## Supporting Information

Internal gradient distributions: A susceptibility-derived tensor delivering morphologies by magnetic resonance

Gonzalo A. Álvarez, Noam Shemesh, and Lucio Frydman

## Supporting Information 1: A formal derivation of the internal gradient distribution tensor

The normalized magnetization arising from an ensemble of non-interacting and equivalent spins under the effects of a sequence of pulses or modulating gradients is  $M(t) = \langle e^{-i\phi(t)} \rangle$ , where the brackets account for an ensemble average over the random phases  $\phi(t)$ . For the spin-echo sequences being considered in this work, the average phase  $\langle \phi(t) \rangle$  will be equal to zero. Assuming that the random phase  $\phi(t)$  has a Gaussian distribution [\[48\]](#page-9-0),  $M(t) = \exp \{-\frac{1}{2}$  $\frac{1}{2} \langle \phi^2(t) \rangle$ , the signal will evidence a decay depending on the attenuation factor  $\beta(t) = \frac{1}{2} \langle \phi^2(t) \rangle$ . With most sources of decoherence normalized out by the constanttime, constant-pulses-number, fixed-number-of-gradients nature of the NOGSE sequences assayed [\[20,](#page-7-0) [21,](#page-7-1) [44\]](#page-9-1), we ascribe to diffusion effects as the sole source of this attenuation. It is then convenient to describe the  $\beta$ -factor in terms of the gradient modulating function  $\vec{G}_{\text{tot}}(t')$  [\[45–](#page-9-2)[47\]](#page-9-3):

<span id="page-0-0"></span>
$$
\beta(TE) = \frac{\gamma^2}{2} \int_0^{TE} dt' \int_0^{TE} dt'' \vec{G}_{\text{tot}}^\dagger(t') \cdot \langle \vec{r}(t') \vec{r}(t'') \rangle \cdot \vec{G}_{\text{tot}}(t'')
$$
(S.1)

$$
= \frac{\gamma^2}{2} \int_{-\infty}^{\infty} dt' \int_{-\infty}^{\infty} dt'' \vec{G}_{\text{tot}}^{\dagger}(t', TE) \cdot \mathbf{g}(t'' - t') \cdot \vec{G}_{\text{tot}}(t'', TE), \tag{S.2}
$$

where in the second equation we redefined the gradient modulation function such that  $\vec{G}_{\text{tot}}(t',TE) = 0$  if  $t' < 0$  or  $t' > TE$  (i.e., outside the total evolution time range). The evolution is given in terms of a tensorial correlation function reflecting the displacements' fluctuations  $\mathbf{g}(\tau) = \langle \Delta \vec{r}(t') \Delta \vec{r}(t' + \tau) \rangle$ ; i.e.  $g_{i,j} = \langle \Delta x_i(t') \Delta x_j(t' + \tau) \rangle$  with i, j representing the spatial axis  $x, y, z$ . This correlation function can be related to a diffusion power spectrum  $\mathbf{D}(\omega)$  [\[4,](#page-6-0) [5,](#page-6-1) [45,](#page-9-2) [46\]](#page-9-4) by a Fourier transform:  $\mathcal{FT}$  {g( $\tau$ )} / √  $\overline{2\pi} = \mathbf{D}(\omega)/\omega^2$ . In the event of anisotropic diffusion, Eq.  $(S.1)$  can thus be recast in its Fourier representation  $[45-47]$  $[45-47]$  as:

$$
\beta(TE) = \frac{\gamma^2}{2} \int_{-\infty}^{\infty} d\omega \vec{\mathcal{G}}_{\text{tot}}^{\dagger}(\omega, TE) \cdot \frac{\mathbf{D}(\omega)}{\omega^2} \cdot \vec{\mathcal{G}}_{\text{tot}}(\omega, TE), \tag{S.3}
$$

where  $\vec{\mathcal{G}}_{\text{tot}}(\omega, TE) = \vec{\mathcal{G}}(\omega, TE) + \vec{\mathcal{G}}_0(\omega, TE)$ , is the filter function introduced in Eq. (1) of the main text.

