

Supplemental Material

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Overview of CNN Model for detection of patients with an LVEF of $\leq 35\%$ using the ECG signal

As previously described,^{1,2} a convolutional neural network (CNN) trained with Keras with a Tensorflow (Google, Mountain View, CA) backend was developed and validated. The only model input reported was a 12-lead ECG. Each 12-lead ECG was a matrix with 12 x 5000 matrix (i.e., 12 leads by 10 seconds duration sampled at 500 Hz) divided to 2 seconds segments with an overlap of one second.³ The network was composed of 6 single lead convolutional layers, each of which was followed by a non-linear “Relu” activation function, a batch-normalization layer⁴ and a max pooling layer⁵. The features extracted from each raw, digital signal ECG lead were fused in another convolutional layer that had access to all leads simultaneously. Following the last convolutional layer, the data were fed to a fully connected network with two hidden layers with dropout layers to avoid overfitting and an output layer that was activated using the “Softmax” function.⁶ The outputs of the softmax layer were compared with the actual label (EF $\leq 35\%$, or EF $>35\%$) and by using an “Adam” optimizer, the different layers were trained to classify each ECG to one of the EF groups. During training, the network was given the actual EF label, whereas during the testing and validation stages, the network was blinded from the EF value, and the model output was compared to the actual EF class (EF $\leq 35\%$, or EF $>35\%$) after the model was run for each ECG sample. While the outcome used to train the model is binary (EF $\leq 35\%$ or EF $>35\%$), the network output is a continuous number between zero and one

24 that represent the probability of the binary outcome ($EF \leq 35\%$). As the output is
25 continuous, the final decision is made by selecting a threshold and testing if the output is
26 above or below that threshold. All possible thresholds with the attendant sensitivity and
27 specificity are displayed in the receiver-operating curve.

28 **References:**

- 29 1. Attia ZI, Kapa S, Yao X, Lopez-Jimenez F, Mohan TL, Pellikka PA, Carter RE, Shah ND, Friedman PA
30 and Noseworthy PA. Prospective validation of a deep learning electrocardiogram algorithm for
31 the detection of left ventricular systolic dysfunction. *J Cardiovasc Electrophysiol.* 2019;30(5):668-
32 674.
- 33 2. Attia ZI, Kapa S, Lopez-Jimenez F, McKie PM, Ladewig DJ, Satam G, Pellikka PA, Enriquez-Sarano
34 M, Noseworthy PA, Munger TM, Asirvatham SJ, Scott CG, Carter RE and Friedman PA. Screening
35 for cardiac contractile dysfunction using an artificial intelligence-enabled electrocardiogram. *Nat*
36 *Med.* 2019;25:70-74.
- 37 3. van Rossum G. Python tutorial, Technical Report CS-R9526. 1995.
- 38 4. Ioffe S and Szegedy C. Batch normalization: accelerating deep network training by reducing
39 internal covariate shift Paper presented at: International Conference on Machine Learning;
40 2015.
- 41 5. Nagi J, Ducatelle F, Di Caro G, Ciresan D, Meier U, Giusti A, Nagi F, Schmidhuber J and
42 Gambardella L. Max-pooling convolutional neural networks for vision-based hand gesture
43 recognition. Paper presented at: 2011 IEEE International Conference 2011.
- 44 6. Cristianini N and Shawe-Taylor J. New York, NY: Cambridge University Press; 1999.

45