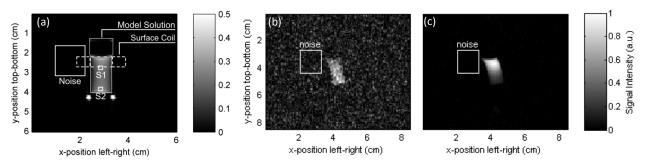
In vivo 13C-MRI using SAMBADENA S2 Fig

Improving SNR with a ¹³C Receive Surface Coil



S2 Fig: (a) Axial ¹H MRI of a ¹³C-enriched model solution (Model solution M1, 3.3 mM 1^{-13} C sodium acetate in 1.2 mL H₂O). The surface loop coil was mounted to M1 as is indicated by a dashed line; the shape of M1 is outlined by a thin solid line. Region of interest (ROI) of signal and noise regions that were used for SNR quantification of scans (b) and (c) are represented by thick solid lines (S1 and S2: 1.25 x 1.66 mm, corresponding to 3 x 3 px in the ¹³C image; Noise: 8.31 x 11.08 mm corresponding to 20 x 20 px in the ¹³C image; MRI: single-shot RARE sequence, 90/180°, RARE factor 36, partial Fourier factor 1.7778, 128 x 64 matrix, FOV (6 cm)², (0.47 x 0.94) mm² in-plane resolution, 6-cm-slice thickness, TR = 3 s, TE = 15 ms, acquisition time 3 s, bandwidth 10 kHz, centred in the isocentre).

Axial ¹³C MRI of M1 recorded using either a ¹H-¹³C transmit-receive volume resonator (b) or the ¹³C surface coil (c). Note that in both cases the volume resonator was used for excitation, as described in the main article. SNR was quantified by dividing the average signal of ROI S1 or S2 (see (a)) by the standard deviation of the noise in the indicated ROI. S1 was adjacent to the coil and S2 at a distance of ~1.3 cm along the symmetry axis of the loop. Using the surface coil, the SNR1 and SNR2 (measured at S1 and S2, respectively) increased from 5.3 to 88.3 and 6.0 to 18.3, respectively, corresponding to a sensitivity enhancement factor of 16.7 or 3.0. Note that the surface coil was mounted on M1 in both images, but used for acquisition only in (c). All images were normalized to the highest signal in the corresponding image (MRI: single-shot RARE sequence, 90/180°, RARE factor 38, partial Fourier factor 1.7778, 128 x 96 matrix, FOV (8.4 cm)2, (0.85 x 0.64) mm² in-plane resolution, 6-cm-slice thickness, TR = 0.487 s, TE = 79 ms, acquisition time 487 ms, bandwidth 10 kHz, centred in the isocentre).