





substrate solution (Table S2) to a final concentration of 5  $\mu\text{M}$  peptide substrate (Table S2) in a final reaction volume of 200  $\mu\text{L}$ . The reaction was monitored using a fluorescent plate reader (BioTek Synergy 4) by measuring the release of 7-methoxycoumarinyl-4-acetyl from the quenched substrate peptide with  $\lambda_{\text{ex/em}}$  of 330 and 405 nm. The induction ratio of TVMV-based protease activities in the inhibited and uninhibited states was calculated by dividing the initial rate in the presence of the activating protease over the initial rate in the absence of the activating protease.

**Enzyme kinetics of TVMV-based signal transducers.** To determine the kinetic parameters, the proteolytic activity of different protease biosensors was measured in protease assay buffer over varying concentrations of the substrate TVMV-DD (Table S2) using the protease concentrations indicated in the figure captions. Measurements were performed in duplicate for each substrate concentration. Initial rates were extracted from the change in fluorescence (after subtracting the background fluorescence with no enzyme) and plotted against the substrate concentration. Kinetic parameters were subsequently obtained by a nonlinear regression fit of the curve to Eq. S1

$$Y = V_{\text{max}} \times \frac{[\text{Substrate}]}{[\text{Substrate}] + K_M} \quad [\text{S1}]$$

To estimate the  $K_i$  of the inhibitory peptide EYVRFAP, 500 nM of the TVMV<sup>T214L, V216W</sup> mutant was assayed with 5  $\mu\text{M}$  of the TVMV-DD substrate in the presence of varying concentrations of the inhibitory peptide EYVRFAPGST. Measurements were performed in duplicate for each inhibitor concentration, and the initial rates were extracted as described above. The  $K_i$  was subsequently determined by a nonlinear regression fit of the curve to Eq. S2 with the  $K_M$  and the substrate concentration set to 65 and 5  $\mu\text{M}$ , respectively

$$Y = V_{\text{max}} \times \frac{[\text{Substrate}]}{[\text{Substrate}] + K_M \times \left(1 + \frac{[\text{Inhibitor}]}{K_i}\right)} \quad [\text{S2}]$$

**Assaying TVMV-based allosteric receptors.** The maximum induction ratios and apparent  $K_d$ s of TVMV-based allosteric receptors were measured in ligand titration experiments. The maximum induction ratios were measured using 250 nM TVMV affinity clamp chimera, whereas the apparent  $K_d$ s for the stronger and weaker binding affinity clamp ligands B1 and B2 were measured using 10 and 100 nM TVMV affinity clamp chimera, respectively. Initial rates were extracted from the change in fluorescence (after subtracting the background fluorescence with no enzyme) and plotted against the ligand concentration. The apparent  $K_d$ s of the different types of receptors were determined by a nonlinear regression fit of the curve to Eq. S3

$$Y = V_0 + (V_{\text{max}} - V_0) \times \frac{([\text{Sensor}] + [\text{Ligand}] + K_d) - \sqrt{([\text{Sensor}] + [\text{Ligand}] + K_d)^2 - (4 \times [\text{Sensor}] \times [\text{Ligand}])}}{2 \times [\text{Sensor}]} \quad [\text{S3}]$$

**Protease cascades.** TVMV- and HCV-based signaling cascades were measured as described above except that the reaction was initiated by the addition of the HCV-based signal amplifier. The concentration of the two different ligands B1 and B2, the HCV-based signal transducers, and the TVMV-based allosteric receptors are indicated in the figure legends. The HCV-based substrate was included at 5  $\mu\text{M}$  (Table S2). Initial rates were extracted from the change in fluorescence (after subtracting the background fluorescence with no enzyme) and plotted against the ligand concentration. The apparent

$K_d$ s were determined by a nonlinear regression fit of the curve to Eq. S3.

