

## **Supplementary Information for**

**Microfluidic protein isolation and sample preparation for high-resolution cryo-EM**

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**Fig. S1.** Image of the magnetic trap set-up. The opposite poles of two 4*.*8W electromagnets **(a)** are facing one another. A microcapillary **(b)**, held with the manipulator arm **(c)**, is placed between the two iron tips **(d)** of the electromagnets. The trapped magnetic plug can be observed with a camera **(e)** via a mirror **(f)**. The photo-cleavable cross-linker can be exposed to UV light using a LED **(g)** emitting light at 365 nm that is deflected by a mirror **(h)**.

## **Supporting Information Text**

**A. Characteristics of the magnetic trap.** The magnetic particle trap consists of two electromagnets arranged with opposite poles facing one another (Fig. [S1\)](#page-1-0). Attached iron tips extend the magnet cores. This concentrates the magnetic flux to a small area and forms a strong field gradient between the two tips (see Fig. [S2\)](#page-2-0). For magnetic particle trapping, the front part of the microcapillary segment just above the nozzle was placed in this region using a motorized XYZ linear translation stage, and the sample was aspirated. The magnetic force acting on the super-paramagnetic particles immobilized the beads.

In experiments, super-paramagnetic beads with sizes from 15 nm to 1000 nm can be trapped and experience a magnetic force  $F_m$  acting on a saturated particle according to:

$$
F_m = V \cdot M_S \cdot \mu_0 \cdot \nabla H \tag{1}
$$

where *V* is the volume of the magnetic particles,  $M<sub>S</sub>$  the saturation magnetization,  $\mu_0$  the magnetic constant, and *H* the magnetic field strength. The current controls the field applied by the electromagnets. Due to the dependence on the volume (*V* ), higher currents are needed in order to trap smaller particles. When the electromagnets are operated at maximum power, the core and the tips significantly heat up. For this reason, a cooling water system was implemented allowing the tips to be cooled to 4 °C by pumping water through a copper tubing twisted around them. Both, the copper tubing and the iron tips were coated with nickel to reduce corrosion. The magnetic trap is mounted on a motorized stage, allowing it to be moved in the vertical direction, independent of the microcapillary manipulator arm. For sample uptake, the magnetic trap and microcapillary were simultaneously moved down to insert the nozzle tip of the capillary into the sample well.

The parts used to build the magnetic trap are summarized in Table [S1.](#page-3-0) Connecting parts were manufactured by the workshop of the Biozentrum, University of Basel, Switzerland. Plans are available upon request. Further cryoWriter parts used for grid preparation are described in [\(1\)](#page-11-1).

Fig. [S2](#page-2-0) shows a finite element simulation of the magnetic flux density within the magnetic trap system, which was caluclated with COMSOL Multiphysics. Soft-iron material properties were applied to the magnet cores and tips using a non-linear B-H curve that includes saturation effects. The windings were modelled with coil features.

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**Fig. S2.** Finite element simulation of the magnetic field generated by the electromagnetic trap system. **(a)** 2D plot of the magnetic flux density around the iron tips (black solid lines). The direction of the magnetic fields is shown with black arrows. The size of the arrows is proportional to the field strength. The values in the color scale are given in Tesla (T). **(b)** Extracted 1D plots of the magnetic flux density from the 2D plot in (a) at the positions indicated with dashed lines. The figure shows that between the tips (x=0) the highest field gradients are observed. This leads to a magnetic force *F<sup>m</sup>* pushing magnetic particles towards this region.

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**Table S1. Parts list of the magnetic trap setup.**

<span id="page-4-0"></span>**B. Enclosure of sample between air bubbles.** The sample can optionally be enclosed between air bubbles that are separated by washing buffer. The air bubbles act as barriers for the protein particles and reduce dilution by diffusion and Taylor dispersion. In this experiment two 6 nL air bubbles separated by 25 nL washing buffer containing 1 mg TMV were used (Fig. [S3\)](#page-4-0).



**Fig. S3.** Illustration of the magnetic particle-plug enclosed between two 6 nL air bubbles for UV exposure and elution. The air bubbles act as barriers preventing diffusion and Taylor dispersion to keep the protein concentration as high as possible.