Considering the applied gradient modulation  $\vec{G}(t', TE)$ , the internal background gradient modulation  $\vec{G}_0(t',TE)$ , and their respective filter functions  $\vec{\mathcal{G}}(\omega, TE)$  and  $\vec{\mathcal{G}}_0(\omega, TE)$ , the argument of the integral defining this attenuation factor can then be expanded as

$$
\vec{G}_{\text{tot}}^{\dagger}(\omega, TE) \cdot \frac{\mathbf{D}(\omega)}{\omega^2} \cdot \vec{\mathcal{G}}_{\text{tot}}(\omega, TE) = \underbrace{\vec{\mathcal{G}}^{\dagger}(\omega, TE)}_{\text{external gradient dephasing}} \cdot \frac{\mathbf{D}(\omega)}{\omega^2} \cdot \vec{\mathcal{G}}(\omega, TE) \cdot \frac{\mathbf{D}(\omega)}{\omega^2} \cdot \vec{\mathcal{G}}_{0}(\omega, TE) \cdot \frac{\mathbf{D}(\omega)}{\omega^2} \cdot \vec{\math
$$

This leads to Eq. (2) of the main text, where  $\beta(TE) = \beta_{G^2}(TE) + \beta_{G_0^2}(TE) + \beta_{\vec{G}\cdot\vec{G}_0}(TE)$ and the normalized spin magnetization becomes

<span id="page-1-0"></span>
$$
M(TE) = M_{G^2}(TE) \times M_{G_0^2}(TE) \times M_{\vec{G}.\vec{G}_0}(TE). \tag{S.5}
$$

Assuming a  $\vec{G}(t', TE) = \vec{G} f(t', TE)$ , involving a strength vector  $\vec{G}$  and a timedependency  $f(t', TE)$ , then  $\vec{\mathcal{G}}(\omega, TE) = \vec{G} F(\omega, TE)$  with  $F(\omega, TE)$  the Fourier transform of  $f(t', TE)$ . The applied gradient diffusion attenuation becomes

$$
M_{G^2}(TE) = \exp\{-\beta_{G^2}(TE)\},\tag{S.6}
$$

where

<span id="page-1-1"></span>
$$
\beta_{G^2}(TE) = \frac{\gamma^2 G^2}{2} \int_{-\infty}^{\infty} d\omega \frac{D_G(\omega)}{\omega^2} |F(\omega, TE)|^2, \qquad (S.7)
$$

and  $D_G(\omega) = \left[\vec{G}^\dagger \cdot \mathbf{D}(\omega) \cdot \vec{G}\right] / G^2$ . Likewise, the pure background gradient decay is independent of the applied gradient

$$
M_{G_0^2}(TE) = \exp\left\{-\beta_{G_0^2}(TE)\right\},\tag{S.8}
$$

where

$$
\beta_{G_0^2}(TE, \vec{G}_0) = \frac{\gamma^2 G_0^2}{2} \int_{-\infty}^{\infty} d\omega \frac{D_{G_0}(\omega)}{\omega^2} |F_0(\omega, TE)|^2, \qquad (S.9)
$$

with  $D_{G_0}(\omega) = \left[\vec{G}_0^{\dagger} \cdot \mathbf{D}(\omega) \cdot \vec{G}_0\right] / G_0^2$ , and we have again assumed that  $\vec{G}_0(t', TE)$  $\vec{G}_0 f_0(t', TE)$  and thereby  $\vec{\mathcal{G}}_0(\omega, TE) = \vec{G}_0 F_0(\omega, TE)$ . Finally, the cross-term attenuation will be

<span id="page-2-0"></span>
$$
\beta_{\vec{G}\cdot\vec{G}_0} \left( TE, \vec{G}, \vec{G}_0 \right) = \frac{\gamma^2}{2} \vec{G}^{\dagger} \cdot \left[ \int_{-\infty}^{\infty} d\omega \, 2 \text{Re} \left\{ F^{\dagger}(\omega, TE) \, \frac{\mathbf{D}(\omega)}{\omega^2} \, F_0 \left( \omega, TE \right) \right\} \right] \cdot \vec{G}_0 = \vec{G}^{\dagger} \cdot \tilde{\mathbf{D}} \cdot \vec{G}_0,
$$
\n(S.10)

where  $\tilde{\mathbf{D}} = \frac{\gamma^2}{2}$  $\frac{\gamma^2}{2} \left[ \int_{-\infty}^{\infty} d\omega \, 2 \text{Re} \left\{ F^{\dagger}(\omega, TE) \, \frac{\mathbf{D}(\omega)}{\omega^2} \, F_0 \left( \omega, TE \right) \right\} \right].$ 

