontaneous circulation of confined active suspensions. *Phys. Rev. Lett.* 109:168105.
- Grosberg, A. Y., Y. Rabin, ..., A. Neer. 1993. Crumpled globule model of three-dimensional structure of DNA. *Europhys. Lett.* 23:373–378.
- Lieberman-Aiden, E., N. L. van Berkum, ..., J. Dekker. 2009. Comprehensive mapping of long-range interactions reveals folding principles of the human genome. *Science*. 326:289–293.
- Bancaud, A., C. Lavelle, ..., J. Ellenberg. 2012. A fractal model for nuclear organization: current evidence and biological implications. *Nucleic Acids Res.* 40:8783–8792.
- Chattoraj, J., C. Caroli, and A. Lemaître. 2011. Robustness of avalanche dynamics in sheared amorphous solids as probed by transverse diffusion. *Phys. Rev. E Stat. Nonlin. Soft Matter Phys.* 84:011501.
- Hatwalne, Y., S. Ramaswamy, ..., R. A. Simha. 2004. Rheology of active-particle suspensions. *Phys. Rev. Lett.* 92:118101.
- Chen, D. T. N., A. W. C. Lau, ..., A. G. Yodh. 2007. Fluctuations and rheology in active bacterial suspensions. *Phys. Rev. Lett.* 99:148302.
- Lau, A. W. C., and T. C. Lubensky. 2009. Fluctuating hydrodynamics and microrheology of a dilute suspension of swimming bacteria. *Phys. Rev. E Stat. Nonlin. Soft Matter Phys.* 80:011917.

Biophysical Journal

Chromatin Hydrodynamics: Supporting Material

Robijn Bruinsma¹, Alexander Y.Grosberg², Yitzhak Rabin³, Alexandra Zidovska^{4,5}

¹ Department of Physics and Astronomy, University of California, Los Angeles, CA, U.S.A.

² Department of Physics and Center for Soft Matter Research, New York University, New York, NY, U.S.A.

³ Department of Physics, Bar Ilan University, Ramat Gan, Israel

⁴ Department of Systems Biology, Harvard Medical School, Boston, MA, U.S.A.

⁵ School of Engineering and Applied Sciences, Department of Physics, Harvard University, Cambridge, MA, U.S.A.

S.1. Hydrodynamic Equations of Motion and Linear Response

In this supplementary section we apply the Doi-Onuki method (Ref. (22) in the main text) to construct the twocomponent hydrodynamic equations for polymer solutions and gels including the linear response of such systems to perturbations.

In general, the relaxation equations for a thermodynamic system close to equilibrium can be phrased as the condition that the Rayleigh Function for the time-dependent thermo-dynamic quantities $x_i(t)$, (i = 1, 2, ..n)

$$\mathcal{R} = W + \sum_{i} \frac{\partial F}{\partial x_i} \left(\frac{dx_i}{dt}\right) \tag{S1}$$

must be minimized with respect to $\frac{dx_i}{dt}$ for fixed x_i (see, for instance, Refs. (23,24) in the main text; see also Ref. (25) for further details of the derivation and its applicability limits). The dissipation function W is quadratic in the generalized velocities $\frac{dx_i}{dt}$ while F is the thermodynamic free energy. The first part of the Rayleigh Function is the energy dissipated per unit time, and the second part the work performed per unit time by the thermodynamic forces. For a polymer network, the thermodynamic variables are the local monomer concentration $\phi(\vec{r})$ and the coarse-grained displacement field $\vec{u}^p(\vec{r})$ of the polymer molecules. For polymer solutions that are not cross-linked, such as chromatin solution, the displacement field is not truly a proper thermodynamic quantity. However, for a visco-elastic medium, the displacement description is maintained and the polymer solution is treated as a polymer network in the limit that the zero-frequency shear modulus vanishes. Only timederivatives of the displacement variables should enter in the final hydrodynamic equations in that case.

In the hydrodynamic description, energy dissipation is dominated by friction associated with relative flow of polymer and solvent, in which case the dissipation function takes the form

$$W = \frac{1}{2} \int d^3 r \zeta \left(\vec{v}^p - \vec{v}^s \right)^2 \,, \tag{S2}$$

with ζ the friction coefficient per unit volume, \vec{v}^s the solvent flow velocity, and $\vec{v}^p = d\vec{u}^p/dt$.

