

1 SUPPLEMENTARY INFORMATION

2 AN OPTOGENETIC DEMONSTRATION OF MOTOR MODULARITY IN THE MAMMALIAN SPINAL CORD

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4 * = equal contributions

5 The analysis in the main text of motoneuronal and interneuronal spinal topography considered
6 only the force fields elicited by the lowest laser power used at each spinal locus examined. We
7 also investigated how sensitive the force-field structure was to the power of the laser used in
8 both mouse types. At various spinal loci, we successively increased the laser power at 2.5 to 15%
9 increments, over 4 to 8 power levels. We then summarized the change of force-field structure
10 induced by power increase by examining the change in the x- and y-components of the force-
11 field vector sum, with its magnitude normalized to unity (with increasing x corresponding to the
12 anterior direction, and increasing y to the dorsal), and also, the change in the average vector
13 magnitude across all vectors in the field, as a function of power level. In both Chat and Thy1
14 mice, increasing stimulation power had the effect of increasing the average magnitude of the
15 force-field vectors (Fig. S1A & S1B, right panel). In the Chat mouse, the overall flow direction of
16 the force-field vectors was not appreciably changed by power increase, as suggested by the
17 relatively constant x- and y-components of the force-field vector sum across the power levels
18 (Fig. S1A, left and middle panels). In the Thy1 mouse, however, increasing laser power
19 decreased the x-component (Fig. S1B, left panel), and either increased or decreased the y-
20 component of the vector sum (Fig. S1B, middle panel). Thus, for the Thy1 mouse, increasing the
21 stimulation power tended to shift the flow of the force-field vectors toward the posterior
22 direction (i.e., decreasing x) by vector rotation through the dorsal (i.e., increasing followed by
23 decreasing y) or ventral direction (i.e., decreasing followed by increasing y).

24
25 We show in Fig. S1 two examples of how increasing the stimulation power can alter the Thy1
26 force field. In the first example, as power was increased the force vectors rotated from the
27 anterior to the dorsal directions (Fig. S1C). In the second example, increasing power had the
28 effect of rotating the vectors from the anterior, then to the ventral, and finally to the
29 posterior/dorsal directions (Fig. S1D).

30 In addition, we also analysed how increasing the stimulation power at the same spinal loci may
31 alter the onset time of force emergence and the degree of vector divergence within the force
32 field, the latter quantified by the circular standard deviation (SD) of the force-vector azimuth
33 angle. In Chat, as compared with Thy1 a greater minimum power laser (usually at 40-50 mW
34 with respect to ~10 mW necessary in the Thy1) was needed to evoke observable hindlimb force;
35 but over the range of power tested, the force onset time remained constant at 6.6 ± 2.0 ms
36 (mean \pm SD; Fig. S2A, red; see also Fig. 1D). In Thy1, as laser power was increased, force onset
37 time decreased from 11.4 ± 5.4 ms (Fig. S2A, blue, bin 1; Fig. 1D) to 4.9 ± 1.2 ms (bin 3)
38 (multiple comparison after Kruskal-Wallis, $p < 0.01$). In fact, the Thy1-onset time was
39 significantly greater than the Chat onset times only at the lowest power ($p < 0.01$), but not at
40 other powers ($p > 0.05$). The higher Thy1-onset time recorded at the lowest power argues that
41 at this stimulation intensity, the force evoked likely resulted from activations of interneurons,
42 which could be one to several synapses away from the motoneurons. At higher power

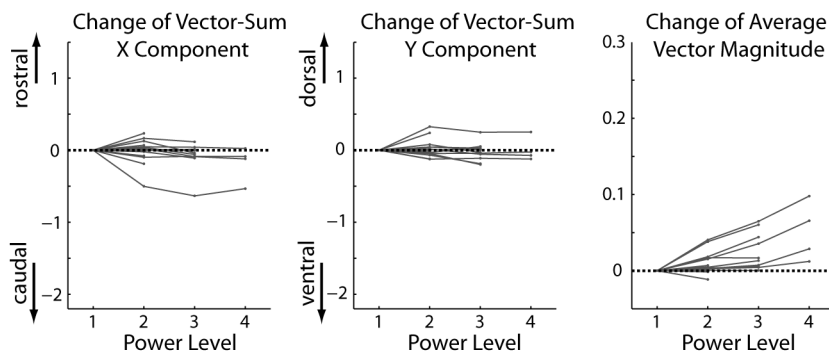
43 intensities, the motoneurons were recruited in addition to the interneurons, thus resulting in
44 the similar onset times between Chat and Thy1.

