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## Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study

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# Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study

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Keywords: Remote monitoring, vital signs, continuous, reliability, validation

Word count:

## Abstract

### Objective

The objective of this study was to validate the accuracy of a wearable remote vital signs monitor to measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk of complications.

### Design

Manually-recorded vital signs data were paired with vital signs data derived from the remote monitor set in patients participating in a trial of continuous remote vital signs monitoring.

### Setting

St James's University Hospital, United Kingdom.

### Participants

51 patients who had undergone major elective general surgery.

### Interventions

The intervention under investigation was the SensiumVitals® monitoring system. This consist of a wireless patch which is worn on the patient's chest and measures heart rate, respiratory rate and temperature continuously. The reference standard was nurse-measured manually-recorded vital signs as part of the National Early Warning Score.

### Primary and secondary outcome measures

The primary outcomes were the 95% limits of agreement between manually-recorded vital signs and wearable vital sign patch recordings of heart rate, respiratory rate and temperature. The secondary outcomes were the average percentage completeness of data for each vital sign.

### Results

There were 2,737 pairs of matched data. Heart rate measurements showed good correlation ( $R^2 = 0.67$ ). There was low correlation for respiratory rate ( $R^2 = 0.01$ ) and temperature ( $R^2 = 0.13$ ). The average completeness of data were 72.8% for temperature, 59.2% for heart rate and 34.1% for respiratory rate. Distributions of respiratory rate in manually-recorded measurements were statistically implausible.

### Conclusions

The remote continuous monitoring system is capable of reliably measuring heart rate, and correlates well with manually-recorded heart rate. The accuracy of respiratory rate and temperature was outside of acceptable limits. Limitations of the remote monitoring system could potentially be

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overcome through better signal processing. Inaccuracies in the manually-recorded data present an opportunity to increase awareness amongst staff about the importance of manual observations.

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## Article Summary: Strengths and limitations of this study

- Surgical patients are a population likely to benefit from continuous physiological monitoring.
- A large number of paired data sets were available for comparison.
- The reference standard is a clinically relevant comparison, and is standard of care throughout the UK.
- The accuracy of the reference standard is user-dependent.

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## 1. Introduction

Physiological monitoring using early warning score systems is effective but limited by its intermittent nature (1). It is hypothesised that continuous vital signs monitoring may allow earlier detection of patient deterioration and thereby improve patient outcomes, but existing evidence is limited (2). A consensus of international experts in safety and healthcare technology concluded that, if technically possible and affordable, all patients who are for active treatment should be continuously monitored (3).

Until recently, continuous vital signs monitoring was limited to critical care areas because it required high staff-to-patient ratios and cumbersome equipment which tethered the patient to the bed-space, thereby inhibiting patient mobility and recovery. When hard-wired monitoring was implemented on a general ward, only 16% of patients remained connected in a 72-hour period (4).

New remote monitoring devices, consisting of wearable sensors and aided by wireless data transmission, allow the patient to ambulate freely whilst enjoying the presumed advantages of extra monitoring. Since 2002, a number of such tools have received the United States Food and Drug Administration (FDA) clearance, indicating that they are safe and effective, but clinical studies are required to demonstrate their utility in the inpatient setting (5,6).

A remote monitoring device with a considerable amount of clinical evidence is the SensiumVitals® patch (Figure 1). Attached to the patient's chest with two ECG electrodes, the device monitors heart rate, respiratory rate and skin temperature continuously. The data are transmitted wirelessly every two minutes to a central monitoring station or a mobile device carried by the patient's nurse. This alerts the healthcare worker when there is deviation from pre-set physiological norms, alerting staff to potential patient deterioration.

The patch records respiratory rate by means of impedance pneumography and heart rate through single-lead ECG activity. Temperature is measured by a temperature-sensitive resistor. Once a physiological signal is fully acquired, it is processed by its associated embedded algorithm running inside the in-built processing unit, which enables the transmission of the resultant values to a nearby intranet hot-spot for onward transmission to the central monitoring system.

The underlying technology incorporated into such devices is well understood, but there is limited evidence for its reliability in the clinical setting. One previous study exists which validated the accuracy of the SensiumVitals® system in 61 hospital patients. The patients were monitored at rest for a maximum of two hours, and the device was tested against a conventional bedside clinical monitor using capnographic respiratory rate (7). This does not reflect the true clinical environment, which challenges such devices to provide monitoring continuity over several days in ambulatory patients.

In this study, we validated the accuracy of the SensiumVitals® system to measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk for complications. The reference standard were manually-recorded vital signs as part of the National Early Warning Score (NEWS). The objective of this study was to assess whether the wireless patch system is able

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3 to reliably measure vital signs continuously in the clinical setting, and to determine how well it  
4 compares to manually-recorded measurements.  
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## 9 2. Methods

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11 Ethical approval was granted on 10th October 2017 by the Yorkshire & The Humber – Leeds West  
12 Research Ethics Committee, ref: 17/YH/0180. Informed consent to participate was obtained from all  
13 participants in the study.  
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### 16 2.1 Study design

17  
18 All participants were enrolled in the TRaCINg study, the protocol for which has been published  
19 previously (8). This was a single-centre, feasibility, randomised, controlled, parallel group trial of  
20 continuous remote vital signs monitoring for patients who had undergone major elective general  
21 surgery at St James's University Hospital, Leeds, United Kingdom. Participants were individually  
22 randomised on a 1:1 basis to receive either remote monitoring plus NEWS or monitoring by NEWS  
23 alone. This paper describes the data from participants randomised to the remote monitoring arm,  
24 who wore the SensiumVitals® patch during their hospital admission.  
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### 28 2.2 Patient and public involvement

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30 Patients and the public were involved in the design of the randomised controlled trial, but were not  
31 involved in the design of this validation study.  
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### 34 2.3 Data collection

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36 Vital signs data was collected for each participant from two sources. The SensiumVitals® vital sign  
37 data were documented at 2-minute intervals and collected from a hospital desktop computer using  
38 data-acquisition software developed by Sensium. These data had been pre-processed to discard  
39 signals that were subject to gross electrical or motion artefact (7).  
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42 NEWS data were collected at regular intervals, depending on the patients' status and based on the  
43 NEWS protocol(9). Typically, vital signs were collected at the bedside by members of the nursing  
44 staff who were blinded to the SensiumVitals® vital sign data: pulse rate was measured using the  
45 pulse oximeter on a multi-parameter portable vital signs monitor; temperature was measured using  
46 a tympanic thermometer; respiratory rate was measured manually. The NEWS scores and their  
47 component parts were documented electronically. Researchers collected manually-recorded heart  
48 rate, respiratory rate and temperature data from the hospital's electronic patient record. Other vital  
49 signs collected by the nursing staff as part of the early warning score, such as oxygen saturations,  
50 were not extracted.  
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### 54 2.4 Data processing

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56 The two data sources were linked using NHS number and timestamp and consolidated into a single  
57 deidentified spreadsheet. Paired data to a NEWS observation was derived from the SensiumVitals®  
58 continuous data set by using the median vital sign value within a  $\pm 10$ -minute window of a manually-  
59 recorded observation. The time window was used to account for differences between the nurses'  
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3 manually-documented times and the automatic timestamps from the vital sign patch. The median  
4 value within this window was used to eliminate the impact of intermittent sensor noise.  
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## 7 2.5 Outcomes

8 The primary outcomes were the 95% limits of agreement between manual nurse observations and  
9 wearable vital sign patch recordings of Heart Rate (HR), Respiratory Rate (RR) and Temperature  
10 (Temp). Following precedent, we defined clinical acceptability to be  $max \pm 10\%$  for HR and RR (or  $\pm 3$   
11 breaths per minute or  $\pm 5$  beats per minute) and  $0.5^\circ\text{C}$  for Temp (10,11). The secondary outcome was  
12 the average percentage completeness of each vital sign.  
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## 15 2.6 Statistical Analysis

16 For each vital sign, we first visually inspected the paired vital sign measurements via scatter plots, in  
17 addition to the raw time series vital signs from the Sensium patch.  
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20 Measurements were then formally compared using Bland-Altman analysis. In this analysis, the mean  
21 difference between the SensiumVitals® data and the nurse observations and the 95% Limits of  
22 Agreement are calculated. We adjusted for repeated measures from the same subject using a model  
23 in which time of measurement is modelled as a random effect. This avoids bias caused by differences  
24 in number of measurements per patient.  
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27 In secondary analysis, we first assessed the average percentage completeness of the data per  
28 patient. The numerator was defined as the number of two-minute periods in which vital sign data  
29 were provided by the patch. The denominator was the number of 2-minute periods that span the  
30 time during which the patch was transmitting data. These time points were preferred to admission  
31 and discharge from ward times because the patch may not have been worn for the patient's entire  
32 ward admission.  
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35 Analyses were undertaken using MATLAB R2017b (The MathWorks Inc., Massachusetts, USA) and  
36 the R Methcomp package (12,13).  
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## 43 3. Results

44 Fifty one patients were recruited to the intervention arm of the TRaCINg study between October  
45 2017 and April 2018. The median number of manually-recorded observation sets was 19 per patient  
46 (range 2 to 73 sets of vital signs measurements). There were 2,737 pairs of matched data available  
47 for analysis. Vital sign traces for one participant over the course of their entire hospital stay are  
48 shown in Figure 2.  
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### 53 3.1 Temperature

54 Figure 3 is a scatterplot of temperatures recorded by nurses versus those measured by the  
55 SensiumVitals® patch. Histograms for each measurement method are presented alongside the x- and  
56 y- axes. There is low correlation between the two measurement methods ( $R^2 = 0.13$ ). The mean and  
57 (standard deviation) of manual temperature and wearable temperature were  $37.1^\circ\text{C}$  ( $0.5^\circ\text{C}$ ) and  
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3 36.4°C (1.0°C). Further inspection of the vital sign time series in Figures 1 and 2 shows multiple  
4 clinically implausible fluctuations of up to 2 °C within 2 hours within each time series. The mean  
5 percentage completeness of temperature data was 72.8%.  
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8 Initial visual inspection was therefore sufficient to show that the patch-derived temperature is not a  
9 suitable proxy for core temperature, as measured by tympanic thermometer. The Bland-Altman  
10 bias (Figure 4) was 0.82°C, with 95% limits of agreement -1.13°C to 2.78°C.  
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### 13 14 15 3.2 Respiratory Rate

16 Figure 5 shows the scatterplot of nurse-recorded respiratory rate against the SensiumVitals® patch  
17 data. There is no correlation between the two measurements methods ( $R^2 = 0.01$ ). The mean and  
18 standard deviation for manual and wearable respiratory rate were 17.6 (1.58) breaths per minute  
19 and 15.0 (5.5) breaths per minute, respectively. The mean percentage completeness of respiratory  
20 rate data was 31.4%.  
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23 Visual inspection of the histogram for manually-recorded respiratory rate shows a large peak at 18  
24 breaths per minute, and a secondary peak at 16 breaths per minute. This result is unexpected for a  
25 natural physiological parameter, which may be expected to vary smoothly over the full range of  
26 values. Inspection of the vital sign patch histogram indicates a significant proportion of  
27 measurements between 5 and 10 breaths per minute. No manually-recorded respiratory rates were  
28 recorded in this range. The Bland-Altman bias (Figure 6) was 2.93 breaths per minute, with 95%  
29 limits of agreement -8.19 to 14.05 breaths per minute.  
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### 33 34 35 3.3 Heart Rate

36 Figure 7 shows the scatterplot of nurse-recorded heart rate against the SensiumVitals® patch. There  
37 is reasonable correlation between the two measurements ( $R^2 = 0.67$ ). The mean and (standard  
38 deviation) for manual and wearable heart rates are 81.6 (16.2) beats per minute (bpm) and 84.3  
39 (19.3) bpm, respectively. The mean percentage completeness of heart rate data was 59.2%. In  
40 addition, visual inspection of the example vital sign traces show good agreement between the  
41 measurements (Figures 1 and 2). The Bland-Altman bias (Figure 8) was 1.85 bpm, with 95% limits of  
42 agreement -23.92 to 20.22 bpm.  
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## 50 4. Discussion

51 In this 51-patient validation study, temperature, respiratory rate, and heart rate measurements  
52 obtained from a wearable vital sign patch were compared with manually-recorded observations by  
53 nursing staff. Heart rate measurements showed good correlation between the two types of  
54 monitoring. There was low correlation between the two measurement methods for respiratory rate  
55 and temperature.  
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3 An advantage of the study design is the collection of a large number of data points for analysis. The  
4 approach is clinically valid, as the NEWS system is the national standard for vital signs monitoring in  
5 the United Kingdom. The surgical patient population is a clinically relevant cohort. There are high  
6 rates of complications after major surgery (14), but many surgical complications, such as sepsis, are  
7 attenuated by early detection. By virtue of their suitability for surgery, patients experiencing severe  
8 complications are likely to be candidates for full active management and escalation of care. They  
9 are therefore a population likely to benefit from continuous physiological monitoring.  
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13 There are few clinical evaluations of continuous vital signs monitoring in the literature. Previous  
14 validation studies have studied participants who are confined to their bed space by wired monitoring  
15 equipment (7,10). This is not a valid approach in the surgical setting, where enhanced recovery  
16 programmes mandate early mobilisation after surgery. In this study, patients were allowed to  
17 ambulate freely as part of their usual postoperative care.  
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20 The findings must be interpreted within the limitations of the study. There were a relatively small  
21 number of patients in the study. Data completeness was low, especially for respiratory rate,  
22 although the data completeness for heart rate and temperature were similar to previous work (10).  
23 The reference standard, whilst clinically relevant, is inherently flawed. Early warning scores such as  
24 NEWS are known to be limited by their user-dependent nature. In addition, manually-collected vital  
25 signs can be subject to the effects of 'white-coat hypertension'; heart rate, respiratory rate and  
26 temperature can be elevated simply by the arousal effect of the nurse interaction.  
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30 Deficits in the manually-recorded observations were particularly evident in the analysis of  
31 respiratory rate. Analysis of the manually-recorded values alone revealed a statistically unlikely  
32 preponderance of 18 breaths per minute, with a secondary peak at 16 breaths per minute. This  
33 casts doubt on the reliability of these manual measurements. It has been well described that  
34 respiratory rate is often miscalculated or omitted when calculated early warning scores (15,16). It is  
35 also recognised that clinical staff detect patient status in advance of manual measurements for an  
36 early warning score system 'by using information not currently encoded within it.'  
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39 The patch data for respiratory rate is also unlikely to be reliable, as a significant proportion of  
40 measurements were between 5 and 10 breaths per minute. This proportion of low values is much  
41 greater than those described in previously derived distributions from larger populations (17). There  
42 are also rapid fluctuations in respiratory rate which are physiologically implausible and may have  
43 been affected by patient movement, speech or coughing.  
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46 The manually-recorded temperature measurements showed plausible distributions and are likely to  
47 be accurate. The low correlation between the nurse-measured temperatures and the patch data can  
48 be explained by the difference in measurement techniques. The patch measures skin temperature  
49 which may not accurately reflect the tympanic temperature measured by the nursing staff. Skin  
50 temperature is highly dependent on environmental factors such as the ambient temperature,  
51 clothing and blankets.  
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54 The reliability of the continuous temperature measurement is, however, limited. The time series  
55 analysis shows evidence of regular patch disconnection, indicated by rapid drops in temperature  
56 followed by increases consistent with conductive heating, or warming back up. These warm-up  
57 periods render the raw signals unreliable, although this limitation may be overcome through better  
58 signal processing. For instance, Clifton et al. used Bayesian change point analysis to detect step  
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3 changes in temperature across a large study population. A similar approach may be used to  
4 determine disconnection on an individual patient basis(18).  
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## 7 8 Conclusions

9 The SensiumVitals® monitoring system is capable of reliably measuring heart rate, and correlates  
10 well with manually-recorded heart rate. The accuracy of respiratory rate and temperature was  
11 outside of acceptable limits. Limitations of the remote monitoring system could potentially be  
12 overcome through better signal processing. Inaccuracies in manually-recorded data present an  
13 opportunity to increase awareness amongst nursing staff about the importance of manual  
14 observations.  
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## 20 21 Figure legends

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24 Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium,  
25 Abingdon, UK.  
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28 Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign  
29 values from the SensiumVitals® patch. The black markers show the median value of the  
30 SensiumVitals® vital signs (evaluated from +-10 mins of the nurse observation time). The red  
31 markers show the manually-recorded vital signs. Where there is a wide difference between the red  
32 and black markers at a single time point, this indicates disagreement between the two vital signs  
33 measurement techniques.  
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36 Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature  
37 observations.  
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39 Figure 4: Bland-Altman plot for temperature with limits of agreement adjusted for repeated  
40 measures.  
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43 Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate  
44 observations; rpm=respirations per minute.  
45

46 Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated  
47 measures.  
48

49 Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate  
50 observations; bpm=beats per minute.  
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53 Figure 8: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.  
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## Competing interests

There are no known conflicts of interest associated with this work and there has been no significant financial support for this work that could have influenced its outcome.

