Article

From Metabolomics to Fluxomics: A Computational Procedure to Translate Metabolite Profiles into Metabolic Fluxes

Sonia Cortassa,¹ Viviane Caceres,¹ Lauren N. Bell,² Brian O'Rourke,¹ Nazareno Paolocci,¹ and Miguel A. Aon^{1,*} ¹Division of Cardiology, Johns Hopkins University School of Medicine, Baltimore, Maryland; and ²Metabolon, Inc., Durham, North Carolina

ABSTRACT We describe a believed-novel procedure for translating metabolite profiles (metabolome) into the set of metabolic fluxes (fluxome) from which they originated. Methodologically, computational modeling is integrated with an analytical platform comprising linear optimization, continuation and dynamic analyses, and metabolic control. The procedure was tested with metabolite profiles obtained from ex vivo mice Langendorff-heart preparations perfused with glucose. The metabolic profiles were analyzed using a detailed kinetic model of the glucose catabolic pathways including glycolysis, pentose phosphate (PP), glycogenolysis, and polyols to translate the glucose metabolome of the heart into the fluxome. After optimization, the ability of the model to simulate the initial metabolite profile was confirmed, and metabolic fluxes as well as the structure of control and regulation of the glucose catabolic network could be calculated. We show that the step catalyzed by phosphofructokinase together with ATP demand and glycogenolysis exert the highest control on the glycolytic flux. The negative flux control exerted by phosphofructokinase on the PP and polyol pathways revealed that the extent of glycolytic flux directly affects flux redirection through these pathways, i.e., the higher the glycolytic flux the lower the PP and polyols. This believed-novel methodological approach represents a step forward that may help in designing therapeutic strategies targeted to diagnose, prevent, and treat metabolic diseases.

INTRODUCTION

Considerable effort has been invested in whole-genome/ proteome screenings to detect genetic loci contributing to the susceptibility of complex human diseases such as diabetes and cancer. As a result, gene/protein changes have been cataloged and with the help of systems biology approaches are now transforming medical and clinical practice (1). Yet, articulating "omics" technologies into quantitative and physiologically meaningful mechanisms remains a challenging (2–4) but promising frontier to explore in the attempt to effectively combat chronic diseases such as diabetes.

The complex nature of a disease often originates from impairment of several steps in different biochemical pathways. For instance, the net effect of an inborn error of metabolism on the organ and organism levels is the alteration of one or more metabolite fluxes (5). A metabolic flux is defined as the rate (i.e., molar per unit time) at which metabolites are converted or transported between compartments in a network of biochemical reactions. Ultimately, it is the concept of metabolic flux that is crucial in the translation of genotype and environmental factors into a healthy or disease phenotype.

Editor: Leslie Loew.

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In systemic disorders like diabetes, a whole network of metabolic fluxes is drastically altered. Metabolic remodeling occurs at the level of the genome, transcriptome, and proteome, including posttranslational modifications (2) but, in the end, enzymatic activities and the resulting metabolite profiles will reflect all those changes. Thus, in principle, a metabolite profile could be translated into the set of fluxes that gave rise to the metabolome.

The set of metabolic fluxes, or fluxome, represents a dynamic picture of the phenotype, inasmuch as it captures the metabolome in its functional interactions with the environment and the genome (4,6). As such, the fluxome integrates information on several cellular processes, and hence it is a unique phenotypic signature of cells (2). A main advantage of fluxomics over genomics and proteomics is that it is based on information from metabolites, which are far fewer than genes or proteins (7). For instance, in the mouse there are ~600 detectable low-molecular-weight intermediates (8), whereas there are ~10,000 proteins and ~22,000 protein-encoding genes (4).

For systemic metabolic remodeling, as occurs in diabetes or cancer, metabolic fluxes become crucial for quantitative interpretation (5). For example, the cardiac redox status plays a relevant role in diabetic cardiomyopathy (9). The myocardial redox balance can change in response to hyperglycemia, a prevalent condition in diabetic patients, due to redirection of glucose catabolic fluxes through the NADPH-consuming (polyol) or NADPH-generating (pentose-phosphate (PP)) pathways, respectively. To assess

Submitted June 25, 2014, and accepted for publication November 14, 2014. *Correspondence: maon1@jhmi.edu

Viviane Caceres' present address is Departamento de Farmacologia, Universidade Federal de São Paulo (UNIFESP/EPM), São Paulo, Brazil. Editor Legito Legut

the extent of flux through different pathways occurring simultaneously, a quantitative systems biology approach is needed.

Herein, we introduce a believed-novel metabolomicfluxomic procedure that enables the translation of high throughput metabolite profiles (metabolome) into the fluxome, from which the profiles emerged. Importantly, this methodology also allows one to determine the structure of control and regulation of the fluxome. Our approach consists of the combination of an analytical platform-comprising several integrated quantitative methodologies-with a detailed computational kinetic model that accounts for regulatory interactions. This analytical procedure, spanning from metabolome to fluxome, is applicable to any metabolic system that can be described by kinetic modeling. The advantage of our approach over existing methodologies (10) is that it incorporates regulatory information (e.g., effectors, feedbacks) crucial for understanding dynamic systems. Heart function is an ideal prototypic system to test the usefulness of the approach proposed herein. Because the heart is constantly changing in response to energy demand, the choice of kinetic modeling is justified because it can account for time-dependent behavior. Applying our procedure and combining metabolic flux estimation with cardiac work measurement will lend insight into mechanisms underlying contractile impairment.

MATERIALS AND METHODS

Computational model description

Kinetic modeling of glycolytic, glycogenolytic, polyol, and PP pathways

The computational model consists of a detailed kinetic scheme of glucose catabolism comprising glycolysis, glycogenolysis, PP, and polyol (marked in *red*) pathways (Fig. 1 and see Section S1 in the Supporting Material). Depicted also are the exchanges with the extracellular medium including input (glucose, O_2) and output (lactate, fructose, xylitol) fluxes (*light-blue arrows*).

The model rate equations account for the effect of known regulatory interactions and effectors, e.g., ATP for glucose 6 phosphate dehydrogenase (G6PDH), AMP for phosphofructokinase (PFK), or GDP for pyruvate kinase (PK). In addition to the metabolite concentrations the rate of



FIGURE 1 Main glucose degradation pathways in the heart. The glycolytic, glycogenolytic, pentose phosphate (PP) and polyol pathways taken into account by the computational kinetic model are displayed, along with extracellular exchanges comprising input (glucose, O2) and output (lactate, fructose, xylitol) fluxes (light-blue arrows). (Red) Intermediates of the polyol pathway. Metabolites: Glc, glucose; Hexose 6P, accounts for Glucose 6-phosphate plus Fructose 6-phosphate; G3P, glyceraldehyde 3-phosphate; 1,3-BPG, 1,3-biphosphoglycerate; 3PG, 3-phophoglycerate; PEP, phosphoenolpyruvate; Pyr, pyruvate; Lac, lactate; Glc1P, glucose 1-phosphate; (Maltose)n, maltooligosaccharides (maltose, malto-triose, -tetraose, -hexaose, etc.); 6PGluc, 6-phosphogluconate; Ru5P, ribulose 5-phosphate; R5P, ribose 5-phosphate; X5P, xylulose 5-phosphate; E4P, erythrose 4-phosphate; S7P, sedoheptulose 7-phosphate. Enzymes: ALR, aldose reductase; SoDH, sorbitol dehydrogenase; HK, hexokinase; GP, glycogen phosphorylase; PGM, phosphoglucomutase; HK, hexokinase; PFK, phosphofructokinase 1; ALD, aldolase; GAPDH, glyceraldehyde 3-phosphate dehydrogenase; PGK, phosphoglycerate kinase; ENOL, enolase; PK, pyruvate kinase; LDH, lactate dehydrogenase; G6PDH, glucose 6-phosphate dehydrogenase; 6PGDH, 6-phosphogluconate dehydrogenase; R5PI, Ribose 5-phosphate isomerase; Transket, transketolase; RuPE, Ribulose-phosphate 3-epimerase; Tkt, transketolase; TAL, transaldolase. To see this figure in color, go online.

pyruvate transport into mitochondria was provided as input. The rate at which pyruvate is consumed by mitochondria was derived from the rate of oxygen consumption reported for ex vivo heart preparations (11), analyzed under similar substrate conditions without external workload as in Langendorff-perfused hearts. Two moles of O_2 will be reduced to H_2O in the respiratory chain per mol of pyruvate consumed by mitochondria.

Next, we describe each pathway accounted for by the model, and in a more detailed manner all rate equations are included in the Supporting Material.

Glycolysis

The model of glycolysis was based on Lambeth and Kushmerick (12), who describe the carbohydrate degradation pathway in mammalian skeletal muscle (see Section S2 in the Supporting Material). This model starts from glucose-6-phosphate and takes into account the steps down to lactate formation, excluding hexokinase (HK). The rate expressions and kinetic parameters of HK are from Lueck and Fromm (13) (see Eq. S2). We have introduced an expression to model glucose transport based on a Fick's law of diffusion, thus dependent on the concentration gradient across the plasma membrane (Eq. 1).

Important regulatory steps are described in the model, such as the rate expression of the following: 1) phosphofructokinase, which includes its inhibition by AMP and ATP, its dependence on substrates ATP and fructose 6P, and products ADP and fructose 1,6-bisphosphate (see Eq. S3); and 2) glyceraldehyde 3-phosphate dehydrogenase, which obeys a reversible reaction accounting for hyperbolic kinetic dependence on glyceraldehyde 3-phosphate and biphosphoglycerate, and negative cooperativity by both NAD and NADH (see Eq. S5) (14).

Glycogenolysis

The glycogen degradation pathway comprises debranching enzymes, phosphorylase a and b, and phosphoglucomutase enzymes (see Eqs. S10–S12). The enzymatic rate expressions were based on the skeletal muscle model (12).

PP pathway

The oxidative and nonoxidative branches of the PP pathway were taken into account by the model (see Eqs. S14–S20 in Section S2.3 in the Supporting Material). The rate expressions for each of the enzymatic steps involved in the PP pathway were based on Nishino et al. (15). These authors parameterized their model according to data from McIntyre et al. (16). G6PDH, the first enzyme of the pathway, was parameterized according to Buckwitz et al. (17) and includes ATP inhibition (see Eq. S14).

Polyols

Activation of the polyol pathway may have adverse consequences for heart function (18). Hyperglycemia (19) and sustained β -adrenergic stimulation are both known to stimulate polyols (20). The sorbitol route included fructose synthesis by sorbitol dehydrogenase, in addition to aldose reductase (see Section S2.4 in the Supporting Material). The rate expression and kinetic parameters of aldose reductase were derived from the work of Grimshaw et al. (21) with kinetic data from Kubiseski et al. (22) and Halder and Crabbe (23) (see Eq. S21). Sorbitol and xylitol dehydrogenases were modeled following the kinetic characterization and parameters determined by Karacaoğlan and Ozer (24) and O'Brien et al. (25) (see Eqs. S22 and S23).

ATPase, nonglycolytic NADH consumption, NADPH consumption, and polyol transport

To achieve steady-state behavior, the model formulation also includes rate expressions accounting for the consumption of adenine and pyridine nucleotides and polyol excretion. We assumed that the kinetic behavior of those processes can be represented by hyperbolic functions (see Eqs. S24–S28). The equation representing ATP hydrolysis was considered irreversible, unlike those corresponding to NAD(P)H consumption, which were modeled as reversible reactions.

Integrated analytical platform

Kinetic modeling of metabolic networks, and their continuation and dynamic analyses

Other than steady-state fluxes (26–29), a realistic representation of transient behavior requires detailed kinetic modeling including mechanistic regulatory information such as flux regulation, e.g., by substrate and product inhibition/activation. Kinetic models can also accommodate the nonlinear behavior imparted by feedback and feedforward regulatory mechanisms. Continuation analyses of nonlinear kinetic models allow the exploration of their qualitative as well as quantitative behavior (30–32).

Computer model simulations as a function of time or analyzed at the steady state were carried out with MATCONT (sourceforge.net/projects/ matcont), a package designed for continuation analysis implemented in the software MATLAB (The MathWorks, Natick, MA) (33,34). The kinetic model of glucose catabolism is represented by a system of ordinary differential equations (ODEs) (see Section S1 in the Supporting Material), which was computed as a function of time until a steady state is reached, i.e., when the state variable derivatives are $<1 \times 10^{-10}$. MATLAB's built-in solver, ODE15s, designed for stiff equations, was used as integrator. This ODE solver adjusts the integration step size during the computation.

Linear optimization of V_{max} in the kinetic model

To quantify metabolic fluxes from metabolite profiles using the kinetic model, we assume the validity of the association/dissociation affinity constants determined in vitro for each of the enzymatic steps. Another assumption is that the metabolite concentrations correspond to a steady state, which is experimentally justified by whole heart analysis after 30 min perfusion under specified conditions (see Preparation and Perfusion of Mouse Hearts). Consequently, the V_{max} of each enzyme is the only unknown kinetic parameter subjected to optimization. Metabolic enzymes may change their amounts after transcriptional-translational regulation, or after posttranslational modifications, which are reflected by their V_{max} values.

