

## Appendix

### A1) Mathematic formulation of the connected steady state system

For our derivation we start with event-based argumentation. The general expression is:

$$F_n = \beta (C_B - C_n) \quad (1a)$$

$$C_{n+1} = C_n + k' F_n \quad (1b)$$

where  $\beta := \mathcal{D} * L^{-1}$ ;  $k' := \frac{1}{v}$ ;  $C_B := C_{blood}$  and  $n \in \mathbb{N}$ . Substituting (1a) into (1b) yields:

$$C_{n+1} = C_n + \Delta (C_B - C_n) = C_n (1 - \Delta) + \Delta C_B.$$

where  $\Delta := k' * \beta$ . Thus  $(C_n)_{n \in \mathbb{N}}$  is an arithmetico-geometric sequence with the recursive relation:

$$C_{n+1} = aC_n + b$$

where  $a := 1 - \Delta$ ;  $b := \Delta * C_B$ . Observe that  $0 < a < 1$  and  $C_0 = 0$  (see Section Formulation of the Connected Steady State Model) and put  $r := \frac{b}{1-a} = C_B$ . It is well known that  $(C_n)_{n \in \mathbb{N}}$  admits the explicit formula:

$$C_n = a^n(C_0 - r) + r = -ra^n + r.$$

Now let  $k'_N := \frac{k'}{N}$  for fixed  $N \in \mathbb{N}$  and let  $(C_{N,n})_{n \in \mathbb{N}}$ ,  $(F_{N,n})_{n \in \mathbb{N}}$  be the corresponding sequences for the concentration and diffusional flux at time  $\frac{n}{N}$ .

As seen above we have

$$C_{N,n+1} = C_{N,n} + k'_N F_{N,n}$$

such that

$$C_{N,n+1} = a_N C_{N,n} + b_N$$

where  $a_N := 1 - \frac{\Delta}{N}$ ;  $b_N := \frac{\Delta}{N} * C_B$ , thus

$$C_{N,n} = (a_N)^n(C_0 - r_N) + r_N = -r_N(a_N)^n + r_N$$

where  $r_N := \frac{b_N}{1-a_N} = C_B$ .

Therefore, a given time  $t = ns = \frac{tN}{N}$  (n being a real number) corresponds to  $n * N$  events of length  $\frac{1}{N} s$  so that we get by approximation for the exact concentration  $C(t)$ :

$$\begin{aligned}
C(t) &= \lim_{N \rightarrow \infty} C_{N,n*N} = \lim_{N \rightarrow \infty} -C_B \left(1 - \frac{k' \beta}{N}\right)^{n*N} + C_B \\
&= \lim_{N \rightarrow \infty} -C_B \left[ \left(1 - \frac{k' \beta}{N}\right)^N \right]^n + C_B \\
&= -C_B e^{-k' \beta n} + C_B \\
&= -C_B e^{-k \beta t} + C_B
\end{aligned}$$

with  $k := \frac{k'}{1s}$ . This also implies the relation for the diffusional flux  $F(t)$  at time  $t$

$$F(t) = \beta(C_B - C(t)) = \beta C_B e^{-k \beta t}$$

Seen on relative levels yields:

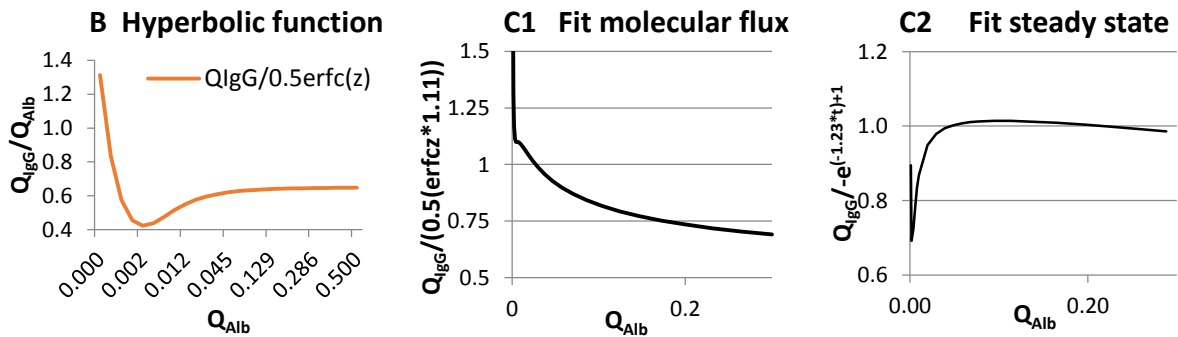
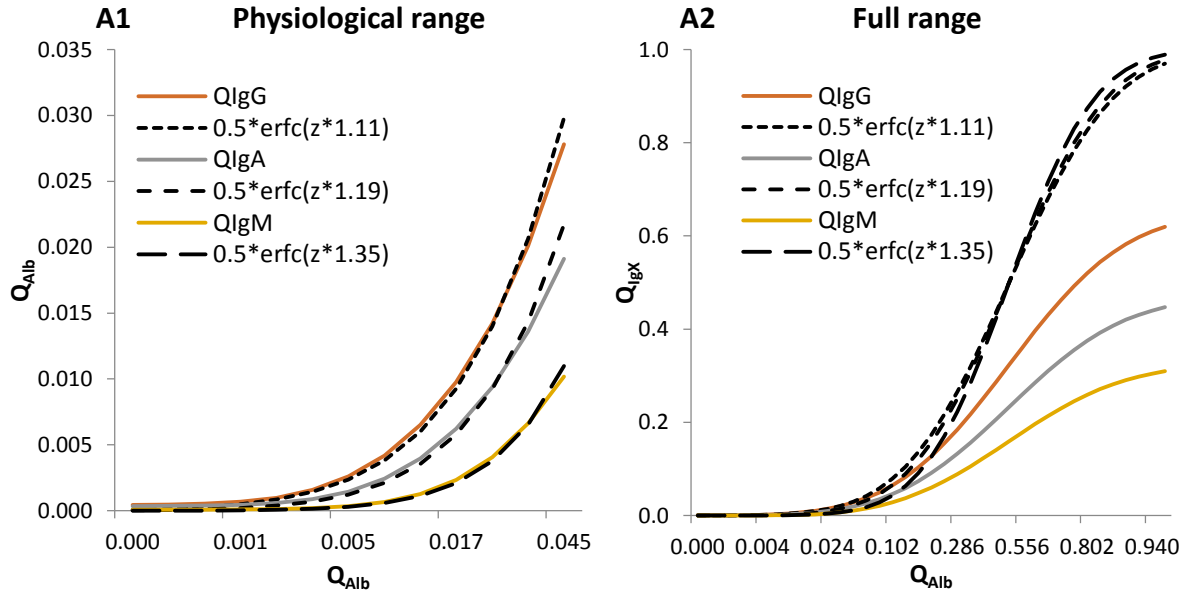
$$\frac{C_{CSF}(t)}{C_{blood}} = \frac{-C_B e^{-k \beta t} + C_B}{C_B} = -e^{-\frac{\beta}{L} k t} + 1 \quad \text{A1}$$

