SUPPLEMENTARY INFORMATION

Visual and modular detection of pathogen nucleic acids with enzyme-DNA molecular complexes

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SUPPLEMENTARY FIGURES

Supplementary Figure 1. Schematics of the enVision microfluidic platform. (a) Exploded schematic and **(b)** sectional side view of the platform. The platform comprises unique assay cassettes and a common signaling cartridge. Each assay cassette is preloaded with unique recognition nanostructures and contains a serpentine microchannel to improve mixing. Polycarbonate membranes are embedded in the common cartridge to immobilize the signaling nanostructures. Fluidic flow from the sample inlet to the common outlet, actuated by withdrawal septum, is indicated in red.

Step 1: Sample loading

Samples are added to the inlets of individual assay cassettes, each preloaded with recognition nanostructures targeting for specific DNA sequences.

Step 2: Recognition

The assay cassettes are mounted onto the common cartridge. A negative pressure is used to actuate parallel fluid flow. Diffusive mixing in the serpentine channel improves sequence recognition and activation of the inactive polymerase if target is present.

Step 3: Target-independent signal enhancement

The active polymerases are transferred into the reaction chambers, where they add HRP to the immobilized universal signaling nanostructures through biotinylated dNTPs.

Step 4: Visual detection

Unbound HRP is removed and HRP substrate is introduced uniformly into the reaction chambers. Development of the HRP substrates leads to direct visual readout.

Different enVision assays with unique recognition nanostructures

Supplementary Figure 2. Device operation.

Supplementary Figure 3. Activity of the recognition nanostructure. (a) A varying amount of inhibitory aptamer was added to a fixed amount of polymerase (5 units) to determine the optimal ratio to complex the recognition nanostructure while maximizing the inhibitory effect. **(b)** To the optimized nanostructure complex, we incubated different amounts of complementary DNA target as well as scrambled oligonucleotide sequence as a control. Note that only complementary target resulted in strong and proportional increase in polymerase activity, while the scrambled oligonucleotide sequence produced negligible activity (**P* < 0.05, ****P* < 0.0005, **** *P* < 0.00005, Student's t test). All measurements were performed in triplicate, and the data are displayed as $mean \pm s.d.$

Supplementary Figure 4. Annealing of the signaling nanostructure. (a) The hairpin signaling nanostructure and its equivalent-sized linear counterpart (with excess primers) were resolved through 8 % native gel electrophoresis at room temperature. The band intensities of the primed and unprimed fractions in each sample were analyzed (***** *P* < 0.000005, Student's t test). **(b)** Melting curve analysis of the self-priming signaling nanostructure and its linear counterpart. SYBR green fluorescence intensities were recorded with increasing reaction temperature to assess the dissociation characteristics of double-stranded DNA. Dotted lines indicate the observed melting temperatures (T_m) of the respective nucleic acids. The nanostructure showed a higher T_m as compared to its linear counterpart (with excess primers). All measurements were performed in triplicate, and the data are displayed as mean ± s.d in **a**.

Supplementary Figure 5: Visual and fluorescence readouts. (a) Optimization of enzyme reactions**.** We measured the real-time activities of DNA polymerase (DNA pol, top) and HRP (bottom), in the presence of control (water) and varying amounts of DNA targets. Polymerase activity was determined via a Taqman assay (fluorescence measurement of 5' exonuclease degradation of Taqman probes), while HRP activity was determined via smartphone intensity measurement. Polymerase activity corresponds to Steps 1-3 in the device operation and HRP activity corresponds to Step 4 (see Supplementary Fig. 2 for more details). The optimized durations for these enzyme reactions were thus determined at ~ 20 min and 3 min, respectively. **(b)** Example images of enVision readouts (top), after image conversion to greyscale (middle) and the distribution of greyscale pixel intensities (bottom). The mean pixel intensity of each spot image was used for signal quantification and normalization. **(c)** Visual detection sensitivity of the enVision system. The detection limit (dotted line) was determined by directly titrating a known amount of target DNA (without asymmetric amplification) and measuring their associated visual signals through the enVision platform at room temperature. All visual signals were acquired through a smartphone. **(d)** Fluorescence detection sensitivity. The detection limit (dotted line) was determined by directly titrating a known amount of target DNA with the recognition nanostructure. The polymerase activity was measured via its 5' exonuclease degradation of fluorescent Taqman probes. All fluorescence signals were acquired though a commercial qPCR fluorescence detector. All measurements were performed in triplicate, and the data are displayed as mean \pm s.d. a.u., arbitrary unit.