As regards the second term of the Rayleigh function (1), the free energy F of the polymer network or solution is com-

posed of two terms. The first term is

$$F_{\phi} = \int d^3 r f(\phi(\vec{r}) \tag{S3}$$

with ϕ the polymer concentration and $f(\phi)$ the equilibrium concentration-dependent free energy density of the polymer network. After imposing the continuity equation

$$\frac{\partial \phi}{\partial t} + \vec{\nabla} \cdot \phi \vec{v}^p = 0 , \qquad (S4)$$

 F_{ϕ} is found to contribute a term

$$\frac{dF_{\phi}}{dt} = -\int d^3r \left(\frac{\partial f}{\partial \phi} \vec{\nabla} \cdot (\phi \vec{v}^p)\right) \tag{S5}$$

to the Rayleigh Function. This term accounts for interactions between the polymer monomers with each other and with the surrounding solvent molecules. The second term is the polymer elastic free energy F_p , which contributes to the Rayleigh Function a term of the form

$$\frac{dF_p}{dt} = -\int d^3r \left(\sigma_{\alpha\beta}(\vec{r})\frac{\partial v^p{}_\alpha}{\partial r_\beta}\right) \,. \tag{S6}$$

Here, $\sigma_{\alpha\beta}$ is the symmetric traceless shear stress tensor of the polymer network. In the main text, the form of the stress tensor for a viscoelastic solution is discussed. Here it will be left unspecified. The part of the stress tensor associated with swelling/compression of the network that has a finite trace is absorbed in the first, concentration dependent, part of the free energy.

The polymer system is compressible: if locally the polymer concentration increases then this is compensated by solvent drainage from the region. The combined polymer-solvent at fixed ϕ will however be assumed to be incompressible. The incompressibility condition

$$\vec{\nabla}\left((1-\phi)\vec{v}^s + \phi\vec{v}^p\right) = 0\,,\tag{S7}$$

is included in the Rayleigh Function by introducing the hydrodynamic pressure $P(\vec{r})$, acting as a Lagrange multiplier. Collecting all terms gives

$$\mathcal{R} = \int d^3 r \left(\frac{1}{2} \zeta (\vec{v}^p - \vec{v}^s)^2 - \frac{\partial f}{\partial \phi} \vec{\nabla} \cdot (\phi v^p) - \sigma_{\alpha\beta} \frac{\partial v^p{}_{\alpha}}{\partial r_{\beta}} - P \vec{\nabla} \left((1 - \phi) \vec{v}^s + \phi \vec{v}^p \right) \right) .$$
(S8)

Finally, in order to apply linear response theory, infinitesimal, time-dependent "fields" $h_i(t)$ are introduced that are thermodynamically conjugate to the thermodynamic parameters x_i in the sense that $dW = \sum_i h_i dx_i$ is the work done by the external fields for an infinitesimal change dx_i of the thermodynamic parameters. The change in the Hamiltonian of the system is of the form $\Delta H = -\sum_i h_i x_i$. The timedependent fields induce time-dependent changes in the thermodynamic parameters:

$$\delta x_i(t) = \int_{-\infty}^t dt' \chi_{ij}(t-t') h_j(t') .$$
 (S9)

where $\chi_{ij}(\tau)$ is the dynamical susceptibility (response function). The Fluctuation-Dissipation (FD) theorem states that the imaginary part of the frequency Fourier transform of the dynamical susceptibility is related to the autocorrelation matrix of the thermodynamic parameters by

$$\operatorname{Im}\left[\chi_{ij}(\omega)\right] = \frac{\omega}{2k_B T} S_{ij}(\omega) , \qquad (S10)$$

where $S_{ij}(t-t') \equiv \langle x_i(t)x_j(t') \rangle$.

For the present case, we introduce an infinitesimal, externally imposed, time-dependent chemical potential $\mu^{(ex)}(\vec{r},t)$ for monomers that is conjugate to the concentration field and an infinitesimal, externally imposed stress tensor $\sigma_{\alpha\beta}^{(ex)}(\vec{r},t)$ that is conjugate to the strain tensor of the polymer network. These fields contribute a term to the Rayleigh Function of the form

$$\delta \mathcal{R} = \int d^3 r \left(-\mu^{(\text{ex})}(\vec{r}, t) \vec{\nabla} \cdot (\phi v^p) - \sigma^{(\text{ex})}_{\alpha\beta}(\vec{r}, t) \frac{\partial v^p{}_{\alpha}}{\partial r_{\beta}} \right) .$$
(S11)

Minimizing the Rayleigh Function gives

$$\zeta(\vec{v}^p - \vec{v}^s) = \vec{\nabla} \left(\overleftarrow{\sigma} + \overleftarrow{\sigma}^{(\mathrm{ex})} \right) - \vec{\nabla} \Pi - \phi \vec{\nabla} \mu^{(\mathrm{ex})} - \phi \vec{\nabla} P ,$$
(S12)

$$\zeta \left(\vec{v}^s - \vec{v}^p \right) = -\left(1 - \phi \right) \vec{\nabla} P \,. \tag{S13}$$