Our derivations also assumed that  $\vec{G}_0$  can be described by a Gaussian distribution. The cross-term contribution to the attenuation factor turns out to be

$$
\beta_{\vec{G}\cdot\vec{G}_0}(TE) = \vec{G}^{\dagger} \cdot \tilde{\mathbf{D}} \cdot \left\langle \vec{G}_0 \right\rangle + \vec{G}^{\dagger} \cdot \tilde{\mathbf{D}} \cdot \left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle \cdot \tilde{\mathbf{D}} \cdot \vec{G},
$$
\n(S.11)

where  $\Delta \vec{G}_0 = \vec{G}_0 - \langle \vec{G}_0 \rangle$  and  $\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \rangle$  is the internal gradient-distribution tensor (IGDT). This second term is always positive, since it is a quadratic term, while the first term depends on the relative sign of the parallel component of  $\begin{bmatrix} \vec{G}^{\dagger} \cdot \tilde{\mathbf{D}} \end{bmatrix}$ to the background gradient  $G_0$ .

For an isotropic diffusion  $\mathbf{D}(\omega) = D(\omega)\mathbf{I}$ , the attenuation factor get the simplified form

$$
\beta_{\vec{G}\cdot\vec{G}_0}(TE) = \tilde{D}_{\text{iso}}\vec{G}^{\dagger}\cdot\left\langle \vec{G}_0 \right\rangle + \tilde{D}_{\text{iso}}^2 \vec{G}^{\dagger}\cdot\left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle \cdot \vec{G},
$$
\n(S.12)\n
$$
\left[ \int_{-\infty}^{\infty} d\omega \, 2\text{Re} \left\{ F^{\dagger}(\omega, TE) \, \frac{D(\omega)}{\omega^2} \, F_0(\omega, TE) \right\} \right].
$$

where  $\tilde{D}_{\text{iso}} = \frac{\gamma^2}{2}$  $\int_{2}^{2}$   $\int_{-\infty}^{\infty} d\omega 2 \text{Re } \left\{$  $\frac{\partial (\omega)}{\omega^2}$   $F_0$   $(\omega, TE)$ oi.

As an example on the use of this formalism, we consider the sequence of Fig. 1 of the main text and assume free diffusion to derive Eq. (3-5) of the main text. For free diffusion only the tail of the displacement power spectrum  $D(\omega) \propto 1/\omega^2$  is important [\[20,](#page-7-0) [44\]](#page-9-1). The purely applied-gradient diffusion term  $M_{G^2}(TE)$  is as derived for a CPMG sequence [\[44\]](#page-9-1)

$$
M_{G^2}(TE) = \exp\left\{-\frac{1}{12}\gamma^2 G^2 D_0 \frac{TE^3}{N^2}\right\},
$$
\n(S.13)

where the delay  $x = TE/N$ . The pure background gradient decay term is in turn the one that corresponds to a spin-echo modulation [\[44\]](#page-9-1)

$$
M_{G_0^2}(TE, N) = \exp\left\{-\frac{1}{12}\gamma^2 G_0^2 D_0 TE^3\right\},
$$
\n(S.14)

which is independent of  $x$ . The cross-term signal-decay contribution is calculated from Eq. [\(S.10\)](#page-2-0) leading to

$$
M_{\vec{G}\cdot\vec{G}_0} (TE) = \exp\left\{\frac{1}{4}\gamma^2 \vec{G} \cdot \vec{G}_0 D_0 \frac{TE^3}{N^2}\right\}.
$$
 (S.15)

Supporting Information 2: sNOGSE/aNOGSE's: Analytical attenuation expressions for the general case of anisotropic diffusion

We calculate next the normalized spin signal arising from Eq.  $(S.5)$ ,

$$
M_{a}^{(s)NOGSE}(TE) = M_{G^2}^{(s)NOGSE}(TE) \times M_{G_0^2}(TE) \times M_{\vec{G}.\vec{G}_0}^{(s)NOGSE}(TE),
$$
 (S.16)

for the symmetric and asymmetric non-uniform gradient spin echo modulations  $\binom{8}{3}$ a NOGSE) introduced in Fig. 2. As described in the main text,