## Author contributions

CD, SN and DW were involved in the conception of the work. CD designed the study. DW provided methodological expertise. SN undertook the data collection. DW and CD performed the analysis and interpretation. CD and DW drafted the article. All authors were involved in critical revision of the article and have given final approval of the version to be submitted.

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## Data sharing statement

Research materials related to this work can be accessed on request from the corresponding author.

## References

1. Downey CL, Tahir W, Randell R, Brown JM, Jayne DG. Strengths and limitations of early warning scores: A systematic review and narrative synthesis. Vol. 76, *International Journal of Nursing Studies*. 2017. p. 106–19.
2. Cardona-Morrell M, Prgomet M, Turner RM, Nicholson M, Hillman K. Effectiveness of continuous or intermittent vital signs monitoring in preventing adverse events on general wards: a systematic review and meta-analysis. Vol. 70, *International Journal of Clinical Practice*. 2016. p. 806–24.
3. DeVita MA, Smith GB, Adam SK, Adams-Pizarro I, Buist M, Bellomo R, et al. Identifying the hospitalised patient in crisis. A consensus conference on the afferent limb of Rapid Response Systems. *Resuscitation*. 2010;81(4):375–82.
4. Bonnici T, Tarassenko L, Clifton D, Watkinson P. The digital patient. *Clin Med (Northfield Ill)*. 2013;13(3):252–7.
5. Michard F. A sneak peek into digital innovations and wearable sensors for cardiac monitoring. *J Clin Monit Comput*. 2017 Apr;31(2):253–9.
6. Hofmann B, Welch H. New diagnostic tests: more harm than good. *Br Med J*. 2017;358:j3314.
7. Hernandez-Silveira M, Ahmed K, Ang S-S, Zandari F, Mehta T, Weir R, et al. Assessment of the feasibility of an ultra-low power, wireless digital patch for the continuous ambulatory monitoring of vital signs. *BMJ Open*. 2015;5(5).
8. Downey CL, Croft J, Buckley H, Randell R, Brown JM, Jayne DG. Trial of Remote Continuous versus Intermittent NEWS monitoring after major surgery (TRaCINg): protocol for a feasibility randomised controlled trial. *Pilot Feasibility Stud*. 2018;4(1):112.
9. Royal College of Physicians. National Early Warning Score (NEWS) 2: Standardising the assessment of acute-illness severity in the NHS. Updated report of a working party. 2017.
10. Breteler MJM, Huizinga E, van Loon K, Leenen LPH, Dohmen DAJ, Kalkman CJ, et al. Reliability of wireless monitoring using a wearable patch sensor in high-risk surgical patients at a step-down unit in the Netherlands: a clinical validation study. *BMJ Open [Internet]*. 2018 Feb 1;8(2). Available from: <http://bmjopen.bmj.com/content/8/2/e020162.abstract>
11. Niven D, Gaudet J, Laupland K, Mrklas K, Roberts D, Stelfox H. Accuracy of peripheral thermometers for estimating temperature: A systematic review and meta-analysis. *Ann Intern Med [Internet]*. 2015 Nov 17;163(10):768–77. Available from: <http://dx.doi.org/10.7326/M15-1150>
12. Carstensen B, Gurrin L, Ekstrom C, Figurski M. MethComp: functions for analysis of agreement in method comparison studies. 2015. p. R package version 1.22.2.
13. R Core Team. R: A language and environment Statistical, statistical computing. 2018. p. R Foundation Computing, Vienna, Austria.

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14. The International Surgical Outcomes Study Group. Global patient outcomes after elective surgery: prospective cohort study in 27 low-, middle-, and high-income countries. *Br J Anaesth*. 2016;117:601–9.
15. Nwulu U, Westwood D, Edwards D, Kelliher F, Coleman J. Adoption of an electronic observation chart with an integrated early warning scoring system on pilot wards: a descriptive report. *Comput Informatics, Nurs*. 2012;30(7):371–9.
16. Ludikhuize J, Smorenburg S, de Rooij S, de Jonge E. Identification of deteriorating patients on general wards; measurement of vital parameters and potential effectiveness of the Modified Early Warning Score. *J Crit Care*. 2012;27(4):424.e7-13.
17. Tarassenko L, Clifton DA, Pinsky MR, Hravnak MT, Woods JR, Watkinson PJ. Centile-based early warning scores derived from statistical distributions of vital signs. *Resuscitation* [Internet]. 2011;82(8):1013–8. Available from: <http://www.sciencedirect.com/science/article/pii/S030095721100195X>
18. Clifton DA, Wong D, Clifton L, Wilson S, Way R, Pullinger R, et al. A Large-Scale Clinical Validation of an Integrated Monitoring System in the Emergency Department. *IEEE J Biomed Heal Informatics*. 2013;17(4):835–42.

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Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium, Abingdon, UK.

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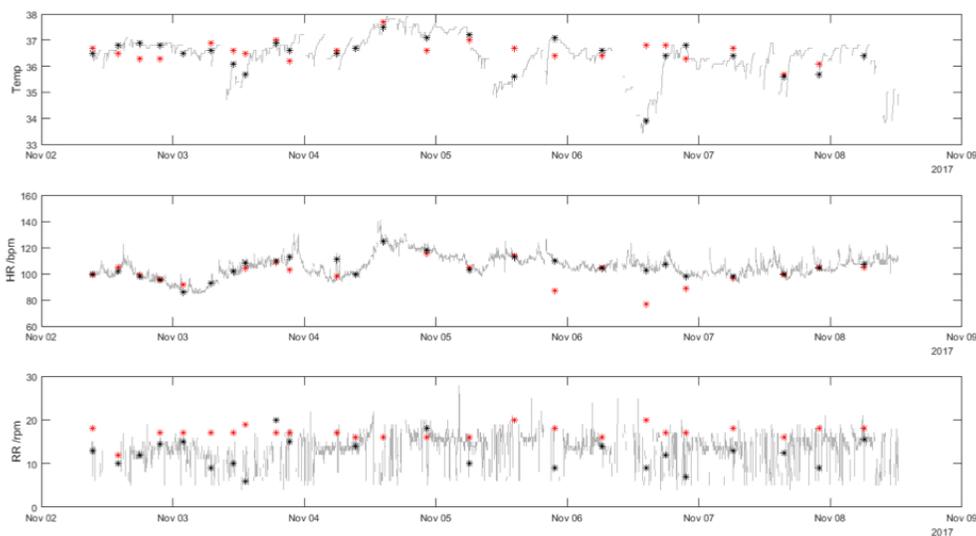


Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign values from the SensiumVitals® patch. The black markers show the median value of the SensiumVitals® vital signs (evaluated from +/-10 mins of the nurse observation time). The red markers show the manually-recorded vital signs. Where there is a wide difference between the red and black markers at a single time point, this indicates disagreement between the two vital signs measurement techniques.

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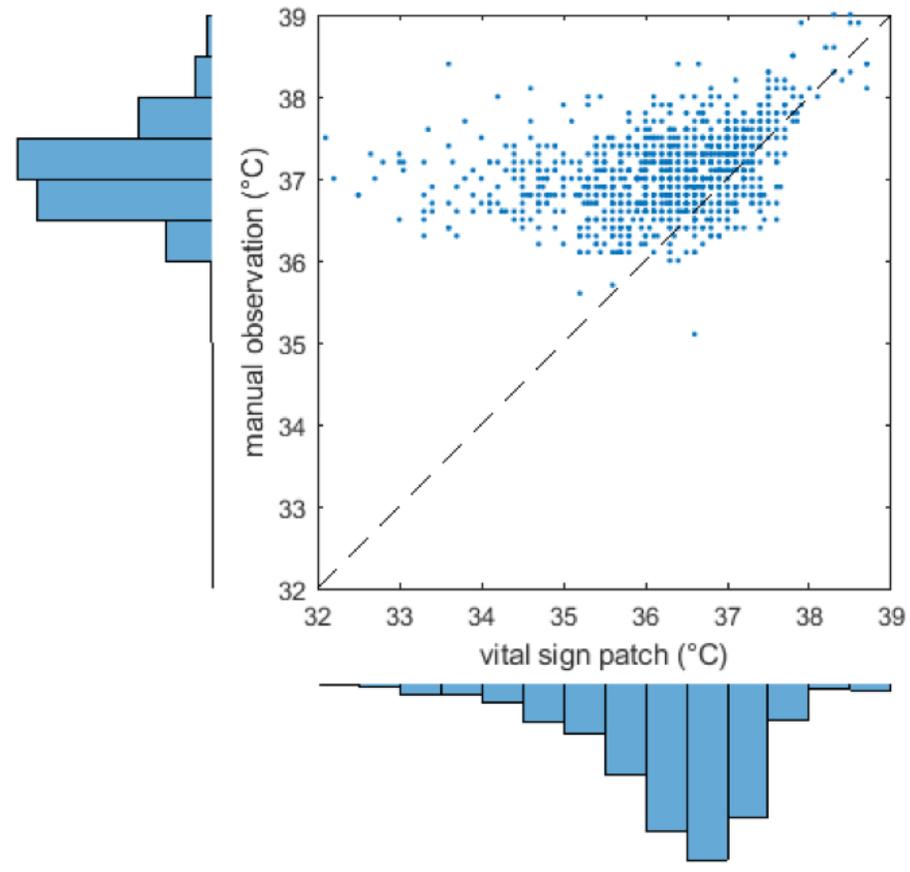


Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature observations.

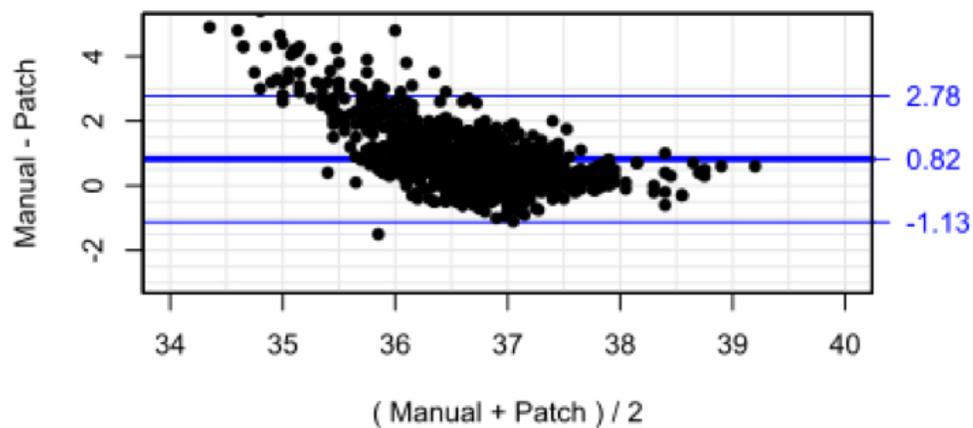


Figure 4: Bland-Altman plot for temperature with limits of agreement adjusted for repeated measures.

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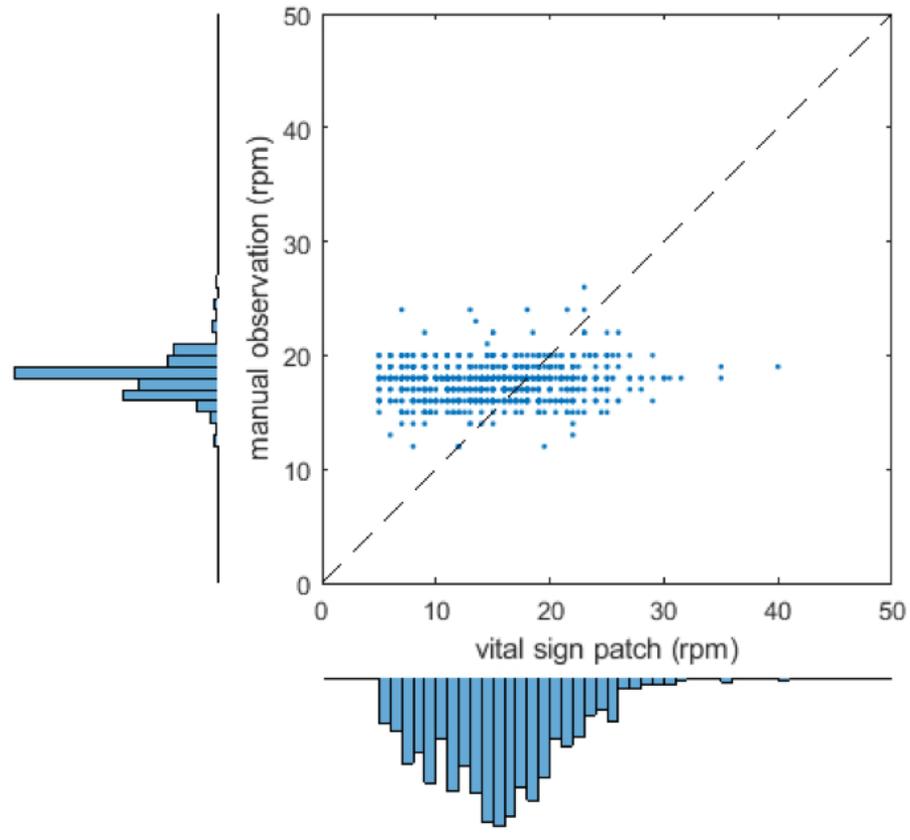


Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate observations; rpm=respirations per minute.

