

## Supplementary Online Content

Ehteshami Bejnordi B, Veta M, Johannes van Diest P, et al; CAMELYON16. Diagnostic assessment of deep learning algorithms for detection of lymph node metastases in women with breast cancer. *JAMA*. doi:10.1001/jama.2017.14585

### **eAppendix.** Deep Learning and Glossary

**eFigure 1.** Two Example Annotated Areas of Whole-Slide Images Taken From the CAMELYON16 Dataset

**eFigure 2.** Use of Immunohistochemistry Staining to Generate Reference Standard

**eFigure 3.** ROC Curves of the Panel of 11 Pathologists for Task 2

**eFigure 4.** FROC Curves of All Participating Teams for Task 1

**eFigure 5.** Example Probability Maps Generated by the Top-Three Performing Systems

**eFigure 6.** ROC Curves of All Participating Teams for Task 2

**eTable 1.** Classification Results by Pathologists for the Whole-Slide Image Classification Task (Sensitivity and Specificity)

**eTable 2.** Classification Results by Pathologists for the Whole-Slide Image Classification Task (Area Under the ROC Curve)

**eTable 3.** Participating Teams in CAMELYON16

**eTable 4.** Summary of Results for the Metastasis Identification Task (Task 1)

**eTable 5.** Summary of Results for the Whole-Slide Image Classification Task (Task 2)

**eMethods.** Methods 1 Through 30

**eResults.**

**eDiscussion.**

**eReferences.**

This supplementary material has been provided by the authors to give readers additional information about their work.

## **eAppendix. Deep Learning and Glossary**

### **Deep Learning.**

Application of traditional machine learning to medical image analysis typically involved human engineers collaborating with physicians to decide what kind of features are needed to recognize lesions or objects of interest in the images. These features were then extracted from medical images and fed to an algorithm which would assess whether the lesion or object was present in the image. Deep learning changes this in two important ways. The first refers to the ‘deep’ part in deep learning; whereas the traditional approach typically consisted of two steps, a deep network consists of many steps, or in deep learning terminology, layers. Each of these layers can perform feature extraction or classification, and because one layer feeds output into the next, features can hierarchically become more complex. The first layers, for example, can identify edges or circles and subsequent layers can combine these into more meaningful objects, eventually leading to complex structures such as faces in natural images. The second major difference with traditional machine learning is that features are no longer manually engineered, but learned automatically by the system. This is done by optimizing deep learning algorithms end-to-end, i.e. given an input, optimize the parameters across layers in such a way that the desired output is most likely. Typically this is done with an algorithm called backpropagation.

Most deep learning algorithms are based on artificial neural networks that are mathematical constructs that stack together ‘nodes’. Nodes consist of simple multiplications and additions, combined with a non-linear transform and multiple nodes form a layer. By selecting how nodes between different layers are connected one can determine how features are extracted. Currently the most popular deep learning algorithm is the convolutional neural network (CNN). In a CNN nodes are connected in such a way that they model a convolution operation, which allows recognition of a single feature (a convolutional filter) across the entire image, making CNNs highly efficient for image processing. CNNs have revolutionized the field of computer visions, breaking records and attaining results that have eluded the community for years<sup>1-4</sup>.

## **Glossary of deep learning and digital pathology terminology**

Model fine-tuning – using the weights of a model that was trained for one task as an initialization for training a model for a different task.

Model ensembling – combining the output from different models (e.g. by averaging the predictions) with the goal of improving the overall performance.

Hard-negative mining – discovering negative samples (in a detection problem) that are non-trivial to distinguish from positive samples.

Data augmentation – applying transformation to the training samples that create new, plausible training samples with the goal of increasing the training set size.

Staining normalization – modifying the color appearance of whole slide images such that it resembles some reference sample with the goal of reducing the appearance variability within a dataset.

Fully convolutional network – neural network consisting only of convolutional layers, or more generally, consisting only of layers that produce outputs for arbitrary input sizes (this enables a model to be trained on small images and then applied to larger images such as whole slide images).

AlexNet<sup>1</sup> – neural network architecture that was the winner of the ImageNet Large Scale Visual Recognition Challenge 2012 for the object detection, localization and classification tasks<sup>5</sup>.

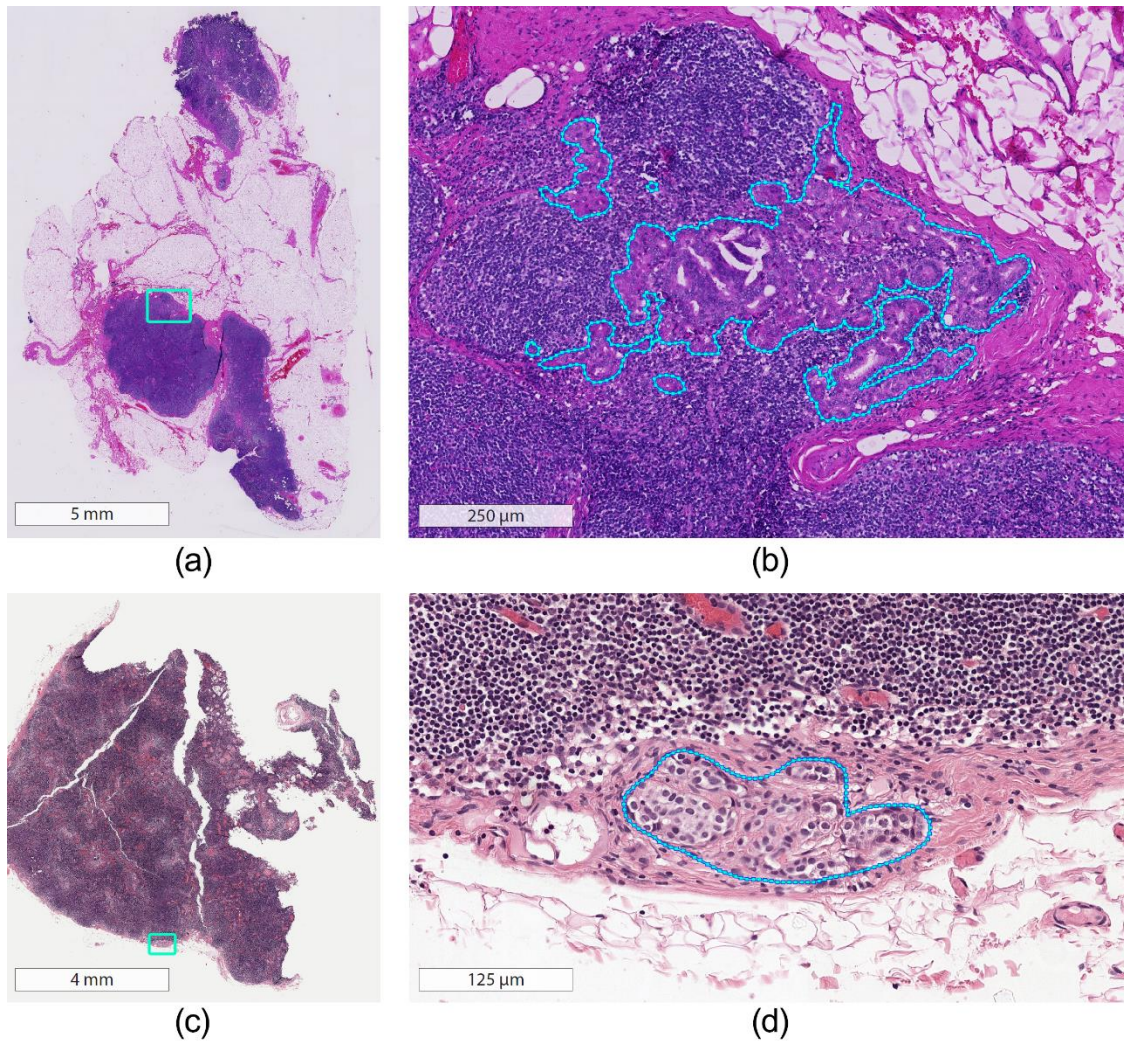
GoogLeNet<sup>3</sup> – neural network architecture that was the winner of the ImageNet Large Scale Visual Recognition Challenge 2014 for the object detection and classification tasks<sup>5</sup>.

VGG-net<sup>6</sup> – neural network architecture that was the winner of the ImageNet Large Scale Visual Recognition Challenge 2014 for the localization task<sup>5</sup>.

ResNet<sup>4</sup> – neural network architecture that was the winner of the ImageNet Large Scale Visual Recognition Challenge 2015 for the object detection, localization and classification tasks<sup>4,5</sup>.

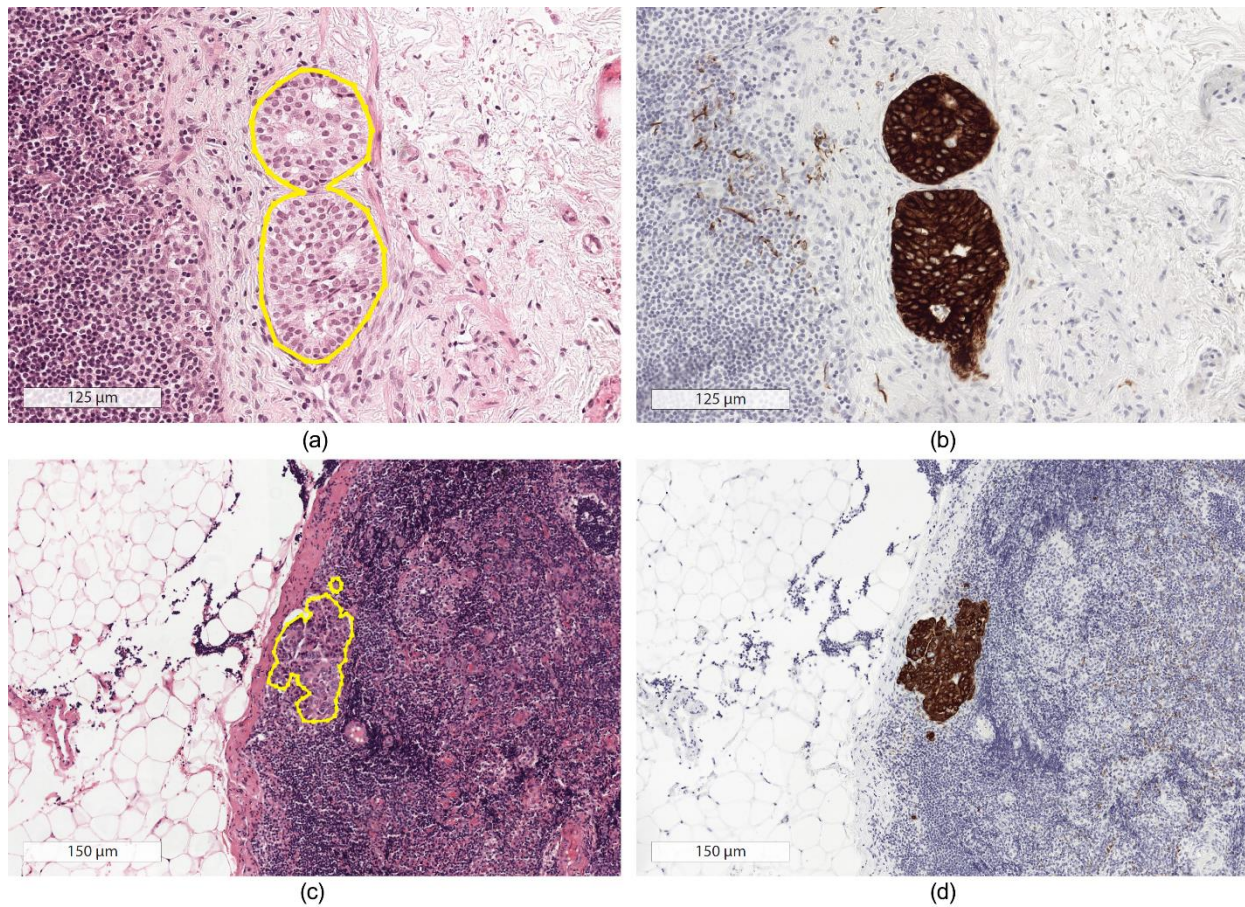
U-Net<sup>7</sup> and SegNet<sup>8</sup> – neural network architectures that were specifically designed for segmentation of biomedical images.

**eFigure 1. Two example annotated areas of whole-slide images taken from the CAMELYON16 dataset**



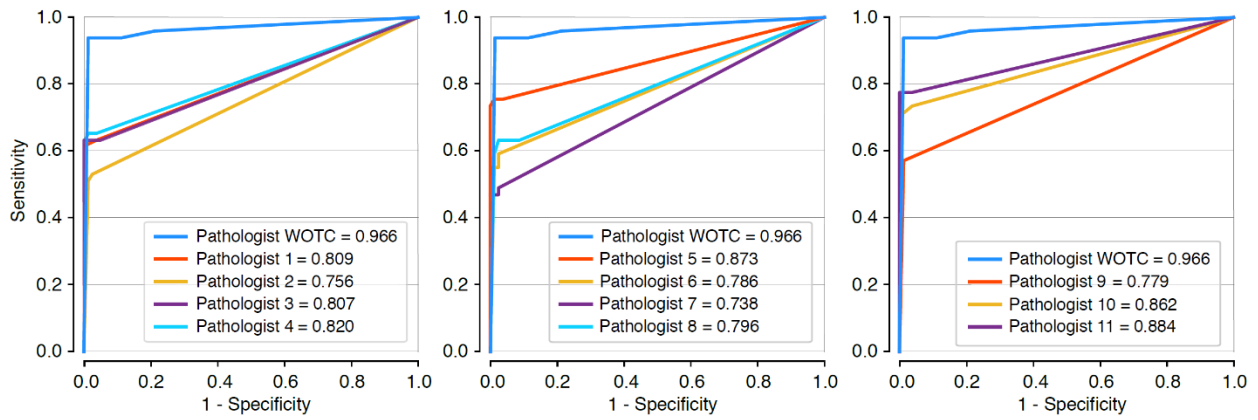
eFigure 1. Two example annotated areas of whole-slide images of hematoxylin and eosin stained lymph node tissue sections taken from the CAMELYON16 dataset. (a) and (c) show overviews of two examples of whole-slide images. (b) and (d) are magnified images, corresponding to rectangle areas in (a) and (c), with detailed annotation of metastatic regions.