45 On the other hand, in both mouse strains the circular SD of the vector azimuth angles did not
46 vary over the range of stimulation power tested ($p > 0.05$; Fig. S2B). The Thy1 values, however,
47 were overall greater than the Chat values ($p < 0.01$; Fig. S2B, *). This result illustrates that even
48 when the motoneurons were activated along with the interneurons, the resulting force fields
49 were still more complex in structure than the Chat fields, further suggesting that the divergence
50 of vectors in Thy1 owes its origin to interneuronal activations.

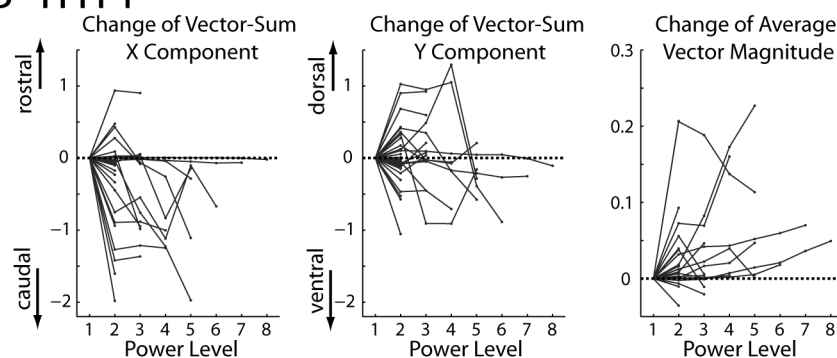
51 Force fields emerged over time and assumed a more stable configuration only after 50 ms from
52 light onset. In Fig. S3, we depict typical time courses of how force fields evolved over the 200-ms
53 stimulation time, for a Chat field (Fig. S3A), a convergent Thy1 field (Fig. S3B), and a divergent
54 Thy1 field (Fig. S3C). The force field's structure stabilized by 25-50 ms for Chat, and by 50-75
55 ms for the Thy1 fields. Prompted by these observations, in all of our analysis for both mouse
56 strains, we constructed a time-invariant force field by obtaining the force vector for each ankle
57 location, and then averaging the force recorded from 50 to 200 ms after stimulation onset (see
58 Methods of main text).