**Protease-based proximity sensors.** Protease-based proximity sensors tagged with FRB and FKBP were measured as described above except that the reaction was initiated by the addition of the FRB-tagged HCV-based signal amplifier. The concentration of rapamycin, the FRB-tagged HCV-based signal transducer, and the FKBP12-tagged TVMV-based signal transducer are indicated in the figure annotations. The HCV-based substrate was included at 5  $\mu\text{M}$  (Table S2). Initial rates were extracted from the change in fluorescence (after subtracting the background fluorescence with no enzyme) and plotted against the concentration of rapamycin. The apparent  $K_d$ s of for rapamycin was determined by a nonlinear regression fit of the curve to Eq. S3.

**Rationale of Protease-Based Signal Transducers.** In the simpler case of a protease-inducible transducer protease, we formulated a mathematical model based on Michaelis–Menten Kinetics defining the parameters modulating the signal output (Fig. S3). For any given autoinhibited transducer protease, the induction of activity is defined as the ratio of enzyme velocities in the cleaved and un-cleaved states, which are subject to intra- and intermolecular inhibition, respectively, as defined by Eq. S4. Residual inhibition by the cleaved product peptides that remains associated with the protease is not taken into account in the model

$$\text{Induction} = \frac{V_{\text{Cleaved}}}{V_{\text{Uncleaved}}} = \frac{\frac{V_{\text{max}} \times [S]}{K_M^{\text{Cleaved}} + [S]}}{\frac{V_{\text{max}} \times [S]}{K_M^{\text{Uncleaved}} + [S]}}$$

Assume competitive inhibition model

$$\text{Induction} = \frac{V_{\text{Cleaved}}}{V_{\text{Uncleaved}}} = \frac{\frac{V_{\text{max}} \times [S]}{K_M \left(1 + \frac{[E]}{K_i}\right) + [S]}}{\frac{V_{\text{max}} \times [S]}{K_M \left(1 + \frac{[I]}{K_i}\right) + [S]}}$$

After cleavage  $[I]^{\text{Cleaved}} = [E]$

$$\text{Induction} = \frac{V_{\text{Cleaved}}}{V_{\text{Uncleaved}}} = \frac{K_M \left(1 + \frac{[I]}{K_i}\right) + [S]}{K_M \left(1 + \frac{[E]}{K_i}\right) + [S]}$$

Simplify

$$\text{Induction} = \frac{V_{\text{Cleaved}}}{V_{\text{Uncleaved}}} = \frac{1 + \frac{[I]}{K_i} + \frac{[S]}{K_M}}{1 + \frac{[E]}{K_i} + \frac{[S]}{K_M}} \quad [\text{S4}]$$

A plot of Eq. S1 illustrates that the induction of activity is linearly proportional to the intramolecular concentration of the AI

