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Supplemental Information

A Synthetic Mammalian Therapeutic Gene Circuit

for Sensing and Suppressing Inflammation

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SUPPLEMENTARY FIGURES

 $Dox -$

 $20'$ ng

 5_{ng}

pAS58

 0_{ng}

 $Dox +$

Supplementary Figure 1 Related to Figure 2

Tuning the elements used for constructing the anti-inflammatory device

(a) Optimization of NF- κ B responsive element. HEK 293T cells were transfected with pAS36 or pAS37 and stimulated with 20 ng/mL IL-1 β (left) or 100 ng/mL TNF α (right). After 24 h luciferase activity was measured by dual luciferase test.

(**b**) Optimization of a minimal promoter. HEK 293T cells were transfected with pAS37 or pAS40 and stimulated with 20 ng/mL IL-1 β (left) or 100 ng/mL TNF α (right). After 24 h luciferase activity was measured by dual luciferase test.

(**c**) The capacity of system activation. Activated anti-inflammatory device supports comparable reporter expression level to the constitutively expressed control (pAS108; P_{CMV} -Luc or pAS109; P_{CMV} -SEAP) as measured by luciferase (left) or SEAP (right). Similarly, sensor and amplifier constructs with 2A peptide-fluorescent protein fusions (pAS97; TRE-P_{NF-KB2}-P_{MIN}-GV16-myc-2A-mCit and pAS98; TRE-UAS-P_{MIN}-GV16-myc-2A-tagBFP) support comparable system activation to the basic sensor and amplifier. For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d. (*n*=4).

(**d**) Validation of the rtTR-KRAB reset repressor. The constitutively expressed rtTR-KRAB $(pAS58; P_{hCMV}-rtTR-NLS-KRAB)$ represses Gal4-VP16 (plasmid pSGVP)-induced activation of the reporter construct (pAS51; TRE-UAS-P_{MIN}-Luc) in the presence of the increasing concentrations of doxycycline (Dox). In the absence of Dox, pAS58 alone did not significantly influence system activation (left). Activated sensor (middle) and amplifier (right) can also be shut down efficiently.

Supplementary Figure 2 Related to the Matematical ODE model

State transition diagram of the genetic circuit.

The state transition diagram of the genetic circuit was constructed using CellDesigner 4.4 software¹³. The state transitions were described with reactions listed in Supplementary Table 5.

Sensor-mCit Amplifier-tagBFP Overlay

 $\mathbf b$

 $\mathbf c$

Supplementary Figure 3 Related to Figure 3

(a) Anti-inflammatory device-engineered HEK 293T cells (reporter pAS72; TRE-UAS-P_{MIN}-SEAP) were stimulated with hIL-1 β for 4 h and then input signal was removed by medium exchange. SEAP production was quantified in the culture supernatants every 24 h along with a medium exchange to observe kinetics of a system activation. Compared to sensor alone (grey bars), setup which included also amplifier construct (black bars) yielded stronger system activation at the later time points indicating its role in the sustained system activation. For detailed information about transfected plasmids and their amounts in each specific experiment, see the Tables S1 and S2, respectively. Error bars indicate s.d. (*n*=4).

(**b**) Demonstration of the system performance by a confocal fluorescence microscopy of antiinflammatory device-engineered HEK 293T cells. Sensor and amplifier constructs were observed directly by in frame fusion via 2A peptide with mCitrine and tagBFP reporter genes, respectively (pAS97; TRE- P_{NFAB2} - P_{MIN} -GV16-myc-2A-mCit and pAS98; TRE-UAS- P_{MIN} -GV16-myc-2A-tagBFP). Twenty-four hours after stimulation, mCitrine and tagBFP positive cells were observed only in the presence of interleukin-1 β (IL-1 β) and absence of doxycycline (Dox). mCherry was used as a transfection control.

(**c**) System functionality is dependent on intracellular Gal4-VP16 transcriptional activator (GV16) meaning it is inevitable that sensor and enhancer are activated in the same cell. Cells were stimulated with IL-1β for 24 h and then observed by a confocal fluorescence microscopy to demonstrate the simultaneous activation of both constructs in the same cell. For detailed information about transfected plasmids and their amounts in each specific experiment, see the Supplementary Table 1 and 2, respectively. Error bars indicate s.d. (*n*=4).

a

Supplementary Figure 4 Related to Figure 4

(a) Concentration of human IL-1 β and TNF α in peritoneal lavage fluid (left), mouse IL-1 β , TNF α and IL-6 in peritoneal lavage fluid (middle) or serum (right) of mice, which were injected i.p. with human IL-1B (300 ng/mouse) or human TNF α (250 ng/mouse) and then sacrificed at different time points.

