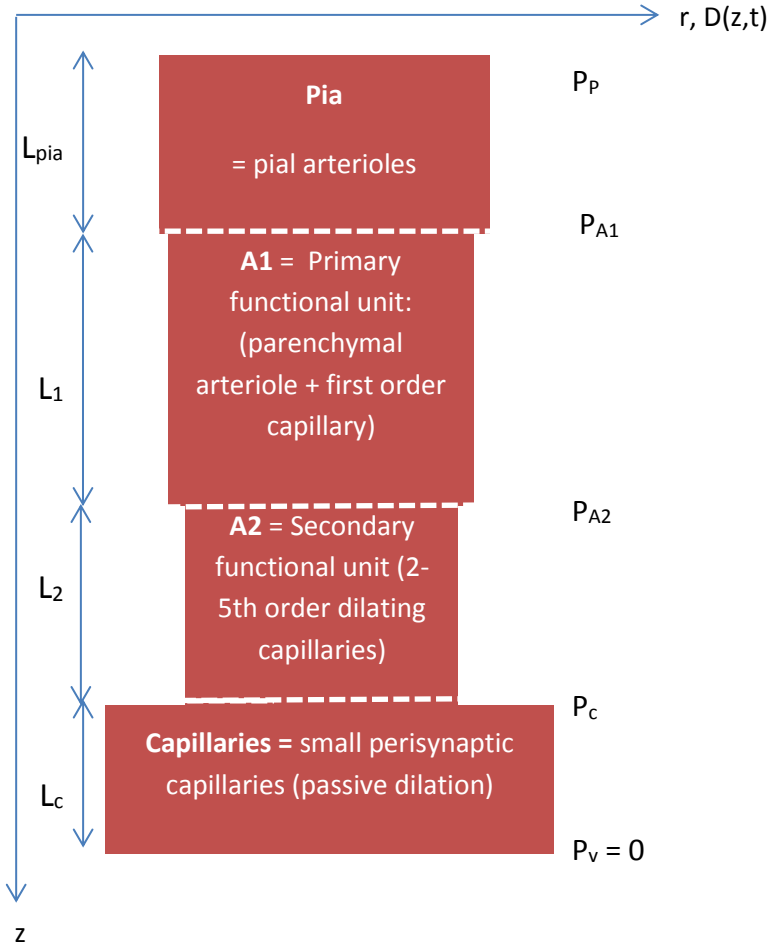


**Data File S1. Related to Star Methods.**

Modeling RBCs velocity and flow in response to diameter changes due to odor application

We used the following compartmental model :



**Order of magnitude of Reynolds Number :**

The Reynolds Number is :  $Re = \rho vL / \mu$

where:

- $\rho$  is the density of the fluid = 1.06 kg/m<sup>3</sup> for blood
- $v$  is the velocity of the fluid with respect to the object  $\sim 10^{-3}$  m/s
- $L$  is a characteristic linear dimension  $\sim 10^{-4}$  m
- $\mu$  is the dynamic viscosity of the fluid

$$\mu = \mu_0 \mu_R$$

$$\mu_0 \sim 6 \cdot 10^{-3} \text{ Pa.s}$$

$\mu_R$  depends on vessel diameter. We used the model from in vitro measurements (Pries et al., 1992) (the best in our case as diameter measurements already exclude glycocalyx) :

$$\mu_r(D) = 1 + (\mu_{r0.45}(D) - 1) \frac{(1-Hd)^{C(D)-1}}{(1-0.45)^{C(D)-1}}$$

With :  $\mu_{r0.45}(D) = 220e^{-1.3D} + 3.2 - 2.44e^{-0.06D^{0.645}}$

And  $C(D) = (0.8 + e^{-0.075D}) \left( \frac{1}{1+10^{-11}D^{12}} - 1 \right) + \frac{1}{1+10^{-11}D^{12}}$  This gives  $Re \sim 10^{-5}$ . Therefore the flow is laminar.

### **Navier Stokes Equations:**

We assume linear gradient of pressure for each compartment. Calling G the pressure gradient  $\frac{\partial P}{\partial z}$ .

We use cylindrical coordinates (r,  $\theta$ , z)

As laminar flow, component of v along r at the end of each segment neglected:  $\vec{v} = v_z(r, z, t)\vec{u}_z$ .