The linearized version of these equation are used in the main text, where $\phi_0 \mu^{(\text{ex})}(\vec{r},t)$ is replaced by the source term $\alpha(\vec{r},t)$ for scalar events and the externally imposed stress $\sigma^{(\text{ex})}$ by the active stress $\sigma^{(\text{ac})}$ for vector events. As shown in the main text, if the fluctuation modes are decomposed into transverse and longitudinal components then the external chemical potential only generates longitudinal modes and the traceless external stress tensor only transverse components. The cross-correlation matrix is thus diagonal. The diagonal components of the dynamical susceptibility are given in the main text, and the final application of the FD theorem is straightforward.

S.2. Green's Function Derivation for a Scalar Event

Assume a scalar event takes place at the origin at time t = 0. The linearized force balance equation is

$$\zeta \left(\vec{v}^p - \vec{v}^s \right) = \vec{\nabla} \overleftarrow{\phi} - K \vec{\nabla} \delta \phi - \phi_0 \vec{\nabla} P + s \vec{\nabla} \delta \left(\vec{r} \right) g(t) .$$
(S14)

In a few lines of algebra, this yields

$$\frac{\partial \delta \phi}{\partial t} = D\nabla^2 \delta \phi - \tilde{s} \nabla^2 \delta(\vec{r}) g(t) - \frac{(1-\phi_0)^2}{\zeta/\phi_0} \vec{\nabla} \cdot \left(\vec{\nabla} \overleftarrow{\sigma}\right) ,$$
(S15)

with $D = K \frac{(1-\phi_0)^2}{\zeta/\phi_0}$ and $\tilde{s} = s \frac{(1-\phi_0)^2}{\zeta/\phi_0}$. We can identify D as the *collective diffusion constant*. This equation can be viewed as defining a *Greens function* for scalar events.

As a concrete example, assume that passive chromatin behaves like a simple Newtonian fluid. The stress tensor term $\vec{\nabla} \cdot (\vec{\nabla} \overleftarrow{\sigma})$ then reduces to $\eta \nabla^2 (\vec{\nabla} \cdot \vec{v}^p)$ with η the viscosity. After applying the continuity equation to eliminate the flow, one obtains:

$$\left(1 - \frac{(1 - \phi_0)^2}{\zeta} \eta \nabla^2\right) \frac{\partial \delta \phi}{\partial t} \simeq D \nabla^2 \delta \phi - \tilde{s} \nabla^2 \delta(\vec{r}) g(t) .$$
(S16)

The term $\frac{(1-\phi_0)^2}{\zeta}\eta\nabla^2$ is small compared to one for wavenumbers $q\xi \ll \sqrt{\eta_0/\eta}$. If one assumes that to be the case then the remaining equation is:

$$\frac{\partial \delta \phi}{\partial t} \simeq D \nabla^2 \delta \phi - \tilde{s} \nabla^2 \delta(\vec{r}) g(t) .$$
 (S17)

If the local change in solubility is permanent, with $g(t) \sim \theta(t)$, then the solution of the equation leads to a Green's function:

$$\delta\phi(\vec{r},t>0) \simeq \frac{\tilde{s}}{D} \left[\delta(\vec{r}) - \frac{e^{-r^2/4Dt}}{(4\pi Dt)^{3/2}}\right]$$
. (S18)

This describes a localized change in concentration at the origin, equal to $(s/K)\delta(\vec{r})$ together with a transient diffusion pulse that travels outwards from the origin. The volume integral over the concentration variation is zero: no new material is introduced by the change in solubility as is physically correct. The linearization condition $\delta\phi \ll \phi_0$ is satisfied provided $s \ll K\xi^3$.