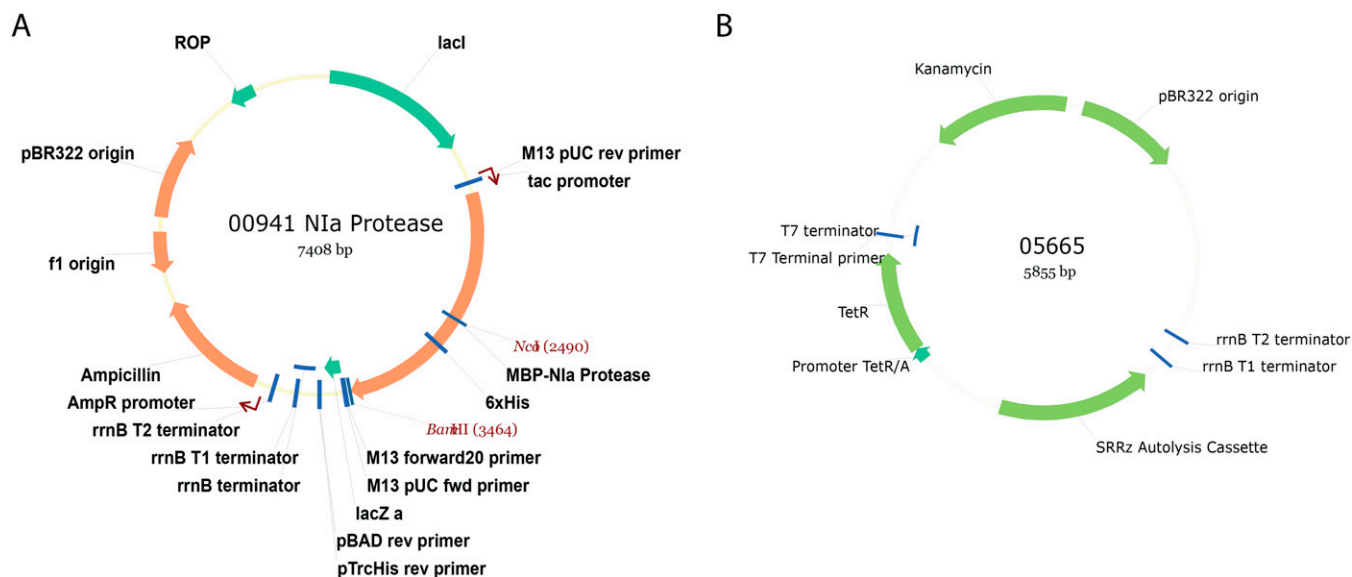
domain in the uncleaved state  $[I]$  (Fig. S3). In practice, this effectively depends on the proximity of the N and C termini to the active site, as well as the structure and length of the connecting linker. The strength of binding of the AI domain  $K_i$  also favorably affects the induction ratio, but must not significantly exceed the operating concentration of the protease transducer to prevent continuing intermolecular inhibition after cleavage. Maximum induction is achieved under saturating reaction conditions at low substrate  $[S]$  and protease transducer concentrations  $[E]$  where competitive inhibition in the intra- and intermolecular states are minimized, and  $[S] \ll K_M$  and  $[E] \ll K_i$ .

**Note on Estimating Signal Amplification Factors.** To obtain an estimate of signal amplification between the one- and two-stage systems, we estimate and compare signal amplification factors both in terms of absolute signal gain and in terms of signal-to-noise ratios. In the former case, protease signals were directly com-

pared with each other, whereas in the latter case, protease signals were additionally normalized over the background signal in the absence of ligand (as denoted by the red traces in Fig. 3 B and C). Moreover, to estimate signal amplification factors, we compare the gradient in the exponential phase (Fig. S7 A and C) as an approximate estimation of increasing concentrations of active HCV, which can thus be more directly compared with the signal generated by TVMV in a single-stage setup. At the same time, we emphasize that it is difficult to compare signal amplification between first- and second-order processes based on one- and two-stage signal amplification systems. However, the fact that we obtain similar  $K_d$  values analyzing one- and two-stage amplification data indicates that the experimental setup and data analysis used are appropriate. Sequences for linkers L1, L2, and L3 encoding for different affinity clamp mutants are summarized in Table S1.