<span id="page-3-0"></span>
$$
M_{G^2}^{sNOGSE}(TE) = M_{G^2}^{aNOGSE}(TE)
$$
\n
$$
(S.17)
$$

as a result of

<span id="page-3-1"></span>
$$
F^{\text{sNOGSE}}(\omega, TE) = F^{\text{aNOGSE}}(\omega, TE) \tag{S.18}
$$

in Eq. [\(S.7\)](#page-1-1). The pure background gradient signal contribution is therefore independent of the applied gradient modulation and direction, providing the same weight for both NOGSE sequences. The cross-term in the attenuation factor for sNOGSE is zero but that for aNOGSE is not, as the products  $F^{sNOGSE\dagger}(\omega, TE) F_0(\omega, TE)$  and  $F^{aNOGSE\dagger}(\omega, TE) F_0(\omega, TE)$  in Eq. [\(S.10\)](#page-2-0) are odd and even functions of  $\omega$ , respectively. This cross-term between the aNOGSE-modulated applied gradient and the background gradient  $G_0$  will be

$$
\beta_{\vec{G}\cdot\vec{G}_0}(TE) = \frac{\gamma^2}{2}\vec{G}\cdot\left[\int_{-\infty}^{\infty} d\omega \, 2\text{Re}\left\{ \left(F^{aNOGSE}(\omega, TE)\right)^{\dagger} \, \frac{\mathbf{D}(\omega)}{\omega^2} \, F_0\left(\omega, TE\right) \right\} \right] \cdot \vec{G}_0 = \vec{G}\cdot\tilde{\mathbf{D}}\cdot\vec{G}_0. \tag{S.19}
$$

As explained in the main text, the measured spin signal decays for the sNOGSE and aNOGSE sequences as described in Fig. 2e, factor out all non-diffusing sources of decoherence after normalizing them by the single-echo signal [\[20,](#page-7-0) [21,](#page-7-1) [44\]](#page-9-1). The amplitude of the

## NOGSE modulation is then

$$
M_{CPMG}(TE)/M_{Single-echo}(TE) = \exp(-\Delta\beta) = \exp\left[-\left(\beta^{CPMG} - \beta^{Single-echo}\right)\right], \quad (S.20)
$$

where the amplitude contrast of the attenuation factors  $\Delta \beta = \beta^{CPMG} - \beta^{Single-echo}$ . As the contribution to the attenuation factor that purely depends of the background gradient is independent of the applied gradient modulation its contribution  $\Delta\beta_{G_0^2}$  is null, and the amplitude of the attenuation factors is then

$$
\Delta \beta = \Delta \beta_{G^2} + \Delta \beta_{\vec{G} \cdot \vec{G}_0}.
$$
\n(S.21)

For the sNOGSE sequence  $\Delta\beta^s = \Delta\beta_{G^2}$  as the cross-term is null, and  $\Delta\beta^a = \Delta\beta_{G^2}$  +  $\Delta\beta_{\vec{G}\cdot\vec{G}_0}$  for the aNOGSE modulation curve. Notice that the contribution of the term that only depends of the applied gradient  $\Delta\beta_{G^2}$  is the same for both sequences according to Eqs. [\(S.17\)](#page-3-0) and [\(S.18\)](#page-3-1). Then by subtracting  $\Delta\beta^a$  and  $\Delta\beta^s$ , the  $\Delta\beta_{\vec{G}\cdot\vec{G}_0}$  cross-term contribution to the amplitude modulation is obtained, where

$$
\Delta\beta_{\vec{G}\cdot\vec{G}_0} = \frac{\gamma^2}{2}\vec{G} \cdot \left[ \int_{-\infty}^{\infty} d\omega \, 2\text{Re} \left\{ \left[ F^{aNOGSE}(\omega, TE) - F^{sNOGSE}(\omega, TE) \right]^{\dagger} \frac{\mathbf{D}(\omega)}{\omega^2} F_0(\omega, TE) \right\} \right] \cdot \vec{G}_0
$$