S.3. Derivation of the dynamic susceptibility

To deal with a distribution of M_s scalar events, write the linearized equations of motion in Fourier transformed form:

$$\zeta(\vec{v}^p - \vec{v}^s) = i\vec{q} \cdot \left(\overleftarrow{\sigma} + \overleftarrow{\sigma}^{(\mathrm{ac})}\right) - i\vec{q}K\delta\phi - i\phi_0\vec{q}P \,.$$
(S19)

Here, $\sigma_{ij}^{(ac)}(\vec{q},\omega) = \delta_{ij}\alpha(\vec{q},\omega)$ with $\alpha(\vec{q},\omega)) = g(\omega) \sum_{k=1}^{M_s} s_k e^{i\left(\omega t_k - \vec{q}\cdot\vec{R}_k\right)}$,

where $g(\omega)$ is the Fourier transform of g(t), the function that defines the time course of scalar event. For instance, if $g(t) = \theta(t)e^{-t/\tau_a}$ (which means, g(t) is zero at t < 0, starts at t = 0, and falls off exponentially with characteristic time τ_a at t > 0), then $g_\omega = \frac{\tau_a}{1-i\omega\tau_a}$. Darcy's Law reduces to:

$$\zeta\left(\vec{v}^s - \vec{v}^p\right) = -i(1 - \phi_0)\vec{q}P, \qquad (S21)$$

(S20)

while the incompressibility condition becomes:

$$i\vec{q}\cdot((1-\phi_0)\vec{v}^s+\phi_0\vec{v}^p)=0$$
, (S22)

and the continuity equation:

$$-\omega\delta\phi + \phi_0 \vec{q} \cdot \vec{v}^p = 0.$$
 (S23)

Next, define $v_{\parallel}^p = \vec{q} \cdot \vec{v}/q$ to be the longitudinal component of the polymer flow field. Eliminating pressure and longitudinal solvent flow leads to an expression for the concentration fluctuations in the hydrodynamic limit:

$$\delta\phi(\vec{q},\omega) = \chi(q,\omega)\alpha(\vec{q},\omega) , \qquad (S24)$$

where

$$\chi(q,\omega) = \frac{iq^2\phi_0}{\omega\left[\frac{\zeta}{(1-\phi_0)^2} + \frac{4}{3}E(q,\omega)q^2\right] + iq^2K\phi_0}$$
(S25)

is the *dynamic susceptibility*. Note, that in the limit of zero frequency, $\chi(q, \omega = 0)$ equals the static osmotic susceptibility 1/K, as it should. The dynamic susceptibility has pole singularities in the lower half of the complex plane at $\omega = -i\Gamma(q)$ with $\Gamma(q)$ the relaxation rate of a collective mode of the system. In section S.7, the specific case of the Maxwell Fluid (MF) is discussed, which has two such collective modes, corresponding to hybridized collective diffusion and stress relaxation.

S.4. Vector Activity Derivation

Vector activity in general represents action of a set of force dipoles. Each force dipole is composed of a pair of collinear opposing forces $f\hat{n}$ and $-f\hat{n}$ exerted in two different points separated by a microscopic distance a. Here \hat{n} is a unit vector marking the direction of force dipole; at the same time vector $a\hat{n}$ connects the points where two forces are applied (such that two forces forming a dipole generate no torque). If \vec{R} is position vector of a center-point of the force dipole, then two forces are exerted in points $\vec{R} - (a/2)\hat{n}$ and $\vec{R} + (a/2)\hat{n}$. In reality there are more than one vector source, and their total

contribution to the divergence of stress tensor (i.e., applied force per unit volume) reads

$$\vec{\nabla} \cdot \overleftarrow{\sigma}^{(\mathrm{ac})}(\vec{r}, t) = \sum_{k=1}^{\mathcal{M}_v} f_k g(t - t_k) \times \\ \times \left[\delta \left(\vec{r} - \vec{R}_k - \frac{a_k}{2} \hat{n}_k \right) + \delta \left(\vec{r} - \vec{R}_k + \frac{a_k}{2} \hat{n}_k \right) \right] ,$$
(S26)

where g(t) describes time development of the event, starting at time t_k for event k, while \mathcal{M}_v the number of vector events. For the case of nucleosome rearrangement events, awould have the typical size of a spacer length between nucleosomes. Given that distance a (any a_k) is microscopic, we can write

$$\delta\left(\vec{r} - \vec{R}_k \pm \frac{a_k}{2}\hat{n}_k\right) \simeq \delta\left(\vec{r} - \vec{R}_k\right) \pm \frac{a_k}{2}\hat{n}_k\vec{\nabla}\delta\left(\vec{r} - \vec{R}_k\right).$$
(S27)

Combining now two of such δ -functions in formula (26), we arrive at

$$\vec{\nabla} \cdot \overleftarrow{\sigma}^{(\mathrm{ac})}(\vec{r}, t) = \sum_{k=1}^{\mathcal{M}_v} f_k a_k \hat{n}_k (\hat{n}_k \cdot \vec{\nabla}) \delta\left(\vec{r} - \vec{R}_k\right) g(t - t_k) \,.$$
(S28)

If all forces are the same, $f_k = f$, and all distances are the same, $a_k = a$, then we arrive at the result used in the main text (Eq. 19).