We used linear optimization (28,35) because the number of $V_{\rm max}$ unknowns (one per step in the network) is larger than the number of metabolites available from metabolomics, implying that the system is underdetermined. Thus, instead of calculating a unique solution for the system, we obtain a volume of possible solutions. This entails that we are able to calculate a range of fluxes compatible with the given initial input, i.e., metabolites concentration profile and exchange fluxes with the extracellular medium. This optimization procedure was inspired by the flux balance analysis developed by Savinell and Palsson (29). For optimization we proceed to represent the rate of each step in the metabolic network by explicit rate expressions that are, in all cases, a linear function of $V_{\rm max}$. The latter assumption is required for applying linear optimization methods.

The method is based on the general equation

$$dx/dt = S * v + b, \tag{1}$$

with dx/dt representing the vector of derivatives of the state variables (intermediary metabolite concentrations); *S* is the stoichiometric matrix of size $n \times m$, with *n* and *m* being the number of metabolites and metabolic fluxes, respectively; and *b* is the vector of transport and demand processes, e.g., biosynthesis. Finally, *v* stands for the vector rates expressed as the rate equation in the model with known kinetic parameters except for V_{max} , which is subjected to optimization. In the network analyzed herein (Fig. 1), n = 19and m = 25; thus, the dimension of the solution space is m-n = 6.

Optimization of the linear algebraic system is performed with the Simplex algorithm (implemented in MATLAB). Maximization of ATP synthesis fluxes or minimization of redox consumption were used as objective functions to constrain the optimization procedure. In Table S24, we quantify the impact of different objective functions on V_{max} (Supporting Material).

Analytical and numerical methods utilized

- 1. The function "linprog" from MATLAB (The MathWorks) was utilized with the Simplex algorithm for optimization of $V_{\rm max}$ values.
- 2. Within the volume of possible solutions, a solution was chosen in order to corroborate that the system is able to reproduce the original metabolite profile. The solution was calculated with the "linsolve" function from MATLAB using six of the maximal values of V_{max} downstream in the metabolic network, e.g., $V_{\text{max},f}^{\text{XDH}}$, $V_{\text{max},f}^{\text{SoDH}}$, $V_{\text{max},f}^{\text{LDH}}$, and E_{TK2} , because they are relatively less interdependent as compared to upstream ones.

After exploring several combinations of the optimized V_{max} values, we chose a solution that fulfilled two conditions: 1) $V_{\text{max}} > 0$ for all enzyme activities in the network, and 2) a solution that belongs to the hypervolume of dimension 6 (see Section S2.2 in the Supporting Material).

With the solution at hand, i.e., the set of optimized V_{max} values, we ran computer simulations to reproduce the initial metabolite profile; once the latter was simulated by the model at steady state, we were also able to obtain the rate or flux through each individual step of the metabolic network. We consider that the set of metabolic fluxes determined correspond to one of the vertices of the volume of solutions corresponding to the fluxome, as illustrated for a simpler system with a two-dimensional solution space (see Fig. S1). To demonstrate the potential of the method, linear algebra functions from the software MATLAB were utilized for matrix calculations to quantitate the main rate-controlling and regulatory steps of the metabolic network, as described next.

Quantifying control and regulatory steps in the metabolic network

Metabolic control analysis quantifies the control in a metabolic pathway through two types of coefficient: the flux (or metabolite concentration) control coefficient and the elasticity coefficient (4,36,37). In general terms, "control" is used to describe quantitatively the effect on flux produced by a change in enzyme activity, whereas "regulation" denotes the modulation of enzyme activity by effectors. In a quantitative sense, regulation refers to how the flux of a pathway is modified through the effect on the rate of an individual step by cellular or external factors, which may include intermediary metabolite, ion concentrations, or pH, and is quantified by the response coefficient. This coefficient measures the fractional change in flux, e.g., glycolysis, in response to a fractional change in an external or internal parameter A (e.g., an effector such as fatty acids) other than enzyme activity (37).

The method of Cortassa et al. (36) and Reder (38) was used to analyze control and regulation of the biochemical network shown in Fig. 1. In addition to the flux and metabolite control coefficients, this method represents a way to analyze, through the response coefficients the sensitivity of the metabolic system to perturbations triggered by an internal change in the system or to an environmental perturbation. The method has been extensively described and validated in Cortassa et al. (36).

The analysis uses the stoichiometric matrix, which defines the structural relationships between the processes and the intermediates participating in the metabolic network, and the elasticity matrix, defined by the dependence of each process in the network upon intermediates and effectors (e.g., metabolites, ions) included in the model (see Section S3 in the Supporting Material). The elasticity matrix is obtained from the derivatives of the rate expressions of individual processes with respect to each intermediate in the metabolic network.

The following matrix relationships were used in the computation of flux and metabolite concentration control coefficients (36),

$$\mathbf{C} = \mathbf{I}\mathbf{d}_r - \mathbf{D}_{\mathbf{x}}\mathbf{v} \ \mathbf{L}(\mathbf{S}_{\mathbf{r}}\mathbf{D}_{\mathbf{x}}\mathbf{v} \ \mathbf{L})^{-1} \mathbf{S}_{\mathbf{r}}, \qquad (2)$$

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$$\mathbf{\Gamma} = -\mathbf{L} \left(\mathbf{S}_{\mathbf{r}} \, \mathbf{D}_{\mathbf{x}} \mathbf{v} \, \mathbf{L} \right)^{-1} \, \mathbf{S}_{\mathbf{r}}, \tag{3}$$

with **C** and **Γ** referring to the matrices of flux- and metabolite-concentration control coefficients, respectively; **Id**_{**r**} is the identity matrix of dimension *r*, the number of processes in the network under study; **D**_x**v** is the elasticity matrix; **S**_{**r**} is the reduced stoichiometric matrix; and **L** is the link matrix that relates the reduced- to the full-stoichiometric matrix of the system.

The stoichiometric matrix S_r is the same one used in the optimization procedure described above, after eliminating redundant rows (see Section S3 in the Supporting Material).

Translating metabolite profiles into metabolic fluxes

To quantitate metabolic fluxes through the glucose degradation pathways (Fig. 1) underpinning the metabolite profile shown Table 1, we followed the flow diagram depicted in Fig. 2.

Conversion of metabolite profiles from relative to quantitative changes

Metabolite profiling performed under controlled conditions informs relative changes in metabolites (see Preparation and Perfusion of Mouse Hearts, and see Section S6 in the Supporting Material). To calculate the fluxes through the network, effective concentrations (in molar units) of metabolites are used. Metabolite concentrations are inputs of the rate expressions from the kinetic model, needed to calculate metabolic fluxes.

The same heart samples that were utilized to perform metabolite profiling, were analyzed by standard enzymatic assay to determine the actual concentration of representative metabolites (glucose, glycerol, glutamate, and lactate) present in the profiles. These metabolite concentration values were used to calibrate the area of the mass spectrometric (MS) peaks to determine the concentrations of all other metabolites present in the MS profiles as follows:

$$Mass_{\text{metabolite}} = \frac{1}{Mean Area_{\text{std}}/Mass_{\text{std}}} \times Area_{\text{metabolite}}.$$
 (4)

*Mean Area*_{std} was determined from the area under the peak of the corresponding molecular ion in the mass spectrum. The *Mass*_{std} was calculated

 TABLE 1
 Comparison of experimental and model-simulated metabolite concentrations

Metabolite	Experimental ^a	Model
Glucose (external)	11	
Glucose (internal)	1.52	1.47
Maltosides	5.6 ± 0.4	5.6
G1P	0.163 ± 0.004	0.15
F6P + G6P	4.06 ± 0.27	4.20
F1,6bP	0.015 ± 0.005	0.0147
G3P	< 0.01	0.009
1,3 DPG	< 0.01	$6.6 imes 10^{-4}$
3-PG	0.57 ± 0.04	0.56
PEP	< 0.01	1.99×10^{-3}
Pyruvate	< 0.01	$8.5 imes 10^{-3}$
Ru5P + X5P	2.58 ± 0.68	2.54
R5P	0.29 ± 0.07	0.39
Sorbitol	0.67 ± 0.32	0.65
Fructose	1.7 ± 1.2	1.72
Xylitol	$0.65~\pm~0.18$	0.66

^aExperimental and model-simulated concentrations are expressed in mmol/L and experimental values are displayed as mean \pm SE (n = 6).



FIGURE 2 Work-flow diagram leading from metabolite profiling to the fluxome, and the analysis of its control and regulatory properties.

from the number of moles determined enzymatically in the same samples that were analyzed by MS multiplied by the mass of the molecular ion. The moles of metabolite in the sample were calculated according to

$$Metabolite (mol) = Mass_{metabolite}/MW molecular ion, (5)$$

where MW stands for molecular weight.

In this procedure, we assume that the area under the peak is proportional to the mass of the molecular ion impacting the MS detector. The sample analyzed by MS corresponded to 20 mg wet weight heart tissue. It was considered that 1 g of wet weight tissue corresponds to 0.42 mL of intracellular water (39).

The metabolite concentrations calculated were used as input data for the model to optimize V_{max} values as described before. After optimization, the model was utilized to simulate the metabolite concentration profile (Table 1). Another input of our procedure is given by the fluxes of exchange with the extracellular medium, i.e., rates of oxygen and glucose consumption, and lactate excretion. These fluxes provide a reference point to estimate the intracellular fluxes. Specifically for this work, we used rates of O₂ consumption reported in How et al. (40).

Preparation and perfusion of mouse hearts

Male wild-type C57BLKS/J-*lepr*⁺/*lepr*⁺ (+/+) mice, 8–10 weeks of age, obtained from Jackson Laboratory (Bar Harbor, ME), were euthanized by pentobarbital injection following the requirements of the Institutional Animal Care/Use Committee at Johns Hopkins University, adherent to National Institutes of Health guidelines. After rapid excision, hearts were retrogradely perfused (employing the Langendorff technique) with Krebs-Henseleit buffer, pH 7.4, containing 1.2 mM P_i, 0.5 mM free Mg²⁺, 1.07 mM free Ca²⁺, and 11 mM glucose as described in Tocchetti et al. (9). Hearts were perfused during ~30 min while paced with a pacing electrode (Radnoti, Monrovia, CA) at 600 bpm (10 Hz, 4 ms duration, 4 V) using a stimulator (Grass Instruments, Quincy, MA).

Vascular tone was assessed through coronary perfusion pressure (CPP) and LV function was monitored with a water-filled, customized latex balloon inserted in the left ventricle and connected to a P23XL pressure transducer with interface cable (Harvard Apparatus Instruments, Holliston, MA) and coupled to a model No. DA100 system (BIOPAC, Santa Barbara, CA) for continuous data recording and offline analysis. LV end-diastolic pressure was set at 5–10 mmHg by adjusting the balloon volume with a Gilmont micrometer syringe (Cole-Parmer, Vernon Hills, IL). The LV-developed (systolic-diastolic) pressure, CPP (both in mmHg), and maximal rates of contraction (dP/dt_{max}) and relaxation (dP/dt_{min}) (both in mmHg/s) were determined. After perfusion, hearts were snap-frozen in liquid nitrogen and sent to Metabolon (Research Triangle Park, NC) for nontargeted metabolite profiling (see Section S4 in the Supporting Material).

RESULTS

Metabolomics analysis of intact mouse hearts

As a first test of our procedure for translating metabolomics into fluxomics, we performed metabolite profiling in intact Langendorff-perfused hearts. Fig. 3 shows the metabolite profiles from the glucose degradation pathways (Fig. 1) as determined in mouse hearts superfused with normal 11 mM glucose. Under these conditions, heart functional variables were (mean \pm SE, n = 6-11 hearts): LV-developed pressure (mmHg) = 54 ± 6.9 ; dP/dt_{max} (mmHg s⁻¹) = 1545 \pm 166; dP/dt_{min} (mmHg s⁻¹) = -1442 \pm 145; CPP (mmHg) = 85.8 \pm 0.97.

Translating metabolite concentrations into metabolic fluxes

The metabolite profile (relative metabolite changes) shown in Fig. 3 constitutes the initial departure point leading to the estimation of metabolite concentration. After optimizing V_{max} , we verified that a solution from the solution space can reproduce the initial metabolite profile by numerical simulation.

Table 1 shows the metabolites concentrations determined experimentally compared with model simulation. Considering experimental error, the computational model accurately reproduced metabolite concentrations from the profile observed experimentally.

