# **Reverse Engineering the Intracellular Self-Assembly of a Functional Mechanopharmaceutical Device**

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#### **Supplementary Methods**

**HPLC analysis.** For the HPLC assay, the mobile phase was methanol:water (80:20) with 0.1% trifluoroacetic acid (1 ml/min flow rate). The stationary phase (column) was a C18 (unbonded silica particles) column (Atlantis $\circledR$  T3, 5 µm, 100Å), and the HPLC was equipped with a UV detector (Waters, Photodiode Array Detector 2996) @ 285 nm detection for CFZ. The retention time for CFZ was determined to be 4.75 min.

**Determination of solubility parameters.** We used a mathematical proof approach to determine  $[CFZH^+]_S$  as detailed below:

First, we calculated [CFZH<sup>+</sup>] using the total solubility  $(S_T)$  at each pH value and the constant intrinsic free base solubility,  $[CFZ]_S$ , using the following equation, which was obtained by rearranging the terms in equation (14) (see main article):

$$
[CFZH^+] = S_T - [CFZ]_S
$$
 (Supplementary Equation 1)

Then, we chose a value, say "y", from the list of the computed [CFZH<sup>+</sup>] values, and let "y" equal  $[CFZH^+]_S$ . By substituting "y' in place of  $[CFZH^+]_S$ , we calculated for total solubility at the different pH values using equation (15) (see main article). Then, we compared this total solubility-pH dataset to that obtained using equation (13) (see main article). Then, we checked if there was the same total solubility value at a given pH in both datasets, which would represent the intersection point of the two solubility-pH curves mentioned previously. This can be represented by the following equation:

 $S_T' = [CFZ]_S + [CFZH^+]_S$ (Supplementary Equation 2)

Where  $S_T$  is the total solubility value at the intersection of the two solubility-pH curves, and both forms of the drug, CFZ and CFZH<sup>+</sup>, are present in equilibrium with their respective solid forms in the solid phase denoted by the subscript *s*.

Moreover, to prove if our earlier assumption ("y" is equal to  $[CFZH^+]_S$ ) was valid, we calculated the total solubility by plugging "y" in place of  $[CFZH^+]_S$ , supplementary equation (2), and checked if it was equal to  $S_T$ . Furthermore, by definition, the pH where both the intrinsic free base and salt forms of the drug are in the solid phase is known as  $pH_{max}$ . Thus, the pH associated with  $S_T$ <sup>'</sup> was deduced to be pH<sub>max</sub>.

**Modeling proton influx.** V-ATPase is an electrogenic proton-pump, which inserts protons from the cytoplasm into the lysosome against an electrochemical gradient upon ATP hydrolysis<sup>1,2</sup>. The rate at which a proton molecule is inserted per second  $(J_{HVATP})$  was obtained from published experimental studies<sup>1</sup> as a function of transmembrane pH gradient ( $\Delta$  pH) in units of pH unit and membrane potential difference, which is also interchangeably known as membrane potential  $(\Delta \Psi)$ , in units of mV. This rate was multiplied by the total number of active V-ATPase molecules per lysosome  $(N<sub>VATP</sub>)$  to obtain the total amount of proton molecules inserted into the lysosome in units of molecules per second, as follows:

 $H_{pump} = N_{VATP} \times J_{H_{VATP}} (\triangle pH, \triangle \Psi)$  (Supplementary Equation 3)

Where lysosomal  $\Delta \Psi$  is dictated by the total net change in lysosomal ion content and is represented by the following relationship<sup>3</sup>:

$$
\Delta \Psi = \frac{F \times V_L}{C' \times S} \times [ (\sum_i Z_i [cations]_i + \sum_i Z_i [anions]_i ) - B ]
$$
 (Supplementary Equation 4)

Where  $V<sub>L</sub>$  is the lysosomal volume in units of L; Faraday's constant (F) which equals 96485 Coulomb/mol and is used to convert the lysosomal ion content in units of moles to units of Coulomb; C' is the specific membrane capacitance per unit area of a biological membrane<sup>4</sup>, which is experimentally approximated to be  $1 \mu$ F/cm<sup>2</sup> and is multiplied by the lysosomal surface area S represented in units of cm<sup>2</sup> to obtain the total lysosomal membrane capacitance;  $Z_i$  is valence for ion i; [cation] the concentration of cation i at a given time *t* in units of Molar; [anion] is the concentration of anion i at a given time *t* in units of Molar; B is the Donnan particles in units of Molar, which are impermeable lysosomal contents defined by initial lysosomal ion concentrations and net change in the intrinsic surface potentials, supplementary equation (5). In the model and simulations communicated herein, the initial lysosomal ions consist of proton, potassium, sodium, and chloride with their respective charge (+ or -1) represented as a coefficient of their respective concentration, which is denoted by the square brackets, supplementary equation (5).