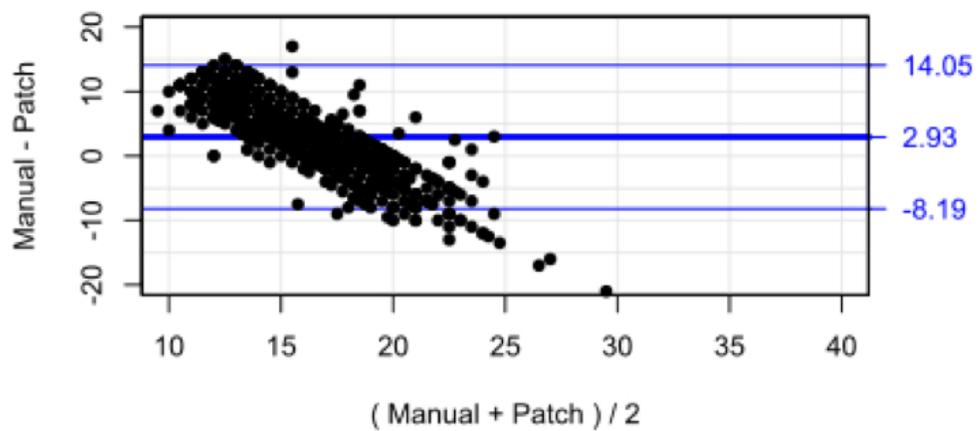


Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated measures.

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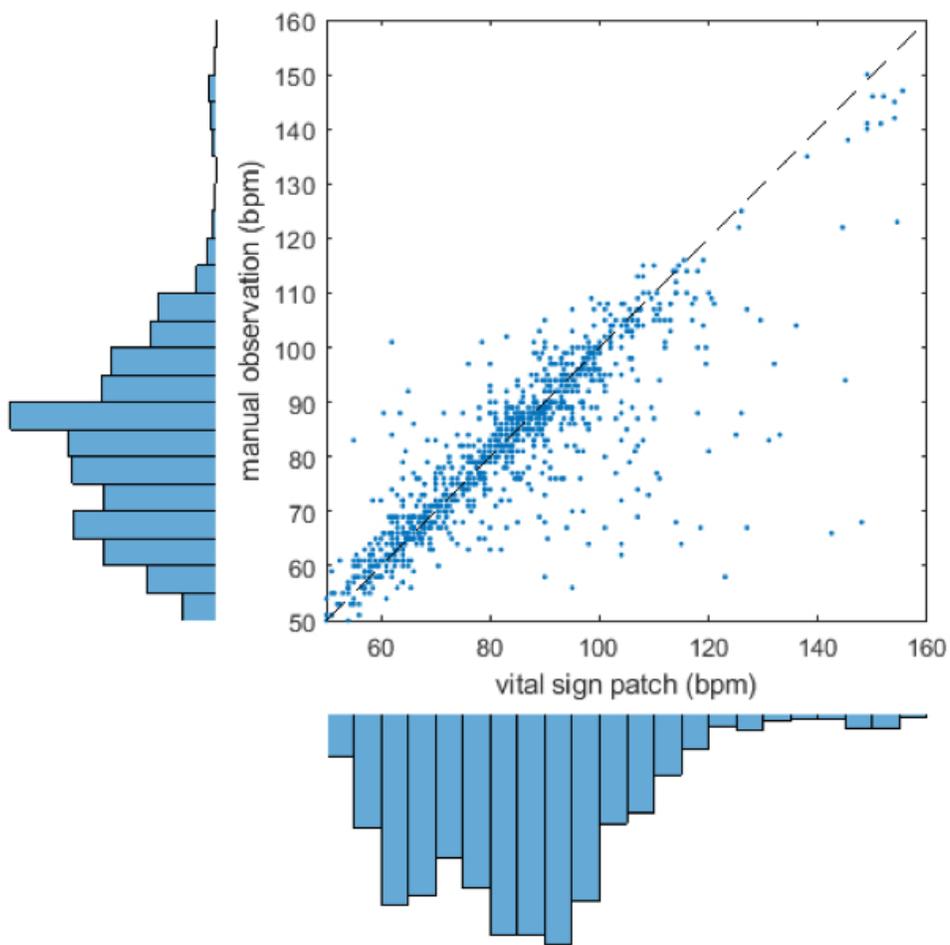


Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate observations; bpm=beats per minute.

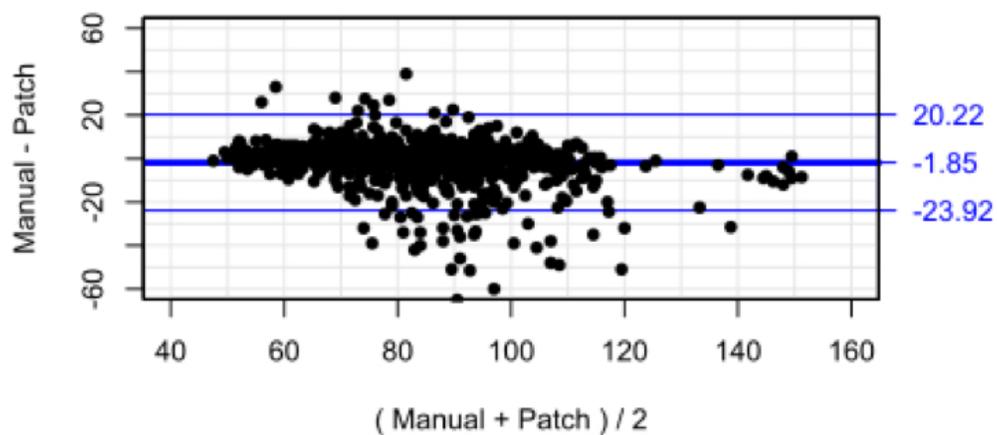


Figure 8: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.

# BMJ Open

## Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study

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# Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study

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Keywords: Remote monitoring, vital signs, continuous, reliability, validation

## Abstract

### Objective

To validate whether a wearable remote vital signs monitor could accurately measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk of complications.

### Design

Manually-recorded vital signs data were paired with vital signs data derived from the remote monitor set in patients participating in a trial of continuous remote vital signs monitoring.

### Setting

St James's University Hospital, United Kingdom.

### Participants

51 patients who had undergone major elective general surgery.

### Interventions

The intervention was the SensiumVitals® monitoring system. This is a wireless patch worn on the patient's chest that measures heart rate, respiratory rate and temperature continuously. The reference standard was nurse-measured manually-recorded vital signs.

### Primary and secondary outcome measures

The primary outcomes were the 95% limits of agreement between manually-recorded and wearable patch vital sign recordings of heart rate, respiratory rate and temperature. The secondary outcomes were the percentage completeness of vital sign patch data for each vital sign.

### Results

1,135 nurse observations were available for analysis. There was no clinically meaningful bias in heart rate (1.85 bpm), but precision was poor (95% limits of agreement -23.92 to 20.22 bpm). Agreement was poor for respiratory rate (bias 2.93 breaths per minute, 95% limits of agreement -8.19 to 14.05 breaths per minute) and temperature (bias 0.82 °C, 95% limits of agreement -1.13 °C to 2.78 °C). Vital sign patch data completeness was 72.8% for temperature, 59.2% for heart rate and 34.1% for respiratory rate. Distributions of respiratory rate in manually-recorded measurements were clinically implausible.

### Conclusions

The continuous monitoring system did not reliably provide heart rate consistent with nurse measurements. The accuracy of respiratory rate and temperature was outside of acceptable limits. Limitations of the system could potentially be overcome through better signal processing. Whilst

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3 acknowledging the time pressures placed on nursing staff, inaccuracies in the manually-recorded  
4 data present an opportunity to increase awareness about the importance of manual observations,  
5 particularly with regard to methods of manual heart rate and respiratory rate measurements.  
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## 12 Article Summary: Strengths and limitations of this study

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- 16 • Surgical patients are a population likely to benefit from continuous physiological monitoring.
- 17 • A large number of paired data sets were available for comparison.
- 18 • The reference standard is a clinically relevant comparison, and is standard of care
- 19 throughout the UK.
- 20 • The accuracy of the reference standard is user-dependent.
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# 1. Introduction

Physiological monitoring using early warning score systems is effective but limited by its intermittent nature (1). It is hypothesised that continuous vital signs monitoring may allow earlier detection of patient deterioration and thereby improve patient outcomes, but existing evidence is limited (2). A consensus of international experts in safety and healthcare technology concluded that, if technically possible and affordable, all patients who are for active treatment should be continuously monitored (3).

Until recently, continuous vital signs monitoring was limited to critical care areas because it required high staff-to-patient ratios and cumbersome equipment which tethered the patient to the bed-space, thereby inhibiting patient mobility and recovery. When hard-wired monitoring was implemented on a general ward, only 16% of patients remained connected in a 72-hour period (4).

New remote monitoring devices, consisting of wearable sensors and aided by wireless data transmission, allow the patient to ambulate freely whilst enjoying the presumed advantages of extra monitoring. Since 2002, a number of such tools have received the United States Food and Drug Administration (FDA) clearance, indicating that they are safe and effective, but clinical studies are required to demonstrate their utility in the inpatient setting (5,6).

A remote monitoring device with a considerable amount of clinical evidence is the SensiumVitals® patch (Figure 1)(7–10). Attached to the patient's chest with two ECG electrodes, the device monitors heart rate, respiratory rate and skin temperature continuously. The data are transmitted wirelessly every two minutes to a central monitoring station or a mobile device carried by the patient's nurse. This alerts the healthcare worker when there is deviation from pre-set physiological norms, alerting staff to potential patient deterioration.

The patch records respiratory rate by means of impedance pneumography and heart rate through single-lead ECG activity. Temperature is measured by a temperature-sensitive resistor. Once a physiological signal is fully acquired, it is processed by its associated embedded algorithm running inside the in-built processing unit, which enables the transmission of the resultant values to a nearby intranet hot-spot for onward transmission to the central monitoring system.

The underlying technology incorporated into such devices is well understood, but there is limited evidence for its reliability in the clinical setting. One previous study exists which validated the accuracy of the SensiumVitals® system in 61 hospital patients. The patients were monitored at rest for a maximum of two hours, and the device was tested against a conventional bedside clinical monitor using capnographic respiratory rate (11). This does not reflect the true clinical environment, which challenges such devices to provide monitoring continuity over several days in ambulatory patients.

In this study, we validated the accuracy of the SensiumVitals® system to measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk for complications. The reference standard were manually-recorded vital signs as part of the National Early Warning Score (NEWS). The objective of this study was to assess whether the wireless patch system is able

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3 to reliably measure vital signs continuously in the clinical setting, and to determine how well it  
4 compares to manually-recorded measurements.  
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## 9 2. Methods

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11 Ethical approval was granted on 10th October 2017 by the Yorkshire & The Humber – Leeds West  
12 Research Ethics Committee, ref: 17/YH/0180. Informed consent to participate was obtained from all  
13 participants in the study.  
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### 16 2.1 Study design

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18 All participants were enrolled in the TRaCINg study, the protocol for which has been published  
19 previously (12). This was a single-centre, feasibility, randomised, controlled, parallel group trial of  
20 continuous remote vital signs monitoring for patients who had undergone major elective general  
21 surgery at St James's University Hospital, Leeds, United Kingdom. Participants were individually  
22 randomised on a 1:1 basis to receive either remote monitoring plus NEWS or monitoring by NEWS  
23 alone. This paper describes the data from participants randomised to the remote monitoring arm,  
24 who wore the SensiumVitals® patch during their hospital admission. The TRaCINg study is listed on  
25 the ISRCTN registry with study ID ISRCTN16601772 (<http://www.isrctn.com/ISRCTN16601772>).  
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### 29 2.2 Patient and public involvement

30 Patients and the public were involved in the design of the randomised controlled trial, but were not  
31 involved in the design of this validation study.  
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### 34 2.3 Data collection

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36 Vital signs data was collected for each participant from two sources. The SensiumVitals® vital sign  
37 data were documented at 2-minute intervals and collected from a hospital desktop computer using  
38 data-acquisition software developed by Sensium. These data had been pre-processed to discard  
39 signals that were subject to gross electrical or motion artefact (11). Patients were allowed to  
40 ambulate whilst wearing the monitoring patch; however, due to the major surgery they had  
41 undergone, most patients remained at their bedsides for the duration of their hospital stay.  
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44 NEWS data were collected at regular intervals, depending on the patients' status and based on the  
45 NEWS protocol(13). Typically, vital signs were collected at the bedside, with the patients either  
46 sitting or lying down, by members of the nursing staff who were blinded to the SensiumVitals® vital  
47 sign data: pulse rate was measured using the pulse oximeter on a multi-parameter portable vital  
48 signs monitor; temperature was measured using a tympanic thermometer; respiratory rate was  
49 measured manually. The NEWS scores and their component parts were documented electronically.  
50 Researchers collected manually-recorded heart rate, respiratory rate and temperature data from the  
51 hospital's electronic patient record. Other vital signs collected by the nursing staff as part of the  
52 early warning score, such as oxygen saturations, were not extracted.  
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### 57 2.4 Data processing

58 The two data sources were linked using NHS number and timestamp and consolidated into a single  
59 deidentified spreadsheet. Paired data to a NEWS observation was derived from the SensiumVitals®  
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3 continuous data set by using the median vital sign value within a  $\pm 10$ -minute window of a manually-  
4 recorded observation. The time window was used to account for differences between the nurses'  
5 manually-documented times and the automatic timestamps from the vital sign patch. The median  
6 value within this window was used to eliminate the impact of intermittent sensor noise.  
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## 9 2.5 Outcomes

11 The primary outcomes were the 95% limits of agreement between manual nurse observations and  
12 wearable vital sign patch recordings of Heart Rate (HR), Respiratory Rate (RR) and Temperature  
13 (Temp). Following precedent, we defined clinical acceptability to be *max*  $\pm 10\%$  for HR and RR (or  $\pm 3$   
14 breaths per minute or  $\pm 5$  beats per minute) and  $0.5^\circ\text{C}$  for Temp (14,15). The secondary outcome was  
15 the average percentage completeness of continuous patch data.  
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## 18 2.6 Statistical Analysis