(**b**) Concentration of mouse IL-1 β , TNF α and IL-6 in peritoneal lavage fluid (left) and serum (right) of mice 72 h after CLP procedure.

(**c**) SEAP levels in serum 24 h post implantation and in the peritoneal lavage fluid 48 h post implantation. For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d.

(**d**) The response of the microencapsulated anti-inflammatory device *in vitro* prior to implantation in mice (left) and secretory *Renilla* luciferase (pAS75; SR-Luc) in peritoneal lavage fluid 48 h after microcapsules implantation. SR-Luc was co-transfected along with the anti-inflammatory device but not with the control microcapsules. SR-Luc is comparable among all groups (right).

(**e**) Validation of the chimeric NF-KB-STAT3 sensor. Cells were transfected with the constructs for the anti-inflammatory device, except for the sensor, where $pAS60$ (TRE- P_{NF} - $_{KB2}$ -P_{MIN}-GV16-myc) was replaced by pAS132 (TRE-P_{NF-KB2-STAT3}-P_{MIN}-GV16-myc). Cells were also transfected with hIL-6 receptor (hIL-6R) where indicated to enable responsiveness to human IL-6. For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d. $(n=4)$.

Supplementary Figure 5 Related to Figure 5

(**a**) Western blot analysis of anti-inflammatory effectors from cell culture. (i) Left: Constitutive (pAS35; P_{cmv} -hIL-1RA-myc); and right: inducible (pAS63; TRE-UAS- P_{MIN} -hIL-1RA) production of human interleukin-1 receptor antagonist (hIL-1RA). (ii) Left: Constitutive (pAS114; P_{CMV} -anti-hTNF α Ab); and right: inducible (pAS113; TRE-UAS- P_{MIN} -anti-hTNF α Ab) production of anti-hTNF α antibody (anti-hTNF α). (iii) Anti-inflammatory devicederived (pAS116; TRE-UAS-P_{MIN}-anti-hTNF α Ab-hIL-1RA) production of hIL-1RA and anti-hTNF α . (iv) Recombinant anti-hTNF α used as a control. Amounts of effectors produced from the anti-inflammatory device are comparable to the amounts from a constitutive expression. Putative glycosylation of hIL-1RA is marked as an asterisk. Anti-hTNFα produced in our system has a putative glycosylation at a heavy chain, resulting in tree bands observed (none, only one or both heavy chains glycosylated, marked as an asterisk). Recombinant control, produced from CHO cells however, shows only one substantial band, implicating that biological activity could not be exactly the same. For detailed information about the transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively.

(**b**) MWCO of the microcapsules. MWCO was determined by FITC-Dextrane (FITC-Dex) of different molecular weights (20 kDa, 70 kDa, 150 kDa, 2000 kDa). Alginate-PLL-alginate microcapsules were incubated overnight at 37 \degree C with the FITC-Dex solution (20 μ g/mL) and then they were washed 3 x using MOPS buffer. Immediately after that, we acquired images using confocal fluorescence microscopy.

(c) All forms of anti-hTNF α are able to cross the membrane of microcapsules as observed by western blot analysis, where all bands are present in both, ruptured and unruptured microcapsules. Microcapsules were ruptured by injecting the suspension through 23G needle. (d) Intracapsular amount of anti-hTNF α produced from double effector (pAS116; TRE-UAS-

 P_{MIN} -anti-hTNF α Ab-hIL-1RA). Concentration, determined in 10 mL of supernatant or in 1 mL suspension of the same, but previously ruptured microcapsules (left) and total amount of anti-hTNF α (right). For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d. (*n*=3).

(**e**) Secretory *Renilla* luciferase (SR-Luc) control for the *in vitro* (left) and *in vivo* (right) production of anti-inflammatory proteins. SR-Luc was measured either in ruptured microcapsules for *in vitro* assay or in the peritoneal lavage fluid 48 h after microcapsules implantation. SR-Luc is comparable among all groups. For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d. (*n*=4).

(**f**) Production of anti-inflammatory effectors from different constructs and different regimes as indicated in the figure. For detailed information about transfected plasmids and their amounts in each specific experiment, see Supplementary table 1 and 2, respectively. Error bars indicate s.d. $(n=4)$.

(g) Constitutive *in vivo* production of hIL-RA from the construct pAS35; P_{cmv} -hIL-1RA-myc. For detailed information about transfected plasmid and its amount see Supplementary table 1 and 2, respectively. Error bars indicate s.d. (*n*=4).

