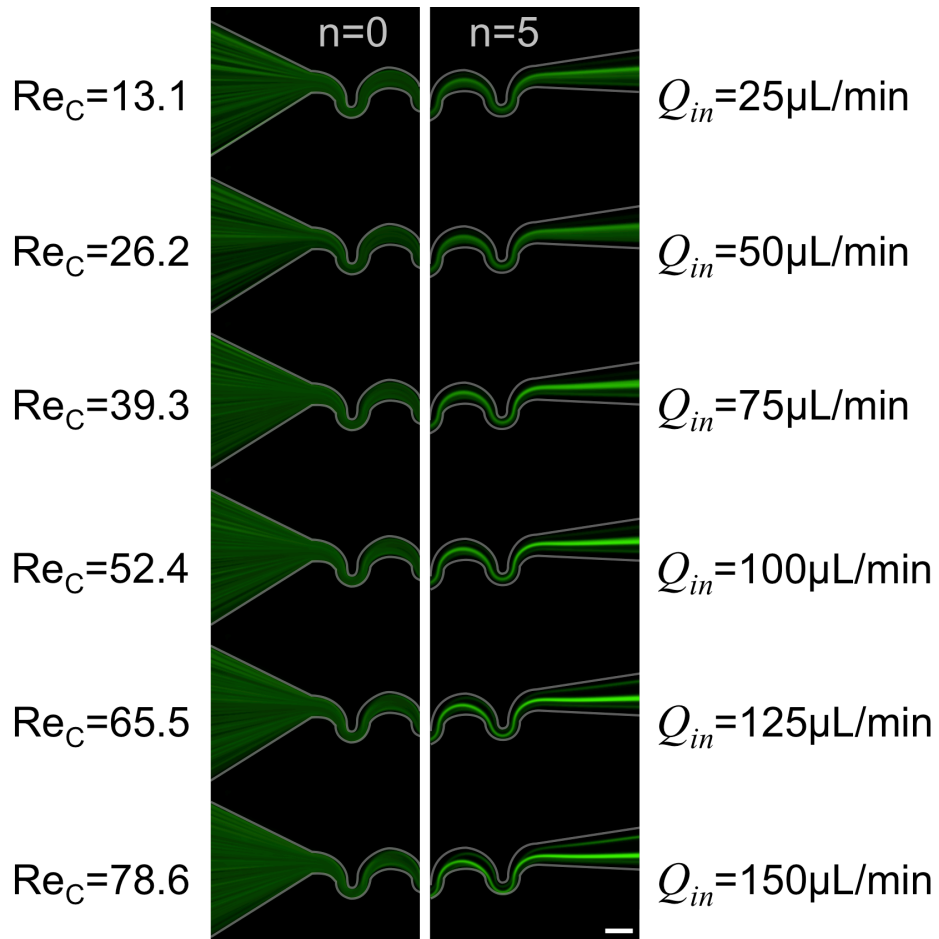


Continuous Flow Microfluidic Bioparticle Concentrator

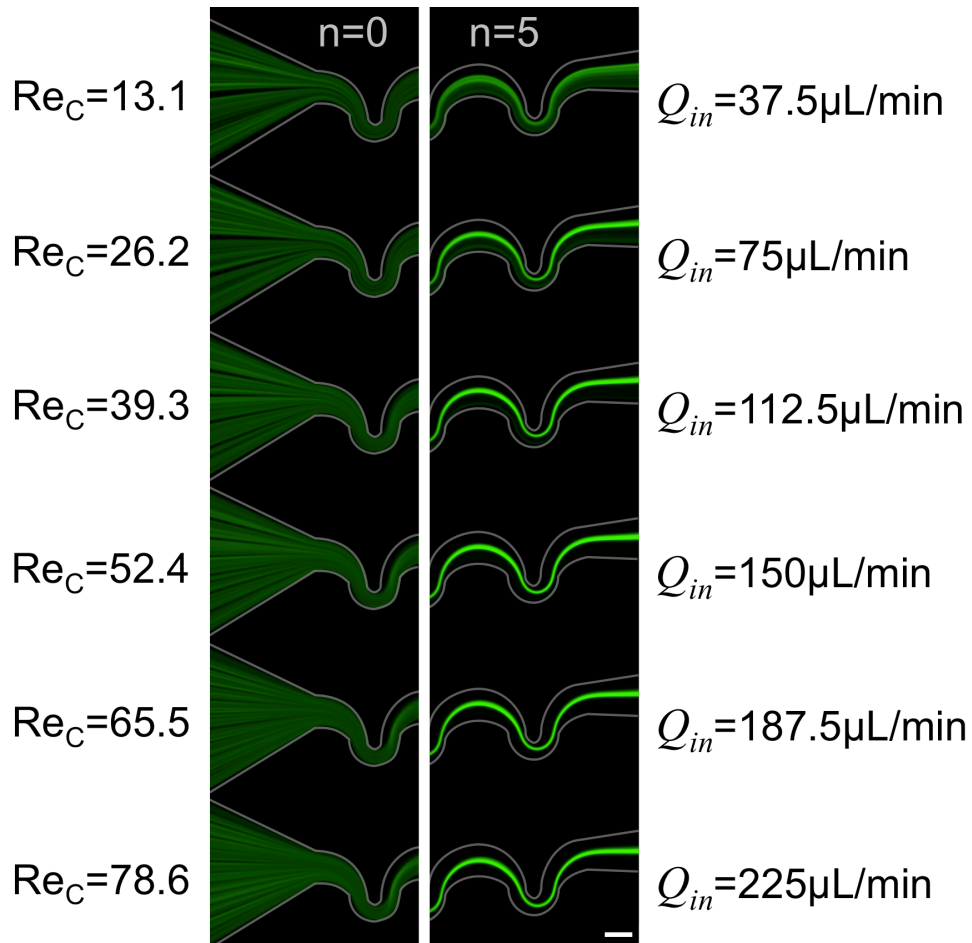
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SUPPLEMENTARY MATERIALS

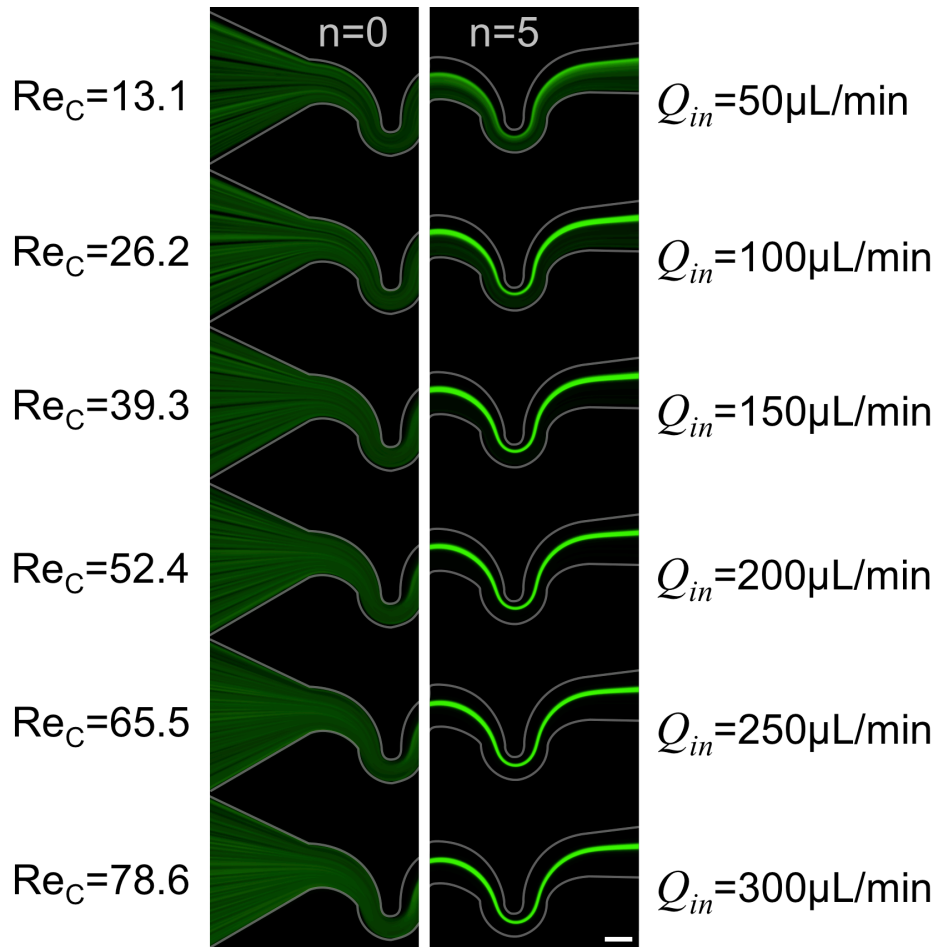
The following 6 figures are from the reference devices of 5 units of different focusing channel widths. Each is run at several flow rates, Q_{in} , to achieve equivalent channel Reynolds numbers, Re_C , in the different width channels. Re_C is defined here as $Re_C = 3\rho U_{Avg} D_h / 2\mu$, where ρ is the fluid density, U_{Avg} is the average velocity of the fluid, D_h is the hydraulic diameter of the focusing channel ($D_h = 2 * \text{height} * \text{width} / (\text{height} + \text{width})$) and μ is the dynamic viscosity of the fluid.