## eFigure 2. Use of immunohistochemistry staining to generate reference standard



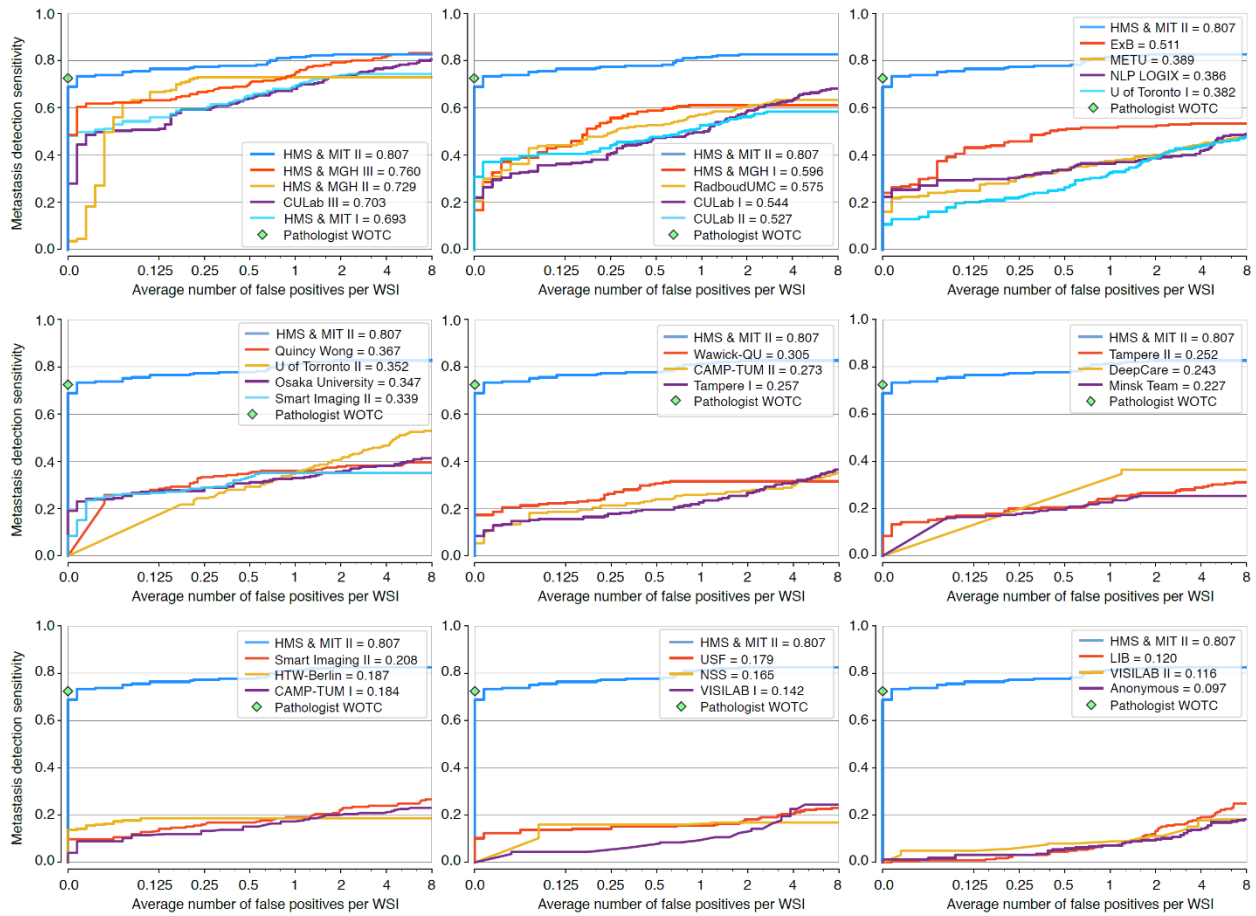
eFigure 2. Side by side visualization of hematoxylin and eosin (H&E) and immunohistochemistry (IHC) staining for generating reference standard. (a) and (c) show two example annotations made for two H&E stained images. (b) and (d) show corresponding tissue areas in (a) and (c), stained with IHC. Note that IHC was only used for generating the reference standard in our challenge. Neither of the pathologists in our observer study nor participants of the challenge had access to this data. Immunohistochemical staining was performed with anti-CK8/18 (anti-cytokeratin mouse monoclonal antibody, clone CAM 5.2, BD Biosciences, San Jose, USA). Binding of the antibody was visualized with a Brightvision® Poly-HRP-Anti Ms/Rb/Rt IgG biotin free detection system using BrightDAB® (Immunologic, Duiven, the Netherlands) as peroxidase-compatible chromogen and hematoxylin counterstaining.

**eFigure 3. ROC curves of the panel of the 11 pathologists for task 2**



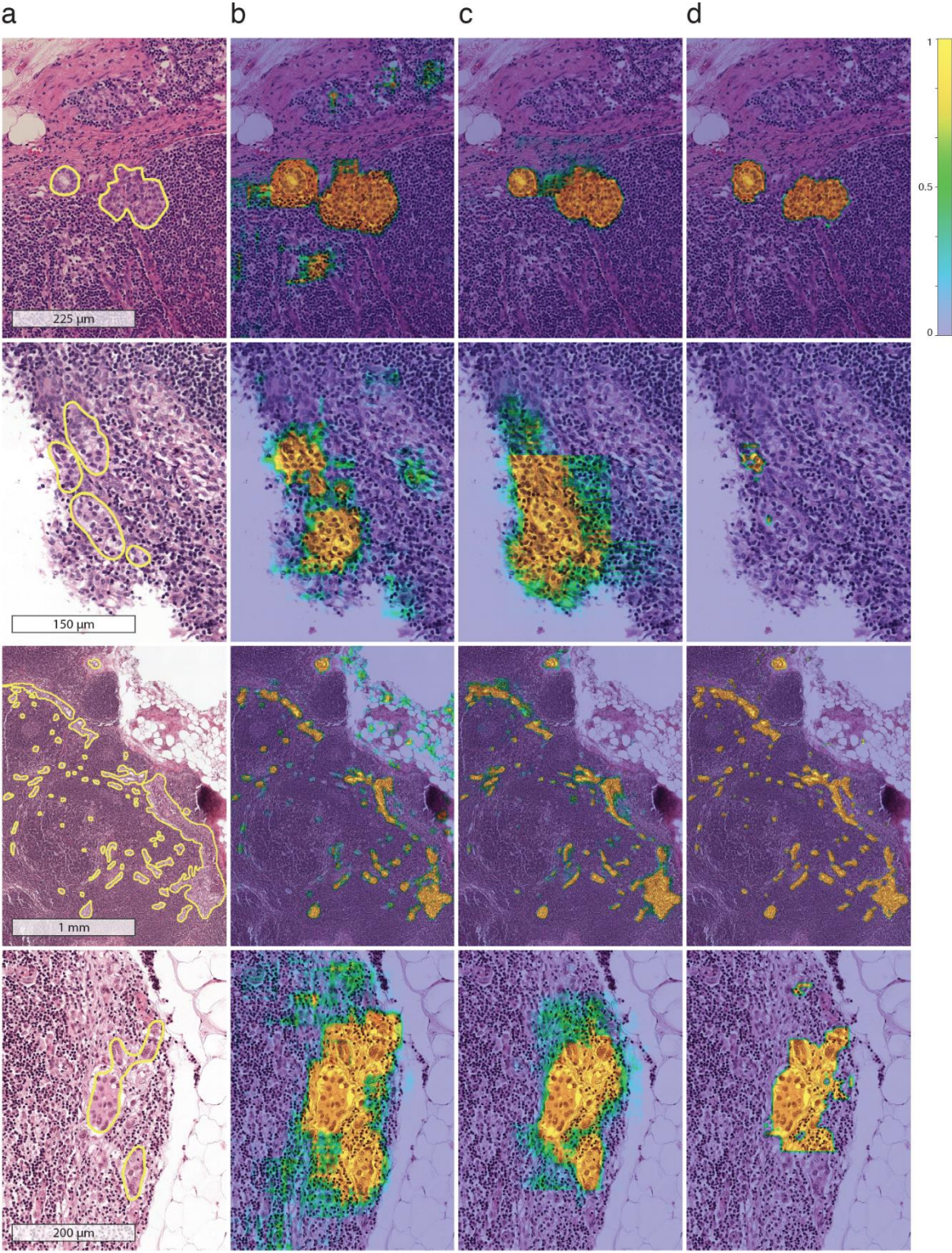
eFigure 3. ROC curves of the panel of 11 pathologists and their corresponding AUCs for task 2 (measured on the 129 whole-slide images in the test set of which 49 contain metastatic regions). All the pathologists scored whole-slide images using five levels of confidence: definitely normal, probably normal, equivocal, not confident, probably tumor, definitely tumor. To ease comparison, the ROC curve of the pathologist without time constraint (pathologist WOTC) is shown in all subfigures.

eFigure 4. FROC curves of all participating teams for task 1



eFigure 4. FROC curves of all the 32 participating teams and their corresponding FROC true positive fraction scores for task 1 (measured on the 129 whole-slide images in the test set of which 49 contain metastatic regions). The operating point of the pathologist who scored the slides without time constraint (WOTC) is shown as a green diamond. The range on the x-axis is linear between 0 and 0.125 and base-2 logarithmic scale between 0.125 and 8. The pathologist did not produce any false positives and achieved a true positive fraction of 0.724 for detecting and localizing metastatic regions. To ease comparison, the FROC curve of the best-performing system (HMS & MIT II) is shown in all subfigures.

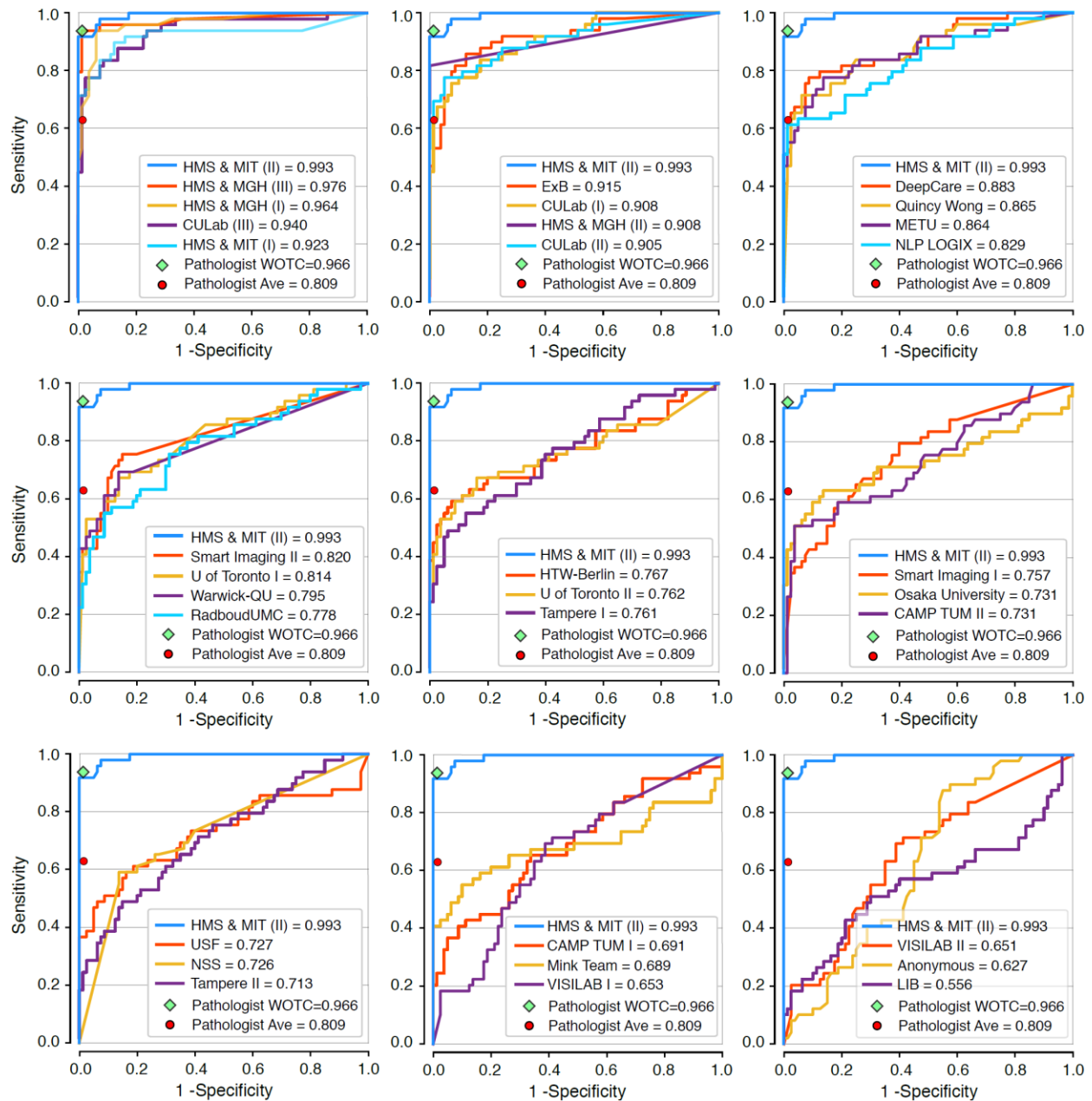
eFigure 5. Example probability maps generated by the top-three performing systems



eFigure 5. Example probability maps generated by the top-three performing systems. (a) Four annotated metastatic lesions in the test set of CAMELYON16. (b-d) Probability maps for teams HMS & MIT II, HMS & MGH III, and CULab III, respectively, overlaid on the original images.



**eFigure 6. ROC curves of all participating teams for task 2**



eFigure 6. ROC curves of all the 32 participating teams and their corresponding AUCs for task 2 (measured on the 129 whole-slide images in the test set of which 49 contain metastatic regions). The operating point of the pathologist who scored the slides without time constraint (WOTC) and the operating point of the mean of the panel of 11 pathologists are shown as green diamond and red circle, respectively. To ease comparison, ROC curve of the best-performing system (HMS & MIT II) is shown in all subfigures.

## eTable 1. Classification results by pathologists for the whole-slide image classification task (sensitivity and specificity)

eTable1. Classification results by the panel of 11 pathologists participating in the simulation exercise and the expert pathologist whiteout time constraint (WOTC) on the CAMELYON16 test set for the whole-slide image classification task (task 2). The performances are measured in 129 whole-slide images in the test set of which 49 contain metastatic regions (comprising of 22 macro and 27 micrometastases, and 38 with primary tumor histotype of infiltrating ductal cancer (IDC) and 11 non-IDC). We report sensitivity and specificity for different scenarios: 1) differentiating all tumor slides from normal slides, 2) differentiating slides with macrometastases from normal slides while excluding micrometastases, 3) differentiating slides with micrometastases from normal slides while excluding macrometastases, 4) differentiating slides with primary tumor histotype of IDC from normal slides while excluding the rarer primary tumor histotypes (non-IDC), and 5) differentiating slides with non-IDC primary histotypes from normal slides while excluding slides with primary tumor histotype of IDC.

| Codename         | All cases   |             | Metastases      |             |                 |             | Histotype   |             |             |             |
|------------------|-------------|-------------|-----------------|-------------|-----------------|-------------|-------------|-------------|-------------|-------------|
|                  |             |             | Macrometastases |             | Micrometastases |             | IDC         |             | Non-IDC     |             |
|                  | Sensitivity | Specificity | Sensitivity     | Specificity | Sensitivity     | Specificity | Sensitivity | Specificity | Sensitivity | Specificity |
| Pathologist 1    | 0.612       | 1           | 0.954           | 1           | 0.333           | 1           | 0.647       | 1           | 0.533       | 1           |
| Pathologist 2    | 0.510       | 0.987       | 0.909           | 0.987       | 0.185           | 0.987       | 0.588       | 0.987       | 0.333       | 0.987       |
| Pathologist 3    | 0.632       | 1           | 0.954           | 1           | 0.370           | 1           | 0.735       | 1           | 0.4         | 1           |
| Pathologist 4    | 0.653       | 0.987       | 0.954           | 0.987       | 0.407           | 0.987       | 0.705       | 0.987       | 0.533       | 0.987       |
| Pathologist 5    | 0.755       | 0.987       | 1               | 0.987       | 0.555           | 0.987       | 0.764       | 0.987       | 0.733       | 0.987       |
| Pathologist 6    | 0.571       | 0.975       | 0.818           | 0.975       | 0.370           | 0.975       | 0.676       | 0.975       | 0.333       | 0.975       |
| Pathologist 7    | 0.469       | 0.975       | 0.863           | 0.975       | 0.148           | 0.975       | 0.529       | 0.975       | 0.333       | 0.975       |
| Pathologist 8    | 0.632       | 0.975       | 0.954           | 0.975       | 0.370           | 0.975       | 0.705       | 0.975       | 0.466       | 0.975       |
| Pathologist 9    | 0.571       | 0.987       | 0.909           | 0.987       | 0.296           | 0.987       | 0.617       | 0.987       | 0.466       | 0.987       |
| Pathologist 10   | 0.734       | 0.962       | 0.954           | 0.962       | 0.555           | 0.962       | 0.794       | 0.962       | 0.6         | 0.962       |
| Pathologist 11   | 0.775       | 1           | 0.954           | 1           | 0.629           | 1           | 0.850       | 1           | 0.6         | 1           |
| Mean pathologist | 0.628       | 0.985       | 0.929           | 0.985       | 0.383           | 0.985       | 0.692       | 0.985       | 0.484       | 0.985       |
| Pathologist WOTC | 0.938       | 0.987       | 1               | 0.987       | 0.888           | 0.9875      | 0.970       | 0.987       | 0.866       | 0.987       |