Fig. 4 depicts a set of fluxes corresponding to the glucose catabolic fluxome (in μ M s⁻¹) exhibited by mouse hearts



FIGURE 3 Metabolome of glucose utilization pathways obtained from intact mouse heart perfused with normal glucose. Represented are the relative metabolite levels detected in hearts perfused with 11 mM glucose under the conditions described in Materials and Methods (n = 6 hearts). Metabolites and their corresponding pathways are indicated on the y axis. The relative scale intensity in the x axis was determined rescaling each biochemical (n = 6) to set the median equal to 1.0 (Metabolon). (*Whiskers plot*) Median and the mean (*line* and *dot* within the *box*, respectively), upper and lower 75 and 25% percentiles of the box. (*Dots*) Outliers beyond the whiskers of the plots. To see this figure in color, go online.



FIGURE 4 The glucose catabolic fluxome in the mouse heart. Depicted are the fluxes (*shaded background*) next to their respective steps in the metabolic network of glucose utilization (Fig. 1) and expressed in μ M s⁻¹ (equivalent to nmol s⁻¹ mL⁻¹ intracellular water). The fluxes correspond to those leading to the metabolite concentrations that reproduced the ones obtained experimentally as shown in Table 1 (see also Materials and Methods). To see this figure in color, go online.

perfused with glucose only. Displayed is the flux distribution through glycolysis, immediately upstream and downstream of the branch toward the polyol (sorbitol), glycogenolytic, and PP routes. The mouse heart was able to sustain a glycolytic flux as high as 41.8 μ M s⁻¹ upstream glyceraldehyde 3-phosphate (G3P) (Fig. 4). The PP pathway sustained a flux that represents 32% of the glycolytic flux (13.6 μ M s⁻¹), and is approximately three orders-of-magnitude higher than the flux through the polyol pathway (Fig. 4). The mouse heart is able to utilize internal stores of glycogen, revealed by glycogenolysis flux values as high as 36.5 μ M s⁻¹ under these conditions.

Together, these data reveal that glucose is actively utilized from both the perfusion solution and internal glycogen stores. Although glucose from glycogen degradation is mainly broken down via glycolysis, other branching pathways such as PP and polyols were active, especially the former.

Control and regulation of the glucose fluxome

Metabolic control analysis was applied to identify and quantify the control of the flux and metabolite concentrations from the glucose fluxome determined (Fig. 4).

The main rate-controlling steps of the glycolytic flux were (Fig. 5 *A*) as follows: PFK \approx glycogenolysis (flux control coefficient, $C \approx 0.65$) > ATP demand with negative control ($C \sim -0.4$) > Glc uptake ($C \sim 0.12$) > G6PDH with negative control (C = -0.05) > HK (C = 0.03).

A positive control, e.g., C = 0.65 for PFK, means that this enzyme controls 65% of the flux through glycolysis, and that an increase in the activity of PFK will increase the glycolytic flux. On the contrary, a negative control, e.g., C = -0.05 for G6PDH, implies that this enzyme controls 5% of the flux, and an increase in its activity will actually decrease the flux through glycolysis.

The control profile of the PP pathway exhibited the same major rate-controlling steps as glycolysis but with much higher flux control coefficients (Fig. 5 *B*): Glycogenolysis C = 2.2 > ATP demand C = -1.1 (negative) > G6PDH C = 0.8 > glucose uptake $C = 0.4 > \text{HK } C \sim 0.1$.

The negative control of PFK on PP flux means that any increase in the flux through glycolysis will have the opposite effect on the PP flux.

The control profile of the polyol pathway leading to sorbitol and fructose (Fig. 5 *C*) displayed a high positive control by the following steps: ATP demand ($C \sim 14$) > glucose uptake ($C \sim 2$) > aldose reductase (C = 1).

A high negative control was exerted by PFK (C = -13) > glycogenolysis, HK, G6PDH (C = -1).

Overall, the control of the glucose catabolic fluxome is highly distributed with glycogenolysis, PFK, and ATP demand as the major rate-controlling steps. The structure of control reveals that an overall increase in the glycolytic flux will decrease the flux redirection through PP and polyols, as revealed by the negative flux control exerted via PFK on both pathways.



FIGURE 5 Control of the glucose fluxome in the heart. The flux control coefficients of the most rate-controlling steps of glucose catabolism are displayed. The bar length indicates the *x*-axis magnitude of the flux control coefficient (CC) of glycolysis (*A*), PP (*B*), and polyol (*C*) pathways. The corresponding enzymatic steps are indicated at the left of each bar plot. The flux CC can be either positive or negative, and in all cases it was verified that the sum of the CC = 1.0, in compliance with the summation theorem.

DISCUSSION

The main contribution of this work is to describe a believed-novel procedure to translate metabolite profiles (metabolome) into the fluxome, from which the metabolome originated. Tested with metabolite profiles obtained from Langendorff-perfused mouse hearts, we were able to quantitatively reproduce the metabolite concentration profile (Table 1) using a set of optimized V_{max} values corresponding to a particular solution from the solution space.

The resulting parameterized computational model was utilized to calculate the structure of control of the glucose fluxome comprising all catabolic routes involved in glucose degradation. The significant control exerted by the ATP demand is expected from an energy demand-led organ like the heart. Preceding metabolic control analysis work in the heart showed that glucose transport and hexokinase were the most rate-controlling steps of the glycolytic flux (41). The main differences between our approach and Kashiwaya et al. (41) are that, in their work, the allosteric property of PFK was not taken into account, nor was the influence of ATP and ADP on various enzymatic steps. Including these regulatory interactions turned out to be important because PFK exerts a high control on glycolysis and exhibits high elasticity with respect to ATP and ADP levels.

Thus, the response coefficients of PFK, with respect to adenine nucleotides, are high and cannot be ignored. That the ATP demand exerts a negative control on the glycolytic flux, appears counterintuitive because one would expect that an increase in energy demand should be followed by an increase, not a decrease, in glycolysis. However, the negative control of glycolysis by ATP demand can be explained according to control by diffuse loops (4,36). In fact, because PFK is a main rate-controlling step of the glycolytic flux, and that this enzyme activity depends on ATP thereby responding positively to its increase, an increase in ATP demand will decrease ATP availability for PFK activity, thus yielding lower flux through glycolysis.

Alternative strategies for the quantitative analysis of metabolomics data have been proposed by Cakmak et al. (42) and Yizhak et al. (43). Our approach differs from theirs in the following ways: 1) we use mechanistic rate expressions that account for experimentally demonstrated kinetics and regulatory interactions; 2) our analytical platform combines existing analytical methods in an integrated manner for qualitative and quantitative analyses both under steady and time-dependent conditions; and 3) we are able to translate large metabolite datasets into a functional fluxome that by accounting for regulatory interactions enables the computation of the structure of control and regulation of the biochemical network from which the metabolite profiles originated.

Comparison with experimental data

Quantitative validation of our calculations comes from the published results of Buchanan et al. (44), who measured the rate of glycolysis and glucose oxidation in working heart preparations from wild-type and diabetic (db/db) mice (Table 2). The equivalent flux measurements in this work (unloaded Langendorff-perfused heart) corresponded to

TABLE 2	Flux values from the literature compared with
fluxome c	alculations

		Flux reported	Flux estimation	
	Tissue source	$\mu M s^{-1}$	$\mu M s^{-1}$	Reference
Glycolysis	mouse working heart	37.5	41.8	(45)
Glc uptake	rat working heart	76.3	9.8	(41)
Glyn utilization	rat working heart	7.67	36.5	(41)
Glycolysis	mouse working heart	54.17	41.8	(44)
Glc oxidation	mouse working heart	5.42	7.79	(44)
G6PDH	mouse liver	45.2	13.6	(46)
6PGDH	mouse liver	107.2	13.6	(46)
Tkl	mouse liver	49.6	4.5	(46)
TAL	mouse liver	45.6	4.5	(46,47)
XyDH	mouse liver	43.8	0.0031	(47)
SoDH	mouse liver	200.9	0.0036	(47)
G6PDH	mouse liver	7.55	13.6	(47)
6PGDH	mouse liver	6.04	13.6	(47)

Abbreviations are as in Fig. 1. Glyn utilization, glycogen utilization; XyDH, xylitol dehydrogenase.

values extrapolated to the y axis (no workload) in Buchanan et al. (44). These authors found ~1:10 between the glucose oxidized (~600–700 nmol min⁻¹ gram dry weight (gdw)⁻¹) versus glucose catabolized through glycolysis (~6–7 μ mol min⁻¹ gdw⁻¹). This result agrees very well with the ratio obtained in our fluxome calculation (Fig. 4).

Considering ~2 mL of intracellular water gdw^{-1} (39), our calculated pyruvate flux [PEP \rightarrow Pyr] value of 88.1 μ M s⁻¹ corresponds to 5.3 μ mol glucose min⁻¹ gdw⁻¹, similar to the 6–7 μ mol min⁻¹ gdw⁻¹ measured directly in Buchanan et al. (44). Because different authors report fluxes in various units, we have translated all values to $\mu M s^{-1}$ for direct comparison with our results (Table 2). Kashiwaya et al. (41) reported values in the same order of magnitude as those estimated herein, i.e., 76.3 μ M s⁻¹ (Table 2, rows 2 and 3). The quantitative discrepancy may be attributed to the difference in species (mouse versus rat) and physiological conditions (Langendorff versus working heart). However, the measurement of glycolytic flux in mouse working heart (also strain C57BL/6) by Dunn et al. (45) rendered a value of 37.5 μ M s⁻¹, which closely agrees with our flux estimation. Likewise, for mouse liver and the same enzymes (G6PDH, P6GDH), different authors (46,47) reported dissimilar fluxes, but one of them was close to our estimated fluxes (Table 2).

Because the volume of possible solutions depends on the choice of objective function to optimize V_{max} , further validation of our procedure will need an independent experimental approach to quantify metabolic fluxes. Table S24 shows V_{max} values for a number of reactions to illustrate how the solution space can change as a function of the optimization criterion. In each case, the values shown in Table S24 correspond to the vertices of the solutions volume defined by the sets of maximal V_{max} values compatible with the objective function chosen. Although the maximal

 $V_{\rm max}$ of some enzymes varies very little with the change in objective function, e.g., xylitol dehydrogenase, others are very sensitive, e.g., glucose transport. Another approach, by Schuetz et al. (48), performed a thorough evaluation of different objective functions (linear and nonlinear ones) with the aim of unraveling the optimization criterion that rules the metabolic network of, e.g., *Escherichia coli* growing in batch or chemostat culture (48), according to the goodness of the flux prediction.

Limitations of this study

Sources of error associated with the flux estimation using the procedure described herein include variability in the experimental determination of metabolite concentrations or reference fluxes (e.g., respiration, lactate secretion). In the case of metabolites, the results from the matrix composed by the derivatives of rate expressions with respect to V_{max} , denoted $D_r V$, will be affected (see Eq. S29). Although controls of recovery with four internal standards were run during metabolite profiling, quantitation of metabolite concentrations from metabolomics data may be subjected to bias due to metabolites extraction and recovery errors. Regarding reference fluxes, vector *b* in Eq. 1 will be influenced. A description of the maximal error associated with the V_{max} estimation based on Savinell and Palsson (29) is included in Section S3 in the Supporting Material.

When applied to cell populations, metabolomics assumes an average cell that ignores cellular heterogeneity. In this sense the metabolite profile represents an average concentration throughout the heart, and only exchanges between the organ and the perfusion buffer are considered. Thus, cellular heterogeneity (e.g., cardiomyocytes, fibroblasts) and compartmentalization are not taken into account.

At this stage, our procedure generates a volume of possible solutions because the number of unknowns $(V_{\rm max})$ (*m*) is larger than the individual metabolite differential equations (*n*). Consequently, a unique solution cannot be determined. A possible way to restrict the solution space would be through the use of uniform sampling Monte Carlo methods such as those described in Price et al. (49).

CONCLUSIONS

We describe a believed-novel integrated procedure for translating metabolomics into fluxomics as applied to a highly dynamic organ such as the heart. This major step forward has relevant implications for complex metabolic disorders. Insights gained from applying control analysis to the fluxome indicate that glucose oxidation redirection toward pathways that may restore (e.g., pentose phosphate) or impair (e.g., polyol) cardiac redox balance, appear to be crucial for improving type-2 diabetic heart function under stressful conditions (9). Our methodological approach may also help in designing therapeutic strategies targeted to prevent cardiac dysfunction and, eventually, heart failure in diabetic patients.

SUPPORTING MATERIAL

Supporting Materials and Methods, one figure, twenty-five tables, and thirty-three equations are available at http://www.biophysj.org/biophysj/ supplemental/S0006-3495(14)03069-0.

ACKNOWLEDGMENTS

In abstract and partial forms this work has been presented at the Biophysical Society meeting in Philadelphia, PA, and at the Keystone Meeting in Colorado, CO, both in February 2013.

L.N.B. is an employee of Metabolon, Inc. and, as such, has affiliations with or financial involvement with Metabolon, Inc. L.N.B. has no other relevant affiliations or financial involvement with any organization or entity with a financial interest in or financial conflict with the subject matter or materials discussed in the manuscript apart from those disclosed.

