

# Droplet Microfluidic Flow Cytometer for Sorting on Transient Cellular Responses of Genetically-Encoded Sensors

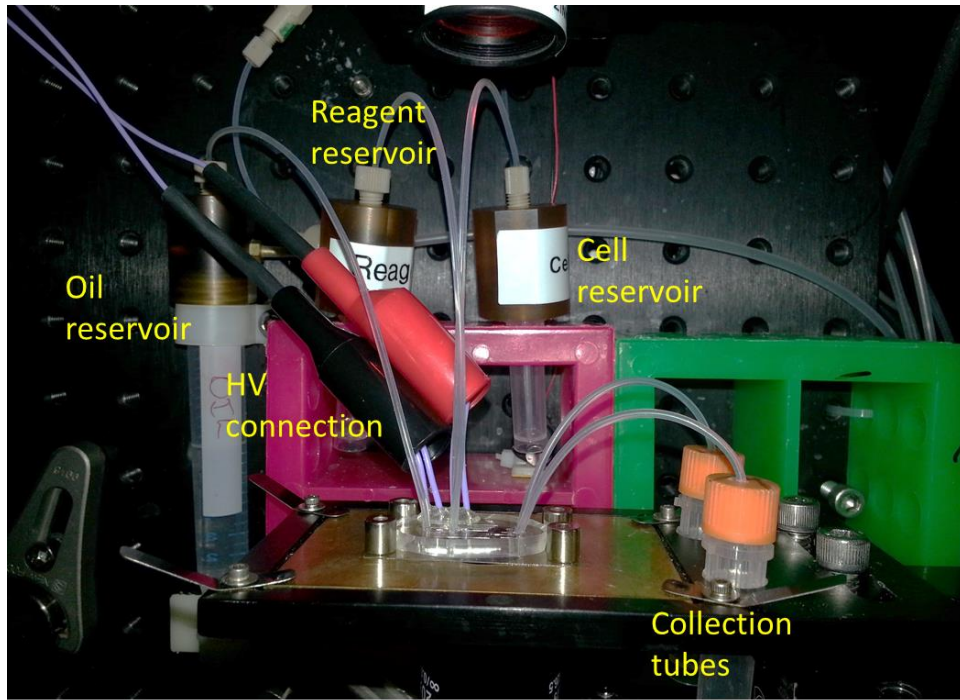
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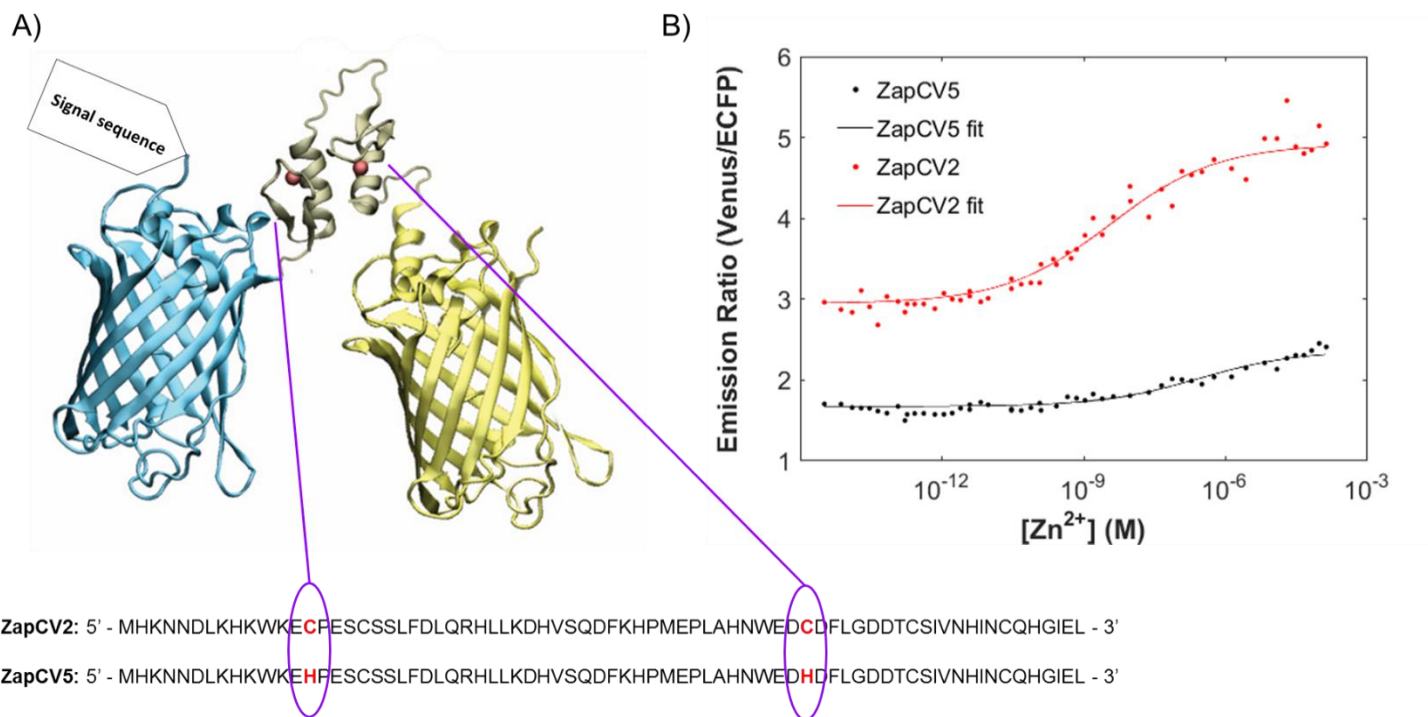
## Supporting Information

