Supplementary Tables

| HVM device | Video format | Description | Approximate field of view | Approximate pixel pitch * |
|---------------|---|---------------------------------------|---------------------------|---------------------------|
| Cytocam IDF | avi, ≤ 716 x 572 px | CCtools AVA 3.x export | 0.5898 mm^2 | 1.2 μm px ⁻¹ |
| Cytocam IDF | mha, $\leq 2208 \text{ x } 1648 \text{ px}$ | CCtools 1.7.x native recording format | 1.7830 mm^2 | 0.7 μm px ⁻¹ |
| Microscan SDF | avi, ≤ 716 x 572 px | AVA 3.x native recording format | 0.5898 mm ² | 1.2 μm px ⁻¹ |

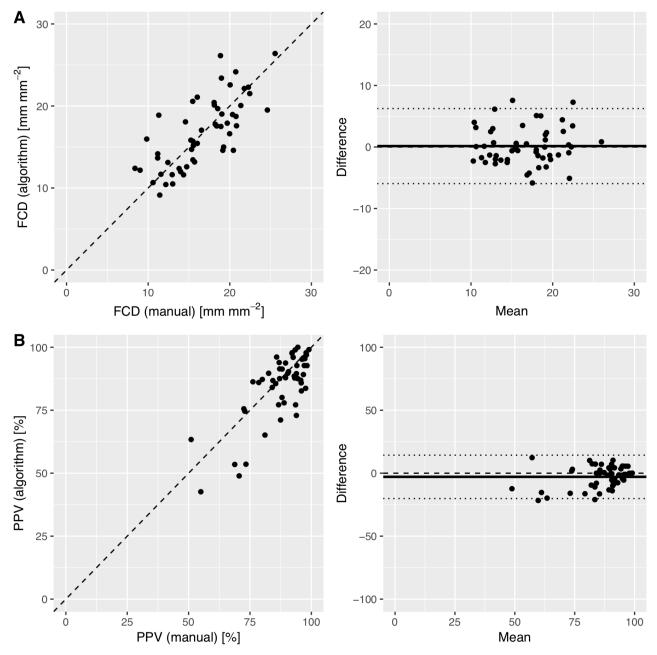
Supplementary Table 1. Combinations of HVM recording devices and video formats. "≤" denotes the possibility of frame downsizing during stabilization procedures preceding analysis. *field of view and pixel pitch were determined for each combination of individual HVM recording device and video format using a formal calibration procedure, approximate mean values are given here for reference. IDF, incident dark field; SDF, sidestream dark field.

| Symbol | Description | Parameter values | |
|--|--|---|---|
| | • | | Cytocam IDF, porcine sublingual microcirculation, AVA 3.x avi |
| Vessel recognition | | | |
| clahe_clip | Contrast enhancement limit for contrast limited adaptive histogram equalization. | | 2, 0 |
| clahe_grid [px] | Grid size for contrast limited adaptive histogram equalization. | | 32, 0 |
| σ [px] | Contrast enhancement limit for contrast limited adaptive histogram equalization. Grid size for contrast limited adaptive histogram equalization. Standard deviation of the the Gaussian kernel used for principal curvature-based region detection ³⁷ . Upper threshold for the linking algorithm, where new lines are created as long as the starting point has a higher second directional derivative ³⁷ . Lower threshold for the linking algorithm, where points are added to the current line as long as they have a higher second directional derivative ³⁷ . Threshold for a high-pass filter for vessel length implemented downstream of the detection and linking algorithms. | | 3, 9 |
| h [px] | Upper threshold for the linking algorithm, where new lines are created as long as the starting point has a higher second directional derivative ³⁷ . | segmentation pas er of parameters li configuration file | 1.1, 0.1 |
| 1 [px] | Lower threshold for the linking algorithm, where points are added to the current line as long as they have a higher second directional derivative ³⁷ . | nber of se number o | 0, 0 |
| min_length [px] | Threshold for a high-pass filter for vessel length implemented downstream of the detection and linking algorithms. | The nun the | 40, 120 |
| capillary_cutoff [µm] | Low-pass cutoff value for mean vessel diameter used for classification as a capillary. | 20 | |
| Space-time diagram | classification as a capital y. | | |
| analysis | | | |
| smooth_σ [px] | Standard deviation of the Gaussian kernel used for Gaussmoothing. | 1 | |
| σ [px] | Standard deviation of the Gaussian kernel used for principal of based region detection ³⁷ . | 1.5 | |
| h [px] | Upper threshold for the linking algorithm, where new lines at if the starting point has a higher second directional deriva | 1.1 | |
| 1 [px] | Lower threshold for the linking algorithm, where points are the current line if they have a higher second directional deri | 0 | |
| min_length [px] | High-pass cutoff value for artefact detection: Threshold for a filter for vessel length implemented downstream of the detection linking algorithms. | 20 | |
| curvature index_cutoff [1] | High-pass cutoff value for artefact detection: proportion of l straight line between start and endpoint of ridge AND actulength. | 0.02 | |
| low_flow_cutoff [μm s ⁻¹] | Low-pass cutoff value for individual RBC path RBCv for R classification of no flow/low flow versus normal flow | 10 | |
| perfused_cutoff [1] | High-pass cutoff value for the proportion of no flow / low fl paths in a per-vessel frequency distribution used for veclassification as perfused. | 0.1 | |

Supplementary Table 2. Set of parameters for vessel detection and space-time diagram analysis using the proposed advanced computer vision algorithm. * depending on validation of combinations of tissue type, HVM recording devices and video formats.

Supplementary Figures

Supplementary Figure 1. Good correlation was observed between manually measured and algorithm-based FCD (A) and PPV (B) in the septic shock model.



FCD and PPV were compared by field of view in the septic shock and control groups (n=53). Good correlation was observed for FCD (r=0.7, p<0.0001, bias 0.2 mm mm⁻², level of agreement -6.0–6.3 mm mm⁻², precision 3.1 mm mm⁻², percentage error 2.9%) and PPV (r=0.8, p<0.0001, bias -3%, level of agreement -20–14%, precision 9%, percentage error -3.3%). Dashed lines represent identity lines. In Bland-Altman analysis, solid line represents bias and dotted lines represent ± 2 σ levels of agreement. FCD, functional capillary density; PPV, proportion of perfused vessels.