Supplementary Information

for

A Multiplexed Device Based on Tunable *Nanoshearing* for Specific Detection of Multiple Protein Biomarkers in Serum

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Supplementary Figure S1 | Design of multiplexed microfluidic device. Schematic of layout editor design of a multiplexed microfluidic device. The device was designed to contain three individual microfluidic channels with inlets and outlet reservoirs.



Supplementary Figure S2 | Fabrication of devices. Schematic illustration of device fabrication. The multiplexed microfluidic device contains an array of the asymmetric electrode pairs within three individual microfluidic channels.



Supplementary Figure S3 | Protein detection using *nanoshearing* **device.** (a) UV-Vis absorbance spectra for serum samples spiked with (black; 100 pg mL⁻¹) and without (blue) HER2 under ac-EHD field strength of f = 1 kHz, $V_{pp} = 100$ mV. (b,c) Representative fluorescence images of the (b) detected protein (intensity: 1.73×10^6 (counts)) and (c) nonspecifically bound detection antibody (intensity: 1.08×10^3 (counts)) under ac-EHD induced fluid flow conditions. Scale bar is 100 µm.



Supplementary Figure S4 | Specificity of protein capture and detection. (a, b) UV-Vis absorbance spectra of HER2 (100 pg mL⁻¹) spiked in serum driven through the devices (a) with (black) and without (red) anti-HER2 capture antibody, and (b) with (black) and without (green) FITC anti-HER2 detection antibody, under ac-EHD field strength of f = 1 kHz, $V_{pp} = 100$ mV. (c) UV-Vis absorbance spectra of device incubated with FITC anti-HER2 detection antibody and target protein.



Supplementary Figure S5 | Protein detection under ac-EHD flow vs hydrodynamic flow. (a-c) UV-Vis absorbance spectra of the detected HER2 protein spiked in human serum at concentration of (a) 1 ng mL⁻¹, (b) 100 pg mL⁻¹ and (c) 1 pg mL⁻¹, respectively under ac-EHD (f = 1 kHz, $V_{pp} = 100$ mV; black) and pressure driven flow (control; red) conditions. Pressure driven flow based devices operated under the rate of 8 µLmin⁻¹ (an equivalent flow rate of that calculated based on the time required to flow 1 mL of serum sample under the given ac-EHD field). Inset shows naked eye detection of the detected HER2 protein under ac-EHD and pressure driven flow conditions. (d) Absorbance peak at 652 nm (A_{652nm}) for HER2 (1 ng mL⁻¹ to 10 fg mL⁻¹) spiked in serum under ac-EHD (f = 1 kHz, $V_{pp} = 100$ mV; black) and pressure driven flow (control; red) conditions. Pressure driven flow based devices operated under the rate of 8 µLmin⁻¹ to 10 fg mL⁻¹ of a equivalent flow rate of that calculated based on the time required to flow rate of that calculated based on the time required to flow rate of that calculated based devices operated under the rate of 8 µLmin⁻¹ (an equivalent flow rate of that calculated based devices operated under the rate of 8 µLmin⁻¹ (an equivalent flow rate of that calculated based on the time required to flow 1 mL of serum sample under the given ac-EHD field). Each data point represents the average of three separate trials (n = 3) and error bars represent standard error of measurements within each experiment.



Supplementary Figure S6 | Specificity of immunocapture. UV-Vis absorption spectra of serum samples spiked with (red; 100 fg mL⁻¹) and without (black) target HER2 protein along with nonspecific PSA and IgG proteins (1 ng mL⁻¹ for both cases) on anti-HER2 functionalized device. The level of background response (nonspecific adsorption of detection antibody; blue) was obtained using serum (without any specific or nonspecific proteins) on the anti-HER2 functionalized device. Data presented was obtained under the ac-EHD field strength of f = 1 kHz at $V_{pp} = 100$ mV.