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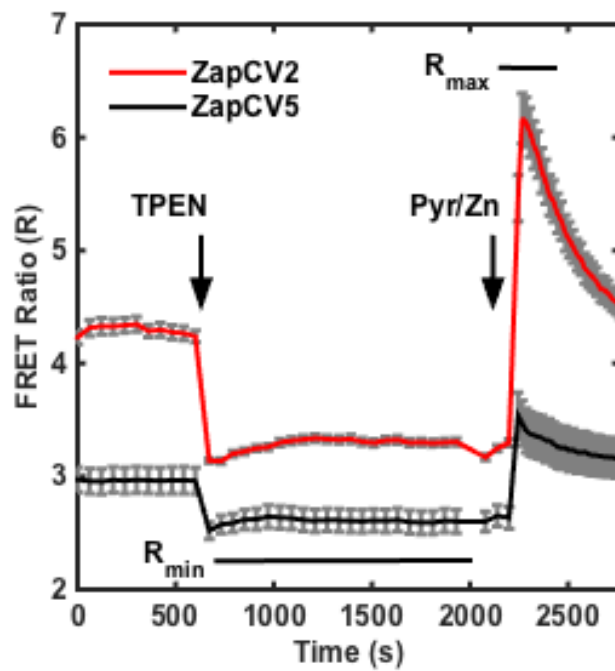
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**Figure S-1:** Picture showing implementation of microfluidic device into the apparatus.



**Figure S-2:** A) A cartoon of a representative FRET-based  $Zn^{2+}$  sensor used in this work. The structure from N-terminus to C-terminus consists of a localization signal sequence, ECFP (blue), Zap1  $Zn^{2+}$  binding domain (green), Venus (yellow).  $Zn^{2+}$  ions are shown as red spheres. Sequences of the  $Zn^{2+}$  binding domains of ZapCV2 and ZapCV5 are shown below with the differing residues bolded and highlighted in red. B) In vitro titration curves showing the binding affinities and Hill coefficients for ZapCV2 and ZapCV5. Experimental details shown below.



**Figure S-3.** Calibration plot with raw FRET ratios for data in Figure 1.

## Sensor construction and characterization

### *Design of ZapCV2 and ZapCV5 Zn<sup>2+</sup> sensors*

ZapCV sensors are modified based on previously characterized ZapCY2 sensors.<sup>1</sup> The FRET acceptor (citrine fluorescent protein, YFP) in ZapCY2 was replaced by circularly permuted (at amino acid 173 position) Venus fluorescent protein, which generated ZapCV2 (YFP changed to Venus). The lower affinity ZapCV5 was created by quick change mutagenesis of the Zn<sup>2+</sup> binding domain (C586H and C623H). The cytosolic NES-ZapCV sensors include an N-terminal nuclear export signal (MLQLPPLERLTL). These sensors were cloned in the pcDNA3.1 and PiggyBac Transposon vector backbone for mammalian cell expression and in the pBAD vector backbone for bacterial expression.