Navier Stokes equations become:

- $div(\vec{v}) = \frac{\partial v_z}{\partial z} = 0$   
 $\Rightarrow \vec{v} = v_z(r, t)\vec{u}_z$  for each segment

- by projecting along the z axis, for each segment:

$$\boxed{\rho \frac{\partial v_z}{\partial t} = -G + \frac{\mu}{r} \frac{\partial}{\partial r} \left( r \frac{\partial v_z}{\partial r} \right)} \quad \text{Eq. 1}$$

The solution of Eq. 1 is given by :

$$\boxed{v_z(r, t) = \frac{G}{4\mu} (R^2 - r^2) - \frac{2GR^2}{\mu} \sum_{n=1}^{\infty} \frac{1}{\lambda_n^3} \frac{J_0\left(\frac{\lambda_n r}{R}\right)}{J_1(\lambda_n)} e^{-\frac{\lambda_n^2 \mu t}{\rho R^2}}} \quad J_0(\lambda_n) = 0 \quad \text{Eq. 2}$$

### **Transient solution:**

The transient component  $\frac{2GR^2}{\mu} \sum_{n=1}^{\infty} \frac{1}{\lambda_n^3} \frac{J_0\left(\frac{\lambda_n r}{R}\right)}{J_1(\lambda_n)} e^{-\frac{\lambda_n^2 \mu t}{\rho R^2}}$  decreases with the following time constants:

$$\tau_n = \frac{\rho R^2}{\lambda_n^2 \mu}$$

$\lambda_n > 2$  and  $R < 20 \mu\text{m}$ . Hence  $\tau_n < \frac{\rho R^2}{4\mu} \sim 2 \cdot 10^{-6} \text{s}$

Therefore transients are negligible at our time scale.

### **Steady-state solution:**

The steady-state solution is:

$$v_z(r) = \frac{G}{4\mu} \left( \left( \frac{D}{2} \right)^2 - r^2 \right) \quad \text{Eq. 3}$$

With D being the diameter of the vessel

We use  $\vec{v} = v \vec{u}_z$  average velocity over section.

$$v = \frac{4}{\pi D^2} \iint v_z(s) ds \quad \text{with} \quad dS = 2\pi r dr$$

$$v = \frac{4}{\pi D^2} \int_0^{D/2} 2\pi r v_z(r) dr$$

$$v = \frac{2G}{\mu D^2} \int_0^{D/2} \left( r \left( \frac{D}{2} \right)^2 - r^3 \right) dr$$

Thus

$$v = \frac{GD^2}{32\pi\mu} \quad \text{Eq. 4}$$

and  $v = \frac{v_z(0)}{2}$

As  $Q = \frac{\pi D^2}{4} v$ :

$$Q = \frac{GD^4}{128\mu} \quad \text{Eq. 5}$$

Furthermore,  $G = \frac{\Delta P}{L}$ , therefore :

For the pia section:

$$Q_{pia}(t) = \pi D_{pia}^4(t) \frac{P_{pia} - P_{A1}(t)}{128\mu_{pia}L_{pia}} \quad \text{Eq. 6}$$

$$v_{pia}(t) = D_{pia}^2(t) \frac{P_{pia} - P_{A1}(t)}{32\mu_{pia}L_{pia}} \quad \text{Eq. 7}$$

For the A1 section:

$$Q_{A1}(t) = \pi D_{A1}^4(t) \frac{P_{A1}(t) - P_{A2}(t)}{128\mu_{A1}L_{A1}} \quad \text{Eq. 8}$$

$$v_{A1}(t) = D_{A1}^2(t) \frac{P_{A1}(t) - P_{A2}(t)}{32\mu_{A1}L_{A1}} \quad \text{Eq. 9}$$

For the A2 section:

$$Q_{A2}(z, t) = \pi D_{A2}^4(t) \frac{P_{A2}(t) - P_c(t)}{128\mu_{A2}L_{A2}} \quad \text{Eq.10}$$

$$v_{A2}(z, t) = D_{A2}^2(t) \frac{P_{A2}(t) - P_c(t)}{32\mu_{A2}L_{A2}} \quad \text{Eq. 11}$$