19 For each vital sign, we first visually inspected the paired vital sign measurements via scatter plots, in  
20 addition to the raw time series vital signs from the Sensium patch.  
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23 Measurements were then formally compared using Bland-Altman analysis. In this analysis, the mean  
24 difference between the SensiumVitals® data and the nurse observations and the 95% Limits of  
25 Agreement are calculated. We adjusted for multiple measurements from the same subject using a  
26 model in which time of measurement is modelled as a random effect(16). This avoids bias caused by  
27 differences in number of measurements per patient. We also reported the Pearson correlation  
28 coefficient and the root mean squared (RMS) error for each vital sign.  
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31 In secondary analysis, we first assessed the average percentage completeness of the continuous  
32 patch data per patient. The numerator was defined as the number of two-minute periods in which  
33 vital sign data were provided by the patch. The denominator was the number of 2-minute periods  
34 that span the time during which the patch was transmitting data. These time points were preferred  
35 to admission and discharge from ward times because the patch may not have been worn for the  
36 patient's entire ward admission. In sensitivity analyses, we repeated both the Bland-Altman  
37 analyses using  $\pm 2$  and  $\pm 2$  minute windows of continuous data.  
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40 Analyses were undertaken using MATLAB R2017b (The MathWorks Inc., Massachusetts, USA) and  
41 the R Methcomp package (17,18).  
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## 48 3. Results

49 Fifty one patients were recruited to the intervention arm of the TRaCINg study between October  
50 2017 and April 2018. The median number of manually-recorded observation sets was 19 per patient  
51 (range 2 to 73 sets of vital signs measurements). There were 1,135 nurse observations available for  
52 analysis. All observations had a documented heart rate. Four observations had missing  
53 observations, 1 for respiratory rate and 3 for temperature. Vital sign traces for one participant over  
54 the course of their entire hospital stay are shown in Figure 2.  
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### 3.1 Heart Rate

Figure 3 shows the scatterplot of nurse-recorded heart rate against the SensiumVitals® patch. There is reasonable correlation between the two measurements ( $R^2 = 0.67$ ,  $p < 0.001$ ). The mean and (standard deviation) for manual and wearable heart rates are 81.6 (16.2) beats per minute (bpm) and 84.3 (19.3) bpm, respectively. The mean percentage completeness of continuous patch data for heart rate was 59.2%. In addition, visual inspection of the example vital sign traces show good agreement between the measurements. The Bland-Altman bias (Figure 4) was 1.85 bpm, with 95% limits of agreement -23.92 to 20.22 bpm. The RMS error was 11.25 bpm. The limits of agreement and RMS error exceeded the acceptability criterion.

### 3.2 Respiratory Rate

Figure 5 shows the scatterplot of nurse-recorded respiratory rate against the SensiumVitals® patch data. There is no correlation between the two measurements methods ( $R^2 = 0.01$ ,  $p < 0.001$ ). The mean and standard deviation for manual and wearable respiratory rate were 17.6 (1.58) breaths per minute and 15.0 (5.5) breaths per minute, respectively. The mean percentage completeness of continuous patch data for respiratory rate data was 31.4%.

Visual inspection of the histogram for manually-recorded respiratory rate shows a large peak at 18 breaths per minute, and a secondary peak at 16 breaths per minute. This result is unexpected for a natural physiological parameter, which may be expected to vary smoothly over the full range of values. Indeed, the peaks do not appear on the vital sign patch histogram. Inspection of the vital sign patch histogram indicates a significant proportion of measurements between 5 and 10 breaths per minute. No manually-recorded respiratory rates were recorded in this range. The Bland-Altman bias (Figure 6) was 2.93 breaths per minute, with 95% limits of agreement -8.19 to 14.05 breaths per minute. The RMS error was 6.14 breaths per minute and the limits of agreement are wider than the pre-specified acceptable error of 3 breaths/min.

### 3.3 Temperature

Figure 7 is a scatterplot of temperatures recorded by nurses versus those measured by the SensiumVitals® patch. Histograms for each measurement method are presented alongside the x- and y- axes. There is low correlation between the two measurement methods ( $R^2 = 0.13$ ,  $p < 0.001$ ). The mean and (standard deviation) of manual temperature and wearable temperature were 37.1°C (0.5°C) and 36.4°C (1.0°C). Further inspection of the vital sign time series in Figures 1 and 2 shows multiple clinically implausible fluctuations of up to 2 °C within 2 hours within each time series. The mean percentage completeness of continuous patch data for temperature was 72.8%.

Initial visual inspection was therefore sufficient to show that the patch-derived temperature is not a suitable proxy for core temperature, as measured by tympanic thermometer. The Bland-Altman bias (Figure 8) was 0.82 °C, with 95% limits of agreement -1.13 °C to 2.78 °C. The RMS error was 1.28 °C. In addition to large systematic bias between the two methods, the limits of agreement did not meet the pre-defined clinical acceptability criterion (0.5°C).

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3 In a sensitivity analysis, all Bland-Altman analyses was repeated using  $\pm 2$  and  $\pm 5$  minute windows of  
4 vital sign patch data. There were no meaningful differences in the bias or limits of agreement  
5 [Supplementary Material].  
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## 12 4. Discussion

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14 In this 51-patient validation study, temperature, respiratory rate, and heart rate measurements  
15 obtained from a wearable vital sign patch were compared with manually-recorded observations by  
16 nursing staff. Whilst there was reasonable correlation between the two methods for heart rate  
17 measurements ( $R^2 = 0.67$ ) there were large discrepancies in many instances, as indicated by the  
18 Bland Altman analysis (bias 1.85 bpm, 95% limits of agreement -23.92 to 20.22 bpm). It is not clear  
19 whether there were errors in the manual observation, in the vital sign patch, or both.  
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23 There was low correlation for respiratory rate ( $R^2 = 0.01$ )(Bland-Altman bias 2.93 breaths per  
24 minute, 95% limits of agreement -8.19 to 14.05 breaths per minute) and temperature ( $R^2 =$   
25 0.13)(Bland-Altman bias 0.82 °C, 95% limits of agreement -1.13 °C to 2.78 °C). The differences  
26 between manual and vital sign patch measurements for all three measured vital signs were outside  
27 of acceptable limits. The average completeness of data were 72.8% for temperature, 59.2% for heart  
28 rate and 34.1% for respiratory rate.  
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31 An advantage of the study design is the collection of a large number of data points for analysis. The  
32 approach is clinically valid, as the NEWS system is the national standard for vital signs monitoring in  
33 the United Kingdom. The surgical patient population is a clinically relevant cohort. There are high  
34 rates of complications after major surgery (19), but many surgical complications, such as sepsis, are  
35 attenuated by early detection. By virtue of their suitability for surgery, patients experiencing severe  
36 complications are likely to be candidates for full active management and escalation of care. They  
37 are therefore a population likely to benefit from reliable continuous physiological monitoring.  
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41 There are few clinical evaluations of continuous vital signs monitoring in the literature. Previous  
42 validation studies have studied participants who are confined to their bed space by wired monitoring  
43 equipment (11,14). In the surgical setting, enhanced recovery programmes mandate early  
44 mobilisation after surgery. In this study, patients were allowed to ambulate freely as part of their  
45 usual postoperative care, which may have produced some motion artefact on the continuous  
46 monitoring data; this may explain why the findings from this study show worse correlation when  
47 compared to previous studies which compared two stationary measurements. The patch algorithms  
48 are designed to identify and reject physiological signals corrupted by significant sources of noise  
49 inherent to the ambulatory nature of wireless monitoring; however, it is possible that respiratory  
50 rate data may have shown artefact from speech.  
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55 The findings must be interpreted within the limitations of the study. There were a relatively small  
56 number of patients in the study. Data completeness from the vital sign patch was low, especially for  
57 respiratory rate, although results for heart rate and temperature were similar to previous work (14).  
58 The reference standard, whilst clinically relevant, is inherently flawed. Early warning scores such as  
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NEWS are known to be limited by their user-dependent nature. Time and staffing pressures placed on nursing staff in an increasingly busy clinical environment may be driving the adoption of time-saving, less accurate techniques; in this study, heart rate was typically inferred from the pulse rate measured by a pulse oximeter, despite the fact that this is known to be less accurate than manual palpation of the radial pulse. In addition, manually-collected vital signs can be subject to the effects of 'white-coat hypertension'; heart rate, respiratory rate and temperature can be elevated simply by the arousal effect of the nurse interaction (20).

Deficits in the manually-recorded observations were particularly evident in the analysis of respiratory rate. Analysis of the manually-recorded values alone revealed a statistically unlikely preponderance of 18 breaths per minute, with a secondary peak at 16 breaths per minute. These peaks were not visible for the vital sign patch, suggesting that this is a measurement artefact in the way that manual measurements are made, rather than a real effect. It has been well described that respiratory rate is often miscalculated or omitted when calculated early warning scores (21,22). It is also recognised that clinical staff detect patient status in advance of manual measurements for an early warning score system 'by using information not currently encoded within it.'

The patch data for respiratory rate is also unlikely to be reliable, as a significant proportion of measurements were between 5 and 10 breaths per minute. This proportion of low values is much greater than those described in previously derived distributions from larger populations (23). There are also rapid fluctuations in respiratory rate which are physiologically implausible and may have been affected by patient movement, speech or coughing.

The manually-recorded temperature measurements showed plausible distributions and are likely to be accurate. The high bias between the nurse-measured temperatures and the patch data can be explained by the difference in measurement techniques. The patch measures skin temperature which may not accurately reflect the tympanic temperature measured by the nursing staff. Skin temperature is highly dependent on environmental factors such as the ambient temperature, clothing and blankets.

The reliability of the continuous temperature measurement is, however, limited. The time series analysis shows evidence of regular patch disconnection, indicated by rapid drops in temperature followed by increases consistent with conductive heating, or warming back up. These warm-up periods render the raw signals unreliable, although this limitation may be overcome through better signal processing. For instance, Clifton et al. used Bayesian change point analysis to detect step changes in temperature across a large study population. A similar approach may be used to determine disconnection on an individual patient basis(24).

## Conclusions

The differences between manual and vital sign patch measurements for all three measured vital signs were outside of acceptable limits. On some occasions, this may be due to artefact in the continuous signal; this could be overcome through better signal processing. Other discrepancies may be due to errors during manual measurement. Whilst acknowledging the time pressures placed on nursing staff, inaccuracies in the manually-recorded data present an opportunity to increase awareness about the importance of manual observations, particularly with regard to methods of manual heart rate and respiratory rate measurements.

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For peer review only

## Figure legends

Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium, Abingdon, UK.

Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign values from the SensiumVitals® patch. The black markers show the median value of the SensiumVitals® vital signs (evaluated from  $\pm 10$  mins of the nurse observation time). The red markers show the manually-recorded vital signs. Where there is a wide difference between the red and black markers at a single time point, this indicates disagreement between the two vital signs measurement techniques.

Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate observations; bpm=beats per minute.

Figure 4: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.

Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate observations; rpm=respirations per minute.

Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated measures.

Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature observations.

Figure 8: Bland-Altman plot for temperature with limits of agreement adjusted for repeated measures.

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## Competing interests

There are no known conflicts of interest associated with this work and there has been no significant financial support for this work that could have influenced its outcome.

## Author contributions

CD, SN and DW were involved in the conception of the work. CD designed the study. DW provided methodological expertise. SN undertook the data collection. DW and CD performed the analysis and interpretation. CD and DW drafted the article. CD, SN, DW and DJ were involved in critical revision of the article and have given final approval of the version to be submitted.

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## Data sharing statement

Research materials related to this work can be accessed on request from the corresponding author.

## References

1. Downey CL, Tahir W, Randell R, Brown JM, Jayne DG. Strengths and limitations of early warning scores: A systematic review and narrative synthesis. Vol. 76, *International Journal of Nursing Studies*. 2017. p. 106–19.
2. Cardona-Morrell M, Prgomet M, Turner RM, Nicholson M, Hillman K. Effectiveness of continuous or intermittent vital signs monitoring in preventing adverse events on general wards: a systematic review and meta-analysis. Vol. 70, *International Journal of Clinical Practice*. 2016. p. 806–24.
3. DeVita MA, Smith GB, Adam SK, Adams-Pizarro I, Buist M, Bellomo R, et al. Identifying the hospitalised patient in crisis. A consensus conference on the afferent limb of Rapid Response Systems. *Resuscitation*. 2010;81(4):375–82.
4. Bonnici T, Tarassenko L, Clifton D, Watkinson P. The digital patient. *Clin Med (Northfield Ill)*. 2013;13(3):252–7.
5. Michard F. A sneak peek into digital innovations and wearable sensors for cardiac monitoring. *J Clin Monit Comput*. 2017 Apr;31(2):253–9.
6. Hofmann B, Welch H. New diagnostic tests: more harm than good. *Br Med J*. 2017;358:j3314.
7. Downey C, Randell R, Brown J, Jayne DG. Continuous Versus Intermittent Vital Signs Monitoring Using a Wearable, Wireless Patch in Patients Admitted to Surgical Wards: Pilot Cluster Randomized Controlled Trial. *J Med Internet Res [Internet]*. 2018 Dec 11;20(12):e10802. Available from: <https://www.jmir.org/2018/12/e10802/>
8. Downey CL, Brown JM, Jayne DG, Randell R. Patient attitudes towards remote continuous vital signs monitoring on general surgery wards: An interview study. *Int J Med Inform*. 2018;114.
9. Hernandez-Silveira M, Wiczorkowski-Rettinger K, Ang S, Burdett A. Preliminary assessment of the SensiumVitals®: A low-cost wireless solution for patient surveillance in the general wards. *Proc Annu Int Conf IEEE Eng Med Biol Soc EMBS*. 2015;2015–Novem:4931–7.
10. Backed I, Evidence BY. Sensium Whitepaper - The Deteriorating Patient. :1–5.
11. Hernandez-Silveira M, Ahmed K, Ang S-S, Zandari F, Mehta T, Weir R, et al. Assessment of the feasibility of an ultra-low power, wireless digital patch for the continuous ambulatory monitoring of vital signs. *BMJ Open*. 2015;5(5).
12. Downey CL, Croft J, Buckley H, Randell R, Brown JM, Jayne DG. Trial of Remote Continuous versus Intermittent NEWS monitoring after major surgery (TRaCINg): protocol for a feasibility randomised controlled trial. *Pilot Feasibility Stud*. 2018;4(1):112.
13. Royal College of Physicians. National Early Warning Score (NEWS) 2: Standardising the assessment of acute-illness severity in the NHS. Updated report of a working party. 2017.
14. Breteler MJM, Huizinga E, van Loon K, Leenen LPH, Dohmen DAJ, Kalkman CJ, et al. Reliability of wireless monitoring using a wearable patch sensor in high-risk surgical patients at a step-down unit in the Netherlands: a clinical validation study. *BMJ Open [Internet]*. 2018 Feb 1;8(2). Available from: <http://bmjopen.bmj.com/content/8/2/e020162.abstract>
15. Niven D, Gaudet J, Laupland K, Mrklas K, Roberts D, Stelfox H. Accuracy of peripheral