S.5. Greens Function: Vector Event

First consider the case of a vector event with long event duration in a medium that can be described as a Netwonian fluid. The source term is then the sum of two time-independent δ -function forces. Each produces a flow field of the form

$$\vec{v}(\vec{r}) = f\,\hat{n} \cdot \overleftrightarrow{S}(\vec{r})/8\pi\eta\,,\tag{S29}$$

where

$$S_{ij}(\vec{r}) = \frac{\delta_{ij}}{r} + \frac{r_i r_j}{r^3}$$
(S30)

is the Oseen tensor. The combined dipole flow field has the form:

$$\vec{v}(\vec{r}) = fa\left(\hat{n}\cdot\vec{\nabla}\right)\left(\hat{n}\cdot\vec{S}\left(\vec{r}\right)\right)/8\pi\eta.$$
 (S31)

The pattern of flow lines is that of extensional flow oriented along the force direction.

For the case of a general linear viscoelastic medium, it is useful to define the transverse projection operator \overrightarrow{P} . In qspace, the projection operator is defined as $P_{ij}(\vec{q}) = \delta_{ij} - \hat{q}_i \hat{q}_j$, where $\hat{q} = \vec{q}/q$ and $\hat{q}_i = q_i/q$. Apply this projection operator to Eqs. 1 and 2 for two-fluid hydrodynamics. This leads to $\vec{v}_{\perp}^p = \vec{v}_{\perp}^s$ and

$$E * \nabla^2 \vec{v}_{\perp} = f a \overleftrightarrow{P} \cdot \hat{n} (\hat{n} \cdot \vec{\nabla}) \delta(\vec{r}) g(t) .$$
 (S32)

The * symbol stands for the convolution of the space-time memory kernel E with the transverse polymer velocity field

(indicated from here on as the flow field itself). After Fourier transform, the flow field produced by the vector event is:

$$\vec{v}_{\perp}(\vec{q},\omega) = ifag(\omega) \frac{\overleftarrow{P}(\vec{q}) \cdot \hat{n}(\hat{n} \cdot \vec{q})}{q^2 E(q,\omega)} .$$
(S33)

The Green's function is the reverse Fourier Transform.

S.6. FSD and PSD

→

S.6.1 Derivation

In this section we discuss the relationship between the FSD, as measured experimentally, and the PSD that is a convenient quantity to compute theoretically. We start from the advective equation of motion of a labelled site of the chromatin moving in the surrounding hydrodynamic flow field

$$\frac{d\vec{r}(t)}{dt} = \vec{v}_p(\vec{r}(t), t) \tag{S34}$$

The tracer displacement between successive measurements is

$$\frac{\vec{r}(t+\Delta t)-\vec{r}(t)}{\Delta t} = \int_{t}^{t+\Delta t} \vec{v}(\vec{r}(t'),t') \frac{dt'}{\Delta t}$$
(S35)

(where we suppressed index p for brevity). Perform a mode expansion of the flow field, according to the Fourier transform convention Eq. 4:

$$\frac{\vec{r}(t+\Delta t)-\vec{r}(t)}{\Delta t} = \int_{t}^{t+\Delta t} \left[\frac{\sum_{\vec{p}} \int_{-\infty}^{\infty} \vec{v}(\vec{p},\omega) e^{-\imath(\vec{p}\cdot\vec{r}(t')+\omega t')} \frac{d\omega}{2\pi}}{\Delta V}\right] \frac{dt'}{\Delta t}$$
(S36)

Multiply by $e^{i\vec{q}\cdot\vec{r}_i(t)}$ and do the summation over $i=1,2,\ldots,N$ tracer particles:

$$\begin{split} F(\vec{q},\Delta t) &= \\ \sum_{i}^{N} \int_{t}^{t+\Delta t} \left[\frac{\sum_{\vec{p}} \int_{-\infty}^{\infty} \vec{v}(\vec{p},\omega) e^{i(\vec{q}\cdot\vec{r}_{i}(t)-\vec{p}\cdot\vec{r}_{i}(t')-\omega t')} \frac{d\omega}{2\pi}}{\Delta V} \right] \frac{dt'}{\Delta t} \end{split}$$
(S37)

