

# 1 **S1 Appendix. Generic Simulation Methods**

## 2 **Retinal Projection**

3 The visual field (i.e. the retinal area on which the stimulus was projected) was  
4 restricted to  $8^\circ$  for all model simulations. The stimuli were projected at the center of this  
5 projection area in sizes as specified in the behavioral studies. The initial values of the cells  
6 in each retinal layer were set to resting potential values (or, in an algorithmic term, steady  
7 state values of the equations) to the adapting light intensity (i.e. uniform illumination over  
8 the entire visual field) in each experiment.

9 We applied foveal photoreceptor density uniformly for the entire visual field (i.e.  
10 projection area) and disregarded the radial density reduction as a function of retinal  
11 eccentricity (fovea v.s. periphery). The foveal cell density was set to 146000  
12 *photoreceptors/mm<sup>2</sup>* (111 x 111 cells per square degree) following Wilson's model [S1].

13 While our assumption on the cell density needs to be interpreted with a caution, we  
14 considered that disregarding the change of the spatial sampling rate across the retinal  
15 surface is rather compatible to the fact that, in reality, observers in the behavioral  
16 experiments [S2,S3] were not restricted from eye movements, in which case the observers  
17 would move their eyes to refocus different areas of the stimulus onto the fovea. This  
18 assumption on cell density is relatively unimportant for the simulations of Reid and  
19 Shapley's experiment in which the maximum size of the stimuli was  $1.8^\circ$ .

## 20 **Luminance Unit**

21 Both of the original models by Wilson [S1] and by van Hateren [S4,S5] are designed  
22 to take in troland (retinal illuminance) values. If the behavioral studies provided luminance  
23 values in *cd/m<sup>2</sup>* for stimulus intensity, the provided values were converted into troland unit.

24 As a standard, we set the pupil diameter to 3 mm, which is the value used in Wilson's  
25 model. Wilson defined the point-spread function of light scatter corresponding to the 3mm  
26 pupil based on Campbell and Gubisch [S6] and we kept all these aspects intact for all the  
27 simulations using Wilson's model.

28 We tested an additional pupil size with van Hateren's model (6.5 mm, from  
29 monocular viewing of 8  $cd/m^2$  field by a 30-year-old person based on the study by [S7]) and  
30 confirmed that the results in this study are unaffected by the assumption on pupil size.  
31 Noting that assuming a larger pupil size yields bigger troland values in retinal inputs than a  
32 smaller pupil size for the same luminance values in  $cd/m^2$ , this means that our results are  
33 robust over different retinal illumination range.

## 34 **Data Acquisition**

35 Since the retinal models compute voltage responses that change across time, it is  
36 rather arbitrary to set a particular point in time in which the cell responses correspond to a  
37 perceptual experience. Given the difficulty, we have chosen the time point for data  
38 acquisition to be at 300 ms after stimulus onset (assuming that a stimulus did not set off  
39 before 300 ms). This time scale allows all the short-term feedback effect (i.e. the inhibitory  
40 feedback from horizontal and amacrine cells in Wilson's model; immediate feedback from  
41 horizontal cell without the effect of adaptive gain in van Hateren's model) to be stabilized,  
42 while this duration is insufficient for the long-term adaptive system to take significant  
43 effect (i.e. interplexiform layer cell feedback to horizontal cells for gain and temporal  
44 change in Wilson's model; adaptive horizontal gain change in van Hateren's model). Thus,  
45 all the data reported in the current study are derived by analyzing the model cell responses  
46 at 300 ms after the stimulus onset.

## 47 **Temporal and Spatial Filtering**

48 For all simulations, the solution of a first-order ordinary differential equation (ODE)  
49 for temporal low-pass filtering was approximated by the modified Tustin method [S8],  
50 which is shown to outperform other ODE approximation schemes in terms of  
51 computational accuracy and speed among autoregressive moving-average filtering  
52 methods. The time step of the temporal evolution was set to 0.1 ms.

53 The spatial filtering was performed by frequency-domain convolution. As explained  
54 in the previous sections (The Model by Wilson and The Model by van Hateren), the spatial  
55 filters were generated in the functional forms described in each of the original papers  
56 (Gaussian point-spread function in Wilson's model; weighted sum of a wide and a narrow  
57 exponential point-spread functions in van Hateren's model, 2007).

## 58 **References**

- 59 S1. Wilson HR. A neural model of foveal light adaptation and afterimage formation. *Vis*  
60 *Neurosci.* 1997;14: 403–423.
- 61 S2. Helson H. Studies of anomalous contrast and assimilation. *J Opt Soc Am.* 1963;53:  
62 179–184.
- 63 S3. Reid RC, Shapley R. Brightness induction by local contrast and the spatial  
64 dependence of assimilation. *Vision Res.* 1988;28: 115–32.
- 65 S4. van Hateren JH. A cellular and molecular model of response kinetics and adaptation  
66 in primate cones and horizontal cells. *J Vis.* 2005;5: 331–347.
- 67 S5. van Hateren JH. A model of spatiotemporal signal processing by primate cones and  
68 horizontal cells. *J Vis.* 2007;7: 1–19.

- 69 S6. Campbell FW, Gubisch RW. Optical quality of the human eye. *J Physiol.* 1966;186:  
70 558–578.
- 71 S7. Watson AB, Yellott JJ. A unified formula for light-adapted pupil size. *J Vis.* 2012;12:  
72 1–16.
- 73 S8. van Hateren JH. Fast recursive filters for simulating Nonlinear dynamic systems.  
74 *Neural Comput.* 2008;20: 1821–1846.