For the capillary section:

$$Q_c(z, t) = \pi D_c^4 \frac{P_c(t)}{128\mu_c L_c} \quad \text{Eq. 12}$$

$$v_c(z, t) = D_c^2 \frac{P_c(t)}{32\mu_c L_c} \quad \text{Eq. 13}$$

### Conservation of flow:

- **Between pia and A1 :**

$$Q_{pia}(t) = Q_{A1}(t)$$

$$\text{Thus } D_{pia}^4(t) \frac{P_{pia} - P_{A1}(t)}{\mu_{pia}L_{pia}} = D_{A1}^4(t) \frac{P_{A1}(t) - P_{A2}(t)}{\mu_{A1}L_{A1}}$$

$$\text{Reformulating : } \mu_{A1}L_{A1}D_{pia}^4(t)(P_{pia} - P_{A1}(t)) = \mu_{pia}L_{pia}D_{A1}^4(t)(P_{A1}(t) - P_{A2}(t))$$

Reformulating :

$$\boxed{\mu_{A1}L_{A1}D_{pia}^4(t)P_{pia} - (\mu_{A1}L_{A1}D_{pia}^4(t) + \mu_{pia}L_{pia}D_{A1}^4(t))P_{A1}(t) + \mu_{pia}L_{pia}D_{A1}^4(t)P_{A2}(t) = 0} \quad \text{Eq. 14}$$

- **Between A1 and A2 :**

$$Q_{A1}(t) = Q_{A2}(t)$$

$$\text{Thus } D_{A1}^4(t) \frac{P_{A1}(t) - P_{A2}(t)}{\mu_{A1}L_{A1}} = D_{A2}^4(t) \frac{P_{A2}(t) - P_c(t)}{\mu_{A2}L_{A2}}$$

$$\text{Reformulating : } \mu_{A2}L_{A2}D_{A1}^4(t)(P_{A1}(t) - P_{A2}(t)) = \mu_{A1}L_{A1}D_{A2}^4(t)(P_{A2}(t) - P_c(t))$$

Reformulating :

$$\boxed{\mu_{A2}L_{A2}D_{A1}^4(t)P_{A1}(t) - (\mu_{A2}L_{A2}D_{A1}^4(t) + \mu_{A1}L_{A1}D_{A2}^4(t))P_{A2}(t) + \mu_{A1}L_{A1}D_{A2}^4(t)P_c(t) = 0} \quad \text{Eq. 15}$$

- **Between A2 and C :**

$$Q_{A2}(t) = Q_c(t)$$

$$\text{Thus } D_{A2}^4(t) \frac{P_{A2}(t) - P_c(t)}{\mu_{A2}L_{A2}} = D_c^4 \frac{P_c(t)}{\mu_c L_c}$$

$$\text{Reformulating : } \mu_c L_c D_{A2}^4(t)(P_{A2}(t) - P_c(t)) = \mu_{A2}L_{A2}D_c^4 P_c(t)$$

Reformulating :

$$\boxed{\mu_c L_c D_{A2}^4(t) P_{A2}(t) - (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4) P_c(t) = 0}$$

Eq. 16

**Expression of  $P_1(t)$ ,  $P_2(t)$  and  $P_c(t)$  from Eq.14, Eq.15 and Eq.16 :**

$\mu_{A2} L_{A2} D_{A1}^4(t)$  Eq. 14 +  $(\mu_{A1} L_{A1} D_{pia}^4 + \mu_{pia} L_{pia} D_{A1}^4(t))$  Eq. 15 gives

$$\begin{aligned} & (\mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} D_{A1}^4(t) P_{pia} + (\mu_{pia} L_{pia} \mu_{A2} L_{A2} D_{A1}^8(t) - (\mu_{A1} L_{A1} D_{pia}^4(t) \\ & + \mu_{pia} L_{pia} D_{A1}^4(t)) (\mu_{A2} L_{A2} D_{A1}^4(t) + \mu_{A1} L_{A1} D_{A2}^4(t))) P_{A2}(t) + (\mu_{A1} L_{A1} D_{pia}^4(t) \\ & + \mu_{pia} L_{pia} D_{A1}^4(t)) \mu_{A1} L_{A1} D_{A2}^4(t) P_c(t) = 0 \end{aligned}$$