 $\mathbf b$

 $\mathbf d$

Supplementary Figure 6 Related to Figure 6

(**a**) The reversibility of the synthetic anti-inflammatory device. Upper left panel: Raw SEAP measurements for *in vitro* shutdown of the system. Anti-inflammatory device-engineered HEK 293T cells (reporter pAS72; TRE-UAS-P_{MIN}-SEAP) were stimulated with interleukin-1 (IL-1β, 1 ng/mL) 6 h after transfection (marked as ON) or left unstimulated (marked as control). 24 h after first stimulation, supernatant containing SEAP was collected and medium was exchanged (indicated by arrows) or in addition, cells were stimulated with IL-1β (1 ng/mL) (marked as ON) or shut down by doxycycline (Dox, 1 µg/mL) (marked as OFF). 48 h and 72 h after first stimulation, procedure was repeated. Upper right panel: Raw SEAP measurements for *in vitro* rebooting of the system shutdown. Anti-inflammatory deviceengineered HEK 293T cells (reporter pAS72; TRE-UAS-P_{MIN-}SEAP) were stimulated with IL-1β (1 ng/mL) 6 h after transfection (marked as ON), shut down by Dox (1 μ g/mL) (marked as OFF) or left unstimulated (marked as control). 24 h after first stimulation, supernatant containing SEAP was collected and medium was exchanged (indicated by arrows) or in addition, cells were stimulated with IL-1β (1 ng/mL) (marked as ON) or left unstimulated (Control). Lower panel: Secretory *Renilla* luciferase (SR-Luc) used for an internal control. Secretory *Renilla* luciferase is comparable among all groups at any time point in *in vitro* reversibility test.

(**b**) SR-Luc corresponding to the *in vivo* restraint of the full system activation

(**c, d**) Shut down of the anti-inflammatory device *in vivo*. The data represent concentrations corresponding to the results represented in Fig. 6c and 6d. The anti-inflammatory deviceengineered HEK 293T cells (effector pAS134; TRE-UAS- P_{MIN} -anti-hTNF α Ab-mIL-10) were microencapsulated, implanted i.p. and fully activated by injection of a combination of 300 ng of hIL-1 β and 250 ng of hTNF α per mouse. After 24 h (thin arrow) the device was shut down by an i.v. Dox injection (20 mg/kg). (c) The device was additionally activated and

shut down after 72 h (thick arrow) to reach the relevant time span needed for an observation of the anti-hTNF α antibody kinetics. Serum was collected at different time points and antihTNF α antibody or mIL-10 levels were measured.

 $\mathbf e$

Supplementary Figure 7 Related to Figure 7

(**a**) A decrease in the system's capacity due to the transient nature of the system. Left: The anti-inflammatory device-engineered HEK 293T cells (reporter $pAS72$; TRE-UAS- P_{MIN} -SEAP) were stimulated with hIL-1 β (1 ng/mL) every 24 h by exchanging the medium (indicated by the arrows). The experiment was started 6 h post transfection, which was represented by 0 h time point. The kinetics of SEAP production was measured every 24 h. Right: The anti-inflammatory device-engineered HEK 293T cells (reporter pAS72; TRE-UAS-P_{MIN}-SEAP) were stimulated with hIL-1β (1 ng/mL) every 48 h by exchanging the medium (indicated by the arrows). The experiment was started 24 h post transfection, which was represented by 0 h time point. The kinetics of SEAP production was measured every 24 h to observe a cumulative SEAP production. Error bars indicate s.d. (*n*=4).

(**b**) DSS-induced colitis increased endogenous inflammatory cytokines in the supernatants of colon biopsy samples but does not activate the device. Left: Concentration of endogenous mIL-1 β and mTNF α in the supernatants of colon biopsy samples on the 8th day of DSSinduced acute colitis $(n=6)$ biopsy samples per mouse, 2 mice per group) Right: The activation of the implanted anti-inflammatory device by DSS. The mice were given either water or 2 % DSS for 8 days and on the $5th$ day of this time-course experimental model, the microcapsules containing anti-inflammatory device-engineered cells (effector construct pAS134; TRE-UAS- P_{MIN} -anti-hTNF α Ab-mIL-10, Supplementary Table 1) were implanted i.p. Positive control group was stimulated with a combination of 300 ng of hIL-1 β and 250 ng of hTNF α per mouse 1 h post implantation. Concentration of anti-hTNF α was measured 72 h post implantation (on the $8th$ day of the experimental colitis model) ($n=3$).

(**c**) A decrease in the system's capacity due to the transient nature of the system. HEK 293T cells were transfected according to the Supplementary Table 2 and lysed after 1 or 5 days. Samples were analyzed by real-time quantitative PCR using the primers to specifically amplify the amplifier or the inducible OFF-switch constructs. The plasmid copy number in the samples was estimated from the standard curves of the known amounts of the respective constructs spiked into the lysate and recalculated per cell $(n = 2$ biological replicates tested at 2 different dilutions of the respective lysate).

