Supporting Information Hao et al. 10.1073/pnas.1413970111

Numerical Methods

To illustrate our numerical method we consider the following diffusion equation:

$$
\frac{\partial X}{\partial t} - D_X \nabla^2 X = F_X \text{ in } \Omega,
$$
 [S1]

where the right-hand side accounts for all of the "active" terms. Let $X_{i,j}^n$ denote a numerical approximation of $X(ih_x, jh_y, n\tau)$, where h_x and h_y are the step size in the x and y directions, respectively, and τ is the time step size. Then, a discretization is derived by the explicit Euler five-point finite difference scheme, that is,

$$
\frac{X_{ij}^{n+1} - X_{ij}^n}{\tau} - D_X \left(\frac{X_{i+1,j}^n + X_{i-1,j}^n - 2X_{i,j}^n}{h_x^2} + \frac{X_{i,j+1}^n + X_{i,j-1}^n - 2X_{i,j}^n}{h_y^2} \right)
$$

= $F_X(X_{i,j}^n)$ in Ω . [S2]

To make the scheme stable, we take $\tau \leq h^2/4D_X$, namely $\tau =$ $0.1(h^2/D_X)$, where $h = h_x = h_y$. To test the convergence, we take $h = 1/N$, where $n = 10, 20, 40, 80, 160,$ and 320. The "exact" solution is taken to be the solution with $h = 640$. The solution is computed up to $t = 60$ d and the L_2 error of the velocity and numerical order of accuracy are listed in Table S1. We can clearly observe the second-order accuracy in this table.

Parameter Estimation

A summary of all of the model parameters is given in Tables S2 and S3.

Eq. 4.

- \bullet d_E: Corneal epithelial half life is at least 4–5 wk (1). We take the tubular epithelial half-life to be 6 wk. Then, $d_E = ln(2)/42=$ 1.65×10^{-2} d⁻¹.
- E^* : We assume that the tubular radius is 10 µm and that the tubules occupy up to 90% of the renal cortex. Accordingly, the density of the tubular epithelial cell (TEC) in healthy tissue is taken to be $E^* = 0.8$ g/mL.
- A_E : The steady state of Eq. 4 in healthy tissue is $A_E d_E E^* = 0$. Hence, $A_E = 8.27 \times 10^{-3}$ g·cm⁻³·d⁻¹.
- \bullet d_{EM} : The TECs are decreased by the activated macrophages. Assuming that if M is large, after a long period the TEC density will decrease by 10% even if TGF-β is not activated. Accordingly, $d_{EM} = 1/10d_E = 1.65 \times 10^{-3} \text{ d}^{-1}$.
- $K_{T_{\beta}}$: Based on ref. 2, the concentration of TGF-β in tumor microenvironment was estimated to be about 10 ng/mL. Because tumors secrete a large amount of TGF-β, $K_{T_{\beta}}$ in our model should be significantly smaller; we take $K_{T_\beta} = 10^{-10}$ g/cm³.
- λ_{ET_β} : We assume that the increase of TEC apoptosis by macrophages is double the natural apoptosis rate when TGF-β is approximately at its saturation value; hence, $\lambda_{ET_8} = 2$.

Eq. 5.

• A_f : Fibroblasts make up 7% of healthy renal tissue (3), so that

$$
f^* = 7 \times 10^{-2} \text{ g/cm}^3
$$

The steady state of Eq. 5 in healthy tissue is $A_f - df = 0$. Because $d_f = 1.66 \times 10^{-2}$ d⁻¹ (4), we get

:

$$
A_f = d_f f^* \approx 1.66 \times 10^{-2} \times 7 \times 10^{-2} = 1.16 \times 10^{-3} \text{ g/cm}^3 \text{ d}^{-1}.
$$

 λ_{mf} : In the cancer microenviroment, the transformation from fibroblast to myofibroblast by TGF-β was represented in ref. 5 by the term $a_{21}T_{\beta}f$, where $a_{21} = 6 \times 10^2 \text{ cm}^3 \text{ g}^{-1} \text{ s}^{-1}$. We assume that in our model myofibroblast production rate is smaller than in ref. 5; this rate in our model has the form $\lambda_{mfT}(T_{\beta}/K_{T_{\beta}}+T_{\beta})f$ and, to compare this with $a_{21}T_{\beta}f$, we take the inhibition $K_{T_{\beta}} + T_{\beta}$ to be $3/2K_{T_\beta}$. We then choose λ_{mTT} such that

$$
\lambda_{mf} \frac{T_{\beta}}{\frac{3}{2}K_{T_{\beta}}} f = \frac{1}{10} a_{21} T_{\beta} f.
$$

Hence, $\lambda_{mfT} = 0.12 \text{ d}^{-1}$.