Supplementary Figure 6. Nested asymmetric amplification. (a) Schematic of the nested amplification. To significantly expand the population of single-stranded DNA for minuscule amounts of samples, a nested asymmetric PCR amplification was employed. The samples were first exponentially amplified, in the presence of equally concentrated dual primers, and subsequently linearly amplified, using an excess of a single primer. **(b)** Efficiency of the nested asymmetric amplification. Amplification products from (1) 1 pmole, (2) 100 fmole, (3) 10 fmole, (4) 1 fmole, (5) 100 amole, (6) 10 amole, (7) 1 amole, and (8) no template control of synthetic HPV16 sequence were analyzed on a 8 % PAGE gel. The upper arrow indicates larger, double-stranded products while the lower arrow corresponds to single-stranded products.

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Supplementary Figure 7. Nucleic acid sequence based amplification (NASBA). (a) Schematic of NASBA. DNA targets were first primed for RNA transcription and single-stranded RNA amplification via the T7 RNA polymerase. The RNA products were then reverse transcribed into cDNA before being subjected to RNA digestion to produce single-stranded DNA products. **(b)** Efficiency of NASBA. Amplification products from (1) 1 pmole, (2) 100 fmole, (3) 10 fmole, (4) 1 fmole, (5) 100 amole, (6) 10 amole, (7) 1 amole, and (8) no template control of synthetic HPV 16 sequence were analyzed on a 8 % PAGE gel. The arrow indicates the expected size of the DNA products.

Supplementary Figure 8. Melting curve analysis of SYBR Green qPCR reactions. Melting curves for primer pairs of **(a)** HPV 6, **(b)** HPV 11, **(c)** HPV 16, **(d)** HPV 18, **(e)** HPV 31, **(f)** HPV 33, **(g)** HPV 58, and **(h)** HPV 66 sequences. Each primer set was tested against target template (blue), off-target template from other HPV subtypes (red), or no template control (water, light blue). All measurements were performed in triplicate, and displayed as line plots of the mean fluorescence intensities.

Supplementary Figure 9. Direct RNA detection. We tested the developed enVision assays (i.e., HPV 16 and HPV 18 assays) for direct detection of DNA (left) and RNA (right) of different HPV subtypes. See Methods for details on the preparation of the RNA targets. All RNA targets were used directly without any cDNA conversion. Targets were considered as either complementary or off-target. The enVision assays demonstrated specific and direct detection of RNA targets, with signals comparable to that of DNA targets. All signals were normalized against each assay's positive DNA signal for relative comparison. All measurements were performed in triplicate, and the data are displayed as mean \pm s.d.

Supplementary Figure 10. enVision logic gates. By varying the combination of recognition nanostructures as well as the ratio of different components (i.e., aptamer, inverter and polymerase) in each nanostructure, we programmed the following logic computations: **(a)** AND gate, **(b)** OR gate, **(c)** NOT gate for HPV 16, **(d)** NOT gate for HPV 18, **(e)** NAND gate, and **(f)** NOR gate. For each gate designed, the components used to establish the configuration are illustrated (top right of each panel). Each gate was tested with different combinations of DNA targets, isolated from HPV 16 (Target 1) and HPV 18 (Target 2). All target combinations and their expected computational outputs are summarized in corresponding truth tables (bottom left of each panel). The observed enVision signals (bottom right of each panel) showed a good agreement with the expected outputs. All signals were normalized to appropriate controls (no-target controls) as previously described. Normalized signals above the detection threshold (i.e., 3x s.d. higher than background signal) were considered as true signals (red bars); otherwise a false signal was called (black bars). All measurements were performed in triplicate, and the data are displayed as mean \pm s.d.