(**d**) Confocal fluorescence microscopy of the microcapsules in the *in vitro* culture as observed 1, 3 or 7 days after microencapsulation procedure. A large majority of the microencapsulated cells remained viable and divided as observed by aggregates formed. Live and dead cells were stained with Hoechst and propidium iodide, respectively.

(**e**) Confocal fluorescence microscopy of the microcapsules after having been implanted in peritoneal cavity of mice for 3 days. Cells remain viable during the course of the experiments, conducted in this study. Live and dead cells were stained with Hoechst and propidium iodide, respectively.

EXTENDED EXPERIMENTAL PROCEDURES

The ability of antibody molecules to transverse the alginate-PLL-alginate membrane

Anti-hTNF α antibody is a glycosylated, 150 kDa molecule and since the ability of antibody molecules to transverse the alginate-PLL-alginate membrane is somewhat controversial^{1,2}, we investigated whether the anti-hTNF α is able to cross the membrane of microcapsules in our system. First, we have shown that 20 kDa, 70 kDa and also 150 kDa, but not 2000 kDa FITC-Dextrane molecules are able to cross the membrane (Supplementary Fig. 5b). Next, we have shown that glycosylated, higher molecular mass forms of the antibody are secreted from the microcapsules, since we detected corresponding bands in the western blot analysis of either intact or ruptured microcapsules (Supplementary Fig. 5c). The intracapsular concentration of anti-hTNF α was somewhat higher than the concentration in the supernatant, nevertheless, the majority of anti-hTNF α was released into the supernatant (Supplementary Fig. 5d).

Confocal fluorescence microscopy related to Supplementary Fig. 3b, 3c, 5b and 7

For the *in vitro* direct observation of the system's performance, HEK 293T cells were seeded onto 8-well microscopic chambers (Ibidi) at a density of 5 x 10^4 cells per well. Cells were transfected with the constructs pAS97 (observation of the sensor activity) and/or pAS98 (observation of the amplifier activity), pAS72, pAS67, pAS58, pAS75 and pmCherry-C1 (detailed description in the Supplementary Table 1). 4 h after transfection, doxycycline (1 μ g/mL) was added to the samples, which we wanted to shut down. 24 h after transfection, the system was stimulated with human IL-1 β (R&D Systems, Inc., Minneapolis, USA) at a final concentration of 1 ng/mL. 4 h after stimulation, medium was removed and cells were washed 3 x using fresh medium to remove an input signal. After 24 h, the responsiveness of the system was visualized and microscopic images were acquired using the Leica TCS SP5 inverted laser-scanning microscope on a Leica DMI 6000 CS module equipped with a HCX PL Fluotar L 20 x, numerical aperture 0.4 (Leica Microsystems, Wetzlar, Germany). A 514nm laser line of a 100-mW argon laser with 25 % laser power was used for mCitrine excitation, and the emitted light was detected between 520 and 580 nm. A 50-mW 405-nm diode laser was used for tagBFP excitation and the emitted light was detected between 420 and 460 nm. A 1-mW 543-nm HeNe laser was used for mCherry excitation and the emitted light was detected between 560 and 630 nm. Leica LAS AF software was used for acquisition and ImageJ software was used for image processing.

To determine an approximate MWCO of the microcapsules, we observed the permeability of microcapsules for fluorescein isothiocyanate-dextran (FITC-Dex, Sigma Aldrich) of different molecular weights (20 kDa, 70 kDa, 150 kDa and 2000 kDa). Alginate-PLL-alginate microcapsules were incubated overnight at 37 \degree C with the FITC-Dex solution (20 μ g/mL) and then they were washed 3 x using MOPS buffer. Immediately after that, we acquired images using confocal fluorescence microscopy. A 488 Argon laser was used for FITC-Dex excitation and the emitted light was detected between 502 and 553 nm.

To observe integrity of microcapsules and viability of cells after 3 day *in vivo* experiment we made peritoneal lavage and collected microcapsules. We stained microcapsules with Hoechst at a final concentration of $1 \mu g/mL$ (ImmunoChemistry Technologies, LLC, 639) for live cells and propidum iodide at a final concentration of $0.6 \mu g/mL$ (Sigma Aldrich, P4864) for dead cells. After 30 min incubation at 37 °C, images were acquired. A 1-mW 543-nm HeNe laser was used for propidium iodide excitation and the emitted light was detected between 600 and 670 nm. A 405 Diode laser was used for Hoechst excitation and the emitted light was detected between 429 and 509 nm. The same procedure was followed for the visualization of the microencapsulated cells after 1, 3 and 7 days in the *in vitro* culture.