**eTable 2. Classification results by pathologists for the whole-slide image classification task (area under the ROC curve)**

eTable2. Classification results by the panel of 11 pathologists participating in the simulation exercise and the expert pathologist without time constraint (WOTC) on the CAMELYON16 test set for the whole-slide image classification task (task 2). The performances are measured in 129 whole-slide images in the test set of which 49 contain metastatic regions (comprising of 22 macro and 27 micrometastases, and 38 with primary tumor histotype of infiltrating ductal cancer (IDC) and 11 non-IDC). We report classification AUC for different scenarios: 1) differentiating all tumor slides from normal slides, 2) differentiating slides with macrometastases from normal slides while excluding micrometastases, 3) differentiating slides with micrometastases from normal slides while excluding macrometastases, 4) differentiating slides with primary tumor histotype of IDC from normal slides while excluding the rarer primary tumor histotypes (non-IDC), and 5) differentiating slides with non-IDC primary histotypes from normal slides while excluding slides with primary tumor histotype of IDC. We used percentile bootstrapping to construct 95% confidence interval. The results of the significance test for comparison of the performance of each pathologist for the detection of micro and macrometastases as well as for comparison of the performance for the detection of IDC and non-IDC metastases are presented (see the statistical analysis section). The p-values were adjusted for multiple comparisons using the Bonferroni correction.

| Codename         | All cases |             | Metastases      |             |                 |             |                                      | Histotype |             |         |             |                                      |
|------------------|-----------|-------------|-----------------|-------------|-----------------|-------------|--------------------------------------|-----------|-------------|---------|-------------|--------------------------------------|
|                  |           |             | Macrometastases |             | Micrometastases |             | Comparis on of detection performance | IDC       |             | Non-IDC |             | Comparis on of detection performance |
|                  | AUC       | 95% CI      | AUC             | 95% CI      | AUC             | 95% CI      |                                      | AUC       | 95% CI      | AUC     | 95% CI      |                                      |
| Pathologist 1    | 0.809     | 0.732-0.876 | 0.976           | 0.918-1.0   | 0.673           | 0.577-0.777 | p<0.001                              | 0.817     | 0.729-0.899 | 0.791   | 0.665-0.916 | p>0.99                               |
| Pathologist 2    | 0.756     | 0.679-0.82  | 0.948           | 0.874-1.0   | 0.599           | 0.510-0.672 | p<0.001                              | 0.785     | 0.696-0.858 | 0.689   | 0.569-0.831 | p>0.99                               |
| Pathologist 3    | 0.807     | 0.738-0.876 | 0.976           | 0.916-1.0   | 0.669           | 0.562-0.757 | p<0.001                              | 0.861     | 0.779-0.937 | 0.685   | 0.566-0.825 | p=0.34                               |
| Pathologist 4    | 0.820     | 0.744-0.885 | 0.976           | 0.915-1.0   | 0.692           | 0.590-0.787 | p<0.001                              | 0.847     | 0.762-0.922 | 0.758   | 0.623-0.891 | p>0.99                               |
| Pathologist 5    | 0.873     | 0.802-0.926 | 1.0             | 1.0-1.0     | 0.769           | 0.659-0.859 | p=0.01                               | 0.878     | 0.797-0.949 | 0.862   | 0.737-0.969 | p>0.99                               |
| Pathologist 6    | 0.786     | 0.711-0.854 | 0.924           | 0.838-0.993 | 0.674           | 0.577-0.76  | p=0.03                               | 0.844     | 0.758-0.921 | 0.656   | 0.543-0.778 | p=0.15                               |
| Pathologist 7    | 0.738     | 0.663-0.805 | 0.930           | 0.843-1.0   | 0.582           | 0.502-0.65  | p<0.001                              | 0.773     | 0.683-0.854 | 0.658   | 0.548-0.791 | p>0.99                               |
| Pathologist 8    | 0.796     | 0.715-0.866 | 0.969           | 0.904-1.0   | 0.654           | 0.549-0.739 | p<0.001                              | 0.835     | 0.743-0.91  | 0.707   | 0.576-0.854 | p>0.99                               |
| Pathologist 9    | 0.779     | 0.707-0.845 | 0.948           | 0.869-1.0   | 0.642           | 0.545-0.72  | p<0.001                              | 0.803     | 0.710-0.884 | 0.727   | 0.599-0.857 | p>0.99                               |
| Pathologist 10   | 0.862     | 0.796-0.927 | 0.976           | 0.917-1.0   | 0.769           | 0.651-0.859 | p=0.01                               | 0.893     | 0.815-0.957 | 0.793   | 0.670-0.919 | p>0.99                               |
| Pathologist 11   | 0.884     | 0.816-0.941 | 0.976           | 0.917-1.0   | 0.808           | 0.704-0.908 | p=0.03                               | 0.924     | 0.845-0.983 | 0.793   | 0.660-0.919 | p=0.25                               |
| Mean pathologist | 0.810     | 0.750-0.869 | 0.964           | 0.930-0.997 | 0.685           | 0.619-0.746 | —                                    | 0.842     | 0.775-0.907 | 0.738   | 0.630-0.846 | —                                    |
| Pathologist WOTC | 0.966     | 0.927-0.998 | 0.994           | 0.977-1.0   | 0.943           | 0.868-0.995 | p=0.87                               | 0.976     | 0.932-1.0   | 0.943   | 0.848-1.0   | p>0.99                               |

### eTable 3. Participating teams in CAMELYON16

eTable3. Teams participating in CAMELYON16. Each method is identified with a codename used in the text. See eMethods for details about each method.

| Codename                | Contributors   | Institutions   | Training Model   |
|-------------------------|--|--|--|
| HMS & MIT (I & II)      | Dayong Wang, Aditya Khosla, Rishab Gargeya, Humayun Irshad, Andrew H Beck                              | Harvard Medical School and Massachusetts Institute of Technology | (Models I & II)<br>22 layer GoogLeNet <sup>3</sup>   |
| HMS & MGH (I, II & III) | Aoxiao Zhong, Quanzheng Li   | Harvard Medical School and Massachusetts General Hospital        | (Model I) 22 layer GoogLeNet <sup>3</sup> ,<br>(Model II) 101 ResNet <sup>4</sup> ,<br>(Model III) 101 fully convolutional ResNet <sup>4</sup> |
| ExB                     | Christian Hass, Urko Sanchez, Ivan Vasilev, Tony Mey, and Elia Bruni                                   | ExB Research and Development GmbH                                | 34 layer ResNet <sup>4</sup>   |
| CULab (I, II & III)     | Hao Chen, Huang-Jing Lin, Qi Dou, and Pheng-Ann Heng   | The Chinese Univ. of Hong Kong                                   | (Model I) VGG-16 <sup>6</sup> ,<br>(Model II) cascade of VGG-16 <sup>6</sup> and ResNet <sup>4</sup> -152<br>(Model III) VGG-16 <sup>6</sup>   |
| Quincy Wong             | Quincy Wong  | Independent participant  | 37 layer SegNet <sup>8</sup>   |
| METU                    | Ugur HALICI, Mustafa Ümit ÖNER, and Rengül Çetin Atalay  | Middle East Technical Univ.                                      | 4 layer CNN  |
| NLP LOGIX               | Matt Berseth   | NLP LOGIX  | 7 layer AlexNet <sup>1</sup>   |
| Smart Imaging (I & II)  | Vitali Khvatkov, Alexei Vylegzhanin  | Smart Imaging Technologies Co.                                   | (Model I) SVM <sup>9</sup> and AdaBoost <sup>10</sup> ,<br>(Model II) Combination of model I and a 22 layer GoogLeNet <sup>3</sup>             |
| U of Toronto (I & II)   | Oren Kraus   | Univ. of Toronto   | (Models I & II)<br>10 layer VGG-like <sup>6</sup> network  |
| Warwick-QU              | Muhammad Shaban, Talha Qaiser, Ruqayya Awan, Korsuk Sirinukunwattana, Yee-Wah Tsang, and Nasir Rajpoot | University of Warwick  | 15 layer U-Net <sup>7</sup>  |
| Radboudumc              | David Tellez   | Radboud Univ. Medical Center                                     | VGG-13 <sup>6</sup>  |
| HTW-Berlin              | Jonas Annuscheit, Peter Hufnagl  | HTW-BERLIN   | CRFasRNN <sup>11</sup>   |
| Tampere I               | Mira Valkonen, Kimmo Kartasalo, Kaisa Liimatainen, Leena Latonen, Pekka Ruusuuvuori                    | Univ. of Tampere   | Random Forests <sup>12</sup>   |
| Osaka University        | Seiryō Watanabe, Shigeto Seno, Yoichi Takenaka, Hideo Matsuda  | Osaka Univ.  | 22 layer GoogLeNet <sup>3</sup>  |
| USF                     | Hady Ahmady Phoulady   | Univ. of South Florida   | Random Forests <sup>12</sup>   |
| NSS                     | Nandakumar P, Sarath PC, Vishnu Prasad M, Yadukrishnan M, and Sreejith Valsan M                        | NSS college of Engineering                                       | Multiple thresholds  |
| Tampere II              | Kaisa Liimatainen, Kimmo Kartasalo, Mira Valkonen, Leena Latonen, Pekka Ruusuuvuori                    | Univ. of Tampere   | 7 layer CNN  |
| CAMP-TUM (I & II)       | Bharti Munjal, Amil George, Shadi Albarqouni, Stefanie Demirci, Nassir Navab                           | Technical Univ. of Munich  | (Model I) 5 layer Agg-Net <sup>13</sup> ,<br>(Model II) 22 layer GoogLeNet <sup>3</sup>  |
| Minsk Team              | Vassili Kovalev, Alexander Kalinovskiy, and Vitali Liauchuk  | United Institute of Informatics Problems                         | 22 layer GoogLeNet <sup>3</sup>  |
| VISILAB (I & II)        | M. Milagro Fernandez-Carrobles, Ismael Serrano, Oscar Deniz, Gloria Bueno                              | Univ. of Castilla-La Mancha                                      | (Model I) Random Forests <sup>12</sup> ,<br>(Model II) 3 layer CNN   |
| Anonymous               | Anonymous  | Anonymous  | Random Forests <sup>12</sup>   |
| LIB                     | R. Venâncio, B. Ben Cheikh, A. Coron, and D. Racoceanu   | Sorbonne Univ.   | SVM <sup>9</sup>   |
| DeepCare                | Tong Xu  | DeepCare Inc.  | 22 layer GoogLeNet <sup>3</sup>  |

**eTable 4. Summary of results for the metastasis identification task (task1)**

eTable4. Results of the submitted algorithms on the CAMELYON16 test set for the metastasis identification task. We report the overall FROC scores and the true positive fraction at several values for the mean number of false positives per whole-slide image (FPs/WSI). The final FROC true positive fraction score (FROC score) that ranked teams in the this task was defined as the mean true positive fraction at 6 predefined false positive rates: 1/4, 1/2, 1, 2, 4, and 8 FPs per whole-slide image. Note that the pathologist scoring without time constraint had an overall true positive fraction of 72.4% without any false positives.

| Codename         | FROC score | True positive fraction at the different false positive values |             |           |           |           |           |
|------------------|------------|---|-------------|-----------|-----------|-----------|-----------|
|                  |            | 1/4 FPs/WSI   | 1/2 FPs/WSI | 1 FPs/WSI | 2 FPs/WSI | 4 FPs/WSI | 8 FPs/WSI |
| HMS & MIT II     | 0.807      | 0.773   | 0.778       | 0.813     | 0.827     | 0.827     | 0.827     |
| HMS & MGH III    | 0.760      | 0.667   | 0.707       | 0.747     | 0.791     | 0.818     | 0.831     |
| HMS & MGH II     | 0.729      | 0.729   | 0.729       | 0.729     | 0.729     | 0.729     | 0.729     |
| CULab III        | 0.703      | 0.591   | 0.640       | 0.680     | 0.733     | 0.769     | 0.804     |
| HMS & MIT I      | 0.693      | 0.596   | 0.649       | 0.693     | 0.738     | 0.742     | 0.742     |
| HMS & MGH I      | 0.596      | 0.556   | 0.587       | 0.609     | 0.609     | 0.609     | 0.609     |
| RadboudUMC       | 0.575      | 0.493   | 0.524       | 0.569     | 0.600     | 0.631     | 0.631     |
| CULab I          | 0.544      | 0.404   | 0.471       | 0.493     | 0.582     | 0.631     | 0.684     |
| CULab II         | 0.527      | 0.440   | 0.476       | 0.524     | 0.560     | 0.582     | 0.582     |
| ExB              | 0.511      | 0.458   | 0.507       | 0.516     | 0.520     | 0.533     | 0.533     |
| METU             | 0.389      | 0.307   | 0.333       | 0.373     | 0.400     | 0.444     | 0.476     |
| NLP LOGIX        | 0.386      | 0.307   | 0.338       | 0.364     | 0.387     | 0.418     | 0.502     |
| U of Toronto I   | 0.382      | 0.244   | 0.293       | 0.351     | 0.409     | 0.467     | 0.529     |
| Quincy Wong      | 0.367      | 0.333   | 0.351       | 0.360     | 0.378     | 0.382     | 0.396     |
| U of Toronto II  | 0.352      | 0.222   | 0.262       | 0.324     | 0.391     | 0.436     | 0.476     |
| Osaka University | 0.347      | 0.289   | 0.311       | 0.329     | 0.356     | 0.382     | 0.413     |
| Smart Imaging II | 0.339      | 0.289   | 0.338       | 0.351     | 0.351     | 0.351     | 0.351     |
| Warwick-QU       | 0.305      | 0.262   | 0.307       | 0.316     | 0.316     | 0.316     | 0.316     |
| CAMP-TUM II      | 0.273      | 0.213   | 0.240       | 0.258     | 0.276     | 0.298     | 0.356     |
| Tampere I        | 0.257      | 0.178   | 0.196       | 0.227     | 0.267     | 0.311     | 0.364     |
| Tampere II       | 0.252      | 0.200   | 0.204       | 0.240     | 0.267     | 0.289     | 0.311     |
| DeepCare         | 0.243      | 0.000   | 0.000       | 0.364     | 0.364     | 0.364     | 0.364     |
| Minsk Team       | 0.227      | 0.178   | 0.196       | 0.227     | 0.253     | 0.253     | 0.253     |
| Smart Imaging I  | 0.208      | 0.160   | 0.169       | 0.191     | 0.222     | 0.240     | 0.267     |
| HTW-Berlin       | 0.187      | 0.187   | 0.187       | 0.187     | 0.187     | 0.187     | 0.187     |
| CAMP-TUM I       | 0.184      | 0.133   | 0.151       | 0.173     | 0.200     | 0.213     | 0.231     |
| USF              | 0.179      | 0.151   | 0.151       | 0.156     | 0.182     | 0.204     | 0.231     |
| NSS              | 0.165      | 0.160   | 0.160       | 0.164     | 0.169     | 0.169     | 0.169     |
| VISILAB I        | 0.142      | 0.062   | 0.084       | 0.093     | 0.142     | 0.227     | 0.244     |
| LIB              | 0.120      | 0.031   | 0.044       | 0.071     | 0.133     | 0.191     | 0.249     |
| VISILAB II       | 0.116      | 0.058   | 0.080       | 0.089     | 0.111     | 0.178     | 0.182     |
| Anonymous        | 0.097      | 0.031   | 0.058       | 0.071     | 0.098     | 0.142     | 0.182     |

**eTable 5. Summary of results for the whole-slide image classification task (task2)**

eTable 5. Results of the submitted algorithms on the CAMELYON16 test set for the whole-slide image classification task. We report classification AUC for different scenarios: 1) differentiating all tumor slides from normal slides, 2) differentiating slides with macrometastases from normal slides while excluding micrometastases, 3) differentiating slides with micrometastases from normal slides while excluding macrometastases, 4) differentiating slides with primary tumor histotype of infiltrating ductal cancer (IDC) from normal slides while excluding the rarer primary tumor histotypes (non-IDC), and 5) differentiating slides with non-IDC primary histotypes from normal slides while excluding slides with primary tumor histotype of IDC.