- 1  
2  
3 thermometers for estimating temperature: A systematic review and meta-analysis. *Ann*  
4 *Intern Med* [Internet]. 2015 Nov 17;163(10):768–77. Available from:  
5 <http://dx.doi.org/10.7326/M15-1150>  
6
- 7 16. Carstensen B, Simpson J, Gurrin LC. Statistical models for assessing agreement in method  
8 comparison studies with replicate measurements. *Int J Biostat*. 2008;4(1).  
9
- 10 17. Carstensen B, Gurrin L, Ekstrom C, Figurski M. MethComp: functions for analysis of  
11 agreement in method comparison studies. 2015. p. R package version 1.22.2.  
12
- 13 18. R Core Team. R: A language and environment Statistical, statistical computing. 2018. p. R  
14 Foundation Computing, Vienna, Austria.  
15
- 16 19. The International Surgical Outcomes Study Group. Global patient outcomes after elective  
17 surgery: prospective cohort study in 27 low-, middle-, and high-income countries. *Br J*  
18 *Anaesth*. 2016;117:601–9.  
19
- 20 20. Franklin SS, Thijs L, Hansen TW, O'Brien E, Staessen JA. White-coat hypertension: new insights  
21 from recent studies. *Hypertension*. 2013;62(6):982–7.  
22
- 23 21. Nwulu U, Westwood D, Edwards D, Kelliher F, Coleman J. Adoption of an electronic  
24 observation chart with an integrated early warning scoring system on pilot wards: a  
25 descriptive report. *Comput Informatics, Nurs*. 2012;30(7):371–9.  
26
- 27 22. Ludikhuizen J, Smorenburg S, de Rooij S, de Jonge E. Identification of deteriorating patients on  
28 general wards; measurement of vital parameters and potential effectiveness of the Modified  
29 Early Warning Score. *J Crit Care*. 2012;27(4):424.e7-13.  
30
- 31 23. Tarassenko L, Clifton DA, Pinsky MR, Hravnak MT, Woods JR, Watkinson PJ. Centile-based  
32 early warning scores derived from statistical distributions of vital signs. *Resuscitation*  
33 [Internet]. 2011;82(8):1013–8. Available from:  
34 <http://www.sciencedirect.com/science/article/pii/S030095721100195X>  
35
- 36 24. Clifton DA, Wong D, Clifton L, Wilson S, Way R, Pullinger R, et al. A Large-Scale Clinical  
37 Validation of an Integrated Monitoring System in the Emergency Department. *IEEE J Biomed*  
38 *Heal Informatics*. 2013;17(4):835–42.  
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Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium, Abingdon, UK.

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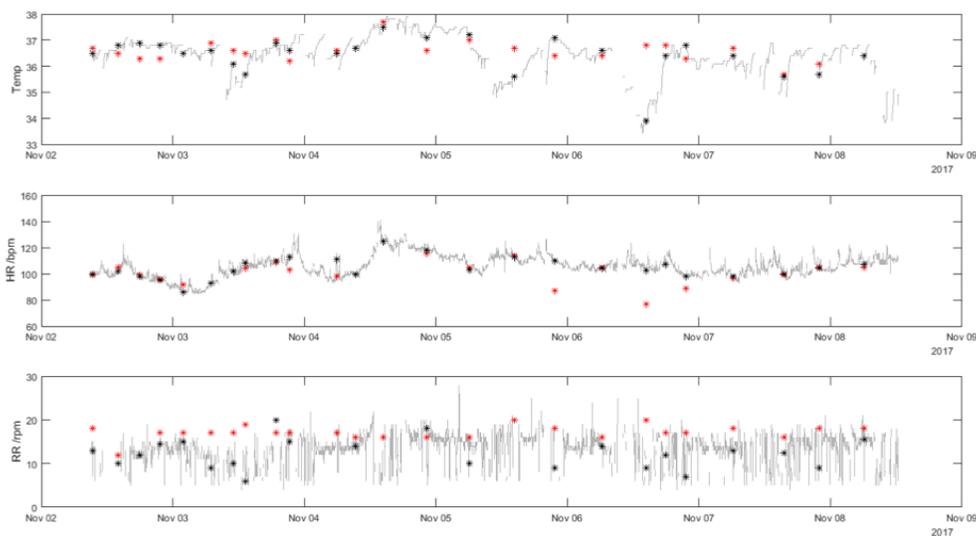


Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign values from the SensiumVitals® patch. The black markers show the median value of the SensiumVitals® vital signs (evaluated from +/-10 mins of the nurse observation time). The red markers show the manually-recorded vital signs. Where there is a wide difference between the red and black markers at a single time point, this indicates disagreement between the two vital signs measurement techniques.

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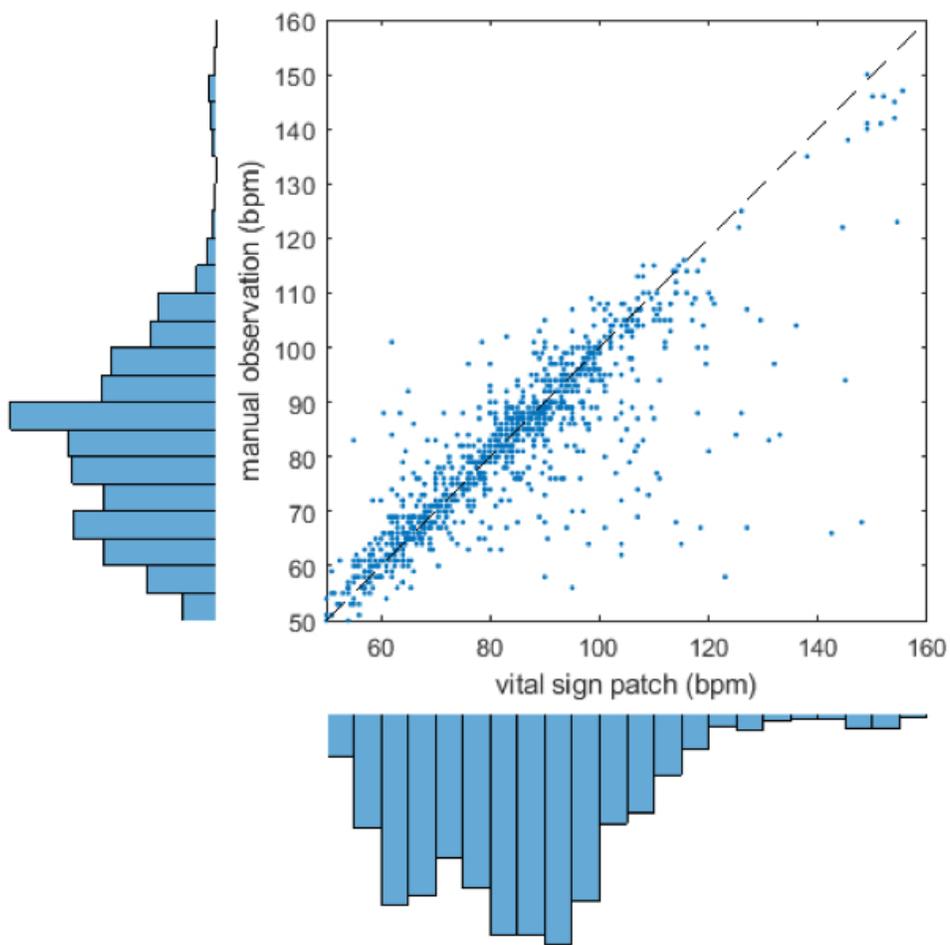


Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate observations; bpm=beats per minute.

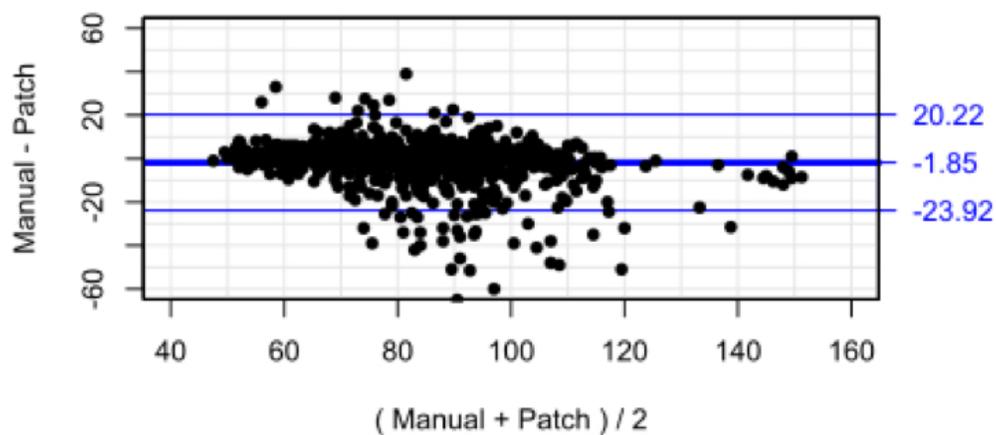


Figure 4: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.

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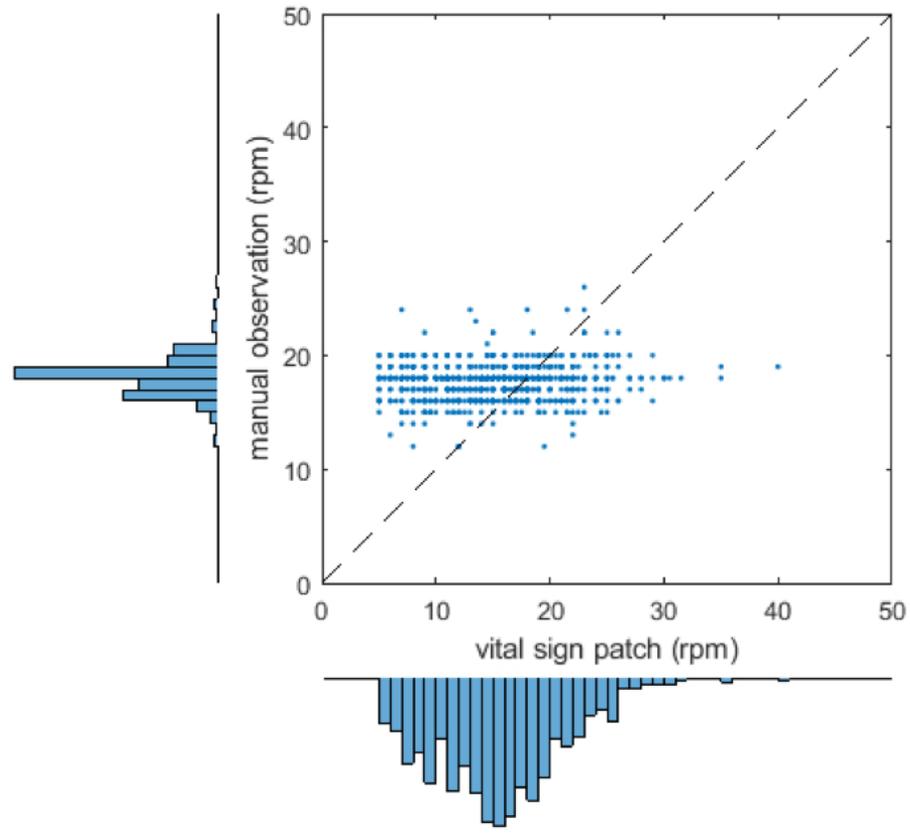


Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate observations; rpm=respirations per minute.

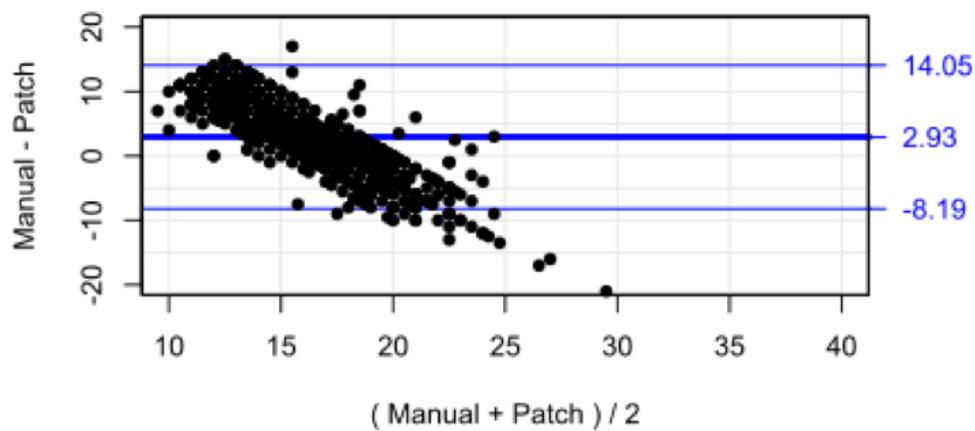


Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated measures.

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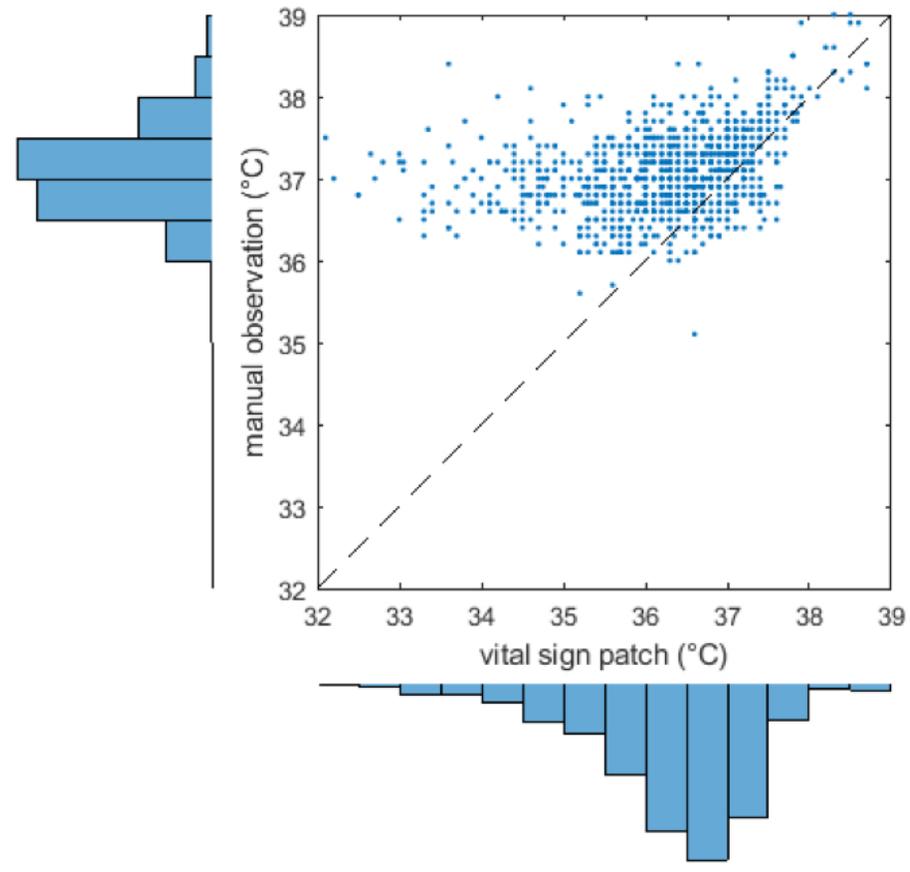


Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature observations.