Reformulating :

$$\begin{aligned} & \mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} D_{A1}^4(t) P_0 \\ & - (\mu_{A1}^2 L_{A1}^2 D_{A2}^4(t) D_{pia}^4(t) + (\mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} \\ & + \mu_{A1} L_{A1} D_{A2}^4(t) \mu_{pia} L_{pia}) D_{A1}^4(t) P_{A2}(t) + (\mu_{A1} L_{A1} D_{pia}^4(t) \\ & + \mu_{pia} L_{pia} D_{A1}^4(t)) \mu_{A1} L_{A1} D_{A2}^4(t) P_c(t) = 0 \end{aligned}$$

Eq. 17

Eq. 17 +  $(\mu_{A1} L_{A1} D_{pia}^4(t) + \mu_{pia} L_{pia} D_{A1}^4(t)) \mu_{A1} L_{A1} D_{A2}^4(t)$  Eq. 16 gives

$$\begin{aligned} & (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4) \mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} D_{A1}^4(t) P_0 + ((\mu_{A1} L_{A1} D_{pia}^4(t) + \\ & \mu_{pia} L_{pia} D_{A1}^4(t)) \mu_{A1} L_{A1} \mu_c L_c D_{A2}^8(t) - (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4) (\mu_{A1}^2 L_{A1}^2 D_{A2}^4(t) D_{pia}^4(t) + \\ & (\mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} + \mu_{A1} L_{A1} D_{A2}^4(t) \mu_{pia} L_{pia}) D_{A1}^4(t)) P_{A2}(t) = 0 \end{aligned}$$

Reformulating :

$$\begin{aligned} & (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4) \mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} D_{A1}^4(t) P_0 - (\mu_{A2} L_{A2} D_c^4 \mu_{A1}^2 L_{A1}^2 D_{A2}^4(t) D_{pia}^4(t) + \\ & (\mu_c L_c D_{A2}^4(t) \mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} + \mu_{A2} L_{A2} D_c^4 (\mu_{A1} L_{A1} D_{pia}^4(t) \mu_{A2} L_{A2} + \\ & \mu_{A1} L_{A1} D_{A2}^4(t) \mu_{pia} L_{pia}) D_{A1}^4(t)) P_{A2}(t) = 0 \end{aligned}$$

Reformulating :

$$\begin{aligned} & D_{pia}^4 (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4) D_{A1}^4(t) P_0 - (\mu_{A1} L_{A1} D_{A2}^4(t) D_{pia}^4 D_c^4 + (\mu_c L_c D_{A2}^4 D_{pia}^4(t) + \\ & D_c^4 (D_{pia}^4(t) \mu_{A2} L_{A2} + D_{A2}^4(t) \mu_{pia} L_{pia}) D_{A1}^4(t)) P_{A2}(t) = 0 \end{aligned}$$

setting

$$\beta(t) = D_{pia}^4(t) (\mu_c L_c D_{A2}^4(t) + \mu_{A2} L_{A2} D_c^4)$$

$$\gamma(t) = \mu_c L_c D_{A2}^4(t) D_{pia}^4(t) + D_c^4 (\mu_{A2} L_{A2} D_{pia}^4(t) + \mu_{pia} L_{pia} D_{A2}^4(t))$$

$$\delta(t) = \mu_{A1} L_{A1} D_c^4 D_{A2}^4(t) D_{pia}^4(t)$$

$$\text{Then } \beta D_{A1}^4(t) P_{pia} - (\delta + \gamma D_{A1}^4(t)) P_{A2}(t) = 0$$

Thus

$$P_{A2}(t) = \frac{\beta(t)D_{A1}^4(t) P_{pia}}{\delta(t)+\gamma(t)D_{A1}^4(t)} \quad \text{Eq. 18}$$

From Eq. 16 :

$$P_c(t) = \frac{\mu_{cL_c}D_{A2}^4(t)P_{A2}(t)}{(\mu_{cL_c}D_{A2}^4(t)+\mu_{A2}L_{A2}D_c^4)}$$

Setting  $\varepsilon(t) = \frac{\mu_{cL_c}D_{A2}^4(t)}{(\mu_{cL_c}D_{A2}^4(t)+\mu_{A2}L_{A2}D_c^4)}$