If the particle displacement over time Δt is such that we can replace $\vec{q} \cdot \vec{r_i}(t') \simeq \vec{q} \cdot \vec{r_i}(t)$, and if the tracers are uniformly distributed over the sample, then only the $\vec{p} = \vec{q}$ mode survives in the sum $\sum_{i}^{N} e^{i((\vec{q}-\vec{p})\cdot\vec{r_i}(t))} \simeq N\delta_{\vec{p},\vec{q}}$ provided that 1/q is large compared at the distance between labelled particles but small compared at the nucleus size: $N/\Delta V \gg q^3 \gg 1/\Delta V$. Under these assumptions:

$$\vec{F}(\vec{q},\Delta t) = \frac{N}{\Delta V} \int_{-\infty}^{\infty} \vec{v}(\vec{q},\omega) \left[\int_{t}^{t+\Delta t} e^{-i\omega t'} \frac{dt'}{\Delta t} \right] \frac{d\omega}{2\pi}$$
$$= \frac{N}{\Delta V} \int_{-\infty}^{\infty} \vec{v}(\vec{q},\omega) e^{-i\omega t} \frac{1-e^{-i\omega\Delta t}}{i\omega\Delta t} \frac{d\omega}{2\pi}$$
(S38)

If $\langle \vec{v} \rangle = 0$ and $\langle \vec{F} \rangle = 0$, one has to look at the second moment. Multiplying by the complex conjugate and doing the ensemble average gives for $S(q, \Delta t) = \left\langle \left| \vec{F}(q, \Delta t) \right|^2 \right\rangle / N$,

$$S(q,\Delta t) \simeq \frac{N}{\Delta V} \int \frac{1 - \cos \omega \Delta t}{(\omega \Delta t)^2} \left(\vec{v}^2 \right)_{\vec{q},\omega} \frac{d\omega}{\pi} \qquad (\textbf{S39})$$

which is the relation between FSD and power spectral densities used in the main text (Eq. 32).

S.6.2 Limiting cases

We conclude by discussing a few limiting cases. In the limit that Δt is small compared to the inverse of all characteristic frequencies, the FSD goes to a constant:

$$S(q, \Delta t \to 0) \simeq \frac{N}{\Delta V} \int (\vec{v}^2)_{\vec{q},\omega} \frac{d\omega}{2\pi}$$
 (S40)

In the limit that Δt is large compared to the inverse of all characteristic frequencies, the FSD reduces to

$$S(q,\Delta t) \simeq \frac{N}{\Delta V} \frac{\left(\vec{v}^2\right)_{\vec{q},0}}{\Delta t} ,$$
 (S41)

the flow spectral density drops as $1/\Delta t$. In the limit of q large compared to the inverse of the spacing between labelled sites, the result is most easily derived directly from the definition of $\vec{F}(\vec{q}, \Delta t)$, Eq. 31 in the main text:

$$S(q,\Delta t) \simeq \frac{\left\langle \Delta r^2 \right\rangle}{\Delta t^2} ,$$
 (S42)

with $\langle \Delta r^2 \rangle$ the mean square displacement of a single labelled genome site after a time Δt . If single-site dynamics is characterized by a power law of the form $\langle \Delta r^2 \rangle \propto \Delta t^{\alpha}$ in the limit of large Δt then the FSD would be proportional to $N/\Delta t^{2-\alpha}$ or large Δt . Here, α is less than one for subdiffusion and α is greater than one for superdiffusion. If the labelled sites would remain localized, which would be the case for a gel, then α would be zero.

S.7. FSD of a Maxwell Fluid

In this section we compute the FSD of a Maxwell Fluid for passive and active fluctuations. A Maxwell Fluid has a complex viscosity $E(\omega) = \frac{\eta}{1-i\omega\tau}$, independent of wavenumber, with τ the stress relaxation time.

S.7.1 Thermal Fluctuations

According to the fluctuation-dissipation theorem, the amplitude of thermal transverse velocity fluctuations depends on the assumed rheology only through the factor $\operatorname{Re}\left[\frac{1}{E(q,\omega)}\right]$.

This equals $1/\eta$ both for a Newtonian Fluid and for a Maxwell Fluid so the spectra of transverse velocity fluctuations of a Maxwell Fluid is that of a Newtonian Fluid:

$$S_{\perp}(q,\Delta t) \simeq [c] \frac{4k_B T}{q^2 \eta \Delta t}$$
 (S43)

The FSD for longitudinal velocity fluctuations is more complex. The dynamic susceptibility for the concentration fluctuations of a Maxwell Fluid is

$$\chi(q,\omega) = \frac{iq^2\phi_0}{\omega\left[\frac{\zeta}{(1-\phi_0)^2} + \frac{4}{3}\frac{\eta q^2}{1-i\omega\tau}\right] + iq^2K\phi_0} .$$
(S44)