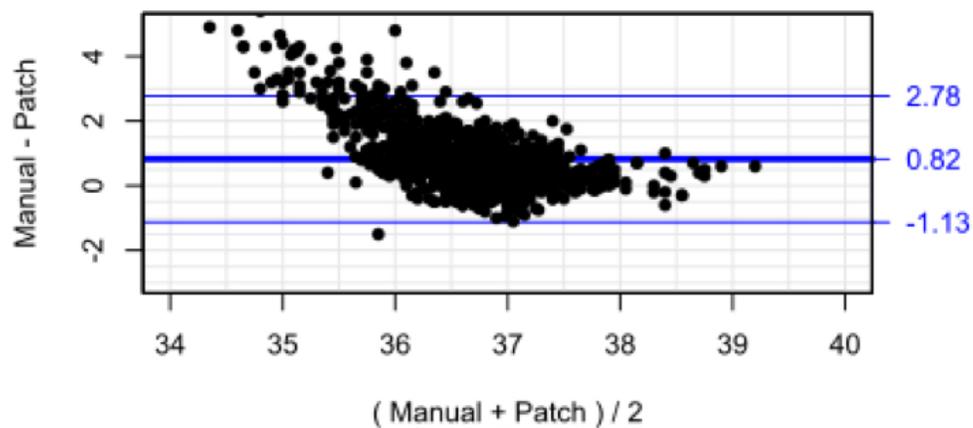


Figure 8: Bland-Altman plot for temperature with limits of agreement adjusted for repeated measures.

## Supplementary Materials

## Sensitivity analysis

Window size	HR (n = 1135)	RR (n = 1134)	Temp (n = 1132)
±2 mins	306	630	212
±5 mins	249	392	174
±10 mins	232	286	147

Missing pairs of data (i.e. no data within n minute window of nurse observation)

Window size	HR (bias, LoA)	RR (bias, LoA)	Temp (bias, LoA)
±2 mins	- 2.74 (-25.39, 19.91)	3.07 (-9.05 to 15.20)	0.82 (-1.21 to 2.86)
±5 mins	-2.35 (-24.68 to 19.98)	3.13 (-8.64 to 14.90)	0.82 (-1.23 to 2.87)
±10 mins	- 1.85 (-23.92 to 20.22)	2.93 (-8.19 to 14.05)	0.82 (-1.13 to 2.78)

Bland-Altman bias and 95% limits of agreement for ±2, ±5, ±10 window lengths of continuous vital sign patch data

# BMJ Open

## Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study from the TRaCINg trial

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<b>Primary Subject Heading</b>:	Surgery
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Keywords:	Vital Signs, continuous, monitoring, validation

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# Reliability of a wearable wireless patch for continuous remote monitoring of vital signs in patients recovering from major surgery: a clinical validation study from the TRaCINg trial

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Keywords: Remote monitoring, vital signs, continuous, reliability, validation

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For peer review only

## Abstract

### Objective

To validate whether a wearable remote vital signs monitor could accurately measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk of complications.

### Design

Manually-recorded vital signs data were paired with vital signs data derived from the remote monitor set in patients participating in the TRaCINg study: a trial of continuous remote vital signs monitoring.

### Setting

St James's University Hospital, United Kingdom.

### Participants

51 patients who had undergone major elective general surgery.

### Interventions

The intervention was the SensiumVitals® monitoring system. This is a wireless patch worn on the patient's chest that measures heart rate, respiratory rate and temperature continuously. The reference standard was nurse-measured manually-recorded vital signs.

### Primary and secondary outcome measures

The primary outcomes were the 95% limits of agreement between manually-recorded and wearable patch vital sign recordings of heart rate, respiratory rate and temperature. The secondary outcomes were the percentage completeness of vital sign patch data for each vital sign.

### Results

1,135 nurse observations were available for analysis. There was no clinically meaningful bias in heart rate (1.85 bpm), but precision was poor (95% limits of agreement -23.92 to 20.22 bpm). Agreement was poor for respiratory rate (bias 2.93 breaths per minute, 95% limits of agreement -8.19 to 14.05 breaths per minute) and temperature (bias 0.82 °C, 95% limits of agreement -1.13 °C to 2.78 °C). Vital sign patch data completeness was 72.8% for temperature, 59.2% for heart rate and 34.1% for respiratory rate. Distributions of respiratory rate in manually-recorded measurements were clinically implausible.

### Conclusions

The continuous monitoring system did not reliably provide heart rate consistent with nurse measurements. The accuracy of respiratory rate and temperature was outside of acceptable limits.

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3 Limitations of the system could potentially be overcome through better signal processing. Whilst  
4 acknowledging the time pressures placed on nursing staff, inaccuracies in the manually-recorded  
5 data present an opportunity to increase awareness about the importance of manual observations,  
6 particularly with regard to methods of manual heart rate and respiratory rate measurements.  
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## 14 Article Summary: Strengths and limitations of this study

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- 18 • Surgical patients are a population likely to benefit from continuous physiological monitoring.
  - 19 • A large number of paired data sets were available for comparison.
  - 20 • The reference standard is a clinically relevant comparison, and is standard of care
  - 21 throughout the UK.
  - 22 • The accuracy of the reference standard is user-dependent.
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# 1. Introduction

Physiological monitoring using early warning score systems is effective but limited by its intermittent nature (1). It is hypothesised that continuous vital signs monitoring may allow earlier detection of patient deterioration and thereby improve patient outcomes, but existing evidence is limited (2). A consensus of international experts in safety and healthcare technology concluded that, if technically possible and affordable, all patients who are for active treatment should be continuously monitored (3).

Until recently, continuous vital signs monitoring was limited to critical care areas because it required high staff-to-patient ratios and cumbersome equipment which tethered the patient to the bed-space, thereby inhibiting patient mobility and recovery. When hard-wired monitoring was implemented on a general ward, only 16% of patients remained connected in a 72-hour period (4).

New remote monitoring devices, consisting of wearable sensors and aided by wireless data transmission, allow the patient to ambulate freely whilst enjoying the presumed advantages of extra monitoring. Since 2002, a number of such tools have received the United States Food and Drug Administration (FDA) clearance, indicating that they are safe and effective, but clinical studies are required to demonstrate their utility in the inpatient setting (5,6).

A remote monitoring device with a considerable amount of clinical evidence is the SensiumVitals® patch (Figure 1)(7–10). Attached to the patient's chest with two ECG electrodes, the device monitors heart rate, respiratory rate and skin temperature continuously. The data are transmitted wirelessly every two minutes to a central monitoring station or a mobile device carried by the patient's nurse. This alerts the healthcare worker when there is deviation from pre-set physiological norms, alerting staff to potential patient deterioration.

The patch records respiratory rate by means of impedance pneumography and heart rate through single-lead ECG activity. Temperature is measured by a temperature-sensitive resistor. Once a physiological signal is fully acquired, it is processed by its associated embedded algorithm running inside the in-built processing unit, which enables the transmission of the resultant values to a nearby intranet hot-spot for onward transmission to the central monitoring system.

The underlying technology incorporated into such devices is well understood, but there is limited evidence for its reliability in the clinical setting. One previous study exists which validated the accuracy of the SensiumVitals® system in 61 hospital patients. The patients were monitored at rest for a maximum of two hours, and the device was tested against a conventional bedside clinical monitor using capnographic respiratory rate (11). This does not reflect the true clinical environment, which challenges such devices to provide monitoring continuity over several days in ambulatory patients.

In this study, we validated the accuracy of the SensiumVitals® system to measure heart rate, respiratory rate and temperature in a post-surgical patient population at high risk for complications. The reference standard were manually-recorded vital signs as part of the National Early Warning Score (NEWS). The objective of this study was to assess whether the wireless patch system is able

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3 to reliably measure vital signs continuously in the clinical setting, and to determine how well it  
4 compares to manually-recorded measurements.  
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## 9 2. Methods

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11 Ethical approval was granted on 10th October 2017 by the Yorkshire & The Humber – Leeds West  
12 Research Ethics Committee, ref: 17/YH/0180. Informed consent to participate was obtained from all  
13 participants in the study.  
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### 16 2.1 Study design

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18 All participants were enrolled in the TRaCINg study, the protocol for which has been published  
19 previously (12). This was a single-centre, feasibility, randomised, controlled, parallel group trial of  
20 continuous remote vital signs monitoring for patients who had undergone major elective general  
21 surgery at St James's University Hospital, Leeds, United Kingdom. Participants were individually  
22 randomised on a 1:1 basis to receive either remote monitoring plus NEWS or monitoring by NEWS  
23 alone. This paper describes the data from participants randomised to the remote monitoring arm,  
24 who wore the SensiumVitals® patch during their hospital admission. The TRaCINg study is listed on  
25 the ISRCTN registry with study ID ISRCTN16601772 (<http://www.isrctn.com/ISRCTN16601772>).  
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### 29 2.2 Patient and public involvement

30 Patients and the public were involved in the design of the randomised controlled trial, but were not  
31 involved in the design of this validation study.  
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### 34 2.3 Data collection

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36 Vital signs data was collected for each participant from two sources. The SensiumVitals® vital sign  
37 data were documented at 2-minute intervals and collected from a hospital desktop computer using  
38 data-acquisition software developed by Sensium. These data had been pre-processed to discard  
39 signals that were subject to gross electrical or motion artefact (11). Patients were allowed to  
40 ambulate whilst wearing the monitoring patch; however, due to the major surgery they had  
41 undergone, most patients remained at their bedsides for the duration of their hospital stay.  
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44 NEWS data were collected at regular intervals, depending on the patients' status and based on the  
45 NEWS protocol(13). Typically, vital signs were collected at the bedside, with the patients either  
46 sitting or lying down, by members of the nursing staff who were blinded to the SensiumVitals® vital  
47 sign data: pulse rate was measured using the pulse oximeter on a multi-parameter portable vital  
48 signs monitor; temperature was measured using a tympanic thermometer; respiratory rate was  
49 measured manually. The NEWS scores and their component parts were documented electronically.  
50 Researchers collected manually-recorded heart rate, respiratory rate and temperature data from the  
51 hospital's electronic patient record. Other vital signs collected by the nursing staff as part of the  
52 early warning score, such as oxygen saturations, were not extracted.  
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### 57 2.4 Data processing

58 The two data sources were linked using NHS number and timestamp and consolidated into a single  
59 deidentified spreadsheet. Paired data to a NEWS observation was derived from the SensiumVitals®  
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3 continuous data set by using the median vital sign value within a  $\pm 10$ -minute window of a manually-  
4 recorded observation. The time window was used to account for differences between the nurses'  
5 manually-documented times and the automatic timestamps from the vital sign patch. The median  
6 value within this window was used to eliminate the impact of intermittent sensor noise.  
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## 9 2.5 Outcomes

11 The primary outcomes were the 95% limits of agreement between manual nurse observations and  
12 wearable vital sign patch recordings of Heart Rate (HR), Respiratory Rate (RR) and Temperature  
13 (Temp). Following precedent, we defined clinical acceptability to be *max*  $\pm 10\%$  for HR and RR (or  $\pm 3$   
14 breaths per minute or  $\pm 5$  beats per minute) and  $0.5^\circ\text{C}$  for Temp (14,15). The secondary outcome was  
15 the average percentage completeness of continuous patch data.  
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## 18 2.6 Statistical Analysis

19 For each vital sign, we first visually inspected the paired vital sign measurements via scatter plots, in  
20 addition to the raw time series vital signs from the Sensium patch.  
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23 Measurements were then formally compared using Bland-Altman analysis. In this analysis, the mean  
24 difference between the SensiumVitals® data and the nurse observations and the 95% Limits of  
25 Agreement are calculated. We adjusted for multiple measurements from the same subject using a  
26 model in which time of measurement is modelled as a random effect(16). This avoids bias caused by  
27 differences in number of measurements per patient. We also reported the Pearson correlation  
28 coefficient and the root mean squared (RMS) error for each vital sign.  
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31 In secondary analysis, we first assessed the average percentage completeness of the continuous  
32 patch data per patient. The numerator was defined as the number of two-minute periods in which  
33 vital sign data were provided by the patch. The denominator was the number of 2-minute periods  
34 that span the time during which the patch was transmitting data. These time points were preferred  
35 to admission and discharge from ward times because the patch may not have been worn for the  
36 patient's entire ward admission. In sensitivity analyses, we repeated both the Bland-Altman  
37 analyses using  $\pm 2$  and  $\pm 2$  minute windows of continuous data.  
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40 Analyses were undertaken using MATLAB R2017b (The MathWorks Inc., Massachusetts, USA) and  
41 the R Methcomp package (17,18).  
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## 48 3. Results

49 Fifty one patients were recruited to the intervention arm of the TRaCINg study between October  
50 2017 and April 2018. The median number of manually-recorded observation sets was 19 per patient  
51 (range 2 to 73 sets of vital signs measurements). There were 1,135 nurse observations available for  
52 analysis. All observations had a documented heart rate. Four observations had missing  
53 observations, 1 for respiratory rate and 3 for temperature. Vital sign traces for one participant over  
54 the course of their entire hospital stay are shown in Figure 2.  
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### 3.1 Heart Rate

Figure 3 shows the scatterplot of nurse-recorded heart rate against the SensiumVitals® patch. There is reasonable correlation between the two measurements ( $R^2 = 0.67$ ,  $p < 0.001$ ). The mean and (standard deviation) for manual and wearable heart rates are 81.6 (16.2) beats per minute (bpm) and 84.3 (19.3) bpm, respectively. The mean percentage completeness of continuous patch data for heart rate was 59.2%. In addition, visual inspection of the example vital sign traces show good agreement between the measurements. The Bland-Altman bias (Figure 4) was 1.85 bpm, with 95% limits of agreement -23.92 to 20.22 bpm. The RMS error was 11.25 bpm. The limits of agreement and RMS error exceeded the acceptability criterion.

### 3.2 Respiratory Rate

Figure 5 shows the scatterplot of nurse-recorded respiratory rate against the SensiumVitals® patch data. There is no correlation between the two measurements methods ( $R^2 = 0.01$ ,  $p < 0.001$ ). The mean and standard deviation for manual and wearable respiratory rate were 17.6 (1.58) breaths per minute and 15.0 (5.5) breaths per minute, respectively. The mean percentage completeness of continuous patch data for respiratory rate data was 31.4%.

Visual inspection of the histogram for manually-recorded respiratory rate shows a large peak at 18 breaths per minute, and a secondary peak at 16 breaths per minute. This result is unexpected for a natural physiological parameter, which may be expected to vary smoothly over the full range of values. Indeed, the peaks do not appear on the vital sign patch histogram. Inspection of the vital sign patch histogram indicates a significant proportion of measurements between 5 and 10 breaths per minute. No manually-recorded respiratory rates were recorded in this range. The Bland-Altman bias (Figure 6) was 2.93 breaths per minute, with 95% limits of agreement -8.19 to 14.05 breaths per minute. The RMS error was 6.14 breaths per minute and the limits of agreement are wider than the pre-specified acceptable error of 3 breaths/min.