Cytokine detection related to Supplementary Fig. 4a, 4b and 7b

Serum and peritoneal lavage fluid of mice were collected as described in the Materials and Methods section (Animal Models) in the main article. Colon biopsy samples were prepared by following the described³ "Full-thickness organ culture" method to determine a concentration of inflammatory cytokines in the supernatants. Inflammatory cytokine levels were measured by a sandwich ELISA according to the manufacturer's instructions (eBioscience) as follows: human IL-1 β was detected by human IL-1 beta ELISA Ready-SET-Go! (eBioscience, 88-7010), human TNF- α by human TNF alpha ELISA Ready-SET-Go! (eBioscience, 88-7346), mouse IL-1 β by mouse IL-1 beta ELISA Ready-SET-Go! (eBioscience, 88-7013), mouse TNF α by mouse TNF alpha ELISA Ready-SET-Go! (eBioscience, 88-7324), mouse IL-6 by mouse IL-6 ELISA Ready-SET-Go! (eBioscience, 88-7064).

Western blotting related to Supplementary Fig. 5a and 5c

Supernatants from pAS35 (CMV promoter-driven hIL-1RA-myc production), pAS113 (NF- κ B-driven anti-hTNF α antibody expression), pAS114 (CMV promoter-driven anti-hTNF α) antibody) and pAS116 (NF- κ B-driven anti-hTNF α antibody-hIL-1RA-myc double effector expression unit) (detailed description in the Supplementary Table 1) were analyzed for hIL-RA-myc and anti-hTNF α antibody expression. 30 μ L of a cell culture supernatant, expressing certain protein was mixed with 4xSDS buffer without reducing agent, boiled for 5 min at 95 °C and centrifuged at 14000g for 3 min. Proteins were resolved on 12 % SDS-PAGE and analyzed by a standard western blotting procedure. hIL-1RA-myc was detected by rabbit antimyc IgG primary antibody (1: 500) (Sigma Aldrich, C3956) and goat polyclonal to rabbit IgG (HRP) secondary antibody (1: 3000) (Abcam, ab6721), while anti-hTNF α antibody was detected by rabbit polyclonal secondary antibody to human $IgG - H$ and L (HRP) (1: 3000) (Abcam, ab 6759). Recombinant anti-hTNF-α-hIgG1 (InvivoGen, htnfa-mab1) and an empty vector pcDNA3.1 were used as controls.

Estimation of the plasmid copy number per cell related to Supplementary Fig. 7c

A decrease in the system's capacity due to the transient nature of the transfection was estimated by real-time quantitative PCR analysis. HEK 293T cells were seeded in 10 cm tissue culture petri dish (TPP), transfected at 50-70 % confluency according to the Supplementary Table 2, washed with PBS twice, trypsinized and collected by centrifugation (1400 rpm, 8 min) 1 or 5 days post transfection. The number of cells was determined by Trypan blue staining. Cell lysis was performed by resuspending the pellet in 500 μ L MQ, incubation at 4 °C for 12 h, freezing at -70 °C, boiling at 95 °C for 10 min and centrifugation (12000 rpm, 20 min). Supernatants were transferred to fresh tubes and stored for analysis at - 20 °C. Samples were diluted 1000-fold or 10000-fold and analyzed by real-time quantitative PCR using the primers to specifically amplify the plasmid encoding the amplifier (F: 5'- ACTGTCCTCCGAGAGATCTTAGAGGG-3' R: 5'-GCGACACTCCCAGTTGTTCTTCAG-3') or the inducible OFF-switch (F: 5'- GGCGGTGGTGCTTTGTCTCC-3' R: 5'-CTCCAGCATCACATTTCTGTACACG-3') constructs. Real-time PCR was performed using Power SYBR Green PCR Master Mix (Roche) in a Roche LightCycler® 480. Known amounts of the corresponding plasmids were spiked into the 1000-fold or 10000-fold diluted lysate of the non-transfected cells (prepared as described above) to obtain the standard curves $(C_t$ plotted against log plasmid copy number) under the same cycling conditions. The plasmid copy number in the samples was estimated from the standard curves and recalculated per cell.