Then  $P_c(t) = \varepsilon(t)P_{A2}(t)$

Thus

$$P_c(t) = \frac{\beta(t)\varepsilon(t)D_{A1}^4(t)P_{pia}}{\delta(t)+\gamma(t)D_{A1}^4(t)} \quad \text{Eq. 19}$$

$$\mu_{A2}L_{A2}D_{A1}^4(t)P_{A1}(t) - (\mu_{A2}L_{A2}D_{A1}^4(t) + \mu_{A1}L_{A1}D_{A2}^4(t)P_{A2}(t) + \mu_{A1}L_{A1}D_{A2}^4(t)P_c(t) = 0$$

From Eq. 15 :

$$P_1(t) = \frac{(\mu_{A2}L_{A2}D_{A1}^4(t)+\mu_{A1}L_{A1}D_{A2}^4(t))P_{A2}(t)-\mu_{A1}L_{A1}D_{A2}^4(t)P_c(t)}{\mu_{A2}L_{A2}D_{A1}^4(t)}$$

Reformulating :

$$P_{A1}(t) = (1 + \frac{\mu_{A1}L_{A1}D_{A2}^4(t)}{\mu_{A2}L_{A2}D_{A1}^4(t)}(1 - \varepsilon(t)))P_{A2}(t)$$

Setting

$$\theta(t) = \frac{\mu_{A1}L_{A1}D_{A2}^4(t)}{\mu_{A2}L_{A2}D_{A1}^4(t)}$$

Then  $P_{A1}(t) = (1 + \theta(t)(1 - \varepsilon(t)))P_{A2}(t)$

Thus

$$P_{A1}(t) = \frac{\beta(t)D_{A1}^4(t)(1+\theta(t)(1-\varepsilon(t))) P_0}{\delta(t)+\gamma(t)D_{A1}^4(t)} \quad \text{Eq. 20}$$

**Equivalent cylinders for each compartment:**

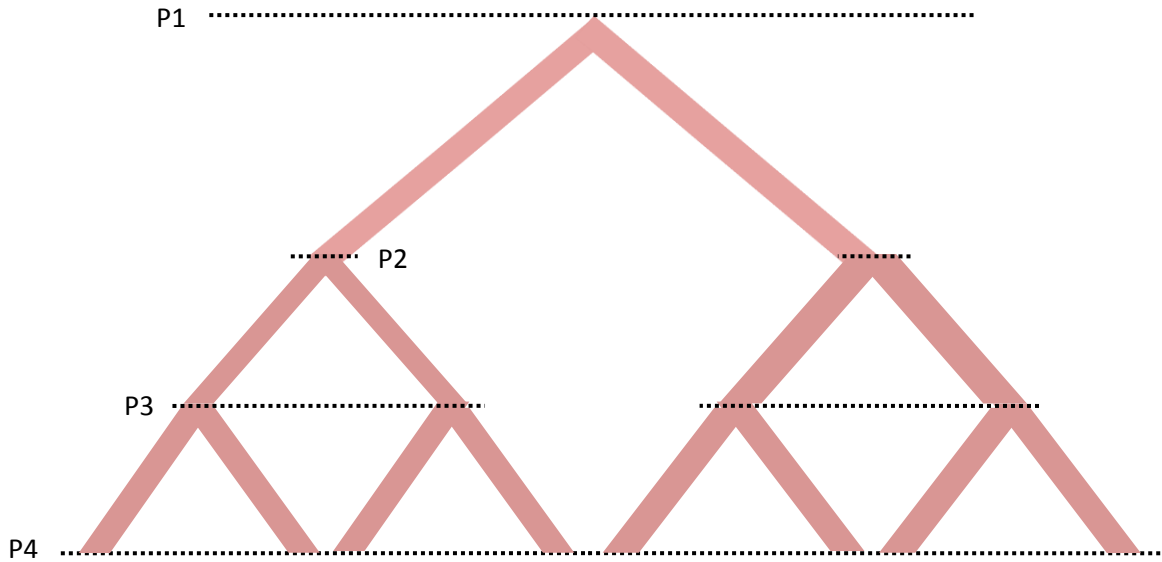
To model a vascular network as a single cylinder we need to estimate its parameters:

Let's assume :

- N primary branches at entrance of the same length L:  
 $Q = N Q_i$   
 where  $Q_i$  is the flow through a individual primary branch. Hence

$$Q(t) = \pi N D_i^4(t) \frac{P_{entrance}(t) - P_{exit}(t)}{128\mu L} \quad \text{Eq. 21}$$

