

1 Accurate whole-night sleep monitoring with
2 dry-contact ear-EEG

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13 **A Supplementary Methods: Feature description**

14 In the following, the estimated power spectral density will be known as 'P', and
15 $P(f)$ or $P([a, b])$ will be taken to mean the estimated power at frequency f , or the
16 total power in frequency band a to b Hz.

17 **A.1 EEG time domain proxies**

18 **F1 - Signal Skewness:** Skewness is the 3rd order moment of the signal which
19 measures the asymmetry of the signal's probability distribution about the
20 mean. Signal skewness is expected to be lower in deep sleep.

21 **F2 - Signal kurtosis:** Signal kurtosis is a measure of the 'tailedness' of the sig-
22 nal, also known as 4rd order moment of the signal. This feature is also a
23 widely used feature to discriminate between sleep stages.

24 **F3 - Zero crossing rate:** Number of times the signal crosses the reference line.
25 Zero crossing rate is known to be quite useful in detection of transient waves
26 like sleep spindles.

27 **F4 - Hjorth mobility:** The ratio between the standard deviation of the signal
28 and its first derivative. This feature provides information about frequency
29 content of the signal and the dominating frequency components.

30 **F5 - Hjorth complexity:** This feature measures how similar the shape of a sig-
31 nal is to a pure sine wave.

32 **F6 - 75th percentile:** The value below which exactly 75% of the measured val-
33 ues fall.

34 **F7 - Channel correlation:** This feature measures the Pearson correlation coef-
35 ficient between ear-EEG derivations. It is the only feature which requires
36 multiple channels and is calculated for all pairs of derivations (in our case
37 there are 3 derivations).

38 **A.2 EMG proxy**

39 These features are calculated based on a 32-80 Hz band-pass filtered version of the
40 original signal.

41 **F8 - EMG power:** Total power in the 32-80 Hz band. This is useful in identifi-
42 cation of the deeper levels of sleep where there is less high frequency activity.

43 **F9 - Minimal EMG power:** This was calculated by dividing each epoch into
44 10 segments and finding the minimum integrated EMG power among these
45 segments.

46 **F10 - Relative EMG burst amplitude:** Is calculated by dividing Maximum
47 EMG signal amplitude by F9.

48 **A.3 EOG proxy**

F11 - Slow eye movement power:

$$F11 = \frac{P([0.5, 2])}{P([0.5, 30])}$$

F12 - Rapid eye movement power:

$$F11 = \frac{P([2, 5])}{P([0.5, 30])}$$

49 **A.3.1 EEG Frequency Domain**

50 In the following, the $\alpha, \beta, \theta, \delta$ bands are defined as, 8-16 Hz, 16-32 Hz, 4-8 Hz and
51 .5-4 Hz, in accordance with [1]:

52 **F13-F16 - Relative power in $\alpha, \beta, \theta, \delta$ bands:** The power in each band related
53 to the total power in the 2-32 Hz frequency band.

54 **F17-F23 - Power ratios:** $\delta/\theta, \theta/\alpha, \alpha/\beta, \beta/\gamma, (\theta + \delta)/(\alpha + \beta)$: The relative power
55 between the specified frequency bands.

56 **F24 - Spectral edge frequency:** The frequency below which 95% of the spec-
57 tral power in the 2-32 Hz band is located.

58 **F25 - Median power frequency:** Is the frequency below which 50% of the spec-
59 tral power in the 2-32 Hz band is located.

60 **F26 - Mean spectral edge frequency difference:** The difference between spec-
61 tral edge frequency (F24) and median power frequency (F25). This feature
62 is successful in separating the REM stage. $F26 = F24 - F25$

63 **F27 - Peak power frequency:** The frequency with highest power in the 2-32
64 Hz band.

65 **F28 - Spectral Entropy:** Spectral Entropy measures the disorder in the power
66 spectral density of the 2-32 Hz frequency band. This feature was calculated
67 as:

$$F28 = - \sum_i P(f_i) \ln(P(f_i)) ,$$

68 with f_i running over all frequency bins P .