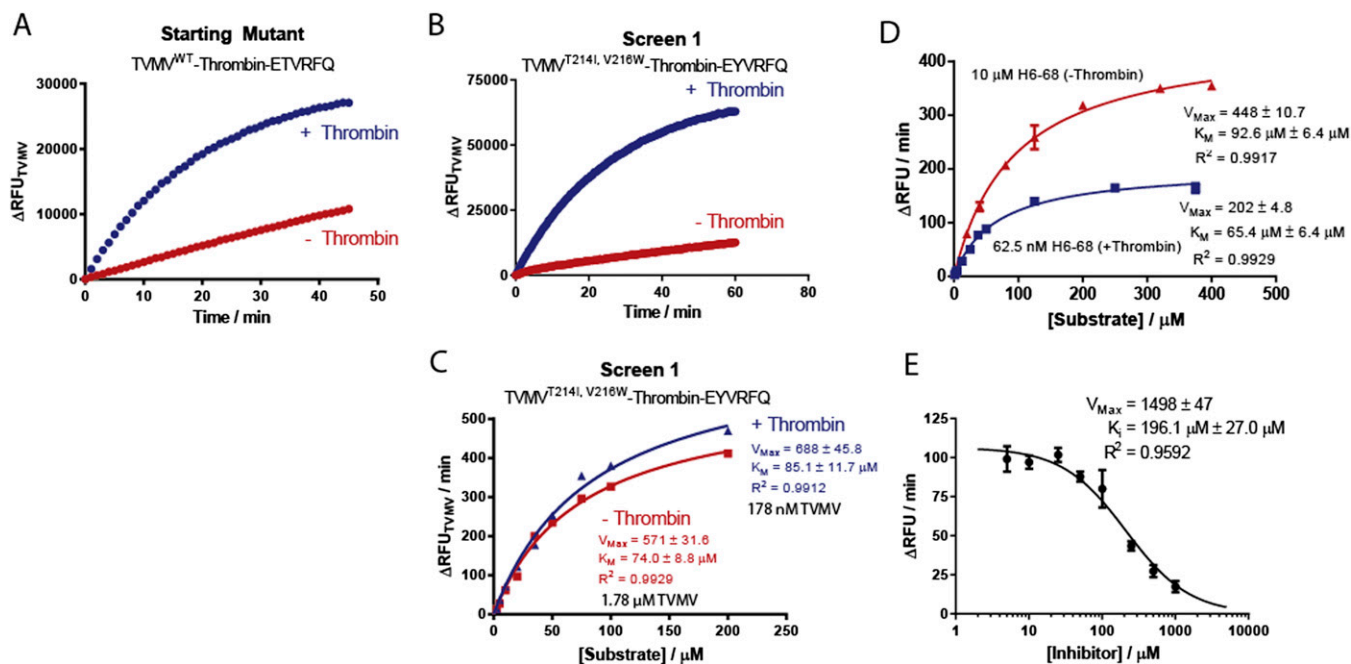
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**Fig. S1.** (A) Plasmid map of the MBP-based expression vector 00941, which was used to express different fusion constructs of TVMV and HCV proteases. (B) Plasmid map of the autolysis vector 05665, which carries the  $\lambda$ -phage derived SRRz autolysis system under the control of the native, tetracycline-inducible bidirectional TetR/A promoter. The SRRz autolysis cassette includes its native 5' UTR.

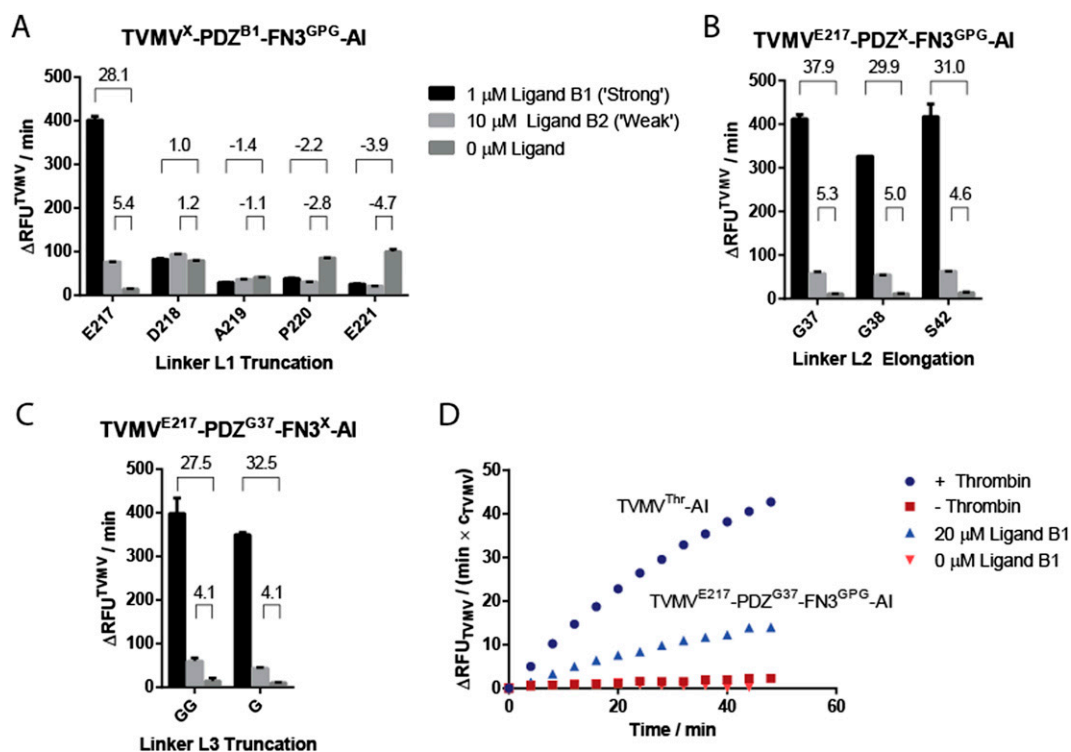
## Engineering TVMV-Based Signal Transducers