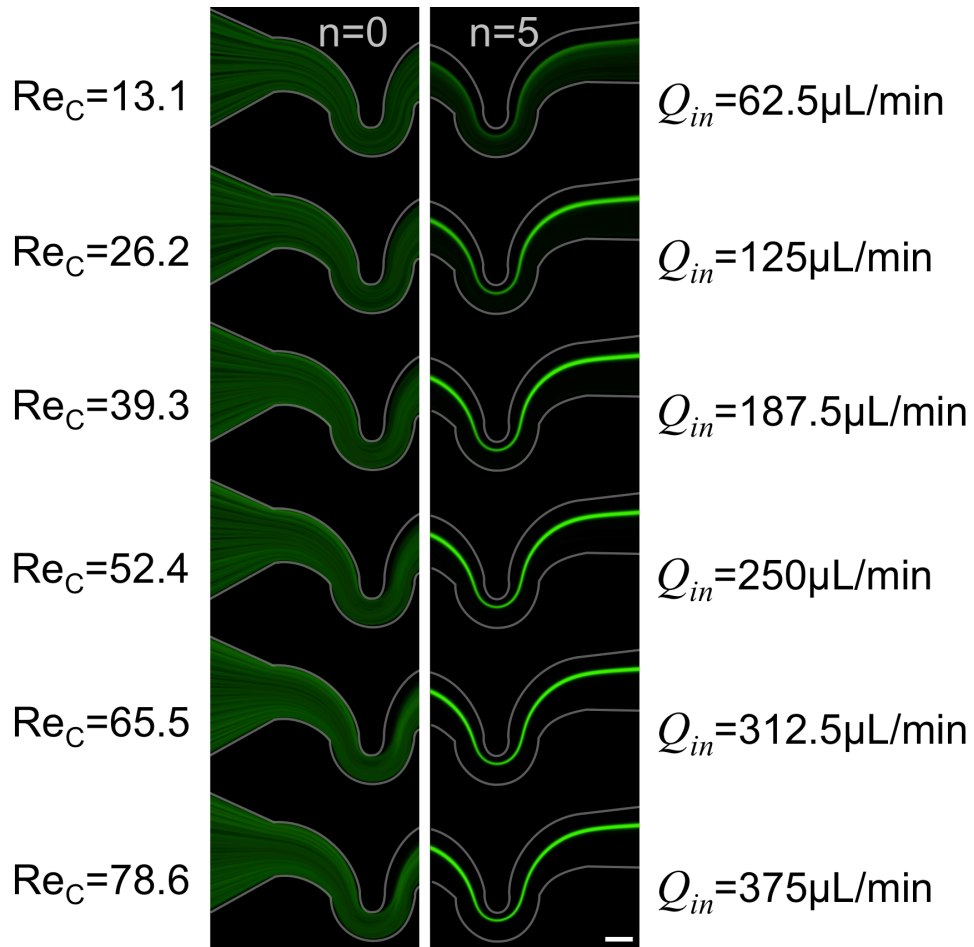
Supplementary Figure 1: Reference images using 9.9µm fluorescent beads for 50µm wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is 100µm.