This work was supported by National Institutes of Health grants R01-HL091923-01 (to M.A.A. and N.P.) and R21HL106054 (to S.C.).

SUPPORTING CITATIONS

References (50–53) appear in the Supporting Material.

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From metabolomics to fluxomics: A computational procedure to translate metabolite profiles into metabolic fluxes

Sonia Cortassa¹, Viviane Caceres[#], Lauren N Bell², Brian O'Rourke¹, Nazareno Paolocci¹ and Miguel A Aon¹

¹Division of Cardiology, Johns Hopkins University School of Medicine, Baltimore, MD

² Metabolon, Inc., Durham, NC

Supporting Material

Symbol	Name	Ordinary differential equation
Glci	Intracellular glucose	$V_T^{Glc} - V_{HK} - V_{ALDR}$
H6P	Hexose 6 phosphate	$V_{HK} + V_{PGLM} - V_{PFK} - V_{G6PD} + V_{TAL} + V_{TK2}$
FBP	Fructose 1,6 bisphosphate	$V_{PFK} - V_{ALD}$
GAP	Glyceraldehyde 3 phosphare	$V_{ALD} - V_{GAPD} + V_{TK1} - V_{TAL} + V_{TK2}$
BPG	1,3 bisphopho-glycerate	$V_{GAPD} - V_{PGK}$
3PG	3 phosphoglycerate	$V_{PGK} - V_{Enol}$
PEP	Phosphoenol- pyruvate	$V_{Enol} - V_{PK}$
Pyr	Pyruvate	$V_{PK} - V_{LDH} - V_{T}^{Pyr}$
Sor	Sorbitol	$V_{ALDR} - V_{SoDH}$
Fru	Fructose	$V_{SoDH} - V_{T}^{Fru}$
6PG	6 phosphogluconate	$V_{G6PD} - V_{6PGO}$
Ru5P	Ribulose 5 phosphate	$V_{6PGO} - V_{R5PI} - V_{Ru5PE}$
R5P	Ribose 5 phosphate	$V_{R5PI} - V_{TK1}$

Section S1. State variables and ordinary differential equations

X5P	Xilulose 5 phosphate	$V_{Ru5PE} - V_{TK1} - V_{TK2} - V_{XyDH}$
S7P	Sedoheptulose 7 phosphate	$V_{TK1} - V_{TAL}$
E4P	Erythrose 4 phosphate	$V_{TAL} - V_{TK2}$
ХуОН	Xylitol	$V_{XyDH} - V_{T}^{XyOH}$
ATP _i ^a	Cytoplasmic ATP	$V_{HK} - V_{PFK} + V_{PGK} + V_{PK} - V_{ATPase}$
NADH ^a		$V_{GAPD} - V_{LDH} + V_{SoDH} + V_{XyDH} - V_{NADHo}$
NADPH ^a		$V_{G6PD} + V_{6GLO} - V_{ALDR} - V_{NADPHO}$
Mal	Sum of maltose with 2, 3, 4, 5 and 6 glc units)	$V_{Gno_is} - V_{PGa} - V_{PGb}$
G1P	Glucose 1 phosphate	$V_{PGa} + V_{PGb} - V_{PGML}$

^a Two versions of the model were formulated: a full version with 22 state variables (n=22) that has 28 rates (m=28), and a reduced version (for simplicity) that did not take into account ATP_i , NADH and NADPH as state variables, thus did not consider V_{ATPase} , V_{NADHo} or V_{NADPHo} . The reduced version of the model that accounted for ATP_i , NADH and NADPH as parameters has n=19 and m=25. Both versions rendered similar results (i.e. for all processes that are common in both models) for the optimization and calculation of the solution that was further analyzed with Metabolic Control Analysis.

Section S2. Rate Equations and parameters included in the model of the glucose catabolic network

S2.1 Glycolysis

Glucose transport:

$$V_T^{Glc} = k_T^{Glc} \left(Glc_o - Glc_i \right)$$
 [Eq. S1]

Being k_T^{Glc} the diffusion constant of glucose adjusted by linear optimization for each experimental condition. Glc_o stands for the concentration of extracellular glucose.

Hexokinase (HK):

$$V_{HK} = V_{\max}^{HK} \cdot \frac{\left(\frac{ATP_i \cdot Glc_i}{K_{MHK}^{ATP} \cdot K_{MHK}^{Glc}} - \frac{\left(C_T^{ad} - ATP_i\right) \cdot H6P}{K_{MHK}^{ATP} \cdot K_{MHK}^{Glc} K_{HK}^{eq}}\right)}{1 + \frac{Glc_i}{K_{MHK}^{Glc}} + \frac{ATP_i \cdot Glc_i}{K_{MHK}^{ATP} \cdot K_{MHK}^{Glc}} + \frac{H6P}{K_{MHK}^{H6P}} + \frac{\left(C_T^{ad} - ATP_i\right)}{K_{MHK}^{ADP}} + \frac{\left(C_T^{ad} - ATP_i\right) \cdot H6P}{K_{MHK}^{ADP} K_{MHK}^{H6P}}}$$
[Eq. S2]

Symbol	Value	Units	Description	Reference
V ^{HK} _{max}	adjusted	mM s ⁻¹	Maximal rate of hexokinase	
$K_{_{MH\!K}}^{_{Glc}}$	0.11	mM	Michaelis constant for glucose	(2)
$K_{MH\!K}^{\ ATP}$	0.17	mM	Michaelis constant for ATP	(2)
$K_{MHK}^{~~G6P}$	1.4×10 ⁻³	mМ	Michaelis constant for H6P	(2)
K_{MHK}^{ADP}	1.2	mM	Michaelis constant for ADP	(2)
$K_{\scriptscriptstyle HK}^{\scriptscriptstyle eq}$	7800	-	Equilibrium constant for HK	(2)
C_T^{ad}	14.0	mM	Total adenine nucleotides pool	(3)

Table S2. Parameter values used in the Hexokinase rate expression

Phosphofructokinase (PFK):

$$V_{PFK} = \frac{\left(V_{\max,f}^{PFK} \frac{ATP_i \cdot H6P}{K_{MPFK}^{ATP} \cdot K_{MPFK}^{H6P}} - V_{\max,r}^{PFK} \frac{\left(C_T^{ad} - ATP_i\right) \cdot FBP}{K_{MPFK}^{ADP} K_{MPFK}^{FBP} K_{PFK}^{eq}}\right)}{\Delta} \times \left(\frac{1 + \alpha \cdot L \cdot \left(\frac{\Delta'}{\Delta}\right)^3}{1 + L \cdot \left(\frac{\Delta'}{\Delta}\right)^4}\right)$$
[Eq.S3]

Being:

$$\Delta = \left(1 + \frac{H6P}{K_{MPFK}^{H6P}}\right) \cdot \left(1 + \frac{ATP}{K_{MPFK}^{ATP}}\right) + \frac{ADP}{K_{MPFK}^{ADP}} + \frac{FBP}{K_{MPFK}^{FBP}} \left(1 + \frac{ADP}{K_{MPFK}^{ADP}}\right)$$
$$\Delta' = \left(1 + \frac{H6P}{K_{MPFK}^{'H6P}}\right) \cdot \left(1 + \frac{ATP}{K_{MPFK}^{'ATP}}\right) + \frac{ADP}{K_{MPFK}^{'ADP}} + \frac{FBP}{K_{MPFK}^{'FBP}} \left(1 + \frac{ADP}{K_{MPFK}^{'ADP}}\right)$$

$$\alpha = \frac{K_{MPFK}^{H6P} K_{MPFK}^{ATP}}{K_{M}^{'H6P} K_{M}^{'ATP}}$$

$$L = L_o \cdot \left[\left(\frac{1 + \frac{ATP}{K_{iPFK}^{ATP}}}{1 + d \frac{ATP}{K_{iPFK}^{ATP}}} \right) \cdot \left(\frac{1 + e \frac{AMP}{K_{aPFK}^{AMP}}}{1 + \frac{AMP}{K_{aPFK}}} \right) \right]^4$$

$$V_{\text{max,r}}^{PFK} = \frac{V_{\text{max,f}}^{PFK} K_{M}^{ADP} K_{M}^{FBP} K_{M}^{FBP}}{K_{M}^{G6P} K_{M}^{ATP}}$$

Table S3. Parameter values used in the phosphofructokinase rate expression

Symbol	Value	Units	Description	Reference
V ^{PFK} _{max,f}	adjusted	mM s ⁻¹	Maximal rate of phosphofructokinase	
K_{MPFK}^{H6P}	0.18	mM	Michaelis constant for H6P	(4)
$K_{MPFK}^{ ATP}$	0.08	mМ	Michaelis constant for ATP	(4)
K _{M PFK} ^{FBP}	4.02	mM	Michaelis constant for H6P	(4)
$K_{MPFK}^{ ADP}$	1.2	mM	Michaelis constant for ADP	(4)
$K_{MPFK}^{\prime H6P}$	20	mM	Michaelis constant for H6P	(4)
$K'_{M PFK}^{ATP}$	0.25	mM	Michaelis constant for ATP	(4)
$K'_{M PFK}^{FBP}$	4.02	mM	Michaelis constant for H6P	(4)
$K_{M\ PFK}^{\prime\ ADP}$	2.7	mM	Michaelis constant for ADP	(4)
L_o	13	mM	Michaelis constant for ADP	(4)
K _{a PFK}	0.06	mM	Activation constant for AMP	(4)
K _{i PFK} ATP	0.87	mM	Inhibition constant for ATP	(4)
d	0.01			(4)
е	0.01			(4)
AMP	0.1	mМ	Concentration of AMP	(3)
$K^{\it eq}_{\it PFK}$	242.0		Equilibrium constant	(4)

Aldolase (ALD):

$$V_{ALD} = V_{\max}^{ALD} \cdot \frac{\left(\frac{FBP}{K_{MALD}} - \frac{(GAP)^2}{K_{MALD}^{FBP}K_{ALD}^{eq}}\right)}{1 + \frac{FBP}{K_{MALD}^{FBP}} + 2\frac{(GAP)}{K_{MALD}^{GAP}}}$$
[Eq. S4]

Table S4. Parameter values used in the Aldolase rate expression

Symbol	Value	Units	Description	Reference
$V_{ m max}^{ALD}$	adjusted	mM s ⁻¹	Maximal rate of aldolase	
K _{M ALD} ^{FBP}	0.05	mM	Michaelis constant for FBP	(4)
$K_{MALD}^{\ \ GAP}$	2.1	mM	Michaelis constant for GAP	(4)
$K^{eq}_{\scriptscriptstyle ALD}$	0.12		Equilibrium constant	(4)

Glyceraldehyde 3 phosphate dehydrogenase (GAPD):

$$V_{GAPD} = \frac{\left(V_{max,f}^{GAPD} \frac{GAP}{K_{MGAPD}^{GAP} K_{MGAPD}^{Pi}} \left(\frac{(C_{T}^{Pyr} - NADH)}{K_{MGAPD}}\right)^{nGD} - V_{max,r}^{GAPD} \frac{BPG}{K_{MGAPD}^{BPG}} \left(\frac{NADH}{K_{MGAPD}^{NADH}}\right)^{nGD}\right)}{\Delta_{GAPD}}$$

$$\left(Eq. S5\right)$$

$$V_{max,r}^{GAPD} = \frac{V_{max,f}^{GAPD} K_{MGAPD}^{NADH} K_{MGAPD}^{BPG}}{K_{MGAPD}^{GAPD} K_{MGAPD}^{Pi} K_{GAPD}^{eq}}}{K_{MGAPD}^{GAPD} K_{MGAPD}^{NAD} K_{GAPD}^{Pi}}\right)^{nGD} + \frac{Pi}{K_{MGAPD}^{Pi}} + \frac{GAP}{K_{MGAPD}^{GAP}} \left(\frac{(C_{T}^{Pyr} - NADH)}{K_{MGAPD}^{ND}}\right)^{nGD}}{K_{MGAPD}^{GAP}} + \frac{Pi}{K_{MGAPD}^{GAP}} + \frac{GAP}{K_{MGAPD}^{GAP}} \left(\frac{(C_{T}^{Pyr} - NADH)}{K_{MGAPD}^{ND}}\right)^{nGD}}{K_{MGAPD}^{GAP}} + \frac{BPG}{K_{MGAPD}^{GAP}} + \left(\frac{NADH}{K_{MGAPD}^{ND}}\right)^{nGD}}{K_{MGAPD}^{GAP}} + \frac{BPG}{K_{MGAPD}^{GAP}} \left(\frac{NADH}{K_{MGAPD}^{ND}}\right)^{nGD}}{K_{MGAPD}^{GAP}} + \frac{BPG}{K_{MGAPD}^{BPG}} \left(\frac{NADH}{K_{MGAPD}^{ND}}\right)^{nGD}}{K_{MGAPD}^{BPG}} + \frac{BPG}{K_{MGAPD}^{BPG}} \left(\frac{NADH}{K_{MGAPD}^{ND}}\right)^{nGD}}$$