59 SUPPLEMENTARY FIGURE

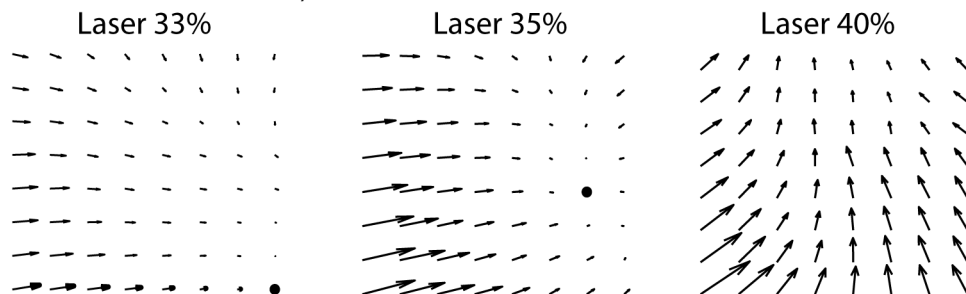
A CHAT



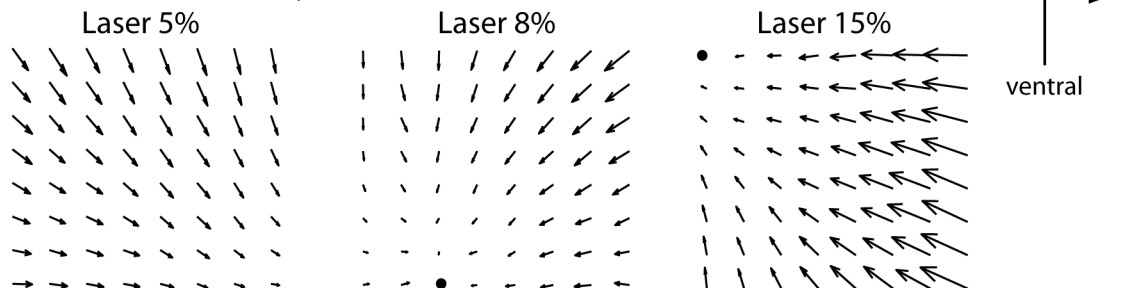
B THY1



C THY1 Mouse T9, 3.04 mm



D THY1 Mouse T7, 4.90 mm

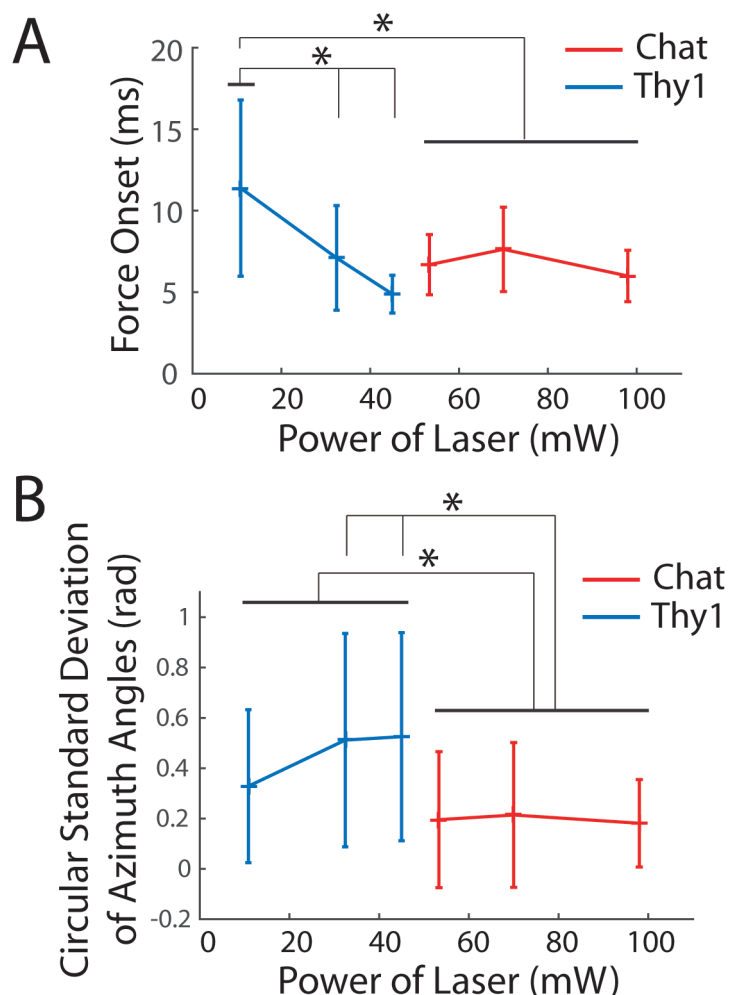


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61 **FIGURE S1. Effect of power increase on the force fields in both Chat and Thy1 mice.** **A**, In
 62 Chat, increasing the stimulation power did not alter the orientation of the force field, as
 63 evidenced by the lack of change of both the x- (left panel) and y- (middle panel) components of the
 64 vector sum as power was increased. Increasing the power, however, did increase the
 65 magnitude of the force vectors (right panel). **B**, In Thy1, increasing the power tended to shift the