### *In vitro characterization of ZapCV2 and ZapCV5*

For *in vitro* studies, the sensors were cloned into pBAD and expressed in Top-10 Escherichia coli with the addition of 0.2% arabinose. Sensor proteins were purified using Ni<sup>2+</sup> ion affinity chromatography and the His tag was removed with TEV protease in 20mM Tris, 100 mM NaCl, pH8 buffer at room temperature overnight (sensor to TEV protease ratio was 10:1). The sensor was then concentrated with an Amicon centrifugal filter to 50-100  $\mu$ M as determined by the absorbance at 516 nm using  $\epsilon = 77000 \text{ M}^{-1} \text{ cm}^{-1}$ .

Purified sensor was titrated with Zn<sup>2+</sup> to determine the disassociation constants of Zn<sup>2+</sup> from the sensors. Zn<sup>2+</sup> titrations were performed in HEPES buffer (150 mM Hepes, 100 mM NaCl, and 10% glycerol, pH 7.4) with 1  $\mu$ M sensor protein, treated for 5 minutes immediately prior to titration with 0.5 mM TCEP, and different concentration of free Zn<sup>2+</sup> as described previously.<sup>1</sup> The *in vitro* fluorescence measurements used for Zn<sup>2+</sup> titrations were made on a Tecan Safire-II fluorescence plate reader using the following parameters: excitation: 420 nm, emission: 435-649 nm, and the emission bandwidth was 10 nm. The apparent dissociation constant was determined using the fitting method described by Pomorski et al.<sup>2</sup> The intensities of the fluorescence emission at 481 nm were used as  $\lambda_1$  and at 529 nm for  $\lambda_2$ . The ratios of these intensities were

plotted against the zinc concentration and fitted using one of the following equations depending on the ratio used ( $\lambda_1/\lambda_2$  vs.  $\lambda_2/\lambda_1$ ).

$$R_{\frac{2}{1}} = \frac{(I_{2b} \cdot Z^n) + (I_{2u} \cdot K_d^n)}{(I_{1b} \cdot Z^n) + (I_{1u} \cdot K_d^n)}$$

$$R_{\frac{1}{2}} = \frac{(I_{1b} \cdot Z^n) + (I_{1u} \cdot K_d^n)}{(I_{2b} \cdot Z^n) + (I_{2u} \cdot K_d^n)}$$

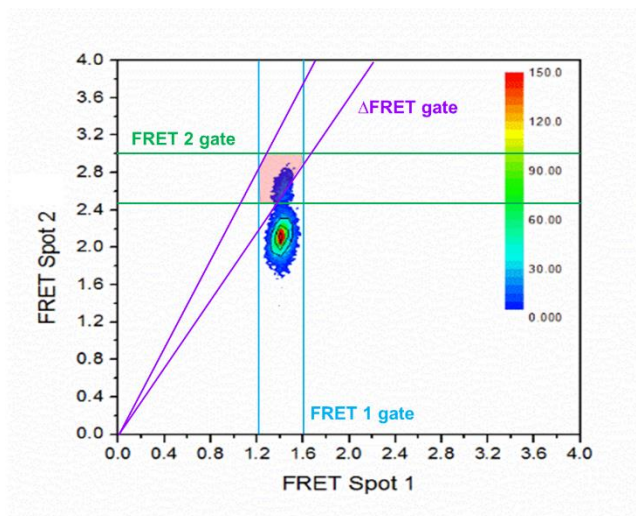
Where the  $I_{2b}$ ,  $I_{2u}$ ,  $I_{1b}$ ,  $I_{1u}$  are fixed using the average intensity at  $\lambda_1$  or  $\lambda_2$  at the five most or least concentrated  $Zn^{2+}$  conditions,  $Z$  is equal to the  $-\log$  of the free zinc concentration,  $K_d$  is the disassociation constant, and  $n$  is the hill coefficient. The reported  $K_d$ 's are the average of 2 or more titrations of the sensor.