Supplementary Table 1. Genetic constructs used and designed in this study

GCGTGCACACCTTTCCAGCTGTGCTGCAGAGCAGCGGCCTGTACAGCCTGAGC AGCGTCGTGACTGTGCCCAGCAGCTCTCTGGGCACCCAGACCTACATCTGCAA CGTGAACCACAAGCCCAGCAACACCAAGGTGGACAAGAAGGTGGAACCCAAG AGCTGCGACAAGACCCACACCTGTCCCCCTTGTCCTGCCCCCGAACTGCTGGG AGGCCCTTCCGTGTTCCTGTTCCCCCCAAAGCCCAAGGACACCCTGATGATCA GCCGGACCCCCGAAGTGACCTGCGTGGTGGTGGATGTGTCCCACGAGGACCCT GAAGTGAAGTTTAATTGGTACGTGGACGGCGTGGAAGTGCACAATGCCAAGA CCAAGCCTAGAGAGGAACAGTACAACTCCACCTACCGGGTGGTGTCCGTGCTG ACCGTGCTGCATCAGGACTGGCTGAACGGCAAAGAGTACAAGTGCAAAGTGT CCAACAAGGCCCTGCCTGCCCCCATCGAGAAAACCATCAGCAAGGCCAAGGG CCAGCCCCGCGAACCCCAGGTGTACACACTGCCCCCAAGCAGGGACGAGCTG ACCAAGAACCAGGTGTCCCTGACCTGTCTCGTGAAAGGCTTCTACCCCAGCGA CATTGCCGTGGAATGGGAGAGCAACGGCCAGCCCGAGAACAACTACAAGACC ACCCCCCCTGTGCTGGACAGCGACGGCTCATTCTTCCTGTACTCCAAGCTGACA GTGGACAAGTCCCGGTGGCAGCAGGGCAACGTGTTCAGCTGCAGCGTGATGCA CGAGGCCCTGCACAACCACTACACCCAGAAGTCCCTGAGCCTGAGCCCCGGCA AGAGAGCCAAGAGAGGATCTGGCGAGGGCAGAGGCAGCCTGCTGACATGTGG CGACGTGGAAGAGAACCCAGGCCCTATGGGAGTGAAAGTGCTGTTTGCTCTGA TCTGCATTGCTGTGGCTGAAGCCGACATCCAGATGACCCAGAGCCCCTCTAGC CTGAGCGCCAGCGTGGGCGACAGAGTGACCATCACATGCAGAGCCAGCCAGG GCATCCGGAACTACCTGGCCTGGTATCAGCAGAAGCCCGGCAAGGCCCCTAAG CTGCTGATCTACGCCGCCTCCACACTGCAGAGCGGAGTGCCCTCCAGATTTTCC GGCAGCGGCTCCGGCACCGACTTCACCCTGACAATCAGCTCCCTGCAGCCAGA GGACGTGGCCACCTACTACTGCCAGCGGTACAACAGAGCCCCCTACACCTTCG GACAGGGCACAAAGGTGGAAATCAAGACCGTGGCCGCTCCCTCCGTGTTCATC TTCCCACCTAGCGACGAGCAGCTGAAGTCCGGCACAGCCTCTGTCGTGTGCCT GCTGAACAACTTCTACCCTCGGGAAGCCAAGGTGCAGTGGAAAGTGGATAAC GCCCTGCAGTCCGGCAACTCCCAGGAAAGCGTGACCGAGCAGGACAGCAAGG ATAGCACCTACAGCCTGTCCTCCACCCTGACCCTGTCCAAGGCCGACTACGAG AAGCACAAGGTGTACGCCTGTGAAGTGACCCACCAGGGCCTGTCCAGCCCCGT GACCAAGAGCTTCAACCGGGGCGAGTGTAGGGCCAAGAGGGGCGCCtaattctaga).

Amino acid sequence with annotation:

MGVKVLFALICIAVAEAEVQLVESGGGLVQPGRSLRLSCAASGFTFDDYAMHWV

Supplementary Table 2. Amount of transfected plasmids used in different experiments

MATHEMATICAL MODEL

Deterministic ODE model

To predict the responsiveness of the device to stimuli and determine the optimal transfection amounts, we constructed a simple deterministic model with ordinary differential equations (ODEs) using CellDesigner 4.4 software¹³. First we constructed a state transition diagram representing the genetic circuit (Supplementary Fig. 2). Next, we characterized the state transitions with the mass action kinetic law.

The formation of a complex between a transcription factor (TF) and its corresponding response element on DNA was expressed as:

$$
\frac{d[TF\text{-}DNA]}{dt} = k_a \cdot [TF] \cdot [DNA] - k_d \cdot [TF\text{-}DNA]
$$

where k_a represents the on-rate constant and k_d represents the off-rate constant.

For protein (P) production, we assumed first-order kinetics:

$$
\frac{d[P]}{dt} = k_s \cdot [TF\text{-}DNA]
$$

and

$$
\frac{d[P]}{dt} = k_l \cdot [DNA]
$$

The protein production rate constant is described with k_s . Parameter k_l corresponds to leaky protein production constant that represents the basal protein synthesis from transcribed genes under the control of an uninduced minimal promoter.