### 3.3 Temperature

Figure 7 is a scatterplot of temperatures recorded by nurses versus those measured by the SensiumVitals® patch. Histograms for each measurement method are presented alongside the x- and y- axes. There is low correlation between the two measurement methods ( $R^2 = 0.13$ ,  $p < 0.001$ ). The mean and (standard deviation) of manual temperature and wearable temperature were 37.1°C (0.5°C) and 36.4°C (1.0°C). Further inspection of the vital sign time series in Figures 1 and 2 shows multiple clinically implausible fluctuations of up to 2 °C within 2 hours within each time series. The mean percentage completeness of continuous patch data for temperature was 72.8%.

Initial visual inspection was therefore sufficient to show that the patch-derived temperature is not a suitable proxy for core temperature, as measured by tympanic thermometer. The Bland-Altman bias (Figure 8) was 0.82 °C, with 95% limits of agreement -1.13 °C to 2.78 °C. The RMS error was 1.28 °C. In addition to large systematic bias between the two methods, the limits of agreement did not meet the pre-defined clinical acceptability criterion (0.5°C).

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3 In a sensitivity analysis, all Bland-Altman analyses was repeated using  $\pm 2$  and  $\pm 5$  minute windows of  
4 vital sign patch data. There were no meaningful differences in the bias or limits of agreement  
5 [Supplementary Material].  
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## 12 4. Discussion

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14 In this 51-patient validation study, temperature, respiratory rate, and heart rate measurements  
15 obtained from a wearable vital sign patch were compared with manually-recorded observations by  
16 nursing staff. Whilst there was reasonable correlation between the two methods for heart rate  
17 measurements, there were large discrepancies in many instances, as indicated by the Bland Altman  
18 analysis. It is not clear whether there were errors in the manual observation, in the vital sign patch,  
19 or both. There was low correlation for respiratory rate and temperature. The differences between  
20 manual and vital sign patch measurements for all three measured vital signs were outside of  
21 acceptable limits.  
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25 An advantage of the study design is the collection of a large number of data points for analysis. The  
26 approach is clinically valid, as the NEWS system is the national standard for vital signs monitoring in  
27 the United Kingdom. The surgical patient population is a clinically relevant cohort. There are high  
28 rates of complications after major surgery (19), but many surgical complications, such as sepsis, are  
29 attenuated by early detection. By virtue of their suitability for surgery, patients experiencing severe  
30 complications are likely to be candidates for full active management and escalation of care. They  
31 are therefore a population likely to benefit from reliable continuous physiological monitoring.  
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35 There are few clinical evaluations of continuous vital signs monitoring in the literature. Previous  
36 validation studies have studied participants who are confined to their bed space by wired monitoring  
37 equipment (11,14). In the surgical setting, enhanced recovery programmes mandate early  
38 mobilisation after surgery. In this study, patients were allowed to ambulate freely as part of their  
39 usual postoperative care, which may have produced some motion artefact on the continuous  
40 monitoring data; this may explain why the findings from this study show worse correlation when  
41 compared to previous studies which compared two stationary measurements. The patch algorithms  
42 are designed to identify and reject physiological signals corrupted by significant sources of noise  
43 inherent to the ambulatory nature of wireless monitoring; however, it is possible that respiratory  
44 rate data may have shown artefact from speech.  
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50 The findings must be interpreted within the limitations of the study. There were a relatively small  
51 number of patients in the study. Data completeness from the vital sign patch was low, especially for  
52 respiratory rate, although results for heart rate and temperature were similar to previous work (14).  
53 The reference standard, whilst clinically relevant, is inherently flawed. Early warning scores such as  
54 NEWS are known to be limited by their user-dependent nature. Time and staffing pressures placed  
55 on nursing staff in an increasingly busy clinical environment may be driving the adoption of time-  
56 saving, less accurate techniques; in this study, heart rate was typically inferred from the pulse rate  
57 measured by a pulse oximeter, despite the fact that this is known to be less accurate than manual  
58 palpation of the radial pulse. In addition, manually-collected vital signs can be subject to the effects  
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3 of 'white-coat hypertension'; heart rate, respiratory rate and temperature can be elevated simply by  
4 the arousal effect of the nurse interaction (20).  
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6 Deficits in the manually-recorded observations were particularly evident in the analysis of  
7 respiratory rate. Analysis of the manually-recorded values alone revealed a statistically unlikely  
8 preponderance of 18 breaths per minute, with a secondary peak at 16 breaths per minute. These  
9 peaks were not visible for the vital sign patch, suggesting that this is a measurement artefact in the  
10 way that manual measurements are made, rather than a real effect. It has been well described that  
11 respiratory rate is often miscalculated or omitted when calculated early warning scores (21,22). It is  
12 also recognised that clinical staff detect patient status in advance of manual measurements for an  
13 early warning score system 'by using information not currently encoded within it.'  
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17 The patch data for respiratory rate is also unlikely to be reliable, as a significant proportion of  
18 measurements were between 5 and 10 breaths per minute. This proportion of low values is much  
19 greater than those described in previously derived distributions from larger populations (23). There  
20 are also rapid fluctuations in respiratory rate which are physiologically implausible and may have  
21 been affected by patient movement, speech or coughing.  
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24 The manually-recorded temperature measurements showed plausible distributions and are likely to  
25 be accurate. The high bias between the nurse-measured temperatures and the patch data can be  
26 explained by the difference in measurement techniques. The patch measures skin temperature  
27 which may not accurately reflect the tympanic temperature measured by the nursing staff. Skin  
28 temperature is highly dependent on environmental factors such as the ambient temperature,  
29 clothing and blankets.  
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32 The reliability of the continuous temperature measurement is, however, limited. The time series  
33 analysis shows evidence of regular patch disconnection, indicated by rapid drops in temperature  
34 followed by increases consistent with conductive heating, or warming back up. These warm-up  
35 periods render the raw signals unreliable, although this limitation may be overcome through better  
36 signal processing. For instance, Clifton et al. used Bayesian change point analysis to detect step  
37 changes in temperature across a large study population. A similar approach may be used to  
38 determine disconnection on an individual patient basis(24).  
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## 42 43 44 Conclusions

45 The differences between manual and vital sign patch measurements for all three measured vital  
46 signs were outside of acceptable limits. On some occasions, this may be due to artefact in the  
47 continuous signal; this could be overcome through better signal processing. Other discrepancies may  
48 be due to errors during manual measurement. Whilst acknowledging the time pressures placed on  
49 nursing staff, inaccuracies in the manually-recorded data present an opportunity to increase  
50 awareness about the importance of manual observations, particularly with regard to methods of  
51 manual heart rate and respiratory rate measurements.  
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## Figure legends

Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium, Abingdon, UK.

Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign values from the SensiumVitals® patch. The black markers show the median value of the SensiumVitals® vital signs (evaluated from  $\pm 10$  mins of the nurse observation time). The red markers show the manually-recorded vital signs. Where there is a wide difference between the red and black markers at a single time point, this indicates disagreement between the two vital signs measurement techniques.

Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate observations; bpm=beats per minute.

Figure 4: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.

Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate observations; rpm=respirations per minute.

Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated measures.

Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature observations.

Figure 8: Bland-Altman plot for temperature with limits of agreement adjusted for repeated measures.

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## Competing interests

There are no known conflicts of interest associated with this work and there has been no significant financial support for this work that could have influenced its outcome.

## Author contributions

CD, SN and DW were involved in the conception of the work. CD designed the study. DW provided methodological expertise. SN undertook the data collection. DW and CD performed the analysis and interpretation. CD and DW drafted the article. CD, SN, DW and DJ were involved in critical revision of the article and have given final approval of the version to be submitted.

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## Data sharing statement

Research materials related to this work can be accessed on request from the corresponding author.

## References

1. Downey CL, Tahir W, Randell R, Brown JM, Jayne DG. Strengths and limitations of early warning scores: A systematic review and narrative synthesis. Vol. 76, *International Journal of Nursing Studies*. 2017. p. 106–19.
2. Cardona-Morrell M, Prgomet M, Turner RM, Nicholson M, Hillman K. Effectiveness of continuous or intermittent vital signs monitoring in preventing adverse events on general wards: a systematic review and meta-analysis. Vol. 70, *International Journal of Clinical Practice*. 2016. p. 806–24.
3. DeVita MA, Smith GB, Adam SK, Adams-Pizarro I, Buist M, Bellomo R, et al. Identifying the hospitalised patient in crisis. A consensus conference on the afferent limb of Rapid Response Systems. *Resuscitation*. 2010;81(4):375–82.
4. Bonnici T, Tarassenko L, Clifton D, Watkinson P. The digital patient. *Clin Med (Northfield Ill)*. 2013;13(3):252–7.
5. Michard F. A sneak peek into digital innovations and wearable sensors for cardiac monitoring. *J Clin Monit Comput*. 2017 Apr;31(2):253–9.
6. Hofmann B, Welch H. New diagnostic tests: more harm than good. *Br Med J*. 2017;358:j3314.
7. Downey C, Randell R, Brown J, Jayne DG. Continuous Versus Intermittent Vital Signs Monitoring Using a Wearable, Wireless Patch in Patients Admitted to Surgical Wards: Pilot Cluster Randomized Controlled Trial. *J Med Internet Res [Internet]*. 2018 Dec 11;20(12):e10802. Available from: <https://www.jmir.org/2018/12/e10802/>
8. Downey CL, Brown JM, Jayne DG, Randell R. Patient attitudes towards remote continuous vital signs monitoring on general surgery wards: An interview study. *Int J Med Inform*. 2018;114.
9. Hernandez-Silveira M, Wieczorkowski-Rettinger K, Ang S, Burdett A. Preliminary assessment of the SensiumVitals®: A low-cost wireless solution for patient surveillance in the general wards. *Proc Annu Int Conf IEEE Eng Med Biol Soc EMBS*. 2015;2015–Novem:4931–7.
10. Backed I, Evidence BY. Sensium Whitepaper - The Deteriorating Patient. :1–5.
11. Hernandez-Silveira M, Ahmed K, Ang S-S, Zandari F, Mehta T, Weir R, et al. Assessment of the feasibility of an ultra-low power, wireless digital patch for the continuous ambulatory monitoring of vital signs. *BMJ Open*. 2015;5(5).
12. Downey CL, Croft J, Buckley H, Randell R, Brown JM, Jayne DG. Trial of Remote Continuous versus Intermittent NEWS monitoring after major surgery (TRaCINg): protocol for a feasibility randomised controlled trial. *Pilot Feasibility Stud*. 2018;4(1):112.
13. Royal College of Physicians. National Early Warning Score (NEWS) 2: Standardising the assessment of acute-illness severity in the NHS. Updated report of a working party. 2017.
14. Breteler MJM, Huizinga E, van Loon K, Leenen LPH, Dohmen DAJ, Kalkman CJ, et al. Reliability of wireless monitoring using a wearable patch sensor in high-risk surgical patients at a step-down unit in the Netherlands: a clinical validation study. *BMJ Open [Internet]*. 2018 Feb 1;8(2). Available from: <http://bmjopen.bmj.com/content/8/2/e020162.abstract>
15. Niven D, Gaudet J, Laupland K, Mrklas K, Roberts D, Stelfox H. Accuracy of peripheral

- 1  
2  
3 thermometers for estimating temperature: A systematic review and meta-analysis. *Ann*  
4 *Intern Med* [Internet]. 2015 Nov 17;163(10):768–77. Available from:  
5 <http://dx.doi.org/10.7326/M15-1150>  
6
- 7 16. Carstensen B, Simpson J, Gurrin LC. Statistical models for assessing agreement in method  
8 comparison studies with replicate measurements. *Int J Biostat*. 2008;4(1).  
9
- 10 17. Carstensen B, Gurrin L, Ekstrom C, Figurski M. MethComp: functions for analysis of  
11 agreement in method comparison studies. 2015. p. R package version 1.22.2.  
12
- 13 18. R Core Team. R: A language and environment Statistical, statistical computing. 2018. p. R  
14 Foundation Computing, Vienna, Austria.  
15
- 16 19. The International Surgical Outcomes Study Group. Global patient outcomes after elective  
17 surgery: prospective cohort study in 27 low-, middle-, and high-income countries. *Br J*  
18 *Anaesth*. 2016;117:601–9.  
19
- 20 20. Franklin SS, Thijs L, Hansen TW, O'Brien E, Staessen JA. White-coat hypertension: new insights  
21 from recent studies. *Hypertension*. 2013;62(6):982–7.  
22
- 23 21. Nwulu U, Westwood D, Edwards D, Kelliher F, Coleman J. Adoption of an electronic  
24 observation chart with an integrated early warning scoring system on pilot wards: a  
25 descriptive report. *Comput Informatics, Nurs*. 2012;30(7):371–9.  
26
- 27 22. Ludikhuizen J, Smorenburg S, de Rooij S, de Jonge E. Identification of deteriorating patients on  
28 general wards; measurement of vital parameters and potential effectiveness of the Modified  
29 Early Warning Score. *J Crit Care*. 2012;27(4):424.e7-13.  
30
- 31 23. Tarassenko L, Clifton DA, Pinsky MR, Hravnak MT, Woods JR, Watkinson PJ. Centile-based  
32 early warning scores derived from statistical distributions of vital signs. *Resuscitation*  
33 [Internet]. 2011;82(8):1013–8. Available from:  
34 <http://www.sciencedirect.com/science/article/pii/S030095721100195X>  
35
- 36 24. Clifton DA, Wong D, Clifton L, Wilson S, Way R, Pullinger R, et al. A Large-Scale Clinical  
37 Validation of an Integrated Monitoring System in the Emergency Department. *IEEE J Biomed*  
38 *Heal Informatics*. 2013;17(4):835–42.  
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Figure 1: The SensiumVitals® monitoring patch. Image reproduced with permission from Sensium, Abingdon, UK.