69 **A.4 Sleep event proxy**

F29 - Spindle probability: This feature introduces a spectral mean frequency measure, inspired by [2]. It is calculated as

$$F29 = \frac{\max(P(11 - 16))}{\langle P(4 - 10) \rangle + \langle P(20 - 30) \rangle}$$

70 where $P(x-y)$ is the set of power estimates for the $[x, y]$ Hz frequency band.

71 **F30: Frequency stationarity:** Each epoch was divided into 31 segments and
72 the periodogram was calculated for each segment. Then, frequency station-
73 arity was computed as the average Pearson correlation between these 31
74 spectra.

75 **F31 - Lowest adj. frequency similarity:** Using the same 31 spectra from F14,
76 F15 was calculated as the lowest Pearson correlation between neighboring
77 segments.

78 **F32 - Maximum B-spline transform:** Maximum absolute value of a contin-
79 uous wavelet transform of the EEG signal. The wavelet type is complex
80 B-spline wavelet with a support of 0.5 s. This feature is successful in detect-
81 ing sleep spindles and inspired by [3].

82 **F33 - Longest sleep spindle** In order to compute this feature, a spindle detec-
83 tion method inspired by [4] was employed. In this method, Teager Energy
84 Operator (TEO) was applied to the 11-16 Hz band pass filtered signal. Con-
85 currently, $P([12, 14]) / (P([4, 11]) + P([13, 32]))$ was computed by using a Short
86 Time Fourier Transform (STFT) applied to the unfiltered data. Finally, a

87 wavelet transform (WT) using B-spline wavelet like F32 was performed. The
88 segments of signal in which $WT > 15$, $TEO > 0.5$ and the STFT power ra-
89 tio > 0.3 were detected as sleep spindles. F33 was computed as the longest
90 length of the detected spindles.

91 **A.5 CWT based features**

92 All the features in this section were computed using the Continuous Wavelet Trans-
93 form (CWT) with a Morse wavelet with parameters (3,60). The traditional fre-
94 quency bands were defined as δ : 0.5-4 Hz, θ : 4-8 Hz, α : 8-12, β : 12-32 Hz and γ :
95 32-100 Hz.

96 **F54-F58 - Power entropy in $\gamma, \alpha, \beta, \theta, \delta$ bands:** The Shannon entropy of the
97 traditional frequency bands.

98 **F59-F63 - Duration of the activation in $\gamma, \alpha, \beta, \theta, \delta$ bands:** Duration of the
99 activation feature, defined as the period where the mean power in each
100 frequency band is higher than a threshold. This threshold is selected as
101 $1.5 \cdot (\text{median power in } 0.5\text{-}100 \text{ Hz})$.

102 **F64-F68 - 75 percentile in $\gamma, \alpha, \beta, \theta, \delta$ bands:** The frequency below which
103 75% of the spectral power in each band is located.

104 **F69-F73 - Relative power in $\gamma, \alpha, \beta, \theta, \delta$ bands:** The ratio of mean power in
105 each band to mean power in 0.5-100 Hz.

106 **F74-F77 - Power ratios in $\gamma, \alpha, \beta, \theta, \delta$ bands:** The ratio of mean power in neigh-
107 bouring frequency bands.

108 **A.6 Non-linear features**

109 **F78-F82 - Multi scale entropy 1-5:** Multi Scale Entropy (MSE) is based on
110 sample entropy to compute the entropy over multiple time scales [5]. This
111 feature has been used in several sleep staging studies before [6, 7]. MSE was
112 computed for 5 scales in this study resulting in features F78-F82.

113 **F83 - Lempel-Ziv complexity:** Lempel-ziv complexity (LZC) is a nonparamet-
114 ric complexity measure that has been applied to solve many different prob-
115 lems including sleep stage classification [8, 9]. It has been found to be effec-
116 tive in separating N1 and REM stages [8].

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