- $λ_{mfG}$: We assume that PDGF and TGF-β affect the transformation from f to m to approximately the same extent $(6-8)$ and take $\lambda_{m f G} = \lambda_{m f T}$.
- λ_{fE} : We assume that in the absence of PDGF the production of fibroblasts by TEC is approximately twice the transformation of fibroblasts into myofibroblasts, that is, $\lambda_{fE}E = 2\lambda_{mf}f_2$ and take λ_{fE} by setting $E = E^*$, $f = f^*$; then $\lambda_{fE} = 1.05 \times 10^{-2}$ d⁻¹.

Eq. 7.

- $\lambda_{\rho T_{\beta}}$: We assume that TGF-β doubles the production of ECM by myofibroblast when TGF-β is approximately at its saturation value. Hence, $\lambda_{\rho T_{\beta}} = 2$.
- λ_{pf} : In the cancer microenvironment, the remodeling rate of ECM is 0.432 d^{-1} (9). We assume that in renal fibrosis the remodeling rate is much smaller and take $\lambda_{\rho f} = 3 \times 10^{-3} \text{ d}^{-1}$. We also assume that the production rate of ECM by myofibroblasts is twice the production rate by fibroblasts (in the absence of TGF-β), namely, $\lambda_{\rho m} = 2\lambda_{\rho f} = 6 \times 10^{-3}$.
- \bullet ρ^* : The steady state of ρ , ρ^* is determined by solving the following steady-state equation in a healthy renal tissue:

$$
\lambda_{\rho f} f\left(1 - \frac{\rho}{\rho_0}\right) - d_{\rho} \rho = 0.
$$

Taking $f = f^*$, $\rho_0 = 10^{-3}$ g/cm³ (9), and $d_\rho = 0.37$ d⁻¹ (10), we get $\rho^* = 3.62 \times 10^{-4}$ g/cm³.

Eq. 8.

- K_P : In ref. 11 it was demonstrated that renal epithelial cells, in response to inflammation by crystals of calcium oxalate monohydrate and excess oxalate ions, secreted monocyte chemotactic protein-1 (MCP-1) at levels of at least 267 pg/mL, which is ∼0.3 ng/mL. We assume that in patients with renal fibrosis the MCP-1 saturation can reach up to $\bar{5}$ ng/mL and take $K_P = 5 \times 10^{-9}$ g/mL.
- λ_{PM} : The degradation rate of MCP-1 is $d_P = 1.73 \text{ d}^{-1} (12)$. We assume that, when M and P are large, the production of MCP-1 by macrophages is three times larger than the degradation of MCP-1, that is, $\lambda_{PM}M_0 = 3d_PK_P$. Because $M_0 = 5 \times$ 10^{-5} g/cm³ (13), we get $\lambda_{PM} = 3d_P K_P/M_0 = 3 \times 10^{-3}$ d⁻¹ .
- \bullet d_{PM} : MCP-1 internalized by macrophages. We assume that the rate of internalization is smaller by a factor of 1/10 than

the rate of production by macrophages when M are P are large, so that

$$
d_{PM}=1/10\lambda_{PM};
$$

hence, $d_{PM} = 2.08 \times 10^{-4} \text{ d}^{-1}$.

SANG

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Eq. 12.

• $\lambda_{T_{\beta}M}$: In the cancer microenvironment, the production rate of TGF-β by TECs is 1.7×10^{-4} d⁻¹ (5). We assume that in our model the production rate by macrophages is much larger and take $\lambda_{T_{\beta}M} = 1.5 \times 10^{-2} \text{ d}^{-1}$.

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Table S1. Accuracy of numerical method

Table S2. Parameter descriptions and values

NAS PNAS

MMP, matrix metalloproteinase; TIMP, tissue inhibitor of metalloproteinase.

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- 2. Miller CC, et al. (2003) Validation of a morphometric method for evaluating fibroblast numbers in normal and pathologic tissues. Exp Dermatol 12(4):403–411.
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- 14. Tietz NW (1999) Clinical Guide to Laboratory Tests (Saunders, Philadelphia), 3rd Ed.

Table S3. Parameter descriptions and values

NAS PNAS

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Table S4. Patient data for different levels of interstitial fibrosis based on kidney biopsy

*The units for urine MCP-1 and urine TGF-^β are nanograms per milligram urine creatinine. †

INF is the degree of interstitial inflammation; 1 and 2 indicate that the degree of interstitial inflammation is <25% and ≥25%, respectively.