### ***Cellular imaging for in vivo calibration***

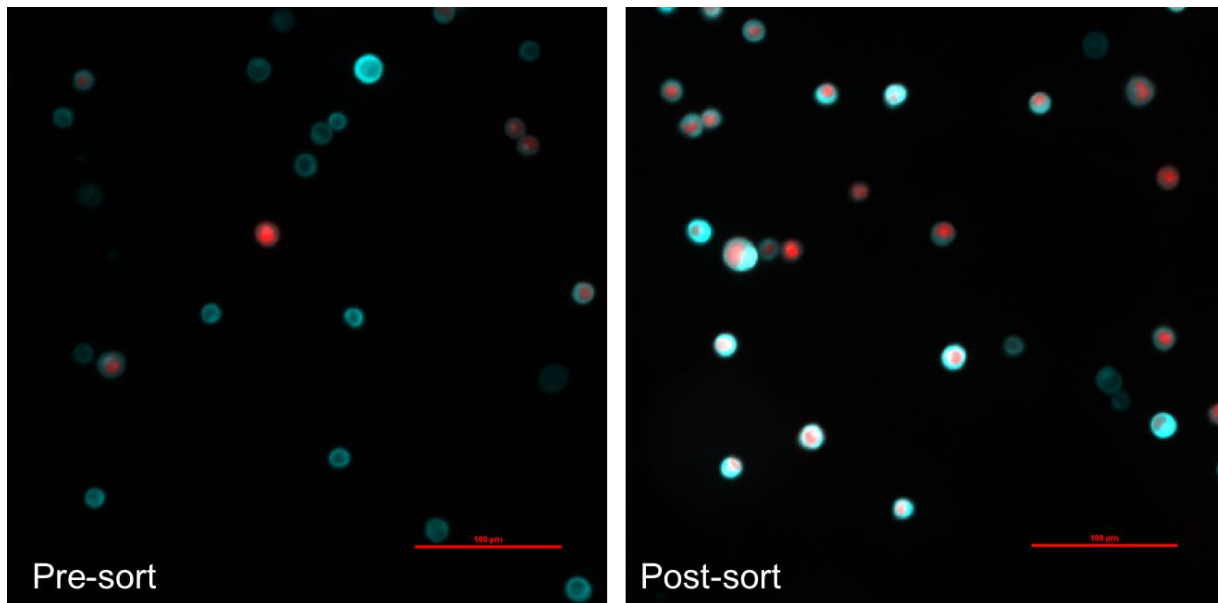
Imaging experiments were performed on a Nikon Ti-E wide-field fluorescence microscope equipped with Nikon elements software, Ti-E perfect focus system, an iXon3 EMCCD camera (Andor), mercury arc lamp, and YFP FRET (434/16 excitation, 458 dichroic, 535/20 emission), CFP (434/16 excitation, 458 dichroic, 470/24 emission), and YFP (495/10 excitation, 515 dichroic, 535/20 emission) filter sets. External excitation and emission filter wheels were controlled by a Lambda 10-3 filter changer (Sutter Instruments), while dichroic mirrors were placed on cubes in the dichroic turret. Images were collected using a 60X oil objective (NA 1.40), 100 ms exposure time, EM gain 1 MHz at 16-bit readout mode with an EM gain multiplier of 100, and a neutral density filter with 12.5% light transmission.

For the calibration experiments shown in Figure 1, sensor constructs were transfected into HeLa cells with TransIT-LT1 (Mirus Bio). Cells were imaged 48 hours post-transfection. Cells were maintained at 37°C and 5% CO<sub>2</sub> in a LiveCell™ environment chamber (Pathology Devices) during the experiment. Cells were imaged in phosphate-free HEPES-buffered HBSS, pH = 7.4 to prevent zinc precipitation. Resting images were collected for 5 minutes, followed by treatment with 150 μM TPEN to collect  $R_{min}$  data until a stable signal was achieved. Cells were then washed with phosphate, calcium, and magnesium-free HEPES-buffered HBSS, pH = 7.4,

then cells were treated with 1  $\mu\text{M}$  pyrithione and 50  $\mu\text{M}$   $\text{ZnCl}_2$  to obtain  $R_{\text{max}}$  data. Resting and  $R_{\text{min}}$  images were collected every 1 minute, and  $R_{\text{max}}$  images were collected every 20 seconds. All data were analyzed in MATLAB (Mathworks). Images were background corrected by drawing a region of interest (ROI) in a blank area of image and subtracting the average fluorescence intensity of the background ROI from the average intensity of each cell. FRET ratios for each cell were calculated by dividing the background-corrected YFP FRET intensity by the background-corrected CFP intensity ( $(I_{\text{cellular FRET}} - I_{\text{background FRET}})/(I_{\text{cellular CFP}} - I_{\text{background CFP}})$ ). This background subtraction and FRET response measurement is done in image post-processing, though it should, in theory, be possible to speed up the process of dynamic range determination by incorporating a real-time algorithm in the acquisition software.