And analogously for the molecular flux:

$$\frac{F_{CSF}(t)}{F_{initial}} = \frac{\beta C_B e^{-k \beta t}}{\beta C_B} = e^{-\frac{\beta}{L} k t} \quad \text{A2}$$

**A2) The conformity of the molecular flux theory and the connected steady state model to the hyperbolic function and their valid range**

**A Molecular flux model - fit to the hyperbolic function**



**Fig. 5. Curve discussion.** A: The function  $0.5 \operatorname{erfc}(z)$ ,  $z = \frac{x}{2\sqrt{D_{Alb}t}}$ , derived from the molecular flux model (Equation 3, Section The Molecular Flux Theory) fitted to the hyperbolic functions for IgG/A/M (Equation 1, Table 1).  $Q_{Alb}$  is represented by  $0.5 \operatorname{erfc}(z)$ . The fitting procedure, see Equations A3/4, is the same as described for the connected steady state system (Section Validation of the Connected-Steady State Model, Equation 12/13).

**A1:** Like the connected steady state model (Figure 3B), the molecular flux model is also adjustable to the hyperbolic function in a certain physiological range.

**A2:** The fit shown over the whole range  $0 \leq Q_{Alb} \leq 1$  shows several aspects: 1. Outside the overlapping range, the  $0.5 \operatorname{erfc}(z)$  function deviates considerably from the hyperbolic function. 2. At  $Q_{Alb} < 0.5$ ;  $Q_{lgM} < Q_{lgA} < Q_{lgG}$  but at  $Q_{Alb} > 0.5$ ;  $Q_{lgM} > Q_{lgA} > Q_{lgG}$ . This does not meet the required boundary conditions (see Section The Molecular Flux Theory and Section The Connected Steady State Model)

**B:** The empirically derived hyperbolic function is only valid in the range in which the function is fitted to the experimental data.  $0.5 \operatorname{erfc}(z)$  is used for  $Q_{Alb}$  values (every other function increasing from 0 to 1 could be used as well). At high  $Q_{Alb}$  values ( $\sim > 0.05$ ) the function tends to  $a/b$  and not to 1; this can also be observed in **Figure 5 A2** (also see Equation 1,

**Table 1).** However, theoretically at  $Q_{Alb} \rightarrow 1$   $Q_{IgX}$  must also tend to 1 and therefore  $Q_{IgG}/Q_{Alb} = 1$ . At  $Q_{Alb} \rightarrow 0$  the hyperbolic function (Equation 1) tends to a-c, resulting in  $Q_{IgG} > Q_{Alb}$  which is impossible since  $Q_{Alb}$  is the faster diffusing molecule.

**C1/2:** Shows the accordance of the empirical hyperbolic function to the two theoretically derived functions.

**C1:** Shows that the function  $0.5 \operatorname{erfc}(z)$ , representing the molecular flux theory, cannot be precisely fitted to the hyperbolic function.

**C2:** In the physiological range the connected steady state system fits precisely to the empirical function and therefore to the experimental data.

The approach to fit the equation derived from the 'molecular flux theory' (Equation 3 in Section The Molecular Flux Theory) to the hyperbolic function (Equation 1) is the same as described for the connected steady state model (Section Validation of the Connected-Steady State Model, Equation 12/13). Equation A3 represents the theoretical function (Equation 3) and Equation A4 represents the empirical hyperbolic function (Equation 1).

$$\overline{Q_{IgX}} = \frac{1}{2} \operatorname{erfc} \left( \frac{x}{2\sqrt{D_{Alb}t}} \sqrt{\frac{D_{Alb}}{D_{IgX}}} \right) = \frac{1}{2} \operatorname{erfc} \left( z * \sqrt{\frac{D_{Alb}}{D_{IgX}}} \right) \quad \text{A3}$$

$$\overline{Q_{IgX}} = \frac{a}{b} \sqrt{\frac{1}{2} \operatorname{erfc}(z) + b^2 - c} \quad \text{A4}$$

with  $z = \frac{x}{2\sqrt{D_{Alb}t}}$