The dispersion relation of the relaxation rates associated with different modes of the system is determined by the poles of the dynamical susceptibility, found by setting the inverse of the dynamical susceptibility to zero. Introducing dimensionless wavenumbers and a dimensionless osmotic modulus through,

$$Q^{2} = \frac{4}{3} \frac{\eta q^{2}}{\zeta} (1 - \phi_{0})^{2}$$
 (S45a)

$$\frac{1}{\kappa} = \frac{4}{3} \frac{\eta}{\tau K \phi_0} \tag{S45b}$$

the mode dispersion $\omega = -i\Gamma(Q)$ must be the solution of the quadratic equation

$$(\tau\Gamma)^2 - \tau\Gamma\left[1 + Q^2(\kappa+1)\right] + Q^2\kappa = 0$$
, (S46)

or, explicitly,

$$\Gamma_1(Q) = \frac{1 + Q^2(\kappa + 1)}{2\tau} - \frac{\sqrt{[1 + Q^2(1 - \kappa)]^2 + 4\kappa Q^4}}{2\tau}$$
(S47a)

$$\Gamma_2(Q) = \frac{1 + Q^2(\kappa + 1)}{2\tau} + \frac{\sqrt{[1 + Q^2(1 - \kappa)]^2 + 4\kappa Q^4}}{2\tau}$$
(S47b)

The two branches are separated by a gap, as shown schematically in Fig. 1. For small wavenumbers, the lower branch approaches Dq^2 , the relaxation rate for collective diffusion with a collective diffusion coefficient $D = K\phi_0(1-\phi_0)^2/\zeta$ that does not depend on the viscosity or the stress relaxation time. For large wavenumbers, the lower branch saturates at $\Gamma_1 \tau = \frac{\kappa}{1+\kappa}$. Concentration fluctuations are most pronounced at a consolute point where the osmotic modulus K vanishes. The relaxation rate of the lower branch goes to zero ("critical slowing down") in that limit for any wavenumber. The upper branch reduces to the relaxation rate $1/\tau$ for shear stress in the small wavenumber limit. For large wavenumbers, the upper branch approaches D_2q^2 with a diffusion coefficient $D_2 = (1 - \phi_0)^2 \left[\frac{4}{3}\eta + K\tau\phi_0\right]/\zeta\tau$ that now does depend on the viscosity and the stress relaxation time.

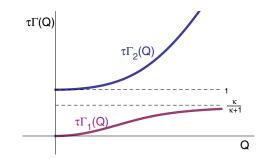


Figure S1 Relaxation rate $\Gamma(Q)$ of a Maxwell Fluid. The lower branch $\Gamma_1(Q)$ represents collective diffusion in the long wavelength limit with a collective diffusion coefficient $D = 3K\phi_0/4\eta$. In the limit that the osmotic modulus *K* vanishes, the lower branch relaxation rate goes to zero for all wavelengths. The upper branch represents stress relaxation for long wavelengths and collective diffusion for short wavelengths.

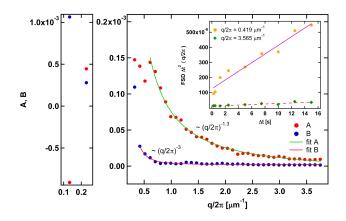


Figure S2 Fit coefficients A(q) and B(q) of the fitting form Eq. 33 for the case of ATP-consuming cells. *Inset:* FSD multiplied by Δt^2 of wildtype (ATP-consuming) cells for two particular fixed values of q as a function of Δt ; solid and dashed lines: linear regression fit. In addition to the Fig. 5 of the main text, we show here left panel which reports data for very small q where completely different scale on the vertical axis has to be used.

The longitudinal contribution to the FSD takes the form

$$\begin{split} S_{||}(q,\Delta t) &= [c] \frac{2k_B T \tau (1-\phi_0)^2}{\phi_0 \zeta \Delta t^2} \times \\ \frac{\left(\frac{1}{\Gamma_1} - \tau\right) \left[1 - e^{-\Gamma_1 \Delta t}\right] - \left(\frac{1}{\Gamma_2} - \tau\right) \left[1 - e^{-\Gamma_2 \Delta t}\right]}{\Gamma_2 - \Gamma_1}. \end{split}$$
(S48)

The full FSD is the sum of the longitudinal and transverse contributions:

$$S(q,\Delta t) = S_{||}(q,\Delta t) + S_{\perp}(q,\Delta t) .$$
 (S49)