Proteins are degraded to amino acids (aa) according to the first order kinetics:

$$
k_{deg} \cdot [P]
$$

where k_{deg} corresponds to the protein degradation constant.

We also took into account the dilution of the device's genetic components due to cell division with dilution constant *kdil*, which corresponds to the cell doubling time.

k_{dil} • [DNA]

As protein turnover is faster than the typical cell doubling $(k_{di} < k_{deg})$, we neglected the dilution of protein moieties.

Furthermore, we assumed the amount of amino acids remained constant over the course of simulation. Thus, the model species amino acids ("aa") served as a source and a sink for protein production and degradation, respectively. Conversely, the species "lost" represented a sink for the DNA constructs lost due to the dilution by cell division. These two model species were defined as boundary conditions in the CellDesigner state transition model (see Supplementary Table 3).

Simulations

The simulations were performed using the integrated SBML ODE Solver¹⁴. We were particularly interested in a behavior of the device in the two limiting cases: where there was no input signal (non-stimulated), i.e. the NF-κB protein complex particle number was set to zero, and where the input signal had maximal value (stimulated). The NF-κB particle number in simulations with stimulated genetic device was set to 24 000 by taking the mean nuclear NF- κ B concentration of roughly 40 nM in persistently stimulated cells¹⁵ and estimating the volume of a cell nucleus to be $1 \cdot 10^{-12}$ L.

$$
N(NF\text{-}\kappa B)=c\cdot V\cdot N_A\approx 24\ 000
$$

The initial quantities of genetic constructs per individual cell were estimated by taking into account the efficiency of transient transfection with polyethylenimine (PEI) and the amount of DNA·PEI complexes that are successfully trafficked to the nucleus. We estimated that 90 % of the cells $(4.10^4 \text{ cells per well in a 96-well plate})$ receive the plasmids and that 0.07 % of the initial DNA quantity reach the nucleus^{16,17}.

$$
N(DNA) = \frac{m(DNA) \cdot 7 \cdot 10^{-4}}{M(DNA) \cdot N(cells) \cdot 0.9} \cdot N_A
$$

The time $t = 0$ in the simulations corresponds to the transfection of the cells with DNA constructs. In time course simulations, the particle number of NF-κB was held at 24 000 for the duration of stimulation (24 h post transfection to the end of the experiment at 48 h time point post transfection), similar to the experiments with cell cultures. In parameter scan experiments, the input signal for stimulated genetic device had maximal value for the duration of the simulation (24 h).

Supplementary Table 3. List of species included in the deterministic model exported from CellDesigner 4.4 software

Class	id	Name	Initial quantity number; <i>(particle</i> N)	Boundary condition	Comment
${\tt GENE}$	s1	sensor	2.2	false	The sensor construct (pAS60).
GENE	s19	amplifier	2.2	false	The amplifier construct (pAS62).
GENE	s28	effector	181.8	false	luciferase effector The construct (pAS51).
GENE	s15	repressor	8.1	false	inducible OFF-switch The construct (pAS58).
GENE	s29	thresholder	425.1	false	"thresholder" construct The (pAS67).
PROTEIN	s54	GV16	0.0	false	The Gal4-VP16 transcriptional activator.
PROTEIN	s11	rtTR-KRAB*	0.0	false	doxycycline-induced The rtTR-KRAB active transcriptional repressor.
PROTEIN	s45	NF-_kappa_B	0.0	false	The NF-KB represents the input signal for the device. In the non-stimulated setting, the quantity initial was $\overline{0}$. Conversely, in simulations of the induced genetic device, the initial quantity was set to 24 000 (estimated from ref. ¹⁵).

Supplementary Table 4. List of parameters included in the deterministic model exported

from CellDesigner 4.4 software

Supplementary Table 5. List of reactions included in the deterministic model exported