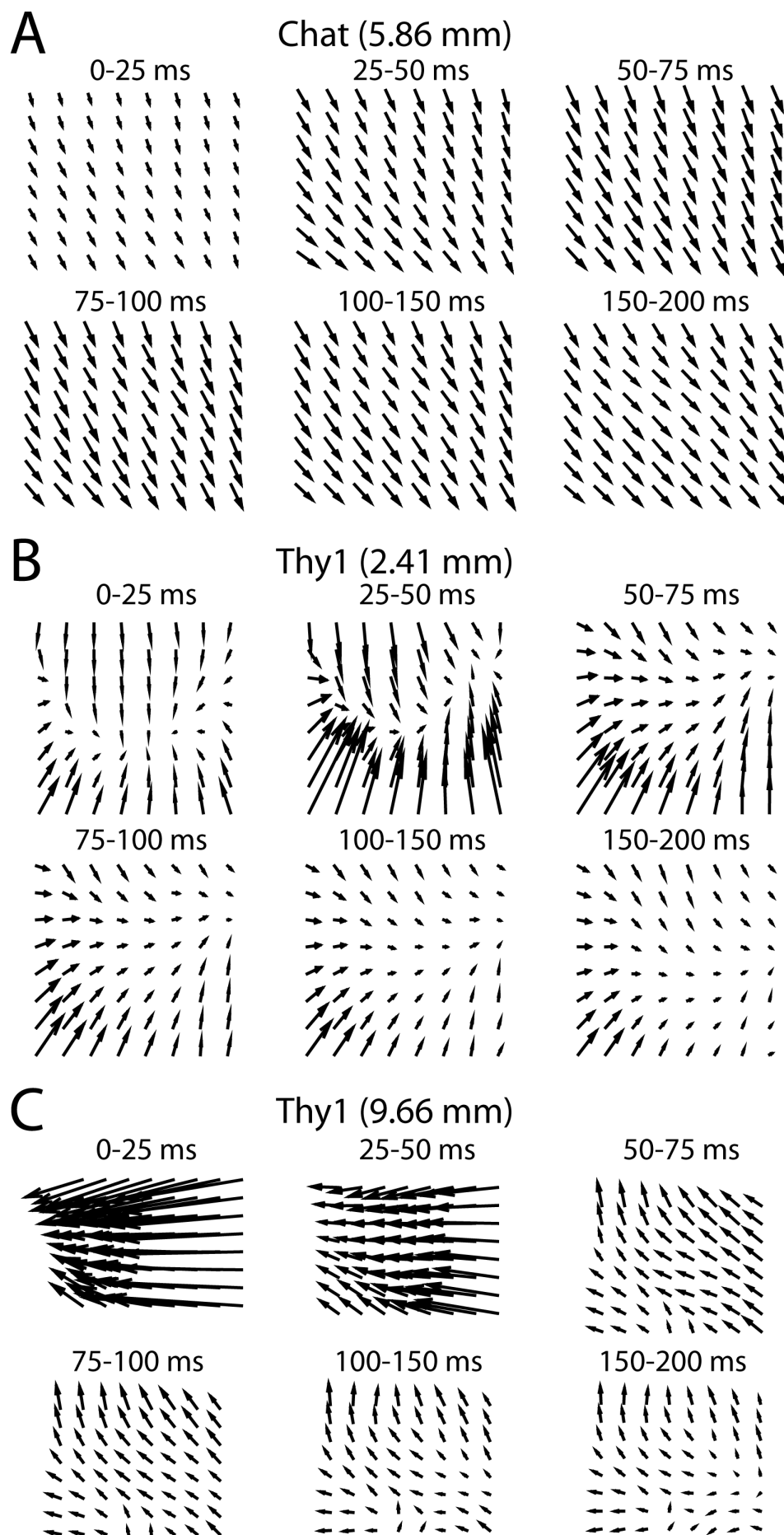
66 force field to a more caudal orientation, as evidenced by a decrease in the x-component (left
 67 panel), but a variable change in the y-component (middle panel), of the field vector sum as
 68 power was increased. **C, D**, Two examples, from two different Thy1 mice and two stimulation
 69 loci, showing how increasing the laser power shifted the force field to a more caudal orientation,
 70 through a rotation towards either the dorsal (panel C) or ventral (panel D) directions.

71



72

73 **FIGURE S2. Effect of power increase on the force onset time and within-field vector**
 74 **divergence in Thy1 and Chat.** **A**, In Thy1 (blue), increasing stimulation power decreased the
 75 force onset time (*; multiple comparison after Kruskal-Wallis, $p < 0.01$) while in Chat (red),
 76 onset time remained fairly constant over the range of power tested. Only at the lowest power
 77 was the Thy1-onset time significantly different from the Chat onset time (*; $p < 0.01$). This result
 78 suggests that at minimum power, the force field evoked in Thy1 likely results from only
 79 interneuronal activations. Note that as compared with Thy1, Chat required larger power
 80 intensities for producing observable forces. **B**, In both Thy1 and Chat, the circular SD of the
 81 vector azimuth angle did not vary over the range of power tested ($p > 0.05$). But the Thy1 values
 82 were significantly greater than the Chat values (*; $p < 0.01$). This suggests that interneuronal
 83 activations were sufficient to produce force fields more complex in structure than the Chat
 84 fields.



86 **FIGURE S3. Time courses of how force fields evolved after laser stimulation onset.** We show
87 the time courses of **A**, a Chat force field (recorded at spinal stimulation locus of 5.86 mm), **B**, a
88 convergent Thy1 force field (at 2.41 mm), and **C**, a divergent Thy1 force field (at 9.66 mm). The
89 six fields in each time course were constructed by averaging force vectors (recorded at 20,000
90 Hz) over the time ranges of 0-25, 25-50, 50-75, 75-100, 100-150, and 150-200 ms, respectively.
91 In all three examples, the structure of the force field stabilized by 50-75 ms.