Symbol	Value	Units	Description	Reference
V ^{GAPD} _{max,(f)(r)}	adjusted	mM s ⁻¹	Maximal rate of GAPD (forward or reverse)	
$K_{\scriptscriptstyle MGAPD}^{\scriptscriptstyle NAD}$	9.0×10 ⁻³	mM	Michaelis constant for NAD	(4)
$K_{\scriptscriptstyle MGAPD}^{\scriptscriptstyle NADH}$	3.3×10 ⁻³	mM	Michaelis constant for NADH	(4)
$K_{\scriptscriptstyle MGAPD}^{\scriptscriptstyle GAP}$	2.5×10 ⁻³	mM	Michaelis constant for GAP	(4)
$K^{\ BPG}_{MGAPD}$	8.0×10 ⁻⁴	mM	Michaelis constant for BPG	(4)
$K_{\scriptscriptstyle MGAPD}^{\scriptscriptstyle Pi}$	0.29	mM	Michaelis constant for Pi	(4)
Pi	3.0	mM	Concentration of phosphate	
nGD	0.64	mM	Cooperativity coefficient	
C_T^{Pyr}	1.0	mM	Total pyridine nucleotides pool	(5)
K^{eq}_{GAPD}	0.089		Equilibrium constant	(4)

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Table S5. Parameter values used in the Glyceraldehyde 3 phosphate dehydrogenase rate expression

Phosphoglycerol kinase (PGK):

$$V_{max,r}^{PGK} = \frac{V_{max,f}^{PGK} K_{M}^{ATP} K_{M}^{BPG} K_{M}^{BPG}}{K_{M}^{BPG} K_{M}^{ADP} K_{PGK}^{eq}} + \frac{(C_{T}^{ad} - ATP)}{K_{M}^{ADP} K_{PGK}^{eq}} + \frac{BPG}{K_{M}^{BPG} K_{M}^{ADP}} + \frac{BPG}{K_{M$$

Symbol	Value	Units	Description	Reference
V ^{PGK} _{max,(f)(r)}	adjusted	mM s ⁻¹	Maximal rate of PGK (forward or reverse)	
K_{MPGK}^{BPG}	2.2×10 ⁻³	mM	Michaelis constant for BPG	(4)
K_{MPGK}^{3PG}	1.2	mM	Michaelis constant for 3PG	(4)
K_{MPGK}^{ADP}	8.0×10 ⁻⁴	mM	Michaelis constant for ADP	(4)
K_{MPGK}^{ATP}	0.35	mM	Michaelis constant for ATP	(4)
K^{eq}_{PGK}	57109		Equilibrium constant	(4)

Table S6. Parameter values used in the Phosphoglycerate kinase rate expression

Enolase (Enol):

 $V_{\max,r}^{Enol} = \frac{V_{\max,f}^{Enol} K_{MEnol}^{PEP}}{K_{MEnol}^{3PG} K_{Enol}^{eq}}$

$$V_{Enol} = \frac{\left(V_{\max,f}^{Enol} \frac{3PG}{K_{MEnol}^{3PG}} - V_{\max,r}^{Enol} \frac{PEP}{K_{MEnol}}\right)}{1 + \frac{3PG}{K_{MEnol}^{3PG}} + \frac{PEP}{K_{MEnol}^{PEP}}}$$

Table S7. Parameter values used in the Enolase rate expression

Symbol	Value	Units	Description	Reference
$V^{Enol}_{\max,({\rm f})({\rm r})}$	Adjusted	mM s ⁻¹	Maximal rate of Enol (forward or reverse)	
$K_{M Enol}^{3 PG}$	0.12	mМ	Michaelis constant for BPG	(4)
$K_{M Enol}^{\ PEP}$	0.37	mМ	Michaelis constant for 3PG	(4)
$K^{\it eq}_{\it Enol}$	0.49		Equilibrium constant	(4)

[Eq. S7]

Pyruvate Kinase (PK):

$$V_{PK} = \frac{\left(V_{\max,f}^{PK} \frac{(C_{T}^{ad} - ATP_{i}) \cdot PEP}{K_{MPK}^{ADP} \cdot K_{MPK}^{PEP}} - V_{\max,r}^{PFK} \frac{ATP_{i} \cdot Py}{K_{MPK}^{ATP} K_{MPK}^{Py} K_{PK}^{eq}}\right) \cdot \left(\frac{1}{1 + L_{PK}}\right)$$

$$\left[\text{Eq. S8} \right]$$

$$U_{PK} = \frac{\left(\frac{C_{T}^{ad} - ATP_{i}}{K_{MPK}^{ADP}} + \frac{PEP}{K_{MPK}^{ADP}} + \frac{(C_{T}^{ad} - ATP_{i}) \cdot PEP}{K_{MPK}^{ADP} \cdot K_{MPK}^{PEP}} + \frac{ATP_{i}}{K_{MPK}^{ATP}} + \frac{Py}{K_{MPK}^{PF}} + \frac{ATP_{i} \cdot Py}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(C_{T}^{ad} - ATP_{i}) \cdot PEP}{K_{MPK}^{ADP} \cdot K_{MPK}^{PEP}} + \frac{ATP_{i}}{K_{MPK}^{ATP}} + \frac{Py}{K_{MPK}^{PF}} + \frac{ATP_{i} \cdot Py}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{ATP} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K_{MPK}^{PF}} + \frac{(1 - 1 - 1 - 1) \cdot PP}{K_{MPK}^{PF} \cdot K$$

Table S8. Parameter v	alues used	in the Pyrı	uvate kinase	rate expression

$V_{\max,(f)(r)}^{PK}$	Adjusted		Value Units Description	
	Aujusicu	mM s ⁻¹	Maximal rate of PK (forward or reverse)	
K_{MPK}^{PEP}	0.08	mM	Michaelis constant for PEP	(4)
K_{MPK}^{Py}	7.05	mM	Michaelis constant for Py	(4)
K_{MPK}^{ADP}	0.3	mM	Michaelis constant for ADP	(4)
K_{MPK}^{ATP}	1.13	mM	Michaelis constant for ATP	(4)
K _{M PK} ^{FBP}	0.005	mM	Michaelis constant for FBP	(5)
$K^{\ GDP}_{MPK}$	0.1	mM	Michaelis constant for GDP	(5)
GDP	0.1	mM	Concentration of GDP	(5)
K^{eq}_{PGK}	10304		Equilibrium constant	(4)

$$V_{LDH} = \frac{\left(V_{\text{max,f}}^{LDH} \frac{NADH}{K_{MLDH}^{NADH} \cdot K_{MLDH}^{Py}} - V_{\text{max,r}}^{LDH} \frac{\left(C_{T}^{Pyr} - NADH\right) \cdot Lac}{K_{MLDH}^{NAD} K_{MLDH}^{Lac} K_{LDH}^{eq}}\right)}{1 + \frac{NADH}{K_{MLDH}^{NADH}} + \frac{Py}{K_{MLDH}^{Py}} + \frac{NADH}{K_{MLDH}^{NADH} \cdot K_{MLDH}^{Py}} + \frac{\left(C_{T}^{Pyr} - NADH\right)}{K_{MLDH}^{NAD}} + \frac{Lac}{K_{MLDH}^{Lac}} + \frac{\left(C_{T}^{Pyr} - NADH\right) \cdot Lac}{K_{MLDH}^{NAD} K_{MLDH}^{Lac}}}$$
[Eq. S9]

$$V_{\max,r}^{LDH} = \frac{V_{\max,f}^{LDH} K_{MLDH}^{NAD} K_{MLDH}^{Lac}}{K_{MLDH}^{Py} K_{MLDH}^{NADH}}$$

Table S9. Parameter values used in the Lactate dehydrogenase rate expression

Symbol	Value	Units	Description	Reference
V ^{LDH} _{max,(f)(r)}	adjusted	mM s ⁻¹	Maximal rate of LDH (forward or reverse)	
$K_{\scriptscriptstyle MLDH}^{\scriptscriptstyle NADH}$	2.0×10 ⁻³	mM	Michaelis constant for NADH	(4)
$K_{\scriptscriptstyle MLDH}^{\scriptscriptstyle NAD}$	0.849	mM	Michaelis constant for NAD	(4)
K^{Py}_{MLDH}	3.35×10 ⁻²	mM	Michaelis constant for Py	(4)
$K_{\scriptscriptstyle MLDH}^{\scriptscriptstyle Lac}$	17	mM	Michaelis constant for BPG	(4)
$K^{\scriptscriptstyle eq}_{\scriptscriptstyle LDH}$	16198		Equilibrium constant	(4)

S2.2 Glycogenolysis

$$V_{Gno_{is}} = V_{max}^{Gno_{is}} \cdot \frac{Glc_n}{Glc_n + K_{MGno_{is}}^{Gno}}$$

[Eq. S10]

Table S10. Parameter values used in the glycogen breakdown rate expressi	ion
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Symbol	Value	Units	Description
$V_{ m max}^{Gno_is}$	adjusted	mM s ⁻¹	Maximal rate of glycogen breakdown
$K^{Gno}_{MGno_is}$	5.0	mM	Michaelis constant for Glycogen
Glc_n	110	mM	Glycogen levels cardiac muscle

Glycogen Phosphorylase (GPa,b):

$$V_{GPa} = \frac{\left(V_{\max,f}^{GPa} \frac{Mal \cdot Pi}{K_{iGPa,f}^{Mal} \cdot K_{MGPa}^{Pi}} - V_{\max,r}^{GPa} \frac{Mal \cdot G1P}{K_{aGPa,b}^{Mal} K_{aGPa}^{G1P}}\right)}{1 + \frac{Mal}{K_{iGPa,f}^{Mal}} + \frac{Pi}{K_{iGPa,f}^{Pi}} + \frac{Mal}{K_{aGPa,b}^{Mal}} + \frac{G1P}{K_{aGPa}^{G1P}} + \frac{Mal}{K_{aGPa,f}^{G1P}} - \frac{Pi}{K_{iGPa,f}^{G1P}} + \frac{Mal}{K_{iGPa,f}^{G1P}} \frac{Pi}{K_{iGPa,b}^{G1P}} + \frac{Mal}{K_{iGPa,b}^{G1P}} \left(\frac{AMP^{nH}}{K_{aGPa,b}^{Mal}} + \frac{Pi}{K_{iGPb,f}^{Mal} \cdot K_{MGPb}^{Pi}} - V_{\max,r}^{GPb} \frac{Mal \cdot G1P}{K_{iGPb,b}^{Mal} K_{iGPb}^{G1P}}\right)}{1 + \frac{Mal}{K_{iGPb,f}^{Mal}} + \frac{Pi}{K_{iGPb,b}^{IP}} + \frac{Mal}{K_{iGPb,b}^{Mal}} + \frac{Pi}{K_{iGPb,f}^{G1P}} + \frac{Mal}{K_{iGPb,f}^{Mal}} + \frac{Pi}{K_{iGPb,f}^{G1P}} + \frac{Mal}{K_{iGPb,f}^{Mal}} \frac{Pi}{K_{iGPb}^{Pi}} + \frac{Mal}{K_{iGPb,b}^{Mal}} \frac{G1P}{K_{iGPb}^{G1P}} \left(\frac{AMP^{nH}}{K_{MGPb}^{MaH}} + \frac{Pi}{K_{iGPb,f}^{Mal} \cdot K_{iGPb,f}^{Mal}} + \frac{Pi}{K_{iGPb,f}^{G1P}} + \frac{Mal}{K_{iGPb,f}^{Mal}} \frac{Pi}{K_{iGPb}^{Pi}} + \frac{Mal}{K_{iGPb,b}^{Mal}} \frac{G1P}{K_{iGPb}^{G1P}} \right)$$

$$V_{GP(a)(b)} = \frac{V_{\max,f}^{GP(a)(b)}K_{iGP,f}^{Mal} K_{iGP}^{G1P}}{K_{iGP,f}^{Mal} K_{GP}^{G1P}}}$$

Table S11. Parameter values used in the Glycogen phosphorylase rate expression

Symbol	Value	Units	Description	Reference
$V_{ m max,f}^{PGa}$	Adjusted	mM s ⁻¹	Maximal rate of GPa, forward	
$V_{ m max,f}^{PGb}$	Adjusted	mM s ⁻¹	Maximal rate of GPb, forward	
$K_{iGPa,f}^{Mal}$	1.7	mМ	Michaelis constant for Mal	(4)
$K_{aGPa}^{\ G1P}$	1.5	mM	Michaelis constant for ADP	(4)