<span id="page-5-0"></span>**C. Data collection and image processing parameters.** The data collection parameters are provided in Table [S2,](#page-5-0) and the main image processing parameter used for the 20S proteasome and TMV are given in Tables [S3](#page-5-1) & [S4.](#page-5-2)







<span id="page-5-2"></span><span id="page-5-1"></span>**Table S3. Image processing parameters used for 20S proteasome structure determination with RELION3.**



**Table S4. Image processing parameters used for helical structure determination of TMV with RELION3.**

<span id="page-6-1"></span>**D. Fourier shell correlation and local resolution histograms.** We used the Fourier shell correlation method [\(2\)](#page-11-2) between two independently refined half-maps ('gold standard') [\(3\)](#page-11-3) to estimate the resolution of our 3D reconstructions (Fig. [S4a](#page-6-0)). A threshold of 0*.*143 on the FSC curve was adopted to define the resolution limit of the reconstruction [\(4\)](#page-11-4). The FSC curves were corrected for artificial correlations introduced by masking [\(5\)](#page-11-5). We found a global resolution of 3*.*5 Å for the 20S proteasome and of 1.9 Å for the TMV. These estimates correlate well with the features observed in the maps (see Fig. 3 of the main text for the 20S proteasome and chapter [G](#page-10-0) for the TMV). The estimated resolution is further corroborated by the local resolution histograms shown in Fig. [S4b](#page-6-0), which display the normalized counts of voxels at each resolution. The resolution for the proteasome varies significantly; for more details, see Chapter [E.](#page-7-0) The local resolution was assessed based on the half-maps using the method described in  $(6)$ , as implemented in RELION3, with a map sampling of 25 Å (Fig. [S4b](#page-6-0)).

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**Fig. S4.** Resolution estimation for the 20S proteasome (blue) and TMV (green). (**a**) Fourier shell correlation from the RELION3 refinement. (**b**) Histograms depicting the normalized voxel counts per resolution range.

<span id="page-7-1"></span><span id="page-7-0"></span>**E. Local resolution map of the 20S proteasome.** Fig. [S5](#page-7-1) shows the local resolution calculated for the 20S proteasome using RELION3. Note that the active domains (indicated by red arrowheads in Fig. [S5\)](#page-7-1) are less well resolved than the other domains, and are associated with the catalytic subunits of the *β*-ring. Interestingly, the resolution of the *α*-ring around the pseudo-seven-fold axis is quite heterogeneous, whereas the *β*-ring exhibits lower resolution around subunits *β*4 and *β*5. Since subunits *β*4, *β*5 and *β*6 are the catalytically active elements [\(7\)](#page-11-7), the lower resolution of subunits *β*4 and *β*5 suggests that these are trapped in various conformations during cryo-EM grid preparation.



**Fig. S5.** Local resolution map for the human 20S proteasome at a global resolution of 3*.*5 Å. (**a**) Side view with annotated Fabs. (**b**) Local resolution of the *α*-subunits. (**c**) Local resolution of the *β*-subunits. The red arrowheads indicate the catalytically active subunits.

<span id="page-8-0"></span>**F. Model building results.** After initial rigid body fitting, the 20S proteasome and TMV models were refined using PHENIX. The models were assessed by the fit to the experimental density and validated with clashscore, Ramachandran statistics, and good bond/angle lengths as shown in Tables [S5](#page-8-0) & [S6.](#page-8-1) Additionally, a random shift (mean 0*.*3 Å) was introduced to the final models and each model was refined with the same settings against one unfiltered half map (half-map 1). The FSC curves of the models against half-map 1 and the other half map (half-map 2) was then calculated (Fig. [S6](#page-9-0) & [S7\)](#page-9-1). The fact the both curves look very similar indicates that no overfitting took place.



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<span id="page-9-1"></span>**Fig. S6.** FSC curve of the final 20S proteasome model versus the full map (all data), against which the model was refined (red). The full map used to calculate the FSC was resolution filtered. FSC curve of the final 20S proteasome model with randomized coordinates shifts (mean shifts of 0.3 Å) versus the first unfiltered half-map (half-map 1) against which it was refined (grey) and versus the second half-map (half-map 2) against which it was not refined (blue).



**Fig. S7.** FSC curve of the final TMV model versus the full map (all data), against which the model was refined (red). The full map used to calculate the FSC was resolution filtered. FSC curve of the final TMV model with randomized coordinates shifts (mean shifts of 0*.*3 Å) versus the first unfiltered half-map (half-map 1) against which it was refined (grey) and versus the second half-map (half-map 2) against which it was not refined (blue).