 $B = [H^+]_{L,initial} + [K^+]_{L,initial} + [Na^+]_{L,initial} - [Cl^-]_{L,initial} - \frac{C \times S}{E \times V}$  $\frac{C \times S}{F \times V_L} \times \{ (\Psi_{in} - \Psi_{out}) +$  $\Psi_{initial}$  (Supplementary Equation 5)

Where  $\Psi_{\text{in}}$  and  $\Psi_{\text{out}}$  are the intrinsic inner and outer surface potentials, respectively, in units of mV, which contribute to the change in ion concentration at membrane surface as described later,  $\Psi_{initial}$  is the initial lysosomal membrane potential which is set to zero mV in order to maintain initial lysosomal membrane electroneutrality.

**Modeling chloride influx.** V-ATPase mediated proton influx into the lysosome is followed by lysosomal membrane potential increase which consequentially arrests further proton influx. Thus, to lower the membrane potential for the continuation of V-ATPase proton-pumping

activity, which is essential to lower lysosomal pH to physiological pH, the removal of lysosomal cation or the insertion of lysosomal anion is required. Accordingly, CLC7 is considered as the primary membrane potential dissipating protein which transports two chloride ions from the cytoplasm to the lysosome for every proton it transports from the lysosome to the cytoplasm<sup>5</sup>. The rate ( $J<sub>CL HClC</sub>$ ) at which the ion transportations occur was empirically derived from a currentvoltage experimental data<sup>3</sup> as a function of chemical ( $\Delta$ pH,  $\Delta$ Cl) and electric potential gradients,  $(\Delta \Psi)$ , as detailed in supplementary equations (6) and (7). This rate was multiplied by the total number of CLC7 molecules per lysosome  $(N<sub>CIC7</sub>)$  in order to obtain the total amount of proton and chloride molecules transported across the lysosomal membrane through CLC7, as follows:

$$
H_{CLC7} = N_{CLC7} \times J_{Cl, H_{CLC7}} (\triangle pH, \triangle CI, \triangle \Psi)
$$
 (Supplementary Equation 6)

$$
Cl_{CLC7} = 2 \times N_{CLC7} \times J_{CL,H_{CLC7}} (\triangle pH, \triangle CL, \triangle \Psi)
$$
 (Supplementary Equation 7)

Where  $\Delta$ Cl is the chloride gradient comprised of the luminal chloride (Cl<sub>L</sub>) and the cytoplasmic chloride (Cl<sub>C</sub>). Moreover, the coefficient 2 in supplementary equation (7) defines the 2:1 stoichiometric relationship between the chloride and proton ions transported by CLC7 across the lysosomal membrane.

**Modeling proton efflux.** In addition to CLC7, the passive diffusion of protons across the lysosomal membrane can also contribute to the dissipation of membrane potential in order to facilitate the proton pumping activity of V-ATPase. This passive proton leak is modeled by supplementary equation (8), which is derived from the Goldman-Hodgkin-Katz (GHK) ion flux equation<sup>6</sup> that is commonly used to describe the passive diffusion of a given ion across a biological membrane, assuming a linear potential gradient across a lipid membrane<sup>3</sup>.

$$
H_{\text{leak}} = (S \times P_{H^+} \times Y \times Z \times \frac{10^{-pH_L} - (10^{-pH_C} \times e^{-Z \times Y})}{1 - e^{-Z \times Y}}) \times N_{\text{av}}
$$
 (Supplementary Equation 8)

Where S is the total lysosomal surface area in units of  $cm<sup>2</sup>$  used to obtain the total amount of proton which passively diffuses across the lysosomal membrane;  $P_H^+$  is the lysosomal membrane proton permeability in units of cm/s; Z is the valence of the ion (i.e.  $+1$  for proton); pH<sub>L</sub> is the luminal pH used to calculate the total free lysosomal proton based on the logarithmic relationship of pH and free proton (pH<sub>L</sub> = -log[H<sup>+</sup>]); pH<sub>c</sub> is the cytoplasmic pH used to calculate the total free cytoplasmic proton based on the logarithmic relationship of pH and free proton (pH<sub>C</sub> = -log[H<sup>+</sup>]);  $N_{av}$  is Avogadro's number used to convert the amount of transported protons in unit of moles to unit of molecules; Y is used to convert proton transportation in unit of charge per second to moles per second and is defined as:  $Y = \frac{\Delta \Psi \times F}{\Delta V \times F}$  $\frac{R+2r}{R \times T}$ , where R is universal gas constant, F is Faraday's constant, and T is absolute temperature. Moreover, for cells at room temperature (25 °C), RT/F equals 25.69 mV<sup>4</sup>, and is used for normalizing the lysosomal membrane potential communicated in this report.