$K^{Mal}_{iGPa,b}$	0.15	mM	Michaelis constant for ATP	(4)
K_{MGPa}^{Pi}	4.0	mM	Michaelis constant for FBP	(4)
K_{iGPa}^{Pi}	4.7	mM	Michaelis constant for GDP	(4)
$K^{Mal}_{iGPb,f}$	15	mM	Michaelis constant for Mal	(4)
K^{G1P}_{iGPb}	7.4	mM	Michaelis constant for ADP	(4)
$K^{Mal}_{iGPb,b}$	4.4	mM	Michaelis constant for ATP	(4)
K_{MGPb}^{Pi}	0.2	mM	Michaelis constant for FBP	(4)
K^{Pi}_{iGPb}	4.6	mM	Michaelis constant for GDP	(4)
$K_{M\ GPb}^{\prime \ AMP}$	1.9×10 ⁻⁶	mM		(4)
nH	1.75		Allosteric coefficient for AMP	(4)
K^{eq}_{GP}	0.42		Equilibrium constant	(4)

Phosphoglucomutase (PGLM):

$$V_{PGLM} = V_{\max,f}^{PGLM} \frac{\left(\frac{G1P}{K_{M}^{G1P}} - \frac{G6P}{K_{M}^{G1P}K_{PGLM}^{eq}}\right)}{1 + \frac{G1P}{K_{M}^{G1P}} + \frac{G6P}{K_{M}^{G6P}}}$$
[Eq. S13]

 Table S12. Parameter values used in the Phosphoglucomutase rate expression

Symbol	Value	Units	Description	Reference
$V_{\max,f}^{PGLM}$	adjusted	mM s ⁻¹	Maximal rate of PGLM	
$K_{\scriptscriptstyle MPGLM}^{ G1P}$	0.063	mM	Michaelis constant for G1P	(4)
$K_{\scriptscriptstyle MPGLM}^{\scriptscriptstyle G6P}$	0.03	mM	Michaelis constant for G6P	(4)
K^{eq}_{PGLM}	16.62		Equilibrium constant	(4)

S2.3 Pentose Phosphate pathway

Glucose 6 phosphate dehydrogenase (G6PDH):

$$V_{G6PD} = \frac{V_{max}^{G6PD} \frac{H6P \cdot (C_T^{PyP} - \text{NADPH})}{K_M^{H6P} \cdot K_M^{NADP}}}{1 + \frac{(C_T^{PyP} - \text{NADPH})}{K_M^{NADP}} \left(1 + \frac{H6P}{K_M^{H6P}}\right) + \frac{NADPH}{K_M^{NADPH}} + \frac{ATP}{K_M^{ATP}}}$$
[Eq. S14]

Table S13. Parameter values used in the Glucose 6 phosphate dehydrogenase rate expression

Symbol	Value	Units	Description	Reference
$V_{\rm max}^{G6PD}$	adjusted	mM s ⁻¹	Maximal rate of LDH (forward or reverse)	
K_{MG6PD}^{H6P}	6.67×10 ⁻³	mМ	Michaelis constant for H6P	(4)
K_{MG6PD}^{NADP}	3.67×10 ⁻³	mM	Michaelis constant for NADP	(4)
$K_{MG6PD}^{ m NADPH}$	3.12×10 ⁻³	mM	Michaelis constant for NADPH	(4)
C_T^{PyP}	0.05	mM	Total concentration of Phospho pyridine nucleotides pool	(6)
K_{MG6PD}^{ATP}	0.749	mM	Michaelis constant for BPG	(4)

6 phosphogluconate dehydrogenase (6 PGO):

[Eq. S15]

$$V_{6PGO} = E_{6PGO} \cdot \frac{\left(k_1k_3k_5k_7k_9(C_T^{PyP} - NADPH) \cdot 6PG - k_2k_4k_6k_8k_{10} NADPH \cdot Ru5P\right)}{\left(k_2k_9(k_4k_6 + k_5k_6 + k_5k_7) + k_1k_9(k_4k_6 + k_5k_6 + k_5k_7)(C_T^{PyP} - NADPH) + k_3k_5k_7k_9 \cdot 6PG + k_2k_4k_6k_8 Ru5P\right)} - k_2k_4k_6k_8 Ru5P + k_2k_{10}(k_4k_6 + k_5k_6 + k_5k_7)NADPH + k_1k_3(k_5k_7 + k_5k_9 + k_6k_9 + k_7k_9)(C_T^{PyP} - NADPH) \cdot 6PG + k_1k_4k_6k_8(C_T^{PyP} - NADPH) \cdot Ru5P + k_3k_5k_7k_{10} \cdot 6PG \cdot NADPH + k_8k_{10}(k_2k_4 + k_2k_5 + k_2k_6 + k_4k_6) \cdot Ru5P \cdot NADPH} - k_1k_3k_8(k_5 + k_6)(C_T^{PyP} - NADPH) \cdot 6PG \cdot Ru5P + k_3k_8k_{10}(k_5 + k_6) \cdot 6PG \cdot Ru5P \cdot NADPH}$$

Table S14. Parameter values used in the 6	phosp	hoglu	iconate d	lehyo	drogenase	e rate exp	ression
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Symbol	Value	Units	Description	Reference
E _{6PGO}	adjusted	mM	Maximal concentration of 6PGO	
k_1	2.4×10 ³	s ⁻¹	Rate constant	(7)

k_2	4.1×10^2	s ⁻¹	Rate constant	(7)
<i>k</i> ₃	2.0×10 ⁶	$\mathrm{mM}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_4	26	$\mathrm{mM}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_5	48.0	s ⁻¹	Rate constant	(7)
k_6	30.0	s ⁻¹	Rate constant	(7)
k_7	6.3×10 ²	s ⁻¹	Rate constant	(7)
k_8	36	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_9	8.0×10 ²	s ⁻¹	Rate constant	(7)
k_{10}	2.25×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)

Ribose 5P Isomerase (R5PI):

$$V_{RSPI} = E_{RSPI} \frac{\left(\frac{k_3 Ru5P}{(k_2 + k_3)} - \frac{k_2 R5P}{(k_2 + k_3)}\right)}{k_1} - \frac{k_2 R5P}{(k_2 + k_3)}}{1 + \frac{Ru5P}{(k_2 + k_3)}} + \frac{R5P}{(k_2 + k_3)}}{k_1}$$
[Eq. S16]

Table S15. Parameter values used in the Ribose 5 phosphate isomerase rate expression

Symbol	Value	Units	Description	Reference
E _{R5PI}	adjusted	mM	Maximal concentration of R5PI	
k_1	60.9	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₂	33.3	s ⁻¹	Rate constant	(7)
<i>k</i> ₃	14.2	$\mathrm{mM}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_4	21.6	$\mathrm{mM}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)

Ribulose 5P Epimerase (Ru5PE):

$$V_{RuSPE} = E_{RuSPE} \left(\frac{\left(\frac{k_3 Ru5P}{(k_2 + k_3)} - \frac{k_2 X5P}{(k_2 + k_3)} \right)}{k_1} - \frac{k_2 X5P}{(k_2 + k_3)} \right) + \frac{Ku5P}{(k_2 + k_3)} + \frac{Ku5P}{(k_2 +$$

Table S16. Parameter values used in the Ribulose 5 phosphate epimerase rate expression

Symbol	Value	Units	Description	Reference
E _{Ru5PE}	adjusted	mM	Maximal concentration of Ru5PE	
k_1	3.91×10 ³	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₂	4.38×10 ²	s^{-1}	Rate constant	(7)
<i>k</i> ₃	3.05×10 ²	s ⁻¹	Rate constant	(7)
k_4	1.49×10 ³	$\mathrm{m}\mathrm{M}^{\mathrm{-1}}\mathrm{s}^{\mathrm{-1}}$	Rate constant	(7)

Transketolase 1 (TK1):

$$V_{TK1} = E_{TK1} \cdot \frac{\left(k_1 k_3 k_5 k_7 \cdot X5P \cdot R5P - k_2 k_4 k_6 k_8 \cdot GAP \cdot S7P\right)}{\left(k_1 k_3 (k_6 + k_7) \cdot X5P + k_5 k_7 (k_2 + k_3) \cdot R5P + k_2 k_4 (k_6 + k_7) \cdot GAP + k_6 k_8 (k_2 + k_3) \cdot S7P + k_1 k_4 (k_6 + k_7) \cdot X5P \cdot R5P + k_4 k_8 (k_2 + k_6) \cdot GAP \cdot S7P + k_5 k_8 (k_2 + k_3) \cdot R5P \cdot S7P + k_1 k_4 (k_6 + k_7) \cdot X5P \cdot GAP\right)}$$

[Eq. S18]

Table S17. Parameter values used in the Transketolase 1 rate expression

Symbol	Value	Units	Description	Reference	
E_{TK1}	adjusted	mM	Maximal concentration of TK1		
k_1	2.16×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)	
k_2	38.0	s ⁻¹	Rate constant	(7)	

<i>k</i> ₃	34.0	s ⁻¹	Rate constant	(7)
k_4	1.56×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₅	3.29×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_6	1.75×10 ²	s ⁻¹	Rate constant	(7)
k_7	40	s ⁻¹	Rate constant	(7)
k_8	44.8	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)

Transaldolase (TAL):

$$V_{TAL} = E_{TAL} \cdot \frac{\left(k_1 k_3 k_5 k_7 . GAP \cdot S7P - k_2 k_4 k_6 k_8 . E4P \cdot H6P\right)}{\left(k_1 k_3 (k_6 + k_7) . S7P + k_5 k_7 (k_2 + k_3) . GAP + k_2 k_4 (k_6 + k_7) E4P + k_6 k_8 (k_2 + k_3) H6P + k_1 k_5 (k_3 + k_7) . S7P . GAP + k_4 k_8 (k_2 + k_6) . E4P . H6P + k_5 k_8 (k_2 + k_3) . S7P . H6P + k_1 k_4 (k_6 + k_7) . GAP . E4P\right)}$$

[Eq. S19]

Table S18. Parameter values used in the transketolase 1 rate expression

Symbol	Value	Units	Description	Reference
E _{TAL}	adjusted	mМ	Maximal concentration of TAL	
k_1	2.16×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₂	4.53	s ⁻¹	Rate constant	(7)
<i>k</i> ₃	16.3	s ⁻¹	Rate constant	(7)
k_4	30.0	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_5	4.9×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₆	60.0	s ⁻¹	Rate constant	(7)
<i>k</i> ₇	17.0	s ⁻¹	Rate constant	(7)
k_8	79.0	$\mathrm{mM}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)

Transketolase 2 (TK2):

$$V_{TK2} = E_{TK2} \cdot \frac{\left(k_1 k_3 k_5 k_7 \cdot X5P \cdot E4P - k_2 k_4 k_6 k_8 \cdot GAP \cdot H6P\right)}{\left(k_1 k_3 (k_6 + k_7) \cdot X5P + k_5 k_7 (k_2 + k_3) \cdot E4P + k_2 k_4 (k_6 + k_7) \cdot GAP + k_6 k_8 (k_2 + k_3) \cdot H6P + k_1 k_5 (k_3 + k_7) \cdot X5P \cdot E4P + k_4 k_8 (k_2 + k_6) \cdot GAP \cdot H6P + k_5 k_8 (k_2 + k_3) \cdot X5P \cdot H6P + k_1 k_4 (k_6 + k_7) \cdot E4P \cdot GAP\right)}$$

[Eq. S20]

Table S19. Parameter values used in the Transketolase 2 rate expression

Symbol	Value	Units	Description	Reference
E _{TK2}	adjusted	mM	Maximal concentration of TK1	
k_1	21.6	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₂	3.8	s ⁻¹	Rate constant	(7)
<i>k</i> ₃	1.72×10 ²	s ⁻¹	Rate constant	(7)
k_4	1.57×10 ²	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
<i>k</i> ₅	2.24×10 ³	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)
k_6	1.75×10 ²	s ⁻¹	Rate constant	(7)
<i>k</i> ₇	40	s ⁻¹	Rate constant	(7)
<i>k</i> ₈	21.3	$\mathrm{m}\mathrm{M}^{-1}\mathrm{s}^{-1}$	Rate constant	(7)