| Codename         | All cases  |                 | Macrometastases |                 | Micrometastases |                  | IDC        |                 | Non-IDC    |                 |
|------------------|------------|-----------------|-----------------|-----------------|-----------------|------------------|------------|-----------------|------------|-----------------|
|                  | AUC        | 95% CI          | AUC             | 95% CI          | AUC             | 95% CI           | AUC        | 95% CI          | AUC        | 95% CI          |
| HMS & MIT II     | 0.993<br>5 | 0.983-<br>0.999 | 0.99<br>05      | 0.973-1.0       | 0.99<br>72      | 0.989-1.0        | 0.99<br>26 | 0.979-1.0       | 0.99<br>54 | 0.983-1.0       |
| HMS & MGH III    | 0.976<br>3 | 0.941-<br>0.999 | 1.0             | 1.0-1.0         | 0.95<br>69      | 0.893 –<br>0.999 | 0.97<br>85 | 0.928-1.0       | 0.97<br>12 | 0.920-1.0       |
| HMS & MGH I      | 0.964<br>3 | 0.928-<br>0.989 | 0.99<br>32      | 0.983-1.0       | 0.94<br>07      | 0.876-<br>0.987  | 0.97<br>24 | 0.946-<br>0.993 | 0.94<br>58 | 0.857-<br>0.997 |
| CULab III        | 0.940<br>3 | 0.888-<br>0.980 | 0.98<br>75      | 0.961-1.0       | 0.90<br>19      | 0.812-<br>0.962  | 0.95<br>29 | 0.909-<br>0.983 | 0.91<br>17 | 0.785-<br>0.991 |
| HMS & MIT I      | 0.923<br>4 | 0.855-<br>0.977 | 0.95<br>96      | 0.862-1.0       | 0.89<br>39      | 0.794-<br>0.971  | 0.90<br>55 | 0.807-<br>0.978 | 0.96<br>42 | 0.915-<br>0.996 |
| ExB              | 0.915<br>6 | 0.858-<br>0.962 | 0.99<br>48      | 0.985-1.0       | 0.85<br>09      | 0.749-<br>0.932  | 0.92<br>76 | 0.855-<br>0.981 | 0.88<br>83 | 0.777-<br>0.973 |
| CULab I          | 0.908<br>7 | 0.851-<br>0.954 | 0.99<br>66      | 0.989-1.0       | 0.83<br>70      | 0.742-<br>0.913  | 0.92<br>90 | 0.868-<br>0.974 | 0.86<br>25 | 0.750-<br>0.960 |
| HMS & MGH II     | 0.908<br>2 | 0.846-<br>0.961 | 1.0             | 1.0-1.0         | 0.83<br>33      | 0.738-<br>0.917  | 0.91<br>18 | 0.833-<br>0.968 | 0.90       | 0.795-1.0       |
| CULab II         | 0.905<br>6 | 0.841-<br>0.957 | 0.99<br>26      | 0.972-1.0       | 0.83<br>47      | 0.722-<br>0.925  | 0.93<br>11 | 0.852-<br>0.983 | 0.84<br>79 | 0.720-<br>0.953 |
| DeepCare         | 0.883<br>3 | 0.806-<br>0.943 | 0.97<br>05      | 0.903-1.0       | 0.81<br>23      | 0.704-<br>0.895  | 0.89<br>32 | 0.808-<br>0.954 | 0.86<br>08 | 0.756-<br>0.973 |
| Quincy Wong      | 0.865<br>4 | 0.789-<br>0.924 | 0.98<br>21      | 0.952-1.0       | 0.77<br>03      | 0.634-<br>0.874  | 0.88<br>88 | 0.805-<br>0.953 | 0.81<br>25 | 0.657-<br>0.940 |
| METU             | 0.864<br>2 | 0.786-<br>0.927 | 0.98<br>97      | 0.982-1.0       | 0.76<br>18      | 0.630-<br>0.867  | 0.88<br>77 | 0.802-<br>0.958 | 0.81<br>08 | 0.655-<br>0.941 |
| NLP LOGIX        | 0.829<br>8 | 0.742-<br>0.899 | 0.98<br>63      | 0.951-1.0       | 0.70<br>23      | 0.564-<br>0.812  | 0.88<br>38 | 0.796-<br>0.947 | 0.70<br>75 | 0.538-<br>0.864 |
| Smart Imaging II | 0.820<br>8 | 0.753-<br>0.894 | 0.98<br>18      | 0.962-<br>0.997 | 0.68<br>95      | 0.566-<br>0.791  | 0.82<br>89 | 0.732-<br>0.913 | 0.80<br>25 | 0.664-<br>0.917 |
| U of Toronto I   | 0.814<br>9 | 0.722-<br>0.886 | 0.95<br>14      | 0.866-<br>0.996 | 0.70<br>37      | 0.563-<br>0.804  | 0.86<br>73 | 0.779-<br>0.931 | 0.69<br>63 | 0.517-<br>0.846 |
| Warwick-QU       | 0.795<br>8 | 0.711-<br>0.871 | 0.99<br>09      | 0.971-1.0       | 0.63<br>68      | 0.513-<br>0.733  | 0.83<br>93 | 0.742-<br>0.915 | 0.69<br>71 | 0.547-<br>0.836 |
| Radboudumc       | 0.778<br>6 | 0.694-<br>0.860 | 0.93<br>18      | 0.866-<br>0.992 | 0.65<br>37      | 0.536-<br>0.779  | 0.79<br>23 | 0.690-0.89      | 0.74<br>75 | 0.591-0.88      |
| HTW-Berlin       | 0.767<br>6 | 0.665-<br>0.853 | 0.95<br>91      | 0.872-<br>0.999 | 0.61<br>15      | 0.459-<br>0.736  | 0.76<br>10 | 0.617-<br>0.872 | 0.78<br>25 | 0.627-<br>0.911 |
| U of Toronto II  | 0.762<br>1 | 0.659-<br>0.846 | 0.96<br>98      | 0.923-<br>0.996 | 0.59<br>28      | 0.442-0.71       | 0.82<br>94 | 0.719-0.91      | 0.60<br>96 | 0.394-<br>0.805 |
| Tampere I        | 0.761<br>2 | 0.662-<br>0.837 | 0.96<br>87      | 0.926-<br>0.994 | 0.59<br>21      | 0.472-<br>0.703  | 0.77<br>72 | 0.647-<br>0.875 | 0.72<br>50 | 0.589-<br>0.843 |
| Smart Imaging I  | 0.757<br>4 | 0.663-<br>0.839 | 0.93<br>86      | 0.880-<br>0.977 | 0.60<br>97      | 0.473-<br>0.719  | 0.77<br>06 | 0.639-<br>0.860 | 0.72<br>75 | 0.597-<br>0.845 |
| Osaka University | 0.731<br>9 | 0.629-<br>0.824 | 0.98<br>52      | 0.964-<br>0.998 | 0.52<br>54      | 0.361-<br>0.662  | 0.80<br>51 | 0.686-<br>0.899 | 0.56<br>58 | 0.364-<br>0.762 |
| CAMP-TUM II      | 0.731<br>6 | 0.633-<br>0.819 | 0.95<br>85      | 0.906-<br>0.995 | 0.54<br>68      | 0.409-<br>0.660  | 0.75<br>96 | 0.640-<br>0.855 | 0.66<br>83 | 0.485-<br>0.827 |
| USF              | 0.727<br>0 | 0.611-<br>0.823 | 0.93<br>80      | 0.840-<br>0.995 | 0.55<br>51      | 0.401-<br>0.674  | 0.77<br>06 | 0.636-<br>0.869 | 0.62<br>83 | 0.427-<br>0.820 |
| NSS              | 0.726<br>9 | 0.635-<br>0.81  | 0.85<br>62      | 0.756-<br>0.928 | 0.62<br>15      | 0.511-<br>0.749  | 0.79<br>25 | 0.686-<br>0.877 | 0.67<br>83 | 0.430-<br>0.739 |
| Tampere II       | 0.713<br>3 | 0.612-<br>0.801 | 0.89<br>09      | 0.782-<br>0.964 | 0.56<br>85      | 0.427-0.67       | 0.77<br>65 | 0.669-<br>0.861 | 0.57<br>00 | 0.398-<br>0.734 |
| CAMP-TUM I       | 0.691<br>1 | 0.580-<br>0.787 | 0.88<br>63      | 0.779-<br>0.959 | 0.53<br>19      | 0.407-0.67       | 0.75<br>40 | 0.649-<br>0.846 | 0.54<br>83 | 0.364-<br>0.742 |
| Minsk Team       | 0.689<br>0 | 0.568-<br>0.804 | 0.76<br>93      | 0.568-<br>0.804 | 0.62<br>36      | 0.507-<br>0.783  | 0.74<br>23 | 0.604-<br>0.855 | 0.56<br>83 | 0.348-<br>0.768 |
| VISILAB I        | 0.653<br>2 | 0.551-<br>0.748 | 0.77<br>56      | 0.671-<br>0.878 | 0.55<br>35      | 0.412-<br>0.673  | 0.68<br>07 | 0.572-<br>0.775 | 0.59<br>08 | 0.428-<br>0.776 |
| VISILAB II       | 0.651<br>3 | 0.549-<br>0.742 | 0.76<br>96      | 0.662-<br>0.873 | 0.55<br>49      | 0.413-<br>0.674  | 0.67<br>65 | 0.564-<br>0.766 | 0.59<br>42 | 0.432-<br>0.779 |
| Anonymous        | 0.627<br>7 | 0.530-<br>0.717 | 0.74<br>20      | 0.629-<br>0.838 | 0.53<br>44      | 0.421-<br>0.631  | 0.63<br>64 | 0.531-<br>0.734 | 0.60<br>79 | 0.472-<br>0.732 |
| LIB              | 0.556<br>1 | 0.434-<br>0.654 | 0.81<br>53      | 0.687-0.91      | 0.34<br>49      | 0.219-0.49       | 0.60<br>51 | 0.467-<br>0.724 | 0.44<br>50 | 0.258-<br>0.650 |

## **eMethods.**

### **CAMELYON16 evaluation metrics.**

In the lesion-based evaluation, a lesion was deemed to be identified if the location of the identified region was within the annotated reference standard lesion. If there were multiple findings for a single reference standard region, only the detection with the highest likelihood was considered while the lower likelihood findings were not considered false positives. All detections that were not within a specific distance (75  $\mu\text{m}$ ) from the reference standard annotations were counted as false positives.

In practice, there can be multiple small tumor regions that lie in the proximity of each other. Pathologists, however, consider all of these clusters as a single region. Therefore, it is important to consider them as a single lesion for the evaluation. We followed the guideline described by Cserni et al.<sup>14</sup> for merging these regions. Regions that were two or five cells apart ( $\sim 75\mu\text{m}$ ) were considered as a single entity. Subsequently, we used the following steps to obtain the evaluation masks: (1) Applying distance transform on the inverse binary mask of reference standard, (2) Thresholding the distance transformed image ( $T=154$ ), (3) Labeling the connected components in the binary image. The resulting evaluation mask was a labeled image in which different tumor regions received different unique labels. This evaluation mask was used for the computation of the FROC curve.

### **Method descriptions.**

This section contains the descriptions of all methods that were submitted to the CAMELYON16 challenge, excluding two teams (Anonymous and NSS) that did not submit sufficient details to be included in this section (The scores and ranking of all teams including these two teams are provided in Table 2. For brevity and improved readability, each method is presented in a standardized and formatted fashion. All methods follow a similar workflow: 1) The whole-slide images are preprocessed, 2) A machine learning model for detection of tumor regions is trained, 3) The machine learning model is used to produce a tumor probability map for the slide and 4) The probability map is post-processed to produce tumor lesion locations and scores, and a score for the entire slide. This general workflow is reflected in the structure of the method description. The **Introduction** section highlights key aspects of the method. The **Preprocessing** section contains the description of the steps that were taken to separate the tissue regions in the slides from the non-relevant background and standardize the tissue appearance (e.g. by performing staining normalization). The **Deep learning framework** section, which is relevant only for methods that

use deep learning as the underlying methodology, contains details regarding the neural network architecture, data sampling policy and optimization procedure that was used to train the models. The methods that are based on conventional machine learning approaches have an analogous **Classification framework** section that describes the classification and feature extraction techniques that were used. The **Metastasis identification task** section describes the steps that were taken to compute the locations of the lesions in the whole-slide images along with corresponding probability scores. Finally, the **Whole-slide image classification task** section describes the steps that were taken to compute the probability score for the whole-slide image.



## METHOD 1

Team name: Minsk Team

Authors: Vassili Kovalev, Alexander Kalinovskiy, and Vitali Liauchuk

Affiliation: Department of Biomedical Image Analysis, United Institute of Informatics Problems, Belarus National Academy of Sciences, Surganova St., 6, 220012 Minsk, Belarus

Email: vassili.kovalev@gmail.com

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: two separate CNNs for different scanner types and two iterations of hard-negative mining.

### **Preprocessing**

- Tissue detection: Color thresholding and morphological operations
- Preprocessing magnification: Image level 7 (pixel size =  $31.1 \times 31.1 \mu\text{m}^2$ )
- Staining normalization: None, separate systems were trained for images from different labs

### **Deep learning framework**

Architecture:

- 22-layer GoogLeNet<sup>3</sup>

Patch sampling:

- Patch size:  $256 \times 256$
- Level: 0 (pixel size =  $0.24 \times 0.24 \mu\text{m}^2$ )
- Number of training samples: 150,000 positive and 150,000 negative
- Patch sampling strategy: Two iterations of hard-negative mining were performed. The training set was expanded with patches from regions of non-tumor tissue that the system was initially misclassifying as metastasis.
- Data augmentation: None

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Random sampling from a uniform distribution
- Batch size: 32
- Batch normalization<sup>15</sup>: Yes
- Regularization: 50% dropout<sup>16</sup> in final layers
- Learning rate: Initialized at 0.01 and decreased to  $1.0 \times 10^{-5}$  with exponential decay
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 280,000 iterations

### **Metastasis identification task**

1. The probability map, generated at level 7, was thresholded at 0.99 and post-processed with morphological filtering.
2. Connected components were extracted.
3. Components smaller than 5 pixels were removed.
4. The morphological skeletons of the remaining connected components were extracted.

5. The center of gravity of the component was calculated.
6. The point on the skeleton closest to the center of gravity was selected as the lesion coordinate.
7. The lesion score was calculated as:  $\min(\frac{\text{region size}}{30}, 1)$ .

#### **Whole-slide image classification task**

A histogram of the probability map was calculated. Subsequently, a logistic regression model was trained to map this histogram to a probability value for the entire image.

#### **Results**

This method achieved an FROC true positive fraction score of 0.227 for task 1 and an AUC of 0.689 (95% CI, 0.568 - 0.804) for task 2. The method ranked 23<sup>rd</sup> and 28<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 2

Team name: Radboudumc

Authors: David Tellez

Affiliation: Radboud University Medical Center Nijmegen, Geert Grootteplein-Zuid 10, 6525GA Nijmegen, The Netherlands

Email: David.TellezMartin@radboudumc.nl

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: augmentation with Gaussian blurring and mapping of the tumor probability maps to slide level scores with a second-stage CNN model.

### **Preprocessing**

- Tissue detection: Color thresholding
- Preprocessing magnification: Image level 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 15-layer VGG-like<sup>6</sup> network

Patch sampling:

- Patch size:  $256 \times 256$
- Level: 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ )
- Number of training samples: 150,000 positive and 150,000 negative
- Patch sampling strategy: Patches were sampled uniformly from positive and negative regions. Normal patches were sampled from negative slides as well as non-metastatic regions in tumor slides.
- Data augmentation: Rotation, vertical and horizontal mirroring and random Gaussian blurring

Parameters:

- Optimization method: ADAM<sup>18</sup>
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 16
- Batch normalization<sup>15</sup>: Yes
- Regularization:  $L_2$ -regularization ( $1.0e-6$ ) and 50% dropout<sup>16</sup>
- Learning rate: Exponential learning rate decay when the validation accuracy plateaued for 2,000 iterations
- Activation function: Leaky ReLU<sup>20</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 20,000 iterations

### **Metastasis identification task**

1. The probability maps were eroded and subsequently thresholded.
2. Connected components were extracted from the thresholded probability map.
3. Multiple points were uniformly sampled per region as lesion detection points.
4. The lesion probability was calculated as the mean probability of the pixels inside the connected component.