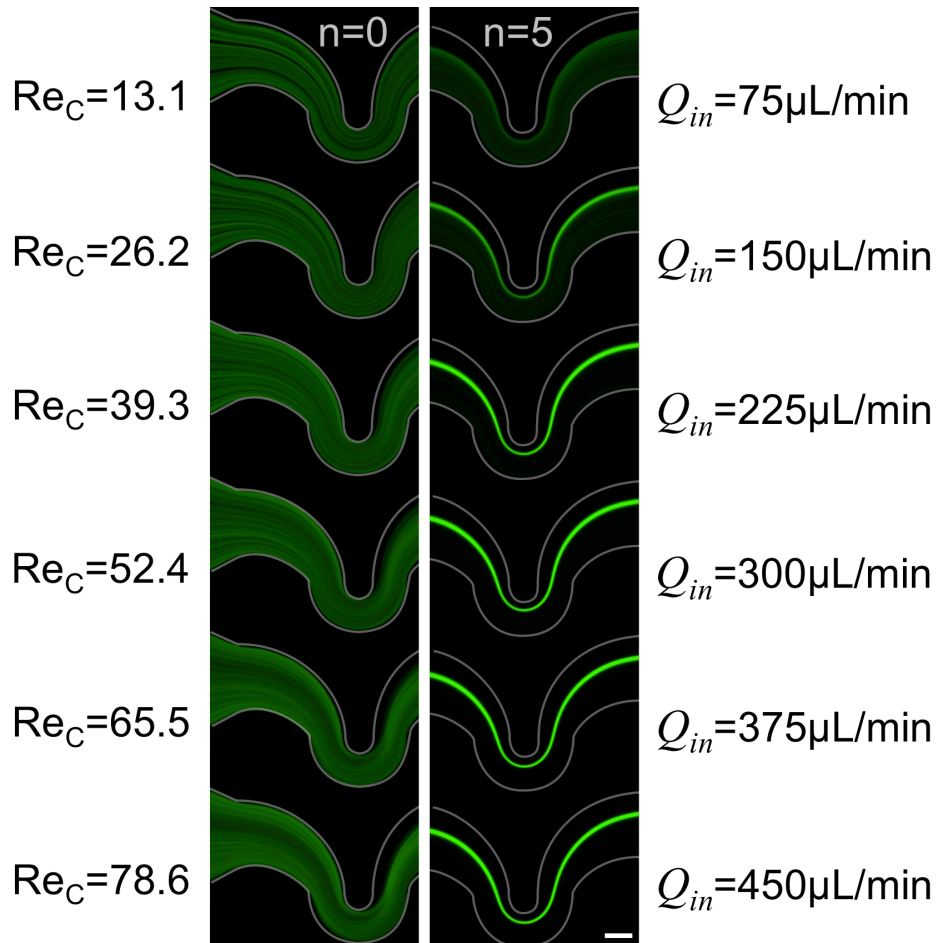
Supplementary Figure 2: Reference images using 9.9 μm fluorescent beads for 75 μm wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is 100 μm .