$$
(S.22)
$$

$$
=\vec{G}\cdot\Delta\tilde{\mathbf{D}}\cdot\vec{G}_0,\tag{S.23}
$$

with  $\Delta \tilde{\mathbf{D}} = \frac{\gamma^2}{2}$  $\frac{\gamma^2}{2} \int_{-\infty}^{\infty} d\omega \, 2 \text{Re} \left\{ \left[ F^{aNOGSE}(\omega, TE) - F^{sNOGSE}(\omega, TE) \right]^{\dagger} \frac{\mathbf{D}(\omega)}{\omega^2} F_0(\omega, TE) \right\}$ . Assuming as before a Gaussian distribution for  $G_0$ ,

$$
\Delta \beta_{\vec{G} \cdot \vec{G}_0} = \vec{G} \cdot \Delta \tilde{\mathbf{D}} \cdot \left\langle \vec{G}_0 \right\rangle + \vec{G} \cdot \Delta \tilde{\mathbf{D}} \cdot \left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle \cdot \Delta \tilde{\mathbf{D}} \cdot \vec{G}.
$$
 (S.24)

where the first term depends on the relative sign of the parallel component of  $\left[\vec{G}\cdot\mathbf{D}(\omega)\right]$ k to the background gradient  $G_0$ , which depends of the anisotropic restricted-diffusion weighting. Notice that the second term is always positive and it contains the IGDT  $\left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle$ . This was the expression used to evaluate the results presented in Fig. 4 after being normalized by  $\Delta\beta^s = \Delta\beta_{G^2}$  to remove the anisotropic weighting due to restricted diffusion effects. For an isotropic diffusion  $\mathbf{D}(\omega) = D(\omega)\mathbf{I}$ , this gets simplified to

$$
\Delta\beta_{\vec{G}\cdot\vec{G}_0} = \Delta\tilde{D}_{\text{iso}}\vec{G}\cdot\left\langle \vec{G}_0 \right\rangle + \Delta\tilde{D}_{\text{iso}}^2\vec{G}\cdot\left\langle \Delta\vec{G}_0\Delta\vec{G}_0 \right\rangle \cdot \vec{G}.\tag{S.25}
$$

where  $\Delta \tilde{D}_{\text{iso}} = \frac{\gamma^2}{2}$  $\frac{\gamma^2}{2} \int_{-\infty}^{\infty} d\omega \, 2 \text{Re} \left\{ \left[ F^{aNOGSE}(\omega, TE) - F^{sNOGSE}(\omega, TE) \right]^{\dagger} \, D(\omega) \, F_0 \left( \omega, TE \right) \right\}.$ 

## Supporting Information 3: sNOGSE/aNOGSE analytical expressions for the case of free, unrestricted diffusion

For free diffusion only the tail of the displacement power spectrum  $D(\omega) \propto 1/\omega^2$  will be important, as it is this short-times regime active before restriction effects are seen, that matters [\[20,](#page-7-0) [44\]](#page-9-1). The purely applied-gradient diffusion term  $M_{G^2}^{s}^{s}$  (TE) is then given by [\[44\]](#page-9-1)

$$
M_{G^2}^{(\text{s})\text{NOGSE}}(TE) = \exp\left\{-\frac{1}{12}\gamma^2 G^2 D_0 \left[ (N-2) x^3 + 2y^3 \right] \right\},\tag{S.26}
$$

where  $(N-2)x+2y = TE_{NOGSE} = TE/2$  (see Fig. 2 of the main text for definitions). The pure background gradient decay term is in turn

$$
M_{G_0^2}(TE, N) = \exp\left\{-\frac{1}{12}\gamma^2 G_0^2 D_0 TE^3\right\},
$$
\n(S.27)

which is independent of  $x$  and  $y$ , and therefore of the applied gradient modulation as was mentioned in the manuscript.

The cross-term signal-decay contribution for sNOGSE is zero as described before, and the one for aNOGSE will be

<span id="page-5-0"></span>
$$
M_{\vec{G}\cdot\vec{G}_0}^{aNOGSE} (TE) = \exp\left\{-\frac{1}{4}\gamma^2 \vec{G}\cdot\vec{G}_0 D_0 TE_{NOGSE} (-1)^{N/2} \left[2y^2 - \left(1 + (-1)^{N/2}\right)x^2\right]\right\}.
$$
\n(S.28)