### **Whole-slide image classification task**

A separate CNN, with the same architecture as the one trained for localizing metastases, was trained taking as input the probability map at low resolution to directly predict whether the slide contains metastasis or not.

### **Results**

This method achieved an FROC true positive fraction score of 0.575 for task 1 and an AUC of 0.779 (95% CI, 0.694 - 0.860) for task 2. The method ranked 7<sup>th</sup> and 17<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 3 & 4

Team name: HMS & MIT (I & II)

Authors: Dayong Wang, Aditya Khosla, Rishab Gargeya, Humayun Irshad, and Andrew Beck

Affiliation: Harvard Medical School (BIDMC) and Massachusetts Institute of Technology (CSAIL), USA

Email: dwang5@bidmc.harvard.edu

### **Introduction**

Two methods were submitted. Both methods are based on deep convolutional neural networks (CNNs). Key aspects include: feature-based post-processing to compute lesion and slide scores and a separately trained model with hard-negative samples. The main difference between the first and second methods are the use of a whole-slide image stain standardization algorithm<sup>21</sup> and more comprehensive data augmentation strategy in the second method.

### **Preprocessing**

- Tissue detection: Conversion to the HSV color space<sup>22</sup> and subsequent Otsu thresholding<sup>23</sup> for each channel. Final tissue mask is achieved by combining the individual channel masks.
- Preprocessing magnification: Image level 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- (Method I) Staining normalization: None
- (Method II) Staining normalization: Whole-slide image color standardizer (WSICS)<sup>21</sup>

### **Deep learning framework**

Architecture:

- 22-layer GoogLeNet<sup>3</sup>

Patch sampling:

- Patch size:  $224 \times 224$
- Level: 0 (pixel size =  $0.24 \times 0.24 \mu\text{m}^2$ )
- Number of training samples: Two million for each class
- Patch sampling strategy: Patches were sampled uniformly from positive and negative regions. Hard-negative mining was performed after initial classification to augment the training set.
- (Method I) Data augmentation: Rotation, random cropping
- (Method II) Data augmentation: Rotation, random cropping and addition of color noise

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Random sampling from a Gaussian distribution
- Batch size: 32
- Batch normalization<sup>15</sup>: No
- Regularization:  $L_2$ -regularization (0.0005) and 50% dropout<sup>16</sup>
- Learning rate: 0.01, multiplied by 0.5 every 50,000 iterations
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 300,000 iterations

### **Metastasis identification task**

1. Obtain probability maps from the initial model (the model without hard-negative mining) and the model with hard-negative mining.

2. Threshold the probability map of the initial model at 0.9.
3. Extract connected components.
4. Take the center point of each connected component as the lesion location.
5. The lesion probability score is calculated as the sum the values in that region in both probability maps.
6. (Method II only) Each lesion score is additionally weighted by the slide-based score (obtained from the whole-slide image classification task).

### **Whole-slide image classification task**

A set of global and local features were calculated for the entire slide. The global features are:

- The ratio between the area of metastatic regions and the tissue area
- The sum of all cancer metastases probabilities detected in the metastasis identification task, divided by the tissue area

These global features were calculated at 5 different thresholds (0.5, 0.6, 0.7, 0.8 and 0.9) resulting in 10 global features.

Local features were calculated based on the two largest metastatic candidate regions at a threshold of 0.5. In total 9 features per region were calculated resulting in a total of 18 features. The local features are:

- Area: The area of connected region
- Eccentricity: The eccentricity of the ellipse that has the same second-moments as the region
- Extend: The ratio of region area over the total bounding box area
- Bounding box area
- Major axis length: The length of the major axis of the ellipse that has the same normalized second central moments as the region
- Max/mean/min intensity: The maximum/mean/minimum probability value in the region
- Aspect ratio of the bounding box
- Solidity: Ratio of region area over the surrounding convex area

Using the 28-length feature vectors a random forest classifier<sup>12</sup> was trained to assign the slide level score.

### **Results**

The first method (HMS & MIT I) achieved an FROC true positive fraction score of 0.693 for task 1 and an AUC of 0.923 (95% CI, 0.855 - 0.977) for task 2. This method ranked 5<sup>th</sup> on both leaderboards. The second method (HMS & MIT II) achieved an FROC true positive fraction score of 0.807 for task 1 and an AUC of 0.993 (95% CI, 0.983 - 0.999) for task 2. This method ranked 1st on both leaderboards.

## METHOD 5

Team name: ExB

Authors: Christian Hass, Elia Bruni

Affiliation: ExB Research and Development

Email: bruni@exb.de

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of the ResNet<sup>4</sup> architecture and varying class balance during training.

### **Preprocessing**

- Tissue detection: The image was divided into 5×5 tiles. For each tile, if the mean color difference between different RGB channels was lower than a threshold, the tile was considered as background.
- Preprocessing magnification: Image level 6 (pixel size = 15.6×15.6 μm<sup>2</sup>)
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 34-layer ResNet<sup>4</sup>

Patch sampling:

- Patch size: 256×256
- Level: 0 (pixel size = 0.24×0.24 μm<sup>2</sup>)
- Number of training samples: 1.6 million
- Patch sampling strategy: Training was started with a balanced sampling between the positive and negative class. As the training proceeded the distribution of positive/negative samples was slowly changed to match the original distribution in the images.
- Data augmentation: Rotation and mirroring

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: MSRA initialization<sup>24</sup>
- Batch size: 16
- Batch normalization<sup>15</sup>: Yes
- Regularization: L<sub>2</sub> regularization (0.0001)
- Learning rate: Initial learning rate of 0.01, which was reduced to 0.001 after 40,000 iterations, and to 0.0001 after 60,000 iterations
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 100,000 iterations

### **Metastasis identification task**

1. Threshold the probability map at level 0 and remove small positive areas (< 834 pixels at a threshold of 0.4) from the probability map
2. Perform regional non-maxima suppression
3. Extract the center of gravity of the remaining regions

4. The lesion score for each region is computed as the maximum probability within the region

#### **Whole-slide image classification task**

The slide score was computed as the maximum score within the slide.

#### **Results**

This method achieved an FROC true positive fraction score of 0.511 for task 1 and an AUC of 0.916 (95% CI, 0.858 - 0.962) for task 2. The method ranked 10<sup>th</sup> and 6<sup>th</sup> in the first and the second leaderboards, respectively.



## METHOD 6

Team name: HTW-Berlin

Authors: Jonas Annuschein, Peter Hufnagl

Affiliation: HTW Berlin, Berlin, Germany

Email: Jonas.Annuschein@student.htw-berlin.de

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of a conditional random field as recurrent neural network<sup>11</sup> on top of a fully convolutional network<sup>25</sup> and the use of a pre-trained network for initialization of weights.

### **Preprocessing**

- Tissue detection: The difference between the red and green channels from the RGB color space was thresholded to identify tissue regions.
- Preprocessing magnification: Image level 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- CRFasRNN<sup>11</sup>

Patch sampling:

- Patch size:  $440 \times 440$
- Level: 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ )
- Number of training samples: 400,000
- Patch sampling strategy: All patches were uniformly sampled from positive slides.
- Data augmentation: Rotation and mirroring

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Pre-trained model trained on the Pascal VOC12 dataset<sup>26</sup>
- Batch size: 1
- Batch normalization<sup>15</sup>: Yes
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: Fine-tuning using a learning rate of  $6.0e^{-13}$
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 3 epochs

### **Metastasis identification task**

1. The probability map was thresholded
2. The center of gravity of each region was considered as the lesion location and the probability value at that location was taken as the lesion score.
3. For low probability regions the surrounding area was scanned and the highest probability was assigned as likelihood for that region to be a metastasis.

### **Whole-slide image classification task**

The slide score was computed as the maximum lesion score within the slide.

### **Results**

This method achieved an FROC true positive fraction score of 0.187 for task 1 and an AUC of 0.768 (95% CI, 0.665 - 0.853) for task 2. The method ranked 25<sup>th</sup> and 18<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 7

Team name: NLP LOGIX

Authors: Matt Berseth

Affiliation: NLP LOGIX, LLC.

Email: matt.berseth@nlplogix.com

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of ADAM optimization<sup>18</sup>, computation of lesion and slide scores with second-stage random forest classifiers<sup>12</sup> and use of GrabCut<sup>27</sup> and watershed transform<sup>28</sup> for lesion segmentation.

### **Preprocessing**

- Tissue detection: The image was divided into non-overlapping 256×256 tiles. Patches that had fewer than 500 unique colors or where the most frequently occurring RGB color code made up more than 90% of the patches pixels were considered background.
- Preprocessing magnification: Image level 0 (pixel size = 0.24×0.24 μm<sup>2</sup>)
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 7-layer AlexNet<sup>1</sup>

Patch sampling:

- Patch size: 256×256
- Level: 0 (pixel size = 0.24×0.24 μm<sup>2</sup>)
- Number of training samples: 250,000
- Patch sampling strategy: 15% positive patches, 85% negative patches
- Data augmentation: Rotation and mirroring

Parameters:

- Optimization method: ADAM<sup>18</sup>
- Weight initialization: Random sampling from a truncated normal distribution
- Batch size: 50
- Batch normalization<sup>15</sup>: Yes
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: 0.0001
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 50,000 iterations (the training was stopped when the validation loss stopped decreasing)

### **Metastasis identification task**

1. Probability map was segmented with GrabCut<sup>27</sup> and watershed segmentation<sup>28</sup>.
2. The center of gravity of each region was considered as the location of the lesion candidate.
3. Summary statistics on cluster size and probability distribution were fed to a random forest classifier<sup>12</sup> to determine the lesion score.

### **Whole-slide image classification task**

Summary metrics from all lesion candidate clusters were calculated and fed to another random forest classifier<sup>12</sup> to determine the slide score.

### **Results**

This method achieved an FROC true positive fraction score of 0.386 for task 1 and an AUC of 0.830 (95% CI, 0.742 - 0.899) for task 2. The method ranked 12<sup>th</sup> and 13<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 8

Team name: Quincy Wong

Authors: Quincy Wong

Affiliation: Independent participant

Email: qwong77@yahoo.ca

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of SegNet<sup>8</sup> architecture (encoder-decoder network) pre-trained with weights from VGG-16<sup>6</sup> and good results with only very limited additional training data.

### **Preprocessing**

- Tissue detection: Tiles containing tissue were selected based on overall intensity value. If the value was too high the tile was considered background.
- Preprocessing magnification: Image level 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 37-layer SegNet<sup>8</sup> (encoder-decoder network)

Patch sampling:

- Patch size:  $480 \times 360$
- Level: 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ )
- Number of training samples: Less than 1000 per class
- Patch sampling strategy: Roughly balanced sampling, manual addition of visually interesting patches
- Data augmentation: Mirroring of only manually selected visually interesting regions

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Pre-trained weights of VGG-16<sup>6</sup>
- Batch size: 2
- Batch normalization<sup>15</sup>: Yes
- Regularization: 50% drop out<sup>16</sup> on selected deeper/middle layers
- Learning rate: 0.001
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 50,000 epochs

### **Metastasis identification task**

1. Candidate lesions were determined by thresholding of the probability map (threshold value of 0.98) and morphologic operations.
2. The regions were downsampled to the resolution of level 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ ).

- Centroids of remaining regions were calculated. Lesions with an area below 50 pixels received a probability penalty of 0.15 for each 4 pixels below 50. Larger centroids were given a bonus but never exceeded 1.0.

### **Whole-slide image classification task**

The slide score were computed as the maximum lesion score within the slide.

### **Results**

This method achieved an FROC true positive fraction score of 0.367 for task 1 and an AUC of 0.865 (95% CI, 0.789 - 0.924) for task 2. The method ranked 14<sup>th</sup> and 11<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 9

Team name: Osaka University

Authors: Seiryō Watanabe, Shigeto Seno, Yoichi Takenaka, Hideo Matsuda

Affiliation: Department of biomedical engineering, Osaka University, Japan

Email: s-wtnb@ist.osaka-u.ac.jp

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of the GoogLeNet<sup>3</sup> architecture and use of an averaging filter in the post-processing stage.

### **Preprocessing**

- Tissue detection: 300×300 tiles were extracted from the image and saved to disk. If the file size (JPEG compressed) was smaller than 18KB the tile was considered background and removed. For the remaining tiles, a threshold of 200 was used on the green and blue color channels to identify background pixels.
- Preprocessing magnification: Image level 0 (pixel size = 0.24×0.24 μm<sup>2</sup>)
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 22-layer GoogLeNet<sup>3</sup>

Patch sampling:

- Patch size: 300×300
- Level: 0 (pixel size = 0.24×0.24 μm<sup>2</sup>)
- Number of training samples: One million
- Patch sampling strategy: Balanced sampling from all training slides
- Data augmentation: None

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Random sampling from a Gaussian distribution
- Batch size: 24
- Batch normalization<sup>15</sup>: No
- Regularization: None
- Learning rate: 0.01
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 10 million iterations

### **Metastasis identification task**

1. Probability maps were generated by first dividing the image at level 0 into non-overlapping patches of size 300×300 and classifying each patch.
2. Pixels in the probability map with a value lower than 0.1 were suppressed.
3. The probability maps were filtered with a local 3×3 averaging filter.
4. The resulting probability map was thresholded (threshold value of 0.5) and the center points of the resulting regions were considered candidate lesions.

5. The lesion scores were computed as the maximum probability value within the regions.

#### **Whole-slide image classification task**

The slide score was computed as the maximum lesion score within the slide.

#### **Results**

This method achieved an FROC true positive fraction score of 0.347 for task 1 and an AUC of 0.732 (95% CI, 0.629 - 0.824) for task 2. The method ranked 16<sup>th</sup> and 23<sup>rd</sup> in the first and the second leaderboards, respectively.



## METHOD 10

Team name: METU

Authors: Ugur Halici, Mustafa Ümit Öner

Affiliation: Departments of Electrical and Electronics Engineering, GSNAS Neuroscience and Neurotechnology, and Graduate School of Informatics, Middle East Technical University, Turkey

Email: halici@metu.edu.tr

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of a custom CNN architecture with relatively few layers yet good performance, and custom confidence filtering for post-processing.

### **Preprocessing**

- Tissue detection: Otsu thresholding
- Preprocessing magnification: Image level 7 (pixel size =  $31.1 \times 31.1 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- Custom CNN – 2 convolutional layers and 2 fully connected layers

Patch sampling:

- Patch size:  $64 \times 64$
- Level: 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ )
- Number of training samples: 240,000 samples per class
- Patch sampling strategy: Negative samples were sampled only from negative slides
- Data augmentation:  $48 \times 48$  random cropping from  $64 \times 64$  patches

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 128
- Batch normalization<sup>15</sup>: No
- Regularization:  $L_2$  regularization (0.0018)
- Learning rate: Initial learning rate was set to 0.1 and updated at 750,000 iterations to 0.01
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 1.125 million iterations

### **Metastasis identification task**

1. The probability map was filtered with Gaussian filters and thresholded.
2. Connected components were extracted. Each connected component was considered a candidate region.
3. For each candidate lesion, the point farthest to the boundaries among points that have probability values in the interval of  $[\max(P) - 0.2, \max(P)]$  was selected as representative.
4. The probability value at the representative location was taken as the lesion score.

**Whole-slide image classification task**

The slide score was computed as the maximum lesion score within the slide.

**Results**

This method achieved an FROC true positive fraction score of 0.389 for task 1 and an AUC of 0.864 (95% CI, 0.786 - 0.927) for task 2. The method ranked 11<sup>th</sup> and 12<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 11

Team name: Warwick-QU

Authors: Muhammad Shaban<sup>1</sup>, Talha Qaiser<sup>2</sup>, Ruqayya Awan<sup>1</sup>, Korsuk Sirinukunwattana<sup>2</sup>, Yee-Wah Tsang<sup>2</sup>, and Nasir Rajpoot<sup>2</sup>

Affiliation: <sup>1</sup>Department of Computer Science and Engineering, College of Engineering, Qatar University

<sup>2</sup>Department of Computer Science, University of Warwick, England

Email: muhammad.shaban@qu.edu.qa

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of a CNN model in the preprocessing stage to segment the tissue regions and use of a U-NET-like<sup>7</sup> architecture for lesion segmentation.