**Modeling the effect of membrane leaflet potentials on ions.** In order to account for the effects of intrinsic external ( $\Psi_{i,out}$ ) and internal ( $\Psi_{i,in}$ ) leaflet potentials of the lysosomal membrane on cytoplasmic and lysosomal ion *i* concentrations, respectively, the individual cytoplasmic and lysosomal ion concentrations are computed using the following relationships, supplementary equations (9 and 10), derived from the GHK equation for a single ion concentration gradient, by setting net current flow equal to zero.

$$
\Delta \Psi_{i,in} = \frac{-Z \times R \times T}{F} \ln \frac{C_{i,in}}{C_{i,L}}
$$
 (Supplementary Equation 9)  
\n
$$
\Delta \Psi_{i,out} = \frac{-Z \times R \times T}{F} \ln \frac{C_{i,out}}{C_{i,C}}
$$
 (Supplementary Equation 10)

Where  $C_{i,in}$  is the internal concentration of a given ion (i) at the membrane surface facing the lysosomal compartment,  $C_{i,L}$  is the concentration of the ion (i) inside the lysosome,  $C_{i,out}$  is the external concentration of the ion (i) at the membrane surface facing the cytoplasmic compartment,  $C_{i,C}$  is the concentration of the ion (i) inside the cytoplasm. All units are molar.

**Governing equations.** Supplementary equations (3-10) were used in supplementary equations (11-13) to further define the ion movements as a function of time, in units of molecules per second.

$$
\frac{dH^+}{dt} = H_{pump} - H_{CLC7} - H_{leak} - H_{sequestered}
$$
 (Supplementary Equation 11)  

$$
\frac{dCl^-}{dt} = 2 \times N_{CLC7} \times J_{CLHCLC7} (\Delta pH, \Delta CI, \Delta \Psi) - Cl_{sequestered}
$$

#### (Supplementary Equation 12)

Moreover, extending supplementary equation (11), we can denote the change in lysosomal pH with respect to time by following the relationship between the lysosomal lumen buffering capacity (β) of the Donnan particles, which sequester non-free lysosomal protons, and free lysosomal protons which give rise to lysosomal pH as follows:

$$
\frac{dpH}{dt} = \frac{(-H_{pump} + H_{CLC7} + H_{leak} + H_{sequencestered})}{V \times N_{av} \times \beta}
$$
 (Supplementary Equation 13)

Where V is the lysosomal volume and is multiplied by  $N_{av}$  to convert the unit of molecules per second to molar per second, where the inverse of  $\beta$  is in units of pH units per molar.

**Numerical analysis.** Supplementary equations (11-13) were solved by numerical integration in Berkeley Madonna® using Rosenbrock stiff solver as a numerical integrator.

**Data visualization**. Multiple individual 2D datasets associated with the parametric simulations performed to generate simultaneous inhibitions of various lysosomal parameters were obtained. The datasets associated with each simultaneous inhibitions of lysosomal parameters were exported from Berkeley Madonna and compiled into three separate matrices in a MS-Excel spreadsheet, such that the first rows and columns of the matrix correspond to the two parameters simultaneously varied in the model simulations to obtain the final lysosomal readout values (lysosomal pH, Cl<sup>-</sup>, and membrane potential), where each makes up the rest of the rows and columns of a single matrix.

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**Supplementary Figure S1.** Fluorescence Microspectroscopy and (inset,  $i =$  brightfield,  $ii =$ green fluorescence, *iii* = far-red fluorescence) Epifluorescence Microscopy of CFZ-H<sup>+</sup>Cl<sup>-</sup> crystals indicating the lack of green fluorescence while being fluorescent in the far-red fluorescence range. The excitation wavelength (nm, Ex) and emission wavelength (nm, Em) are shown on the X-axis and Y-axis, respectively. The normalized fluorescence yield is shown by a

contour plot that was normalized using a control slide first and then to the maximum measured fluorescence yield. The colors as shown represent contour levels from 0-1 in steps of 0.2. The green, red, and far-red fluorescence bandwidths are overlaid on top of the normalized fluorescence spectra.