<span id="page-10-0"></span>**G. Three-dimensional map of TMV.** Fig. [S8](#page-10-1) demonstrates the high quality of the microfluidic grid preparation. We report here the map of TMV at a global resolution of 1*.*9 Å. Compared to the 20S proteasome, this map has both higher global resolution (see FSC curve in [D,](#page-6-1) Fig. [S4a](#page-6-0)) and less variable local resolution (Fig. [S4b](#page-6-0)) due to the higher rigidity of the structure and the helical symmetry averaging imposed on the reconstruction.

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**Fig. S8.** 3D reconstruction of TMV at a global resolution of 1*.*9 Å showing the top view (**(a**) and the side view (**b**) of the electron density map. The zoom-in (**c**) demonstrates the high resolution features of the map. At this resolution it is possible to see the holes of the aromatic rings (**d**).

## <span id="page-11-0"></span>**References**

- <span id="page-11-1"></span>1. Claudio Schmidli, Luca Rima, Stefan A Arnold, Thomas Stohler, Anastasia Syntychaki, Andrej Bieri, Stefan Albiez, Kenneth N Goldie, Mohamed Chami, Henning Stahlberg, and Thomas Braun. Miniaturized sample preparation for transmission electron microscopy. *JoVE*, (137):e57310, 2018. .
- <span id="page-11-2"></span>2. George Harauz and Marin van Heel. Exact filters for general geometry three dimensional reconstruction. *Optik*, 78(4):146–156, 1986. ISSN 0030-4026. URL <http://md1.csa.com/partners/viewrecord.php?requester=gs{&}collection=TRD{&}recid=1507969EA>.
- <span id="page-11-3"></span>3. Sjors H.W. W Scheres and Shaoxia Chen. Prevention of overfitting in cryo-Em structure determination. *Nat. Methods*, 9(9): 853–854, jul 2012. ISSN 15487091. . URL <http://dx.doi.org/10.1038/nmeth.2115>.
- <span id="page-11-4"></span>4. Peter B Rosenthal and Richard Henderson. Optimal determination of particle orientation, absolute hand, and contrast loss in single-particle electron cryomicroscopy. *J. Mol. Biol.*, 333(4):721–745, oct 2003. ISSN 0022-2836. . URL <http://www.sciencedirect.com/science/article/pii/S0022283603010222>.
- <span id="page-11-5"></span>5. Shaoxia Chen, Greg McMullan, Abdul R. Faruqi, Garib N. Murshudov, Judith M. Short, Sjors H.W. W Scheres, and Richard Henderson. High-resolution noise substitution to measure overfitting and validate resolution in 3D structure determination by single particle electron cryomicroscopy. *Ultramicroscopy*, 135(0):24–35, dec 2013. ISSN 0304-3991. . URL [http://dx.doi.org/10.1016/j.ultramic.2013.06.004http://www.sciencedirect.com/science/article/pii/S0304399113001472](http://dx.doi.org/10.1016/j.ultramic.2013.06.004 http://www.sciencedirect.com/science/article/pii/S0304399113001472).
- <span id="page-11-6"></span>6. Giovanni Cardone, J Bernard Heymann, and Alasdair C Steven. One number does not fit all: Mapping local variations in resolution in cryo-EM reconstructions. *J. Struct.l Biol.*, 184(2):226–236, 2013. ISSN 1047-8477. .
- <span id="page-11-7"></span>7. Paula C. A. da Fonseca and Edward P. Morris. Cryo-EM reveals the conformation of a substrate analogue in the human 20S proteasome core. *Nat. Commun.*, 6(7573), July 2015. ISSN 2041-1723. .
- <span id="page-11-8"></span>8. Andrew Leaver-Fay, Gary J. Kapral, Ian W. Davis, Jack Snoeyink, Jane S. Richardson, Jeremy N. Block, Laura W. Murray, Vincent B. Chen, III Arendall, W. Bryan, Xueyi Wang, and David C. Richardson. MolProbity: all-atom contacts and structure validation for proteins and nucleic acids. *Nucleic Acids Research*, 35(suppl\_2):W375–W383, 07 2007. ISSN 0305-1048. . URL <https://dx.doi.org/10.1093/nar/gkm216>.