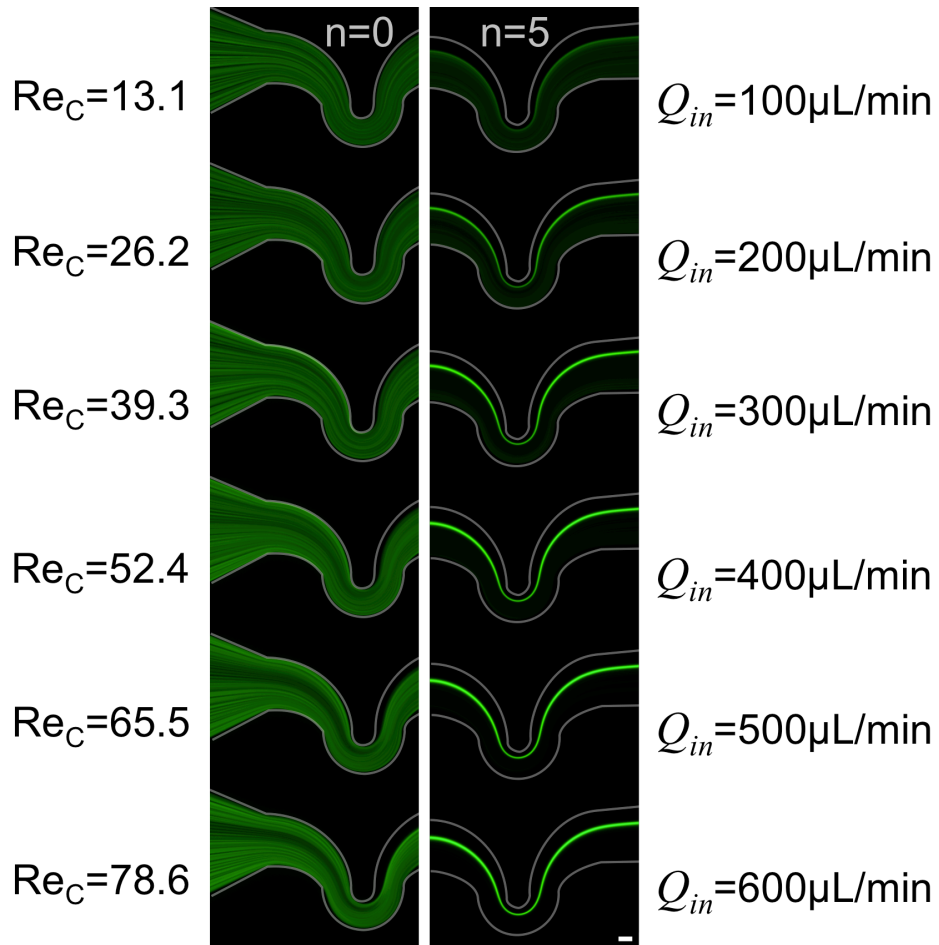
Supplementary Figure 3: Reference images using 9.9 μm fluorescent beads for 100 μm wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is 100 μm .