S2.4 Polyol Pathway

Aldose Reductase (ALDR):

$$V_{ALDR} = E_{ALDR}. \frac{\left(k_{1}.NADPH.Glc_{i} - \frac{k_{2}.(C_{T}^{PyP} - NADPH).Sor}{K_{ALDR}^{eq}}\right)}{\left(k_{2}k_{ia}k_{b} + k_{2}k_{b}.NADPH + k_{2}k_{a}Glc_{i} + \frac{k_{1}k_{q}}{K_{eq}^{eq}}Sor + \frac{k_{1}k_{p}}{K_{ALDR}^{eq}}(C_{T}^{PyP} - NADPH)\right)}{\left(\dots + k_{2}.Glc_{i}.NADPH + \frac{k_{1}k_{q}}{k_{ia}K_{ALDR}^{eq}}Sor.(C_{T}^{PyP} - NADPH) + \frac{k_{2}k_{a}}{k_{iq}}.Glc_{i}.(C_{T}^{PyP} - NADPH)\right)}\right]$$
[Eq. S21]
$$\dots + \frac{k_{1}}{K_{ALDR}^{eq}}Sor.NADPH + \frac{k_{2}}{k_{ip}}.Glc_{i}.NADPH.Sor + \frac{k_{1}}{k_{ib}K_{ALDR}^{eq}}Glc_{i}.(C_{T}^{PyP} - NADPH).Sor\right)$$

$$V_{ALDR}^{eq} = \frac{k_1 k_p k_{iq}}{k_2 k_b k_{ia}}$$

Symbol	Value	Units	Description	Reference
E _{ALDR}	adjusted	mM	Maximal concentration of ALDR	
k_1	0.33	s ⁻¹	Rate constant	(8)
<i>k</i> ₂	0.037	s ⁻¹	Rate constant	(8)
k_a	6.9×10 ⁻⁴	mM	Michaelis constant for NADPH	(8)
k_{b}	46	mM	Michaelis constant for Glc	(8)
k_p	3.8×10 ²	mМ	Michaelis constant for Sor	(8)
k_q	1.5×10 ⁻²	mМ	Michaelis constant for NADP	(8)
k _{ia}	4.1×10 ⁻⁴	mM	Dissociation constant for NADPH	(8)
k_{ib}	9.2×10 ⁻²	mM	Dissociation constant for Glc	(8)
k_{ip}	1.3×10^{3}	mM	Dissociation constant for Sor	(8)
k_{iq}	8.3×10 ⁻³	mM	Dissociation constant for NADP	(8)

Table S20. Parameter values used in the Aldose reductase rate expression

Sorbitol Dehydrogenase (SoDH):

$$V_{SoDH} = V_{\max,f}^{SoDH} \frac{\left(C_{T}^{Pyr} - NADH\right) . Sor}{K_{iSoDH}^{NAD} . K_{MSoDH}^{Sor} + K_{MSoDH}^{Sor} \left(C_{T}^{Pyr} - NADH\right) + K_{MSoDH}^{NAD} . Sor + \left(C_{T}^{Pyr} - NADH\right) . Sor}$$

$$\dots - V_{\max,r}^{SoDH} \frac{NADH . Fru}{K_{iSoDH}^{NADH} . K_{MSoDH}^{Fru} + K_{MSoDH}^{Fru} . NADH + K_{MSoDH}^{NADH} . Fru + NADH . Fru}$$
[Eq. S22]

$$V_{\max,r}^{SoDH} = \frac{V_{\max,f}^{SoDH} K_{MSoDH}^{Fru} K_{MSoDH}^{NADH}}{K_{MSoDH}^{Sor} K_{MSoDH}^{NAD} K_{SoDH}^{eq}}$$

Symbol	Value	Units	Description	Reference
$V_{\max,f}^{SoDH}$	adjusted	mM s ⁻¹	Maximal concentration of SoDH	
$K_{{\scriptscriptstyle M}{\scriptscriptstyle SoDH}}^{{\scriptscriptstyle NADH}}$	1.0×10 ⁻²	mМ	Michaelis constant for NADH	(9)
$K_{\scriptscriptstyle MSoDH}^{\scriptscriptstyle Fru}$	1.0×10 ³	mM	Michaelis constant for Fru	(9)
$K_{\scriptscriptstyle MSoDH}^{ Sor}$	9.6	mM	Michaelis constant for Sor	(9)
$K_{M SoDH}^{NAD}$	2.0	mМ	Michaelis constant for NAD	(9)
K_{iSoDH}^{NADH}	1.0×10 ⁻²	mМ	Dissociation constant for NADH	(9)
K_{iSoDH}^{NAD}	2.0	mМ	Dissociation constant for NAD	(9)
$K^{\it eq}_{\it SoDH}$	9.25×10 ⁻²		Equilibrium constant	(9)

Table S21. Parameter values used in the Sorbitol dehydrogenase rate expression

Xylitol Dehydrogenase (XDH):

$$V_{XDH} = V_{\max,f}^{XDH} \frac{NADH . X5P}{K_{iXDH}^{NADH} . K_{MXDH}^{Xy} + K_{MXDH}^{Xy} . NADH + K_{MXDH}^{NADH} . X5P + NADH . X5P}$$

$$(Eq. S23]$$

$$\dots - V_{\max,r}^{XDH} \frac{(C_T^{Pyr} - NADH) . XyOH}{K_{iXDH}^{NAD} . K_{MXDH}^{NADH} + K_{MXDH}^{NyOH} . (C_T^{Pyr} - NADH) + K_{MXDH}^{NAD} . XyOH + (C_T^{Pyr} - NADH) . XyOH}$$

$$V_{\max,r}^{XDH} = \frac{V_{\max,f}^{XDH} K_{MXDH}^{XyOH} K_{MXDH}^{NAD}}{K_{MXDH}^{XyOH} K_{MXDH}^{NAD}} K_{XDH}^{NAD} K_{XDH}^{NAD} K_{XDH}^{NAD}}$$

Symbol	Value	Units	Description	Reference
$V_{\max,f}^{XDH}$	adjusted	mM s ⁻¹	Maximal concentration of XDH	
$K_{M XDH}^{NADH}$	1.0×10 ⁻²	mM	Michaelis constant for NADH	(9)
K _{M XDH}	8.08×10 ⁻¹	mM	Michaelis constant for XyOH	(10)

$K_{M XDH}^{Xy}$	20.0	mM	Michaelis constant for X5P	(10)
$K_{M XDH}^{NAD}$	2.0	mM	Michaelis constant for NAD	(9)
K_{iXDH}^{NADH}	1.0×10 ⁻²	mM	Dissociation constant for NADH	(9)
K_{iXDH}^{NAD}	2.0	mM	Dissociation constant for NAD	(9)
K^{eq}_{XDH}	0.24		Equilibrium constant	(9)

S2.5 ATPase, non-glycolytic NADH consumption, NADPH consumption, polyol transport

The rate expressions corresponding to NADH, NADPH and ATP consumption as well as polyol transport have been added to the present computational model to enable steady state behavior. Standard hyperbolic relations were assumed for each of the rate expressions.

$$V_{ATPase} = V_{max}^{ATPase} = \frac{\frac{ATP}{K_{MATPase}^{ATP}}}{1 + \frac{ATP}{K_{MATPase}^{ATP}}}$$
[Eq. S24]
$$V_{NADHc} = V_{max}^{NADHc} = \frac{\frac{NADH}{K_{MADHc}^{NADH}} - \frac{(C_T^{Pyr} - NADH)}{K_{MADHc}^{NADHc}}}{1 + \frac{NADH}{K_{MADHc}^{NADH}} + \frac{(C_T^{Pyr} - NADH)}{K_{MADHc}^{NADH}}}$$
[Eq. S25]
$$V_{NADPHc} = V_{max}^{NADPHc} \cdot \frac{\frac{NADPH}{K_{MADHc}^{NADH}} - \frac{(C_T^{Pyr} - NADPH)}{K_{MADHc}^{NADH}}}{1 + \frac{NADPH}{K_{MADHc}^{NADH}} + \frac{(C_T^{Pyr} - NADPH)}{K_{MADHc}^{NADH}}}$$
[Eq. S26]
$$V_{NADPHc} = k_{FuT} \frac{Fru}{K_{FuT}^{FuT} + Fru}$$
[Eq. S27]
$$V_{rourr} = k_{wourr} \frac{XyOH}{X_{WOH}^{NADH}}$$
[Eq. S28]

$$V_{XyOHT} = k_{XyOHT} \frac{XyOH}{K_{XyOHT}^{XyOH} + XyOH}$$
[Eq. S2

 Table S23. Parameter values

	Symbol	Value	Units	Description
-	V_{\max}^{ATPase}	adjusted	mM s ⁻¹	Maximal Rate of ATPase
	K_{MATP}^{ATP}	9.0	mM	Michaelis constant for ATP
	V_{\max}^{NADHc}	Adjusted	mM s ⁻¹	Maximal rate of NADH consumption
	$K_{_{MNADHc}}^{_{NADH}}$	0.05	mM	Michaelis constant for NADH
	$K_{_{MNADHc}}^{_{NAD}}$	0.7	mM	Michaelis constant for NAD
	$V_{\rm max}^{\it NADPHc}$	Adjusted	mM s ⁻¹	Maximal rate of NADPH consumption
	$K_{_{MNADPHc}}^{_{NADPH}}$	2.5×10 ⁻²	mM	Michaelis constant for NADPH
	$K_{M NADP hc}^{NADP}$	7.5×10 ⁻³	mM	Michaelis constant for NADP
	k _{FruT}	Adjusted	mM s ⁻¹	Rate constant of Fru transport
	K_{FruT}^{Fru}	3.0	mM	Michaelis constant for Fru
	k _{xyOHT}	Adjusted	mM s ⁻¹	Rate constant of XyOH transport
	$K_{_{XyOHT}}^{_{XyOH}}$	1.5	mM	Michaelis constant for XyOH

Table S24. Selected V_{max} values obtained with different optimization criteria

V _{max}	(I) ^a	(II)	(III)	(IV)
$k_{\scriptscriptstyle T}^{\scriptscriptstyle Glc}$	0.00084 ^{b, c}	0.00308	0.00184	1.00
V_{\max}^{HK}	0.0387	0.0571	0.00	0.0596
$V_{\max, f}^{PFK}$	0.00452	4.9×10^{-7}	0.00322	0.00
$V_{\max,(f)(r)}^{GAPD}$	0.00792	0.00792	0.0197	0.00792

$V_{\max,(f)(r)}^{PGK}$	0.0622	0.675	0.0622	0.0622
$V_{ m max}^{G6PD}$	0.00	0.0512	0.00	0.0512
E _{ALDR}	0.00	0.0626	0.0626	0.0626
$V_{\max,f}^{XDH}$	0.234	0.764	1.00	0.764
$V^{Gno_is}_{ m max}$	0.00137	0.0195	0.0032	0.019

^a Optimization criteria: (I) Minimization of ATP and NADPH generation; (II) Maximization of ATP generation; (III) Maximization of NADH generation; (IV) Maximization of Pentose Phosphate flux.

Objective functions follow the general form: minimize $Z = \sum ci \times Vi$, max, where Z is the objective function and *ci* (weighing coefficient) can be one or zero for each *i* reaction in the network according to the optimization criterion. For maximization purposes, the minimization of the negative of Z is performed.

^b Vmax values are expressed in mM s⁻¹ units, or mM in case of E_{ALDR} or s⁻¹ in case of k_T^{Glc}

^c Vmax correspond to the maximal values in the volume of solutions, i.e. these values delimit the coordinates of the vertices of the volume of solutions obtained with each objective function (see Fig.S1 below for illustration).

Section S3. Maximal relative error associated with the calculation of V_{max}

A source of error associated with the estimation of the fluxes according to the present procedure is given by the variability in the experimental determination of metabolites concentration. This source of error will affect the matrix that contains the derivatives of rate expressions with respect to V_{max} . Equation 1 from the main text can be rewritten as

$$S_t \cdot \mathbf{D}_r \mathbf{V} \cdot V_{max} = b_t$$
 [Eq. S29]

Being S_t a square matrix obtained by appending the stoichiometric matrix S with a matrix of size $p \times m$, where p=m-n, and contains 1 and 0. Obtaining a non-singular square matrix is required in order to be able to invert it. b_t the vector of transport and demand processes, e.g. biosynthesis, is also appended with a vector containing p elements that correspond to the measured flux rates. $\mathbf{D_rV}$ is the diagonal matrix of the derivatives of the rate expressions with respect to the V_{max} of each rate.

In addition to variability in the experimental values of the transport or demand processes taken into account in vector b_t , sources of variability in the determination of metabolites or in parameter values in each rate expression, such as the affinities of enzymes for their respective substrates, or effectors are reflected by the variability of D_rV .

$$S_t \cdot \Delta \mathbf{D}_r \mathbf{V} \, \Delta V_{max} = \Delta b_t \qquad [Eq. \, S30]$$

Following the treatment in (11), the matrix norm can be obtained:

$$\| S_t \| . \| \mathbf{D}_r \mathbf{V} \| . \| V_{max} \| \le \| b_t \|$$
 [Eq. S31]

which can be rearranged as

$$\|\Delta V_{max}\| \le \|\mathbf{S}_{t}^{-1}\| \cdot \|\Delta \mathbf{D}_{t}\mathbf{V}^{-1}\| \cdot \|\Delta b_{t}\| \qquad [Eq. S32]$$

Equations S31 and S32 lead to an expression for the maximum relative error in the determination of V_{max} as follows:

$$\frac{\left\|\Delta V_{\max}\right\|}{\left\|V_{\max}\right\|} \leq \frac{\left\|S_{t}^{-1}\right\|}{\left\|S_{t}\right\|} \cdot \frac{\left\|\Delta D_{r}V^{-1}\right\|}{\left\|D_{r}V^{-1}\right\|} \cdot \frac{\left\|\Delta b_{t}\right\|}{\left\|b_{t}\right\|}$$
[Eq. S33]

Section S4. Estimation of the error associated with the computed V_{max} values due to variability in metabolites concentration

For the present work we estimated the error arising from variability in the concentration of metabolites. The results were obtained by computing the values of the V_{max} that would be obtained if all the metabolites values were $S_{av} - \Delta S$, or $S_{av} + \Delta S$, with S_{av} being the experimentally determined mean concentration value informed in Table 1 and ΔS the standard error. The V_{max} at both extremes ($S_{av} - \Delta S$ and $S_{av} + \Delta s$) was calculated, and the largest value of $\Delta V_{max} = V_{max} (S_{av}) - V_{max} (S_{av} - \Delta s)$ or $= V_{max} (S_{av}) - V_{max} (S_{av} + \Delta s)$. Since different values of ΔV_{max} were obtained at both extremes, the value informed in Table S25 corresponds to the largest ΔV_{max} estimated.