Notice that the sign of the attenuation factor for this cross-term contribution depends of the relative sign of  $G_{\parallel}G_0$ , where  $G_{\parallel}$  is the applied component of the G-gradient that is parallel to the background gradient vector. The extremes of this attenuation arise for  $x = y =$  $TE_{NOGSE}/N$  (CPMG-like modulation)

$$
\beta_{\vec{G}\cdot\vec{G}_0}^{CPMG}(TE) = -\frac{1}{4}\gamma^2 \vec{G} \cdot \vec{G}_0 D_0 \frac{TE_{NOGSE}^3}{N^2} \left( (-1)^{N/2} - 1 \right),\tag{S.29}
$$

and for  $y = TE_{NOGSE}/2$  and  $x = 0$  (single-echo modulation)

$$
\beta_{\vec{G}\cdot\vec{G}_0}^{Single-echo} (TE) = -\frac{1}{8} \gamma^2 \vec{G} \cdot \vec{G}_0 D_0 TE_{NOGSE}^3 (-1)^{N/2} . \tag{S.30}
$$

Given the  $(-1)^{N/2}$  factor in Eq. [\(S.28\)](#page-5-0) it follows that if  $N/2$  is even,  $\beta_{\vec{G}\cdot\vec{G}_0}^{CPMG}(TE) = 0$  and the contrast contribution for the difference of attenuation factors is

$$
\Delta\beta_{\vec{G}\cdot\vec{G}_0} = \frac{1}{8}\gamma^2 \vec{G}\cdot\vec{G}_0 D_0 T E_{NOGSE}^3; \tag{S.31}
$$

i.e., it depends on the relative sign of  $G_{\parallel}$  and  $G_0$ . If  $N/2$  is odd  $\beta_{\vec{G}\cdot\vec{G}_0}^{CPMG}(TE) \neq 0$ ; but for  $N/2$  odd the attenuation decays with  $1/N^2$ , and this makes the contrast lower. Assuming a Gaussian distribution for  $G_0$ ,

$$
\beta_{\vec{G}\cdot\vec{G}_0}(TE) = -\frac{1}{4}\gamma^2 D_0 TE_{NOGSE}(-1)^{N/2} (2y^2 - \left(1 + (-1)^{N/2}\right)x^2) \vec{G} \cdot \langle \vec{G}_0 \rangle \n+ \frac{1}{32}\gamma^4 D_0^2 TE_{NOGSE}^2 \left[2y^2 - \left(1 + (-1)^{N/2}\right)x^2\right]^2 \langle \left[\vec{G} \cdot \left(\vec{G}_0 - \langle\vec{G}_0\rangle\right)\right]^2 \rangle. (S.32)
$$

The attenuation factor contrast amplitude is then

$$
\Delta\beta_{\vec{G}\cdot\vec{G}_0} = \frac{1}{8}\gamma^2 D_0 T E_{NOGSE}^3 \vec{G} \cdot \left\langle \vec{G}_0 \right\rangle + \frac{1}{128} \gamma^4 D_0^2 T E_{NOGSE}^6 \vec{G} \cdot \left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle \cdot \vec{G}, (S.33)
$$
  
where  $\left\langle \Delta \vec{G}_0 \Delta \vec{G}_0 \right\rangle$  is the IGDT.