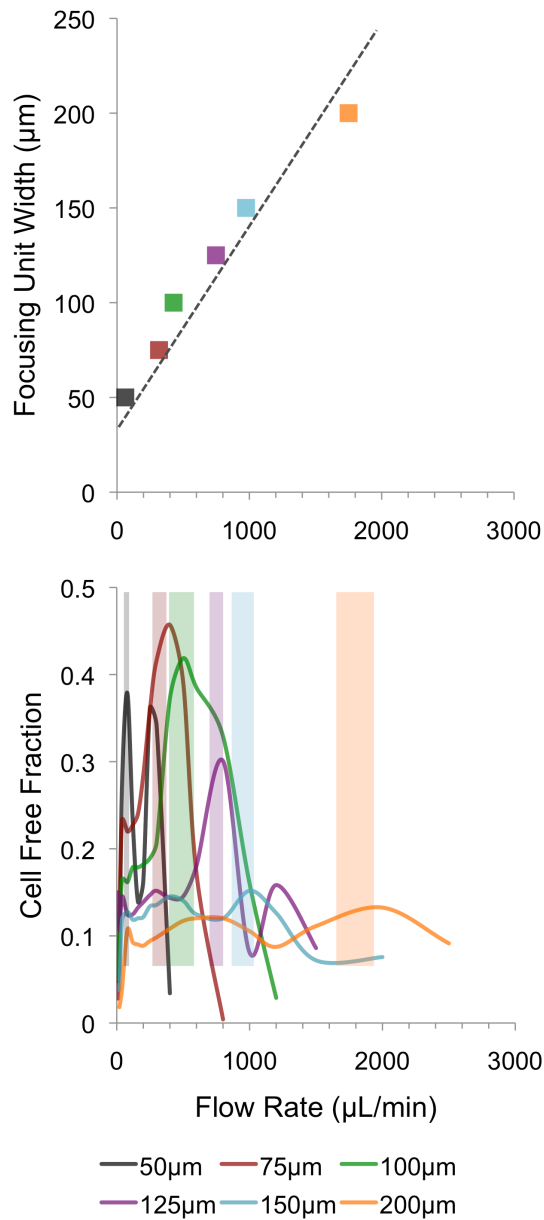
Supplementary Figure 4: Reference images using 9.9 μm fluorescent beads for 125 μm wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is 100 μm .



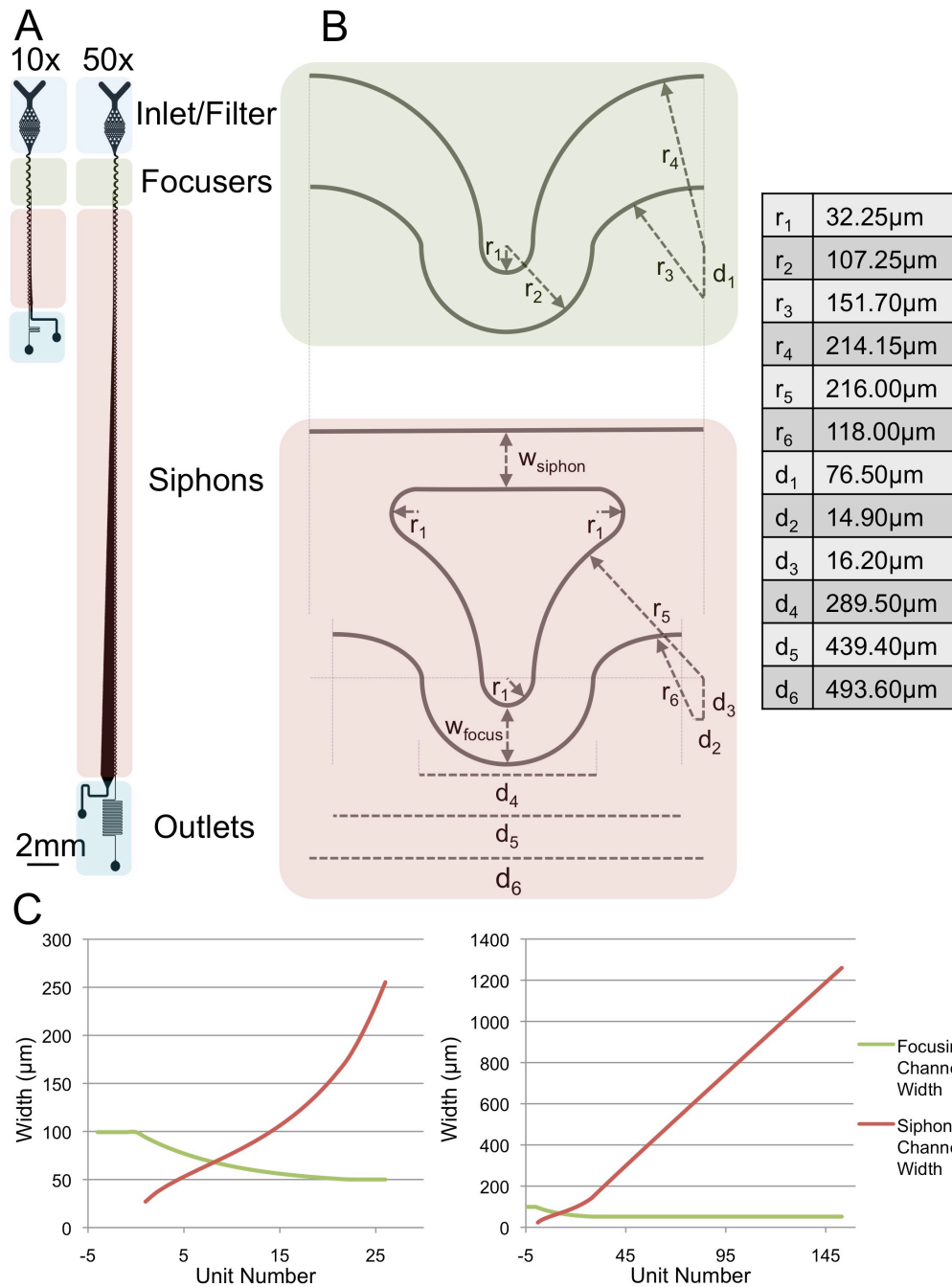
Supplementary Figure 5: Reference images using $9.9\mu\text{m}$ fluorescent beads for $150\mu\text{m}$ wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is $100\mu\text{m}$.