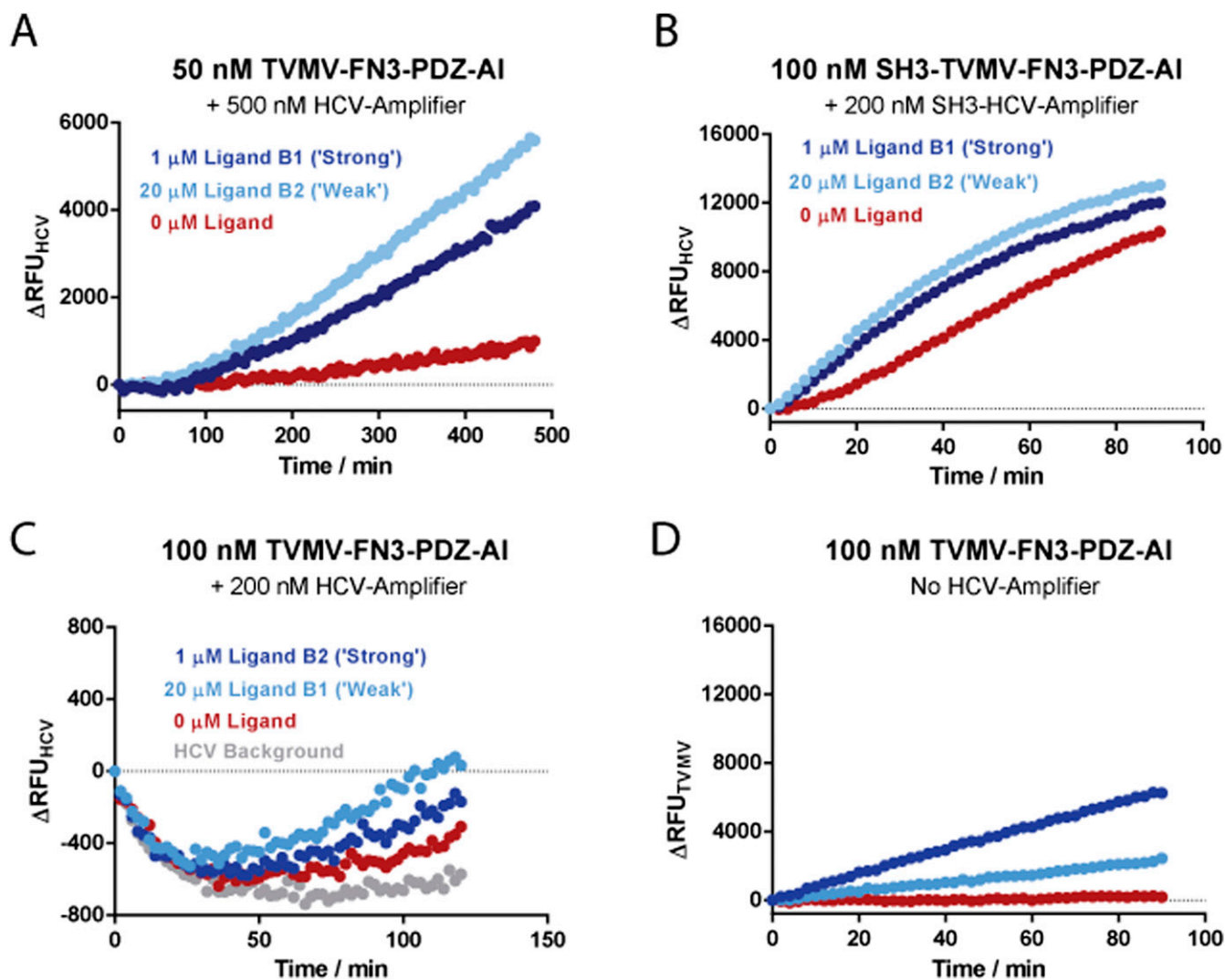
**Fig. S2.** Engineering TVMV-based signal transducers. (A) To create an artificially autoinhibited version of TVMV, its N-terminal cleavage product ETVRFQ was fused to its C terminus via a linker encoding a thrombin cleavage site, yielding a TVMV-based signal transducer (Starting Mutant), which activity could be induced by approximately fivefold following thrombin cleavage. Protease activities were measured using 892 nM TVMV and 5  $\mu\text{M}$  TVMV substrate. (B) To improve the performance of the module, a library screen was devised to enhance the interactions affinity between TVMV and its AI domain. This screen yielded a mutant protease, TVMV<sup>T214I, V216W</sup>, and an altered N-terminal cleavage product EYVRFQ serving as an AI domain (screen 1). Although the induction ratio improved slightly, to  $\sim$ 13-fold, this was still considered insufficient for practical applications. Protease activities were measured using 892 nM TVMV and 10  $\mu\text{M}$  TVMV substrate. (C) Notably, equivalent  $K_m$ s were determined for the TVMV-based protease activities before and after thrombin mediated activation, which suggests that the majority of background activity can be attributed to proteases that lack an AI domain as a result of premature termination of translation or proteolytic degradation. In the autoinhibited state, kinetic parameters were determined using 1.78  $\mu\text{M}$  TVMV. In the activated state following thrombin cleavage, the kinetic parameters were determined using 178 nM TVMV. (D) Michaelis–Menten kinetics of mutant TVMV<sup>V214I, T216W</sup> in its activated (at 62.5 nM) and autoinhibited from (at 10  $\mu\text{M}$ ) assayed with varying concentrations of protease substrate TVMV-DD (Table S2). The kinetic parameters were determined by plotting the initial rates against the substrate concentration and the curve fit by nonlinear regression to Eq. S1. The  $K_m$  value for the thrombin activated form is in agreement with previously measured values for an equivalent substrate of WT TVMV using an HPLC-based assay (1). For the autoinhibited form, the  $K_m$  value associated with the residual activity is  $\sim$ 70-fold weaker but still comparable to the uninhibited enzyme, indicating that this activity is still predominantly due to a population of uninhibited proteases. (E) Titration of 500 nM solution of the TVMV<sup>T214I, V216W</sup> mutant with increasing concentrations of the peptide derived from the autoinhibitor EYVRFAGST. The  $K_i$  value was determined by plotting the initial rates against the ligand concentration and the curve fit by nonlinear regression to Eq. S2.