Supplementary Figure 11. Multiplexed amplification of genomic DNA. Full gel

electropherogram of amplification products from CaSki genomic DNA. Genomic DNA was amplified in the presence of different HPV 16 locus primers: (1) E1, (2) L1, (3) L2, (4) combined primers of E1, L1 and L2, as well as (5) no primers. Lane 7 was loaded with 15 bp DNA ladder. Arrow indicates the position of the 50 bp band.

Supplementary Figure 12. Multiplexed enVision detection of genomic DNA. Equal amounts of cellular genomic DNA (top: CaSki, middle: HeLa, bottom: C33-a) were incubated directly with specific recognition nanostructures against different HPV subtypes (left: HPV 16, right: HPV 18). Samples were treated with individual recognition nanostructures (i.e., E1, L1 and L2) or a pool of three structures simultaneously (combined). All signals were normalized as a percentage of the maximal signal observed for each HPV subtype. The multiplexed measurements correlated well with the known HPV infections of the cell lines, as reported by previous literatures (red: present, white: absent). Note that the single locus measurement could miss positive infection (e.g., HeLa, HPV 18 locus L2). All measurements were performed in triplicate, and the data are displayed as $mean \pm s.d.$

Supplementary Figure 13. Comparison of enVision and LAMP design and performance. (a) Comparison of probe options found in the highly variable regions of the E1, L1 and L2 loci in different HPV subtypes. Probe options were identified for the enVision system (left) as well as LAMP (right). The enVision platform not only generated more probe choices but also provided comprehensive coverage for all regions tested. **(b)** Comparison of enVision performance (left) with that of top-ranked LAMP primer sets (right) for HPV subtyping in cellular genomic DNA. enVision had 83.3% sensitivity (5/6) and 100% specificity (12/12) while LAMP had 50.0% sensitivity (3/6) and 75.0% specificity (9/12). Multi-loci measurements were made across different cell lines of known infections. All signals were normalized to appropriate controls (no-target controls) as previously described. Note that only the enVision technology showed accurate HPV subtyping, as compared to known cellular infection status (red bar: present, white bar: absent). LAMP

demonstrated significant false positives (e.g., CaSki cells, HPV 18; HeLa cells, HPV 16). All measurements were performed in triplicate, and the data are displayed as mean \pm s.d.

Supplementary Figure 14. Multiplexed enVision detection in clinical samples. High-coverage multi-loci enVision assays (simultaneous detection of E1, L1 and L2) were performed in clinical endocervical brush samples (*n* = 35 patients) for molecular subtyping of HPV 16 (top panel) and HPV 18 (bottom panel). All measurements were performed in triplicate, and the data are displayed as mean \pm s.d.

Supplementary Figure 15. Clinical validation with Taqman fluorescence assays. Taqman assays were designed to detect the HPV 16 E1, L1 and L2 loci, respectively. All clinical validation assays were performed with qPCR analysis. Relative quantitation was performed for each sample by normalizing with respective GAPDH expression. Note that the data correlated well to the signals detected with the enVision platform to identify previously undetectable infections (see Fig. 5c). All measurements were performed in triplicate, and the data are displayed as mean \pm s.d.

Supplementary Table 1. Oligonucleotides used for activity and sensitivity characterization.

Supplementary Table 2. Nanostructures for HPV pan-detection and specific subtyping.

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Supplementary Table 3. SYBR Green qPCR primers and RNA templates.

Supplementary Table 4. Nanostructures for multi-loci HPV detection.

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Supplementary Table 5. Nanostructures for enVision logic gates.

Supplementary Table 6. Top-ranked LAMP primers for different HPV loci.

Top-ranked LAMP primers were determined from their Δ*G, the change in free energy during LAMP reaction.*

Supplementary Table 7. Comparison of detection technologies.

CI, confidence interval.

SUPPLEMENTARY REFERENCES

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