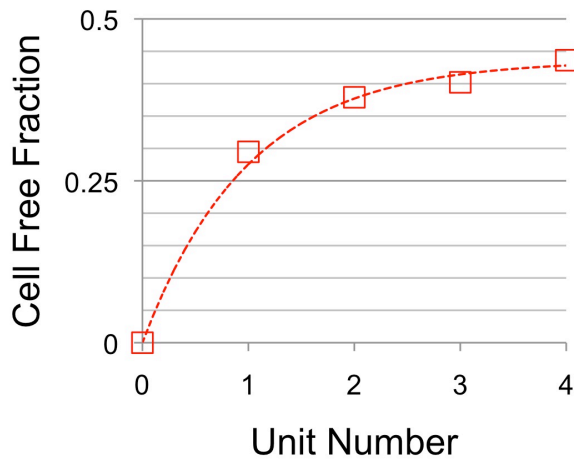
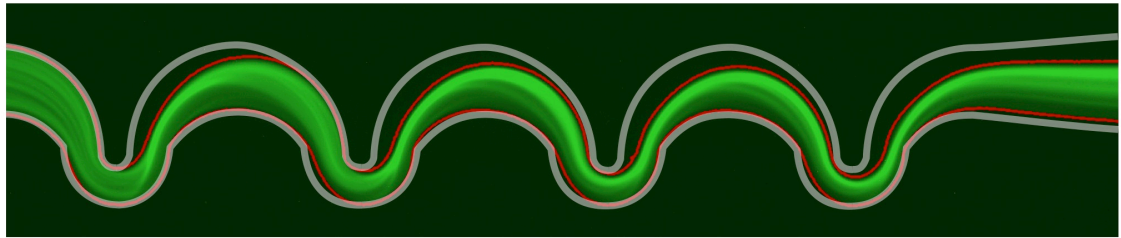
Supplementary Figure 6: Reference images using 9.9 μm fluorescent beads for 200 μm wide asymmetrically curved focusing channels. Images are taken at the beginning (left) and end (right) of the 5 focusing units at increasing flow rates from the top to bottom row. Scale bar is 100 μm .