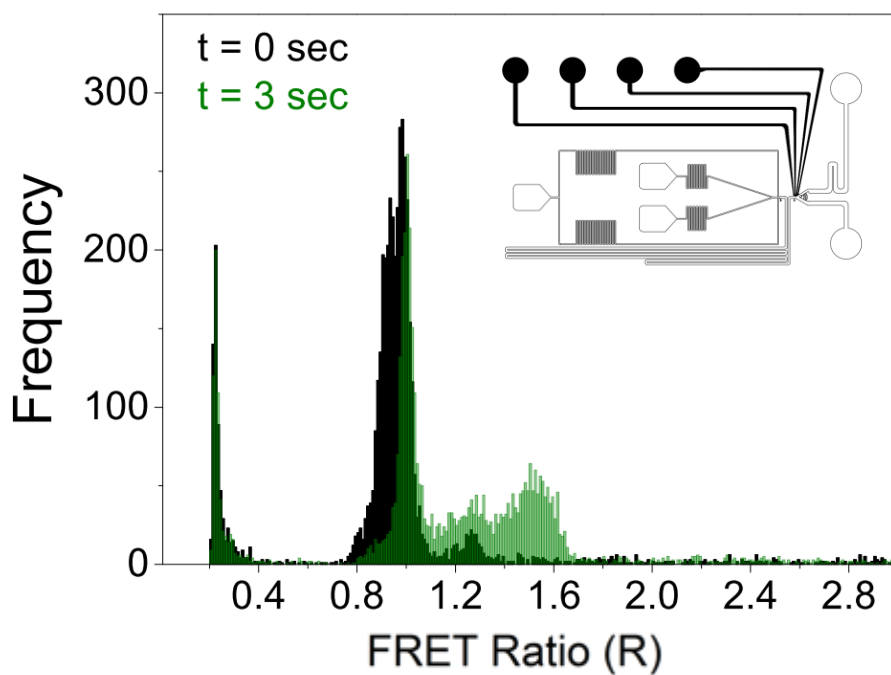
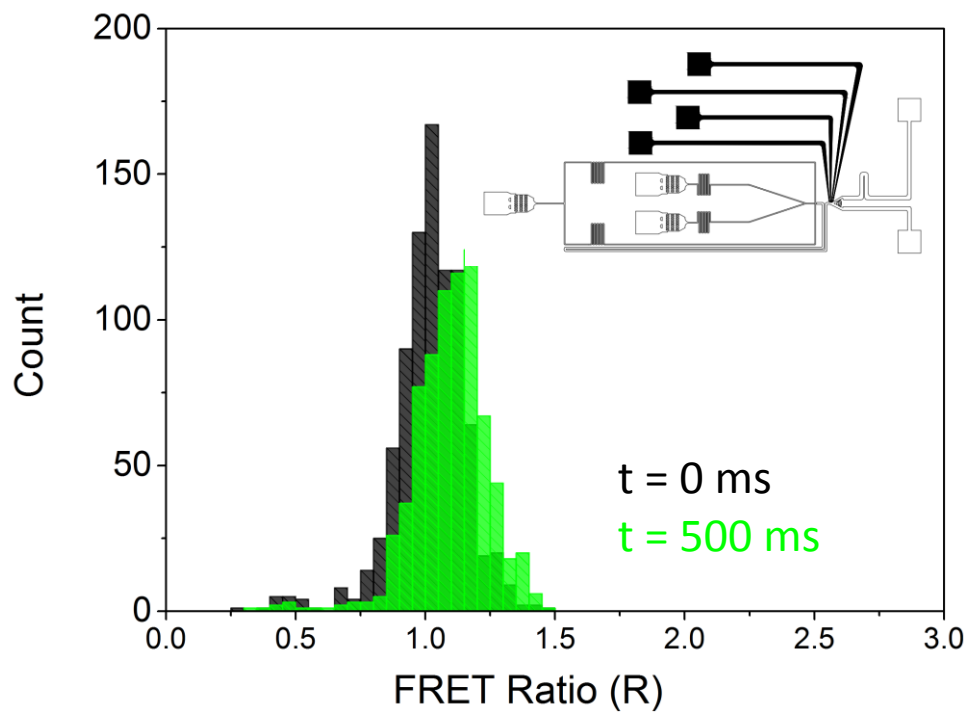