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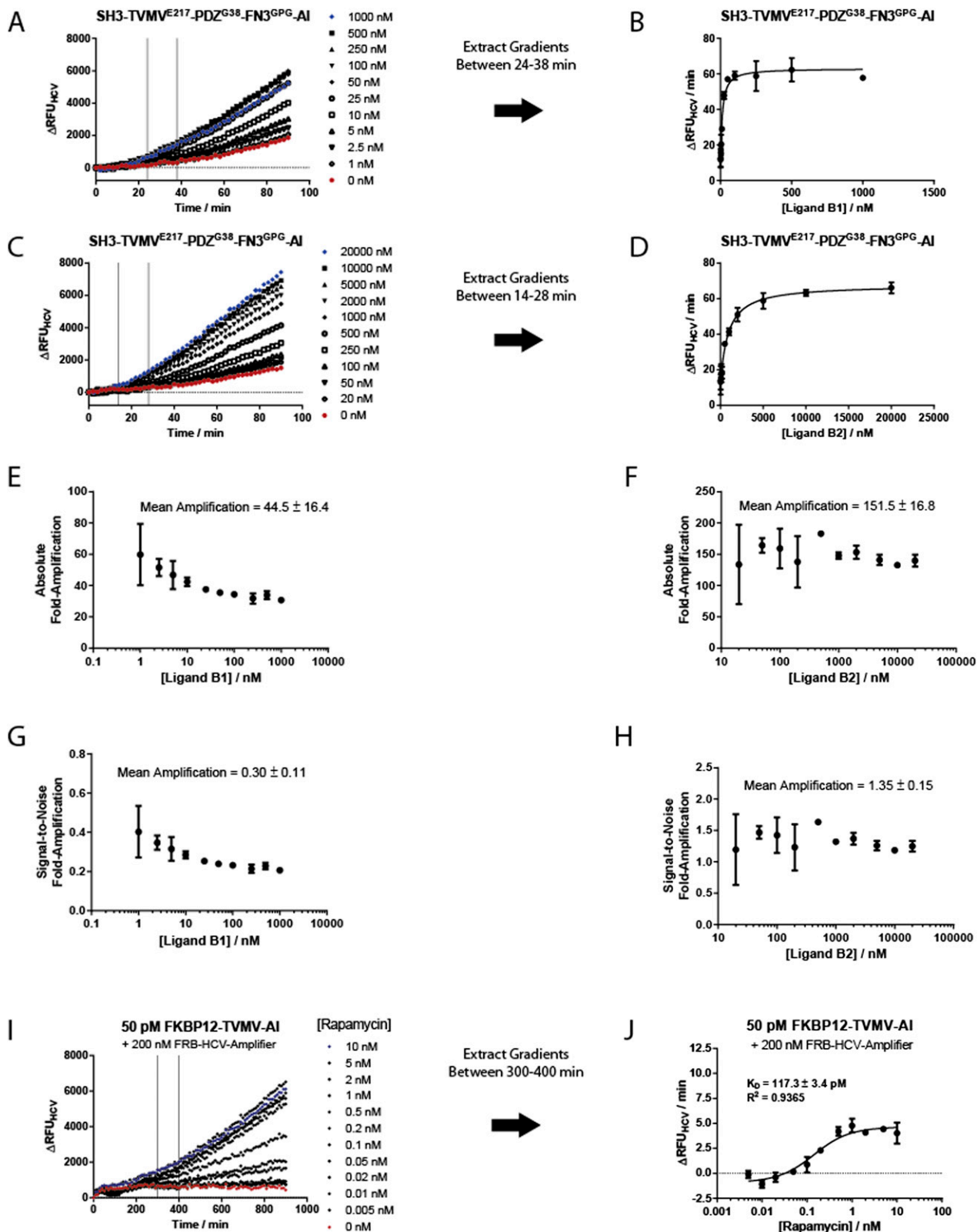