V _{max}	V_{max}	$\Delta V_{max}/V_{max}{}^a$
$k_{\scriptscriptstyle T}^{\scriptscriptstyle Glc}$	0.00308	0.58
V_{\max}^{HK}	0.0571	0.82
$V_{\max, \mathrm{f}}^{PFK}$	4.9×10^{-7}	0.13
$V_{\max,(f)(r)}^{GAPD}$	0.00792	0.0072
V ^{PGK} _{max,(f)(r)}	0.675	0.0067
V_{\max}^{G6PD}	0.0512	0.091
E_{ALDR}	0.0626	0.46
$V_{\max,f}^{XDH}$	0.764	0.28
$V^{Gno_is}_{ m max}$	0.0195	0.28

Table S25. Estimated relative error in V_{max} values

 ${}^{a}\Delta V_{max}/V_{max}$, where V_{max} corresponds to calculated V_{max} at the Sav, and ΔV_{max} is the largest value calculated at both extremes.

Section S5. Matrixes used in the optimization of V_{max} values and Control Analysis (see Sections 2.2 - 2.4 from *Modeling and Experimental Methods* in the main text for further explanation).

Stoichiometry matrix (for internal metabolites):

Stoichiometry matrix (for external metabolites):

Elasticity matrix:

$\left[\frac{\partial V_T^G}{\partial GL}\right]$		0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0]
$\frac{\partial V_{HI}}{\partial Glo}$	ті <u>К</u>	$\frac{\partial V_{HK}}{\partial H6P}$		0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{HK}}{\partial ATP}$	0	0	-	$\frac{\partial V_{HK}}{\partial ADP}$	C) ()	0	0	
0	$\frac{\partial V_{I}}{\partial H}$	$\frac{PFK}{6P}$	$\frac{\partial V_{PI}}{\partial FB}$	$\frac{\overline{K}}{P}$	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{PFK}}{\partial ATP}$	0	C)	$\frac{\partial V_{PFK}}{\partial ADP}$. () ()	0	0	
0	0	$\frac{\partial V_{Al}}{\partial FP}$		$\frac{\partial V_{\lambda}}{\partial G}$	AD	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0 ()	0	0	0	0	0			
0	0	0	$\frac{\partial V_{G}}{\partial G}$	APD AP	$\frac{\partial V_0}{\partial B}$	GAPD PG	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{GA}}{\partial NAI}$		0	0	<u> </u>	V _{gapd} NAD	0)	0	0
0	0	0	0	$\frac{\partial V}{\partial B}$	PGK BPG	$\frac{\partial V_p}{\partial 3H}$	P <u>GK</u>	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{PGK}}{\partial ATP}$	0	()	$\frac{\partial V_{PGK}}{\partial ADP}$	- (0 0	0	0	0	
0	0	0	0	0	$\frac{\partial V}{\partial 3}$, _{Enol} PG	$\frac{\partial V_{En}}{\partial PE}$	$\frac{nol}{P}$	0	0	0	0	0	0	0	0	0	0	0) ()	0	0	0	0	0			
0	0	0	0	0	0	$\frac{\partial V}{\partial P}$	$\frac{V_{PK}}{EP}$	$\frac{\partial V_{PK}}{\partial Pv}$	_	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{PK}}{\partial ATP}$	0	0	$\frac{\partial}{\partial z}$	$\frac{\partial V_{PK}}{ADP}$	0	0	()	0	
0	0	0	0	0	0	0	$\frac{\partial V_I}{\partial F}$	<u></u> У	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{II}}{\partial NAI}$	он ОН	0	0	$\frac{\partial V}{\partial N}$	_{LDH} AD	0	0	0		
0	0	0	0	0	0	0	$\frac{\partial V_{I}}{\partial P}$	$\frac{Py}{r}$	0	0	0	0	0	0	0	0	0	0	0	0 ()	0	0	0	0				
0	$\frac{\partial V_{\alpha}}{\partial H}$	6PD	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial A}$, <u>G6PD</u> 1TP	0	$\frac{\partial V}{\partial NA}$, _{G6PD} IDPH	, ()	0	∂V _{Ge} ∂NA	DP	0	0
0	0	0	0	0	0	0	0	$\frac{\partial V_6}{\partial 6}$	<u>pgo</u> PG	$\frac{\partial V}{\partial R}$	Capago Ru5P	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial NA}$, 6PGO DPH	- ()	0	$\frac{\partial V_{6F}}{\partial NA}$	DP	0	0
0	0	0	0	0	0	0	0	$\frac{\partial V_i}{\partial R_i}$	_{к5РІ} 15Р	$\frac{\partial V}{\partial I}$	$\frac{V_{R5PI}}{R5P}$	0	0	0	0	0	0	0	0	0	0	0	0	0	0				
0	0	0	0	0	0	0	0	$\frac{\partial V_{R}}{\partial R}$	u <u>5PE</u> u5P	0	$\frac{\partial}{\partial t}$	V_{Ru5PE}	0	0	0) () 0	0	0	0	0	0	0	0	0				
0	0	0	$\frac{\partial V_{j}}{\partial G_{i}}$	$\frac{K1}{4P}$	0	0	0	0	0	0	$\frac{\partial V}{\partial R}$	<u>ткі</u> 5Р	$\frac{\partial V_{T}}{\partial X5}$	$\frac{1}{P}$	$\frac{\partial V_{TK}}{\partial S7}$	<u>1</u> P	0 0) () 0	0	0	0	0	0	0		0	0	
0	$\frac{\partial V_{i}}{\partial H}$	<u>тк2</u> 6Р	0	$\frac{\partial V}{\partial G}$	$\frac{TK2}{AP}$	0	0	0	0	0	0	0	$\frac{\partial V_{I}}{\partial X}$	$\frac{K2}{5P}$	0	$\frac{\partial V_T}{\partial E^4}$	P	0	0 0	0	0	() () (0	0	0	0	
0	$\frac{\partial V}{\partial H}$	<u>TAL</u> 6P	0	$\frac{\partial V}{\partial G}$	TAL AP	0	0	0	0	0	0	0	0	$\frac{\partial V_{\eta}}{\partial S_{\eta}}$	$\frac{ML}{P}$	$\frac{\partial V_T}{\partial E4}$	$\frac{\mu}{P}$	0	0 0	0	0	0	0	() ()	0	0	
$\frac{\partial V_{Al}}{\partial Gl}$	lc_i	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial}{\partial t}$	V _{ALDR} Sor	0	0	0	0	$\frac{\partial V}{\partial NA}$, _{ALDR} DPH	- 0) (0 -	∂V _{AL} ∂NAI	DP	0	0
0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial t}$	Sor	$\frac{\partial \tilde{c}}{\partial t}$	V _{soDH} Fru	0	0	$rac{\partial V_{So}}{\partial NAI}$	DH DH	0	0	<u> 16</u>	V _{sodh} NAD	0) (0	0
0	0	0	0	0	0	0	0	0	0	0	<u>16</u> 0.	$\frac{V_{XyDH}}{X5P}$	0	0	0	0	$\frac{\partial V}{\partial X}$	yoh YyOH	0	$\frac{\partial V_{j}}{\partial NA}$	_{KyDH} IDH	0	0		9V _{xydh} 9NAD		0	0	0
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial}{\partial}$	V ^{Fru} FruT	0	0	0	0	0	0	0	0	0				
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial}{\partial z}$	$\frac{V_{XyOH}^{XyOH}}{XyOH}$	0	0	0	0	0	0	0	0				
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial t}$, ATPase ATP	0	0	0	0	0	0	0				
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial N}$	∕ _{NADH₀} IADH	0	0	$\frac{\partial I}{\partial t}$	V _{NADHo} NAD	0	0 0)	0		
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_{N}}{\partial NA}$	DPH	0	() -	∂V _{nadi} ∂NAL	<u>PHo</u> DP	0	0		
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_G}{\partial M}$	al	$\frac{\partial V_{GI}}{\partial G1}$	$\frac{P_a}{P}$			
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V_G}{\partial M}$	al	$\frac{\partial V_{GI}}{\partial G1}$	$\frac{P_b}{P}$			
0	$\frac{\partial V_{\mu}}{\partial H}$	^{PGLM}	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	$\frac{\partial V}{\partial C}$, _{pglm} 31P			
0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0					



Figure S1. Space solution of a hypothetical metabolic network

Because in the network shown in the left panel there are 3 fluxes and only 1 metabolite, the solution space is 2-dimensional thus corresponding to a surface of solutions. According to the procedure described in Methods, section 2.3 of the main text, the solution chosen fulfils two conditions: *(i)* Vmax>0 for all enzymes in the network; and *(ii)* belongs to the solution space, more precisely, to the vertices (right panel, thick white arrows). Adapted from Price et al. (1)

Section S6. Sample Preparation and Metabolic Profiling

The non-targeted metabolic profiling platform employed for this analysis combined three independent platforms: ultrahigh performance liquid chromatography/tandem mass spectrometry (UHPLC/MS/MS) optimized for basic species. UHPLC/MS/MS optimized for acidic species. and gas chromatography/mass spectrometry (GC/MS). Samples were processed essentially as described previously (12, 13). For each sample, an equivalent amount of heart tissue was used for analysis. Using an automated liquid handler (Hamilton LabStar, Salt Lake City, UT), protein was precipitated with methanol that contained four standards to report on extraction efficiency. The resulting supernatant was split into equal aliquots for analysis on the three platforms. Aliquots, dried under nitrogen and vacuumdesiccated, were subsequently either reconstituted in 50µL 0.1% formic acid in water (acidic conditions) or in 50µL 6.5mM ammonium bicarbonate in water, pH 8 (basic conditions) for the two UHPLC/MS/MS analyses or derivatized to a final volume of 50µL for GC/MS analysis using equal parts bistrimethyl-silyl-trifluoroacetamide and solvent mixture acetonitrile:dichloromethane:cyclohexane (5:4:1) with 5% triethylamine at 60°C for one hour. In addition, three types of controls were analyzed in concert with the experimental samples: aliquots of a "client matrix" formed by pooling a small amount of each sample served as technical replicates throughout the data set, extracted water samples served as process blanks, and a cocktail of standards spiked into every analyzed sample allowed instrument performance monitoring. Experimental samples and controls were randomized across one platform run day.

For UHLC/MS/MS analysis, aliquots were separated using a Waters Acquity UPLC (Waters, Millford, MA) and analyzed using an LTQ mass spectrometer (Thermo Fisher Scientific, Inc., Waltham, MA) which consisted of an electrospray ionization (ESI) source and linear ion-trap (LIT) mass analyzer. The MS instrument scanned 99-1000 m/z and alternated between MS and MS² scans using dynamic exclusion with approximately 6 scans per second. Derivatized samples for GC/MS were separated on a 5% phenyldimethyl silicone column with helium as the carrier gas and a temperature ramp from 60°C to 340°C and then analyzed on a Thermo-Finnigan Trace DSQ MS (Thermo Fisher Scientific, Inc.) operated at unit mass resolving power with electron impact ionization and a 50-750 atomic mass unit scan range.

Metabolites were identified by automated comparison of the ion features in the experimental samples to a reference library of chemical standard entries that included retention time, molecular weight (m/z), preferred adducts, and in-source fragments as well as associated MS spectra, and were curated by visual inspection for quality control using software developed at Metabolon (14).

For statistical analyses and data display purposes, any missing values were assumed to be below the limit of detection and these values were imputed with the compound minimum (minimum value imputation). Statistical analysis of log-transformed data was performed using "R" (http://cran.r-project.org/), which is a freely available, open-source software package. A two-way ANOVA is used to identify biochemicals that differ significantly between experimental groups. *P*-values ≤ 0.05 are considered statistically significant and *p*-values < 0.10 are reported as trends. Multiple comparisons are accounted for by estimating the false discovery rate (FDR) using q-values (15).

Supporting References

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