

Supplementary Figure 1| Guide stars of progressively longer wavelengths can be used for direct wavefront sensing at increasingly large depth in the cortex of the living mouse. Typical SH images of guide stars obtained at different depths by TPE of: YFP in sparsely labeled L5 pyramidal neurons (left column); tdTomato in densely labeled cortical neurons (middle column); and the directly injected ICG (right column) in the cortex of a living mouse.

Supplementary Figure 2| Performance comparison of guide stars generated by TPE of YFP, tdTomato or IGC in the cortex of a living mouse. (a) Signal-to-background ratio (SBR) of guide-star images on the SH sensor (**Supplementary Figure 1**) generated by TPE of YFP, tdTomato, or ICG at different depths in the cortex of the living mouse. Each circle is the SBR of the guide-star image formed by a single lenslet. The averages of each data set at different depths are connected by solid lines. **(b)** Data in (a) represented as box-and-whisker plots (circles indicate outliers). **(c)** Scattering and extinction coefficients of the live mou[s](#page-16-0)e cortex at different wavelengths¹. (d) The total number of fluorescence photons emitted within the cortex from the guide star that is required for an average spot localization precision of 1/5 pixel size on the SH sensor (1 pixel size equals 1.07 µm at sample plane). The calculation was done for a NA 1.1 objective using the extinction coefficients in (c). The localization precision is estimated based on the theory by Thompson, et al²[.](#page-16-1)

Supplementary Figure 3| Correction of cranial-window-induced aberration. (a-b) *In vivo* TPE fluorescence images of axons and dendrites at 15 µm depth in the cortex of a Thy1-YFPH mouse as acquired **(a)** without AO and **(b)** with AO corrections. The objective correction ring was adjusted to optimize imaging in water (i.e., without any correction for the cranial window aberration). Scale bar is 20 µm. **(c)** Corrective wavefront for the cranial-window-induced aberration.

Supplementary Figure 4| Image comparison with different correction schemes. Comparative in vivo TPE fluorescence images of the same field of neurons 500 µm deep in the cortex of a Thy1-YFPH mouse as acquired with: **(a)** the objective correction ring optimized for imaging in water, and no AO used; **(b)** the objective correction ring optimized for imaging into water through a 170 µm thick cranial window, and no AO used; **(c)** same as (b), except with additional AO correction carried out on the surface of the cortex to correct any residual aberrations at that position; **(d)** same as (b), except with additional AO correction carried out at the 500 μ m depth where the images were taken. Scale bar is 20 μ m.

Supplementary Figure 5| Resolution enhancement after AO correction. (a) Single-plane TPE fluorescence images of a dendritic branch at 550 µm below pia in a Thy1-YFPH mouse before (with only correction ring) and after AO correction. Scale bar is 2 µm. **(b)** Line intensity profiles of the feature (the neck of a dendritic spine) indicated by arrows in (a). Image of the spine neck after AO correction has a full width at half maximum of 430 nm.

Supplementary Figure 6| **Zernike modes for the corrective wavefront of Fig. 1c, measured at 600 µm depth in the mouse cortex.** Amplitudes of Zernike modes in a modal decomposition of the wavefront. Inset shows the wavefront as calculated from the first 9, 19, or 29 modes, respectively.

Supplementary Figure 7| Required cranial window diameter for imaging 750µm below pia with a 1.1 NA objective.

Supplementary Figure 8| Effects of hemoglobin absorption on direct wavefront sensing *in vivo***. (a)** Blood (black) absorbs visible fluorescence, but **(b)** transmits NIR ICG fluorescence for wavefront sensing. The dashed circle in (a) corresponds to that in (b). Scale bar is 50 μ m.

Supplementary Figure 9| Experimental schematics. (a) Two photon scanning & AO mode: Near-infrared (NIR) pulsed excitation (red) is directed into the system by dichroic mirror D3, reflected off a deformable mirror, and scanned by a pair of galvanometer mirrors (Galvo X and Y) before entering the rear pupil of a 1.1 NA water-dipping objective. The deformable mirror, Galvos X and Y, and the objective rear pupil are all mutually conjugate, so that the phase pattern from the deformable mirror is stationary at the rear pupil even while scanning. The emitted visible signal fluorescence is collected by the objective, reflected from dichroic mirror D1, and focused onto a photomultiplier tube PMT1. The NIR fluorescence from the TPE guide star (orange) is descanned by the galvos, separated from the NIR excitation by dichroic beamsplitter D2, and then sent to a Shack-Hartmann (SH) sensor to determine the aberrated wavefront of the emission. **(b)** Confocal scanning mode: visible excitation light (blue) is reflected by dichroic mirror D4 and follows the same light path as NIR excitation to the objective. The emission retraces the excitation path, except that it transmits through dichroic mirror D4 and enters another photomultiplier tube PMT2 after going through a pinhole that is conjugated to the objective focus.

Supplementary Table 1| Acquisition parameters for images in the main text.

Supplementary Table 1 (cont'd)| Acquisition parameters for images in the main text.

Supplementary Table 2| Acquisition parameters for supplementary figure 1.

Supplementary Table 3| Acquisition parameters for images in supplementary figures.

Supplementary Table 4| Acquisition parameters for images in supplementary movies.

Supplementary Table 4 (cont'd 2)|Acquisition parameters for images in supplementary movies.

Supplementary References:

- 1. Jacques, S.L. Optical properties of biological tissues: a review. *Phys Med Biol* **58**, R37-61 (2013).
- 2. Thompson, R.E., Larson, D.R. & Webb, W.W. Precise nanometer localization analysis for individual fluorescent probes. *Biophys J* **82**, 2775-2783 (2002).