**Supplementary Figure S2.** Epifluorescence microscopy of RAW264.7 cells when incubated with CFZ (10  $\mu$ M), Lysotracker® Blue (LB, 1 and 20  $\mu$ M) at  $t = 1$  hour. Scale bar, 10  $\mu$ m. At 1 hour, green fluorescence spots indicative of CFZ are visible as mild diffuse staining rather than punctate staining observed at *t* = 24 hours. Vesicular staining pattern of LB, visible as blue

punctate spots when incubated on its own, are absent when co-incubated with CFZ at both  $LB =$ 1 and 20 μM. The control images were taken at *t* = 24 hours post initiation of experiments.



**Supplementary Figure S3.** Pearson's Colocalization Coefficient for multiple cell ROIs  $(n = 70)$ as obtained post epifluorescence microscopy of RAW264.7 cells incubated with CFZ (10 μM) at  $t = 24-72$  hours. Fluorescence channel description is provided in Supplementary Table S2. The scatter distribution is further annotated with four horizontal lines denoting the Mean  $\pm$  S.E. (same color lines as the distribution), Mean (green line) and the Median (black line) of the distribution.  $*$  *-p* < 0.005.



**Supplementary Figure S4.** Viability of RAW264.7 cells treated with a) BafA1 and b) NPPB in the presence of CFZ (0-10  $\mu$ M). Data was collected at n = 6 with  $*$  -  $p < 0.05$ ,  $**$  -  $p < 0.01$ ,  $***$ - *p* < 0.001. Each point is compared in a pair-wise independent Student *t*-test.



**cytoplasmic chloride on the lysosomal accumulation of CFZ-H <sup>+</sup>Cl- . a**, V-ATPase inhibition showed a more substantial effect than cytoplasmic chloride inhibition on the accumulation of  $CFZ-H<sup>+</sup>Cl<sup>-</sup>$  at the rate of 0.01 picomol/cell/day, as reflected by the changes in the lysosomal pH, CI, and membrane potential values of the CFZ-H<sup>+</sup>CI containing lysosome from that of the CFZ-H<sup>+</sup>Cl<sup>-</sup> free lysosome. **b**, V-ATPase inhibition generally showed a more substantial effect than cytoplasmic chloride inhibition although the simultaneous inhibition of both parameters showed even more pronounced effect on the physiological accumulation of CFZ-H<sup>+</sup>Cl<sup>-</sup> at the rate of 0.01 picomol/cell/day, as reflected by the changes in the lysosomal pH, Cl, and membrane potential values of the CFZ-H<sup>+</sup>Cl<sup>-</sup> containing lysosome from respective baseline physiological values. Arrow signs represent values outside of the axes plot range.



**cytoplasmic chloride on the lysosomal accumulation of CFZ-H <sup>+</sup>Cl-at a higher dose. a**, V-ATPase inhibition showed a more substantial effect than cytoplasmic chloride inhibition on the accumulation of CFZ-H<sup>+</sup>Cl<sup>-</sup> at the rate of 0.1 picomol/cell/day, as reflected by the changes in the lysosomal pH, Cl<sup>-</sup>, and membrane potential values of the CFZ-H<sup>+</sup>Cl<sup>-</sup> containing lysosome from that of the CFZ-H<sup>+</sup>Cl<sup>-</sup> free lysosome. **b**, V-ATPase inhibition generally showed a more substantial effect than cytoplasmic chloride inhibition although the simultaneous inhibition of both parameters showed even more pronounced effect on the physiological accumulation of  $CFZ-H<sup>+</sup>CI$  at the rate of 0.1 picomol/cell/day, as reflected by the changes in the lysosomal pH,  $CI$ , and membrane potential values of the CFZ-H<sup>+</sup>Cl<sup>-</sup> containing lysosome from respective baseline physiological values. Arrow signs represent values outside of the axes plot range.



## **Supplementary Table S1.** Model Parameters

<sup>*a*</sup>Baseline input values are literature values<sup>7-11</sup> representing physiological lysosomes and are in agreement with previously published model<sup> $2,3$ </sup>.

<sup>*b*</sup>Estimated intrinsic surface potentials for inner (Ψ<sub>in</sub>) and outer (Ψ<sub>out</sub>) leaflets of the lysosomal membrane accounted for when modeling membrane transporter mediated dynamic lysosomal and cytoplasmic ion concentrations at the membrane surface<sup>2</sup>.

### **Supplementary Table S2.** Fluorescence in RAW264.7 cells. (Channels (Ex/Em)) – Blue

(350/405 nm), Green (490/510 nm), Red (590/610 nm), and Far-Red (640/670 nm).