from CellDesigner 4.4 software

SUPPLEMENTARY REFERENCES

- 1. King, GA, Daugulis, AJ, Faulkner, P and Goosen, MFA. (1987). Alginate-Polylysine Microcapsules of Controlled Membrane Molecular Weight Cutoff for Mammalian Cell Culture Engineering. *Biotechnol. Prog.* **3**: 231–240.
- 2. Dubrot, J, Portero, A, Orive, G, Hernández, RM, Palazón, A, Rouzaut, A, *et al.* (2010). Delivery of immunostimulatory monoclonal antibodies by encapsulated hybridoma cells. *Cancer Immunol. Immunother.* **59**: 1621–1631.
- 3. Wirtz, S, Neufert, C, Weigmann, B and Neurath, MF (2007). Chemically induced mouse models of intestinal inflammation. *Nat. Protoc.* **2**: 541–546.
- 4. Fussenegger, M, Morris, RP, Fux, C, Rimann, M, von Stockar, B, Thompson, CJ, *et al.* (2000). Streptogramin-based gene regulation systems for mammalian cells. *Nat. Biotechnol.* **18**: 1203–1208.
- 5. Sadowski, I, Ma, J, Triezenberg, S and Ptashne, M (1988). GAL4-VP16 unusualy potent transcription activator. *Nature* **335**: 563–564.
- 6. Szulc, J, Wiznerowicz, M, Sauvain, M, Trono, D and Aebischer, P (2006). A versatile tool for conditional gene expression and knockdown. *Nat. Methods* **3**.
- 7. Fussenegger, M, Mazur, X and Bailey, JE (1997). A Novel Cytostatic Process Enhances the Ovary Cells. *Biotechnol Bioeng*. **20**:927-939.
- 8. Lebar, T, Straz, M, Bezeljak, U, Golob, A, Jerala, M, Kadunc, L, *et al.* (2014). A bistable genetic switch based on designable DNA-binding domains. **29**: 5007
- 9. Gibson, DG, Young, L, Chuang, R-Y, Venter, JC, Hutchison, CA and Smith, HO (2009). Enzymatic assembly of DNA molecules up to several hundred kilobases. *Nat. Methods* **6**: 343–345.
- 10. Kim, JH, Lee, SR, Li, LH, Park, HJ, Park, JH, Lee, KY, *et al.* (2011). High cleavage efficiency of a 2A peptide derived from porcine teschovirus-1 in human cell lines, zebrafish and mice. *PLoS One* **6**: 1–8.
- 11. Stern, B, Olsen, LC, Tröße, C, Ravneberg, H and Pryme, IF (2007). Improving mammalian cell factories : The selection of signal peptide has a major impact on recombinant protein synthesis and secretion in mammalian cells. *Trends Cell Mol. Biol.* **2**: 1–17.
- 12. Abbott Biotechnology Ltd. Human antibodies that bind human $TNF\alpha$. US Patent 6,090,382 filed 9 Feb. 1996, and issued 18 Jul. 2000.
- 13. Funahashi, A, Morohashi, M, Kitano, H and Tanimura, N (2003). CellDesigner: a process diagram editor for gene-regulatory and biochemical networks. *Biosilico* **1**: 159–162.
- 14. Machné, R, Finney, A, Müller, S, Lu, J, Widder, S and Flamm, C (2006). The SBML ODE Solver Library: A native API for symbolic and fast numerical analysis of reaction networks. *Bioinformatics* **22**: 1406–1407.
- 15. Hoffmann, A, Levchenko, A, Scott, ML and Baltimore, D (2002). The IkappaB-NFkappaB signaling module: temporal control and selective gene activation. *Science* **298**: 1241–1245.
- 16. Kichler, A, Leborgne, C, Coeytaux, E and Danos, O (2001). Polyethyleniminemediated gene delivery: A mechanistic study. *J. Gene Med.* **3**: 135–144.
- 17. Pollard, H, Remy, JS, Loussouarn, G, Demolombe, S, Behr, JP and Escande, D (1998). Polyethylenimine but not cationic lipids promotes transgene delivery to the nucleus in mammalian cells. *J. Biol. Chem.* **273**: 7507–7511.
- 18. Hong, M, Fitzgerald, MX, Harper, S, Luo, C, Speicher, DW and Marmorstein, R (2008). Structural Basis for Dimerization in DNA Recognition by Gal4. *Structure* **16**: 1019–1026.
- 19. Bergqvist, S, Alverdi, V, Mengel, B, Hoffmann, A, Ghosh, G and Komives, E a (2009). Kinetic enhancement of NF-kB - DNA dissociation by IkBa. **2009**: 1–6.
- 20. Eden, E, Geva-Zatorsky, N, Issaeva, I, Cohen, A, Dekel, E, Danon, T, *et al.* (2011). Proteome half-life dynamics in living human cells. *Science* **331**: 764–768.
- 21. Sotiropoulos, V and Kaznessis, YN (2007). Synthetic tetracycline-inducible regulatory networks: computer-aided design of dynamic phenotypes. *BMC Syst. Biol.* **1**: 7.
- 22. Ignowski, JM and Schaffer, D V. (2004). Kinetic analysis and modeling of firefly luciferase as a quantitative reporter gene in live mammalian cells. *Biotechnol. Bioeng.* **86**: 827–834.
- 23. Salghetti, SE, Muratani, M, Wijnen, H, Futcher, B and Tansey, WP (2000). Functional overlap of sequences that activate transcription and signal ubiquitin-mediated proteolysis. *Proc. Natl. Acad. Sci. U. S. A.* **97**: 3118–3123.