### **Preprocessing**

- Tissue detection: Fully convolutional CNN
- Preprocessing magnification: Image level 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ )
- Staining normalization: Reinhard staining normalization<sup>29</sup>

### **Deep learning framework**

Architecture:

- 15-layer U-NET<sup>7</sup>

Patch sampling:

- Patch size:  $428 \times 428$
- Level: 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ )
- Number of training samples: 8,000 positive and 12,000 negative
- Patch sampling strategy: Positive patches were extracted from all metastasis annotations. Negative patches were extracted with random sampling. Spectral clustering was applied to find visually distinct patches for training for both classes.
- Data augmentation: None

Parameters:

- Optimization method: Adadelta<sup>30</sup>
- Weight initialization: Random initialization
- Batch size: 10
- Batch normalization<sup>15</sup>: No
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: initially set to 0.001
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 120,000 iterations

### **Metastasis identification task**

1. Two binary lesion masks were computed using two different thresholds.
2. Lesion regions with an area ratio of less than 0.2 (computed as the area ratio of the same lesion in the two thresholded masks) were removed from further consideration.
3. The lesion centroid was extracted as the lesion location.

4. The lesion score was extracted as the minimum probability within the lesion weighted by its area.

#### **Whole-slide image classification task**

The probability of the largest tumor region was used as slide probability score.

#### **Results**

This method achieved an FROC true positive fraction score of 0.305 for task 1 and an AUC of 0.796 (95% CI, 0.711 - 0.871) for task 2. The method ranked 18<sup>th</sup> and 16<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 12 & 13

Team name: CAMP-TUM (I & II)

Authors: Bharti Munjal, Amil George, Shadi Albarqouni, Stefanie Demirci, Nassir Navab

Affiliation: Technische Universitat Munchen, Computer Aided Medical Procedure (CAMP), Munich, Germany

Email: shadi.albarqouni@tum.de

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Two submissions were made based on two different network architectures. Key aspects of the method with better performance include: use of the GoogLeNet<sup>3</sup> architecture, hard-negative mining and postprocessing with a random forest classifier<sup>12</sup> trained with region-level features.

### **Preprocessing**

- Tissue detection: Otsu thresholding<sup>23</sup>
- Preprocessing magnification: Image level 3 (pixel size =  $1.94 \times 1.94 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- Method (I): 5-layer AggNet<sup>13</sup> (multi-scale network)
- Method (II): 22-layer GoogLeNet<sup>3</sup>

Patch sampling:

- Patch size: Patches of size  $33 \times 33$  (method I) and  $224 \times 224$  (method II) were extracted from level 3 (pixel size =  $1.94 \times 1.94 \mu\text{m}^2$ ) and level 6 (pixel size =  $15.6 \times 15.6 \mu\text{m}^2$ ), respectively.
- Number of training samples: 2 million patches for method I and 240,000 patches for method II.
- Patch sampling strategy: Initially a CNN model was trained with uniformly sampled patches from level 6. Subsequently, a new CNN model was trained with patches sampled from level 3 including false positives of the first model. Normal patches were sampled from both positive and negative slides.
- Data augmentation: Rotation and flipping.

Parameters:

- Optimization method: Adaptive gradient descent (AdaGrad)<sup>31</sup>
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 32
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: 0.0001
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 1.1 million iterations

### **Metastasis identification task**

For each slide, a probability map was produced using the CNN model trained with patches from level 3. Candidate metastatic regions were detected by smoothing the probability maps with a Gaussian filter and thresholding with a threshold value optimized on a validation set. For method II, further postprocessing was performed. For each candidate in the resulting probability map, the area, orientation, major/minor axis length ratio, and probability map

statistics (max, min, and mean) were extracted. The final probability score for each candidate was produced with a random forest classifier<sup>12</sup> trained with these features.

### **Whole-slide image classification task**

For each slide, a probability score was produced by averaging the probability values of the top three candidate metastases.

### **Results**

The first method (CAMP-TUM I) achieved an FROC true positive fraction score of 0.184 for task 1 and an AUC of 0.691 (95% CI, 0.580 - 0.787) for task 2. This method ranked 26<sup>th</sup> and 27<sup>th</sup> on the first and second leaderboards, respectively. The second method (CAMP-TUM II) achieved an FROC true positive fraction score of 0.273 for task 1 and an AUC of 0.737 (95% CI, 0.633 - 0.819) for task 2. This method ranked 19<sup>th</sup> and 22<sup>nd</sup> on the first and second leaderboards, respectively.

## METHOD 14

Team name: TAMPERE II

Authors: Kaisa Liimatainen, Kimmo Kartasalo, Mira Valkonen, Leena Latonen, Pekka Ruusuvaori

Affiliation: BioMediTech, University of Tampere, Finland

Email: kaisa.liimatainen@tut.fi

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). A key aspect of this method is the use of a VGG-like<sup>6</sup> CNN model.

### **Preprocessing**

- Tissue detection: Otsu thresholding<sup>23</sup> applied to the S component of the HSV color space<sup>22</sup> and morphological operations to remove spurious regions.
- Preprocessing magnification: Image level 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 7-layer VGG-like<sup>6</sup> architecture with five convolutional and two fully connected layers

Patch sampling:

- Patch size:  $32 \times 32$
- Level: 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Number of training samples: 32,000 from both classes
- Patch sampling strategy: Normal patches were uniformly sampled from both negative and positive slides.
- Data augmentation: Translation and flipping

Parameters:

- Optimization method: Stochastic gradient descent with momentum<sup>32</sup>
- Weight initialization: Random sampling from a uniform distribution
- Batch size: 16
- Regularization: None
- Learning rate: Initial learning rate of 0.01 with momentum of 0.9
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 20,000 iterations

**Metastasis identification task**

For each slide, a probability map at image level 6 was produced with the trained CNN model. Candidate metastatic regions were detected by max-filtering of the probability map with 3×3 kernel, thresholding, and removal of small connected components. The remaining connected components in the thresholded probability map were considered candidate regions with probability scores equal to the maximum probability value within the region.

**Whole-slide image classification task**

The slide score was computed as the maximum lesion score within the slide.

**Results**

This method achieved an FROC true positive fraction score of 0.252 for task 1 and an AUC of 0.713 (95% CI, 0.612 - 0.801) for task 2. The method ranked 21<sup>st</sup> and 26<sup>th</sup> in the first and the second leaderboards, respectively.



## METHOD 15 & 16

Team name: VISILAB (I & II)

Authors: M. Milagro Fernandez-Carrobles, Ismael Serrano, Oscar Deniz, Gloria Bueno

Affiliation: VISILAB, E.T.S.I.I, University of Castilla-La Mancha, Ciudad Real, Spain

Email: Gloria.Bueno@uclm.es

### **Introduction**

This method is based on a random forest classifier<sup>12</sup> using texture features. The authors performed a comparative analysis with a CNN-based method (method II).

### **Preprocessing**

- Tissue detection: Color thresholding
- Preprocessing magnification: Level 6 (pixel size =  $15.55 \times 15.55 \mu\text{m}^2$ )
- Staining normalization: None

### **Classification framework:**

Classifier:

- Method I: Random forest classifiers<sup>12</sup> with 50 decision trees
- Method II: 3-layer CNN with two convolutional layers

Features for metastasis identification (method I):

- Haralick texture features<sup>33</sup>

Features for whole-slide image classification (method I):

- Morphometric features: Area, convex area, convex hull, Euler number, extent, fill area, major axis length, minor axis length, perimeter, solidity.
- Geometric features: Bounding box, centroid, eccentricity, equivalent diameter, orientation, extrema.

Patch sampling:

- Patch size: For method I, patches of size  $400 \times 400$  from level 0 were extracted. These patches were resampled to a size of  $40 \times 40$  for the CNN used in method II.
- Number of training samples: 90,000 positive samples and 8.5 million negative samples
- Patch sampling strategy: Uniform sampling. Normal patches were sampled from both negative and positive slides.

Parameters (method II):

- Optimization method: Stochastic gradient descent with momentum<sup>32</sup>
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 64
- Regularization:  $L_2$  regularization (0.0005)
- Learning rate: 0.0005 with momentum 0.9
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 480 iterations

### **Metastasis identification task**

For method I, for each slide, all non-overlapping regions of size 400×400 from level 0 were classified as metastasis or non-metastasis using the random forest classifier and Haralick texture features. For method II, the probability maps were generated using the trained CNN. In both methods, the resulting probability map was thresholded with a threshold value of 0.7, and post-processed with morphological operators to connect neighboring regions using a dilation operation with a disk-shaped structuring element with radius 10.

### **Whole-slide image classification task**

For each region, several morphometric and geometric features (in the probability map) were extracted such as: area, bounding box, centroid, convex area, convex hull, eccentricity, equivalent diameter, Euler number, extent, filled area, major axis length, minor axis length, orientation, perimeter, extrema and solidity (features from the MATLAB *regionprops* function). Subsequently, for each slide, these region-based features were summarized by calculating the mean, standard deviation, sum, minimum, maximum, median, mode, variance, covariance, kurtosis and skewness of each feature. Finally an SVM classifier was used to compute a score for each slide.

### **Results**

The first method (VISILAB I) achieved an FROC true positive fraction score of 0.142 for task 1 and an AUC of 0.653 (95% CI, 0.551 - 0.748) for task 2. This method ranked 29<sup>th</sup> on both leaderboards. The second method (VISILAB II) achieved an FROC true positive fraction score of 0.116 for task 1 and an AUC of 0.651 (95% CI, 0.549 - 0.742) for task 2. This method ranked 31<sup>st</sup> and 30<sup>th</sup> on the first and second leaderboards, respectively.

## METHOD 17 & 18

Team name: U of Toronto (I & II)

Authors: Oren Kraus

Affiliation: University of Toronto, Electrical and Computer Engineering, Canada

Email: oren.kraus@mail.utoronto.ca

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: use of multiple CNN models trained at different magnification levels and use of learned deconvolutional layers for upsampling. Two different approaches for merging the results from multiple CNNs were investigated, which resulted in two submissions.

### **Preprocessing**

- Tissue detection: Otsu thresholding<sup>23</sup>
- Preprocessing magnification: Image level 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- 10-layer VGG-like<sup>6</sup> fully convolutional neural network<sup>25</sup>

Patch sampling

- Patch size:  $300 \times 300$  tiles from levels 2 (pixel size =  $0.97 \times 0.97 \mu\text{m}^2$ ), 3 (pixel size =  $1.9 \times 1.9 \mu\text{m}^2$ ), 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ ) and 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ ).
- Number of training samples: 18,432
- Patch sampling strategy: For positive slides, one third of the patches were sampled from positive regions, one third from metastasis border regions, and one third from negative regions. The number of patches sampled from each slide was proportional to the tissue area.
- Data augmentation: Rotation, translation, and flipping

Parameters:

- Optimization method: Adam<sup>18</sup>
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 16
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: 0.0003
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 3.6 million iterations

### **Metastasis identification task**

Two different approaches were used for computing probability maps. The first method took the mean across different scales as the final probability map. In the second method, the outputs of the CNNs trained at different magnification were used as inputs to another CNN model that produced a merged probability map. The final probability map was thresholded and postprocessed with morphological operators to identify positive regions. The probability score of each region was defined as the maximum value of the probability map within the region.

### **Whole-slide image classification task**

The probability score for each whole-slide image was produced with a logistic regression classifier trained with features describing the detected metastatic regions: mean, min., max. probability score and size features.

### **Results**

The first method (U of Toronto I) achieved an FROC true positive fraction score of 0.352 for task 1 and an AUC of 0.815 (95% CI, 0.722 - 0.886) for task 2. This method ranked 15<sup>th</sup> on both leaderboards. The second method (U of Toronto II) achieved an FROC true positive fraction score of 0.382 for task 1 and an AUC of 0.762 (95% CI, 0.659 - 0.846) for task 2. This method ranked 13<sup>th</sup> and 19<sup>th</sup> on the first and second leaderboards, respectively.

## METHOD 19

Team name: USF

Authors: Hady Ahmady Phoulady

Affiliation: University of South Florida, Tampa, USA

Email: parham.ap@gmail.com

### **Introduction**

This method is based on a random forest classifier<sup>12</sup> using color and texture features. A key aspect of this method is the use of a lymphocyte probability map in the preprocessing step to exclude non-tumor regions.

### **Preprocessing**

- Tissue detection: Thresholding of a lymphocyte probability map using a hierarchical multilevel thresholding method<sup>34</sup> to exclude non-tumor regions
- Preprocessing magnification: Level 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ )
- Staining normalization: None

### **Classification framework:**

Classifier:

- Random forest classifier<sup>12</sup>

Features:

- Grayscale intensity histogram
- Gray-level concurrence features<sup>33</sup>
- Local binary patterns<sup>35</sup>

Patch sampling:

- Patch size:  $101 \times 101$
- Level: 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ )
- Number of training samples: 500,000 positive samples and one million negative samples
- Patch sampling strategy: Patches were sampled with higher frequency in metastatic regions. Normal patches were sampled from both negative and positive slides.

### **Metastasis identification task**

The random forest classifier was used to produce a probability map that was post-processed with Gaussian filtering and thresholded to obtain metastatic regions. Each region was assigned a probability score equal to the mean of the probability of the region.

### **Whole-slide image classification task**

The probability score for each whole-slide image was computed as the weighted arithmetic mean (with weights 3 and 1) of the two metastatic regions with the highest probability scores.

### **Results**

This method achieved an FROC true positive fraction score of 0.179 for task 1 and an AUC of 0.727 (95% CI, 0.611 - 0.823) for task 2. The method ranked 27<sup>th</sup> and 24<sup>th</sup> in the first and the second leaderboards, respectively.

## METHOD 20

Team name: TAMPERE I

Authors: Mira Valkonen, Kimmo Kartasalo, Kaisa Liimatainen, Leena Latonen, Pekka Ruusuvaori

Affiliation: BioMediTech, University of Tampere, Finland

Email: valkonen.mira@gmail.com;

### **Introduction**

This method is based on a random forest classifier<sup>12</sup> using texture features. A key aspect of this method is the use of nuclei density features.

### **Preprocessing**

- Tissue detection: Otsu thresholding<sup>23</sup> applied to the S component from the HSV color space<sup>22</sup> and morphological operations to remove spurious regions.
- Preprocessing magnification: Image level 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Staining normalization: Histogram matching

### **Classification framework:**

Classifier:

- Random forest classifier<sup>12</sup> with 50 classification trees

Features:

- Gray-level concurrence features<sup>33</sup>
- SIFT descriptors<sup>36</sup>
- Local binary patterns<sup>35</sup>
- Histogram of oriented gradients (HOG)<sup>37</sup>
- The independent elements of the co-variance matrix of the ellipses fitted to the extracted maximally stable extremal regions (MSER)<sup>38</sup> and number of MSER regions.
- All texture features were extracted from both the hematoxylin and eosin channels obtained with color deconvolution<sup>39</sup>.
- Nuclei density descriptors (mean inter-nuclei distance and number of nuclei) from watershed-based nuclei segmentation.

Patch sampling:

- Patch size:  $200 \times 200$
- Level: 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Number of training samples: 200,000 positive samples and 200,000 negative samples
- Patch sampling strategy: Normal patches were randomly sampled from both negative and positive slides, including metastatic region borders.

### **Metastasis identification task**

For each slide, a probability map was produced with the trained random forest classifier. Candidate metastatic regions were detected by max. filtering of the probability map, thresholding, and connected component analysis. The connected components in the thresholded probability map were considered candidate regions with probability scores equal to the mean probability value within the region.

### **Whole-slide image classification task**

The slide score was computed as the maximum score within the slide.