- [1] Callaghan, P. T. Principles of Nuclear Magnetic Resonance Microscopy (Oxford University Press, 1993).
- [2] Price, W. S. Pulsed-field gradient nuclear magnetic resonance as a tool for studying translational diffusion: Part 1. basic theory. Concepts Magn. Reson. 9, 299–336 (1997).
- [3] Sen, P. N. Time-dependent diffusion coefficient as a probe of geometry. Concepts Magn. Reson. 23, 1–21 (2004).
- <span id="page-6-0"></span>[4] Grebenkov, D. S. NMR survey of reflected brownian motion. Rev. Mod. Phys. 79, 1077–1137 (2007).
- <span id="page-6-1"></span>[5] Gore, J. C. et al. Characterization of tissue structure at varying length scales using temporal diffusion spectroscopy. *NMR in Biomedicine* **23**, 745–756 (2010).
- [6] Mitra, P. P., Sen, P. N., Schwartz, L. M. & Le Doussal, P. Diffusion propagator as a probe of the structure of porous media. Phys. Rev. Lett. 68, 3555–3558 (1992).
- [7] Basser, P., Mattiello, J. & LeBihan, D. J. Magn. Reson., Series B 103, 247 (1994).
- [8] Basser, P., Mattiello, J. & LeBihan, D. MR diffusion tensor spectroscopy and imaging. Biophys. J. 66, 259–267 (1994).
- [9] Kukla, V. et al. NMR studies of single-file diffusion in unidimensional channel zeolites. Science 272, 702–704 (1996).
- [10] Kuchel, P. W., Coy, A. & Stilbs, P. NMR "diffusion-diffraction" of water revealing alignment of erythrocytes in a magnetic field and their dimensions and membrane transport characteristics. Magn. Reson. Med. 37, 637–643 (1997).
- [11] Mair, R. W. et al. Probing porous media with gas diffusion NMR. Phys. Rev. Lett. 83, 3324–3327 (1999).
- [12] Peled, S., Cory, D. G., Raymond, S. A., Kirschner, D. A. & Jolesz, F. A. Water diffusion, t2, and compartmentation in frog sciatic nerve. Magn. Reson. Med. 42, 911–918 (1999).
- [13] Song, Y.-Q., Ryu, S. & Sen, P. N. Determining multiple length scales in rocks. Nature 406, 178–181 (2000).
- [14] LeBihan, D. Looking into the functional architecture of the brain with diffusion MRI. Nat. Rev. Neurosci. 4, 469–480 (2003).
- [15] Song, Y.-Q., Zielinski, L. & Ryu, S. Two-dimensional NMR of diffusion systems. Phys. Rev. Lett. **100**, 248002 (2008).
- [16] Lawrenz, M. & Finsterbusch, J. Double-wave-vector diffusion-weighted imaging reveals microscopic diffusion anisotropy in the living human brain. Magn. Reson. Med. 69, 1072–1082 (2013).
- [17] Hertel, S. A. et al. Magnetic-resonance pore imaging of nonsymmetric microscopic pore shapes. Phys. Rev. E 92, 012808 (2015).
- [18] Ong, H. H. et al. Indirect measurement of regional axon diameter in excised mouse spinal cord with q-space imaging: simulation and experimental studies. Neuroimage 40, 1619–1632 (2008).
- [19] Budde, M. D. & Frank, J. A. Neurite beading is sufficient to decrease the apparent diffusion coefficient after ischemic stroke. Proc. Natl. Acad. Sci. U. S. A. 107, 14472–14477 (2010).
- <span id="page-7-0"></span>[20] Álvarez, G. A., Shemesh, N. & Frydman, L. Coherent dynamical recoupling of diffusion-driven decoherence in magnetic resonance. Phys. Rev. Lett. 111, 080404 (2013).
- <span id="page-7-1"></span>[21] Shemesh, N., Álvarez, G. A. & Frydman, L. Measuring small compartment dimensions by probing diffusion dynamics via non-uniform oscillating-gradient spin-echo (NOGSE) NMR. J. Magn. Reson. 237, 49–62 (2013).
- [22] Assaf, Y. & Basser, P. J. Composite hindered and restricted model of diffusion (CHARMED) MR imaging of the human brain. Neuroimage 27, 48–58 (2005).
- [23] Panagiotaki, E. et al. Compartment models of the diffusion MR signal in brain white matter:

A taxonomy and comparison. Neuroimage 59, 2241–2254 (2012).