**Figure S-4:** Contour plot for the data shown in Figure 5.

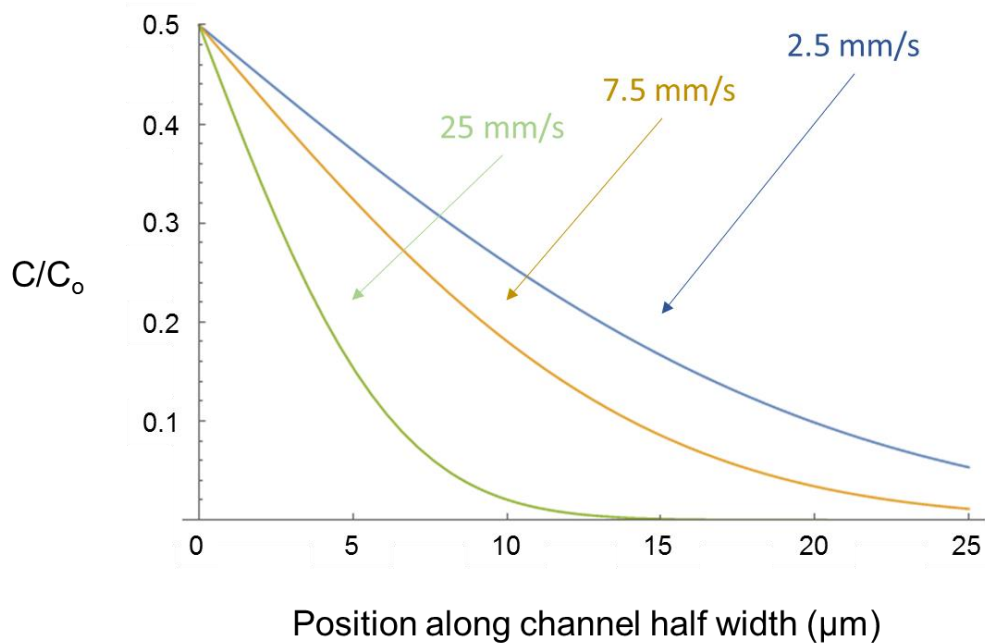


**Figure S-5:** Representative, pseudo-colored images using CFP (434/16 excitation, 458 dichroic, 470/24 emission) and mCherry channels (560/20 excitation, 585 LP, 610/50 emission) showing pre- and post-sort collections of cells used to collect data in Figure 5. Images were collected using a 20X air objective (NA 0.8), 100 ms exposure time for CFP and 200 ms for mCherry, EM gain 1 MHz at 16-bit readout mode with an EM gain multiplier of 100, and a neutral density filter with 12.5% light transmission. Cell expressing ZapCV2 are coexpressed with an NLS-mCherry. Scale bar = 100  $\mu$ M.





**Figure S-6:** Top: FRET histogram of a screening run of cells stably expressing NES-ZapCV2 with a time delay of 500 ms and delay length of 40 mm. Bottom: FRET histogram of a screening run of cells expressing a virally-transduced stable line of ZapCY1, a sensor used in a previous study,<sup>3</sup> at a time delay of 3 seconds and a delay length of 115 mm.



**Figure S-7:** A slice of the calculated concentration profile at  $x = 300 \mu\text{m}$  (where  $x$  is the distance along the axis of flow) after the mixing junction. The  $y$ -axis shows the concentration  $C$ , normalized by the input concentration  $C_0$ . The  $x$ -axis is the position along the width of the channel, beginning in the middle. Equation used is  $\frac{C(x,y)}{C_0} = \frac{1}{2} \left( 1 - \text{erf} \left( \frac{y\sqrt{U}}{\sqrt{4D_{\text{eff}}x}} \right) \right)$ , where  $y$  is the distance perpendicular the axis of flow,  $U$  is the flow velocity, and  $D_{\text{eff}}$  is the effective diffusion constant (estimated at  $1\text{E-}9 \text{ cm}^2/\text{s}$  for the small ion/ionophore complex). Plotted at a series of flow velocities relevant to chip operation.

## References

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- (2) Pomorski, A.; Kochańczyk, T.; Miłoch, A.; Krężel, A. *Anal. Chem.* **2013**, *85*, 11479.
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