### **Results**

This method achieved an FROC true positive fraction score of 0.257 for task 1 and an AUC of 0.761 (95% CI, 0.662 - 0.837) for task 2. The method ranked 20<sup>th</sup> on both leaderboards.

## METHOD 21 & 22

Team name: SMART IMAGING (I & II)

Authors: Vitali Khvatkov, Alexei Vylegzhanin

Affiliation: Smart Imaging Technologies Co., US

Email: vitali.khvatkov@simagis.us

### **Introduction**

This team submitted two methods for evaluation. The first method uses a conventional machine learning approach, while the second method is based on a combination of deep learning and conventional machine learning using handcrafted features. Key aspects include: multiscale analysis, use of nuclei density features and use of the GoogLeNet<sup>3</sup> architecture. The proposed solution is available on the Simagis Live platform (<http://web-pathology.net>).

### **Preprocessing**

- Tissue detection: Ensemble of SVM classifiers with 27 color and texture features
- Preprocessing magnification: Image level 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ )
- Staining normalization: Transform color coordinates to modified HSV color space<sup>22</sup> as follows, (1) transform color to HSV space; (2) shift Hue by 160 by subtracting/adding 160 from/to H value, (3) trim white color by removing pixels with V (value) above 0.9 threshold, (4) cluster to 3 phase system by K-mean clustering of pixel colors in modified HSV color system. Normalized images have been used in all detection/classification steps of the algorithm.

### **Classification framework (method I):**

Classifier:

- Ensemble of SVM classifiers<sup>9</sup> used to classify patches at 3 different resolutions.
- Candidate regions produced by the SVM classifiers were further processed using multiscale cascade of AdaBoost<sup>10</sup> models.

Features:

- Combination of rotation-invariant local binary patterns<sup>35</sup> and color features (features selection and optimization was done using the *caret* package in R).

Patch sampling:

- Patch sampling strategy: Normal patches were sampled from both positive and negative slides. The patch sizes for the different resolutions are given in the table below.

| Level   | Pixel Size ( $\mu\text{m}$ )     | Patch Size (pixels) | Patches from "tumor" class | Patches from "negative" class |
|---------|----------------------------------|---------------------|----------------------------|-------------------------------|
| Level 1 | $0.24 \times 0.24 \mu\text{m}^2$ | 16x16               | 12630                      | 11449                         |
| Level 2 | $0.49 \times 0.49 \mu\text{m}^2$ | 64x64               | 6296                       | 7907                          |
| Level 3 | $1.90 \times 1.90 \mu\text{m}^2$ | 128x128             | 6296                       | 7907                          |

### **Deep learning framework (method II)**

Architecture:

- 22-layer GoogLeNet<sup>3</sup>



#### Patch sampling:

- Patch size: 128×128 from
- Level: 1 (pixel size = 0.49×0.49 μm<sup>2</sup>)
- Number of training samples: 14,000
- Patch sampling strategy: Equal number of positive and negative patches were randomly sampled. Normal patches were sampled from both negative and positive slides.
- Data augmentation: Translation, rotation, and flipping

#### Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Xavier's method<sup>19</sup>
- Batch size: 128
- Regularization: 50% dropout<sup>16</sup>
- Learning rate: 0.01
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 420,000 iterations

#### Metastasis identification task

The probability maps for the first method were computed using the Adaboost classifier. The probability maps for the second method were produced with a combination of the Adaboost and CNN classifiers. Candidate lesions were localized with the geographic clustering algorithm<sup>40</sup>. Geographic clustering algorithm identified geographic clusters of tiles and center of cluster on slide. The composite probability for each candidate was computed as weighted mean of probability of tiles in the cluster. The weights for each cluster member (tile) was computed using the measure of “compactness”.

#### Whole-slide image classification task

The slide scores were produced with a SVM classifier that uses features that summarize the distribution of the candidate lesions in the slide.

#### Results

The first method (SMART IMAGING I) achieved an FROC true positive fraction score of 0.208 for task 1 and an AUC of 0.757 (95% CI, 0. 0.663 - 0.839) for task 2. This method ranked 24<sup>th</sup> and 21<sup>st</sup> on the first and second leaderboards, respectively. The second method (SMART IMAGING II) achieved an FROC true positive fraction score of 0.339 for task 1 and an AUC of 0.821 (95% CI, 0.753 - 0.894) for task 2. This method ranked 17<sup>th</sup> and 14<sup>th</sup> on the first and second leaderboards, respectively.

## METHOD 23, 24 & 25

Team name: CULab (I, II & III)

Authors: Hao Chen, Huang-Jing Lin, Qi Dou, and Pheng-Ann Heng

Affiliation: Department of Computer Science and Engineering, The Chinese University of Hong Kong, Sha Tin, Hong Kong

Email: jackie.haochen@gmail.com

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). There are three submissions by this team, each employing a different CNN architecture. A key aspect of the best performing method is the use of a fully convolutional architecture for dense predictions.

### **Preprocessing**

- Tissue detection: Color thresholding
- Preprocessing magnification: Image level 5 (pixel size =  $7.8 \times 7.8 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- Method I: VGG-16<sup>6</sup>
- Method II: Cascade of two CNNs<sup>41</sup>. The first CNN (VGG-16) works with lower magnification images (level 1), has very high sensitivity and quickly eliminates many negative regions. The second CNN, a 152-layer ResNet architecture<sup>4</sup>, refines the results from the first model.
- Method III: Fully convolutional network adapted from VGG-16<sup>6</sup> for dense predictions

Patch sampling:

- Patch size:  $224 \times 224$  for second CNN of method II;  $244 \times 244$  for other networks.
- Level: 0 (pixel size =  $0.24 \times 0.24 \mu\text{m}^2$ ) used for method III and the second CNN of method II. Level 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ ) used for method I and the first CNN of method II.
- Number of training samples: 15 million (5% positive)
- Patch sampling strategy: Uniform sampling
- Data augmentation: Translation and flipping

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Pre-trained with the ImageNet dataset<sup>5</sup>
- Batch size: 10 for ResNet-152, and 50 for the other architectures
- Regularization:  $L_2$  regularization (0.0005)
- Learning rate: Initially set at 0.001 and decreased by a factor of 10 every 100,000 iterations.
- Activation function: ReLU<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 300,000 iterations

### **Metastasis identification task**

For each slide, a probability map was produced using the trained CNN model (at level 0 with a stride of 32). Candidate metastatic regions were detected by filtering the probability map with a median filter (kernel size of  $3 \times 3$ )

and thresholding. Each connected component in the resulting probability map was considered a candidate detection with a probability score equal to the maximum probability value within the region. This procedure was used for all three methods.

### **Whole-slide image classification task**

The slide score was computed as the maximum score within the slide.

### **Results**

The first method (CULab I) achieved an FROC true positive fraction score of 0.544 for task 1 and an AUC of 0.909 (95% CI, 0.851 - 0.954) for task 2. This method ranked 8<sup>th</sup> and 7<sup>st</sup> on the first and second leaderboards, respectively. The second method (CULab II) achieved an FROC true positive fraction score of 0.527 for task 1 and an AUC of 0.906 (95% CI, 0.841 - 0.957) for task 2. This method ranked 9<sup>th</sup> on both leaderboards. The third method (CULab III) achieved an FROC true positive fraction score of 0.703 for task 1 and an AUC of 0.942 (95% CI, 0.888 - 0.980) for task 2. This method ranked 4<sup>th</sup> on both leaderboards.

## METHOD 26

Team name: DeepCare

Authors: Tong Xu

Affiliation: DeepCare Inc.

Email: txu@deepcare.com

### **Introduction**

This method is based on deep convolutional neural networks (CNNs). Key aspects include: the use of the pre-trained GoogLeNet<sup>3</sup> architecture and a second-stage SVM classifier for computing slide scores.

### **Preprocessing**

- Tissue detection: Multi-thresholding in the HSV<sup>22</sup> color space.
- Preprocessing magnification: Image level 3 (pixel size =  $1.94 \times 1.94 \mu m^2$ )
- Color normalization: None

### **Deep learning framework**

Architecture:

- 22-layer GoogLeNet<sup>3</sup>

Patch sampling:

- Patch size: 256×256
- Level : 0 (pixel size =  $0.24 \times 0.24 \mu m^2$ )
- Number of training samples: 700,000
- Patch sampling strategy: Patches were uniformly sampled from positive and negative regions. Negative samples were taken from both positive and negative slides. For positive slides, additional negative samples were taken from regions bordering metastatic regions.
- Data augmentation: Mirroring and rotation of the positive samples

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Pretrained GoogLeNet model with the ImageNet dataset<sup>5</sup>
- Batch size: 64
- Batch normalization<sup>15</sup>: Yes
- Regularization: L<sub>2</sub> regularization (0.0005)
- Learning rate: Initialized at 0.01 and decreased every 100,000 iterations by a factor of 0.1
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy
- Number of training epochs/iterations: 120,000 iterations

### **Metastasis identification task**

Using the trained GoogLeNet model, a probability map was generated for each slide. Candidate regions were produced with connected component analysis. Regions with an area smaller than 20 pixels were rejected as false positives. The lesion scores were computed as the mean of the probability values within the region. The center of gravity and the probability score of the lesions with a probability higher than 0.85 were reported.

### **Whole-slide image classification task**

For each whole-slide image, five binary masks containing metastatic connected components were generated by applying multiple thresholds of 0.5, 0.6, 0.7, 0.8 and 0.9 on the probability map. Subsequently, two types of features including 5 shape and 3 statistics-based probability features were extracted from the five multi-thresholded regions. These features include:

- Area
- Eccentricity
- Major and minor axis length of the ellipse that has the same normalized second central moments as the region
- Ratio of pixels in the region to the pixels in the total bounding box
- The mean, maximum, and variance of the probability values inside the multi-thresholded regions of each candidate

Overall, a 40-dimensional feature vector was extracted from each candidate region. The normalized 40-dimensional feature vectors were then fed into a SVM classifier<sup>9</sup> to discriminate between tumor and non-tumor regions. The trained SVM classifier was used to discriminate annotated metastases in positive slides from candidate findings in negative whole-slide images. The probability score for the whole-slide images were computed as the weighted mean of the detected tumor regions present in the whole-slide images.

### **Results**

This method achieved an FROC true positive fraction score of 0.243 for task 1 and an AUC of 0.883 (95% CI, 0.806 - 0.943) for task 2. The method ranked 22<sup>nd</sup> and 10<sup>th</sup> on the first and second leaderboards, respectively.

## METHOD 27

Team name: LIB

Authors: R. Venâncio, B. Ben Cheikh, A. Coron, and D. Racoceanu

Affiliation: Sorbonne Université, UPMC Univ Paris 06, CNRS, INSERM, Laboratoire d'Imagerie Biomédicale (LIB), Paris, France

Email: rui.venancio.t@gmail.com

### **Introduction**

This method is based on a SVM<sup>9</sup> classifier using color and texture features for automated detection of metastatic cancer from whole-slide images of sentinel lymph nodes.

### **Preprocessing**

- Tissue detection: *K*-means clustering
- Preprocessing magnification: Level 4 (pixel size =  $3.9 \times 3.9 \mu\text{m}^2$ )
- Staining normalization: Reinhard staining normalization<sup>29</sup>

### **Classification framework:**

Classifier:

- SVM<sup>9</sup>

Features:

- Haralick texture features<sup>33</sup>
- Law's texture energy measures<sup>42</sup>
- Features were selected with sequential forward selection

Patch sampling:

- Patch size:  $800 \times 800$
- Level: 0 (pixel size =  $0.24 \times 0.24 \mu\text{m}^2$ )
- Number of training samples: 1,100 positive and 1,130 negative
- Patch sampling strategy: Patches were sampled uniformly from positive and negative regions. Negative samples were taken from both positive and negative slides.

### **Metastasis identification task**

The slides were divided in rectangular patches. Each patch was classified as positive or negative. The centroids of regions larger than four connected positive patches were selected as candidate lesion locations. The lesion scores were calculated as the mean of the probability values of all patches within the region.

### **Whole-slide image classification task**

If the number of positive patches in a whole-slide image was larger than 11, the mean of the probabilities of all positive patches was calculated and reported as the whole-slide score.

### **Results**

This method achieved an FROC true positive fraction score of 0.120 for task 1 and an AUC of 0.556 (95% CI, 0.434 - 0.654) for task 2. The method ranked 30<sup>th</sup> and 32<sup>nd</sup> on the first and second leaderboards, respectively.

## METHOD 28, 29 & 30

Team name: HMS-MGH (I, II & III)

Authors: Aoxiao Zhong, Quanzheng Li

Affiliation: Gordon Center for Medical Imaging, Clinical Data Science Center, Harvard Medical School, Massachusetts General Hospital

Email: zhongaoxiao@gmail.com

### **Introduction**

Three methods were submitted. The first two submissions are similar to the methods of the Harvard & MIT team, based on patch-wise classification using GoogLeNet<sup>3</sup> and ResNet-101<sup>4</sup>, respectively. The third submission is based on dense prediction using fully convolutional ResNet-101 architecture with atrous convolution and atrous spatial pyramid pooling<sup>43</sup>.

### **Preprocessing**

- Tissue detection: Otsu thresholding<sup>23</sup>
- Preprocessing magnification: Image level 5 (pixel size =  $0.78 \times 0.78 \mu\text{m}^2$ )
- Staining normalization: None

### **Deep learning framework**

Architecture:

- Method I: GoogLeNet<sup>3</sup>
- Method II: ResNet-101<sup>4</sup>
- Method III: Fully convolutional ResNet-101 architecture with atrous convolution and atrous spatial pyramid pooling (deeplab v2<sup>43</sup>)

Patch sampling:

- Patch size:  $224 \times 224$  for methods I and II, and  $512 \times 512$  for method III
- Level: 0 (pixel size =  $0.24 \times 0.24 \mu\text{m}^2$ ) for methods I and II, and level 1 (pixel size =  $0.49 \times 0.49 \mu\text{m}^2$ ) for method III
- Number of training samples: 400,000 with 25% of positive patches for methods I and II. On-line sampling with approximately 25% positive samples for method III.
- Patch sampling strategy: Negative patches were sampled from both negative slides and normal regions in positive slides.
- Data augmentation: Mirroring and random cropping for all methods

Parameters:

- Optimization method: Stochastic gradient descent
- Weight initialization: Pre-trained model with the ImageNet dataset<sup>5</sup> for methods I and II, and pre-trained model with the MS-COCO dataset<sup>44</sup> for method III.
- Batch size: 64 for method I, 128 for method II, 10 for method III
- Regularization:  $L_2$  regularization was used for all methods. The regularization coefficients were 0.0002, 0.0001, and 0.0005 for methods I, II and III, respectively.
- Learning rate: The learning rate was initialized at 0.001 and divided by 10 when the error plateaued for method I and II. The learning rate was initialized at  $2.5 \times 10^{-4}$  and multiplied by 0.9 every 40,000 iterations for method III.
- Activation function: ReLu<sup>17</sup>
- Loss function: Cross-entropy

- Number of training epochs/iterations: 150,000 iterations for method I, 180,000 iterations for method II and 40,000 iterations for method III

### **Metastasis identification task**

1. Perform connected component analysis of the thresholded probability map (the threshold was set to 0.9 for methods I and II and 0.95 for method III).
2. The centroids of the connected components were used as candidate location.
3. The mean probability values of the connected components were used as the lesion scores.
4. Regions with major-axis length smaller than 200  $\mu\text{m}$  were removed as false positives.

### **Whole-slide image classification task**

Higher level features were extracted from the tumor heatmaps (computed using the *regionprops* function in *skimage*<sup>45</sup>) with thresholds of 0.5 and 0.9 for methods I and II, and thresholds of 0.5 and 0.95 for method III. All these features are computed for the largest detected candidate in the whole-slide image:

- The major axis length
- The ratio between the area of the candidate region and the total bounding box area
- Eccentricity of the ellipse that has the same second-order moments as the region
- Total area
- Mean intensity

A random forest classifier<sup>12</sup> was trained with these features and subsequently used to produce the probability score for each slide.