- [24] Warren, W. S. et al. MR Imaging Contrast Enhancement Based on Intermolecular Zero Quantum Coherences. Science 281, 247 –251 (1998).
- [25] Sen, P. & Axelrod, S. Inhomogeneity in local magnetic field due to susceptibility contrast. J. Appl. Phys. 86, 4548–4554 (1999).
- [26] Faber, C., Pracht, E. & Haase, A. Resolution enhancement in in vivo NMR spectroscopy: detection of intermolecular zero-quantum coherences. J. Magn. Reson. **161**, 265–274 (2003).
- [27] Pathak, A., Ward, B. & Schmainda, K. A novel technique for modeling susceptibility-based contrast mechanisms for arbitrary microvascular geometries: The finite perturber method. Neuroimage 40, 1130–1143 (2008).
- [28] Wharton, S. & Bowtell, R. Whole-brain susceptibility mapping at high field: A comparison of multiple- and single-orientation methods. Neuroimage 53, 515–525 (2010).
- [29] Lee, J. et al. Sensitivity of MRI resonance frequency to the orientation of brain tissue microstructure. Proc. Natl. Acad. Sci. U. S. A. 107, 5130–5135 (2010).
- [30] de Rochefort, L. et al. Quantitative susceptibility map reconstruction from MR phase data using bayesian regularization: Validation and application to brain imaging. Magn. Reson. Med. **63**, 194–206 (2010).
- [31] Li, W., Wu, B., Avram, A. & Liu, C. Magnetic susceptibility anisotropy of human brain in vivo and its molecular underpinnings. Neuroimage 59, 2088–2097 (2012).
- [32] Liu, C. & Li, W. Imaging neural architecture of the brain based on its multipole magnetic response. Neuroimage 67, 193–202 (2013).
- [33] Chen, W., Foxley, S. & Miller, K. Detecting microstructural properties of white matter based on compartmentalization of magnetic susceptibility. Neuroimage  $70$ , 1–9 (2013).
- [34] Liu, C. Susceptibility tensor imaging. Magn. Reson. Med. 63, 1471–1477 (2010).
- [35] Lee, J. et al. T-2\*-based fiber orientation mapping. Neuroimage 57, 225–234 (2011).
- [36] Oh, S., Kim, Y., Cho, Z. & Lee, J. Origin of b-0 orientation dependent  $r^*(2)$  (=1/T<sup>\*</sup>(2)) in white matter. *Neuroimage* **73**, 71–79 (2013).
- [37] Liu, C., Li, W., Wu, B., Jiang, Y. & Johnson, G. 3D fiber tractography with susceptibility tensor imaging. Neuroimage 59, 1290–1298 (2012).
- [38] Haacke, E., Xu, Y., Cheng, Y. & Reichenbach, J. Susceptibility weighted imaging (SWI). Magn. Reson. Med. 52, 612–618 (2004).
- [39] Thomas, B. P. et al. High-Resolution 7t MRI of the Human Hippocampus In Vivo. J. Magn. Reson. Imaging 28, 1266–1272 (2008).
- [40] Yao, B. et al. Susceptibility contrast in high field MRI of human brain as a function of tissue iron content. Neuroimage 44, 1259–1266 (2009).
- [41] Shmueli, K. et al. Magnetic susceptibility mapping of brain tissue in vivo using MRI phase data. Magn. Reson. Med. 62, 1510–1522 (2009).
- [42] Haacke, E. M., Mittal, S., Wu, Z., Neelavalli, J. & Cheng, Y.-C. N. Susceptibility-Weighted Imaging: Technical Aspects and Clinical Applications, Part 1. Am. J. Neuroradiology 30, 19–30 (2009).
- [43] Han, S. et al. Magnetic field anisotropy based MR tractography. J. Magn. Reson. 212, 386–393 (2011).
- <span id="page-9-1"></span>[44] Álvarez, G. A., Shemesh, N. & Frydman, L. Diffusion-assisted selective dynamical recoupling: A new approach to measure background gradients in magnetic resonance. J. Chem. Phys. 140, 084205 (2014).
- <span id="page-9-4"></span><span id="page-9-2"></span>[45] Stepisnik, J. Time-dependent self-diffusion by NMR spin-echo. Physica B 183, 343–350 (1993).
- [46] Callaghan, P. T. & Stepisnik, J. Frequency-domain analysis of spin motion using modulatedgradient NMR. J. Magn. Reson. 117, 118–122 (1995).
- <span id="page-9-3"></span>[47] Stepisnik, J., Lasic, S., Mohoric, A., Sersa, I. & Sepe, A. Spectral characterization of diffusion in porous media by the modulated gradient spin echo with CPMG sequence. J. Magn. Reson. 182, 195–199 (2006).
- <span id="page-9-0"></span>[48] Stepisnik, J. Validity limits of gaussian approximation in cumulant expansion for diffusion attenuation of spin echo. *Physica B* 270, 110–117 (1999).
- [49] Zheng, G. & Price, W. Suppression of background gradients in (b-0 gradient-based) NMR diffusion experiments. Concepts Magn. Reson. 30A, 261–277 (2007).
- [50] Cho, H., Ryu, S., Ackerman, J. & Song, Y. Visualization of inhomogeneous local magnetic field gradient due to susceptibility contrast. J. Magn. Reson. 198, 88–93 (2009).