- Each of the primary branches divides M-1 times and each sub-branch of the same length  $L_i$  and diameter  $D_i$



$$L_j = L/M$$

$$\text{At order } j \text{ between } 1 \text{ and } M : Q_{j+1}(t) = Q_j(t) / 2$$

where  $Q_j$  is the flow through an individual arteria at order  $j$

$$\text{Hence } Q_j(t) = Q_1(t) / 2^{j-1}$$

$$Q_j(t) = \pi D_i^4(t) \frac{P_j(t) - P_{j+1}(t)}{128\mu L_j}$$

$$\Rightarrow Q_j(t) = \pi M D_i^4(t) \frac{P_j(t) - P_{j+1}(t)}{128\mu L}$$

$$\Rightarrow \frac{128\mu L Q_1(t)}{\pi M D_i^4(t)} = 2^{j-1} (P_j(t) - P_{j+1}(t))$$

$$\Rightarrow P_{j+1}(t) = P_j(t) - \frac{128\mu L Q_1(t)}{2^{j-1} \pi M D_i^4(t)}$$

$$\Rightarrow P_{j+1}(t) = P_1(t) - \frac{128\mu L Q_1(t)}{\pi M D_i^4(t)} \sum_{k=1}^j \frac{1}{2^{k-1}}$$

$$P_{j+1}(t) = P_1(t) - \frac{256\mu L Q_1(t)}{\pi M D_i^4(t)} \left(1 - \left(\frac{1}{2}\right)^j\right) \quad \text{Eq. 22}$$

The flow through the vascular network i is :  $Q(t) = Q_1(t)$

$$\text{From Eq.22 : } P_M(t) = P_1(t) - \frac{256\mu L Q_1(t)}{\pi M D_i^4(t)} \left(1 - \left(\frac{1}{2}\right)^{M-1}\right)$$

Therefore

$$Q(t) = \frac{\pi M 2^{M-2} D_i^4(t)}{128\mu L (2^{M-1}-1)} (P_1(t) - P_M(t)) \quad \text{Eq. 23}$$

Combination of both levels give:

$$Q(t) = \frac{\pi N M 2^{M-2} D_i^4(t)}{128\mu L (2^{M-1}-1)} (P_1(t) - P_M(t)) \quad \text{Eq. 24}$$

To simplify we define:  $D_{NM}(t) = \left(\frac{NM 2^{M-2}}{2^{M-1}-1}\right)^{1/4} D_i(t)$

Then

$$Q(t) = \frac{\pi D_{NM}^4(t)}{128\mu L} (P_1(t) - P_M(t)) \quad \text{Eq. 25}$$

At order j between 1 and M :

$$v_j(t) = D_i^2(t) \frac{P_j(t) - P_{j+1}(t)}{32\mu L_j} = M D_i^2(t) \frac{P_j(t) - P_{j+1}(t)}{32\mu L}$$

$$\text{But } P_j(t) - P_{j+1}(t) = \frac{128\mu L Q_1(t)}{2^{j-1} \pi M D_i^4(t)} = \frac{128\mu L Q(t)}{2^{j-1} \pi M D_i^4(t)} = \frac{N 2^{M-2}}{2^{j-1} (2^{M-1}-1)} (P_1(t) - P_M(t))$$

Therefore

$$v_j(t) = \frac{N M 2^{M-2} D_i^2(t) (P_1(t) - P_M(t))}{2^{j-1} (2^{M-1}-1) 32\mu L} \quad \text{Eq.26}$$

The average speed is then:

$$v(t) = \frac{\sum_{j=1}^M 2^{j-1} v_j(t)}{\sum_{j=1}^M 2^{j-1}} = \frac{\sum_{j=1}^M \frac{N M 2^{M-2} D_i^2(t) (P_1(t) - P_M(t))}{(2^{M-1}-1) 32\mu L}}{2^M - 1}$$

Thus

$$v(t) = \frac{2^{M-2} M^2 N D_i^2(t) (P_1(t) - P_M(t))}{(2^M - 1) (2^{M-1} - 1) 32\mu L} \quad \text{Eq.27}$$



**Model input parameters: estimates of compartment length and branching**

	<i>pia</i>	<i>A1</i>	<i>A2</i>	<i>Capillaries</i>
<i>L</i>	300	100	100	300
<i>N</i>	1	1	4	3
<i>M</i>	2	2	4	2