гı

S.7.2 Active Vectorial Fluctuations

The FSD for transverse velocity fluctuations in the presence of active vectorial sources in a Maxwell Fluid has the form

$$S_{\perp}(q,\Delta t) \simeq \frac{|c|}{q^2 \eta^2 \pi} \times \int \left(\vec{\beta}^2\right)_{\vec{q},\omega} \left(1 + (\omega\tau)^2\right) \frac{1 - \cos\omega\Delta t}{(\omega\Delta t)^2} d\omega$$
(S50)

This depends in general on the form of the active structure factor. We will consider the case in which there are no spatial or temporal correlations between the active events and where the direction of the active forces is random in space. In that case (see Eq. 30), $\left(\vec{\beta}^2\right)_{\vec{q},\omega} = \frac{2}{15} \frac{m(fa)^2 \tau_a^2}{(\omega \tau_a)^2 + 1}$ with $m = \mathcal{M}/\Delta V \Delta T$ the number of active vector events per unit vol-

ume per unit time. This results in a FSD

$$S_{\perp}(q,\Delta t) = \frac{2}{15} [c] \frac{m(fa)^2 \tau \tau_a^2}{q^2 \eta^2 \Delta t^2} \times \left[\left(\frac{\tau}{\tau_a} - \frac{\tau_a}{\tau} \right) \left(1 - e^{-\Delta t/\tau_a} \right) + \frac{\Delta t}{\tau} \right]$$
(S51)

In the two limits of Δt large and small to τ_a this expression is proportional to $1/(q^2\Delta t)$ and thus of the same form as the equilibrium FSD.

S.7.3 Active Scalar Fluctuations

The FSD for active scalar sources in a Maxwell Fluid is

$$S_{||}(q,\Delta t) \simeq [c] \frac{q^2 (1-\phi_0)^4}{\pi \zeta^2 \Delta t^2} \times \int (\alpha^2)_{\vec{q},\omega} \frac{(1-\cos\omega\Delta t)(1+(\omega\tau)^2)}{\left|(\omega+i\Gamma_1)(\omega+i\Gamma_2)\right|^2} d\omega$$
(S52)

In the absence of correlations between active events (Eq. 14), $(\alpha^2)_{\vec{q},\omega} = \frac{m\langle s^2 \rangle \tau_a^2}{(\omega \tau_a)^2 + 1}$ with $m = \mathcal{M}/\Delta V \Delta T$ the number of scalar events per unit time per unit volume:

$$\begin{split} S_{||}(q,\Delta t) &\simeq [c] \frac{m \left\langle s^2 \right\rangle q^2 (1-\phi_0)^4 \tau_a^2}{\zeta^2 \tau^2 \Delta t^2} \times \\ & \left[\frac{\left(1 - (\Gamma_2 \tau)^2\right) \left(1 - e^{-\Gamma_2 \Delta t}\right)}{\Gamma_2 \left[\Gamma_1^2 - \Gamma_2^2\right] \left[1 - (\Gamma_2 \tau_a)^2\right]} + \\ & \frac{\left(1 - (\Gamma_1 \tau)^2\right) \left(1 - e^{-\Gamma_1 \Delta t}\right)}{\Gamma_1 \left[\Gamma_2^2 - \Gamma_1^2\right] \left[1 - (\Gamma_1 \tau_a)^2\right]} + \\ & \frac{\tau_a \left(\tau_a^2 - \tau^2\right) \left(1 - e^{-\Delta t/\tau_a}\right)}{\left[1 - (\Gamma_2 \tau_a)^2\right] \left[1 - (\Gamma_1 \tau_a)^2\right]} \end{split} \end{split}$$
(S53)

The FSD is proportional to $1/\Delta t$ for Δt small compared to the three relaxation times τ_a , $1/\Gamma_2$, and $1/\Gamma_1$. In the longtime limit that Δt is large compared to these three relaxation

Chromatin Hydrodynamics: Supporting Material

times, the FSD is dominated by the slowest of the three relaxation rates. If the slowest relaxation rate is collective diffusion - the only gapless mode - then for long wavelengths

$$S_{||}(q,\Delta t) \simeq [c] \frac{m \left\langle s^2 \right\rangle (1-\phi_0)^4 \tau_a^2}{\zeta^2 \Delta t^2 D} , \qquad (S54)$$

with $D = K\phi_0(1 - \phi_0)^2/\zeta$ the collective diffusion coefficient. The FSD depends on Δt as $1/\Delta t^2$ but it is independent of wavenumber. If the duration of the active event is the longest time scale then the FSD

$$S_{||}(q,\Delta t) \simeq [c] \frac{m\langle s^2 \rangle (1-\phi_0)^4 q^2 \tau_a^5}{\zeta^2 \Delta t^2}$$
 (S55)

is proportional to q^2 .