### **Results**

The first method (HMS-MGH I) achieved an FROC true positive fraction score of 0.596 for task 1 and an AUC of 0.965 (95% CI, 0.928 - 0.989) for task 2. This method ranked 6<sup>th</sup> and 3<sup>rd</sup> on the first and second leaderboards, respectively. The second method (HMS-MGH II) achieved an FROC true positive fraction score of 0.729 for task 1 and an AUC of 0.908 (95% CI, 0.846 - 0.961) for task 2. This method ranked 3<sup>rd</sup> and 8<sup>th</sup> on the first and second leaderboards, respectively. The third method (HMS-MGH III) achieved an FROC true positive fraction score of 0.760 for task 1 and an AUC of 0.976 (95% CI, 0.941 - 0.999) for task 2. This method ranked 2<sup>nd</sup> on both leaderboards.



## eResults

### Stratification according to metastasis size and primary tumor histotype in task 2

The pathologists' results were further analyzed in two subcategories: analysis according to metastasis size and primary tumor histotype (eTable 1 and eTable 2 in the Supplement). Pathologist without time constraint achieved a better sensitivity and AUC for detecting macrometastases (sensitivity of 100% and AUC of 0.994 (95% CI, 0.977-1.0)) and metastases originating from infiltrating ductal carcinoma (IDC) (sensitivity of 97.0% (95% CI, 89.7%-100%) and AUC of 0.976 (95% CI, 0.932-1.0)) compared to micrometastases (sensitivity of 88.8% (95% CI, 75.0%-100%) and AUC of 0.943 (95% CI, 0.868-0.995)) and non-IDC cases (sensitivity of 86.6% (95% CI, 66.7%-100%) and AUC of 0.943 (95% CI, 0.848-1.0)), respectively (no statistically significant difference for comparison of AUCs,  $p=0.87$  (Bonferroni corrected) for comparison of the performance for the detection of micro and macrometastases, and  $p>0.99$  for comparison of the performance for the detection of IDC and non-IDC cases). For all 11 pathologists in the simulated routine diagnostic setting, the performance was significantly higher (See eTable 2 for individual p-values) for detection of macrometastases (mean sensitivity of 92.9% (95% CI, 90.5%-95.8%) and mean AUC of 0.964 (range, 0.924-1.0)) compared to micrometastases (mean sensitivity of 38.3% (95% CI, 32.6%-52.9%) and mean AUC of 0.685 (range, 0.582-0.808)). We also observed that metastases originating from IDC (mean sensitivity of 69.2% (95% CI, 65.4%-77.4%) and mean AUC of 0.842 (range, 0.773-0.924)) were more often detected compared to non-IDC cases (mean sensitivity of 48.4% (95% CI, 43.2%-59.7%) and mean AUC of 0.738 (range, 0.656-0.862)) (but not significantly, see eTable2 for the p-values for each pathologist).

The top-ranking systems performed similarly to the best performing pathologists in detecting macrometastases. The performance of the algorithms in detecting micrometastases, however, was considerably more variable. Many of the top-ranked algorithms achieved better AUCs than the best pathologist in the panel of 11 (best pathologist AUC = 0.808 (95% CI, 0.704-0.908) versus best algorithm AUC = 0.997 (95% CI, 0.989-1.0)) in detecting micrometastases. The AUC of the two leading algorithms (AUC = 0.997 (95% CI, 0.989-1.0) and 0.957 (95% CI, 0.893-0.999), respectively) even surpassed that of the pathologist without time constraint (AUC = 0.9430 (95% CI, 0.868-0.995)).

With regard to the primary tumor histotype, the majority of the algorithms had higher AUCs for detecting IDC metastases than metastases of other types. The top-four performing algorithms achieved higher AUCs than the panel of 11 pathologists in detecting metastases of both IDC and non-IDC histotypes (see eTables 2 and eTable5).

## **eDiscussion**

### **Potential reasons for large variability in CNN performance**

The modest performance of some of the algorithms based on convolutional neural networks (CNN), in many cases, could be attributed to choosing a low magnification to process the slide, or selecting a very small patch size for training. Consequently, the system either lacks the detailed information present in the higher magnifications or loses the contextual information that could be captured by a larger patch size. Despite using the right magnification, patch size and state-of-the-art CNN architectures, achieving satisfactory results can be challenging. Training deep learning models can involve many hyperparameter settings (e.g. learning rate, regularization strength, mini-batch size, etc.). Successful and efficient training and debugging of large scale CNNs requires careful selection and adjustment on these hyperparameters, and finding out the relation between hyperparameters and validation errors.

### **Properties of the top-performing algorithms**

We can summarize the main properties of the high-ranked teams based on 4 main characteristics: network architecture, patch-sampling strategy, preprocessing and data augmentation, and network ensemble.

One common property of the leading teams is that they all used very deep state-of-the-art CNN architectures such as GoogLeNet<sup>3</sup>, VGG-Net<sup>6</sup>, and ResNet<sup>4</sup>. The leading team, HMS & MIT (II), trained a 22-layer GoogLeNet model and enriched the training data by adding false positive findings produced by an initial model. By doing this, the network becomes more knowledgeable on recognizing the more difficult normal regions. The CNNs used in systems HMS & MGH (III), HMS & MGH (II), and CULab (III) were ResNet-101, GoogLeNet-22 and VGG-Net-16, respectively, all initialized by weights from pre-trained networks and fine-tuned with the challenge data. ResNet-101 was pre-trained on the MS-COCO dataset<sup>44</sup> and the other two models were pre-trained on the large scale 1000-class ImageNet dataset<sup>5</sup>. The high performance of these methods is in accordance with previous studies which have validated the efficacy of transfer learning strategies<sup>46-48</sup>. Some of the key factors contributing to the outstanding performance of the HMS & MIT (II) system were the use of the whole-slide image color standardizer (WSICS) algorithm<sup>21</sup> to normalize the appearance of whole-slide images, and the incorporation of a more rigorous data augmentation strategy including rotation, flipping, random cropping, and the addition of random offsets to each RGB color channel. The ResNet-101 model used in the system of HMS & MGH (III) used very large image patches of size 512×512 that were more than double the input size of all the other systems used in this challenge. On top of

that, the use of atrous convolution (dilated convolution) and spatial pyramid pooling<sup>43</sup> enabled the system to capture objects as well as image context at multiple scales.

Another factor contributing to the success of some of the top-ranking algorithms is the use of network ensembles. The winning team used an ensemble of a network trained on standardized whole-slide images and a network trained on original whole-slide images to report the probabilities for each finding. The first submission of this team, HMS & MIT (I), ranking fifth, used an ensemble of two networks (networks trained before and after hard-negative mining).

To generate a slide based score for the second task, the majority of the teams assigned the maximum probability among the detected lesions in the whole-slide image as the confidence score for that slide. Prior to this assignment, they mostly removed small areas of positive findings, and/or applied Gaussian/median filtering. Although this approach worked well for many of the teams, including CU-Lab (III) and ExB research that were ranked fourth and sixth in the image classification task, it may not take into account metastases characteristics (e.g. slides containing multiple high-score findings or slides containing larger metastases could have increased chance of containing metastases). In contrast, the systems HMS & MIT (I & II) used a random forest classifier employing a variety of geometrical and morphological features extracted from each probability map. Details of these features can be found in **eMethods**. The use of a learning-based algorithm to produce a confidence score from a whole-slide image probability map is likely the centerpiece of this algorithm that makes it the top-performing system for the first task.

Finally, one interesting property of the top-performing system HMS & MIT (II) in the metastasis identification task is that it uses the output of the discriminative classifier that produces a slide-based confidence score, to weigh the score of each finding in the second task. This top-down analysis reduces the number of false-positives, particularly in normal slides.

## eReferences

1. Krizhevsky A, Sutskever I, Hinton GE. Imagenet classification with deep convolutional neural networks. Paper presented at: Advances in neural information processing systems2012.
2. Farabet C, Couprie C, Najman L, LeCun Y. Learning hierarchical features for scene labeling. *IEEE Trans. Pattern Anal. Mach. Intell.* 2013;35(8):1915-1929.
3. Szegedy C, Wei L, Yangqing J, et al. Going deeper with convolutions. Paper presented at: IEEE Conference on Computer Vision and Pattern Recognition; 7-12 June 2015, 2015.
4. He K, Zhang X, Ren S, Sun J. Deep residual learning for image recognition. Paper presented at: IEEE Conference on Computer Vision and Pattern Recognition; 27-30 June 2016, 2016.
5. Russakovsky O, Deng J, Su H, et al. ImageNet large scale visual recognition challenge. *Int. J. Comput. Vis.* 2015;115(3):211-252.
6. Simonyan K, Zisserman A. Very deep convolutional networks for large-scale image recognition. *arXiv preprint arXiv:1409.1556.* 2014.
7. Ronneberger O, Fischer P, Brox T. U-net: Convolutional networks for biomedical image segmentation. Paper presented at: International Conference on Medical Image Computing and Computer-Assisted Intervention2015.
8. Kendall A, Badrinarayanan V, Cipolla R. Bayesian segnet: Model uncertainty in deep convolutional encoder-decoder architectures for scene understanding. *arXiv preprint arXiv:1511.02680.* 2015.
9. Cortes C, Vapnik V. Support-vector networks. *Mach. Learn.* 1995;20(3):273-297.
10. Viola P, Jones M. Fast and robust classification using asymmetric adaboost and a detector cascade. Paper presented at: Advances in Neural Information Processing Systems2002.
11. Zheng S, Jayasumana S, Romera-Paredes B, et al. Conditional random fields as recurrent neural networks. Paper presented at: Proceedings of the IEEE International Conference on Computer Vision2015.
12. Breiman L. Random forests. *Mach. Learn.* 2001;45(1):5-32.
13. Albarqouni S, Baur C, Achilles F, Belagiannis V, Demirci S, Navab N. AggNet: Deep learning from crowds for mitosis detection in breast cancer histology images. *IEEE Trans. Med. Imaging.* 2016;35(5):1313-1321.
14. Cserni G, Bianchi S, Boecker W, et al. Improving the reproducibility of diagnosing micrometastases and isolated tumor cells. *Cancer.* 2005;103(2):358-367.
15. Ioffe S, Szegedy C. Batch normalization: Accelerating deep network training by reducing internal covariate shift. *arXiv preprint arXiv:1502.03167.* 2015.
16. Srivastava N, Hinton GE, Krizhevsky A, Sutskever I, Salakhutdinov R. Dropout: A simple way to prevent neural networks from overfitting. *J. Mach. Learn. Res.* 2014;15(1):1929-1958.
17. Nair V, Hinton GE. Rectified linear units improve restricted boltzmann machines. Paper presented at: Proceedings of the 27th International Conference on Machine Learning2010.
18. Kingma D, Ba J. Adam: A method for stochastic optimization. *arXiv preprint arXiv:1412.6980.* 2014.
19. Glorot X, Bengio Y. Understanding the difficulty of training deep feedforward neural networks. Paper presented at: aistats2010.
20. Maas AL, Hannun AY, Ng AY. Rectifier nonlinearities improve neural network acoustic models. Paper presented at: ICML Workshop on Deep Learning for Audio, Speech and Language Processing2013.
21. Ehteshami Bejnordi B, Litjens G, Timofeeva N, et al. Stain specific standardization of whole-slide histopathological images. *IEEE Trans. Med. Imaging.* 2016;35(2):404-415.

22. Joblove GH, Greenberg D. Color spaces for computer graphics. *SIGGRAPH Comput. Graph.* 1978;12(3):20-25.
23. Otsu N. A threshold selection method from gray-level histograms. *Automatica.* 1975;11(285-296):23-27.
24. He K, Zhang X, Ren S, Sun J. Delving deep into rectifiers: Surpassing human-level performance on imagenet classification. Paper presented at: Proceedings of the IEEE International Conference on Computer Vision2015.
25. Long J, Shelhamer E, Darrell T. Fully convolutional networks for semantic segmentation. Paper presented at: Proceedings of the IEEE Conference on Computer Vision and Pattern Recognition2015.
26. Everingham M, Eslami SMA, Van Gool L, Williams CKI, Winn J, Zisserman A. The pascal visual object classes challenge: A retrospective. *Int. J. Comput. Vis.* 2015;111(1):98-136.
27. Rother C, Kolmogorov V, Blake A. Grabcut: Interactive foreground extraction using iterated graph cuts. Paper presented at: ACM transactions on graphics (TOG)2004.
28. Meyer F. Topographic distance and watershed lines. *Signal processing.* 1994;38(1):113-125.
29. Reinhard E, Adhikhmin M, Gooch B, Shirley P. Color transfer between images. *IEEE Computer Graphics and Applications.* 2001;21(5):34-41.
30. Zeiler MD. ADADELTA: an adaptive learning rate method. *arXiv preprint arXiv:1212.5701.* 2012.
31. Duchi J, Hazan E, Singer Y. Adaptive subgradient methods for online learning and stochastic optimization. *J. Mach. Learn. Res.* 2011;12(Jul):2121-2159.
32. Rumelhart DE, Hinton GE, Williams RJ. Learning representations by back-propagating errors. *Cognitive modeling.*5(3):1.
33. Haralick RM, Shanmugam K, Dinstein I. Textural features for image classification. *IEEE Trans. Syst. Man Cybern.* 1973;SMC-3(6):610-621.
34. Ahmady Phoulady H, Goldgof DB, Hall LO, Mouton PR. Nucleus segmentation in histology images with hierarchical multilevel thresholding. Paper presented at: Proceedings of SPIE Medical Imaging2016.
35. Ojala T, Pietikainen M, Maenpaa T. Multiresolution gray-scale and rotation invariant texture classification with local binary patterns. *IEEE Trans. Pattern Anal. Mach. Intell.* 2002;24(7):971-987.
36. Lowe DG. Distinctive image features from scale-invariant keypoints. *Int. J. Comput. Vis.* 2004;60(2):91-110.
37. Dalal N, Triggs B. Histograms of oriented gradients for human detection. Paper presented at: IEEE Computer Society Conference on Computer Vision and Pattern Recognition2005.
38. Matas J, Chum O, Urban M, Pajdla T. Robust wide-baseline stereo from maximally stable extremal regions. *Image and vision computing.* 2004;22(10):761-767.
39. Ruifrok AC, Johnston DA. Quantification of histochemical staining by color deconvolution. *Anal. Quant. Cytol. Histol.* 2001;23(4):291-299.
40. Ester M, Kriegel H-P, Sander J, Xu X. A density-based algorithm for discovering clusters in large spatial databases with noise. Paper presented at: Proceedings of the Second International Conference on Knowledge Discovery and Data Mining1996.
41. Chen H, Dou Q, Wang X, Qin J, Heng PA. Mitosis detection in breast cancer histology images via deep cascaded networks. Paper presented at: Proceedings of the thirtieth AAAI Conference on Artificial Intelligence2016.
42. Laws KI. Rapid Texture Identification. Paper presented at: Proceedings of SPIE Medical Imaging1980.

43. Chen L, Papandreou G, Kokkinos I, Murphy K, Yuille AL. Deeplab: Semantic image segmentation with deep convolutional nets, atrous convolution, and fully connected crfs. *arXiv preprint arXiv:1606.00915*. 2016.
44. Lin T, Maire M, Belongie S, et al. Microsoft coco: Common objects in context. Paper presented at: European Conference on Computer Vision2014.
45. Van der Walt S, Schönberger JL, Nunez-Iglesias J, et al. scikit-image: image processing in Python. *PeerJ*. 2014;2:e453.
46. Bengio Y. Deep learning of representations for unsupervised and transfer learning. Paper presented at: Proceedings of the 2011 International Conference on Unsupervised and Transfer Learning Workshop2011.
47. Yosinski J, Clune J, Bengio Y, Lipson H. How transferable are features in deep neural networks? Paper presented at: Advances in neural information processing systems2014.
48. Sharif Razavian A, Azizpour H, Sullivan J, Carlsson S. CNN features off-the-shelf: An astounding baseline for recognition. Paper presented at: Proceedings of the IEEE Conference on Computer Vision and Pattern Recognition Workshops2014.