451x300mm (72 x 72 DPI)

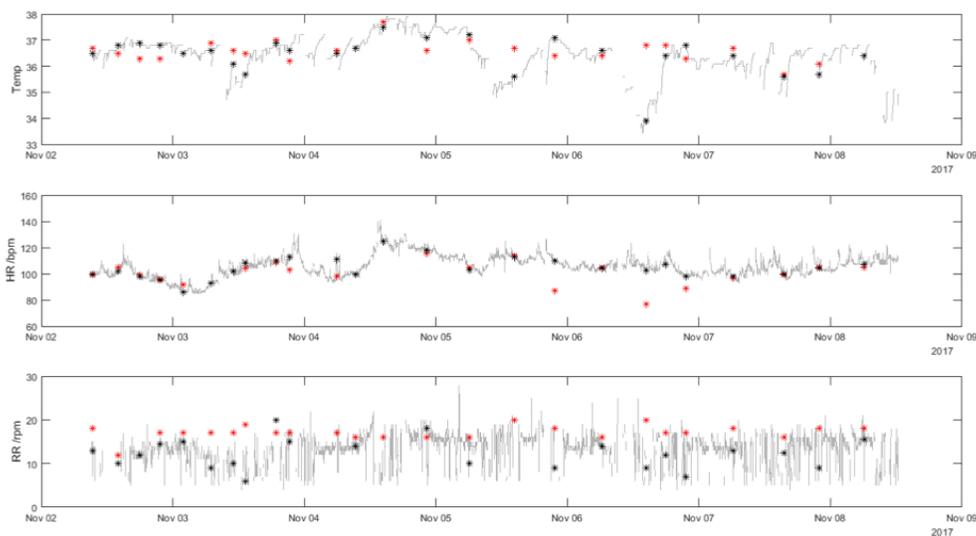


Figure 2: Vital signs data for a single participant. The grey lines show the minute-by-minute vital sign values from the SensiumVitals® patch. The black markers show the median value of the SensiumVitals® vital signs (evaluated from +/-10 mins of the nurse observation time). The red markers show the manually-recorded vital signs. Where there is a wide difference between the red and black markers at a single time point, this indicates disagreement between the two vital signs measurement techniques.

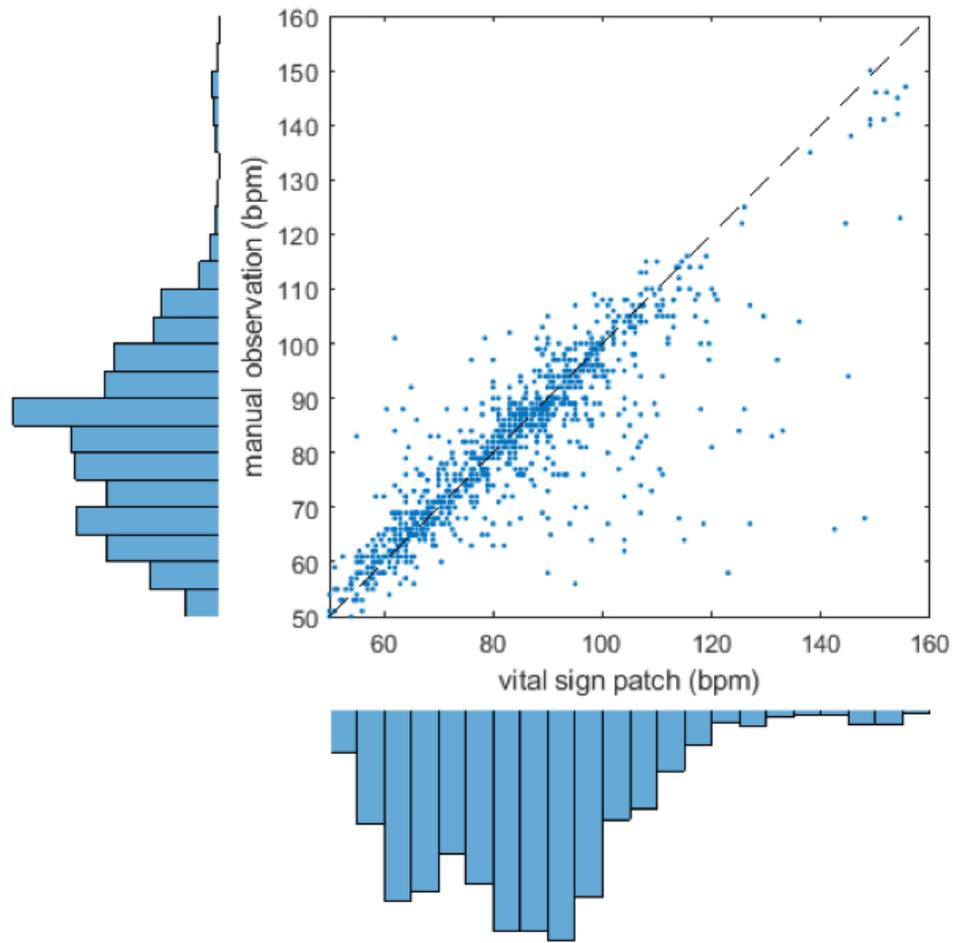


Figure 3: Scatter plot and marginal histogram of paired manual and SensiumVitals® heart rate observations; bpm=beats per minute.

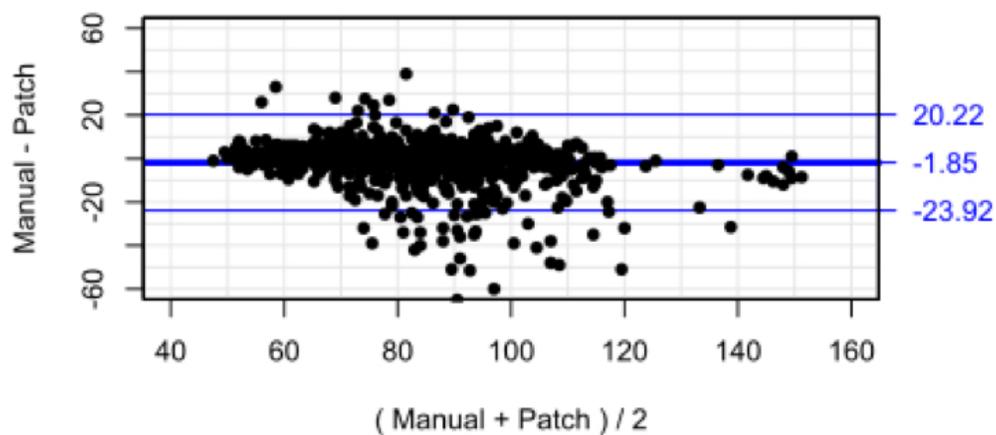


Figure 4: Bland-Altman plot for heart rate with limits of agreement adjusted for repeated measures.

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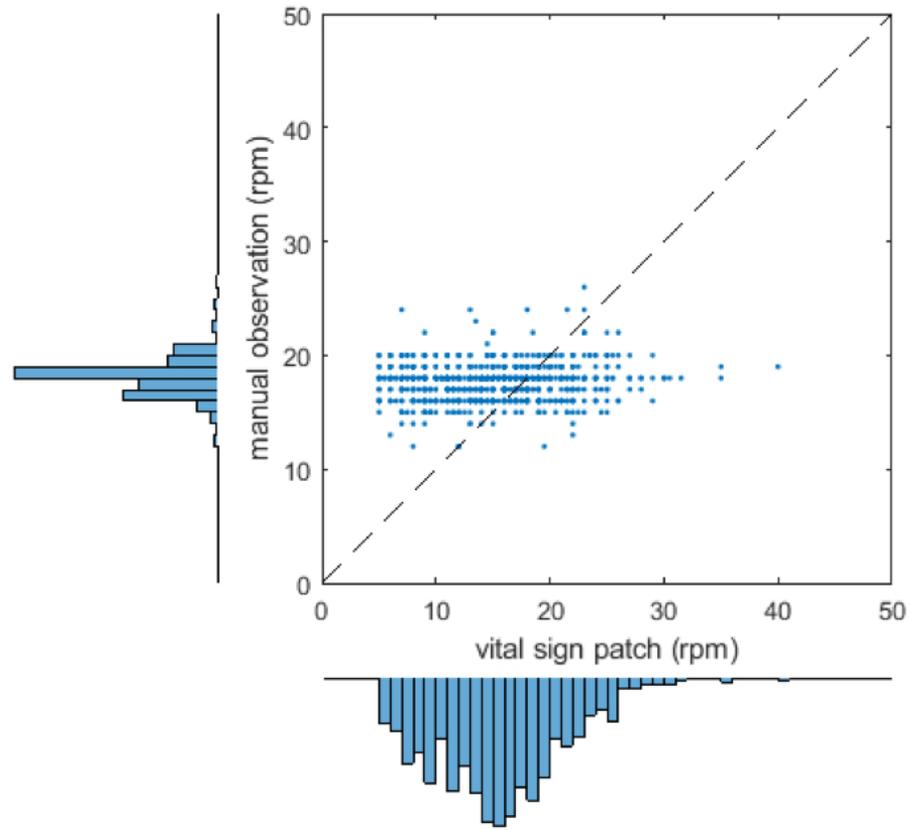


Figure 5: Scatter plot and marginal histogram of paired manual and SensiumVitals® respiratory rate observations; rpm=respirations per minute.

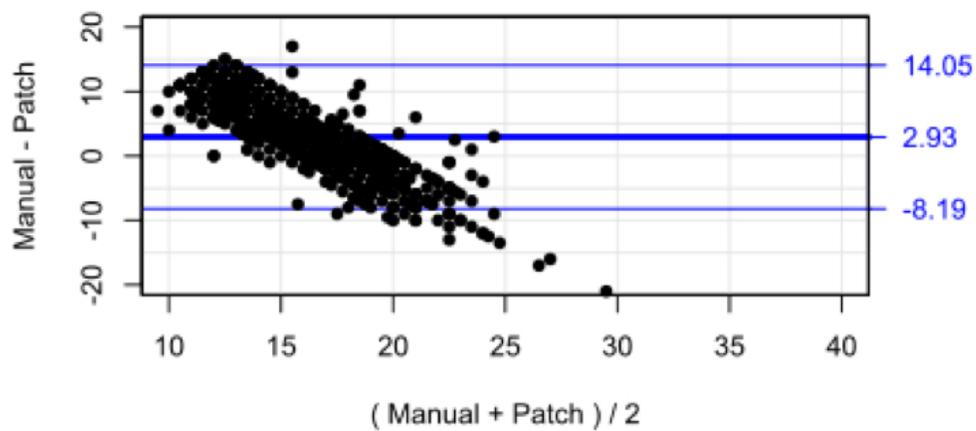


Figure 6: Bland-Altman plot for respiratory rate with limits of agreement adjusted for repeated measures.

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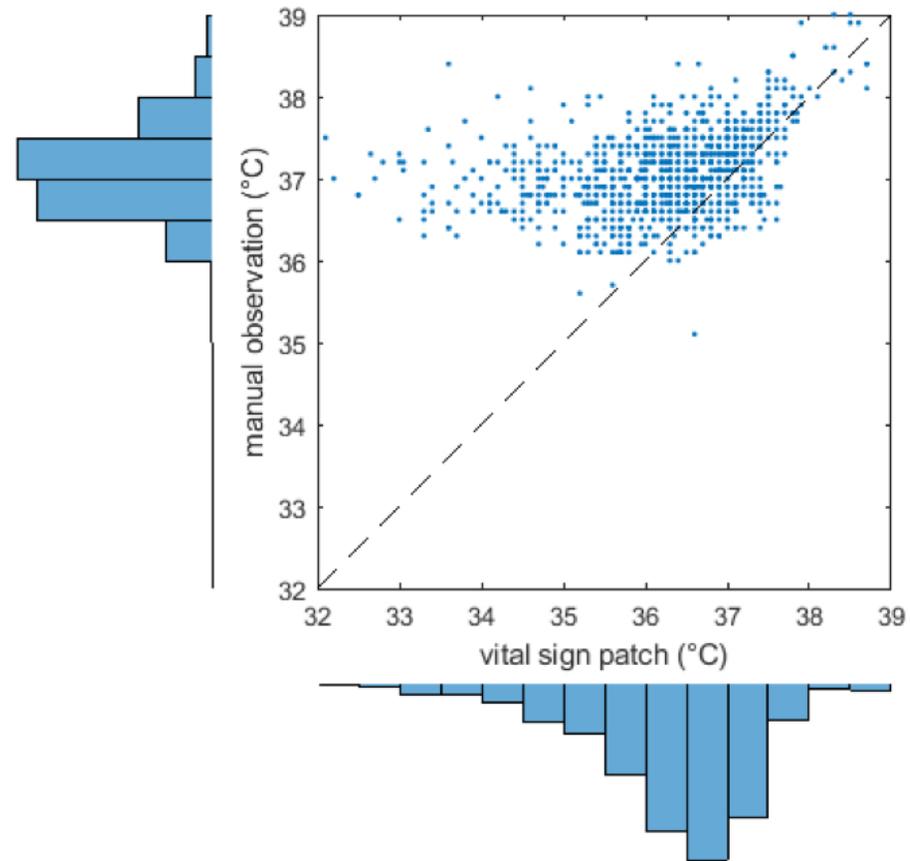


Figure 7: Scatter plot and marginal histogram of paired manual and SensiumVitals® temperature observations.

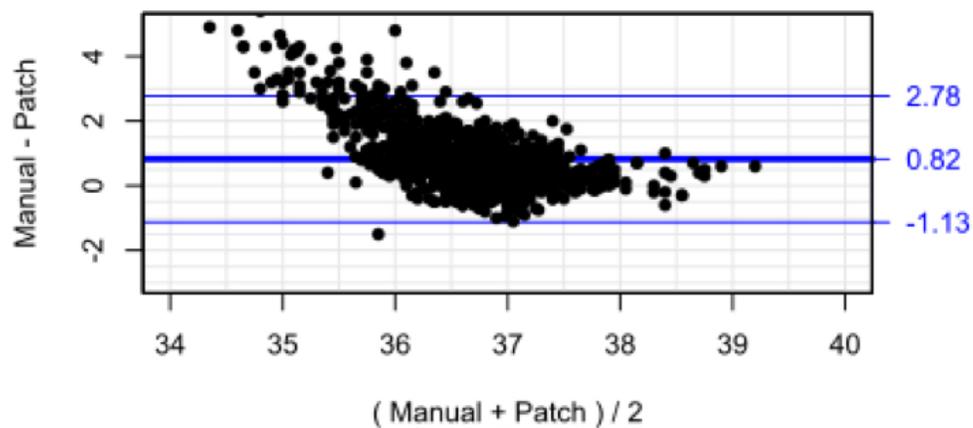


Figure 8: Bland-Altman plot for temperature with limits of agreement adjusted for repeated measures.

## Supplementary Materials

## Sensitivity analysis

Window size	HR (n = 1135)	RR (n = 1134)	Temp (n = 1132)
±2 mins	306	630	212
±5 mins	249	392	174
±10 mins	232	286	147

Missing pairs of data (i.e. no data within n minute window of nurse observation)

Window size	HR (bias, LoA)	RR (bias, LoA)	Temp (bias, LoA)
±2 mins	- 2.74 (-25.39, 19.91)	3.07 (-9.05 to 15.20)	0.82 (-1.21 to 2.86)
±5 mins	-2.35 (-24.68 to 19.98)	3.13 (-8.64 to 14.90)	0.82 (-1.23 to 2.87)
±10 mins	- 1.85 (-23.92 to 20.22)	2.93 (-8.19 to 14.05)	0.82 (-1.13 to 2.78)

Bland-Altman bias and 95% limits of agreement for ±2, ±5, ±10 window lengths of continuous vital sign patch data