**Fig. S5.** Engineering TVMV-based ligand receptors. (A) The starting mutant TVMV<sup>E221</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI responded to the addition of either ligand B1 or B2 in a switch-OFF fashion. Further shortening L1 by three amino acids yielded a ligand sensor TVMV<sup>D218</sup>-PDZ<sup>B1</sup>-FN3<sup>GPG</sup>-AI that exhibited relatively low activities, but was largely unresponsive to the addition of either ligand B1 or B2. A single amino acid truncation then induced a sharp transition in the switching behavior yielding a ligand sensor TVMV<sup>E217</sup>-PDZ<sup>B1</sup>-FN3<sup>GPG</sup>-AI that responded to the addition of the two different ligands B1 and B2 in 30- and 4-fold switch-ON fashions, respectively. (B) Elongation of linker L2 (connecting the PDZ domain with the FN3 domain) based on switch-ON mutant TVMV<sup>E217</sup>-PDZ<sup>B1</sup>-FN3<sup>GPG</sup>-AI by a single glycine residue yielded mutant TVMV<sup>E217</sup>-PDZ<sup>G37</sup>-FN3<sup>GPG</sup>-AI with a 37-fold induction ratio for ligand B2. Inserting up to four additional amino acids reduced the induction ratio down to 30-fold. (C) Further truncation of the GPG motif in linker L3 (connecting the FN3 domain with the AI domain) based on switch-ON mutant TVMV<sup>E217</sup>-PDZ<sup>G37</sup>-FN3<sup>GPG</sup>-AI down to two or a single glycine residue did not appreciably alter the induction ratio. (D) Comparing the activities of TVMV-based signal transducer and TVMV-based allosteric protease receptor. Under full induction conditions, the TVMV-based allosteric protease receptor achieves 34% activity of the TVMV-based signal transducer (as judged by the concentration normalized initial rates over the first 12 min).