Supplementary Figure 7: (Top) Plot of optimal flow rate versus focusing channel width, defined as the flow rate at which the cell free layer is maximized in the reference devices. Data is collected using fluorescently labeled buffy coat diluted to 1M cells/mL of 1% F68 in 1X PBS buffer. (Bottom) Related reference data showing the cell free fraction relationship with the focusing channel width across different ranges of flow rates.



Supplementary Figure 8: (A) Schematics of the 10x and 50x volume reduction devices. (B) Dimensions of the two main units that are then scaled by the focusing channel width, w_{focus} : focusing channel without a siphon channel (top) and with a siphon channel bottom as well as the key dimensions. (C) The width of the focusing channel and side channel along each device given by unit for the 10x device (left) and 50x device (right). The channel depth is $52 \pm 2 \mu\text{m}$.

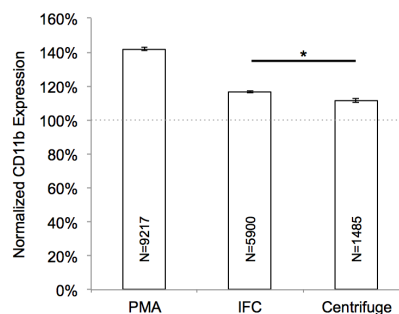


Supplementary Figure 9: Image of the cell free layer formation in a 100µm wide focusing channel across four focusing units. The red outline shows the 10% intensity threshold cutoff for determining the width of the particle distribution.

Supplementary Figure 10: (Movie) High-speed imaging results of the operation of the 10x volume reduction device at an input concentration of 5M white blood cells per mL at a flow rate of 500µL/min. Notice that near the outlet cells begin to be lost as the particles become too crowded within the focusing channels.

Supplementary Figure 11: (Movie) High-speed imaging results of the operation of the 50x volume reduction device at an input concentration of 5M white blood cells per mL at a flow rate of 500µL/min. Notice that near the outlet cells begin to be lost as the particles become too crowded within the focusing channels and the relative velocity of the cells within the focusing channel is noticeably different from those which are within the siphon channel likely indicating a different in effective viscosity due to particle volume fraction.

Leukocyte Activation Measurement: Relative activation of leukocytes was measured using imaging flow cytometry (Amnis Image Stream X) quantifying the CD11b expression of white blood cells exposed to different processing conditions. After concentration/exposure each sample was stained for 30 minutes with CD11b (AF388 Stemcell Technologies 60040AD – 2 μ L added to 400 μ L sample) and CD45 (PE Miltenyi Biotech 103-098-141 – 0.3 μ L added to 400 μ L sample) and 15 minutes with 1.25 μ M DRAQ5 (Life Technologies). A positive control was accomplished by exposing DLD isolated white blood cells to 0.2 μ M PMA (Sigma-Aldrich P1585 – phorbol 12-myristate 13-acetate) also known as TPA (12-O-Tetradecanoylphorbol-13-acetate), a potent agonist, for 30 minutes in an incubator and then stained. Isolated white blood cells were also diluted to 100,000 WBCs per mL and then concentrated using either a 50x inertial focusing siphon concentrator device or centrifugation in a 15mL conical at 125 r.c.f. for 5 minutes. Supplementary Figure 12 presents the relative average CD11b expression as compared to the average expression for the input WBCs isolated using DLD (only CD11b positive events are counted in the statistics). The only non-significant difference between the different test conditions was between the IFC and centrifugation conditions that were not significantly different (*p=0.0943).



Supplementary Figure 12: Relative CD11b expression of CD11b positive events between different test cases. White blood cells isolated using deterministic lateral displacement (DLD WBCs), DLD WBCs treated with 0.2 μ M PMA for 30 minutes at 37C (PMA - positive control), cells concentrated using the microfluidic inertial focusing concentrator (IFC) and cells concentrated using a 5 minute centrifugation at 125 r.c.f. Population means are plotted with standard error

shown with error bars. All comparisons were significant ($p < 0.0001$) except for the IFC and centrifugation conditions that were not significantly different ($*p = 0.0943$).