**Fig. S6.** Integrated signal sensing and signal amplification. (A) Signal transmission between a TVMV affinity clamp chimera and an HCV-based amplifier in the absence of scaffolding interactions. Time-resolved trace of HCV protease activities in signal sensing and amplification circuit based on a TVMV affinity clamp chimera (50 nM TVMV<sup>E217</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI) and an HCV-based signal amplifier (500 nM HCV<sup>TVMV</sup>-AI). Here, the TVMV-specific cleavage site in the HCV-based signal amplifier constitutes the only molecular recognition element that mediates signal transmission between the sensor and the amplifier. (B) Signal transmission between a TVMV affinity clamp chimera and an HCV-based amplifier in the presence of SH3-dependent scaffolding interactions based on an unscaffolded TVMV affinity clamp chimera (50 nM TVMV<sup>E217</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI) and an HCV-based signal amplifier (500 nM HCV<sup>TVMV</sup>-AI). (C) Comparing the time resolved traces of protease activities at high sensor concentrations in an integrated ligand sensing and amplification circuit based on an unscaffolded TVMV-based ligand sensor (100 nM TVMV<sup>E217</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI) and an HCV-based signal amplifier (200 nM SH3-HCV<sup>TVMV</sup>-AI) and (D) the TVMV-based ligand sensor (100 nM TVMV<sup>E217</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI) on its own; here, scaffolding interactions are necessary for efficient signal transmission. RFU units generated through the cleavage of TVMV- and HCV-specific peptide protease substrates in the two different systems scale by a factor 1.8–1 (Fig. S4C).





**Fig. S7.** Two-component signaling systems based on autoinhibited TVMV and HCV proteases. (A–D) Determination of the apparent  $K_{dS}$  in the two-stage amplification system. In the two-stage signal sensing and amplification system, the apparent  $K_{dS}$  of the receptor protease (SH3-TVMV<sup>E217</sup>-PDZ<sup>G38</sup>-FN3<sup>GPG</sup>-AI) for ligands B1 and B2 were determined by plotting the observed change in fluorescence between (A) 24–38 min and (C) 14–28 min (as denoted by the vertical lines). The background fluorescence in the absence of enzyme was subtracted and the resulting values plotted against the ligand concentration and (B and D) fitted by the nonlinear regression to Eq. S3. Considering the irreversibility of HCV-based signal amplifier activation by the TVMV-based ligand sensor, the time window for recording the change in fluorescence was deliberately chosen before full activation of the HCV-based signal amplifier has occurred. (E and F)

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